

Cardiac morphology and function reference values derived from a large subset of healthy young Caucasian adults by magnetic resonance imaging

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Introduction

Measurement of cardiac anatomy and assessment of heart function are among the most important clinical tasks in cardiology in order to distinguish between health and disease, and to determine accurate risk stratification and therapy.

Cardiovascular magnetic resonance (CMR) is precise and highly reproducible and has now become the gold standard for cardiac morphology and heart function. Several groups have previously presented CMR reference values for healthy people using fast gradient echo or steady-state free precession (SSFP) sequences, $1-15$ $1-15$ $1-15$

which were gathered in a recent review.¹⁶ However, sample sizes are often limited, and data focused on young adults are scarce. Precise morphologic measures in this range of ages are essential, especially in the context of most acquired cardiac diseases, but also in milder forms of congenital heart disease that might not have been diagnosed during infancy (such as atrial septal defects or compaction disorders for instance), where only subtle changes in anatomy and function may occur in early stages. In most studies, 'healthy' status was defined loosely on clinical examination and electrocardiogram (ECG) and did not exclude smoking or obesity.

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The aims of the current study are to (1) establish comprehensive, accurate, gender-specific CMR reference values for young healthy Caucasian men and women in whom cardiovascular disease and risk factors were specifically excluded and (2) evaluate if age, gender, and body surface area (BSA) have influence on these parameters during early years of adulthood.

Material and methods

Study population

We prospectively recruited 434 Caucasian adults (196 men and 238 women) at the Quebec Heart and Lung Institute through phone, email, and word-of-mouth invitation (Figure 1). Eligibility criteria were age between 18 and 35 years (although CMR was performed in 3 at 36 years because of 1-month delay from consent to imaging), at least 3 out of 4 grandparents who were Caucasian and North American-born, and apparent good health defined by the absence of known congenital or acquired cardiovascular disease, hypertension, dyslipidemia, diabetes or renal, hepatic, haematologic, and systemic inflammatory disorders. Exclusion criteria were smoking (\geq 1 cigarette/ day), BMI \geq 30, pregnancy or breastfeeding within the past year, abnormal 12-lead ECG, elevated fasting glucose, abnormal plasma lipid profile (total, LDL-, or HDL-cholesterol, or triglycerides), elevated troponins or N-terminal pro-b-type natriuretic peptide (Nt-pro-BNP), and contra-indications to CMR. We also excluded those with exercise habits significantly beyond average for the population (sustained >5 h of aerobic exercise per week) because of known effects on cardiac morphology.

Figure 1 Flow chart detailing consented participants with inclusion/exclusion criteria and reasons for exclusion.

CMR images were evaluated for gross congenital anomalies to exclude previously unknown congenital cardiac conditions. The institutional Ethics Committee approved the study, and all patients provided written informed consent.

CMR acquisition protocol

Imaging was performed with a 1.5-Tesla Philips Achieva scanner operating release 2.6 level 3 (Philips Healthcare, Best, The Netherlands). Cine imaging of cardiac morphology and function was performed by SSFP technique at 30 phases per cardiac cycle in held end expiration; 8–14 contiguous parallel short-axis (8 mm thickness, 0 mm gap) and 3 radial long-axis planes were performed covering the entire cardiac volume. Typical parameters included TR/TE 3.17/1.58 ms, flip angle 60° , and number of excitations of 1, yielding an in-plane spatial resolution of 1.6 \times 2 mm and a mean temporal resolution of 33 ms.

CMR image analysis

Image analysis was performed offline in a core laboratory using a standardized approach by trained technicians [4 technicians with a total experience of 15 years (2–4 years each) dedicated reading in the laboratory] supervised by an experienced cardiologist (E.L.) following the American Heart Association (AHA) 17-segment model (cmr⁴² version 3.4.1, Circle Vascular Imaging, Canada).[17](#page-9-0) Cardiac volumes and function measurements were performed as previously described by our group and others, using the contiguous short-axis multi-slice acquisition with delineation of atria/ventricles confirmed in matched long-axis planes. $4,18-20$ $4,18-20$ $4,18-20$ $4,18-20$ Participants did not undergo gadolinium contrast injection.

Ventricles

For ventricular volume analysis, the endocardial border was semiautomatically determined on the left ventricle (LV) for all 30 phases

Figure 2 Detailed contouring of the four cardiac chambers in contiguous SSFP short-axis slices at end-diastole (A) and end-systole (B). Red: LV endocardial border, green: LV epicardial border, purple: LV papillary muscle border, yellow: RV endocardial border, orange: LA endocardial border, blue: RA endocardial border.

Figure 2 (Continued).

of the cardiac cycle and the cardiac phases that demonstrated the largest and smallest ventricular cavity volumes were defined as end-diastole (ED) and end-systole (ES), respectively (Figure [2](#page-2-0)). For the LV, the endocardial border was defined as the boundary between the myocardium and ventricular blood pool, from the most apical to the most basal slice. Manual correction of automated LV endocardial border and papillary muscles tracing was performed when necessary. Papillary muscles were included when measuring mass (equivalent to weighting the LV) and excluded when measuring volumes (equivalent to blood pool techniques). $20,21$ At the base of the heart, careful differentiation of ventricle from the atrium and aorta/pulmonary artery relied on examination of matching long-axis planes. If the basal slice contained both ventricular and atrial wall, the contours were drawn up to the junction of the atrium and the ventricle and the appropriate volume attributed to the ventricle. Similarly, if the aortic valve appeared in the basal slice, blood volume up to the aortic valve was included in the LV volume. For the right ventricle (RV), endocardial border was manually traced both in ED and ES from

the most apical to the most basal slice. Trabeculations and moderator band of the RV were ignored, and a smooth endocardial border was drawn. The moderator band was included in blood pool.^{[20](#page-9-0)} In basal slices, the RV outflow tract was accounted for in the RV volume, with a particular attention paid to include only the portion of volume below the level of the pulmonary valve.

For LV mass measurement, the epicardial border was semiautomatically traced followed by manual correction to follow the middle of the chemical shift artefact line when necessary.²⁰ Epicardial fat was excluded from the epicardial border.

The LV and RV ED volumes (LV-EDV, RV-EDV), ES volumes (LV-ESV, RV-ESV), stroke volumes (LV-SV, RV-SV), ejection fraction (LV-EF, RV-EF), and LV mass were computed using Simpson's rule. The LV-EDV, RV-EDV, LV-ESV, RV-ESV, and LV mass were normalized to BSA calculated by the Dubois formula.²² Segmental wall thickness was measured at ED by the centreline method (mean of 20–30 chords/segment), following the AHA 17-segment model definition. Segmental systolic wall

thickening (segmental function) was defined for each individual segment as the difference between wall thickness at ED and thickness at ES (wall thickening) divided by wall thickness at ED to provide per cent thickening. As is customary, segment 17 (apex) was excluded from functional analysis. We uncovered high intra/inter-observers variability for RV mass in our preliminary analysis and elected not to report such unreliable measurements.

Atria

Atria images were obtained during the same acquisition as ventricles (full coverage of the cardiac silhouette in short axis); hence, slice thickness and gap were the same. In order to better discriminate between atria and ventricles, the long-axis planes were used to place a boundary at the level of the atrio-ventricular valve annulus. LA and RA endocardial borders were manually traced in atrial ED and ES phases on contiguous short-axis slices as detailed previously, ED referring to the atrial diastole (maximum volume). The atrial appendage was included in the total LA and RA volumes, but the pulmonary veins were excluded. Volumes were calculated from Simpson's rule.^{[23](#page-9-0)}

Statistical analysis

Continuous variables were tested for normality by the Shapiro–Wilk test and reported as means \pm SDs. Categorical variables were expressed as a percentage and compared with the χ^2 test. Gender

Table | Population characteristics

Data are presented as means \pm SD. P-value is for t-test between genders.

BP, blood pressure; Nt-pro-BNP, N-terminal pro-b-type natriuretic peptide; NS, non-significant.

Table 2 Global left ventricle parameters

Data are presented as means \pm SD (5th and 95th percentiles). P-value is for t-test between genders. NS, non-significant.

differences were compared using Student's t-tests. Differences between basal, mid-ventricular, and apical LV thickness and thickening were assessed using one-way analysis of variance (ANOVA) followed by Tukey's post hoc test. Intra- and inter-observer agreement (on 50 and 25 patients, respectively) was evaluated by absolute intraclass correlation coefficient (ICC) and by the Bland–Altman method. Association between morphological parameters indexed to BSA and age was assessed with linear regressions. All multivariable linear regression analyses included age, gender, and BSA. Statistical analyses were performed with Stata 13.0 (StataCorp LP, College Station, TX, USA). Statistical significance was set at $P < 0.05$.

Results

Characteristics of the population

The mean age of the 434 young adults (45% male) was $26.2 + 4.5$ years. The sample characteristics are presented in Table [1](#page-4-0).

Ventricle volumes, function, and mass

The values for LV volumes, function, and mass are presented in Table [2](#page-4-0). LV-EDV, LV-ESV and LV-SV values were lower for women than men. LV-EF was similar in both sexes. LV mass was greater in men than in women. After normalizing to BSA, volumes and mass were still greater in men. LV wall thickness and thickening are pre-sented in Figure [3](#page-6-0) and Table 3. LV wall thickness was less in women than men (Figure 3 and Table 3). Mean values for systolic wall thickening (segmental function) were $56 \pm 17\%$ for basal segments, $72 + 19%$ for mid-ventricular segments, and $78 + 34%$ for apical segments, with no difference between genders. When progressing from the base to the apex, there was a gradual decrease in the thickness of myocardial segments, along with a gradual increase in systolic wall thickening (ANOVA $P < 0.01$, Table [3](#page-6-0)).

The values for RV volumes and function are reported in Table [4](#page-6-0). Similarly to LV parameters, the values for RV-EDV, RV-ESV and RV-SV were lower for women than men. RV-EF was identical between genders. Volumes remained greater in men after normalizing to BSA.

In multivariable analysis, gender and BSA were independently associated with LV and RV parameters ($P < 0.001$), except for LV-EF and RV-EF. Age was found to have an independent influence on most ventricular measurements (all $P < 0.002$), except for LVand RV-SV, and LV mass. The associations with age remained significant even after adjustment for systolic, diastolic, or mean arterial pressure levels. In further analysis taking into account gender, age was no longer independently associated with LV- and RV-EDV, RV-ESV, and RV-EF in women. Evolution of LV- and RV-EDV (normalized to BSA) with age is illustrated for men and women in Figure [4](#page-7-0).

Atrial volumes and function

The values for LA and RA volumes and function are presented in Ta-bles [5](#page-7-0) and [6](#page-8-0), respectively. Men had greater LA- and RA-EDV, RA-ESV, and RA-SV than women. However, the values for LAand RA-EF were lower in men compared with women. After BSA normalization, LA- and RA-EDV, and RA-ESV remained significantly greater in men than women.

In multivariable analysis, BSA was independently associated with all atrial parameters (all $P < 0.01$), except for LA-EF. Gender was

Figure 3 Segmental left ventricular wall thickness at enddiastole for men (A) and women (B). Thickness is reported per standardized AHA segment in mm (bold) with 5th and 95th percentile limits (beneath in brackets). Basal slice: I, anterior; II, anteroseptal; III, inferoseptal; IV, inferior; V, inferolateral; VI, anterolateral. Mid-cavity slice: VII, anterior; VIII, anteroseptal; IX, inferoseptal; X, inferior; XI, inferolateral; XII, anterolateral. Apical slice: XIII, anterior; XIV, septal; XV, inferior; XVI, lateral.

independently associated with LA-EF ($P < 0.03$) as well as RA-EDV and RA-ESV ($P < 0.01$) but not with LA volumes. Age was found to have an independent influence on LA parameters ($P < 0.01$), except for LA-EF. The associations with age remained significant even after adjustment for systolic, diastolic, or mean arterial pressure levels. Evolution of LA-EDV and RA-EDV (normalized to BSA) with age is illustrated for men and women in Figure [4](#page-7-0). Age was not independently associated with any RA parameter.

Intra- and inter-observer variabilities

Intra-observer agreement by ICC was 0.98 for LV-EDV (mean difference 2.5 mL, limits of agreement -0.7 to 5.6 mL), 0.96 for RV-EDV (2.3 mL, -3.4 to 8.1 mL), 0.95 for LA-EDV (0.7 mL,

Table 3 Segmental left ventricle end-diastolic wall thickness and end-systolic wall thickening (function)

Data are presented as means \pm SD (5th and 95th percentiles). P-value is for t-test between genders.

NS, non-significant.

 $*P < 0.05$ vs. basal segments.

 $\frac{6}{5}P < 0.05$ vs. mid segments.

Table 4 RV parameters

Data are presented as means \pm SD (5th and 95th percentiles). P-value is for t-test between genders. NS, non-significant.

 -2.1 to 4.3 mL), and 0.94 for RA-EDV (0.8 mL, -1.7 to 4.8 mL), all $P < 0.001$. Inter-observer agreement was 0.93 for LV-EDV (4.2 mL, -8.5 to 16.8 mL), 0.92 for RV-EDV (6.5 mL, -14.8 to 24.6 mL), 0.89 for LA-EDV (4.3 mL, -5.1 to 14.1 mL), and 0.90 for RA-EDV $(3.8 \text{ mL}, -3.2 \text{ to } 10.8 \text{ mL})$, all $P < 0.01$.

Discussion

Several groups have worked to establish reference values using the SSFP technique.^{4,5,9,11,[13](#page-9-0)–[15](#page-9-0)} We observed some differences between our findings and those from Maceira et al., which are currently widely employed as a clinical standard.^{9,11} In the current study, we delineated the endocardium by semi-automated circular contouring with

inclusion of trabeculations in ventricular volumes. This method is reported to be more reproducible than manual delineation of trabeculations but results in reduced LV mass and increased LV volumes.²⁴ This may explain why we observe lower LV mass in both genders and higher volumes in men of our sample in comparison with Maceira et al. who used a semi-automated method that included portions of trabeculations. Nevertheless, we identify lower LV volumes in women, even after normalization to BSA. We also measure greater RV volumes in both genders, no doubt due to the inclusion of trabeculations and the moderator band in the blood pool in order to reduce variability. The differences between our findings and those of Maceira et al. are particularly pronounced when comparing limit values, which are more useful in clinical practice than are mean values.

Figure 4 Evolution of end-diastolic chamber volumes with age for young adult men and women. Linear regressions with 95% confidence intervals of volumes normalized to BSA for LV-EDV (A), RV-EDV (B), LA-EDV (C), and RA-EDV (D).

Table 5 Left atrium parameters

Data are presented as means \pm SD (5th and 95th percentiles). P-value is for t-test between genders. NS, non-significant.

 $Table 6$ $Dight$ atrium

Data are presented as means \pm SD (5th and 95th percentiles). P-value is for t-test between genders.

One of the main advantages of our study is that the large size of our cohort allowed us to describe limit values using the 5th and 95th percentiles. Due to the smaller size of prior cohorts, previous studies described limit values on the basis of descriptions or graphic representations of 95% confidence interval to the mean. However, the latter methods may be misleading, since they actually reflect the reliability of the mean's estimation rather than the true range of values, and are strongly dependent on sample size.

We observed greater variability in atrial measurements compared with ventricles. This is undoubtedly related to the difficulty in identifying a definite border between the connections of pulmonary arteries and vena cava to the atria, adding two extra difficulties to delineating the RA and four extra difficulties to delineating the LA.

Influence of body size and ethnicity

In addition to the impact of a greater sample size, discrepancies compared with previous studies may be explained by the exclusive presence of Caucasian individuals having at least three out of four North American-born grandparents. Indeed, most previous studies have not taken into account ethnic origins, while ethnicity influences $BSA₁⁷$ $BSA₁⁷$ $BSA₁⁷$ itself a strong independent predictor of ventricular volumes and mass.^{[9](#page-9-0),[11](#page-9-0)} Furthermore, genetic factors may induce significant variability in cardiac morphology independent of BSA.^{[25,26](#page-9-0)} Thus, ethnicity should be taken into account when reporting and developing normal reference values.

Influence of sex status

Although previous studies have described higher ventricular mass and volumes in men compared with women, these differences did not always persist after normalization to BSA.^{[4](#page-9-0),[5](#page-9-0),[9,11](#page-9-0)} Similar discrep-ancies have been reported for atria as well.^{[5,8](#page-9-0)} As described in recent large scale CMR studies, $15,27$ our data are consistent with the presence of sex-related differences, even after adjustment for age and BSA (with the exception of the LA). As previously reported by Dawson et al.,^{[28](#page-9-0)} we also observe differences in ED wall thickness in men vs. women, even after normalization to BSA. Thus, the greater LV mass observed in men is not exclusively explained by larger ventricle volume. However, gender dimorphism disappears when

considering systolic wall thickening, where segmental function remains comparable in women vs. men, contrary to what was previ-ously reported by Ubachs et al.^{[29](#page-9-0)}

Influence of age

Our results indicate that age is independently associated with all LV and RV volumes, with the exception of SV. These findings are consistent with the majority of previous studies, $2,3,6,9,11,13$ even if the age range of our population was narrow. Although age is no longer independently associated with LV-EDV, RV-EDV, and RV-EF when examining women only, we cannot discount the possibility that such sex-specific differences in the effect of age may result from either a lack of statistical power in this narrow range of ages or by the overriding influence of BSA. In contrast to volume measurements, LV mass is not associated with age in our sample. Of note, results from previous studies were not always consistent, as some have reported that age had either $no^{1,9,14,15,30}$ or minimal influence^{[31,32](#page-9-0)} on LV mass, whereas others found a relationship variably limited to either women 33 or men.⁵

We also observed that LA volume was associated with age, even after adjustment for gender and BSA. These results are consistent with previous observations, 34 including in children and adolescents, 35 but to our knowledge, this is the first time that this association is described in young adult women and men.

Strengths and limitations

Normality was defined by the absence of cardiovascular disease, and for the first time major risk factors including smoking and obesity. However, normality has no absolute definition, and despite our best efforts, there is no fail-safe method to ensure exclusion of all volunteers with mild subclinical disease. A second relative limitation is that it is not possible to extend our results to populations other than Caucasians, and similar studies should be performed for each specific ethnic group. By the same token, this may constitute one of the greatest strengths of our work since variability related to ethnicity was strongly reduced. Our results are derived from a young adult cohort and cannot be recommended for older individuals. Finally, the subjects were invited to participate through phone, email, and word of mouth, which is expected to bias towards a healthy sample.

Conclusion

This study, the largest to date, provides sex-specific normal reference values for both left and right ventricular and atrial volumes, LV mass, and functions in healthy young Caucasian adults by SSFP CMR. As CMR is increasingly solicited to discriminate normality from equivocal disease in young otherwise healthy adults, such reliable reference values should prove valuable to better define the limits of normality for research and clinical practice alike.

Conflict of interest: None declared.

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