



Published in final edited form as:

Biomaterials. 2017 March ; 120: 81–93. doi:10.1016/j.biomaterials.2016.11.035.

Myosin Phosphorylation on Stress Fibers Predicts Contact Guidance Behavior across Diverse Breast Cancer Cells

Juan Wang¹ and Ian C. Schneider^{1,2,*‡}

¹Department of Chemical and Biological Engineering, Iowa State University

²Department of Genetics, Development and Cell Biology, Iowa State University

Abstract

During cancer progression the extracellular matrix is remodeled, forming aligned collagen fibers that proceed radially from the tumor, resulting in invasion. We have recently shown that different invasive breast cancer cells respond to epitaxially grown, aligned collagen fibrils differently. This article develops insight into why these cells differ in their contact guidance fidelity. Small changes in contractility or adhesion dramatically alter directional persistence on aligned collagen fibrils, while migration speed remains constant. The directionality of highly contractile and adhesive MDA-MB-231 cells can be diminished by inhibiting Rho kinase or $\beta 1$ integrin binding. Inversely, the directionality of less contractile and adhesive MTLn3 cells can be enhanced by activating contractility or integrins. Subtle, but quantifiable alterations in myosin II regulatory light chain phosphorylation on stress fibers explain the tuning of contact guidance fidelity, separate from migration per se indicating that the contractile and adhesive state of the cell in combination with collagen organization in the tumor microenvironment determine the efficiency of migration. Understanding how distinct cells respond to contact guidance cues will not only illuminate mechanisms for cancer invasion, but will also allow for the design of environments to separate specific subpopulations of cells from patient-derived tissues by leveraging differences in responses to directional migration cues.

Keywords

Topography; epitaxial growth; mica; collagen; contractility; paxillin

Introduction

Migration is an important cell behavior that occurs during many pathological and physiological processes. For instance, during cancer invasion and metastasis, faster migration occurs through altered signaling pathways, cytoskeletal dynamics and adhesive

[‡]Author for correspondence (phone: (515) 294-0450, fax: (515) 294-2689, ians@iastate.edu).

^{*}Present address: Iowa State University, Department of Chemical and Biological Engineering, 2114 Sweeney Hall, Ames, IA, 50011-2230

Publisher's Disclaimer: This is a PDF file of an unedited manuscript that has been accepted for publication. As a service to our customers we are providing this early version of the manuscript. The manuscript will undergo copyediting, typesetting, and review of the resulting proof before it is published in its final citable form. Please note that during the production process errors may be discovered which could affect the content, and all legal disclaimers that apply to the journal pertain.

structures. In addition to faster migration, it is well known that the tumor microenvironment (TME) presents directional cues for cancer cells, allowing for more efficient cell migration towards blood vessels, lymph vessels and along nerve fibers. Directed migration comes in various flavors, one of which is contact guidance, or directed cell migration along aligned fibers or fiber-like structures. Contact guidance has been shown to be a powerful modulator of breast cancer metastasis, due to the robustly aligned collagen emanating radially from the TME [1], but other cancers likely share similar signatures [2]. Furthermore, this aligned fiber structure likely enhances stromal and immune cell migration towards the tumor [3, 4]. Understanding how contact guidance operates across different cells is a critical aspect of understanding the biology of tumor invasion and metastasis. In addition, fabricating tumor mimicking environments that allow for the separation and expansion of patient-derived cells for drug screening applications will require both the ability to make complex structures as well as the understanding of how cells respond to those structures.

There have been numerous approaches for fabricating contact guidance cues in 2D and 3D environments [5-8]. Controlling 3D contact guidance cues is more difficult and imaging cells embedded within these environments can pose challenges, so most of the work has been conducted in 2D environments. Most contact guidance work has been carried out on gratings [9-12] that present either micro- or nano- sized grooves and ridges from 50 nm to 50 μm in width with depths ranging from 30 nm to 3 μm . In addition to gratings, lines of extracellular matrix (ECM) have been printed such that cells occupy one line and move randomly in 1D [13, 14] or span several lines [15-18]. Finally, aligned collagen fibrils have been epitaxially grown on mica [19]. Epitaxial growth of aligned collagen has several advantages. This contact guidance cue is formed using a native ECM protein and certain *in vivo* structural characteristics of collagen fibrils like D-banding are retained [20]. These substrates have been used to assess contact guidance in fibroblasts [21]. In addition, we recently used these substrates to show that cancer cells that migrate with similar speed, but different migration mode, sense contact guidance cues with vastly different directional fidelity [22].

While all cells share basic migration steps including adhesion and contractility that results in traction generation or tail retraction, these steps are regulated differently among cells. Migration phenotypes have begun to be more rigorously defined and are commonly referred to as migration modes. Different signaling pathways are required for each migrational mode and blocking or enhancing certain pathways can allow a cell to switch between modes. Adhesion is regulated by integrin binding to ECM proteins like collagen. Integrins are activated either by intracellular focal adhesion (FA) molecules or manganese ions (Mn^{2+}), resulting in higher affinity interactions with the ECM [23]. In particular, $\beta 1$ integrin activation seems to increase traction force [24]. Attenuating integrin interactions with the ECM switches cells from a mesenchymal to amoeboid mode of migration [25]. Integrins initiate the assembly of FAs and recruitment of FA proteins such as paxillin. Paxillin is phosphorylated on several sites including pY118 that leads to FA turnover and maturation [26, 27]. Paxillin phosphorylation and the accompanying FA turnover and maturation are brought on by myosin-mediated contractility that is controlled by the phosphorylation of myosin II regulatory light chain (MRLC) by myosin light chain kinase (MLCK) and Rho kinase (ROCK) [26-28]. In the context of migration modes, the amoeboid mode depends on

Rho/ROCK signaling to generate cortical contractility and blocking ROCK activity can switch cells from amoeboid to mesenchymal migration [29, 30]. However, much of the work outlining the differences in migration modes has been carried out in randomly migrating cells with no external directional cue.

Both adhesion and contractility are important during contact guidance. Work on gratings has shown that directional fidelity is dependent on FA maturation [31, 32], however the role of paxillin phosphorylation in contact guidance is not clear. Cells spreading on gratings requires myosin contractility through the Rho/ROCK pathway for directional alignment [33, 34], but other Rho GTPases like Cdc42 and Rac [35, 36] and MLCK [37] are dispensable. In addition, contact guidance in 3D systems depends on ROCK, but not MLCK phosphorylation of MRLC [6]. However, no study has examined the role of MRLC phosphorylation on stress fibers or paxillin phosphorylation in FAs during contact guidance. Furthermore, no study has examined contact guidance fidelity in response to adhesion and contractility perturbations across cell lines that migrate with different migration modes.

In this paper, we benchmark contact guidance on epitaxially grown collagen fibrils with two other common contact guidance cues (μ CP lines and gratings) in MDA-MB-231 (mesenchymal) and MTLn3 (amoeboid) cells. We show that both cell lines migrate similarly on μ CP collagen and gratings. However, epitaxially grown, aligned collagen fibrils generated distinct migration behavior as we have demonstrated before [22]. MDA-MB-231 cells sense contact guidance with high fidelity, but MTLn3 cells, sense contact guidance cues with low fidelity. We then perturb ROCK-mediated contractility and β 1 integrin-mediated adhesion and show that directionality can be tuned up or down in cells roughly independent of cell speed. MDA-MB-231 cells can be made to be less directional after contractility or adhesion inhibition, whereas MTLn3 cells can be made to be more directional after contractility or adhesion enhancement. The perturbations that generate these dramatic changes in directionality alter MRLC and paxillin phosphorylation when localized to stress fibers and in FAs. Additionally, while dual perturbations of contraction and adhesion yield synergistic migration speed responses, additive or saturated directionality responses are observed, suggesting that contraction and adhesion have overlapping roles in modulating cell directionality. Finally, while MRLC phosphorylation on stress fibers is poorly predictive of cell migration speed on contact guidance cues, directionality is directly proportional to MRLC phosphorylation on stress fibers across numerous conditions and cell lines.

Materials and methods

Cell culture and reagents

A human mammary basal/claudin low carcinoma cell line (MDA-MB-231, ATCC, Manassas, VA, USA) was cultured in Dulbecco's Modified Eagles Medium (DMEM) (Sigma Aldrich, St. Louis, MO, USA) containing 10% fetal bovine serum (FBS) (Gibco, Grand Island, New York, USA) and 1% penicillin-streptomycin (pen-strep) (Gibco) at 37°C in 5% CO₂. A rat mammary basal adenocarcinoma cell line (MTLn3, Jeffrey E. Segall, Albert Einstein College of Medicine) was authenticated using IDEXX BioResearch (Westbrook, Maine, USA) and cultured in MEM α (Gibco) supplemented with 5% FBS (Gibco) and 1% pen-strep (Gibco) at 37°C in 5% CO₂. Imaging media for MDA-MB-231

and MTLn3 cells was the same as the subculturing media, with the exception that no phenol red was included and that 12 mM HEPES (Sigma Aldrich) was included.

Collagen substrate treatment

High concentration non pepsin treated rat tail collagen type I (Corning, Corning, NY, USA) was used for the contact guidance cues. Four different types of contact guidance cues were made. The first two substrates involved depositing heterotrimeric collagen onto functionalized glass. Collagen was adsorbed ($3 \mu\text{g ml}^{-1}$ in solution for 1 hr) or microcontact printed onto no. 1 1/2-22 mm square coverslips (Corning). Cover slips were cleaned [38] and functionalized with 1% aminopropyltriethylsilane (Fisher Scientific, Hampton, New Hampshire, USA) in 10 mM acetic acid (Alfa Aesar, Ward Hill, MA, USA) and 6% glutaraldehyde (Electron Microscopy Sciences, Hatfield, PA, USA) in phosphate buffered saline (PBS) without calcium and magnesium (Gibco). Polydimethylsiloxane (PDMS) stamps were made by mixing 184 Silicone Elastomer Base (Dow Corning, Midland, MI, USA) with its curing agent in a 10:1 weight ratio and then allowing it to spread on top of a silicon master fabricated at the Minnesota Nanocenter (University of Minnesota, Minneapolis, MN, USA). The master coated with PDMS was exposed to a vacuum to remove any air bubbles and then cured for 1 hr at 60°C . PDMS stamps were sonicated in double distilled water and in 100% ethanol. A $200 \mu\text{l}$ collagen solution of $60 \mu\text{g ml}^{-1}$ collagen I in 0.5 M acetic acid was applied to each stamp. After 40 min incubation, the collagen solution was removed and then the stamp was placed on the functionalized coverslip and allowed to incubate for 15 min. Later, the stamp was removed generating lines $3 \mu\text{m}$ in width spaced $3 \mu\text{m}$ apart (Fig. 1C) [15].

The third substrate involved generating a grating. Shallow and deep gratings containing ridges and grooves (shallow: $0.1 \mu\text{m}$ deep with $1.5 \mu\text{m}$ pitch and deep: $3 \mu\text{m}$ deep with $6 \mu\text{m}$ pitch, Fig. 1D-H) were prepared from CD-Rs and the masters used for μCP mentioned above. Commercial CD-Rs consist of layers including polycarbonate, dye, gold, lacquer and polymer coatings. A thin layer (50-100 nm) of gold is coated on the dye and polycarbonate layers which have a spiraling pregroove. To expose the pregroove, the lacquer and polymer coatings on the CD-Rs were removed [39]. The CD-Rs were cut to size first and then immersed in concentrated nitric acid (Sigma) for 4 min. The lacquer and polymer coatings delaminated spontaneously, exposing the gold grating. Then the CD-R pieces were washed with deionized water and ethanol several times and dried with nitrogen gas. The prepared grating topography was transferred to PDMS as was done for the μCP and cells were plated on the PDMS generated grating. Gratings were inverted on a $150 \mu\text{l}$ collagen solution of $3 \mu\text{g ml}^{-1}$ collagen I in 0.5 M acetic acid.

The final substrate involved assembling aligned collagen fibrils on atomically smooth mica. Collagen fibrils were epitaxially grown on $15 \text{ mm} \times 15 \text{ mm}$ pieces of muscovite mica (highest grade VI, Ted Pella, Redding, CA, USA) that were freshly cleaved using tape [22]. Collagen type I was diluted ($10 \mu\text{g ml}^{-1}$) in the buffer solution consisted of 50 mM Tris-HCl (Fisher Scientific) and 200 mM KCl (Fisher Scientific) at pH 9.2. After incubation of 6-18 hrs the collagen solution was washed with deionized water, the mica was laid against the edge of a tissue culture dish and the mica was allowed to dry overnight and was used the

next day. This protocol generated aligned collagen fibrils over the entire mica substrate (Fig. 1A&B).

Characterizing substrates

A Dimension 3100 scanning probe microscope with Nanoscope IV controller (Veeco Metrology, LLC, Santa Barbara, CA) was used to obtain height images of collagen fibrils on mica. Imaging was conducted in tapping mode using silicon TESP7 AFM tips (Veeco Metrology, LLC, Santa Barbara, CA) with a spring constant of ~ 79 N/m and resonance frequency of ~ 269 kHz. Collagen fibrils were marked through attachment of 40 nm carboxylate-functionalized polystyrene spheres with embedded fluorophore (580/605) (Molecular Probes, Eugene, OR, USA) diluted into PBS. Aligned fibrils on a mica substrate were incubated with the fluorescent spheres for 1 hr. After the sample was dried at room temperature, the fluorescent spheres were imaged by epifluorescence using at 10 \times (NA 0.5, Nikon, Tokyo, Japan) with a charge-coupled device (CoolSNAP HQ2, Photometrics, Tucson, AZ, USA) attached to an inverted microscope (Ti-E, Nikon) that was driven by μ Manager [40]. A P-7 Stylus Profiler (KLA Tencor corporation, Milpitas, California, USA) was utilized to perpendicularly scan the line of shallow and deep gratings.

Live cell imaging

Cells were plated at 40,000-50,000 cells ml⁻¹ in 2 ml of media in 35 mm dishes. MDA-MB-231 cells were incubated for 2 hrs supplemented with blebbistatin (Sigma Aldrich), ML-7 (Sigma Aldrich), Y-27632 (Calbiochem, Billerica, MA, USA), P5D2 β 1 integrin blocking antibody (mouse mAb, ascites, from Mark Ginsberg, University of California, San Diego) [41], calyculin A (Santa Cruz Biotechnology, Dallas, TX, USA) and MnCl₂ (Fisher) and MTLn3 cells were incubated for 12 hrs with supplemented with calyculin A, MnCl₂, Y-27632, and P5D2 on contact guidance cues in imaging media. Substrates with attached cells were inverted onto two strips of double sided tape attached to a microscope slide to generate a flow chamber. The chamber was filled with imaging media and sealed with a 1:1:1 mixture of vasoline, lanolin and paraffin wax. Chambers were imaged by phase contrast microscopy on a heated stage at 37°C every 2 min for 12 hrs. Images were captured at 10 \times (NA 0.50, Nikon) as described above.

Cell centroids were identified and tracked manually using the MTrackJ plugins of ImageJ (National Institutes of Health, Bethesda, MD, USA). Cell speed and directionality were calculated over a time lag of 2 min averaged over 12 hrs as described in a previous paper [15].

Fluorescence imaging

Cells were plated at 40,000-50,000 cells ml⁻¹ in 2 ml of media in 35 mm dishes. MDA-MB-231 cells with 1 μ M Y-27632 were incubated for 5 hours, MDA-MB-231 cells with 0.1 μ l ml⁻¹ P5D2 antibody were incubated for 12 hrs and MTLn3 cells with 0.01 nM calyculin A and 0.1 mM MnCl₂ were incubated for 12 hours on highly aligned type I collagen fibrils, fixed with 4% paraformaldehyde (Fisher), permeabilized with 0.5% triton-X (Fisher) and stained for F-actin, pS19-myosin regulatory light chain (pS19-MRLC), and pY118-paxillin (pY118-Pax), a FA protein. F-actin was stained using alexa 488-phalloidin (Molecular

Probes) and pS19-MRLC (mouse mAb, 1:50, 3675, Cell Signaling Technology, Danvers, Massachusetts, USA) and pY118-Pax (rabbit pAb, 1:100, 2541, Cell Signaling Technology, Danvers, Massachusetts, USA) were stained using antibodies [42]. The secondary antibodies were donkey anti-mouse Cy3 and anti-rabbit Cy5 antibody (715-165-150 & 711-175-152, 1:400, Jackson Immuno Research, West Grove, PA, USA). Fixed and stained cells were imaged by epifluorescence using a 20× air objective (NA 0.45, Nikon) and a 60× oil objective (NA 1.49, Nikon) on the same microscope as described above.

Fluorescence intensity was calculated using home build macros in ImageJ (National Institutes of Health). Whole cell raw fluorescence intensity was calculated by adjusting the threshold of a population of cells in one image (20×) or one cell (60×), outlining them and logging the average thresholded intensity. The local background was calculated from the average grey value of bands around each thresholded cell. Fluorescence was calculated as the difference between whole cell raw fluorescence and background fluorescence. Stress fiber and FA raw fluorescence intensity was calculated by first generating a stress fiber or FA mask using the F-actin or pY118-Pax images, respectively. Images were background subtracted using a rolling ball radius method (2 pixels) and a threshold was adjusted to clearly visualize stress fibers or FAs, which were logged as regions of interest (ROIs). These ROIs were used to make a mask that defined regions in the pS19-MRLC image to compute the stress fiber or FA raw fluorescence intensity. The average length to width ratio of stress fibers was computed by fitting ellipses to each stress fiber and computing the average for each condition. Background fluorescence was calculated around the cell as described above and fluorescence was calculated as the difference between whole cell raw fluorescence and background fluorescence.

Confocal imaging was carried out using 63× (NA 1.40, Leica Microsystems, Exton, PA, USA) on a SP5X MP confocal microscope (Leica Microsystems). *Z*-slices were taken at 0.42 μm steps. Stacks of F-actin and pMRLC images were analyzed in Image J. They were first filtered using a mean filter. Contrast was adjusted to scale F-actin and pMRLC intensity similarly and the F-actin and pMRLC channels were merged. Voxel depths in image properties were changed to the slice distance and orthogonal views were produced in the *xz*- and *yz*-planes.

Statistics

The number of experiments and cells were stated in all the figure legends. At least three independent experiments were conducted. In general, means were calculated with error bars representing 95% confidence intervals. Differences between control and perturbation experiments were determined using a two-tailed student's *t*-test and significance was assigned when $p < 0.05$. Predicted dual perturbation 95% confidence intervals were calculated by summing the standard deviations of each perturbation and calculating a *t*-value with a weighted average of the total number of experiments.

Results

Diverse contact guidance cues elicit distinct migration responses

It has been shown that contact guidance drives cell migration along the long axis of aligned ECM fibers or fiber mimics. While several methods have been used to present contact guidance cues, a direct comparison between methods is lacking. Consequently, we compared a topographical cue (gratings) and a chemical cue (μ CP lines of collagen) to highly aligned epitaxially grown collagen fibrils (Fig. 1). We chose to examine two breast cancer cell lines (MDA-MB-231 and MTLn3 cells) (Fig. 2). These cells have distinct migration modes in 3D (Fig. 2B) [30, 43] and engage in contact guidance on aligned collagen fibrils with dramatically different fidelity [22]. MDA-MB-231 and MTLn3 cells are highly invasive [44, 45] and they both metastasize to the lung *in vivo* [45-47]. MDA-MB-231 cells have been shown to be quantitatively more invasive than MTLn3 cells [44]. MDA-MB-231 cells elongate on most contact guidance cues and often times exhibit bifurcated extensions (Fig. 2A). MTLn3 cells on the other hand only elongate on μ CP lines of collagen and usually exhibit a much more spread phenotype with one broad protrusion (Fig. 2A). We quantified both the contact guidance fidelity by calculating the directionality of movement (Fig. 2C), which is the projection of movement in the direction of the contact guidance cue and the migration speed (Fig. 2D). Migration on uniform surfaces of collagen result in low values of directionality and approximately equal speeds in both cell lines. The strength of each contact guidance cue differs. Shallow gratings induce weak contact guidance, whereas deep gratings induce high contact guidance. Both grating conditions resulted in relatively high cell speed. μ CP lines of collagen induce strong contact guidance in a similar fashion to deep gratings. Neither gratings nor μ CP result in large differences in directionality between MDA-MB-231 and MTLn3 cells. On highly aligned collagen fibrils, the contact guidance response was intermediate. Interestingly, MDA-MB-231 cells had almost a three-fold higher directionality than MTLn3 cells on highly aligned collagen fibrils ($p < 0.05$), while at the same time migrating at roughly the same speed (Figs. 1C and D). Given these differences between MDA-MB-231 and MTLn3 cells in contact guidance on highly aligned collagen fibrils, we were interested in determining why these cells respond uniquely to one particular directional cue.

Contractility and adhesion are regulators of migration mode-dependent contact guidance efficiency

Several studies have shown that modulating contractility and adhesion through Rho-family GTPases and integrin activation engenders plasticity to cells, allowing them to switch between migrational modes [25, 29, 48]. In addition, MDA-MB-231 and MTLn3 cells exert different traction forces on their surroundings [30, 49, 50]. Traction force is intimately tied to both contraction and adhesion. Consequently, contractility and adhesion likely play roles in determining contact guidance efficiency between cells of different migration modes. Because MDA-MB-231 cells exert more traction force, we sought to decrease either the contractility or adhesion. Conversely, MTLn3 cells exert less traction force, so we sought to increase either the contractility or adhesion. Therefore, MDA-MB-231 cells on highly aligned collagen fibrils were treated with blebbistatin (myosin II inhibitor, [51]), ML-7 (myosin light chain kinase inhibitor, [52]), Y-27632 (Rho kinase inhibitor, [53]) or P5D2

antibody (β 1-integrin adhesion inhibitor, [41]) (Fig. 3 & 4). MTLn3 cells on the same substrates were treated with calyculin A (myosin phosphatase inhibitor, [54]) or $MnCl_2$ (integrin activator, [55]) (Fig. 5 & 6). We examined contact guidance behavior as well as the spatial distribution and abundance of actomyosin cytoskeletal and FA markers, namely F-actin, MRLC S19 phosphorylation (pS19-MRLC) and paxillin pY118 phosphorylation (pY118-Pax). F-actin and pS19-MRLC tended to localize on stress fiber structures in both MDA-MB-231 and MTLn3 cells, although there was some areas where F-actin showed brighter staining than pS19-MRLC (lamellipodial extensions) or where pS19-MRLC showed brighter staining than F-actin (lamella regions) (Fig. S1).

We first examined MDA-MB-231 cells with decreased contractility. Our approach was to use sub-maximal inhibitor concentrations, allowing us to tune the contractility in small increments, but also to limit off target effects. ROCK seems to be unique in its effect on contact guidance (Fig. 3C). The only perturbation that affects cell speed was blocking myosin II activity using blebbistatin (Fig. 3D). Doses of blebbistatin above 30 μ M completely inhibit cell migration (data not shown), precluding our ability to calculate directionality. Blocking MLCK or myosin II activity diminishes directionality only slightly (Fig. 3C). On the other hand, blocking ROCK with sub-maximal doses of Y-27632 dramatically diminishes the directionality, while not affecting speed to a great extent (Fig. 3C and D), demonstrating that directionality and speed have different dose responses. In addition, we tested whether adhesion modulation regulates migration directionality. Submaximal doses of P5D2, a β 1 integrin blocking antibody, decreases cell directionality, but not cell speed. This mimics what is seen with ROCK inhibition. Both ROCK inhibition and β 1 integrin blocking result in lower whole cell F-actin content, pS19-MRLC and pY118-Pax (Fig. 3E-G). These perturbations also result in shorter and less dense F-actin bundles (Fig. 4C and D) and less pS19-MRLC localized to stress fibers and FAs (Fig. 4E and G). Finally, pY118-Pax at FAs is also decreased (Fig. 4F). Given that decreases in ROCK-mediated contractility and β 1 integrin-mediated adhesion result in decreased directionality in mesenchymal mode MDA-MB-231 cells, we decided to increase contractility and adhesion in amoeboid cells to see if a mirrored result could be generated.

MTLn3 cells were treated with a contractility enhancer, calyculin A, a myosin phosphatase inhibitor that enhances MRLC phosphorylation. High doses of calyculin A are toxic and arrest migration (Fig. 8B and data not shown), but lower doses increase directionality by almost two-fold (Fig. 5C). Migration speed is only decreased by \sim 20% (Fig. 5D). Similar to MDA-MB-231 cells the dose response of directionality in response to contractility is different than that for speed in MTLn3 cells. Additionally, when adhesion is enhanced by adding $MnCl_2$, which activates integrins and increases their affinity towards their ligands, MTLn3 directionality increases (Fig. 5C). Migration speed is unaffected (Fig. 5D). Changing the contractility and adhesion with submaximal doses of either calyculin A or $MnCl_2$ results in no large changes in whole cell pS19-MRLC or pY118-Pax level (Fig. 5F-G). However, stress fibers appear robustly in MTLn3 cells treated with either calyculin A or $MnCl_2$ (Fig. 6A-D). In addition, the pS19-MRLC level on stress fibers increases as well as the pY118-Pax levels in FAs (Fig. 6E-G).

Decreasing contractility or adhesion in MDA-MB-231 cells results in diminished directionality and increasing contractility or adhesion in MTLn3 cells results in enhanced directionality. Speed is unaffected. However, we were interested if MDA-MB-231 cells could be made more directional and MTLn3 cells could be made less directional on aligned fibrils. Consequently, we used calyculin A and MnCl_2 to enhance contractility and adhesion in MDA-MB-231 cells (Fig. S2A). Directionality is enhanced, but speed is diminished. However, Y-27632 and P5D2 antibody treatment of MTLn3 cells do not affect directionality or speed (Fig. S2B).

Contractility and adhesion inhibition have a synergistic effect on speed, but additive or saturated effect on directionality

In Fig. 3, we showed evidence that inhibiting ROCK-mediated contractility or $\beta 1$ integrin-mediated adhesion in MDA-MB-231 cells diminishes directionality. However, we were also interested in how simultaneous changes in contractility and adhesion affect cell migration. Here, we propose three possibilities to describe the response of dual perturbations (Fig. S3A). The change in level of the cell response (migration directionality or speed) between control and inhibition 1 in isolation and control and inhibition 2 in isolation is denoted by I_1 and I_2 , respectively (Fig. S3A). The predicted change in cell response when two perturbations are used simultaneously is $I_1 + I_2$. If the response is additive, the predicted response should match the measured response. If the response is synergistic, then the predicted level will be larger than experimental level. Saturated cell responses occur when the predicted level is smaller than the expected level. Since maximum concentrations of inhibitors completely blocked cell migration (data not shown), precluding our ability to calculate directionality, we probed sub-maximum concentrations that perturbed directionality, but kept speed roughly unchanged. Thus, we investigated dose responses of Y-27632 or P5D2 antibody on MDA-MB-231 cells (Fig. 7A-D). At higher concentrations of Y-27632 (0.5 μM) cell directionality decreases to untreated levels (black bars, Fig. 7A), but larger concentrations of Y-27632 (1 μM) dramatically decreases cell directionality (gray bar, Fig. 7A). Maximally disrupting ROCK activity (10 μM Y-27632, white bar) decreases directionality to the same extent as 1 μM Y-27632 (Fig. 7A). Because the dose response of directionality and speed were different, we defined a dose as a low dose if it does not interrupt either directionality or speed (black bars). We defined a dose as a submaximal dose if it interrupts directionality, but not speed (grey bars). Finally, maximal doses interrupt both directionality and speed (white bars). We then treated MDA-MB-231 cells with intermediate or sub-maximal concentrations of Y-27632 and P5D2 antibody and analyzed cell speed and directionality. After blocking ROCK and $\beta 1$ integrin adhesion with low doses of Y-27632 and P5D2 antibody or a low dose of Y-27632 and submaximal dose of P5D2 antibody, cell directionality exhibits an additive relationship, because no difference is seen between the predicted and experimental levels. Only when two sub-maximal doses are used does a saturated response ensue (Fig. 7E). This represents a lower bound on changing directionality through contraction or adhesion that is well above 0. Interestingly, blocking ROCK and $\beta 1$ integrin adhesion with low or submaximal doses of Y-27632 and P5D2 antibody produces synergistic effects on speed (Fig. 7F).

Contractility and adhesion enhancers have an additive or saturated effect on both directionality and speed

When a perturbation enhances a response, the definitions for synergistic and saturated are inverted. The change in level of the cell response between control and enhancer 1 in isolation and control and enhancer 2 in isolation is denoted by E_1 and E_2 , respectively (Fig. S3B). The predicted change in cell response when two perturbations were used simultaneously is $E_1 + E_2$. If the response is additive, the predicted response should match the measured response. If the response is synergistic, then the predicted level will be smaller than the experimental level. Saturated cell responses occur when the predicted level is larger than the expected level. For the same reasons described above we probed sub-maximum concentrations that perturbed directionality, but kept speed unchanged. Thus, we investigated dose responses of calyculin A or MnCl_2 on MTLn3 cells (Fig. 8A-D). Mildly enhancing contractility (black bars, 0.001 nM calyculin A) does not change MTLn3 cell directionality. At 0.002 nM calyculin A (gray bars), cell directionality quantitatively increases, while speed remains roughly constant. At higher concentrations of 0.01 nM calyculin A (white bars), cell directionality increases further, but migration speed also decreases. Calyculin A concentrations above 0.01 nM were not assessed due to cell toxicity or complete inhibition of cell migration. Low doses, submaximal and maximal doses are defined as mentioned above. Enhancing contractility and adhesion with intermediate doses of calyculin A and MnCl_2 results in additive cell directionality. Only when a maximal and submaximal dose of calyculin A and MnCl_2 were combined is a saturated directionality response observed (Fig. 8E and F). Again, directionality appears to reach a saturating level that is well below the maximum of 1. Speed on the other hand is additive (Fig. 8E and F).

Discussion

In this paper we show that the way in which contact guidance cues are presented robustly controls the directional fidelity of cancer cells. Shallow gratings are relatively weak directional cues, whereas deep gratings and μCP lines of collagen are potent. Epitaxially grown, aligned collagen fibrils result in intermediate potency, but result in differences between two model breast cancer cell lines: MDA-MB-231 and MTLn3 cells. MDA-MB-231 cells are more directional than MTLn3 cells and this may translate to quantitatively higher invasion and migration that is seen *in vivo* [44]. Small decreases in ROCK-mediated contractility or $\beta 1$ integrin-mediated adhesion (Fig. 9B, blue oval with black circles) decreases directional fidelity in MDA-MB-231 cells (mesenchymal), whereas small increases (Fig. 9A, yellow oval with black circles) increases directional fidelity. On the other hand, small decreases in ROCK-mediated contractility or $\beta 1$ integrin-mediated adhesion (Fig. 9B, blue oval with gray squares) does not affect directionality greatly in MTLn3 cells (amoeboid), but does decrease speed, whereas small increases (Fig. 9A, yellow oval with gray squares) increases directionality and decreases speed. Inhibiting contractility or making large decreases in ROCK-mediated contractility diminishes both speed and directionality in MDA-MB-231 cells (Fig. 9A, purple oval). Interestingly, the level of phosphorylation of pS19-MRLC in stress fibers and pY118-Pax in FAs appear to predict cell directionality (Fig. 9C and D). These same conditions do not result in large changes in cell speed (Fig. 9E and F), indicating that directionality correlates sensitively to changes in ROCK-mediated myosin

contractility and paxillin phosphorylation. When both contractility and adhesion are tuned the resultant directionality is often additive, i.e. the result was the sum of the changes seen in each single perturbation. Saturation is also observed indicating that there are limits in the ability to tune contact guidance fidelity in different cell types by altering contractility and adhesion. Migration speed on the other hand, is either additive or synergistic.

Potency of contact guidance cues in directing cell migration

Numerous approaches have been used to study contact guidance *in vitro*. However, these contact guidance cues could either be potent or weak, so much work has focused on what features of the cue enhance or degrade contact guidance fidelity. On gratings cell alignment percentage or average directionality increases with increased pitch size (ridge + groove width), but more sensitively with increased groove depth. The feature size used in this paper matches previously work [10, 11, 56, 57] on non-cancer cells. Directionality from cell migration tracks was not assessed in any of these studies, but static images were used to calculate the percentage of cells aligned to within 10°. This percentage was 60% for fibroblasts and 10-20% for epithelial cells. The cell directionality was greater than 0.9 for fibroblasts, whereas endothelial and smooth muscle cells showed a directionality of 0.3, indicating that the phenotypes of the cancer cells examined in this paper lie closer to the endothelial or smooth muscle cells. More contractile cells like fibroblasts seem to engage in higher fidelity contact guidance than less contractile cells like epithelial cells [9, 56-59]. In addition to gratings, μ CP has been used as a contact guidance cue. The average directionality increases with increased line period [60, 61], spacing [15, 16] and adhesiveness [15, 16]. The directionality of MTLn3 cells in this study matches well with what we have seen previously [15]. When comparing gratings to μ CP lines of ECM, others have shown that gratings are less potent than lines at dimensions that approximately match ours [62], whereas larger dimensions show that gratings are more potent [63]. We show that indeed potency depends on grating depth, but under the conditions that we probed no cell type differences were found.

However, only when we used epitaxially grown, aligned collagen fibers did we observe large differences between cell lines. First, it is possible that tuning either the gratings to be more potent or the μ CP lines to be less potent would result in similar cell type differences. Indeed, others have seen cell type differences on gratings [9, 56-59]. Potency of the contact guidance cue is an important factor for *in vitro* studies. Directed migration *in vivo* often does not occur with high fidelity, because of noise in the directional signal. This noise can lead to dramatically different directional sensing outputs [64], so intermediate potencies are likely more appropriate environments. Second, it is possible that the structure of collagen is important. Epitaxially grown, aligned collagen fibers form D-bands structures with periodic gaps and overlap regions that match well with collagen structures *in vivo* [20]. However, both μ CP lines of collagen and gratings are coated with heterotrimeric unpolymerized collagen. Cells might be able to sense D-banding, thus increasing directional fidelity [21]. Third, it is possible that the mechanical properties govern this difference. Both gratings and μ CP lines of collagen are stiff. However, epitaxial collagen assembled onto mica is only weakly attached to the surface and fibrils can be remodeled through cell traction force.

Future work will be focused on transferring collagen fibers to flexible substrates and examining the role of mechanics in governing contact guidance in these systems.

Myosin phosphorylation on stress fibers and paxillin phosphorylation in adhesions as mediators of contact guidance

Others have shown that contact guidance depends on myosin contractility. Inhibiting myosin contractility decreases alignment in smooth muscle cells [32], endothelial cells [34], MTLn3 cells [15] and neurons [37, 65]. Interestingly, contact guidance of T cells seems to be unaffected by decreases in contractility [66]. This is consistent with the fact that T cells exert weak traction forces. This observation agrees largely with our data showing that MTLn3 directionality does not decrease below the control condition in response to decreases in contractility or adhesion (Fig. 9A and B) and further suggests that additional factors set the range over which cells can tune their directionality on contact guidance cues. In our previous work, MTLn3 cell directionality did decrease in response to decreases in contractility, but this was on a much more potent contact guidance cue, μ CP lines of collagen [15]. The Rho/ROCK pathway seems to be the determining factor for directional fidelity in osteoblasts [33], endothelial [34], stem cells [33] epithelial cells [35, 36] and neuron cells [37] and both increases and decreases can tune up or down the alignment of cells [35]. The Rho/ROCK pathway also appears to control contact guidance in 3D [6]. Other Rho GTPases like Cdc42 or Rac [35, 36] and other myosin kinases like MLCK are unimportant [37]. The dependence of directionality on Rho/ROCK is distinct to 1D, 2D or 3D random migration systems, where Rac seems to be the driver of “directional migration” or persistence [67]. Furthermore, in random motility others have shown a correlation between speed and directional persistence [68]. However, we observe that directionality and speed are not highly correlated (Fig. 9A and B). In random motility systems, polarization acts to enhance speed, such that as directionality increases, speed increases as well through an F-actin retrograde flow-dependent mechanism. Contact guidance likely relies on extrinsic polarity that is brought about through the formation of contractile stress fibers templated by the aligned collagen fibers and that operates differently than intrinsic polarity present during random migration.

In comparison to contractility, there have been fewer studies examining the requirements of adhesion during contact guidance. Recently, β 1 integrin was shown to be important in confined migration [69] and β 1 integrin is important in generating traction forces [24]. Both of these lines of evidence indicate a role for β 1 integrin during contact guidance. In addition, others have shown that contact guidance fidelity is dependent on FA maturation [31], which was assayed through morphological analysis of FAs, but no compositional analysis was performed. Paxillin phosphorylation can mark FA maturation, but it also marks FAs with high turnover, allowing cells to pull up FAs oriented away from the direction of the contact guidance cue leading to enhanced orientation along the contact guidance cue [32]. In addition to contact guidance, paxillin regulates durotaxis [70]. In particular, inhibition of the phosphorylation of Y118 abrogates durotaxis by inhibiting force fluctuations at FAs. While contact guidance is not the same as durotaxis it does share some features [71], particularly in the context of epitaxially grown, aligned collagen fibers. Cells can deform the collagen fibrils attached to the mica. The observed stiffness in the longitudinal direction is likely

higher than that in the perpendicular direction. This could be thought of as setting up a circumferential gradient in observed stiffness based on the orientation of the cells, forcing cells to turn towards the stiffer direction, i.e. the longitudinal direction. This could explain similarities in the contractile and adhesion apparatus used in contact guidance and durotaxis.

Contractility and adhesion balancing regulate contact guidance

While both ROCK-mediated contractility and $\beta 1$ integrin-mediated adhesion appear to regulate contact guidance, their roles in controlling directionality are similar. We first posited a role for contractility in contact guidance from earlier work [15], however this was on μ CP lines that resulted in higher cell directionality. Our hypothesis was that while migration speed is a biphasic function of contraction and adhesion, directionality was more or less monotonic with a possible saturation point. Indeed, we observe saturating behavior for both MDA-MB-231 (Fig. 7) and MTLn3 (Fig. 8), when combinations of larger perturbations are used. The current reason for this saturation behavior is not known, however it is not due to the stalling of migration. For small perturbations, the effects on contraction and adhesion are approximately additive, suggesting that both contractility and adhesion share in determining directionality through stress fiber formation brought on by MRLC phosphorylation. A recent modeling effort has examined dual perturbations in contractility (motor function) and adhesion (clutch function) in regulating the stiffness at which the maximum migration speed occurs [72]. Combinations of perturbations of parameters that describe both the motor and clutch function cooperate to change the sensitivity of the optimal stiffness. We also see changes in speed under dual perturbations that are additive, but some are synergistic, i.e. the experimental response is more dramatic than the predicted response. Feedback between contractility and adhesion might allow sensitivity in regulating migration speed during contact guidance, even though smaller single perturbations seem to more dramatically affect directionality during contact guidance.

We are beginning to understand the cytoskeletal structures, FA species and intracellular signaling that is intrinsic to different forms of directional migration. Non-overlapping structures and pathways seem to distinguish different directional sensing mechanisms. While chemotaxis, directed migration in response to a soluble gradient, appears to be dependent on Cdc42 [73], N-WASP [74] and cofilin [75], haptotaxis, directed migration in response to a insoluble matrix-bound gradient, appears to be heavily dependent on Rac, Wave and Arp2/3 [76, 77]. Durotaxis on the other hand requires the cycling of paxillin phosphorylation and FA force [70]. Finally, contact guidance requires ROCK-mediated contractility and results in changes in paxillin phosphorylation. Discovering the signaling pathways during each form of directed migration will further our ability to predict migrational responses in the environments including the TME where multiple directional cues are presented.

Conclusions

In this paper we show that the potency of different contact guidance cues varies dramatically. μ CP lines of collagen are highly potent, whereas gratings are less potent. Epitaxially grown, aligned collagen fibrils represent intermediate potency that illuminates differences among breast cancer cells with different migration mode. MDA-MB-231 cells (mesenchymal mode)

sense contact guidance with high fidelity, but this directional fidelity can be decreased by inhibiting ROCK-mediated contractility and $\beta 1$ integrin-mediated adhesion. In contrast, MTLn3 cells (amoeboid mode) sense contact guidance with low fidelity, but this directional fidelity can be increased by enhancing contractility or activating integrins. Dual perturbations of contractility and adhesion result in additive changes in directionality, indicating that alterations in contraction and adhesion are interchangeable. Perturbations in contractility and adhesion that generate dramatic changes in directionality alter MRLC and paxillin phosphorylation slightly on a whole cell level, but much more intensely when localized to stress fibers and in FAs. MRLC phosphorylation on stress fibers and paxillin phosphorylation in FAs are poorly predictive of cell migration speed on contact guidance cues, but predict directionality well across different contractility and adhesion perturbations in two cell lines with distinct motility modes.

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

Acknowledgments

We acknowledge Andrew Hillier, Joseph Petefish, Zhiqi Yao and Mir Md Hossen with help in preparing and characterizing the collagen fibrils and gratings. ICS acknowledges support from the National Institutes of Health/ National Cancer Institute [R03CA184575] for general project funding. The content is solely the responsibility of the authors and does not necessarily represent the official views of the NIH.

References

1. Provenzano PP, Eliceiri KW, Campbell JM, Inman DR, White JG, Keely PJ. Collagen reorganization at the tumor-stromal interface facilitates local invasion. *BMC Med.* 2006; 4
2. Hanley CJ, Noble F, Ward M, Bullock M, Drifka C, Mellone M, et al. A subset of myofibroblastic cancer-associated fibroblasts regulate collagen fiber elongation, which is prognostic in multiple cancers. *Oncotarget.* 2016; 7:6159–74. [PubMed: 26716418]
3. Malik R, Lelkes PI, Cukierman E. Biomechanical and biochemical remodeling of stromal extracellular matrix in cancer. *Trends Biotechnol.* 2015; 33:230–6. [PubMed: 25708906]
4. Peranzoni E, Rivas-Caicedo A, Bougherara H, Salmon H, Donnadieu E. Positive and negative influence of the matrix architecture on antitumor immune surveillance. *Cell Mol Life Sci.* 2013; 70:4431–48. [PubMed: 23649148]
5. Guo C, Kaufman LJ. Flow and magnetic field induced collagen alignment. *Biomaterials.* 2007; 28:1105–14. [PubMed: 17112582]
6. Riching KM, Cox BL, Salick MR, Pehlke C, Riching AS, Ponik SM, et al. 3D Collagen Alignment Limits Protrusions to Enhance Breast Cancer Cell Persistence. *Biophysical Journal.* 2014; 107:2546–58. [PubMed: 25468334]
7. Singh S, Bandini SB, Donnelly PE, Schwartz J, Schwarzbauer JE. A cell-assembled, spatially aligned extracellular matrix to promote directed tissue development. *J Mat Chem B.* 2014; 2:1449–53.
8. Amatangelo MD, Bassi DE, Klein-Szanto AJP, Cukierman E. Stroma-derived three-dimensional matrices are necessary and sufficient to promote desmoplastic differentiation of normal fibroblasts. *Am J Pathol.* 2005; 167:475–88. [PubMed: 16049333]
9. Clark P, Connolly P, Curtis ASG, Dow JAT, Wilkinson CDW. Topographical control of cell behavior 2. Multiple grooved substrata. *Development.* 1990; 108:635–44. [PubMed: 2387239]
10. Teixeira AI, Abrams GA, Bertics PJ, Murphy CJ, Nealey PF. Epithelial contact guidance on well-defined micro- and nanostructured substrates. *Journal of Cell Science.* 2003; 116:1881–92. [PubMed: 12692189]

11. Loesberg WA, te Riet J, van Delft F, Schon P, Figdor CG, Speller S, et al. The threshold at which substrate nanogroove dimensions may influence fibroblast alignment and adhesion. *Biomaterials*. 2007; 28:3944–51. [PubMed: 17576010]
12. Tuft BW, Li SF, Xu LJ, Clarke JC, White SP, Guymon BA, et al. Photopolymerized microfeatures for directed spiral ganglion neurite and Schwann cell growth. *Biomaterials*. 2013; 34:42–54. [PubMed: 23069708]
13. Doyle AD, Wang FW, Matsumoto K, Yamada KM. One-dimensional topography underlies three-dimensional fibrillar cell migration. *Journal of Cell Biology*. 2009; 184:481–90. [PubMed: 19221195]
14. Maiuri P, Terriac E, Paul-Gilloteaux P, Vignaud T, McNally K, Onuffer J, et al. The first World Cell Race. *Current Biology*. 2012; 22:R673–R5. [PubMed: 22974990]
15. Romsey NR, Hou Y, Rodriguez LL, Schneider IC. The Number of Lines a Cell Contacts and Cell Contractility Drive the Efficiency of Contact Guidance. *Cell Mol Bioeng*. 2014; 7:122–35.
16. Borghi N, Lowndes M, Maruthamuthu V, Gardel ML, Nelson WJ. Regulation of cell motile behavior by crosstalk between cadherin- and integrin-mediated adhesions. *Proc Natl Acad Sci U S A*. 2010; 107:13324–9. [PubMed: 20566866]
17. Csucs G, Quirin K, Danuser G. Locomotion of fish epidermal keratocytes on spatially selective adhesion patterns. *Cell Motility and the Cytoskeleton*. 2007; 64:856–67. [PubMed: 17712861]
18. Kandere-Grzybowska K, Campbell CJ, Mahmud G, Komarova Y, Soh S, Grzybowski BA. Cell motility on micropatterned treadmills and tracks. *Soft Matter*. 2007; 3:672–9.
19. Jiang FZ, Horber H, Howard J, Muller DJ. Assembly of collagen into microribbons: effects of pH and electrolytes. *Journal of Structural Biology*. 2004; 148:268–78. [PubMed: 15522775]
20. Fang M, Goldstein EL, Matich EK, Orr BG, Holl MMB. Type I Collagen Self-Assembly: The Roles of Substrate and Concentration. *Langmuir*. 2013; 29:2330–8. [PubMed: 23339654]
21. Poole K, Khairy K, Friedrichs J, Franz C, Cisneros DA, Howard J, et al. Molecular-scale topographic cues induce the orientation and directional movement of fibroblasts on two-dimensional collagen surfaces. *J Mol Biol*. 2005; 349:380–6. [PubMed: 15890202]
22. Wang J, Petefish JW, Hillier AC, Schneider IC. Epitaxially Grown Collagen Fibrils Reveal Diversity in Contact Guidance Behavior among Cancer Cells. *Langmuir*. 2015; 31:307–14. [PubMed: 25531276]
23. Cluzel C, Saltel F, Lussi J, Paulhe F, Imhof BA, Wehrle-Haller B. The mechanisms and dynamics of $\alpha v \beta 3$ integrin clustering in living cells. *The Journal of Cell Biology*. 2005; 171:383–92. [PubMed: 16247034]
24. Lin GL, Cohen DM, Desai RA, Breckenridge MT, Gao L, Humphries MJ, et al. Activation of beta 1 but not beta 3 integrin increases cell traction forces. *FEBS Lett*. 2013; 587:763–9. [PubMed: 23395612]
25. Carragher NO, Walker SM, Carragher LSA, Harris F, Sawyer TK, Brunton VG, et al. Calpain 2 and Src dependence distinguishes mesenchymal and amoeboid modes of tumour cell invasion: a link to integrin function. *Oncogene*. 2006; 25:5726–40. [PubMed: 16652152]
26. Pasapera AM, Schneider IC, Rericha E, Schlaepfer DD, Waterman CM. Myosin II activity regulates vinculin recruitment to focal adhesions through FAK-mediated paxillin phosphorylation. *Journal of Cell Biology*. 2010; 188:877–90. [PubMed: 20308429]
27. Zaidel-Bar R, Milo R, Kam Z, Geiger B. A paxillin tyrosine phosphorylation switch regulates the assembly and form of cell-matrix adhesions. *Journal of Cell Science*. 2007; 120:137–48. [PubMed: 17164291]
28. Webb DJ, Donais K, Whitmore LA, Thomas SM, Turner CE, Parsons JT, et al. FAK-Src signalling through paxillin, ERK and MLCK regulates adhesion disassembly. *Nature Cell Biology*. 2004; 6:154–+. [PubMed: 14743221]
29. Sahai E, Marshall CJ. Differing modes of tumour cell invasion have distinct requirements for Rho/ROCK signalling and extracellular proteolysis. *Nature Cell Biology*. 2003; 5:711–9. [PubMed: 12844144]
30. Wyckoff JB, Pinner SE, Gschmeissner S, Condeelis JS, Sahai E. ROCK- and myosin-dependent matrix deformation enables protease-independent tumor-cell invasion in vivo. *Current Biology*. 2006; 16:1515–23. [PubMed: 16890527]

31. Cassidy JW, Roberts JN, Smith CA, Robertson M, White K, Biggs MJ, et al. Osteogenic lineage restriction by osteoprogenitors cultured on nanometric grooved surfaces: The role of focal adhesion maturation. *Acta Biomater.* 2014; 10:651–60. [PubMed: 24252447]
32. Saito AC, Matsui TS, Ohishi T, Sato M, Deguchi S. Contact guidance of smooth muscle cells is associated with tension-mediated adhesion maturation. *Experimental Cell Research.* 2014; 327:1–11. [PubMed: 24825188]
33. Calzado-Martin A, Mendez-Vilas A, Multigner M, Saldana L, Gonzalez-Carrasco JL, Gonzalez-Martin ML, et al. On the role of RhoA/ROCK signaling in contact guidance of bone-forming cells on anisotropic Ti6Al4V surfaces. *Acta Biomater.* 2011; 7:1890–901. [PubMed: 21115140]
34. Franco D, Klingauf M, Bednarzik M, Cecchini M, Kurtcuoglu V, Gobrecht J, et al. Control of initial endothelial spreading by topographic activation of focal adhesion kinase. *Soft Matter.* 2011; 7:7313–24.
35. Rajnicek AM, Foubister LE, McCaig CD. Alignment of corneal and lens epithelial cells by cooperative effects of substratum topography and DC electric fields. *Biomaterials.* 2008; 29:2082–95. [PubMed: 18281089]
36. Rajnicek AM, Foubister LE, McCaig CD. Prioritising guidance cues: Directional migration induced by substratum contours and electrical gradients is controlled by a rho/cdc42 switch. *Developmental Biology.* 2007; 312:448–60. [PubMed: 17976566]
37. Ferrari A, Cecchini M, Serresi M, Faraci P, Pisignano D, Beltram F. Neuronal polarity selection by topography-induced focal adhesion control. *Biomaterials.* 2010; 31:4682–94. [PubMed: 20304485]
38. Waterman-Storer, CM. Microtubule/Organelle Motility Assays Current Protocols in Cell Biology. John Wiley & Sons, Inc.; 2001.
39. Singh BK, Hillier AC. Surface plasmon resonance imaging of biomolecular interactions on a grating-based sensor array. *Analytical Chemistry.* 2006; 78:2009–18. [PubMed: 16536440]
40. Edelstein, A., Amodaj, N., Hoover, K., Vale, R., Stuurman, N. Computer Control of Microscopes Using μ Manager. John Wiley & Sons, Inc.; 2010.
41. Dittel BN, McCarthy JB, Wayner EA, Lebien TW. Regulation of Human B-cell Precursor Adhesion to Bone-marrow Stromal Cells by Cytokines That Exert Opposing Effects on the Expression of Vascular Cell-adhesion Molecule-1 (VCAM-1). *Blood.* 1993; 81:2272–82. [PubMed: 7683214]
42. Schneider IC, Hays CK, Waterman CM. Epidermal Growth Factor-induced Contraction Regulates Paxillin Phosphorylation to Temporally Separate Traction Generation from Deadhesion. *Molecular Biology of the Cell.* 2009; 20:3155–67. [PubMed: 19403690]
43. Wolf K, Mazo I, Leung H, Engelke K, von Andrian UH, Deryugina EI, et al. Compensation mechanism in tumor cell migration: mesenchymal-amoeboid transition after blocking of pericellular proteolysis. *Journal of Cell Biology.* 2003; 160:267–77. [PubMed: 12527751]
44. Zhou ZN, Sharma VP, Beaty BT, Roh-Johnson M, Peterson EA, Van Rooijen N, et al. Autocrine HBEGF expression promotes breast cancer intravasation, metastasis and macrophage-independent invasion in vivo. *Oncogene.* 2014; 33:3784–93. [PubMed: 24013225]
45. Wang Y, Lam JB, Lam KSL, Liu J, Lam MC, Hoo RLC, et al. Adiponectin modulates the glycogen synthase kinase-3 beta/beta-catenin signaling pathway and attenuates mammary tumorigenesis of MDA-MB-231 cells in nude mice. *Cancer Research.* 2006; 66:11462–70. [PubMed: 17145894]
46. van Nimwegen MJ, Verkoeijen S, van Buren L, Burg D, de Water BV. Requirement for focal adhesion kinase in the early phase of mammary adenocarcinoma lung metastasis formation. *Cancer Research.* 2005; 65:4698–706. [PubMed: 15930288]
47. Doerr R, Zvibel I, Chiuten D, Dolimpio J, Reid LM. Clonal growth of tumors on tissue-specific biomatrices and correlation with organ specificity of metastases. *Cancer Research.* 1989; 49:384–92. [PubMed: 2910457]
48. Sanz-Moreno V, Gadea G, Ahn J, Paterson H, Marra P, Pinner S, et al. Rac Activation and Inactivation Control Plasticity of Tumor Cell Movement. *Cell.* 2008; 135:510–23. [PubMed: 18984162]
49. Kraning-Rush CM, Carey SP, Califano JP, Smith BN, Reinhart-King CA. The role of the cytoskeleton in cellular force generation in 2D and 3D environments. *Phys Biol.* 2011; 8

50. Mierke CT, Rosel D, Fabry B, Brabek J. Contractile forces in tumor cell migration. *Eur J Cell Biol.* 2008; 87:669–76. [PubMed: 18295931]
51. Straight AF, Cheung A, Limouze J, Chen I, Westwood NJ, Sellers JR, et al. Dissecting temporal and spatial control of cytokinesis with a myosin II inhibitor. *Science.* 2003; 299:1743–7. [PubMed: 12637748]
52. Saitoh M, Ishikawa T, Matsushima S, Naka M, Hidaka H. Selective-inhibition of Catalytic Activity of Smooth-muscle Myosin Light Chain Kinase. *Journal of Biological Chemistry.* 1987; 262:7796–801. [PubMed: 3108259]
53. Uehata M, Ishizaki T, Satoh H, Ono T, Kawahara T, Morishita T, et al. Calcium sensitization of smooth muscle mediated by a Rho-associated protein kinase in hypertension. *Nature.* 1997; 389:990–4. [PubMed: 9353125]
54. Takai A, Bialojan C, Troschka M, Ruegg JC. Smooth-muscle Myosin Phosphatase Inhibition and Force Enhancement by Black Sponge Toxin. *FEBS Lett.* 1987; 217:81–4. [PubMed: 3036577]
55. Bazzoni G, Shih DT, Buck CA, Hemler ME. Monoclonal-antibody 9EG7 Defines a Novel Beta(1) Integrin Epitope Induced by Soluble Ligand and Manganese, but Inhibited by Calcium. *Journal of Biological Chemistry.* 1995; 270:25570–7. [PubMed: 7592728]
56. Fraser SA, Ting YH, Mallon KS, Wendt AE, Murphy CJ, Nealey PF. Sub-micron and nanoscale feature depth modulates alignment of stromal fibroblasts and corneal epithelial cells in serum-rich and serum-free media. *J Biomed Mater Res Part A.* 2008; 86A:725–35.
57. Biela SA, Su Y, Spatz JP, Kemkemer R. Different sensitivity of human endothelial cells, smooth muscle cells and fibroblasts to topography in the nano-micro range. *Acta Biomater.* 2009; 5:2460–6. [PubMed: 19410529]
58. Clark P, Connolly P, Curtis ASG, Dow JAT, Wilkinson CDW. Cell guidance by ultrafine topography *in vitro*. *Journal of Cell Science.* 1991; 99:73–7. [PubMed: 1757503]
59. Pot SA, Liliensiek SJ, Myrna KE, Bentley E, Jester JV, Nealey PF, et al. Nanoscale Topography-Induced Modulation of Fundamental Cell Behaviors of Rabbit Corneal Keratocytes, Fibroblasts, and Myofibroblasts. *Invest Ophthalmol Vis Sci.* 2010; 51:1373–81. [PubMed: 19875665]
60. Clark P, Connolly P, Moores GR. Cell guidance by micropatterned adhesiveness *in vitro*. *Journal of Cell Science.* 1992; 103:287–92. [PubMed: 1429909]
61. Kasten A, Naser T, Brullhoff K, Fiedler J, Muller P, Moller M, et al. Guidance of Mesenchymal Stem Cells on Fibronectin Structured Hydrogel Films. *PLoS One.* 2014; 9
62. Britland S, Morgan H, WojakStodart B, Riehle M, Curtis A, Wilkinson C. Synergistic and hierarchical adhesive and topographic guidance of BHK cells. *Experimental Cell Research.* 1996; 228:313–25. [PubMed: 8912725]
63. Charest JL, Eliason MT, Garcia AJ, King WP. Combined microscale mechanical topography and chemical patterns on polymer cell culture substrates. *Biomaterials.* 2006; 27:2487–94. [PubMed: 16325902]
64. Tonazzini I, Meucci S, Faraci P, Beltram F, Cecchini M. Neuronal differentiation on anisotropic substrates and the influence of nanotopographical noise on neurite contact guidance. *Biomaterials.* 2013; 34:6027–36. [PubMed: 23694901]
65. Spedden E, Wiens MR, Demirel MC, Staii C. Effects of Surface Asymmetry on Neuronal Growth. *PLoS One.* 2014; 9
66. Kwon KW, Park H, Song KH, Choi JC, Ahn H, Park MJ, et al. Nanotopography-Guided Migration of T Cells. *J Immunol.* 2012; 189:2266–73. [PubMed: 22844118]
67. Pankov R, Endo Y, Even-Ram S, Araki M, Clark K, Cukierman E, et al. A Rac switch regulates random versus directionally persistent cell migration. *Journal of Cell Biology.* 2005; 170:793–802. [PubMed: 16129786]
68. Maiuri P, Rupprecht JF, Wieser S, Rupprecht V, Benichou O, Carpi N, et al. Actin Flows Mediate a Universal Coupling between Cell Speed and Cell Persistence. *Cell.* 2015; 161:374–86. [PubMed: 25799384]
69. Paul CD, Shea DJ, Mahoney MR, Chai A, Laney V, Hung WC, et al. Interplay of the physical microenvironment, contact guidance, and intracellular signaling in cell decision making. *Faseb Journal.* 2016; 30:2161–70. [PubMed: 26902610]

70. Plotnikov SV, Pasapera AM, Sabass B, Waterman CM. Force Fluctuations within Focal Adhesions Mediate ECM-Rigidity Sensing to Guide Directed Cell Migration. *Cell*. 2012; 151:1513–27. [PubMed: 23260139]
71. Janson IA, Putnam AJ. Extracellular matrix elasticity and topography: Material-based cues that affect cell function via conserved mechanisms. *J Biomed Mater Res Part A*. 2015; 103:1246–58.
72. Bangasser BL, Rosenfeld SS, Odde DJ. Determinants of Maximal Force Transmission in a Motor-Clutch Model of Cell Traction in a Compliant Microenvironment. *Biophysical Journal*. 2013; 105:581–92. [PubMed: 23931306]
73. Allen WE, Zicha D, Ridley AJ, Jones GE. A role for Cdc42 in macrophage chemotaxis. *Journal of Cell Biology*. 1998; 141:1147–57. [PubMed: 9606207]
74. King SJ, Worth DC, Scales TME, Monypenny J, Jones GE, Parsons M. beta 1 integrins regulate fibroblast chemotaxis through control of N-WASP stability. *Embo J*. 2011; 30:1705–18. [PubMed: 21427700]
75. Mouneimne G, DesMarais V, Sidani M, Scemes E, Wang WG, Song XY, et al. Spatial and temporal control of cofilin activity is required for directional sensing during chemotaxis. *Current Biology*. 2006; 16:2193–205. [PubMed: 17113383]
76. Wu CY, Asokan SB, Berginski ME, Haynes EM, Sharpless NE, Griffith JD, et al. Arp2/3 Is Critical for Lamellipodia and Response to Extracellular Matrix Cues but Is Dispensable for Chemos taxis. *Cell*. 2012; 148:973–87. [PubMed: 22385962]
77. King SJ, Asokan SB, Haynes EM, Zimmerman SP, Rotty JD, Alb JG, et al. Lamellipodia are crucial for haptotactic sensing and response. *Journal of Cell Science*. 2016; 129:2329–42. [PubMed: 27173494]

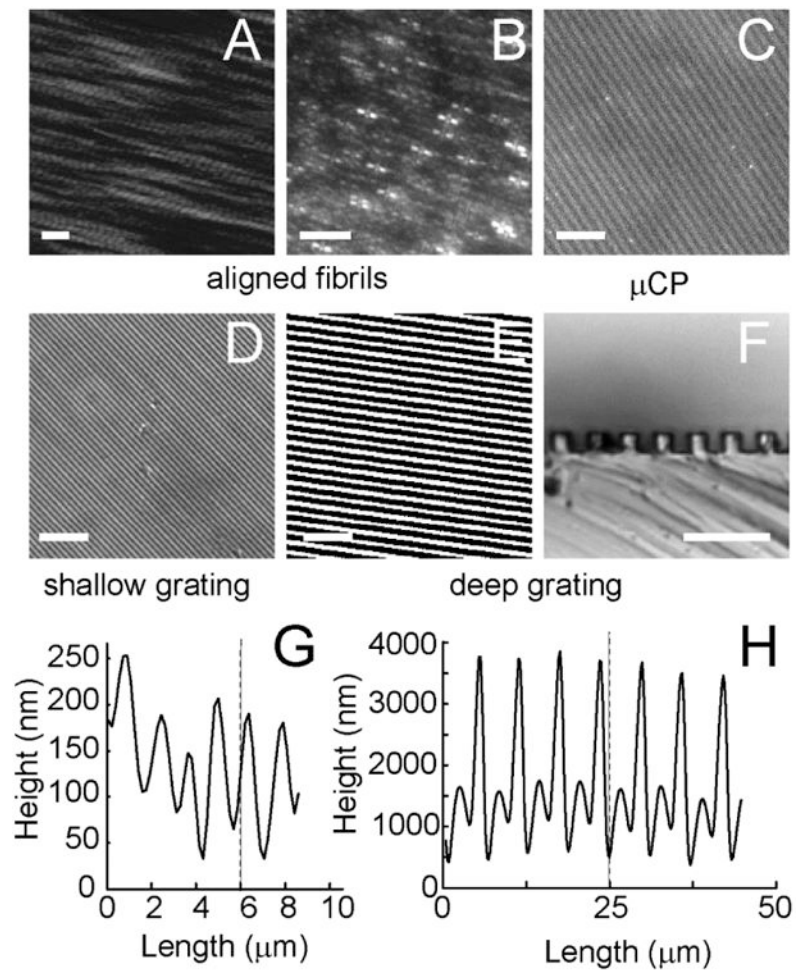


Figure 1. Length Dimensions of different substrates

(A) Epitaxially grown, aligned collagen fibril image taken using atomic force microscopy. Calibration bar length = 200 nm. (B) aligned collagen fibrils binding carboxylate-functionalized 40 nm polystyrene fluorescent spheres and imaged under fluorescence microscopy. (C) μ CP of alexa 555 collagen. Phase contrast imaging of a (D) shallow grating and (E, F) deep grating taken through the substrate (D, E) and of a slice of substrate laid on its edge (F). Calibration bar length = 30 μ m (D, E) or 5 μ m (F).

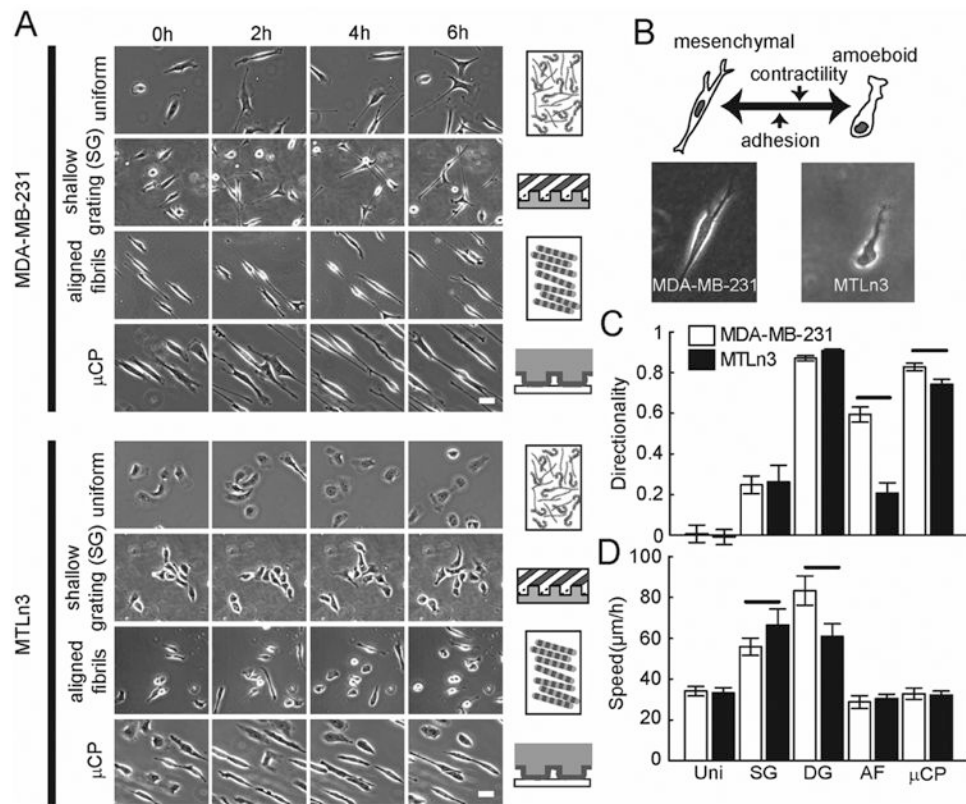


Figure 2. Migration of MDA-MB-231 and MTLn3 cells on three different contact guidance substrates

(A) Schematics of different contact guidance cues (center). Phase contrast images of MDA-MB-231 (left) and MTLn3 (right) cells at different time points during migration. Calibration bar length = 30 μm . (B) Morphology of MDA-MB-231 and MTLn3 cells in a 2 mg ml^{-1} 3D collagen gel. Migration (C) directionality and (D) speed of MDA-MB-231 and MTLn3 cells. Uni: Uniform, SG: Shallow grating, DG: Deep grating, AF: epitaxially grown aligned collagen fibrils, μCP : microcontact printed collagen ($N_{\text{experiments}} = 3$ and $N_{\text{cells per experiment}} = 50$). Error bars are 95% confidence intervals. Solid black lines indicate that the means are statistically significant ($p < 0.05$ using two-tailed student's t -test).

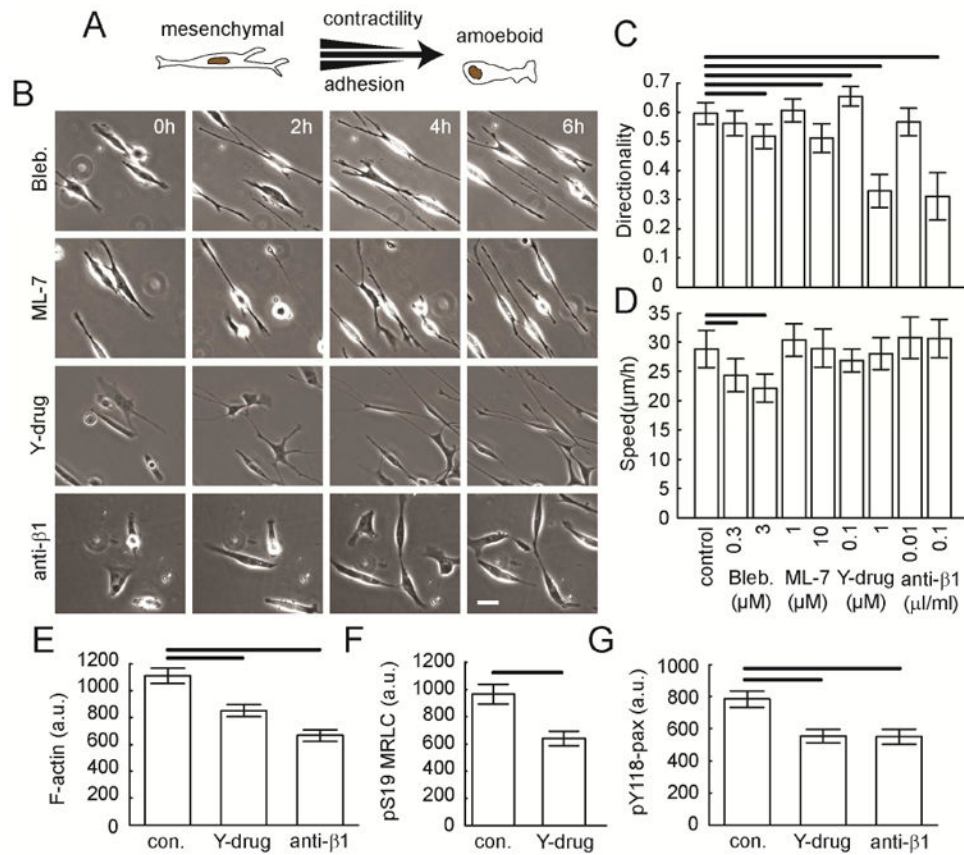


Figure 3. Migration after decreasing contraction or adhesion in a mesenchymal mode migrator MDA-MB-231 cells on aligned collagen fibrils in the presence of contractility inhibitors (blebbistatin, ML-7, Y-27632) or a $\beta 1$ integrin adhesion inhibitor (P5D2 antibody). (A) Schematic of motility modes and contact guidance response. (B) Phase contrast images of MDA-MB-231 cells at different time points during migration in the presence of inhibitors. Calibration bar length = 30 μm . Migration (C) directionality and (D) speed of MDA-MB-231 cells in the presence of inhibitors ($N_{\text{experiments}} = 3$ and $N_{\text{cells per experiment}} = 60$). MDA-MB-231 cells on aligned collagen fibrils and treated with either Y-27632 (1 μM) or P5D2 antibody (0.1 $\mu\text{l/ml}$) were stained for (E) F-actin, (F) pS19-MRLC and (G) pY118-Pax. Images were taken using epifluorescence microscopy. Whole cell average grey value was calculated. Error bars are 95% confidence intervals. Solid black lines indicate that the means are statistically significant ($p < 0.05$ using two-tailed student's t -test).

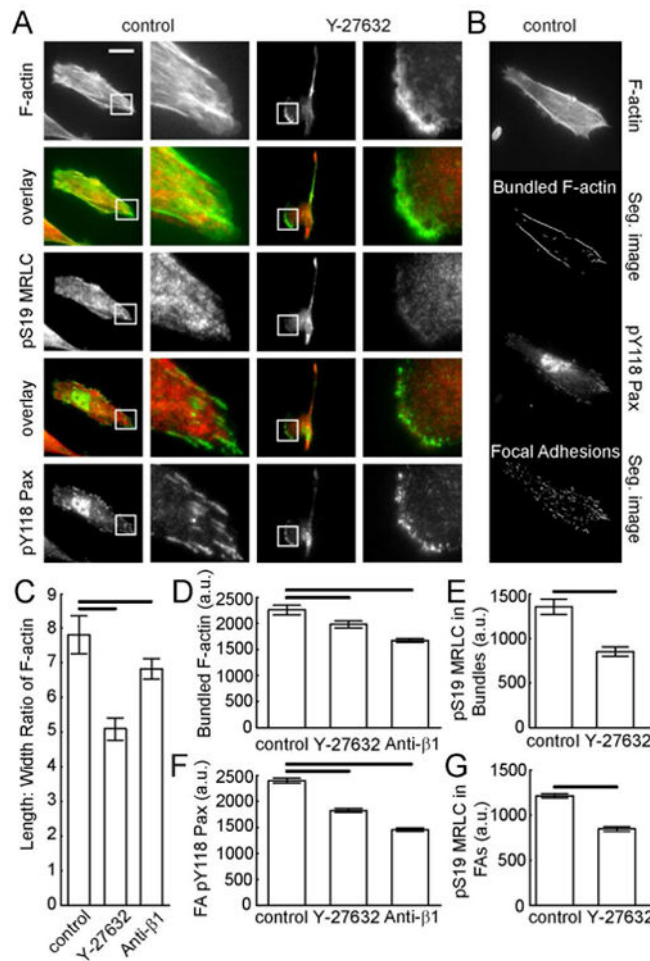


Figure 4. Phosphorylated MRLC and paxillin after decreasing contraction or adhesion in a mesenchymal mode migrator

MDA-MB-231 cells on aligned collagen fibrils in the presence of a contractility inhibitor (Y-27632, 1 μM) or a $\beta 1$ integrin adhesion inhibitor (P5D2 antibody, 0.1 $\mu\text{l/ml}$). (A) Epifluorescence images of MDA-MB-231 cells stained for F-actin (top), pS19-MRLC (middle) and pY118-Pax (bottom). Overlays of F-actin and pS19-MRLC or pY118-Pax and pS19-MRLC are included. Zoomed region is indicated by the white box and is shown to the right. Calibration bar length = 30 μm . (B) Sample images showing segmented F-actin bundles and FAs. (C) Average aspect ratio of F-actin bundles. (D) Mean grey value of segmented F-actin bundles. (E) Mean grey value of pS19-MRLC within regions on F-actin bundles. (F) Mean grey value of pY118-Pax on segmented FAs. (G) Mean grey value of pS19-MRLC on segmented FAs. ($N_{\text{experiments}} = 3$ and $N_{\text{cells per experiment}} = 26$). Error bars are 95% confidence intervals. Solid black lines indicate that the means are statistically significant ($p < 0.05$ using two-tailed student's t -test).

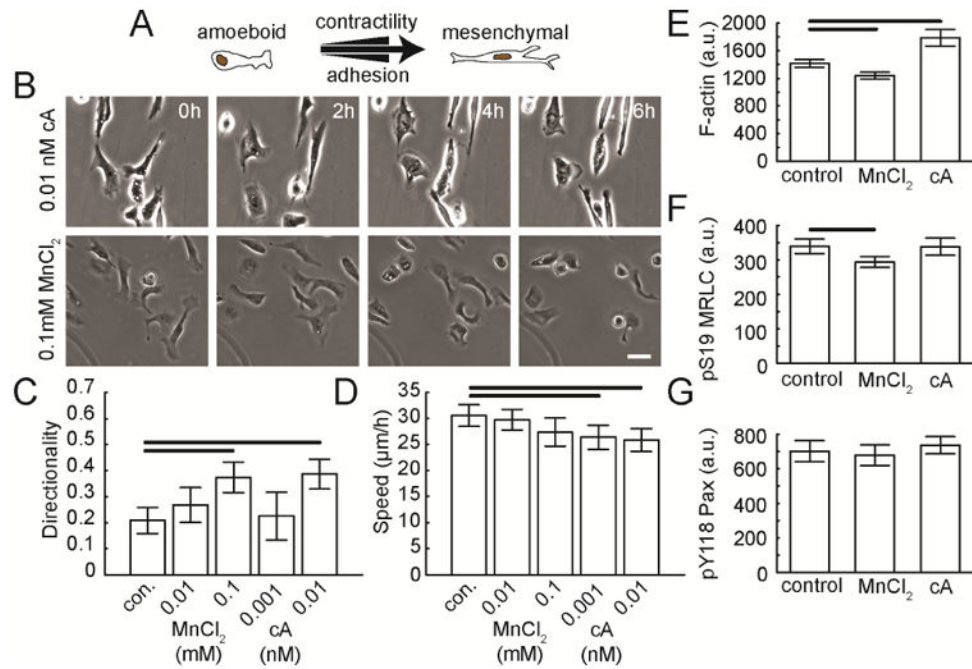


Figure 5. Migration after increasing contraction or adhesion in an amoeboid mode migrator MTLn3 cells on aligned collagen fibrils in the presence of contractility enhancer (calyculin A (cA), 0.01 nM) or integrin activator (MnCl₂, 0.1 mM). (A) Schematic of motility modes and contact guidance response. (B) Phase contrast images of MTLn3 cells at different time points during migration in the presence of enhancers. Calibration bar length = 30 µm. Migration (C) directionality and (D) speed of MTLn3 cells in the presence of enhancers ($N_{\text{experiments}} = 3$ and $N_{\text{cells per experiment}} = 90$). MTLn3 cells on aligned collagen fibrils and treated with either cA or MnCl₂ were stained for (E) F-actin, (F) pS19-MRLC and (G) pY118-Pax and images were taken using epifluorescence microscopy. Whole cell average grey value was calculated. Error bars are 95% confidence intervals. Solid black lines indicate that the means are statistically significant ($p < 0.05$ using two-tailed student's t -test).

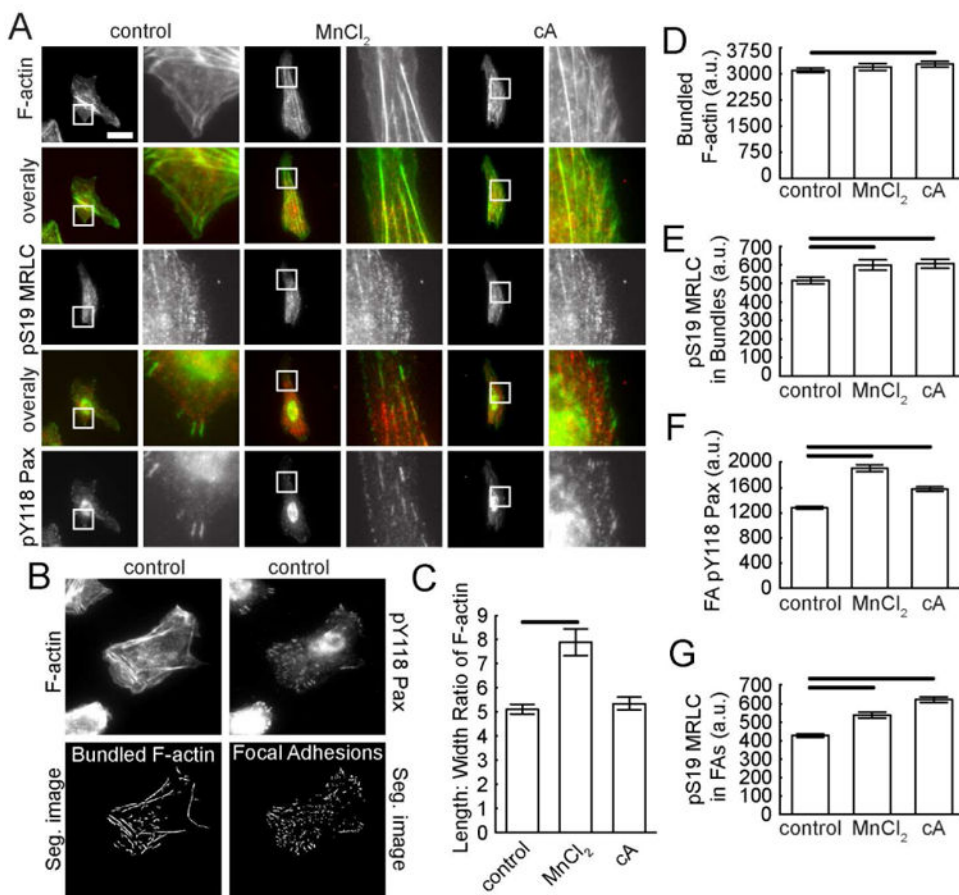


Figure 6. Phosphorylated MRLC and paxillin after increasing contraction or adhesion in an amoeboid mode migrator

MTLn3 cells on aligned collagen fibrils in the presence of a contractility enhancer (cA, 0.01 nM) or integrin activator (MnCl₂, 0.1 mM). (A) Epifluorescence images of MTLn3 cells stained for F-actin (top), pS19-MRLC (middle) and pY118-paxillin (bottom). Overlays of F-actin and pS19-MRLC or pY118-Pax and pS19-MRLC are included. Zoomed region is indicated by the white box and is shown to the right. Calibration bar length = 30 μ m. (B) Sample images showing segmented F-actin bundles and FAs. (C) Average aspect ratio of F-actin bundles. (D) Mean grey value of F-actin on segmented F-actin bundles. (E) Mean grey value of pS19-MRLC within regions delineated by segmented F-actin bundles. (F) Mean grey value of pY118-Pax on segmented FAs. (G) Mean grey value of pS19-MRLC within regions delineated by segmented FAs ($N_{\text{experiments}} = 3$ and $N_{\text{cells per experiment}} = 27$). Error bars are 95% confidence intervals. Solid black lines indicate that the means are statistically significant ($p < 0.05$ using two-tailed student's t -test).

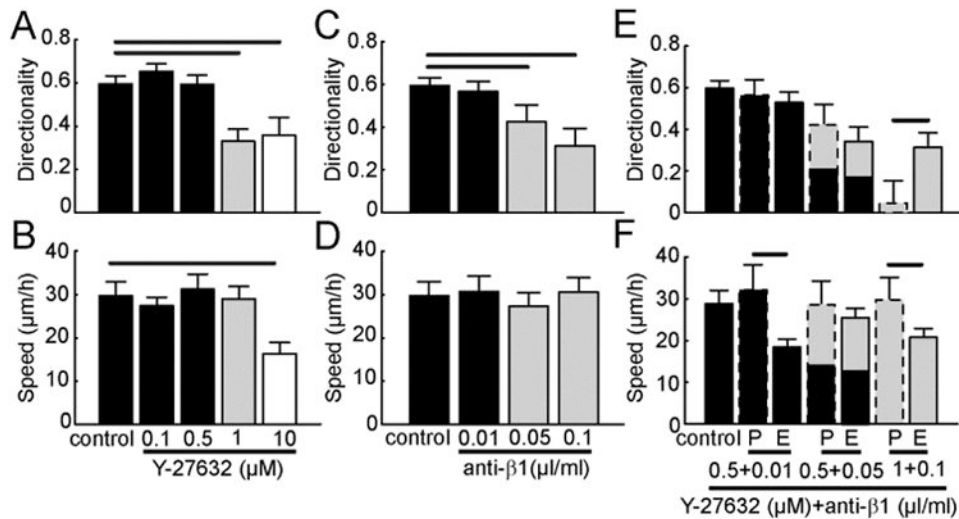


Figure 7. Simultaneously tuning contractility and adhesion in a mesenchymal mode migrator MDA-MB-231 cells on aligned collagen fibrils in the presence of single inhibitor (Y-27632 or P5D2) or combination of inhibitors (Y-27632 and P5D2). Migration (A) directionality and (B) speed of MDA-MB-231 cells in the presence of only Y-27632. Migration (C) directionality and (D) speed of MDA-MB-231 cells in the presence of only P5D2. Migration (E) directionality and (F) speed of MDA-MB-231 cells in the presence of both Y-27632 and P5D2. Black bars are conditions that show similar migration directionality and speed as compared to control. Grey bars are conditions that show different migration directionality, but similar migration speed as compared to control. White bars are conditions that show different migration directionality and speed as compared to control. Predicted (P) values for migration directionality and speed under dual perturbations are calculated from the single cue experiments and are marked with dashed lines. Experimental (E) values for migration directionality and speed under dual perturbations are marked with solid lines. ($N_{\text{experiments}} = 3$ and $N_{\text{cells per experiment}} = 60$). Error bars are 95% confidence intervals. Predicted dual perturbation 95% confidence intervals are propagated from the single perturbation experiments. Black lines indicate that the means for different conditions are statistically significant. Statistical significance was determined for $p < 0.05$ using two-tailed student's t -test.

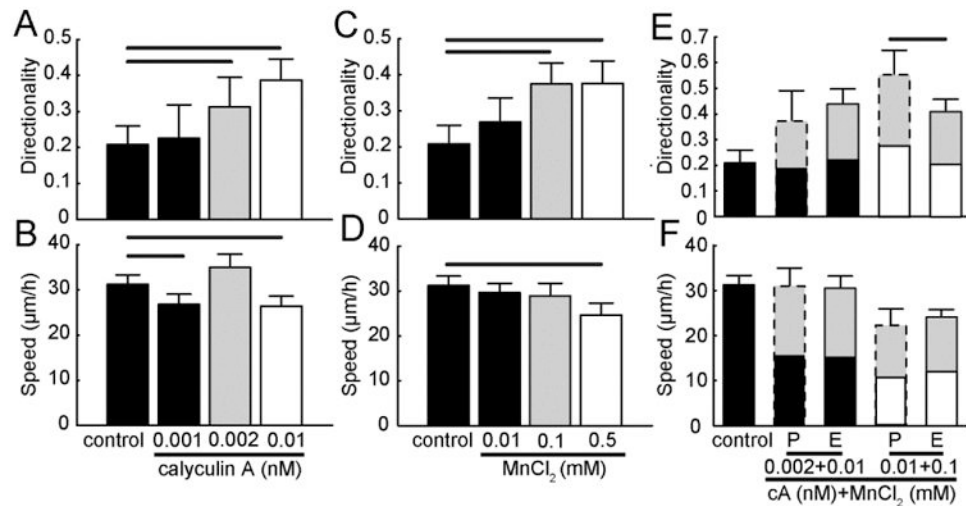


Figure 8. Simultaneously tuning contractility and adhesion in an amoeboid mode migrator MTLn3 cells on aligned collagen fibrils in the presence of single activator (calyculin A or MnCl_2) or combination of inhibitors (calyculin A and MnCl_2). Migration (A) directionality and (B) speed of MTLn3 cells in the presence of only calyculin A. Migration (C) directionality and (D) speed of MTLn3 cells in the presence of only MnCl_2 . Migration (E) directionality and (F) speed of MTLn3 cells in the presence of both calyculin A and MnCl_2 . Black bars are conditions that show similar migration directionality and speed as compared to control. Grey bars are conditions that show different migration directionality, but similar migration speed as compared to control. White bars are conditions that show different migration directionality and speed as compared to control. Predicted (P) values for migration directionality and speed under dual perturbations are calculated from the single cue experiments and are marked with dashed lines. Experimental (E) values for migration directionality and speed under dual perturbations are marked with solid lines ($N_{\text{experiments}} = 3$ and $N_{\text{cells per experiment}} = 90$). Error bars are 95% confidence intervals. Predicted dual perturbation 95% confidence intervals are propagated from the single perturbation experiments. Black lines indicate that the means for different conditions are statistically significant. Statistical significance was determined for $p < 0.05$ using two-tailed student's t -test.

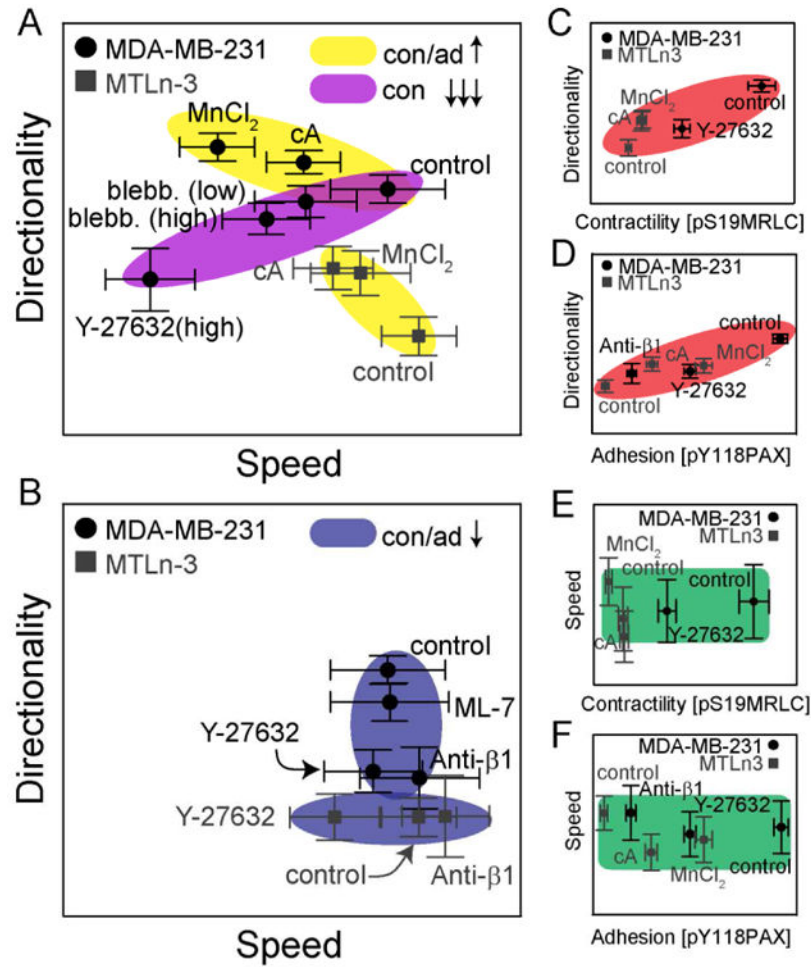


Figure 9. Schematic showing directionality and speed dependence on contractility and adhesion across different cell lines

(A and B) Migration directionality as a function of migration speed across different cell lines and perturbations. Colored regions represent classes of similar perturbations (Yellow: contractility and adhesion increases, Purple: large changes in contractility and Blue: contractility and adhesion decreases). Migration (C and D) directionality and (E and F) speed in MDA-MB-231 cells (black) and MTLn3 (grey) cells as a function of contractility and adhesion as measured by pS19-MRLC (contractility) and pY118-Pax (adhesion) signals. Axes ranges are not explicitly defined, but are function of the migration directionality, migration speed or staining intensity. Error bars are 95% confidence intervals.