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## A Meta-Analysis of the Effects of Aging on Motor Cortex Neurophysiology Assessed by Transcranial Magnetic Stimulation

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### Abstract

**Objective**—Transcranial magnetic stimulation (TMS) is a non-invasive tool used for studying cortical excitability and plasticity in the human brain. This review aims to quantitatively synthesize the literature on age-related differences in cortical excitability and plasticity, examined by TMS.

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**Methods**—A literature search was conducted using MEDLINE, Embase, and PsycINFO from 1980 to December 2015. We extracted studies with healthy old (50–89 years) versus young (16–49 years) individuals that utilized the following TMS measures: resting motor threshold (RMT), short-interval cortical inhibition (SICI), short-latency afferent inhibition (SAI), cortical silent period (CSP), intracortical facilitation (ICF), and paired associative stimulation (PAS).

**Results**—We found a significant increase in RMT ( $g = 0.414$ , 95% confidence interval (CI) [0.284, 0.544],  $p < 0.001$ ), a significant decrease in SAI ( $g = 0.778$ , 95% CI [0.478, 1.078],  $p < 0.001$ ), and a trending decrease in LTP-like plasticity ( $g = -0.528$ , 95% CI [-1.157, 0.100]  $p < 0.1$ ) with age.

**Conclusions**—Our findings suggest an age-dependent reduction in cortical excitability and sensorimotor integration within the human motor cortex.

**Significance**—Alterations in the ability to regulate cortical excitability, sensorimotor integration and plasticity may underlie several age-related motor deficits.

### Keywords

Aging; Transcranial Magnetic Stimulation; Motor Cortex; Cortical Plasticity; Cortical Excitability; Gamma-Amino Butyric Acid

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## 1 Introduction

Due to increases in life expectancy and aging of the baby boomer population, we will have more individuals reaching advanced old age than ever before. By 2050 the number of adults aged 65 years and over is estimated to reach nearly 1.5 billion world-wide, representing 16% of the world's population (NIH, 2011). With a rapidly aging global population the economic, societal, and personal costs of neurodegenerative and neuropsychiatric diseases are expected to spike. This will present a significant burden to families, support workers, and health care providers. An enhanced understanding of the impact of aging on cortical functioning may help provide more insight into age-related illnesses.

Normal aging is characterized by neurophysiological and neuroanatomical changes of the brain. These changes are thought to underlie the decline in sensorimotor control and function that can accompany advancing age. An inability to modulate cortical excitability is suggested to underlie several motor deficits that healthy older adults may experience in daily life such as the deterioration of fine motor skills (Calautti et al. , 2001), impaired coordination skills (Swinnen et al. , 1998, Serrien et al. , 2000, Heuninckx et al. , 2004), and a decline in reaction times (Bedard et al. , 2002).

The primary inhibitory neurotransmitter in the brain is gamma-aminobutyric acid (GABA). GABA plays a central role in mediating cortical excitability (DeFelipe et al. , 1986, Schieber et al. , 1993). Cortical pyramidal cell activity is modulated by excitatory inputs, excitatory post-synaptic potentials (EPSPs), and inhibitory inputs, inhibitory post-synaptic potentials (IPSPs) (Krnjevic, 1997). The inhibitory inputs are produced by GABAergic interneurons that terminate on these cells (Krnjevic, 1997). The selective attenuation of cortical pyramidal activity by inhibitory GABA interneurons is termed cortical inhibition (Daskalakis et al. , 2007). Recent studies suggest a direct correlation between a decreased ability to modulate

cortical inhibition and motor retardation in healthy older adults (Fujiyama et al. , 2012b, Heise et al. , 2013, Levin et al. , 2014).

GABAergic neurotransmission is also central to the induction and maintenance of neuroplasticity (Daskalakis et al. , 2007). The brain's ability to adapt to internal and external stimuli is dependent on neuroplasticity; a process by which the brain reorganizes and generates new neural pathways. The induction and maintenance of neuroplasticity is contingent upon activity-dependent alterations in synaptic strength (van Mier et al. , 1998, Daskalakis et al. , 2008). The most extensively studied forms of neural plasticity are: long-term potentiation (LTP) and long-term depression (LTD). LTP, the strengthening of neuronal connections in highly activated pathways, increases the likelihood of synaptic firing to additional stimuli; conversely LTD, the weakening of poorly activated pathways, reduces the likelihood of synaptic firing (Hebb, 1949). Age-related deficits in LTP-like plasticity may underlie motor learning deficits observed in healthy older adults.

Transcranial magnetic stimulation (TMS) is a non-invasive brain stimulation tool used to assess cortical excitability and plasticity, *in-vivo* (Rossini et al. , 2015). Two TMS paradigms used to index cortical inhibition are: short-interval cortical inhibition (SICI) (Kujirai et al. , 1993) and cortical silent period (CSP) (Cantello et al. , 1992). SICI is a paired-pulse TMS paradigm that requires the paired delivery of two TMS stimuli, whereby a subthreshold conditioning stimulus precedes a suprathreshold test stimulus by 1–4 ms (Kujirai et al. , 1993). In contrast, CSP is a single-pulse paradigm that requires the delivery of a suprathreshold TMS pulse to the contralateral motor cortex during voluntary contraction of the target muscle (Cantello et al. , 1992). The suprathreshold TMS pulse evokes a motor-evoked potential (MEP) followed by a period of suppressed electromyography (EMG) activity. The duration of the silent period is measured from the onset of the MEP to the return of EMG activity (Cantello et al. , 1992).

An extensive body of literature suggests SICI and CSP represent GABA<sub>A</sub> and GABA<sub>B</sub> inhibitory neurotransmission respectively. For instance, the pharmacological profiles of SICI and CSP differ greatly. Benzodiazepines (e.g. lorazepam) act as positive allosteric modulators at GABA<sub>A</sub> receptors and reliably facilitate SICI. Conversely baclofen, a GABA<sub>B</sub> receptor agonist, prolongs CSP duration (Paulus et al. , 2008). In addition to differing pharmacological profiles, GABA<sub>A</sub> receptor-mediated IPSP peaks at 20ms while the GABA<sub>B</sub> receptor-mediated IPSP peaks at 150–200ms; this corresponds to the time course of SICI and CSP duration (McCormick, 1989, Davies et al. , 1990, Sanger et al. , 2001).

As well as cortical inhibition, TMS protocols are used to index cortical excitability. Cortical excitability can be assessed using the following TMS paradigms: resting motor threshold (RMT) and intracortical facilitation (ICF). The RMT measures general neuronal membrane excitability and is defined as the minimum intensity that evokes an MEP > 50µV in a muscle at rest in 5 out of 10 trials (Rossini et al. , 1994). ICF is a paired-pulse TMS paradigm that involves the paired delivery of a subthreshold conditioning stimulus preceding a suprathreshold test stimulus by 10–25ms, resulting in MEP facilitation (Kujirai et al. , 1993, Nakamura et al. , 1997). Pharmacological studies suggest ICF indexes N-methyl-D-aspartate (NMDA) glutamate-mediated excitatory neurotransmission (Paulus et al. , 2008).

Paired associative stimulation (PAS) is a TMS paradigm used to induce LTP and LTD-like cortical plasticity. PAS involves pairing repetitive, low-frequency peripheral median nerve stimulation (MNS) with TMS stimulation to the motor cortex. To induce potentiation of cortico-motor excitability (LTP-like plasticity) the MNS must precede the TMS stimulus by an interstimulus interval (ISI) of 25ms; to induce depression (LTD-like plasticity) the MNS must precede the TMS stimulus by 10ms (Stefan et al. , 2000, Weise et al. , 2013).

Glutamatergic NMDA receptors represent the molecular basis of LTP and LTD (Miyamoto, 2006, Zorumski et al. , 2012). PAS-induced facilitation of cortical excitability is critically dependent on NMDA receptor function. For example, blockade of NMDA receptors prevents PAS-induced facilitation of cortico-motor excitability (Ridding et al. , 2010). Therefore, PAS-induced cortical plasticity, LTP, and LTD are thought to rely on shared neuronal mechanisms (Luscher et al. , 2012). This review will quantitatively assess the effect of age on PAS-induced LTP-like plasticity.

The impact of age on sensorimotor integration can be evaluated using the TMS paradigm short-latency afferent inhibition (SAI). SAI requires median nerve stimulation paired with a single TMS pulse to the motor cortex. If the ISI is 20ms, the afferent nerve conditioning produces a marked decrease in EMG activity from the single TMS pulse (Classen et al. , 2000, Tokimura et al. , 2000). At the biological level, SAI is thought to primarily index cholinergic transmission. For example, scopolamine, a muscarinic acetylcholine receptor antagonist, selectively reduces the SAI cortical response in healthy subjects (Di Lazzaro et al. , 2000).

A limited number of TMS studies have examined the impact of healthy aging on cortical excitability and plasticity in healthy older adults. The trends in the current literature remain inconclusive and a synthesis of findings is lacking. Thus, we undertook a meta-analysis to quantitatively synthesize the literature on TMS measures of cortical excitability and plasticity in healthy older adults compared to younger adults - refer to Table 1 for an overview of the included TMS studies.

## 2 Methods

### 2.1 Data Sources

A literature search was conducted using MEDLINE, EMBASE, and PsycINFO from 1980 through December 2015. This search was supported by a hand search of bibliographies. Please refer to the Supplementary File for a description of the exact terms used in the literature search.

### 2.2. Inclusion Criteria

Selected studies had to meet the subsequent inclusion criteria:

1. Studies assessed one or more of the following TMS measures in the left motor cortex: RMT, SIC1, SAI, CSP, ICF, and/or PAS.
2. To be consistent, we used studies that used the right hand muscles for EMG recordings.

3. Studies included a healthy old (≥ 50 years) and healthy young (< 50 years) group.
4. Studies provided adequate data to perform a Hedge's *g* analysis: mean, standard deviation (SD), and sample size of groups.
5. The manuscript was written in English and had a minimum sample size of more than three participants in order to calculate the effect size.

There is no universal definition of old age because the definition is context-dependent. The majority of the included studies used a cut off between 50 and 60 years of age to delineate young versus old adults. Due to the limited number of studies on TMS and normal aging, we chose to delineate young and old adults at the age of 50 to include the maximum number of studies in our analyses.

### 2.3 Study Exclusion

The number of studies and reasons for exclusion were as follows: insufficient data (8), EMG recording from leg muscles (3), tested the right hemisphere (2), no young comparison group (1), and did not meet age range inclusion criteria (2). Refer to Figure 1 for the PRISMA flow diagram. We chose to exclude TMS studies examining interhemispheric inhibition to primarily focus on the effects of aging on the left motor cortex.

### 2.4 Handedness

The majority of the summarized studies included participants who were right-handed, thereby left-hemisphere dominant. Five of the 31 studies (Rossini et al. , 1992, Fujiyama et al. , 2011, Opie et al. , 2014, Young-Bernier et al. , 2014, Young-Bernier et al. , 2015) did not explicitly state the handedness of the participants. A total of three studies included both right and left-handed participants (Matsunaga et al. , 1998, Fujiyama et al. , 2009, Young-Bernier et al. , 2012b).

### 2.5 Data extraction

The data obtained from each study was as follows: (1) number of healthy old and young participants, (2) the mean and SD of the outcome measure. If the published content provided insufficient data for the quantitative analysis, the corresponding authors were contacted to request additional data.

### 2.6 Quantitative Analysis

**2.6.1 Hedge's *G***—We used the Hedge's *g*, a standardized meta-analytic technique, to perform the quantitative analysis. For all included TMS measures the Hedge's *g* effect size, *p*-value, and 95% confidence interval (CI) were calculated (healthy older versus young adults) in a fixed effects model. The Comprehensive Meta-Analysis Version 3.0 (Biostat, Englewood, New Jersey) was used to conduct the analyses. The sample size of the individual studies influenced the weight given to their means and SDs in the analyses.

**2.6.2 Test of Publication Bias**—The *N* fail-safe value represents the amount of non-significant unpublished studies that would render the effect size non-significant (Møller et

al. , 2001). For all analyses, a p-value of 0.05, 2-tailed was used. A minimum of three studies were required for the  $N$ fail-safe analysis.

**2.6.3 Test of Heterogeneity**—Clinical heterogeneity and methodological heterogeneity contribute to statistical heterogeneity. Statistical heterogeneity results in a greater difference between intervention effects than one would anticipate due to chance alone (2011). From here on statistical heterogeneity will be referred to as heterogeneity. We utilized the Cochran Q, p-value and  $I^2$  test to determine whether there are actual differences underlying the studies' results (heterogeneity), or whether the differences between findings were due to random error (homogeneity) alone. The Q statistic informs us of the presence versus absence of heterogeneity across studies (Huedo-Medina et al. , 2006). The power of the Cochran's Q is low when a small number of studies is used. In these circumstances, the  $I^2$  value is a more reliable measure for analyzing the heterogeneity in the included studies' results (Higgins et al. , 2003). The  $I^2$  statistic quantifies the degree of heterogeneity present across studies (Higgins et al. , 2002, Higgins et al. , 2003). The  $I^2$  value is a percentage and ranges from no heterogeneity (0%) to high heterogeneity (100%) (Ried, 2006).

### 3 Results

#### 3.1 Impact of age on RMT

Older adults demonstrated significantly greater RMT values compared to young adults. This analysis compared 485 older to 453 young adults from a total of 29 studies. The Hedge's g value was  $g=0.414$ , 95% CI [0.284, 0.544],  $p<0.001$ . The test of heterogeneity reached statistical significance ( $Q=70.101$ ,  $df(Q)=28$ ,  $p<0.001$ ,  $I^2=60.06$ ), indicating that the variation across studies was mostly due to heterogeneity not chance. The  $N$ -failsafe value was 269 unpublished studies. Refer to Fig. 2 for the Hedge's g forest plot for RMT comparing older versus young adults (Rossini et al. , 1992, Matsunaga et al. , 1998, Kossev et al. , 2002, Sale et al. , 2005, Hortobagyi et al. , 2006, Muller-Dahlhaus et al. , 2008, Tecchio et al. , 2008, Fujiyama et al. , 2009, Pellicciari et al. , 2009, Rogasch et al. , 2009, Smith et al. , 2009, Cirillo et al. , 2010, Fathi et al. , 2010, Cirillo et al. , 2011, Clark et al. , 2011, Degardin et al. , 2011, Fujiyama et al. , 2011, Levin et al. , 2011, Saisanen et al. , 2011, Smith et al. , 2011a, Smith et al. , 2011b, Bernard et al. , 2012, Fujiyama et al. , 2012a, Fujiyama et al. , 2012b, Young-Bernier et al. , 2012a, Cuypers et al. , 2013, Hinder et al. , 2013, Opie et al. , 2014, Young-Bernier et al. , 2014).

#### 3.2 Impact of age on SICI

Older adults showed a slight reduction in SICI compared to young adults, however this was not statistically significant. This analysis compared 187 older to 169 young adults from a total of 11 studies (Rogasch et al. , 2009, Smith et al. , 2009, Cirillo et al. , 2010, Cirillo et al. , 2011, Fujiyama et al. , 2011, Marneweck et al. , 2011, Saisanen et al. , 2011, Smith et al. , 2011b, Fujiyama et al. , 2012b, Hinder et al. , 2013, Opie et al. , 2014). The Hedge's g was  $g=0.063$ , 95% CI [-0.145, 0.271],  $p=0.550$ . Refer to Fig. 3 for the forest plot for the SICI Hedge's g analysis comparing older versus young adults. Although the Cochran's Q barely reached statistical significance ( $Q= 18.383$ ,  $df(Q)= 10$ ,  $p= 0.049$ , the  $I^2$  value (45.60) indicates that the inconsistency among studies was moderately large. Since there were no

significant differences observed between the two groups for SICI, the *N*-failsafe value was 0 unpublished studies.

### 3.3 Impact of age on SAI

Older adults exhibited significantly reduced levels of SAI compared to young adults. This analysis compared 93 older and 91 young adults from 4 studies. The Hedge's *g* was  $g=0.778$ , 95% CI [0.478, 1.078],  $p<0.001$ . The test of heterogeneity reached significance ( $Q=11.138$ ,  $df(Q)=3$ ,  $p=0.011$ ,  $I^2=73.07$ ) indicating the variation across studies was largely due to heterogeneity. The *N*-failsafe value was 19 unpublished studies. Refer to Fig. 4 for the forest plot of the for the SAI analysis comparing older versus young adults (Degardin et al. , 2011, Young-Bernier et al. , 2012b, Young-Bernier et al. , 2014, Young-Bernier et al. , 2015).

### 3.4 Impact of age on CSP

The CSP duration between the older and young adults was not significantly different. This analysis compared 54 older to 54 young adults from 4 studies (Sale et al. , 2005, Fujiyama et al. , 2009, Degardin et al. , 2011, Fujiyama et al. , 2012a). The Hedge's *g* was  $g=-0.167$ , 95% CI [-0.536, 0.202],  $p=0.376$ . The test of heterogeneity did not reach significance ( $Q=3.322$ ,  $df(Q)=3$ ,  $p=0.345$ ,  $I^2=9.68$ ), meaning the variance among studies can be explained mostly by chance. The *N*-failsafe value was 0 unpublished studies. Refer to Fig. 5 for the Hedge's *g* analysis for CSP of older versus young adults.

### 3.5 Impact of age on ICF

Old adults demonstrate a slight reduction in ICF compared to young adults which did not reach significance. This analysis compared 60 old to 39 young adults from 3 studies (Smith et al. , 2009, Saisanen et al. , 2011, Smith et al. , 2011b). The Hedge's *g* was  $g=-0.004$ , 95% CI [-0.408, 0.401],  $p=0.986$ . The Cochran's *Q* failed to reach significance ( $Q=2.860$ ,  $df(Q)=2$ ,  $p=0.239$ ,  $I^2=30.08$ ), but the  $I^2$  value indicates a moderate effect of heterogeneity. The *N*-failsafe value was 0 unpublished studies. Refer to Fig. 6 for the forest plot of the ICF analysis comparing older adult to young adults.

### 3.6 Impact of age on PAS

This analysis compared the MEP change at Post-PAS 10 minutes for 20 older versus 29 young adults from 2 studies (Muller-Dahlhaus et al. , 2008, Tecchio et al. , 2008). There was a trending decrease in LTP-like plasticity with age. The Hedge's *g* was  $g=-0.528$ , 95% CI [-1.157, 0.100],  $p=0.099$ . The test of heterogeneity was statistically significant ( $Q=9.183$ ,  $df(Q)=1$ ,  $p=0.002$ ,  $I^2=89.11$ ) because this analysis only included 2 published studies, the *N*-failsafe value was incalculable. Refer to Fig. 7 for the forest plot of the Hedge's *g* analysis for Post-PAS 10 minutes of older compared to young adults.

## 4 Discussion

To our knowledge, this is the first quantitative summary of the impact of age on cortical excitability and LTP-like plasticity assessed by TMS. We found that older adults demonstrated a significant reduction in the RMT compared to young adults. No significant

differences were observed for SICI, CSP, and ICF with age. However, older adults exhibited a significant reduction in SAI compared to young adults. We also observed a trending age-related decrease in PAS-induced LTP-like plasticity.

Our finding of an increased RMT with age is consistent with the majority of the literature (Rossini et al. , 1992, Peinemann et al. , 2001, Levin et al. , 2011, Cuypers et al. , 2013). An age-related increase in RMT suggests hypo-excitability in older adults. The cause of this hypo-excitability is multi-faceted with contributing factors such as central nervous system (CNS) decline and age-related anatomical and functional integrity changes (Oliviero et al. , 2006).

I-waves are produced by high frequency, repetitive discharge of corticospinal fibers. They are thought to originate in the motor cortex through the activation of cortico-cortical projections terminating on corticospinal neurons (Ziemann et al. , 2000). An age-related reduction in the synchronization of I-waves, deficits in recruiting later I-waves in the descending volley, and loss of both cortical and spinal motoneurons may underlie the observed age-related decrease in cortical excitability (Eisen et al. , 1996, Kimura, 2001, Pitcher et al. , 2003).

In addition to CNS changes, alterations in the peripheral nervous system (PNS) may also contribute to the observed hypo-excitability in older adults. It has been established that the neuromuscular system undergoes structural and functional alterations with age. Aging is generally associated with a loss of motor units and muscle mass atrophy. Motor unit loss has been proposed as the principal mechanism for decreased muscle strength and mass in older adults (Doherty et al. , 1993, Mesrati et al. , 2004). However, compensatory collateral innervation by the remaining motor units has been observed in older adults to counterbalance the loss of motor units (Doherty et al. , 1993, Mesrati et al. , 2004). A decrease in the motor units innervating the target muscle may contribute, in part, to the age-related decrease in RMT. Future studies assessing the impact of age on TMS measures should assess age-related PNS changes that may impact interpretation of said measures. For example, the Hoffman reflex (H-reflex) is often used as an estimate of the number of motor neurons capable of activation in a given state. Additionally, the compound muscle action potential (M-max) is used to assess the entire motor neuron pool, i.e. maximum muscle activation. Both the H-reflex and M-max have shown a gradual decrease with age suggesting a general age-related decrease in spinal pathway excitability (Scaglioni et al. , 2003, Kido et al. , 2004).

Gray matter reductions and widespread cortical thinning with age have been reported in several brain regions, such as the primary motor cortex (Salat et al. , 2004, Lemaitre et al. , 2005, Giorgio et al. , 2010, Clark et al. , 2011). In contrast, Bashir et al. found no difference in cortical thickness between young and old adults (Bashir et al. , 2014). RMT values are affected by the cortex-to-coil distance (Stokes et al. , 2005). Congruent with previous findings (Kozel et al. , 2000, McConnell et al. , 2001), Stokes et al. (2005) demonstrate a steep linear relationship between RMT and cortex-to-scalp distance in healthy participants. The studies included here did not control for age-related motor cortical thinning. An



increased cortex-to-coil distance may partially underlie the decreased excitability observed in older adults.

Congruent with the majority of the literature, we found no significant age effect on ICF (Peinemann et al. , 2001, Smith et al. , 2009). However, McGinley et al. have demonstrated a decrease in ICF with age (McGinley et al. , 2010). In line with this study, several animal studies using rat and monkey aging models not only show an age-related loss of NMDA receptor binding in multiple neocortical and subcortical regions (Wenk et al. , 1991), but highlight the association between the loss of NMDA receptors and decline in motor function (Ossowska et al. , 2001). Further investigations are needed to elucidate the age-related changes in glutamatergic neurotransmission within the human motor cortex and their functional consequences.

Previous TMS studies primarily investigated SAI effects on individuals diagnosed with Alzheimer's, Parkinson's disease and dysexecutive syndromes, using healthy older adults as "normal" age-matched controls. However, due to the absence of a young comparison group, the possible age effects on SAI were not accounted for in these studies. To date, a small handful of studies have examined the effect of age on SAI. Oliviero et al. did not find any significant impact of aging on SAI (Oliviero et al. , 2006). More recently, Degardin et al. demonstrated a slightly greater SAI in older compared to young adults; however, this result was not statistically significant (Degardin et al. , 2011). However, Young-Bernier's group have shown that older adults have a selective decrease in MEP inhibition at an ISI of 20ms (Young-Bernier et al. , 2012a, Young-Bernier et al. , 2012b, Young-Bernier et al. , 2014, Young-Bernier et al. , 2015), suggesting a decrease in central cholinergic function in normal aging. Congruent with these findings, our analysis revealed significantly decreased MEP inhibition in older compared to younger adults.

Age-related dysfunctional modulation of cholinergic transmission may underlie the observed age-related decrease in SAI. The cholinergic hypothesis of aging was proposed over two decades ago and hypothesized that disturbed cholinergic neurotransmission occurs in normal aging and plays a critical role in memory and cognitive disturbances associated with increased age (Bartus et al. , 1982). Increased aging is associated with a reduction in the choline acetyltransferase (CAT) enzyme, which synthesizes acetylcholine (Perry, 1980). There is inconsistency with regards to muscarinic receptor binding changes with age. For instance, some studies show reduced muscarinic receptor binding with age (White et al. , 1977) but other do not (Davies et al. , 1978, Perry, 1980). Moreover, the motor cortex is densely innervated by cholinergic inputs from the nucleus basalis of Meynert, which has shown significant neuronal loss with aging (McGeer et al. , 1984).

There is general consensus in the literature for a strong association between cholinergic dysfunction, memory loss and cognitive deficits. However, the association between cholinergic deficits and motor performance is less clear. Young-Bernier et al. provide the first set of evidence for the impact of age on cholinergic transmission and decline in motor performance (Young-Bernier et al. , 2012a). SAI predicted motor performance for three complex motor tasks assessing dexterity and processing speed. These tasks are inextricably linked with executive control which is critically dependent on cholinergic modulation.

SAI is critically dependent on intact cortico-cortical connections between the somatosensory and primary motor cortices. Alongside CNS alterations, age-related PNS changes may account for the observed disruption of sensorimotor integration. For example, a decrease in SAI may be due to a reduction or loss of sensory fibers and/or a decrease in axonal conduction speed (Degardin et al. , 2011).

A role for GABA<sub>A</sub> receptor-mediated inhibitory neurotransmission in SAI's neurophysiological response has been suggested through pharmacological studies. For example lorazepam, a GABA<sub>A</sub>-receptor antagonist, decreases (Di Lazzaro et al. , 2005b) and diazepam, GABA agonist, enhances (Di Lazzaro et al. , 2005a) SAI effects. Since GABA<sub>A</sub> receptors mediate both SAI and SICI, they are vulnerable to age-related deficits in GABAergic neurotransmission (Young-Bernier et al. , 2012a). However, our analysis did not demonstrate age-related changes in SICI or CSP.

The above finding is consistent with several TMS studies investigating cortical inhibition using the same TMS paradigms (Rogasch et al. , 2009, Cirillo et al. , 2010, Smith et al. , 2011a, Opie et al. , 2014). Yet, there are a number of conflicting results within the literature. For example, Peinemann et al. and Marneweck et al. reported a reduction in SICI with age (Peinemann et al. , 2001, Marneweck et al. , 2011). In contrast, Smith et al. and McGinley et al. reported an increase in SICI with age (Smith et al. , 2009, McGinley et al. , 2010).

Animal models have been used to explore the impact of age on GABAergic neurotransmission. A large number of animal studies show an age-related decline of GABA-mediated inhibition. This was indexed by findings such as a decline in the total number of GABAergic neurons (Hua et al. , 2008), alterations in GABA<sub>A</sub> receptor subunit composition and function (Caspary et al. , 1999, Yu et al. , 2006, Schmidt et al. , 2010), loss of the amount of GABA neurotransmitter, and a reduction in glutamic acid decarboxylase (GAD) (Ling et al. , 2005). The majority of these studies have investigated GABA in the prefrontal, primary visual and auditory cortices. Variations in neurotransmitter distribution, receptor density, and cortical architecture between cortical regions outside of and those comprising the motor system hinder the translatability of these results to the motor cortex (Hasan et al. , 2013). Therefore, there is ongoing uncertainty around the effect of aging on motor cortical GABAergic neurotransmission that remains unresolved based on the studies included in this analysis and amongst other studies that have employed related neurophysiological measures.

Older adults have consistently demonstrated a reduction in the ability to coordinate movements (Greene et al. , 1996, Serrien et al. , 2000, Heuninckx et al. , 2004) and slowed reaction times (Salthouse, 1991, Morgan et al. , 1994, Salthouse, 1996, Hunter et al. , 2001). To effectively perform coordinated movements successful inhibition of conflicting neuronal outputs is necessary (Baldissera et al. , 2005, Fujiyama et al. , 2009). There is growing evidence for a relationship between impairments in modulating cortical inhibition and age-related decline in motor function. One study suggests a correlation between resting state GABA neurotransmission and older adults' modulatory capacity of cortical inhibition (Heise et al. , 2013). Studies on functional changes in inhibitory TMS measures after behavioral tasks may produce greater changes between older and younger adults.

We observed a trending decrease in PAS-induced motor cortical response with age. This finding is congruent with previous TMS reports of an age-related decline in LTP-like plasticity (Muller-Dahlhaus et al. , 2008, Tecchio et al. , 2008, Fathi et al. , 2010, Todd et al. , 2010, Freitas et al. , 2011). Indirect evidence for reduced plasticity with age has also been brought to light using related neurophysiological measures investigating use-dependent plasticity (Sawaki et al. , 2003) and motor cortical excitability changes (Rogasch et al. , 2009).

Changes in motor cortical excitatory and inhibitory neurotransmission may provide one possible mechanism for reduced LTP-like plasticity with age. PAS-induced LTP-like plasticity may, to some extent, be driven by an increase in excitability of either excitatory interneurons or corticospinal neurons at the post-synaptic level (Wolters et al. , 2003). This suggests that deficient excitatory neurotransmission may underlie deficient LTP-like plasticity. This is in line with our RMT results wherein older adults demonstrated a reduction in cortical excitability indexed by an increase in RMT. However, these results should be interpreted with caution as further research is needed to determine the causal link, or lack thereof, between increased RMT and deficient PAS. With regards to GABA, pharmacological studies demonstrate conflicting results for GABA<sub>B</sub> receptor mediated modulation of LTP. For instance, GABA<sub>B</sub> antagonists can produce both facilitation (Olpe et al. , 1990, Olpe et al. , 1993) and reduction of LTP (Davies et al. , 1991, Olpe et al. , 1993). Likewise, baclofen, a GABA<sub>B</sub> agonist, can enhance LTP (Mott et al., 1990) and decrease PAS-induced LTP-like plasticity (McDonnell et al. , 2007). In summary, our analysis did not demonstrate a significant age-related change in GABAergic neurotransmission.

As well as changes in excitatory and inhibitory neurotransmission, dysfunctional sensorimotor integration may also play a role in the age-related decline of LTP-like plasticity. Direct communication between the sensory afferent signal with motor cortex output requires intact projections from the somatosensory cortex into the motor cortex (Fathi et al. , 2010). For PAS, synchronization of the electrical afferent input and TMS stimulus is imperative. A disruption of these projections may disrupt the synchronization, thereby reducing or completely abolishing LTP-like plasticity induction.

Instead of studying age-related cortical changes due to single neurotransmitter systems, it is necessary to investigate the interaction of several neurotransmitters in the aging brain. In addition to GABA and glutamate, dopamine, acetylcholine, and norepinephrine influence the induction and maintenance of synaptic plasticity. Dopamine is a major hetero-synaptic modulator of synaptic plasticity (Jay, 2003) and is essential for motor memory encoding and motor skill acquisition (Jay, 2003, Floel et al. , 2005, Molina-Luna et al. , 2009). Dopaminergic neurotransmission deteriorates with age in the human brain. It is possible that disruption of the basal ganglia-thalamocortical loop, due to an age-related decrease in striatal dopamine, may underlie age-related reductions in LTP-like plasticity. Additionally, acetylcholine and norepinephrine are crucial in facilitating use-dependent plasticity within the motor cortex (Butefisch et al. , 2002, Sawaki et al. , 2002, Meintzschel et al. , 2006). Use-dependent plasticity and LTP appear to share the same neurobiological basis. Further research is required to explore the impact of age-related changes in dopaminergic, cholinergic and adrenergic neurotransmission on LTP-like motor cortical plasticity.

## 5 Limitations

This study has several limitations. First, the number of published studies assessing the impact of age on cortical excitation, inhibition, and LTP-like plasticity were limited and their sample sizes were small. The broad age range of the included studies is a limitation and may obscure differences between young and old subjects. To fully understand the effects of aging, an individual subject level meta-analysis that stratified based on different age subgroups (early, mid, and late-life), would be required. In order to summarize the findings, we focused on resting baseline measures. Functional changes in these measures after behavioral tasks were beyond the scope of the analysis, but such studies may yield greater changes between older and younger adults. This study focused on TMS measures limited to the motor cortex. However, other brain regions play a more central role in motor learning, skill acquisition and, execution. Brain regions such as the prefrontal cortex, basal ganglia, and cerebellum are recruited and contribute to maintenance of balance, gait, coordination, reaction time, and fine and gross motor skills. An issue of “supply and demand” arises as these areas are the most susceptible to the impact of age (Seidler et al. , 2010).

The tests of heterogeneity for the majority of the TMS paradigms indicate that the differences between the studies’ results were mostly due to moderate to high heterogeneity, not chance. CSP is unique in the fact that the variability among studies can be explained mostly by chance ( $I^2=19.6\%$ ), not heterogeneity. The high heterogeneity in our analyses may be due to inter-individual variability among subjects caused by factors such as gender, physical activity, education level, skull thickness, and history of synaptic activation.

Human error, specifically unintentional coil movement, is also a limitation of the reviewed studies (Saisanen et al. , 2011). Even slight shifts in coil orientation may result in activation of different, unintended neuronal populations. Neuronavigation allows for highly accurate coil placement and any shifts in coil orientation can be monitored and adjusted in real time, significantly reducing the possibility of human error.

For PAS, Mueller-Dahlhaus et al. report only two-thirds of young healthy subjects demonstrate an LTP-like enhancement in MEP amplitude. Orientation differences of sulci, gyri and/or motor cortical neurons have been speculated to contribute to this variability (Muller-Dahlhaus et al. , 2008). Our PAS analysis was further limited by the data we were able to acquire. We were only able to analyze MEP amplitude changes at 10 minutes post-PAS. Further studies looking at MEP amplitude changes at several time intervals post-PAS (e.g. 0, 15, 30, 60 minutes) are required in order to develop a more concrete understanding of age-related alterations in PAS-induced LTP-like plasticity.

The last and most significant limitation is the large variability in TMS methodologies between studies. A number of measures could be standardized to facilitate a more accurate comparison of TMS data across studies. SICI and ICF should be measured using a conditioning stimulus of 80% RMT that precedes a suprathreshold test stimulus at an intensity that evokes a peak-to-peak MEP amplitude of 1mV (Kujirai et al. , 1993). SICI measurements should use interstimulus intervals of 2ms and 4ms and ICF should be evaluated at interstimulus intervals of 10, 15, and 20ms (Kujirai et al. , 1993, Nakamura et

al. , 1997). CSP should be evaluated using a test stimulus of 140% RMT while the contralateral muscle is active at 20% of maximum contraction (Cantello et al. , 1992). PAS should be evaluated by low-frequency electrical stimulation of the peripheral median nerve preceding a test stimulus to the contralateral motor cortex at an intensity that evokes peak-to-peak MEP amplitude of 1mV. The electrical stimulus should precede the TMS stimulus by either 25ms to evoke LTP-like plasticity or by 10ms to induce LTD-like plasticity (Stefan et al. , 2000, Weise et al. , 2013). A consistent approach would allow for more pooling of data across research groups.

## 6 Conclusion

Despite these limitations, this meta-analysis provides a current summary of studies conducted to date and a framework for future motor cortical studies that compare old and young adults. TMS is a unique tool that allows for the *in-vivo* examination of cortical physiology. With the aging population an enhanced understanding of the impact of age on cortical functioning is necessary and may provide insight into age-related illnesses.

## Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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## Abbreviations

<b>TMS</b>	Transcranial Magnetic Stimulation
<b>GABA</b>	Gamma-aminobutyric acid
<b>RMT</b>	Resting motor threshold
<b>SICI</b>	Short-interval cortical inhibition
<b>SAI</b>	Short-latency afferent inhibition
<b>CSP</b>	Cortical silent period
<b>ICF</b>	Intracortical facilitation
<b>PAS</b>	Paired associative stimulation
<b>LTP</b>	Long-term potentiation
<b>LTD</b>	Long-term depression
<b>NMDA</b>	N-methyl-D-aspartate
<b>EMG</b>	Electromyography

<b>ISI</b>	interstimulus interval
<b>CI</b>	confidence interval
<b>SD</b>	standard deviation
<b>CNS</b>	central nervous system
<b>PNS</b>	peripheral nervous system

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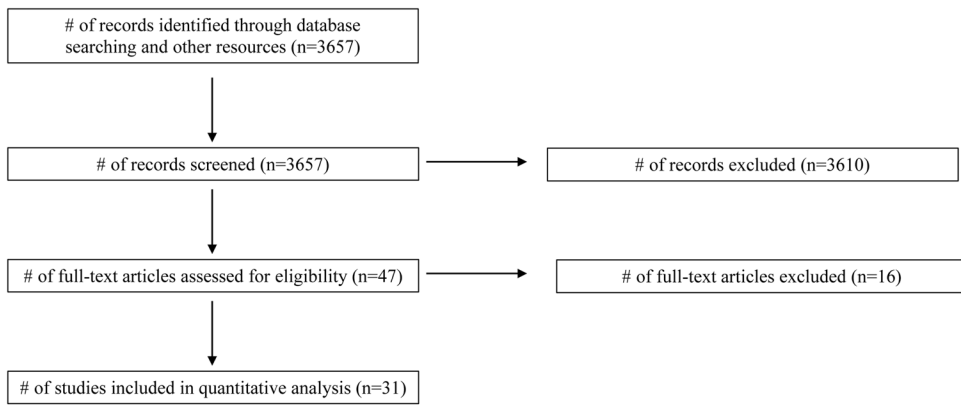
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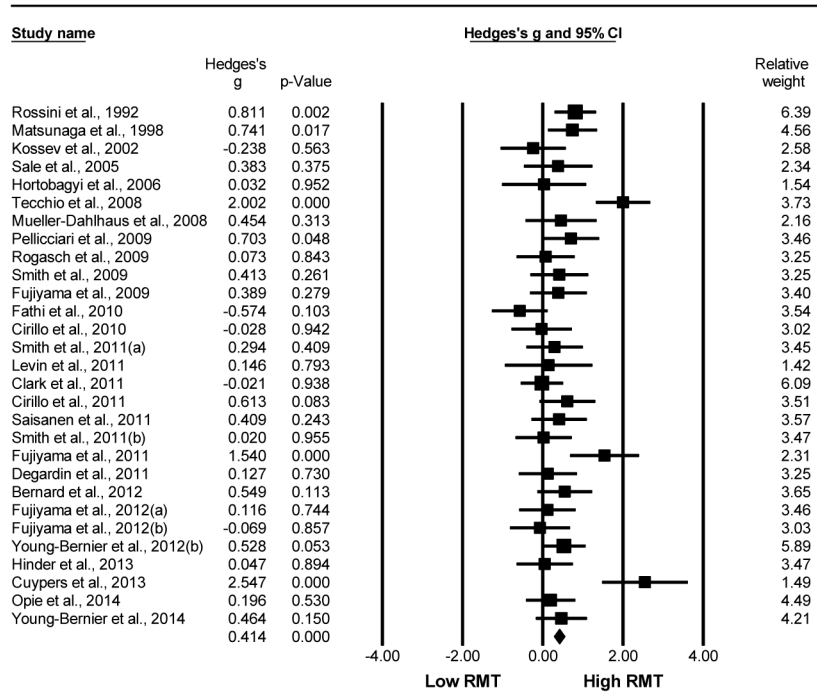
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**Highlights**

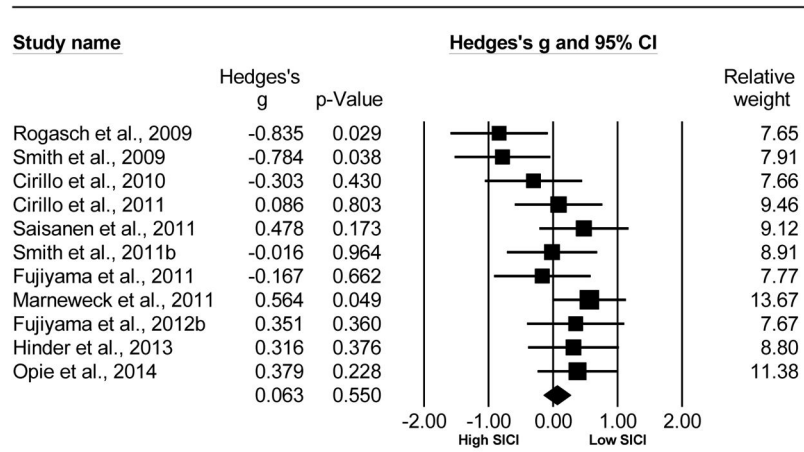
1. TMS measures of motor cortical excitation, inhibition and plasticity were assessed in young vs older adults.
2. Age-related motor cortical hypo-excitability and a trending decrease in LTP-like plasticity observed.
3. Older adults showed deficits in sensorimotor integration in comparison to young adults.



**Fig. 1.**  
PRISMA diagram.



**Fig. 2.** Forest plot of the Hedge's g analysis comparing the RMT of older to young adults.



**Fig. 3.** Forest plot of the Hedge's g analysis comparing SICI in older to young adults.

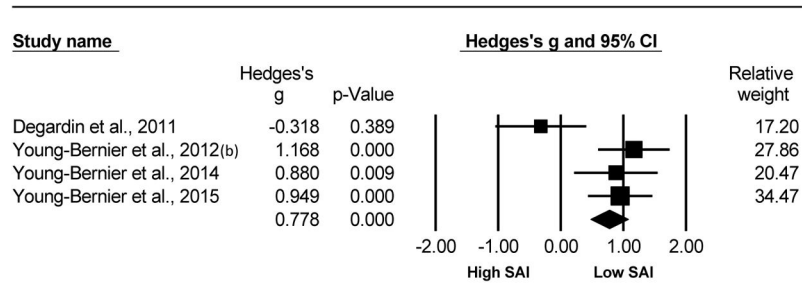
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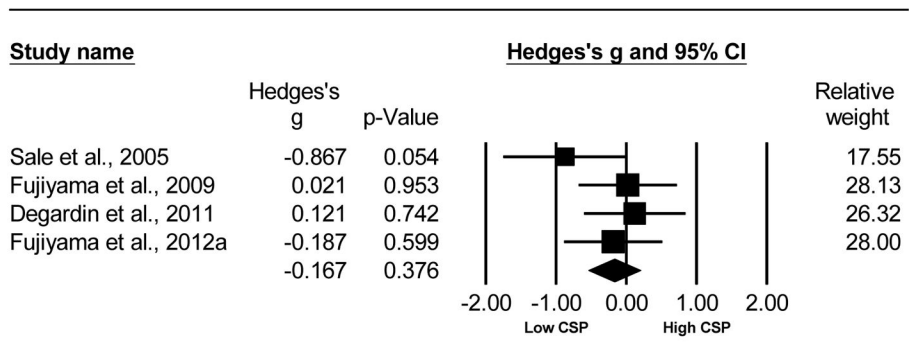
**Fig. 4.** Forest plot of the Hedge’s g analysis comparing the SAI of older versus young adults.

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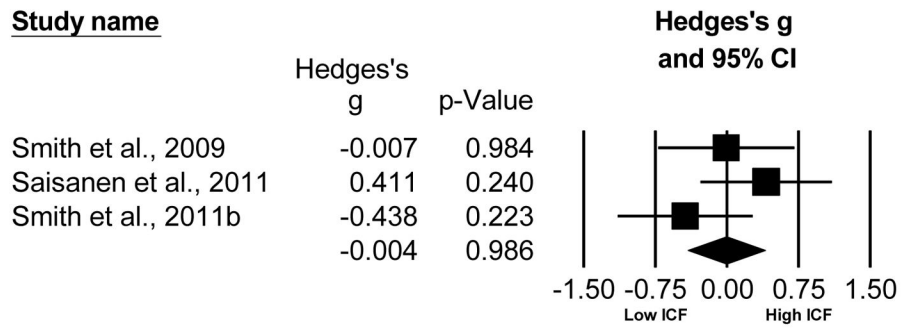
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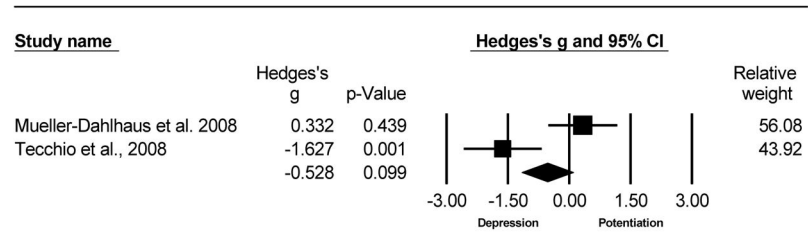
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**Fig. 5.** Forest plot of the Hedge's g analysis comparing the CSP of older versus young adults.



**Fig. 6.**  
Forest plot of the Hedge's g analysis comparing ICF of older versus young adults.



**Fig. 7.**

Forest plot of the Hedge's g analysis comparing the MEP change (Post-PAS MEP/Pre- PAS MEP) 10 minutes after PAS for older versus young adults.

**Table 1**  
Overview of TMS studies on the effects of aging on motor cortical neurophysiology.

Study	Demographic characteristics			TMS protocol	Mean±SD	Hedge's g
	Group	No. of subjects [m/f]	Age (years±SD)			
Rossini et al., 1992	YA OL	25 [10/15] 40 [14/26]	39.4±3.5 43.9±6.4	RMT	39.40±3.5 43.90±6.4	0.811
Matsunaga et al., 1998	YA OL	22 [11/11] 21 [9/12]	54.3±7.3 61.4±11.2	RMT	54.30±7.3 61.40±11.2	0.741
Kossev et al., 2002	YA OL	11 [m/f] 11 [m/f]	53.67±8.9 51.73±6.6	RMT	53.670±8.9 51.730±6.6	-0.238
Sale et al., 2005	YA OL	10 [5/5] 10 [5/5]	40±3.16 42±6.32	RMT	40.00±3.16 42.00±6.32	0.383
Hortobagyi et al., 2006	YA OL	6 [2/4] 6 [1/5]	42±6.1 42.3±10.5	RMT	42.00±6.1 42.30±10.5	0.032
Tecchio et al., 2008	YA OL	25 [12/13] 25 [12/13]	45.9±7 62.3±9	RMT	45.90±7.0 62.30±9.0	2.002
Mueller-Dahlhaus et al., 2008	YA OL	14 7	41.6±6.36 45.3±10.32	Post-PAS 10	0.856±0.44 0.443±0.11	-1.627
Pellicari et al., 2009	YA OL	16 [8/8] 16 [8/8]	52.5±7.2 58.3±8.8	RMT	52.50±7.2 58.30±8.8	0.703
Rogasch et al., 2009	YA OL	14 [8/6] 14 [8/6]	43.71±7.23 44.14±3.74	RMT	43.71±7.23 44.14±3.74	0.073
Smith et al., 2009	YA OL	13 [13/0] 16 [16/0]	36.45±7.1 39.35±6.6	RMT	36.45±7.10 39.35±6.60	0.413
Fujiyama et al., 2009	YA OL	15 [6/9] 15 [6/9]	39.73±4.34 41.33±3.64	RMT	39.73±4.34 41.33±3.64	0.389

Study	Demographic characteristics			TMS protocol	Mean±SD	Hedge's g
	Group	No. of subjects [m/f]	Age (years±SD)			
Authors				CSP	150.080±19.25 150.580±26.38	0.021
Fathi et al., 2010	YA OL	16 [14/2] 16 [11/5]	56±12 50±8	RMT	56.00±12.0 50.00±8.0	-0.574
Cirillo et al., 2010	YA OL	12 [5/7] 14 [7/7]	45.08±8.59 44.86±6.86	RMT	45.08±8.59 44.86±6.86	-0.028
Smith et al., 2011(a)	YA OL	13 18	35.46±7.01 37.67±7.52	RMT	35.46±7.01 37.67±7.52	0.294
Levin et al., 2011	YA OL	6 5	44.8±5.6 46±9.4	RMT	44.80±5.6 46.00±9.4	0.146
Clark et al., 2011	YA OL	27 [8/19] 27 [12/15]	49.3±7.1 49.1±11.4	RMT	49.30±7.10 49.10±11.4	-0.021
Cirillo et al., 2011	YA OL	16 [7/9] 16 [7/9]	41.63±9.99 47.38±8.22	RMT	41.63±9.99 47.38±8.22	0.613
Saisanen et al., 2011	YA OL	11 29	60.1±7.8 66.2±16.4	RMT	60.10±7.8 66.20±16.4	0.409
				SICI	0.63±0.59 1.30±1.56	0.478
				ICF	1.79±1.40 2.44±1.60	0.411
Smith et al., 2011(b)	YA OL	15 [15/0] 15 [15/0]	44.5±10 44.7±9.2	RMT	44.50±10.0 44.70±9.2	0.02
				SICI	0.618±0.33 0.613±0.27	-0.016
				ICF	1.375±0.39 1.206±0.36	-0.438
Fujiyama et al., 2011	YA OL	13 [4/9] 13 [4/9]	43.75±1.47 47.08±2.57	RMT	43.75±1.47 47.08±2.57	1.54
Marneweck et al., 2011	YA OL	25 [12/13] 24 [11/13]	18-29 59-88	SICI	0.508±0.14 0.486±0.11	-0.167
				SICI	0.30±0.41 0.61±0.65	0.564

Study	Demographic characteristics			TMS protocol	Mean±SD	Hedge's g
	Group	No. of subjects [m/f]	Age (years±SD)			
Authors Degardin et al., 2011	YA	14 [8/6]	26.4±2.7	RMT	41.1±22.45	0.127
	OL	14 [6/8]	62.4±7.1		44.1±23.57	-0.318
Bernard et al., 2012	YA	16	57.6±4.91	RMT	57.60±4.91	0.549
	OL	17	62.75±11.83		62.75±11.83	
Fujiyama et al., 2012(a)	YA	15 [7/8]	41.8±6.32	RMT	41.80±6.32	0.116
	OL	15 [6/9]	42.6±7.09		42.60±7.09	
Fujiyama et al., 2012(b)	YA	13 [3/10]	46.77±13.02	RMT	46.77±13.02	-0.069
	OL	13 [3/10]	45.85±12.93		45.85±12.93	
Young-Bernier et al., 2012(b)	YA	24 [11/13]	22.67±3.49	RMT	66.00±11.55	0.528
	OL	31 [13/18]	70.29±3.81		72.55±12.71	
Hinder et al., 2013	YA	15 [7/8]	49.3±8.50	RMT	49.30±8.50	0.047
	OL	15 [5/10]	49.7±7.90		49.70±7.90	
Cuyppers et al., 2013	YA	14 [6/8]	39.6±4.5	RMT	39.60±4.50	2.547
	OL	10 [2/8]	51.8±4.8		51.80±4.80	
Opie et al., 2014	YA	22	46.36±7.31	RMT	46.36±7.31	0.196
	OL	18	48.17±10.74		48.17±10.74	
Young-Bernier et al., 2014	YA	20 [7/13]	22.3±3.2	RMT	0.443±0.28	0.379
	OL	18 [9/9]	70.1±5.6		0.597±0.51	
Young-Bernier et al., 2015	YA	33 [13/20]	22.4±3.2	SAI	42.6±9.3	0.464
	OL	31 [13/18]	70.2±4.9		46.2±11.2	
					19.43±12.13	0.880
					42.07±34.79	
					20.43±13.12	0.949
					74.83±80.31	

YA healthy young adults; OA healthy older adults; RMT resting motor threshold; SICI short-interval cortical inhibition; SAI short-latency afferent inhibition; CSP cortical silent period; ICF intracortical facilitation; PAS paired-associative stimulation

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