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# Three-Dimensional Culture Systems in Cancer Research: Focus on Tumor Spheroid Model

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# Abstract

Cancer cells propagated in three-dimensional (3D) culture systems exhibit physiologically relevant cell-cell and cell-matrix interactions, gene expression and signaling pathway profiles, heterogeneity and structural complexity that reflect *in vivo* tumors. In recent years, development of various 3D models have improved the study of host-tumor interaction and use of high-throughput screening platforms for anti-cancer drug discovery and development. This review attempts to summarize the various 3D culture systems, with an emphasis on the most well characterized and widely applied model - multicellular tumor spheroids. This review also highlights the various techniques to generate tumor spheroids, methods to characterize them, and its applicability in cancer research.

# Keywords

tumor emboli; apoptosis; high throughput screening; inflammatory breast cancer; oxidative stress; invasion

# 1. Introduction

Compelling evidence from two decades of research has revealed the critical role of tumor microenvironment (TME) in cancer development and progression (Mbeunkui *et al.*, 2009; D Quail *et al.*, 2013). The cellular components of the TME (transformed epithelial cells, cancer associated fibroblasts (CAFs), tumor infiltrating mesenchymal stem cells (MSCs), tumor infiltrating lymphocytes (TILs), and endothelial cells) interact with tumor cells and impact various biological characteristics such as proliferation, migration, and therapeutic resistance

**Conflict of interest:** 

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(Wong *et al.*, 2000; Zhu *et al.*, 2009; Joyce *et al.*, 2009; Loebinger *et al.*, 2009; Baker *et al.*, 2012; DF Quail *et al.*, 2013; Kyurkchiev *et al.*, 2014; Smith *et al.*, 2014; Fedorenko *et al.*, 2015; Karakasheva *et al.*, 2015; Yulyana *et al.*, 2015). The non-cellular components of the TME (extracellular matrix (ECM), growth factors, cytokines, and chemokines) play an equally significant role in cancer progression, by presenting cues that affect fundamental aspects of tumor-cell biology (Paszek *et al.*, 2005; Levental *et al.*, 2009; Lu *et al.*, 2012). Dynamic changes in ECM architecture are detected and transduced through transmembrane cell adhesion molecules like integrin, which in turn can activate signaling pathways, causing changes in tumor cell behavior (Fiorilli *et al.*, 2008).

In two-dimensional (2D) culture systems, cells are grown as monolayers on flat solid surface, lacking cell-cell and cell-matrix interactions that are present in native tumors. Additionally, 2D-cultured cells are stretched and undergo cytoskeletal rearrangements acquiring artificial polarity, which in turn causes aberrant gene and protein expression (Cukierman et al., 2001; Nickerson et al., 2001; Kelm et al., 2003; Delarue et al., 2014). In contrast, three-dimensional (3D) culture systems offer the unique opportunity to culture cancer cells alone or with various cell types in a spatially relevant manner, encouraging cellcell and cell-matrix interactions that closely mimic the native environment of tumors (Baal et al., 2009). These interactions cause the 3D-cultured cells to acquire morphological and cellular characteristics relevant to in vivo tumors (Ma et al., 2012). Some examples include breast cancers cells co-cultured with luminal cells, myoepithelial cells and stromal fibroblasts in 3D exhibit features reflective of ductal carcinoma in situ (Holliday et al., 2009); Ewing tumor MCTS closely resemble patient tumors in context of ERK1/2 MAPK and PI3K  $\pm$  AKT pathway activation, cell-cell junctions and proliferative index (Lawlor et al., 2002). Comparison of gene and protein expression reveal that metabolic, cell stressresponse, structural, signal transduction, and cellular transport proteins are expressed at elevated levels in spheroids compared to 2D-cultured cells (Hickey et al., 2008; Weigelt et al., 2008). Moreover, cell adhesion and junction proteins that influence cell aggregation and compaction can be upregulated in spheroids compared to cells in monolayer (Kang et al., 2007; Oktem et al., 2014). Taken together these studies demonstrate the advantages of using 3D culture systems for *in vitro* oncology studies, as they allow evaluation of TME's effect on tumor, bridging the gap between 2D culture models and *in vivo* whole animal systems.

# 2. Various 3D culture models of tumor

The predominant 3D culture models of cancer include: a) tumor tissue explant, b) "tumor on a chip", and c) multicellular tumor spheroids (MCTS) (Figure 1, Table 1).

#### 2.1. Tumor tissue explant

"Tumor tissue explant" is one of the earliest 3D models of cancer and involves culturing excised human tumors in tissue culture plates (Ritter *et al.*, 2007). This model has been used mainly for *in vitro* testing of drug efficacy. In this method, tumor tissue collected after biopsy is cleared of necrotic tissue and is placed on collagen-coated surface, where it adheres to or gets embedded within the collagen (Figure 1A). Media is added and the tumor is cultured for a desired period of time, followed by intratumoral injection with test

compounds (Freeman *et al.*, 1986). Preservation of the original tumor tissue architecture, including the cellular and non-cellular components of the TME, is one of the advantages of this technique. However, the major drawback of this model is lack of reproducibility owing to natural heterogeneity of donor tissues. Additional limitations of tumor tissue explants include difficulty in application of investigative techniques like imaging and flow cytometry, and maintenance of culture for more than 3 weeks without tissue degeneration.

## 2.2. "Tumor on a chip"

"Tumor on a chip" is a revolutionary microengineered biomimetic model that involves fabrication of a functional unit of tumor on a microfluidic device. The device allows coculture of tumor cells with other cell types in a spatially relevant manner replicating the tumor microenvironment (Albanese *et al.*, 2013; Esch *et al.*, 2015). The microfluidic device consists of microwells ( $250 \mu m - 450 \mu m$ ), connected by vasculature mimicking microfluidic channels, the geometries of which can vary from simple and straight to a complex array of micro-channels. An array of micro-channels are etched or molded onto surfaces of inert materials, such as glass, silicon, and polydimethylsiloxane (PDMS). The tumor cells grow above underlying layers of matrix coated porous membrane and endothelial cells, while immune cells and circulating tumor cells (CTC) navigate through the micro-channels (Figure 1B). Custom microfabrication of the chip and real time data recording are some of the advantages of this technique. Thus, "Tumor on a chip" model provides new avenues for genomic and drug screenings, in addition to detection of circulating tumor cells (CTC) (Alessandri *et al.*, 2013).

#### 2.3. Multicellular tumor spheroids (MCTS)

MCTS is the most well characterized organotypic model of cancer. MCTS are constructed from tumor cells alone or in combination with other cell types with or without scaffolds (Baal *et al.*, 2009) (Figure 1C). Tumor spheroids display various morphologies depending on the inherent nature of the cell and the culture conditions (Figure 2A).

MCTS is an attractive model as it recapitulates the *in vivo* tumor cell characteristics with respect to growth kinetics, cellular heterogeneity, signal pathway activity, and gene expression (Table 2) (Friedrich et al., 2009). Large MCTS (>500µm in diameter) display physiochemical gradients similar to micrometastases and avascular tumors of size 0.5- $1 \text{mm}^3$ , caused due to limited diffusion of O<sub>2</sub>, nutrients, metabolic waste, and soluble factors (cytokines, growth factors, and chemokines), making them an ideal model for studying the effects of these physiochemical gradients on tumor cell characteristics (Groebe et al., 1991; Mehta *et al.*, 2012). Hypoxia induced by  $O_2$  deficiency triggers changes in gene expression, promoting aerobic glycolysis and lactic acid production, lowering pH (0.6 pH units) of the inner layer of cells (Alvarez-Pérez et al., 2005). Additionally, metabolic waste buildup triggers necrotic death of cells at the core. Cross-section of MCTS reveals concentric rings of heterogeneous cell populations, comprising of an innermost layer of necrotic cells with apoptotic cells in the peri-necrotic zone, surrounded by a middle layer of quiescent viable cells, and an outermost layer of highly proliferative and migratory cells (Figure 2B) (Bell et al., 2001; Hirschhaeuser et al., 2010). A large number of cancer cells have been cultured using MCTS model (Table 3). This model is of particular significance for studying cancers

that are characterized by pathological presence of a closely packed tumor cell cluster called a "tumor embolus". Inflammatory breast cancer (IBC), a lethal subtype of breast cancer, is an example of such a cancer. IBC is marked by the presence of dermal and stromal tumor emboli in breast tissue, a hallmark of the disease. Upon obstructing lymphatic vessels, tumor emboli prevent proper drainage of the lymph fluid, causing skin reddening and painful swelling of breast tissue (Vermeulen *et al.*, 2010; Lehman *et al.*, 2013). IBC cells display high ALDH positivity, express high levels of E-cadherin, and interestingly, continue to express elevated levels of epithelial cell markers like E-cadherin, while gaining mesenchymal and stem-like characteristics (Nguyen *et al.*, 2006; Charafe-jauffret *et al.*, 2010; Cohen *et al.*, 2015). In addition, activation of anti-apoptotic and antioxidant signaling cascades allow the IBC cells to survive in the presence of various cell death signals, leading to therapeutic resistance (Thomas *et al.*, 2011; Allensworth *et al.*, 2013; Williams *et al.*, 2013; Price *et al.*, 2015; Evans, 2016). In particular, the MCTS model has been identified to possess features that are more suitable for high throughput screening assays (Kunz-Schughart *et al.*, 2004).

# 3. Techniques for generating MCTS

Several methods have been developed over the years to generate spheroids, such as matrixon top, matrix embedded, matrix-encapsulation, spinner flasks, micropatterned plates, ultralow attachment plates, hanging drop, magnetic levitation, and magnetic 3D printing (Figure 3). Each technique possesses certain advantages and limitations, as summarized in Table 4. Spheroid size and complexity depend on the growth kinetics of individual cell types, cell density during seeding, duration of culture, and spatial limitations, such as the diameter of culture wells. Since spheroid size and heterogeneity can influence robustness of endpoint assays, it is critical to generate spheroids of uniform size and complexity for biochemical assays and high throughput screening. Typically 48-hour long cultures generate small spheroids (200µm in diameter) of uniform size and homogeneity (Winters *et al.*, 2006), whereas long-term cultures (>4 days) generate large (>500µm in diameter) heterogeneous spheroids with hypoxic core and cells of different proliferation kinetics, thereby making them suitable for pathophysiological studies.

#### 3.1. Scaffold-based MCTS

In scaffold-based MCTS, the biologically active scaffolds not only support 3D organization of cancer cells but also act as a source of external cues that promote cell-cell and cell-matrix interactions and influence tumor cell functions. The scaffolds that are commonly used in 3D culture systems include ECM-based natural hydrogels, synthetic hydrogels, and engineered hydrogels that mimic native ECM (synthetic hydrogel with integrin binding motif).

Hydrogels are water-insoluble, extensive network of cross-linked synthetic or natural polymers with tissue-like elastic properties. Hydrogels possess high water retaining capacity due to interconnected microscopic pores (Tibbitt *et al.*, 2009), which facilitates easy transport of O<sub>2</sub>, nutrients, metabolic wastes, growth and other soluble factors through the porous channels (Nguyen *et al.*, 2002). Hydrogels are derived from natural, synthetic or semi-synthetic, engineered polymers, and each of which possess certain advantages and

disadvantages (Table 5A). Matrigel is a popular commercially available ECM-based natural hydrogel derived from secreted basement membrane extracts of Engelbreth-Holm-Swarm (EHS) mouse sarcoma cells. Matrigel is rich in ECM components, such as laminin, collagen, heparin sulfate proteoglycans, entactin, and several soluble factors. Hydrogels constructed from natural polymers have endogenous chemokines and growth factors, which contribute to the viability and growth-promoting properties of natural hydrogels. However, the endogenous soluble factors add variability to the culture conditions making it difficult to obtain reproducible assay results. The presence of integrin-binding ligands on the natural polymers allows signal transduction through the transmembrane proteins and enable cells to respond to changes in the microenvironment. In addition, the hydrogels constructed from natural polymers have low tensile strength, increasing the likelihood of rapid degradation upon manipulation of their physical properties. In contrast, hydrogels constructed from synthetic polymers [poly (ethyl glycol), poly (vinyl alcohol), poly (2hydroxy methacrylate)], poly-2-hydroxyethyl-methacrylate are biologically inert but have high tensile strength, tunable mechanical properties, and give reproducible assay results. Swelling properties and permeability of synthetic hydrogels can be adjusted with external stimuli (Ahmed, 2015), such as changes in pH (Gupta et al., 2002), temperature (Klouda et al., 2008), light (Tomatsu et al., 2011), and electric field (Murdan, 2003) (Table 5B). This greater control of hydrogel swelling facilitates controlled release of biological factors (cytokines, chemokines, growth or angiogenic factors) and drugs with distinct kinetics (Richardson et al., 2001; Ehrbar et al., 2008). Semi-synthetic bioengineered hydrogels (PEGylated fibrinogen) (Mironi-Harpaz et al., 2014) are becoming increasingly popular nowadays, where motifs or active peptide sequences, such as integrin-binding sites Arg-Gly-Asp (RGD), (found within fibronectin), Tyr-Ile-Gly-Ser-Arg (YIGSR), and Ile-Lys-Val-Ala-Val (IKVAV) (found within laminin) are incorporated within the polymeric backbone. Magnetic hydrogels are infused with magnetic nanoparticles, which allow for greater control of the swelling and collapsing properties of the hydrogels using an external magnetic field (Jaganathan et al., 2014; Bumpers et al., 2015). Nano magnetic particles, such as magnetite (Fe3O4) (Souza et al., 2010), ferric oxide (Fe<sub>2</sub>O<sub>3</sub>) (Liu *et al.*, 2010), cobalt ferrite (CoFe<sub>2</sub>O<sub>4</sub>) (Giani *et al.*, 2012), iron platinum (FePt) are incorporated into hydrogels by crosslinking, blending, and in situ precipitation (Li et al., 2013).

The hydrogelation process of some natural and synthetic hydrogels involves pH or temperature adjustments, which if exceedingly harsh can destroy cells. In contrast, self-assembling peptide-based molecular hydrogels (h9e, RADA16-I) require mild hydrogelation conditions and allow cells to remain viable during culture (Huang *et al.*, 2012; Cormier *et al.*, 2013). Some of the advantages of peptide-based hydrogels include easy recovery of cells post culture (Huang *et al.*, 2013), engineering of hydrogels with enhanced gel-strength, biocompatibility and biodegradability via manipulation of peptide composition, length, and stereochemistry.

**3.1.1 Matrix- on-top and matrix embedded**—In this technique, cells are either seeded on top of a solidified layer of matrix or seeded along with liquid matrix such that the cells get embedded within the matrix upon gelation (Figure 3A). In both techniques, wells of the tissue culture plate are first pre-coated with a matrix, such as Matrigel, Methylcellulose,

etc. Chilled Matrigel is dispensed onto the pre-chilled surface of the well and placed at 37°C to allow gelation. Alternatively, warm 1% agarose solution is dispensed into the wells with a hot micropipette tip, which undergoes gelation at room temperature. In matrix-on-top method, cells in single cell suspension are seeded on top of solidified matrix, followed by gentle agitation during incubation at 37°C. The cells spontaneously aggregate to form spheroids while remaining attached to the matrix (Allensworth *et al.*, 2015; Ingeson-carlsson *et al.*, 2015). In matrix embedded technique, cells suspended in liquefied matrix (chilled Matrigel) are dispensed onto the matrix pre-coated well and incubated at 37°C during which cells get embedded within the matrix upon gelation (Lee *et al.*, 2007). This technique is commonly used to generate mammospheres. Post-culture processing and imaging of spheroids are relatively easy with the matrix-on-top method.

**3.1.2. Matrix encapsulation**—Matrix-encapsulated tumor spheroids are created using microfluidic devices and hydrogels. Although microfluidic devices with various designs are available, the basic principal remains the same, which involves enclosing droplets of cell suspension in a hydrogel shell forming microcapsules. One such microfluidic device comprises of three glass capillary tubes, which are filled with the cell suspension in the innermost capillary tube, calcium-free solution in the middle capillary tube, and a hydrogel solution in the outermost capillary tube (Figure 3B) (Alessandri et al., 2013). When droplets of cell suspension mixed with hydrogel falls into the calcium bath, the hydrogel undergoes gelation forming cellular microcapsules. The tumor cells within microcapsule assemble to form matrix-encapsulated spheroids. The calcium-free solution serves as a barrier, preventing diffusion of intracellular calcium to the hydrogel contained in outermost tube, which upon premature gelation may choke up the device. Self-assembling peptidehydrogels minimize risk of damaging the microfluidic device as they do not require calcium for gelation (Mendes et al., 2012). To encapsulate cells, peptide solution (lyophilized powder of in-vitro synthesized peptides dissolved in sodium bicarbonate) is mixed with cell suspension followed by gelation at physiological temperature. Typically, the capsules are  $200-300 \ \mu\text{m}$  in diameter and the shell thickness ranges from 5–35  $\mu\text{m}$ . One of the advantages of this technique is that it allows fabrication of uniform sized microcarriers, thereby yielding homogenous spheroids. However, compaction induces slower growth rate and increased necrosis at the core.

**3.1.3. Spinner flasks**—Spinner flasks or bioreactors are more common for large-scale production of tumor spheroids, where cells are grown as multicellular spherical aggregates in stirred suspension culture (Kunz-Schughart *et al.*, 1998). Two of the most commonly used bioreactors are spinner flasks and rotating flasks. The spinner flasks contain a magnetic stirrer at the center of the flask that ensures continuous distribution of  $O_2$  and nutrients throughout the medium. Stationary scaffolds are placed inside the flask suspended through a rod and the cells flow across the surface of the scaffolds through the moving fluid (Figure 3C). However, cells experience sheer force generated by continuous motion of the stirring bar, which adversely affects cellular physiology (Lin *et al.*, 2008). Rotating flasks function similarly to the spinner flasks, but instead of using a stirring bar to keep the cells in suspension, the culture flask itself is rotated causing the cells to experience less force (Goodwin *et al.*, 1993; Muhitch *et al.*, 2000). Moreover, rotational speed of the flasks can be

adjusted to obtain spheroids of desired sizes. One of the advantages of this technique is uncomplicated nutrient and waste product exchange. However, a homogenous distribution of cells throughout the scaffold is not achieved as most cells are predominantly found towards the periphery. The rotating flasks consist of a cylindrical vessel that is rotated at a constant speed such that the downward gravitational force is counterbalanced by upward hydrodynamic force, resulting in maintenance of the cells and scaffold in suspension (Figure 3C). The rotating fluid allows thorough mixing of nutrients and O<sub>2</sub> throughout the media while remaining gentle to cells.

**3.1.4. Micropatterned plates**—Micropatterned plates consist of hydrogel-coated microwells of uniform size  $(150 - 600 \ \mu\text{m})$ . These plates yield large number of spheroids of uniform dimensions, making them ideal for high-throughput screening. In this technique, a glass plate is first coated with a layer of 3-trimethoxysilyl polymethacrylate (TMS-PA) followed by an even layer of hydrogel, such as polyethylene glycol dimethacrylate (PEGDMA). Polydimethylsiloxane (PDMS) stamp with micropillars are photocrosslinked to PEGDMA to construct microwells. The TMS-PA pre-coating ensures covalent attachment of the hydrogel microwells onto the glass plate (Figure 3D) (Singh *et al.*, 2015). In direct photo patterning, UV exposure produces reactive oxygen species (ROS), which in turn makes the protein-repellent part of a molecule that has been grafted on the substrate to detach, allowing ECM protein to further bind onto the substrate (Théry, 2010). One advantage of direct photo patterning is that it does not require etching, like micro-contact printing (Monjaret *et al.*, 2015). Some of the drawbacks of micropatterning include unequal protein transfer onto the substrate during stamping, requirement of dedicated chemistry to engineer photosensitive materials, and use of bio-incompatible photosensitizers.

#### 3.2. Scaffold-free MCTS

Scaffold-free methods are suitable for culturing tumor cells, particularly inflammatory breast cancer cells that secrete ECM proteins and undergo self-aggregation into highly organized three-dimensional tissue-like structures. Compared to scaffold-based MCTS that comprise of compactly arranged cells with fibronectin expression localized to the peripheral rim, scaffold-free MCTS is comprised of loosely arranged cells with even distribution of fibronectin throughout the spheroid (Alessandri *et al.*, 2013).

**3.2.1. Ultra-low attachment plates**—In ultra-low attachment plates (ULA) the wells are coated with an inert substrate (polystyrene), which blocks cell attachment and causes cells in suspension to aggregate into visible spheroids (Figure 3E)(Kelm *et al.*, 2003; Vinci *et al.*, 2012). In forced aggregation a mixture of multiple cell types of arbitrary numbers are seeded into an ultra-low attachment plate. The cells are briefly centrifuged at 200g for 5 minutes, allowing them to aggregate into multicellular heterogeneous spheroids (Baraniak *et al.*, 2012; Zimmermann *et al.*, 2014).

**3.2.2. Hanging drop**—Hanging drop is a scaffold-free technique. In this technique, droplets of cell suspension are dispensed onto the underside of a petri dish lid from which they hang due to surface tension. The cells in suspension spontaneously aggregate into spheroids under gravity. The petri dish contains phosphate buffered saline (PBS), which

prevents dehydration of the droplets (Jørgensen *et al.*, 2014) (Figure 3F). More recently, spheroid culture array plates have replaced the use of petri dishes. These array plates consist of an upper compartment with tiny holes to deploy hanging drops and a bottom compartment to hold PBS (Tung *et al.*, 2011)(Torisawa *et al.*, 2007). Although spheroids of defined size are obtained by this technique, it is one of the most labor-intensive methods to culture MCTS. Another drawback of this technique, which affects cell viability, is elevated osmolarity caused by evaporation of media from the droplets. To circumvent rapid evaporation of media relatively large volumes of droplets (e.g.  $15-30 \mu$ L) are dispensed. However, this limits the number of number of spheroids that can be obtained in a given area.

**3.2.3. Magnetic levitation and bioprinting**—Magnetic levitation and 3D bioprinting have similar working principles. Both these techniques employ super paramagnetic iron oxide nanoparticles (SPIONs) that act as patterning agents to guide self-assembly of cells into spheroids under magnetic forces. Semi-confluent adherent cells are incubated overnight with SPIONS to allow cellular uptake (Whatley *et al.*, 2014). Excess SPIONS are washed off and the magnetically labeled cells are trypsinized, counted, and re-seeded in low attachment plates. Immediately afterwards, a magnet is placed on top of the plate lid (in magnetic levitation) or beneath the plate (in magnetic bioprinting), during which the SPION labeled cells are pulled up or down respectively under magnetic forces. The cells self-aggregate into spheroids within few hours (Tseng *et al.*, 2015; Leonard *et al.*, 2016) (Figure 3G).

# 4. Tools for characterization of MCTS

Biochemical assays, microscopy, and flow cytometry are commonly applied for phenotypic and morphological analysis of tumor spheroids, to evaluate efficacy of anti-cancer agents, disrupt spheroid formation, and change tumor cell characteristics in pre-formed spheroids.

#### 4.1. Microscopy

To measure the total cell count in MCTS, the spheroids are usually enzymatically disintegrated into single cell suspension, stained with trypan blue, and viewed under bright field microscope. However, this technique is incompatible with endpoint analysis that requires viable spheroids, as cell viability is poorly affected following destruction of spheroid integrity. High Content Assay (HCA) is a nondestructive live-cell imaging technique that allows simultaneous quantitative analysis of total cell count, density, dimensions, growth kinetics, nuclear mass, and mitochondrial membrane potential of live MCTS (Sirenko *et al.*, 2015). HCA also allows high throughput screening of anti-cancer drug candidates (Arora *et al.*, 2014).

Scanning electron microscopy generates high-resolution images of the superficial topography of MCTS, whereas transmission electron microscopy and multiphoton microscopy generates high-resolution 3D images of the internal structures of large MCTS (Ma *et al.*, 2012). Confocal images of spheroids provide insightful information about cytoskeletal organization and in situ protein expression (Weiswald *et al.*, 2010). The different biological zones (the outer proliferative rim, middle quiescent zone, and the dark necrotic core) can be visualized by staining MCTS cryosections with hematoxylin and eosin (Ma *et al.*, 2012). Confocal and fluorescent microscope images of MCTS that are

immunostained with antibodies against fibronectin, laminin, collagen IV, tenascin and other ECM proteins, are able to show ECM deposition (Correa de Sampaio *et al.*, 2012). Staining with Hoechst or DAPI, phalloidin, Ki-67, caspases, Annexin V, Propidium iodide, and TUNEL can provide additional information about the morphology, cytoskeletal arrangement, proliferation, and live/dead status of the cells in spheroid (Bell *et al.*, 2001; Ingeson-carlsson *et al.*, 2015). Ultra-structural changes that occur during apoptosis and necrosis can be further visualized by electron microscopy (Bell *et al.*, 2001; Uroukov *et al.*, 2008).

Imaging large spheroids (>150 µm) by confocal microscopy is extremely challenging, mostly due to poor light and antibody penetration, and attenuation of fluorescent signal by light scattering. Additionally, mobility of spheroids in suspension makes imaging of live spheroids challenging. To stabilize the spheroids, a thermo-reversible cell-mounting agent called CyGEL is used. CyGEL is an inert, optically clear liquid with low auto-fluorescence, which rapidly reverts to a gel state above 21°C. CyGEL restricts spheroid movement without compromising the viability, morphology, and protein expression in spheroids (Robertson et al., 2010). Additionally, the small size and fragile nature of spheroids require special fixing and sectioning techniques (Olsen et al., 2014). High quality confocal images are obtained by culturing spheroids on clear glass bottom plates and using wet immersion objective (Roux et al., 2008). Compared to confocal microscopy, selective plane illumination microscopy (SPIM) creates high contrast images of large spheroids and allows monitoring of live cell division dynamics in spheroids. In SPIM, the specimen is illuminated perpendicularly to the axis of the microscope objective. This allows sequential focal sectioning of the specimen, resulting in high-resolution images (Verveer et al., 2007; Lorenzo et al., 2011). SPIM is specifically useful for obtaining high-resolution images of the hypoxic core in spheroids, which is difficult to image by conventional light microscopy. However, spatial variations in refractive index caused due to heterogeneity in spheroids may cause major shift in the light path, resulting in obscure images.

#### 4.2. Biochemical assays

Poor O<sub>2</sub> delivery coupled with metabolic waste accumulation affects viability of MCTS. Acid phosphatase (AP) and Resazurin are sensitive and high-throughput-compatible assays that measure cell viability (Vinci *et al.*, 2012; Wen *et al.*, 2013; Ivanov *et al.*, 2014). Acid phosphatase released from the MCTS catalyzes dephosphorylation of the phosphate group of p-nitrophenyl phosphate (AP substrate) yielding a yellow colored product, which can be read by a colorimeter. The intensity of yellow color is an indication of the acid phosphatase activity and is therefore an indirect measurement of the number of live cells within MCTS. Resazurin reduction assay is a fluorescent assay that measures viability based on the metabolic activity of live cells. Dehydrogenase enzymes released by the metabolically active cells reduce the non-fluorescent blue substrate resazurin to fluorescent resorufin, the intensity of which can be read by a fluorescent plate reader. The relative fluorescence units are proportional to the number of metabolically live cells in MCTS.

#### 4.3. Flow cytometry

Flow cytometry allows quantitative measurement of cell viability, proliferation kinetics, apoptosis and CSC phenotype analysis in MCTS. For live/dead cell analysis single cells are

stained with calcein-AM and ethidium homodimer, which live cells and cells with damaged membrane respectively. Staining patterns enable quantification of viable cells and identification of the distinct subpopulations in MCTS – calcein stained proliferating cells; Calcein and ethidium-1 stained quiescent cells; and ethidium-1 stained cells of the necrotic core (Ma *et al.*, 2012). However, spheroids are trypsinized into single-cell suspension for flow analysis, which destroys spheroid integrity, affecting cell viability in MCTS. In contrast, COPAS flow cytometers, which specially engineered fluidic system enabling measurement of particles ranging in size from 20–1500  $\mu$ m, is a non-destructive technique that allows analysis of intact MCTS. Thus, COPAS flow cytometers allow accurate determination of viability and provide insightful knowledge about the cancer stem cells niche in MCTS.

# 5. Applications of tumor spheroids in cancer research

#### 5.1. Hypoxia, oxidative stress, and cancer-cell metabolism

In large MCTS (>500 µm) O<sub>2</sub> and ATP deficiency induces hypoxia (Bertuzzi et al., 2010). Increased ROS accumulation during oxidative stress stabilizes the transcription factor hypoxia inducible factor-1a (HIF-1a). HIF-1a has been shown to cause metabolic switch in tumor cells by modulating expression of genes involved in glucose uptake, glycolytic pathway, and glutamine consumption (Chandel et al., 2000; Sulkowska et al., 2009). This metabolic transition from mitochondrial oxidative phosphorylation to aerobic glycolysis and lactic acid fermentation, known as Warburg effect, generates ATP independently of oxygen. Increased glycolysis and lactate production causes slower cell cycle, acidification of the TME, and increased secretion of pro-angiogenic factors and ECM constituents. Lactic acid modulates activation and antigen expression abilities of dendritic cells (Gottfried et al., 2016). Interestingly, upregulation of glucose uptake in itself can activate oncogenic signaling pathways, such as EGFR,  $\beta$ 1 integrin, MEK, and AKT, leading to loss of tissue polarity and increased growth (Onodera et al., 2014). Studies have indicated that tumor spheroids display significantly increased glucose consumption and lactate production compared to 2D-cultured cancer cells (Khaitan et al., 2006; Liao et al., 2014). Changes in the expression and activity of metabolic enzymes and substrate transporters also contribute to metabolic shift in cancer cells. For example, expression and activity of glucose transporter 1 (GLUT1) and several glycolytic enzymes, such as hexokinase, phosphofructokinase-1, pyruvate kinase and lactate dehydrogenase, glucose-6-phosphate dehydrogenase, and malate dehydrogenase increase during log phase of tumor spheroids (Longati et al., 2013; Bloch et al., 2014). Additionally, genes that are involved in lipid metabolism and de-novo lipogenesis are significantly upregulated in spheroids, which helps cancer cells to survive in low exogenous fat environment as commonly found in tumors (Smans et al., 2014; Takahashi et al., 2015).

 $O_2$  consumption by spheroids is determined by culturing spheroids in Oxoplates, a specially designed plate coated with a mixture of an oxygen-sensing indicator and reference dyes. Fluorescence intensities of the oxygen-sensing indicator and reference dyes are measured every few minutes for several hours, and total cell number is counted. Oxygen concentration at each time point (pO<sub>2</sub>) is calculated using the formulae as described in (Cook *et al.*, 2012). Oxygen consumption rate is measured by calculating the ratio of oxygen concentration at

each time point, divided by the total cells. The level of intracellular ROS is measured using the fluorescent dye 2,7-dichlorodihydrofluorescein diacetate (H2DCF-DA). Multicellular tumor spheroids are incubated with H2DCF-DA, which after cellular uptake is converted into a membrane-impermeable non-fluorescent polar derivative (H2DCF), catalyzed by cellular esterases. H2DCF is rapidly oxidized to fluorescent 2,7-dichlorofluorescein (DCF), and the fluorescence is read by confocal microscopy (Artenberg *et al.*, 2003).

Direct measurement of hypoxia involves insertion of polarographic electrodes into spheroids, a technique restricted by both spatial and temporal dimensions. Some of the noninvasive methods of measuring hypoxia in MCTS include autoradiography, staining with fluorescent probes, immunohistochemistry, magnetic resonance imaging (MRI), and positron emission tomography (PET). Spheroids are incubated with a radiotracer fluoromisonidazole (<sup>3</sup>H-FMISO) that is taken up by live cells. Autoradiography reveals zones of heavily <sup>3</sup>H-FMISO labeled (white silver grains) live proliferating cells, intermediately labeled quiescent cells, and unlabeled (dark) necrotic core (Rasey et al., 1985). Perkin Elmer's in vivo near-infrared (NIR) agents allow visualization of hypoxic areas and quantification of cancer-associated biomarkers in live tumor microtissue or spheroids (Waschow et al., 2012). Fluorescent-based probes allow detection of hypoxic regions within MCTS by confocal or fluorescent microscopy. Non-fluorescent reductasebased probes are reduced to fluorescent probes by reductases, such as nitro-reductase (NTR), quinone-reductase (QR) and azo-reductase (AzoR), that are abundantly present in hypoxic regions (Hirokazu et al., 2010; Kehua et al., 2013; L Zhao et al., 2013; Sun et al., 2015). Necrotic areas within MCTS are visualized by confocal examination after labeling the cells with the hypoxic marker pimonidazole, a 2-nitroimidazole compound, which forms covalent bonds with cellular macromolecules at oxygen levels below 1.3% (Senkowski et al., 2015).

To measure glucose uptake, MCTS are stained with a fluorophore-labeled variant of 2deoxy-D-glucose called IRDye800CW-2DG, followed by counter-staining with DRAQ5, an infrared dye that binds stoichiometrically to DNA. Detection of fluorescence using Odyssey infrared imaging system allows measurement of glucose uptake by cells. Another technique called imaging bioluminescence allows mapping and quantitative measurement of ATP, glucose, and lactate concentrations in different regions of the spheroid at high spatial resolution (Walenta *et al.*, 2000). All these metabolites are measured based on an ATP dependent reaction, wherein luciferin is catalyzed by luciferase to oxoluciferin emitting light, the intensity of which is proportional to the tissue content of the metabolites (Tamulevicius *et al.*, 2000). Glucose is avidly consumed by cancer cells and is metabolized into lactate and CO<sub>2</sub>, resulting in acidification of the interstitial space. Lactate release by spheroids into the culture media can be measured using lactate assay kits or YSI 2700 SELECT<sup>TM</sup> Biochemistry Analyzer (Longati *et al.*, 2013).

#### 5.2. Cancer cell invasion and migration

The features of cell migration on soft 3D matrix and stiff 2D surfaces are distinct. Migration of cells in 2D surfaces is lamellopodia-driven and accompanied by formation of focal adhesions which are integrin-based structures formed along the contact site of cell with the

ECM substrate. In contrast, cells navigating through the matrix release matrix degrading metalloproteases (Zaman *et al.*, 2006) and form invadopodia, which are spindle-like projections that radiate from the spheroid in all directions (Wolf, 2003; Stylli *et al.*, 2008). Both focal adhesions and invadopodia mediate strong cell-substrate adhesion. The traction forces emanating from surfaces of a moving cell are transmitted intracellularly through these cell-adhesion molecules leading to activation of signal pathways and consequent changes in gene expression (Hynes, 1992; Schwartz *et al.*, 1995; Geiger *et al.*, 2011; Creed *et al.*, 2015).

There are several methods to determine invasive potential of cells in spheroid. In modified Boyden chamber-based invasion assay, a thin layer of spheroid and liquid matrix mixture is coated onto the underside of an insert covering the entire surface of the porous membrane. The spheroids get embedded within the matrix upon gelation at room temperature (Figure 4A). Serum free media is added to the bottom chamber and media supplemented with growth factors that act as a chemoattractant is added to the top chamber. Within few hours cells begin to disseminate from the spheroid, proteolytically cleave through the matrix and migrate towards the upper chamber (Lehman et al., 2013). The invasive potential of cells through cellular barrier can be evaluated by further modifying the assay where endothelial cells are plated atop the porous membrane. After 24 hours, media is aspirated from the insert; spheroid-matrix layer is removed from the underside of the insert, and stained with crystal violet to visualize the invasive cells that have migrated to the upper side of the membrane. Alternatively, cells that have been genetically modified to express fluorescent protein can be imaged and counted by fluorescence microscopy. However, Boyden chamberbased assay does not allow real-time monitoring of cell invasion and the assay needs to be terminated with a limited window. Real Time Cell Analyzer (RTCA) is an alternative technique that allows precise and continuous monitoring of invasion over the course of the assay. RTCA assay uses specially designed culture plates called CIM plates that have goldcoated microelectrodes placed underneath an ECM coated microporous membrane. The membrane is situated at the interface of upper and lower chambers of a two chamber well (Figure 4B). A monolayer of mesothelial or endothelial cells are seeded on top of the matrix to further assess the invasive potential of cancer cells through the cellular barrier. Invasive cells from the MCTS migrate through the matrix/cell/microporous membrane and upon breaching the membrane cause electrical impedance, which is measured by xCELLigence RTCA instrument (Bilandzic et al., 2014). Celigo cytometer also allows real time monitoring of the invasive front, capturing images and calculating area occupied by the leading edge of invading cells (Vinci et al., 2012) (Figure 4C). Invasive index of cells are calculated as the percentage of cells with invasive extensions within the total number of cells (De Wever et al., 2014). Further, sophisticated techniques are available to study migratory patterns of spheroids guided by electric field or gradients of O2 (S Zhao et al., 2013; Mosadegh et al., 2015).

#### 5.3. Cancer stem cells and their niche

Cancer is thought to arise from cancer stem cells (CSC) or cancer cells with stemness that have the ability to self-renew, and differentiate into different cell types contributing to tumor heterogeneity. Flow cytometric analysis of CD44<sup>+</sup>/CD24<sup>-/low</sup> and CD133 CSC involve enzyme-assisted dissociation of tumor into single cell suspension. Unfortunately, sample

preparation destroys tumor tissue integrity, which prevents investigation of CSC niche in tumors. Flow cytometric analysis of intact MCTS using COPAS flow cytometers can provide insightful knowledge about the CSC niche. COPAS flow cytometers consist of specially engineered fluidic system that enables measurement of particles ranging in size from 20–1500 µm. Another non-destructive method of studying CSC niche in MCTS involves confocal microscopy. MCTS generated from adherent cells that have been prelabeled with nucleoside analogue (EdU) are cultured for 7 to 14 days. During this time the nucleoside analogue is diluted in the actively diving cells while being retained in the quiescent cells. The MCTS are fixed, permeabilized, and stained with nuclear stain (TO-PO-3) and visualized by confocal microscopy. Quantification of the cells that retain both EdU and TO-PO-3 reveal percentage of the "label retaining cells" (Robertson *et al.*, 2010).

#### 5.4. Tumor-microenvironment signaling crosstalk

Our current knowledge of the oncogenic signaling pathways and their therapeutic interventions are mostly based on 2D-cultured cells. However, compelling evidences from several studies suggest that the signaling pathways are activated differently in cells within MCTS compared to cells in monolayers. Some recent examples include identifying HER2 homodimerization in MCTS as opposed to HER2 and HER3 heterodimerization in 2Dcultured cells (Pickl et al., 2009), higher HER3 and EGFR activation in tumor spheroids compared to 2D-cultured cells (Pickl et al., 2009), and higher rate of acquired resistance to TRAIL-mediated apoptosis due to decreased expression of death receptors (DR4 and DR5) in breast MCTS (Chandrasekaran et al., 2014). One of the reasons for differential pathway activation between 2D- and 3D-cultured cells is difference in extracellular cues arising from the TME. The ECM components, such as laminin and fibronectin, provide crucial cues that influence cellular functions through activating intracellular signaling pathways. Sitting at the cell-matrix interface, integrins play a critical role in sensing changes in ECM and relaying them intracellularly by activating downstream signaling pathways. For example, binding of integrin  $\alpha$ 9 $\beta$ -1 to tenascin activates MAPK pathway that promotes survival and proliferation of the medulloblastoma cells (Fiorilli *et al.*, 2008). Integrin  $\alpha V\beta 3$ , overexpressed at the invasive front of malignant melanoma cells and angiogenic blood vessels, increases metastatic potential of melanoma cells (Felding-Habermann et al., 1992; Brooks et al., 1994). The role of focal adhesion kinase (FAK) has been observed in promoting anchorageindependent growth of breast cancer spheroids (Tancioni et al., 2015). Hence, culturing cells in laminin rich ECM (Ir-ECM), ECM rich natural hydrogels, and synthetic hydrogels with integrin binding sites may provide the framework needed to study the ECM cues and their role in cancer progression. Spheroids cultured by matrix on-top and matrix-embedded methods enable the study of signal transduction between the ECM and tumor cells, and allow for the evaluation of their effect on the biological properties of tumor cells (Lee et al., 2007; Ritter et al., 2007; Pickl et al., 2009). Similarly cells in the TME play a critical role in cancer progression. Co-culturing MCTS with other cells types, such as immune cells and fibroblasts, can provide insights into host tumor cell interactions (Hauptmann et al., 1993; Esendagli, 2014). Microfluidic devices are suitable for such studies as tumor cells can be cocultured with multiple cell types in presence of the ECM components.

#### 5.5. Anti-cancer drug discovery

At the pre-clinical stage of drug discovery, in-vitro models are commonly used for highthroughput screening due to its low cost and rapid turnaround time compared to animalbased studies. However, the drug activity may differ considerably depending on the in-vitro model used for testing. For example, monolayers of breast cancer and HeLa cells are more sensitive to drugs compared to spheroids of these cells (Ma *et al.*, 2012; Abuelba *et al.*, 2015; Lovitt *et al.*, 2015). Although several findings suggest that heterogeneity and physiochemical gradients in tumor spheroids reduce their sensitivity to drugs compared to monolayer of cells, it does not necessarily hold true under all circumstances. A recent study recently demonstrated higher sensitivity of the breast tumor spheroids to trastuzumab compared to 2D cultured cells, as the cells of the spheroid displayed increased activation and dependence to Her2 and Her3 signaling (Pickl *et al.*, 2009). Trastuzumab blocked Her2 and Her3 activation and proliferation of spheroids but not 2D-cultured cells. Another study showed that RAF and MEK inhibitors block the invasion of thyroid carcinoma spheroids (SW1736) but have no effect on migration of SW1736 monolayer cells (Ingeson-carlsson *et al.*, 2015).

Differences in drug distribution and penetration, generation of hypoxia and ROS, enhanced expression of multidrug resistant genes, activation of survival pathways increased cell-cell and cell-matrix adhesions, may explain the differences in drug activity between 3D-cultured and 2D-cultured cells (Vinci et al., 2012). Several studies have shown that increased cell-cell and cell-matrix adhesions may activate downstream signaling pathways leading to changes in gene expression, influencing sensitivity of the cancer cells to drugs. For example, enhanced expression of cell-adhesion molecules, such as lumican, SNED1, DARP32, and miR-146a, increases chemotherapeutic resistance in pancreatic tumor spheroids (Huanwen et al., 2009; Longati et al., 2013). Similarly, interaction of B1-integrin with collagen I, collagen IV, laminin, and fibronectin protects breast cancer and lung cancer cells lines from the cytotoxic effects of various chemotherapeutic drugs (Sethi et al., 1999; Aoudjit et al., 2001). Inhibition of integrin  $\beta$ 1 significantly increases the sensitivity of Her2 hyperactivated breast cancer spheroids to trastuzumab and pertuzumab (Weigelt et al., 2010). Lamininmediated signaling through focal adhesion kinase (FAK) promotes resistance in pancreatic cancer cell spheroids to gemcitabine (Huanwen et al., 2009). Insulin like growth factor-1 receptor upon interacting with fibronectin protects DU145 (prostate cancer cell spheroids) from cytotoxic effects of ceramide and docetaxel (Thomas et al., 2010). Additionally, increased resistance to chemotherapeutic drugs in spheroids may be attributed to activation of hypoxia resistant metabolic pathways, leading to enrichment of CSCs in spheroids (Liao et al., 2014). Generation of ROS in Nox-1 high prostate tumor spheroids drives overexpression of multidrug resistance transporter P-glycoprotein, thereby promoting drug resistance (Wartenberg et al., 2005). Moreover, the effect of tumor-stromal interactions on drug sensitivity of tumor cells can be very complex and context dependent, as demonstrated by a study where colon tumor spheroid co-cultured with stromal cells and treated with various combinations of drugs (Cetuximab, Trastuzumab, Vorinostat and Everolimus, 5-FU/ oxaliplatin (FO), 5-FU/irinotecan (FI)) revealed that different microenvironment compositions alter sensitivity of tumor spheroids to drugs (Ingo et al., 2015). This finding underscores the importance of incorporating TME as a critical factor during high-throughput

screenings. Poor vascularization and ECM mediated physical interference can slow down drug penetration, distribution, and immune cell infiltration within tumors (Netti *et al.*, 2000). High-resolution 3D images of effector cell (NK cell, Cytotoxic T cell) infiltrating spheroids can be obtained using scanning electron microscopy and transmission electron microscopy (Ma *et al.*, 2012; Klöss *et al.*, 2015). Multi-photon microscopy enables visualization of the penetration of fluorescently labeled drugs and nanoparticles into spheroids (Ma *et al.*, 2012; Zipfel *et al.*, 2003).

# 6. Concluding remarks

In this review, we discussed about three different 3D models of cancer, while putting emphasis on MCTS as a tool for cancer research. We mainly focused on three key components - techniques for generating spheroids, assays for spheroid characterization, and their applications in oncology research. Although tumor spheroid is one the most widely used in-vitro 3D models, it presents some basic challenges to researchers, such as variability in spheroid size and homogeneity, poor light scattering, and impenetrability of antibodies inside the spheroid posing difficulties in imaging. Size, cell number, and cell density profoundly affect generation of the pathophysiological gradients and biological zones in MCTS, influencing their response to drugs. On one hand compact spheroids present challenges in imaging and drug distribution, on the other hand spheroids made of loosely arranged cells require special care in handling, as they tend to disintegrate easily. Although spheroids present physiochemical gradients and cellular heterogeneity like in-vivo tumors, geometry of drug penetration in spheroids is not exactly similar to in-vivo tumors, largely due to lack of vasculature in spheroids. However, uptake of fluorescent anthracyclines, radio-labeled and superparamagnetic-iron-oxide-nanoparticle-labeled drugs in spheroids still provide insights about tissue penetration and distribution properties of drugs (Bichay et al., 1990). Lastly, automation of scaffold-based spheroids may be impractical as matrix (agarose, Matrigel, cellulose, hydrogel etc.) is temperature sensitive and needs active temperature-control, which might be challenging for automated liquid handling platforms. However, recent advances in imaging and nanotechnology have enabled researchers to overcome some of the technical difficulties associated with spheroids.

Although organotypic 3D models considerably reduce the time and cost of drug discovery, until we have more sophisticated whole organ culture systems, animal models will still be needed for validating the toxicity and in-vivo activities of drugs. Microfluid-based 3D models of cancer are catching up fast, as they present unique customizable options that can be multiplexed with microscopy. Research groups in Japan recently constructed well organized three dimensional cerebral cortex, pituitary gland and optic cup (eyelids) *in vitro* (Eiraku *et al.*, 2008, 2011; Suga *et al.*, 2011), thus providing a glimpse of the future possibilities of 3D culture systems. In the near future we will have more advanced cancer models, resulting from the collaboration of tissue engineering and cancer biology, which will allow more intense interrogation of the signaling pathways and their inhibitors. The application of such culture system will not just be limited to studying diseases, but will also revolutionize the field of organ transplantation.

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# Abbreviations

2D	Two-dimensional		
3D	three-dimensional		
ТМЕ	tumor microenvironment		
IBC	inflammatory breast cancer		
MTCS	multicellular tumor spheroids		
ECM	extracellular matrix		
O <sub>2</sub>	oxygen		
CSC	cancer stem cells		

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#### Figure 1.

Schematic representing the various 3D models of cancer. **A.** Excised tumor biopsy is processed to remove the excess fat and necrotic cells, and cut into small pieces. After washing the tumor in PBS, it is placed on a tissue culture plate that has been coated with a matrix, such as Matrigel of methylcellulose, to which the tumor sits atop firmly or is embedded. Media is added and the tumor is cultured for the duration of the experiment. **B.** "Tumor on a chip" represents a vasculature mimicking microfluidic device consisting of PDMS chambers with highly organized microchannels and pneumatic chamber (dark grey) on either sides. The microchannels (pink) contain media, in which immune cells and circulating tumor cells navigate. The top chamber contains matrix coated (yellow) porous membrane (green), with a monolayer of endothelial cells on top. The tumor cells are loaded through an inlet into the top chamber. Cells that have been genetically modified to express fluorescent protein can be observed in real time to monitor their functional changes, such as invasion, and migration. **C.** Schematic depicting tumor spheroid formation where tumor spheroids have been generated by culturing tumor cells alone or in combination with fibroblasts.



# Figure 2.

A: Schematic representing the various morphologies of tumor spheroids. Tumor spheroids adapt various shapes depending upon the culture conditions and inherent nature of the tumor cells. **B.** Schematic representing the presence of physiochemical gradients in a spheroid and the resulting complexity in spheroid composition. Availability of the  $O_2$  (blue triangle) and nutrients (yellow triangle) diminishes with increasing depth of the spheroid. Whereas, metabolic waste accumulation (red triangle) is highest at the core compared to the peripheral layer of the spheroid. Hypoxia at the core (blue arrow) of the spheroid triggers necrosis (black circle), which precedes a layer of apoptotic cells. A middle layer of quiescent cells is sandwiched between the necrotic core and the peripheral layer of proliferating cells.



#### Figure 3.

Schematic explains the various methods to generate tumor spheroids. Figures AD represent scaffold-based methods, whereas figures E-F represent scaffold-free methods.



#### Figure 4. Schematic representing the various spheroid-based invasion assays

**A.** In modified-Boyden chamber based invasion assay, a thin layer of spheroid and matrix mixture is coated on the. Within 72 hours, cells begin to disseminate from the spheroid, proteolytically cleave through the matrix and migrate towards the bottom chamber through a matrix coated porous membrane located at the interface of upper and lower chambers. A layer of endothelial cells placed on top of the matrix coated porous membrane allow to determine the invasive potential of the cells through matrix and cellular barriers. B. The schematic represents a CIM plate, which has similar components as Boyden chamber. However, the detection system is different in xCelligence, where invasive potential of tumor cells is determined by measuring electrical impendence imposed by them. **C.** Spheroid is seeded on a layer of matrix, such as Matrigel, Methylcellulose, and Collagen type I, which is followed by a second layer of matrix. Cells from the embedded spheroid detach from the spheroid, radiating outward, which is measured in real time by Celigo Cytometer.

# 3D culture systems of tumor



Key features of tumor cells in monolayer, spheroids and *in-vivo* tumors.

Features	Cells in monolayer	Spheroids	In-vivo tumor
Spatial restriction of cells	1	x	X
Concentration gradient of O2, nutrients, and metabolic wastes	×	1	1
Heterogenous clonal subpopulations	1	1	1
Hypoxic core	×	1	1
Biological zones - proliferative, quiescent and necrotic zones	×	1	1
Cancer stem cell niche	×	1	1
Glucose flux rate	low	high	high
Gene expression profile	Different	Similar	Similar

List of cancer cells that have been cultured in 3D systems.

Tumor type	Cell Line	Biomaterial	Applications	Refrence
Breast Cancer	BT-20, MCF-7	Polydimethylsiloxane (PDMS)	Findings suggested that the 3D spheroids are more resistant than 2D cultured cells to TRAIL mediated apoptosis and have stem like characteristics (CD44 <sup>hi</sup> , CD24 <sup>lo</sup> , ALDH <sup>hi</sup> caused due to activation of COX-2/PGE-2 signaling pathways.	Chandrasekaran, PlosOne, Oct 2014, volume 9, Issue 10
	25 cell lines of Luminal, Basal A and B subtyes.	Matrigel	Comparative analysis of gene expression and signaling was performed between 25 B C cells grown in 2D and 3D cultures.	Paraic A Kenny, Molecular Oncology, 2007
Lung cancer	H1437, H356, H2170, A549, Chago Kl, H23, H1703	Laminin rich ECM	Lung cancer cells grown on laminin rich ECM can be differentiated into different subtypes based on their growth patterns as smooth and branched structures.	Magdelena A cinchona, Intergrated Biol 2012, volume 4, issue 4.
Prostate Cancer	RWPE-2 LNCaP	Polydimethylsiloxane (PDMS)	Findings suggested that the 3D spheroids are more resistant that the 2D cultured cells to chemotherapeutic drugs	Karen F Chambers et al PlosONe, Nov 2014, Volume 9, Issue 11.
	PC-3, PC-3M, PrCa, MDA-Pca-2b, NCI-H660	Matrigel	PrCa did not form spheroids whereas, PC-3 and PC-3M form well differentiated spheroids which transform into invasive cells. Targeting P13K pathway blocked growth of the invasive cells in spheroids.	Harma V. Virtanen, PlosOne, 2010, Volumes, Issues 5.
Colorectal Cancer	SW-480, HT-29, DLD-1, LOVO, CACO-2, CACO-205, COLO-206F,	Laminin rich ECM	The migratory, invasive or proliferative capacity of the cells did not change on forming spheroids. However, the gene expression profile of the spheroids altered significantly compared to 2D cultures. Also inhibition of EGFR is less effective in spheroids.	Anna C Luca, Plos One, 2013, Volume 8, Issue 3.
Ovarian cancer	MLS	Agar	Growth and radiation sensitivity was measured in 3D spheroids of 100 uM diameter consisting of 20 cell cluster.	R.M. Sutherland, British Journal of Cancer, 1989
	HEYA8, SKOV3, HEY,	Ultra-low attachment plate	Differential viral oncolytic efficacy was measured in 3D models of epithelial ovarian cancer	Trevor G Shepherd, Molecular Therapy- Oncolytics, 2015

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Advantages and disadvantages of the different techniques employed to generate spheroids.

Techniques	Advantages		Disadvantages		Applications	
Matrix on-top and matrix-embedded	•	Cells can be recovered post-culture if self- aggregating protein based hydrogel is used.	•	Hydrogel require special handling. Yields heterogenous spheroids requiring sorting before assay.		Ideal for evaluation of cell-cell and cell- matrix interactions, drug screening, cancer cell metabolism.
			·	Challenging to stain and image matrix- embedded spheroids.		Allow hypoxia related studies. Allow evaluation of cancer
Matrix encapsulation (microfluidic device)	•	Yields homogenous spheroids circumventing the need for sorting before assay.	•	Slower growth rate due to confinement. Increased occurrence of necrosis due to confinement.		stem cell niche.
			·	Capsule may burst if the matrix shell is thin.		
Micropatterned plates	•	Spheroids can be imaged with relative ease. Post culture recovery is possible ECM component is present.	•	Well surface needs to be coated tp create low adhesion surface. Generates spheroids of variable sizes. Multiple spheroids in a well can overwhelm assay chemistry.		
Hanging drop	•	Large number of spheroids obtained in a limited space. Reduced reagent consumption. Post culture recovery is possible.	•	Labor- intensive. For long term culturing, spheroids are transferred from the hanging drop to a second plate that can hold larger	•	Ideal for studying invasive potential of cancer cells. Allow evaluation of cancer stem cell niche.

Techniques	Advantages		Disadvantages		Applications	
				volume of media. Spheroids are transferred to a secondary plate for end- point analysis.	·	Ideal for drug screening.
Ultra low attachment plates	•	Inexpensive and easy to handle. Large number of spheroids can be obtained in a limited space (96 well or 384 well).	•	Generates spheroids of variable sizes. May have a mixture of attached cells and spheroids		
		End-point analysis can be done on the same plate. Post culture recovery is				
		easy. Can be multiplexed with imaging and other biochemical assays.				
Magnetic levitation and Magnetic Bio- printing	•	End point analysis can be done on the same plate. Can be multiplexed with imaging and other biochemical assays.	• • •	Limited number of spheroids Cells need to be pre- treated with magnetic beads. Beads are expensive. Beads at high concentration might be toxic for cells		

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#### Table 5A

# Hydrogel subtypes based on their source:

Subtypes	Advantages		Disadvantages	
Polymeric natural hydrogels	•	Contains integrin binding sites that allows cell attachment and	•	Physical and mechanical properties are unknow.
		microenvironment and cells.	•	Poor mechanical properties, tend to
	•	Biodegradable.		dissociate easily.
	•	Low reproducibility	•	Limited tunable properties
	•	Promotes viability, growth, differentiation, and allow migration of cells	•	Introduces variables into the culture conditions.
		ingration of cens.	•	Contains endogenous growth factors and cytokines.
			•	Immunogenic
			•	Spheroids generated in 4– 5 days.
			•	Challenging to handle at low temperatures.
			•	Post culture recovery is limited.
Polymeric synthetic hydrogels	•	Physical and mechanical	•	Biologically inert
		properties are know.	•	Not biodegradable.
	•	Posses tunable properties – responds to changes in pH, temperature, light etc.	•	Spheroids generated in 4– 5 days.
	•	Higher reproducibility,	•	Porosity can be controlled.
			•	Post culture recovery is limited.
Semisynthetic hydiogels	•	Physical and mechanical properties are know and can be controlled.	•	May require harsh pH and temperature adjustments for hydrogelation, which
	•	Contains active motifs and		can damage cells.
		binding ligands.	•	Spheroids generated in 4– 5 days.
	•	Higher reproducibility.	•	Post culture recovery is
	•	Requires addition of exogenous growth and other soluble factors.		innited.
	•	Distribution and concentration of ligand binding sites can be controlled.		
Molecular peptide hydrogels	•	Biologically active.	•	Spheroids generated in 4–
	•	Posses enhanced biodegradability	Post culture	Post culture recovery of
	•	Can be enzymatically cleaved.		after dissolution of the
	•	Control the length of the peptide and its composition.		matrix.
	•	Self-assembling, undergoes hydrogelation at physiological temperature.		

Subtypes	Advantages		Disadvantages
	•	Cells remain viable during hydrogelation and cell recovery.	

#### Table 5B

# Hydrogel subtypes based on their tunable properties:

Types of hydrogels	Advantages	Disadvantage
Thermo-responsive The swelling properties can be controlled by adjusting temperature		High gelling temperature adjustments if too harsh can damage cells
pH-responsive	The swelling properties can be controlled by adjusting pH	pH adjustments if too harsh can damage cells
Electo-responsive	The swelling properties can be controlled by application of mild electric field	Hydrogels generally shrink, affecting culture conditions
Magnetic hydrogels	The swelling properties can be controlled by subjecting them under magnetic field	Overnight pretreatment required to coat cells with the magnetic hydrogel