IMPACT OF VALVULOARTERIAL IMPEDANCE ON CONCENTRIC REMODELING IN AORTIC STENOSIS AND ITS REGRESSION AFTER VALVE REPLACEMENT

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BACKGROUND: Left ventricle (LV) in patients with aortic stenosis (AS) faces a double hemodynamic load incorporating both valvular stenosis and reduced systemic arterial compliance (SAC). This study aimed to evaluate the impact of global LV afterload on LV hypertrophy (LVH) before and after aortic valve replacement (AVR).

METHODS: The study cohort included 453 patients (247 males; mean age, 64 ± 11 years) who underwent AVR. Pre- and post-AVR echocardiographic examinations were retrospectively analyzed including an index of valvuloarterial impedance (Z_{VA}) and LV mass index/LV end-diastolic volume index (LVMI/LVEDVI) as a parameter of LVH.

RESULTS: Pre-AVR IVMI/IVEDVI was 2.7 ± 0.9 g/mL with an aortic valve area (AVA) of 0.6 ± 0.2 cm². Z_{VA} was 5.9 ± 1.9 mm Hg/mL/m² and showed a stronger correlation ($\beta = 0.601$, p < 0.001) with pre-AVR IVMI/IVEDVI than indexed AVA ($\beta = 0.061$, p = 0.19), transvalvular peak velocity ($\beta = 0.211$, p < 0.001). During a median follow-up of 3.5 years, patients had a $18.8 \pm 10.4\%$ decrease in the IV geometry index with a decrease in SAC from 1.20 ± 0.48 to 1.00 ± 0.38 mL/m²/mm Hg (p < 0.001). Pre-AVR IV ejection fraction (r = 0.284, p < 0.001) and Z_{VA} (r = 0.523, p < 0.001) were independent factors associated with IVH regression in 322 patients with follow-up duration >1 year after AVR.

CONCLUSION: Z_{VA} is a major determinant of concentric remodeling in AS before AVR and LVH regression after AVR, which should be incorporated in routine evaluation of AS.

KEY WORDS: Aortic stenosis · Left ventricular hypertrophy · Afterload · Echocardiography.

INTRODUCTION

Recent clinical investigations showing a high prevalence of reduced systemic arterial compliance (SAC) in patients with degenerative aortic stenosis (AS) have established a new concept: the left ventricle (LV) in calcific AS faces a double hemodynamic load incorporating both valvular and arterial pressure overloading. ¹⁻⁶⁾ This supports the idea that degenerative AS

should be considered as a potential manifestation of a systemic process, rather than as a disease solely limited to the aortic valve. The valvuloarterial impedance (Z_{VA}) is a new index to assess this global LV afterload in AS during non-invasive echocardiographic examination and it has been proved to be an independent determinant of LV intrinsic myocardial dysfunction. Many LV deformational indices, not the conventional

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LV ejection fraction (EF), showed a good correlation with Z_{VA}^{899} and prognostic implications predicting symptom development and even mortality have been confirmed in several outcome studies. Thus, Z_{VA} with certain cut-off values has been proposed as a more useful prognostic index than conventional indices including a transvalvular pressure gradient and valve orifice area. However, Z_{VA} does not separate the relative contributions of AS, the associated hypertension, and low SAC of the global LV afterload, and cannot be used in isolation as a standalone parameter. Moreover, in patients with low flow and low gradient AS, Z_{VA} fails to provide prognostic information. These findings necessitate other approaches to prove the clinical usefulness and physiologic significance of Z_{VA} .

LV hypertrophy (LVH) is a classic compensatory mechanism for LV pressure overloading in AS patients and is a fundamental pathologic change. However, the relationship between Z_{VA} and the development of LVH or LVH regression after aortic valve replacement (AVR) has not been investigated. In this study, we addressed this issue to evaluate the physiologic role of Z_{VA} and SAC measurements in patients with severe AS.

METHODS

SUBJECTS

We included patients with severe AS who had undergone uneventful AVR and a comprehensive echocardiographic evaluation before and after AVR [2.4 years after surgery (interquartile range 0.7–4.7)] at our institution from March 2000 to March 2006. Patients who had coexistent moderate to severe aortic regurgitation or mitral valve disease were excluded. Patients with occult coronary artery disease who needed concurrent bypass surgery were included. The study cohort included 453 consecutive patients (247 males; mean age, 63.9 \pm 10.9 years) and their echocardiographic and clinical data were used for the analysis. This retrospective study was approved by our Institutional Review Board.

ECHOCARDIOGRAPHY

Comprehensive 2-dimensional and Doppler echocardiographic examinations were performed in all patients. We followed the standards and techniques recommended by the American Society of Echocardiography. LV mass was calculated using the formula recommended by the society ¹³⁾ and LV geometry index was defined by the ratio of LV mass index (LVMI) to LV end-diastolic volume index (LVEDVI). ¹⁴⁾ Doppler echocardiographic assessment of AS severity included measuring peak velocities and the mean transvalvular pressure gradient with calculation of the aortic valve area (AVA) using the continuity equation.

 Z_{VA} , global LV afterload in AS patients, was calculated using the formula: $Z_{VA} = [(systolic brachial artery pressure + mean net pressure gradient) / stroke volume index].¹⁾ The mean net$

pressure gradient was calculated with the equation proposed by Baumgartner and Otto⁷⁾ to obtain a more accurate estimate of LV systolic pressure. LV stroke volume index was divided by aortic pulse pressure to calculate SAC.

STATISTICAL ANALYSIS

Continuous data were expressed as mean \pm SD. Data acquired before and after AVR were analyzed using the paired t-test. Categorical data were given as a percentage and compared with a chi-square test. A forward stepwise linear regression analysis was performed to identify the variables that are independently associated with LV geometry and its change after AVR. Variables with a p value < 0.1 in univariate analysis were entered in the multivariate analysis. A value of p < 0.05 was considered statistically significant. We used the Hittner, May, and Silver's test to assess comparison of two overlapping correlations based on dependent groups. All statistical analyses were performed using the Statistical Package for the Social Sciences (SPSS) version 18.0 for Windows (SPSS Inc., Chicago, IL, USA) and R program version 3.1.1 (http://www.r-project.org).

RESULTS

PATIENT CHARACTERISTICS

Clinical and hemodynamic characteristics before AVR are summarized in Table 1. Hypertension and diabetes mellitus were present in 177 (39.1%) and in 65 patients (14.3%), respectively. The pre-AVR LVMI was 153 \pm 44 g/m². The dominant surgical procedure was AVR with a mechanical prosthe-

Baseline characteristics	
Age, years	63.9 ± 10.9
Male, n (%)	247 (54.5)
Body surface area, m ²	1.66 ± 0.17
Hypertension, n (%)	177 (39.1)
Diabetes mellitus, n (%)	65 (14.3)
LV ejection fraction, %	58.2 ± 12.3
Systolic blood pressure, mm Hg	121.7 ± 17.2
Diastolic blood pressure, mm Hg	71.6 ± 11.6
Heart rate, bpm	66 ± 13
LV mass index, g/m ²	153.4 ± 43.8
LVEDV index, mL/m ²	61.7 ± 24.8
Stroke volume index, mL/m ²	34.0 ± 10.6
LV mass index/LVEDV index, g/mL	2.70 ± 0.89
Systemic arterial compliance, mL/mm Hg	1.20 ± 0.49
Aortic valve area, cm ²	0.61 ± 0.17
Transvalvular peak velocity, m/sec	5.01 ± 0.72
Mean transvalvular pressure gradient, mm Hg	63.0 ± 19.1
Z_{VA} , mm $Hg/mL/m^2$	5.92 ± 1.91

AVR: aortic valve replacement, LV: left ventricle, LVEDV: LV end-diastolic volume, Z_{VA} : valvuloarterial impedance

sis. It was performed in 264 patients (58.3%) and concomitant coronary artery bypass graft surgery was performed in 107 patients (23.6%). Table 2 shows the echocardiographic parameters before and after AVR. As expected, LVMI and LVEDVI decreased significantly after AVR with the index of LV geome-

Table 2. Hemodynamic and echocardiographic characteristics before and after AVR among patients followed up more than 1 year

	Before AVR	After AVR	p value	
Hemodynamic characteristics				
Systolic blood pressure, mm Hg	121.9 ± 16.6	124.6 ± 15.1	0.016	
Diastolic blood pressure, mm Hg	71.4 ± 10.9	70.8 ± 9.8	0.423	
Systolic arterial compliance, mL/mm H	1.20 ± 0.48	1.00 ± 0.38	< 0.001	
Echocardiographic characteri	istics			
LV ejection fraction, %	58.7 ± 12.1	62.7 ± 7.2	< 0.001	
LV mass index, g/m ²	152.5 ± 43.4	93.6 ± 28.0	< 0.001	
LVEDV index, mL/m ²	61.5 ± 24.1	51.7 ± 16.7	< 0.001	
LV mass index/LVEDV index, g/mL	2.67 ± 0.84	1.86 ± 0.57	< 0.001	
Transvalvular peak velocity, m/sec	5.00 ± 0.72	2.91 ± 1.63	< 0.001	
Mean pressure gradient, mm Hg	62.6 ± 19.0	18.2 ± 8.8	< 0.001	

AVR: aortic valve replacement, LV: left ventricle, LVEDV: LV end-diastolic volume

try being significantly regressed after AVR. Effective AVA increased from 0.6 ± 0.2 to 1.4 ± 0.4 cm² after AVR (p < 0.001) and SAC decreased from 1.20 ± 0.49 to 1.04 ± 0.40 mL/mm Hg (p < 0.001).

DETERMINANT OF LV GEOMETRY INDEX BEFORE AVR

Transvalvular peak velocity (r = 0.211, p < 0.001) and thus the Doppler-derived pressure gradient (r = 0.194, p < 0.001) showed a weak positive correlation with the ratio of LVMI and LVEDVI (Fig. 1), whereas there was no significant correlation between the indexed AVA and the LV geometry index (r = -0.061, p = 0.192). Z_{VA} had a good positive correlation with the LV geometry index (r = 0.601, p < 0.001) (Fig. 1). The correlation between Z_{VA} and the LV geometry index was significantly higher than that between LV geometry and the transvalvular pressure gradient or peak velocity (Table 3). Other variables associated with the LV geometry index included age (r = 0.091, p = 0.053), female gender (r = -0.135, p = 0.004), and LV EF (r = 0.267, p < 0.001). Multivariate analysis showed that female gender (r = -0.071, p = 0.046), LV EF (r = 0.354, p< 0.001), and Z_{VA} (r = 0.664, p < 0.001), were independent factors of the LV geometry index. Z_{VA} showed an excellent correlation with SAC before AVR (Fig. 2). Even after exception for patients with LV dysfunction (LV EF lower than 50%), female (r = -0.101, p = 0.013), LV EF (r = 0.126, p = 0.001), and Z_{VA} (r = 0.69, p < 0.001) were associated with LV geometry index before AVR.

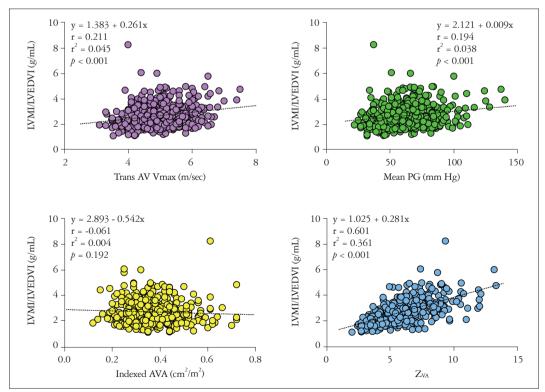


Fig. 1. Correlation between the various hemodynamic variables with LVMI/LVEDVI in patients with severe aortic stenosis. AV: aortic valve, PG: pressure gradient, AVA: aortic valve area, LVMI: left ventricle mass index, LVEDVI: left ventricle end-diastolic volume index, Z_{VA} : valvuloarterial impedance, Vmax: transvalvular peak velocity.

REGRESSION OF LV GEOMETRY AFTER AVR

Because the effect of time duration for LVH regression, we excluded patients with follow up interval less than 1 year (Fig. 3). Finally, a total of 322 patients were analyzed for LVH re-

Table 3. Comparison of correlation coefficients

	r	Z value	p value
LVMI/LVEDVI vs. Z _{VA}	0.602		
LVMI/LVEDVI vs. AV Vmax	0.211	7.608	< 0.001
LVMI/LVEDVI vs. indexed AVA	-0.061	10.161	< 0.001
LVMI/LVEDVI vs. AV mean PG	0.193	7.927	< 0.001

LVMI: left ventricle mass index, LVEDVI: left ventricular end-diastolic volume index, Z_{VA}: valvuloarterial impedance, AV: aortic valve, AVA: aortic valve area, PG: pressure gradient, Vmax: transvalvular peak velocity

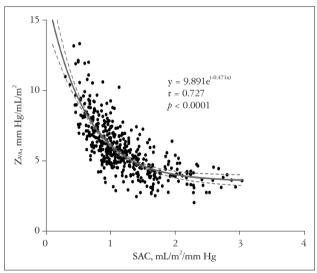


Fig. 2. Correlation between Z_{VA} and SAC. SAC: systemic arterial compliance, Z_{Va} : valvuloarterial impedance.

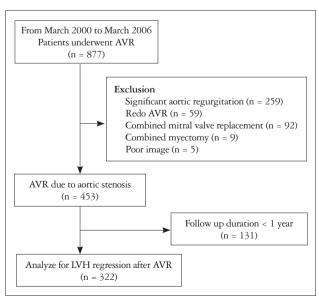


Fig. 3. Study flow. AVR: aortic valve replacement, LVH: left ventricle hypertrophy.

gression. The median echocardiographic follow-up duration was 3.49 years (interquartile range 2.18–5.37) an patients had a 30.6 \pm 32.1% decrease in the LV geometry index (from 2.68 \pm 0.84 to 1.86 \pm 0.57, p < 0.001) and a 25.5 \pm 27.4% decrease in the LVMI (from 152 \pm 43 to 94 \pm 28 g/m², p < 0.001) with a decrease of SAC from 1.20 \pm 0.48 to 1.00 \pm 0.38 mL/m²/ mm Hg (p < 0.001).

And a degree of reduction in indexed SAC between before AVR and last echocardiography was lower (-0.04 \pm 0.38 vs. -0.19 \pm 0.33, p < 0.001) in aged 65 or older group (n = 165) compared with younger group (age < 65, n = 157) but changes in LVMI or LV geometric index were not different between groups. Among these patients, the difference of indexed SAC is higher in patients with bicuspid aortic valve (-0.16 \pm 0.35 vs. -0.07 \pm 0.37, p = 0.03) compared to other etiology of AS but the amount of LVH regression (0.89 \pm 0.86 vs. 0.73 \pm 0.92, p = 0.099) was not different. In multivariate liner regression analysis, not bicuspid aortic valve but age (r = 0.223, p < 0.001) was an independent associated factor for change in SAC index after AVR.

Multivariate analysis showed that the pre-AVR LV EF (r = 0.284, p < 0.001) and Z_{VA} (r = 0.523, p < 0.001) were independent factors associated with the amount of LV mass regression after AVR (Table 4). Patients who showed significant regression of LVH, defined as a difference in the LVH geometry index statistically higher than the median value (0.70 g/mL),

Table 4. Factors associated with LV mass regression after AVR

	Univariate analysis	M	Multivariate analysis	
	p value	r	SE	p value
Age	0.997			NS
Female	0.791			
Diabetes	0.086			
Hypertension	0.705			
End-stage renal disease	0.374			
Combined coronary artery bypass graft	0.272			
Previous myocardial infarction	0.584			
Angiotensin-converting-enzyme inhibitor	0.057			NS
Angiotensin II receptor blocker	0.495			
Z_{VA}	< 0.001	0.523	0.026	< 0.001
Preoperative LV ejection fraction	< 0.001	0.284	0.003	< 0.001
Indexed aortic valve area	0.165			
Changes of effective orifice area	0.897			
Changes of mean pressure gradient	0.001			NS
Changes of systolic arterial compliance	-0.026			NS
Last mean pressure gradient	0.736			
Follow up duration	0.045			NS

LV: left ventricle, AVR: aortic valve replacement, Z_{VA}: valvuloarterial impedance

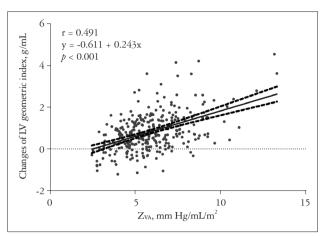


Fig. 4. Correlation between Z_{VA} and changes in LVMI/LVEDVI after aortic valve replacement. Z_{VA} : valvuloarterial impedance, LV: left ventricle, LVMI: LV mass index, LVEDVI: LV end-diastolic volume index.

had a higher Z_{VA} (6.4 ± 1.8 mm Hg/mL/m² vs. 5.2 ± 1.6 mm Hg/mL/m², p < 0.001) without any difference in SAC index after AVR than those without significant LVH regression (-0.08 ± 0.31 mm Hg/mL/m² vs. -0.15 ± 0.41 mm Hg/mL/m², p = 0.103). The difference in LVH parameters after AVR showed a positive correlation with Z_{VA} (r = 0.491, p < 0.001) (Fig 4).

DISCUSSION

The major finding of this study was that Z_{VA} representing the total load to LV is an independent factor associated with LVH in patients with severe AS requiring AVR and it is also associated with remodeling of LV geometry after successful AVR. Our finding that the association of Z_{VA} with pre- and post-AVR LV geometry is more powerful compared to the conventional indices representing the severity of valvular stenosis per se, such as pressure gradient and AVA, is a strong evidence to support the important physiologic meaning of systemic arterial loading in these AS patients.

LVH IN AS BEFORE AND AFTER AVR: ROLE OF SYSTEMIC ARTERIAL LOADING

The absence of an association between the magnitude of LVH and classic indices of AS severity such as AVA has been reported by many other investigators, $^{15-17)}$ indicating the complex nature of LVH. Our observation that Z_{VA} is more strongly correlated with the LV geometry index than does the transvalvular pressure gradient or AVA suggests a significant physiologic impact of total LV afterload on the development of LVH. Thus, although genetic factors such as polymorphism of the angiotensin converting enzyme genotype $^{18-20)}$ have been suggested to explain the lack of a correlation between valve stenosis and the hypertrophic response in AS patients, we believe that triggering effects of global LV afterload or systemic arterial loading associated with the pathogenesis of LVH should not be underestimated when the feasibility and advantage of

comprehensive physiologic assessment, including both valvular and arterial components, is taken into consideration.

AVR is a definite treatment option to improve survival in symptomatic AS patients, but persistent LVH or incomplete reverse remodeling after successful AVR have been well recognized, and results in diastolic dysfunction and poor long-term outcomes. 14)16)21) Persistent LVH, even several years after AVR, may be related to patient prosthesis mismatch, and several technical alterations and valvular substitutes aimed at decreasing the valvular gradient have been proposed. However, the valvular gradient alone cannot explain the lack of LVH regression completely, and several preoperative variables, including LV EF, cardiothoracic ratio, anti-anginal medications, and LV dysfunction, are associated with LVH regression. 22) The association between pre-AVR LV function and LV mass regression is conceivable, considering that the transition from hypertrophy to heart failure marks the tipping point at which the LV fails in the face of an increased pressure afterload and is no longer able to maintain forward flow through the valve. This key progression is associated with increased myocyte apoptosis and fibrosis and it is postulated that these two processes are responsible for the transition from hypertrophy to heart failure.²³⁾ This is believed to herald the onset of symptoms, adverse events, and a poor prognosis. Irreversible myocardial fibrosis has been confirmed to be an integral part of the hypertrophic process.²⁴⁾ Recent clinical studies using cardiac magnetic resonance imaging with gadolinium enhancement, which allows non-invasive visualization of replacement fibrosis, confirmed that a significant proportion of AS patients showed fibrosis, which is associated with a more advanced hypertrophic response and is irreversible after successful AVR. 25-27) Our finding that pre-AVR LV EF was an independent factor associated with LVH regression after AVR is compatible with previous observations, and supports the idea that, despite many limitations, LV EF could be a useful marker for intrinsic contractility and maybe provide useful histopathologic information in AS patients.

Arterial hypertension is an independent factor associated with poor LV mass regression after AVR, 21,28) but how hypertension affects LVH regression has not been established. Measurement of Z_{VA} and SAC before and after AVR was performed in our study, as we believe that it can provide some insight into mechanism of LVH regression. A previous assumption was that SAC would be generally unchanged by AVR because only the valve, and not the aorta, is replaced at the time of operation. 1)29) However, we have confirmed that SAC decreases significantly during follow-up after uneventful AVR. This is conceivable considering the advanced age of the AS patient population. Our finding that the association between Z_{VA} and the amount of LVH regression is a consequence of relief of LV afterload from AVR, emphasizes the importance of the hemodynamic contribution of LV afterload in LVH regression. This suggests that Z_{VA} or SAC could be used as a therapeutic target after AVR. The efficacy of load-independent LV mass regression using angiotensin II receptor blockade on successful LV mass regression has been reported in an animal model and in AS patients. Although it is controversial whether the positive effect of this drug is truly load-independent or effective via a reduction of LV afterload, as the data regarding the change in LV afterload or arterial stiffness with this medication are not available, the potential impact of LV afterload manipulation after AVR should be adequately addressed in future investigations.

LIMITATIONS

Cardiac magnetic resonance imaging was not performed in our study and may be argued that the echocardiographic assessment of LV mass for comparison of absolute changes within subjects can be problematic due to its dependence on image quality. However, the reliability of echocardiographic measurement has been thoroughly validated in a previous study, where an absolute change in between-study assessment of LVMI > 18 g/m² was shown to have a $\geq 95\%$ likelihood of representing a true change in LV mass. In our study, the mass index changed from 152 \pm 43 to 94 \pm 28 g/m², indicating a 25.5 \pm 27.4% decrease, which is sufficient to guarantee the reliability of our measurement.

An inappropriately high LV mass before AVR and persistent LVH after AVR²⁵⁾ have been confirmed to be associated with poor long-term outcomes, and the necessity of adding LVH criteria to the current guideline for surgical intervention has been suggested. However, the effect of LV mass regression on survival after AVR remains controversial²⁸⁾ and our study could not address this question due to the short follow-up period. Further clinical investigations with a longer follow-up are necessary to evaluate the real clinical impact of pharmacological modulation of global LV afterload after uneventful AVR.

CLINICAL IMPLICATIONS

The absence of any association between the indices representing valvular pressure overloading and the degree of LVH in AS patients can be easily explained by the addition of arterial pressure overloading. Additionally, Z_{VA} representing total LV afterload seems to be a critical step in understanding the degree of LVH before AVR and the amount of LV mass regression after AVR. Thus, we believe that Z_{VA} should be incorporated in routine evaluation of AS.

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