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## ***In vivo* photoacoustic tumor tomography using a quinoline-annulated porphyrin as NIR molecular contrast agent**

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### **Abstract**

The synthesis and photophysical properties of a tetra-PEG-modified and freely water-soluble quinoline-annulated porphyrin are described. We previously demonstrated the ability of quinoline-annulated porphyrins to act as an *in vitro* NIR photoacoustic imaging (PAI) contrast agent. The solubility of the quinoline-annulated porphyrin derivative in serum now allowed the assessment of the efficacy of the PEGylated derivative as an *in vivo* NIR contrast agent for the PAI of an implanted tumor in a mouse model. A multi-fold contrast enhancement when compared to the benchmark dye ICG could be shown, a finding that could be traced to its photophysical properties (short triplet lifetimes, low fluorescence and singlet oxygen sensitization quantum yields). A NIR excitation wavelength of 790 nm could be used, fully taking advantage of the optical window of tissue. Rapid renal clearance of the dye was observed. Its straight-forward synthesis, optical properties with the possibility for further optical fine-tuning, nontoxicity, favorable elimination rates, and contrast enhancement make this a promising PAI contrast agent. The ability to conjugate the PAI chromophore with a fluorescent tag using a facile and general conjugation strategy was also demonstrated.

### **Introduction**

The development of new—or the refinement of existing—imaging techniques of biological processes and tissue is arguably one of the leading driving forces in contemporary biomedical chemistry.<sup>1</sup> Photoacoustic imaging (PAI) is a rapid and non-invasive imaging modality that combines optical and ultrasound imaging.<sup>2</sup> Photoacoustic signals are optically generated and ultrasonically detected. It thus can take advantage of the optical window of tissue and provides the deep probing depth (multiple cm) and spatial resolution (sub-mm) of ultrasound.

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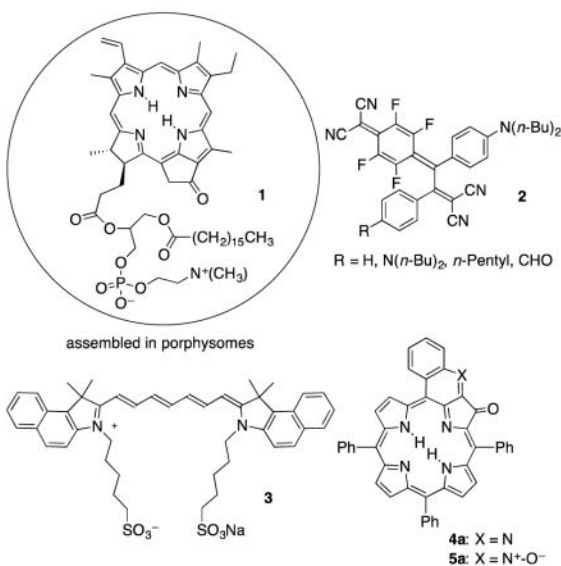
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PAI is the consequence of a number of physical effects:<sup>2c</sup> The absorption of a light pulse by a chromophore causes it to enter an excited state. Good PAI chromophores relax rapidly primarily along non-radiative pathways, causing a transient rise in temperature (in the mK regime) around the closest vicinity of the absorbing dye, leading to a localized thermal-elastic expansion. Thus, if the light source is a pulsed laser, light absorption generates a wideband ultrasonic wave. This signal can be acquired with standard ultrasonic transducers known from traditional ultrasound imaging. Furthermore, using wavelengths within the optical window of tissue (~700–1100 nm; the wavelength of maximum penetration of breast tissue is ~725 nm; whole blood has an absorption minimum at ~710 nm),<sup>3</sup> dyes many centimeters deep within tissue can be probed. If such a NIR laser beam is scanned across an object, the photoacoustic data can be used to reconstruct 2D or 3D photoacoustic maps. The laser light energy used for *in vivo* imaging experiments is generally well below the standard thresholds above which tissue damages can be expected. Variants of PAI are photoacoustic tomography (PAT)<sup>2a</sup> for large-scale imaging and photoacoustic microscopy (PAM)<sup>4</sup> for small scale, high-resolution image generation.

Endogenous chromophores, primarily hemoglobin, can be used as PAI dyes.<sup>5</sup> This allowed for the imaging of the blood content of the vascular network in rodent brains<sup>4</sup> or cancer in breast<sup>6</sup> and ovary tissues,<sup>7</sup> the mapping of mesoscopic biological objects or whole animals.<sup>2a</sup> However, particularly cancers in their early stages, cannot be detected by their intrinsic vascular contrast. Therefore, the use of exogenous contrast agents is required to achieve a suitable signal to noise ratio and to allow the PAI of deeply-seated organs or lesions.<sup>5</sup>

A number of nano- or micro-scale agents have been introduced as PAI or multimodal contrast agents in recent years, with some showing good *in vivo* imaging results.<sup>8</sup> Among them are metal-based nanoparticles, combined with and without organic dyes, and nanotubes. However, the use of nanoparticles is not without problems with respect to biodistribution, toxicity, or homogeneity.<sup>9</sup> Alternative approaches have been the use of molecular dyes assembled into vesicles, most prominent among them porphyrins made from chlorins or bacteriochlorins, such as pyropheophyrin derivative **1**,<sup>8b, 10</sup> microbubbles,<sup>8c, d</sup> or nanodroplets.<sup>8e</sup> Also developed were photoacoustic probes that are generated in tissue.<sup>11</sup> Conspicuously rare in the contemporary literature are small molecular contrast agents designed for PAI.<sup>5</sup> One example is **2**, shown to be a suitable contrast agent for imaging dissolved oxygen using photoacoustic lifetime imaging.<sup>12</sup> One of the oldest and best studied PAI contrast agents is the FDA-approved ocular angiographic dye indocyanine green (ICG, **3**), and related derivatives.<sup>13</sup> ICG possesses NIR absorption ( $\lambda_{\max} \sim 800$  nm) properties but is otherwise far from ideal. For instance, ICG is fluorescent. Thus, a portion of the absorbed light is not translated into a photoacoustic signal, diminishing its effectiveness as a PAI contrast agent. ICG is confined to the vasculature space and it clears rapidly ( $t_{1/2} < 4$  min),<sup>14</sup> complicating longitudinal *in vivo* studies. Irrespective of these shortcomings, the broad utilization of ICG suggests its use as a benchmark dye. The absence of the development of many molecular contrast agents highlights the fact that reliable structure-function relationships that might guide the rational development of photoacoustic dyes suitable for their use in biological contexts has not been derived.



We recently reported the synthesis of *meso*-tetraphenylporphyrin-derived quinoline-annulated porphyrins, such as **4a** or **5a**.<sup>15</sup> As a consequence of the extended  $\pi$ -conjugation and their annulation-induced non-planarity of the porphyrinic chromophore, the photophysical properties of quinoline-annulated porphyrins are significantly altered when compared to those of the parent porphyrin. While regular porphyrins generally do not absorb much past 650 nm, quinoline-annulated porphyrins possess  $\lambda_{\text{max}}$  bands in the 750 nm range. We have further shown that the bis-annulated systems and quinoline-annulated chlorins (in which another pyrrole was modified by a non-pyrrole heterocycle) are accessible by step-wise conversion of **5a**, further manipulating the optical properties of this family of porphyrinoids.<sup>15</sup> Complementary syntheses of some of these derivatives and related chromophores are also known.<sup>16</sup>

Crucially, quinoline-annulated porphyrins **4a** and **5a** were shown to be primarily relaxing rapidly non-radiatively, making them very good photoacoustic dyes.<sup>17</sup> We demonstrated a  $\sim 2.5$ -fold PAI contrast enhancement for **4a** over pure blood or ICG in phantom tissue experiments. The realization of the combination of a NIR-absorbing chromophores showing good photoacoustic signal generation efficiency is difficult, as the direct comparison of a number of NIR dyes absorbing in the same wavelength range has shown.<sup>17</sup> Despite the promise of **4a** or **5a** as PAI contrast agents, however, their insolubility in aqueous solutions (in the absence of a formulation vehicle like Cremophore EL®) prevented their *in vivo* assessment.

We report here firstly the development of a quinoline-annulated porphyrin-based single-molecule, serum-soluble PAI contrast agent and the evaluation of its efficacy as an *in vivo* PAI contrast agent for the detection of implanted tumors in a mouse model. A multi-fold contrast enhancement when compared to ICG was found, a finding that could be traced to its photophysical properties. Its nontoxicity and renal clearance rates will be demonstrated. We also prepared a water-soluble quinoline-annulated derivative of the quinoline annulated porphyrin carrying a small fluorescent tag designed to facilitate the biodistribution studies of

this intrinsically non-fluorescent chromophore. Alas, it was not fluorescent enough to be of utility. Nonetheless, the experiment demonstrated a facile and general conjugation strategy for these chromophores.

## Results and Discussion

### Synthesis of a freely water-soluble quinoline-annulated porphyrin

A number of strategies were established to render *meso*-arylporphyrins water-soluble.<sup>18</sup> Among them are their functionalization with anionic (carboxylate, sulfonate, phosphonate) or cationic (pyridinium) groups or their decoration with (multiple) polyethylene glycol (PEG) chains. We chose the PEG-strategy for the charge neutrality of the final products and previous reports indicating their suitability for tumor targeting.<sup>18e, 19</sup> We found that quinoline-annulated porphyrin **4a** is chemically stable under the classic acidic methoxy deprotection conditions (BBR<sub>3</sub>) but not to, for example, classic basic saponification reaction conditions (NaOH, wet THF). We thus chose the phenol-protected *meso*-tetrakis(*p*-methoxyphenyl)porphyrin **6b** as the basis for the formation of the quinoline-annulated porphyrin chromophore,<sup>15a</sup> with the intent to deprotect and PEG-ylate the phenolic oxygens using standard Williamson alkylation strategies at the last stages of the dye synthesis pathway. This strategy was successful as demonstrated by the synthesis of the water-soluble dyes **4d** and **4e** (Scheme 1).

*p*-Methoxy-derivatized quinoline-annulated porphyrin **4b** was synthesized from *meso*-tetrakis(*p*-methoxyphenyl)porphyrin **6b** using the dihydroxylation @ oxidation @ oximation @ annulation route established earlier for this chromophore class;<sup>15a</sup> all intermediates showed the expected spectroscopic and analytical properties (see ESI). However, some notable deviations from the established protocols were implemented. The oxidation of diolchlorin **7** required the use of Dess-Martin Periodinane (DMP) for its smooth conversion to the corresponding 2,3-dioxochlorin **8**.<sup>20</sup> The generally used oxidant DDQ failed to produce this dione;<sup>21</sup> instead dehydration to the corresponding enol was observed (the reaction was not further investigated). Oxime **9** formed smoothly; its treatment with *p*-TSA under forcing conditions (toluene, reflux) produced the quinoline annulated porphyrin **4b** in acceptable yields, but this product was contaminated with the corresponding *N*-oxide **5b**. Because their separation was tedious, we treated oxime **9** with DDQ, thus forming *N*-oxide **5b** as the exclusive product in near-quantitative yields. We attribute the electron-rich nature of the *p*-OMe-substituted oxime to the facile annulation and oxidation. *N*-Oxide **5b** could be readily reduced to quinoline annulated porphyrin **4b** by heating to reflux in pyridine. Similarly readily losses of the *N*-oxide were observed previously.<sup>15a</sup> Quinoline-annulated porphyrin *N*-oxide **5b** was also susceptible to a BBR<sub>3</sub>-mediated deprotection of the methoxy groups and concomitant reduction of the *N*-oxide, without any noticeable degradation of the macrocycle, generating the phenolic quinoline-annulated porphyrin **4c** in five linear steps from porphyrin **6b**.

Phenol-derivatized quinoline-annulated porphyrin **4c** could be PEG-ylated with a methoxy-capped PEG-mesylate using a short PEG chain (n = 4), forming **4d**, as well as a longer chain (avg. MW 550, n ~ 12), forming **4e**. ESI+ MS and <sup>1</sup>H NMR spectra of **4d** and **4e** confirmed

that all four non-equivalent phenolic OH-groups were PEG-ylated. The mass spectra of **4e** reflect the chain length inhomogeneity of the longer PEG-chain (see ESI). Because of the homogeneity of the shorter PEG derivative, we used this derivative for the determination of the photophysical properties of the water-soluble quinoline-annulated porphyrins.

### Photophysical properties and solubility of PEGylated quinoline-annulated porphyrins **4d** and **4e**

The presence of the four *p*-methoxy groups in **4b** (or the four *p*-OH groups in its deprotected derivative **4c**) is reflected in a slight red-shift of its optical spectrum ( $\lambda_{\max} = 762$  nm for **4b**,  $\lambda_{\max} = 748$  nm for **4c**) when compared to the spectrum of **4a** ( $\lambda_{\max} = 728$  nm), but the overall characteristics of the quinoline-annulated porphyrins are not altered (Figure 1A).<sup>17</sup>

The shorter PEG derivative **4d** is highly soluble in CH<sub>2</sub>Cl<sub>2</sub> as well as alcoholic solvents, but is only slightly soluble in pure water. The PEG-ylated quinoline-annulated porphyrin **4e** is freely soluble in alcohols, water, serum, and PBS buffer. As expected, the PEGylated derivatives **4d** and **4e** possess a  $\lambda_{\max}$  value of 764 nm in CH<sub>2</sub>Cl<sub>2</sub>. Both compounds exhibit some modest degree of solvatochromism. The spectrum of **4e** in water, for example is slightly blue-shifted and overall broadened (Figure 1B).

The dissolution of 100 mg **4e**/mL PBS was readily possible, forming a 33.3 mM solution. The solubility is therefore ~ 2 orders of magnitude higher than the reported value for ICG in water.<sup>22</sup> The Lambert-Beer law is maintained for aqueous concentrations up to 0.03 mM (the upper limit we could measure in a 1 mm path length cell) but the addition of the surfactant Triton™ X-100 to dilute solutions slightly blue-shifts and enhances the Soret band (see ESI), suggesting that **4e** is somewhat aggregated in aqueous solution. The solutions are stable; no significant changes were observed in the UV-vis spectra of the solutions over many hours, and with only the onset of minor shifts after two weeks (in the dark at 4 °C).

The fluorescence quantum yield  $\phi$  for **4e** in CH<sub>2</sub>Cl<sub>2</sub> as well as H<sub>2</sub>O were determined to be significantly below 0.1%. Transient absorption spectra (in the range from 450 to 900 nm) for **4e** in both solvents with pump-probe delay times from 0 to 15000 ps delivered no reliable ISC-quantum yield or S<sub>1</sub>-lifetime data. Correspondingly, **4e** in CH<sub>2</sub>Cl<sub>2</sub>, H<sub>2</sub>O, as well as H<sub>2</sub>O-Triton™ X-100 solutions showed no sign for the generation of singlet oxygen (<sup>1</sup>O<sub>2</sub>), as measured by the time-resolved NIR luminescence spectra of solutions of **4e** (at O.D. = 0.1 at the excitation  $\lambda$  of 532 nm) at 1270 and 1210 nm.

Thus, PEGylated quinoline-annulated porphyrin **4e**, like its parent compound,<sup>17</sup> absorbs strongly within the spectroscopic window of tissue, is non-emissive, and not generating <sup>1</sup>O<sub>2</sub>. These are excellent properties for a photoacoustic imaging agent.

### Ex vivo Photoacoustic Signal Generation of Water-soluble Quinoline-annulated Porphyrin **4e**

The strength of a photoacoustic (PA) signal generated by an irradiated sample is dependent upon the excitation source, absorption coefficient of the sample, solvent, and its Grüneisen parameter that represents the efficiency of the photoacoustic signal generation.<sup>3b</sup> We previously demonstrated in tissue phantom studies the 2.5-fold increase of the photoacoustic

signal resulting from quinoline-annulated porphyrin **4a** (dissolved in PBS–1% DMF–1% Cremophore EL®) over the signal resulting from blood at identical absorbance values.<sup>17</sup> Water-soluble quinoline-annulated porphyrin **4e** dissolved in water exhibits a similarly excellent performance. In detail, the relative *ex vivo* photoacoustic signal generation efficiency of the dye **4e** placed in a translucent polyethylene tube submerged in a water bath was compared against that of day-old rat blood in the same setup and otherwise identical irradiation and detection conditions. The concentration of **4e** was adjusted so as to possess the identical absorbance value of the blood sample at 790 nm, the wavelength of the laser used to excite the dye. The co-registered pulse-echo and photoacoustic tomography (PE-PAT) images clearly show that the tube filled with **4e** generated a 4-fold stronger signal, thus generating a much higher contrast image than the blood sample (in water, 1 cm scan depth; Figure 2A and 2B).

In tissue, light is significantly scattered and absorbed. The fat emulsion Intralipid® provides a strongly scattering medium for light.<sup>23</sup> Thus, at 2.5 cm depth, only a small fraction of the light energy is delivered to the targets.<sup>3b</sup> In fact, at the light level used in the experiment, the blood sample could not provide any PA signal higher than the noise level (Figure 2C), while the tube filled with **4e** still delivered well-resolved and high-contrast images (Figure 2D), demonstrating its potential as a PAI contrast agent.

#### Toxicity of PEGylated quinoline-annulated porphyrin **4e**

Anesthetized 6 week old BALB/c mice were treated with 100  $\mu$ L of a 33.3 mM PBS solution of **4e** via retro-orbital injection and their heart rates were monitored for 3 h after injection. No signs of distress of the mice were observed. They also lived for several weeks after the injection with normal weight gain, and showed no abnormal behavior. The majority of the dye is excreted via the renal pathway within the first hour after injection (see also below). These are all promising preliminary indications for the absence of any acute toxicity of the PEG-ylated quinoline-annulated porphyrin **4e**.

#### The use of quinoline-annulated porphyrin **4e** as an *in vivo* PAI contrast agent

As a result of the solubility, apparent non-toxicity, and high PA signal generation efficiency of the PEG-ylated dye **4e**, we tested the efficacy of this dye as an *in vivo* PAT contrast agent in a mouse model. The dye **4e** (100  $\mu$ L of a 33.3 mM of **4e** in PBS) was administered via retro-orbital injection<sup>24</sup> to anesthetized BALB/c mice with tumors (7–10 mm) implanted in their flanks, and the PE and co-registered PE-PAT images were recorded, beginning 1 min after injection (Figure 3A–B). The PE image shows the outline of the tumor and serves as backdrop to the PA image. Before injection, only few pixels of the PA image possess high enough signal strength to exceed a threshold value (25% of the maximum PA signal after injection). Proximately after injection (1 min), a ~ 4-fold increase in the PAT signal strengths originating from the tumor site were recorded. The enhancement of the PA signal was monitored for 45 min after injection, seeing a gradual loss of the signal strength, but even after 45 min, an at least 2-fold PA signal enhancement was still achieved (Figure 4). The effect of PEG-ylation on increasing the blood circulation time of small molecules has been described.<sup>25</sup>



In comparison, injection of 100  $\mu$ L ICG solution of identical absorbance at 780 nm as **4e** at 790 nm ([ICG] = 1.33 mM) provided a significantly lower PA signal strength enhancement (~1.6-fold) (Figures 3C–D), with no enhancement after less than 30 min (Figure 4). Thus, the rate at which dye **4e** is excreted (via renal pathways, see below) is significantly slower than the rapid excretion rate of ICG.<sup>14</sup>

### Renal filtration of quinoline-annulated porphyrin **4e**

An early indication for the biodistribution of dye **4e** was the observation of the color of the urine excreted by the mice immediately after the imaging experiments (after ~45 min) to the color of the dye (Figure 5). This suggested a very efficient renal filtration of the dye. Using UV-vis spectroscopic and HPLC-MS analyses of the urine extracts, we were able to show that **4e** was excreted in unaltered form (see ESI).

### Fluorescent-tagging of quinoline-annulated porphyrin **4e**

Quinoline-annulated porphyrin **4e** is non-fluorescent. However, the recording of fluorescent images of organs or the measurement of the dye-specific fluorescence of organ or biofluid extracts are convenient methodologies to track the biodistribution of any fluorophore. Thus, we opted to prepare a fluorophore-tagged derivative of quinoline-annulated porphyrin **4e**. Recognizing that FRET processes might be operative that quench the fluorescence of the tag at the absorption maxima of quinoline-annulated porphyrins, we looked for fluorophores that emit in an area of relative minor absorption of these chromophores (Figure 1).

BODIPYs are well-established low molecular weight fluorophores of high brightness and multiple options to adjust their optical spectra.<sup>26</sup> Furthermore, a recent report describing the reaction of *meso*-mercapto-BODIPY derivative **10** with phenols to generate the *meso*-phenoxy-BODIPY derivative **11** (Scheme 2)<sup>27</sup> seemed most suitable for our task of tagging a tetra-phenol-derived quinoline-annulated porphyrin. Moreover, the emission  $\lambda_{\text{max}}$  of 495 nm for **11** lies within the target range, and the attachment of the fluorophore at the most distal position to the porphyrinic chromophore would also reduce the chances for any FRET.

Thus, we chose to attach a single BODIPY moiety to one of the four phenolic oxygens of tetraol **4c**, followed by exhaustive PEG-ylation of the remaining three phenol functionalities (Scheme 3).

In anticipation of the copper-catalyzed reaction chosen for the conjugation of the fluorescent tag to quinoline-annulated porphyrin **4c**, its central cavity was protected by insertion of zinc(II). A Cu(I) thiophene-carboxylate (CuTC)-mediated reaction of *meso*-mercapto-BODIPY **10**,<sup>27</sup> followed by an acid-mediated removal of the zinc protecting group using a mineral acid wash, generated quinoline-annulated porphyrin **4f** in which one of the phenolic oxygens was derivatized with the BODIPY group, while the other three groups remained unmodified (as per ESI+ MS). The lack of regioselectivity of this reaction is reflected in the complex <sup>1</sup>H NMR spectrum of this compound (see ESI). The three phenolic oxygens of **4f** were then PEG-ylated using the long PEG mesylate as described above. Product **4g**, a deep yellow oil, shows the expected composition (as per MALDI MS). It is freely water-soluble. The presence of the BODIPY is seen in the (complex) <sup>1</sup>H NMR spectrum of **4g** by the

observation of the diagnostic peaks for the  $\alpha$ - and  $\beta$ -protons of the BODIPY moiety (at  $\delta = 6.5$ – $7.0$  ppm). Its  $^{19}\text{F}$  NMR spectrum indicates the presence of fluorine atoms at  $\delta = -146.4$  to  $-146.6$  ppm, the typical range for BODIPY fluorine atoms.

The UV-vis spectrum of non-PEGylated derivative **4f** is derived from a linear addition of the spectrum of tetraol **4c** and BODIPY **11** (Figure 6A), with only some minor shifts and broadening likely derived from the presence of four regioisomers. Upon PEGylation of **4f**, the UV-vis spectrum is further broadened, with retention of the overall character of the quinoline-annulated derivatives (Figure 6B).

When dyad **4g** is excited at the  $\lambda_{\text{max}}$  value of the BODIPY moiety (at 441 nm), the molecule emits at 485 nm, this emission can be attributed to the BODIPY portion of **4g**.<sup>27</sup> However, the fluorescence yield  $\phi$  for **4g** is estimated to lie below 0.3%, i.e., much lower than the fluorescence yield  $\phi$  for **11**.<sup>27</sup> This suggests that some FRET (or other quenching) mechanisms are operative in **4g**, but that this quenching is not efficient enough to entirely switch off the fluorescence of the BODIPY moiety. The low fluorescence yield further questions the possibility of tracking dyad **4g** in tissue using a fluorescence scanner.

### Biodistribution study of BODIPY-tagged quinoline-annulated porphyrin **4g**

The biodistribution of the BODIPY-labeled derivative **4g** in the tumor and other organs was studied by *ex vivo* fluorescent imaging, following the injection of **4g** into 4 BALB/c mice as described for **4e**. The mice were sacrificed after 15 or 120 min after injection, the organs extracted, and their radiant efficiency fluorescent images recorded ( $\lambda_{\text{exc}} = 465$  nm; GFP emission filter). Unfortunately, however, the high amount of tissue auto-fluorescence in that wavelength, did not allow the recording of high-contrast images. We note, however, that the tumor was yellow stained, suggesting an accumulation of the dye **4g** in the tumor. Similarly, the tumor was visibly dark brown stained after the injection of **4e** (see ESI).

## Conclusions

In conclusion, we have demonstrated the *in vivo* efficacy of freely serum-soluble quinoline-annulated porphyrin derivative **4e** as a molecular contrast agent for photoacoustic tomography. The solubilization of the quinoline-annulated porphyrin followed a straight-forward PEGylation strategy, with the lengths of the PEG chains determining the solubility of the final product. The product appeared to be low acute toxicity, accumulated in the tumor site, and was rapidly excreted in unaltered fashion via renal pathways. The solubilisation strategy is conceivably also suitable to other quinoline-annulated porphyrin derivatives. Conjugation of the non-fluorescent PEGylated quinoline-annulated porphyrin to a fluorophore was also demonstrated, but the hopes to utilize this derivative for the tracking of the biodistribution of the contrast agent using fluorescence imaging was not fulfilled. Nonetheless, the flexible derivatization strategy points the way toward the conjugation to other molecules.



## Experimental section

### Synthesis: Materials and instrumentation

All solvents (Aldrich, Acros) and reagents MeO-PEG<sub>4</sub>-OMs (Aldrich) and MeO-PEG<sub>12</sub>-OMs (Creative Peg Works), CuTC (Aldrich) were reagent grade, or better, and were used as received. *meso*-Tetrakis(*p*-methoxyphenyl)-2,3-dihydroxychlorin (**7**),<sup>28</sup> and BODIPYs **10** and **11** were prepared as described previously.<sup>27</sup>

Analytical (aluminum backed, silica gel 60, 250 μm thickness) and preparative (20 × 20 cm, glass backed, silica gel 60, 500 μm thickness) TLC plates, and the flash column silica gel (standard grade, 60 Å, 32–63 μm) used were provided by Sorbent Technologies, Atlanta, GA.

<sup>1</sup>H and <sup>13</sup>C NMR spectra were recorded on Bruker Avance II 400 and Bruker Avance I 500 instruments in the solvents indicated, and were referenced to residual solvent peaks. High and low resolution ESI mass spectra were provided by the Mass Spectrometry Facilities at the Department of Chemistry, University of Connecticut. MALDI MS Spectra were provided by the Mass Spectrometry & Proteomics Facility at the University of Notre Dame. UV-vis and fluorescence spectra were recorded on Cary 50 and Cary Eclipse photospectrometers, Varian Inc, respectively, and IR spectra on a Bruker Alpha-P FT-IR spectrometer using a diamond ATR unit.

***meso*-Tetrakis(*p*-methoxyphenyl)-2,3-dioxoporphyrin (**8**)**—Diol **7** (270 mg, 3.51 × 10<sup>-4</sup> mol) was dissolved in CH<sub>2</sub>Cl<sub>2</sub> (60.0 mL) in a round-bottom flask equipped with a magnetic stir bar. To the stirring solution was added Dess-Martin periodinane (590 mg, 1.39 × 10<sup>-3</sup> mol, 4 equiv) in portions at ambient temperature. When the starting material was consumed (reaction control by UV-vis and TLC), the reaction was quenched by addition of a sat'd aq NaHCO<sub>3</sub> solution. The organic layer was isolated and washed with H<sub>2</sub>O (3 × 30 mL). The organic layer was dried over anhyd Na<sub>2</sub>SO<sub>4</sub> and evaporated to dryness by rotary evaporation, and the residue purified by column chromatography (silica-CH<sub>2</sub>Cl<sub>2</sub>) to yield **8** as a dark blue powder in yields ranging from 65 to 90% (243 mg): *R*<sub>f</sub> (CH<sub>2</sub>Cl<sub>2</sub>-silica) = 0.52; <sup>1</sup>H NMR (400 MHz, CD<sub>2</sub>Cl<sub>2</sub>) δ 8.81 (d, <sup>3</sup>*J* = 4.9 Hz, 1H), 8.65 (d, <sup>3</sup>*J* = 4.9 Hz, 1H), 8.61 (s, 1H), 8.06 (d, <sup>3</sup>*J* = 8.6 Hz, 2H), 7.84 (d, <sup>3</sup>*J* = 8.6 Hz, 2H), 7.31–7.24 (m, 4H), 4.07 (two overlapping s, 6H), -1.90 (br s, 1H, exchangeable with D<sub>2</sub>O); <sup>13</sup>C NMR (100 MHz, CD<sub>2</sub>Cl<sub>2</sub>): δ 188.2, 159.9, 159.6, 155.64, 155.62, 155.59, 140.9, 140.2, 138.4, 135.3, 134.1, 133.8, 133.4, 131.8, 128.4, 128.0, 123.9, 113.4, 112.65, 112.54, 112.47, 55.5, 55.4 ppm; UV-vis (CH<sub>2</sub>Cl<sub>2</sub>) λ<sub>max</sub> (log ε) 410 (5.26), 477 (4.26) nm; FT-IR (neat, diamond ATR) 1730 (ν<sub>C=O</sub>) cm<sup>-1</sup>; HR-MS (ESI<sup>+</sup>, 100% CH<sub>3</sub>CN, TOF) *m/z* calcd for C<sub>48</sub>H<sub>37</sub>N<sub>4</sub>O<sub>6</sub> ([M·H]<sup>+</sup>) 765.2713, found 765.2726.

***meso*-Tetrakis(*p*-methoxyphenyl)-2-hydroxyimino-3-oxoporphyrin (**9**)**—Dione **8** (94 mg, 1.2 × 10<sup>-4</sup> mol) was dissolved in pyridine (30.0 mL) in a round bottom flask equipped with a magnetic stir bar and N<sub>2</sub> inlet. Hydroxylamine hydrochloride (NH<sub>2</sub>OH·HCl, 850 mg, ~100 equiv) was added, and the mixture was stirred at ambient temperature. When the starting material was consumed (after about 24 h; reaction control by TLC), the reaction mixture was evaporated to dryness by rotary evaporation. The residue was taken up in

CH<sub>2</sub>Cl<sub>2</sub> and filtered through a glass frit (M). The volume of the filtrate was reduced and submitted to column chromatography (silica-CH<sub>2</sub>Cl<sub>2</sub>/1% MeOH) to afford the olive-green product **9** in 60% yield, (58 mg): *R*<sub>f</sub> (silica-CH<sub>2</sub>Cl<sub>2</sub>/1% MeOH) = 0.65; <sup>1</sup>H NMR (400 MHz, CD<sub>2</sub>Cl<sub>2</sub>) δ 15.78 (br s, 1H, exchangeable with D<sub>2</sub>O), 8.81 (d, <sup>3</sup>*J* = 5.7 Hz, 2H), 8.62 (t, <sup>3</sup>*J* = 8.4 Hz, 4H), 8.03 (dd, <sup>3</sup>*J* = 8.4, <sup>4</sup>*J* = 2.0 Hz, 4H), 7.85 (dd, <sup>3</sup>*J* = 8.4 Hz, 4H), 7.27-7.19 (m, 8H), 4.05 (s, 12H), -2.23 (br s, 1H exchangeable with D<sub>2</sub>O), -2.36 (br s, 1H exchangeable with D<sub>2</sub>O) ppm; <sup>13</sup>C NMR (100 MHz, CD<sub>2</sub>Cl<sub>2</sub>) δ 188.2, 159.82, 159.75, 159.6, 156.4, 154.9, 151.9, 145.4, 141.1, 139.8, 138.9, 138.80, 137.98, 135.4, 134.4, 133.6, 133.50, 133.47, 132.1, 128.6, 128.4, 127.63, 127.57, 123.8, 121.8, 115.8, 113.0, 112.7, 112.4, 112.2, 55.5, 55.42, 55.39, 53.8 ppm; UV-vis (CH<sub>2</sub>Cl<sub>2</sub>) λ<sub>max</sub> (log ε) 410 (5.44), 465 (sh), 613 (4.04), 670 (sh) nm; FT-IR (neat, diamond ATR): 1732 (ν<sub>C=O</sub>) cm<sup>-1</sup>; HR-MS (ESI<sup>+</sup>, 100% CH<sub>3</sub>CN, TOF) *m/z* calcd for C<sub>48</sub>H<sub>38</sub>N<sub>5</sub>O<sub>6</sub> ([M·H]<sup>+</sup>) 780.2822, found 780.2801.

**meso-Tris(*p*-methoxyphenyl)(*p*-methoxy)quinoline-annulated porphyrin *N*-Oxide (**5b**)**—Oxime **9** (14.7 mg, 1.88 × 10<sup>-5</sup> mol) was dissolved in CH<sub>2</sub>Cl<sub>2</sub> (10.0 mL) in a round bottom flask equipped with a magnetic stir bar. To the stirring solution was added 2,3-dichloro-5,6-dicyano-1,4-benzoquinone (DDQ, 9 mg, 2 equiv) and the mixture was stirred at ambient temperature. When the starting material was consumed (after 0.5 h; reaction control by UV-vis and TLC), the reaction mixture was filtered through a plug of silica gel. The filtrate was washed with water (2 × 10 mL), dried over anhyd Na<sub>2</sub>SO<sub>4</sub>, and evaporated to dryness by rotary evaporation. The resulting residue was purified by column chromatography (silica-CH<sub>2</sub>Cl<sub>2</sub>/1% MeOH) to afford the brown product **5b** in 97% yield (14 mg): *R*<sub>f</sub> (silica-CH<sub>2</sub>Cl<sub>2</sub>/2% MeOH) = 0.22; <sup>1</sup>H NMR (400 MHz, CDCl<sub>3</sub>) δ 8.54 (d, <sup>3</sup>*J* = 4.2 Hz, 1H), 8.41 (d, <sup>3</sup>*J* = 4.9 Hz, 1H), 8.35-8.28 (m, 3H), 8.19 (dd, <sup>3</sup>*J* = 4.3 Hz, 2H), 8.03 (d, <sup>3</sup>*J* = 2.0 Hz, 1H), 7.86-7.80 (m, 4H), 7.68-7.65 (m, 2H), 7.23-7.20 (m, 4H), 7.16-7.10 (m, 3H), 4.08-4.04 (m, 10H), 3.89 (s, 3H), -0.32 (br s, 2H, exchangeable with D<sub>2</sub>O) ppm; <sup>13</sup>C NMR (100 MHz, CDCl<sub>3</sub>) δ 185.0, 159.9, 159.6, 159.3, 159.0, 155.9, 153.6, 145.9, 143.7, 143.5, 141.6, 138.2, 135.6, 135.5, 135.2, 134.9, 134.3, 133.7, 133.4, 133.3, 133.10, 132.98, 132.94, 131.0, 129.3, 127.7, 127.4, 127.3, 124.5, 123.8, 122.7, 120.9, 113.2, 113.1, 112.6, 112.5, 102.1, 101.9, 56.0, 55.6, 55.54, 55.47 ppm; UV-vis (CH<sub>2</sub>Cl<sub>2</sub>) λ<sub>max</sub> (log ε) 422 (5.02), 504 (4.27), 543 (4.16), 751 (4.09) nm; FT-IR (neat, diamond ATR): 1686 (ν<sub>C=O</sub>) cm<sup>-1</sup>; HR-MS (ESI<sup>+</sup>, 100% CH<sub>3</sub>CN, TOF) *m/z* calcd for C<sub>48</sub>H<sub>36</sub>N<sub>5</sub>O<sub>6</sub> ([M·H]<sup>+</sup>), 778.2666, found 778.2693.

**meso-Tris(*p*-methoxyphenyl)(*p*-methoxy)quinoline-annulated porphyrin (**4b**)**—Quinoline *N*-oxide **5b** (23.7 mg, 3.05 × 10<sup>-5</sup> mol) was dissolved in pyridine (25.0 mL) and heated to reflux. When the starting material was consumed (after 48 h; reaction control by TLC and UV-vis), the solvent was evaporated and the remaining residue was purified by preparative TLC (silica-CH<sub>2</sub>Cl<sub>2</sub>/2% MeOH) and solvent exchanged from CH<sub>2</sub>Cl<sub>2</sub> to MeOH to afford the brown powder **4b** in 44% yield (10 mg): *R*<sub>f</sub> (silica-CH<sub>2</sub>Cl<sub>2</sub>/2% MeOH) = 0.54; <sup>1</sup>H NMR (400 MHz, CD<sub>2</sub>Cl<sub>2</sub>): δ 8.97 (two overlapping d, <sup>3</sup>*J* = 7.5 Hz, 2H), 8.37 (dd, <sup>3</sup>*J* = 7.9, <sup>4</sup>*J* = 4.9 Hz, 2H), 8.22 (d, <sup>3</sup>*J* = 4.6 Hz, 1H), 8.16 (d, <sup>3</sup>*J* = 4.4 Hz, 2H), 8.00-7.97 (m, 3H), 7.89 (d, <sup>3</sup>*J* = 8.5 Hz, 2H), 7.73 (d, <sup>3</sup>*J* = 8.4 Hz, 2H), 7.54 (dd, <sup>3</sup>*J* = 9.1, <sup>4</sup>*J* = 2.7 Hz, 1H), 7.28 (d, <sup>3</sup>*J* = 8.5 Hz, 2H), 7.22 (dt, <sup>3</sup>*J* = 5.3, <sup>4</sup>*J* = 3.3 Hz, 4H), 4.09 (s, 3H), 4.06 (two overlapping singlets, 6H), 4.03 (s, 3H), 1.07 (s, 2H, exchangeable with D<sub>2</sub>O); <sup>13</sup>C NMR

(100 MHz, CD<sub>2</sub>Cl<sub>2</sub>): δ 202.2, 180.4, 160.2, 159.8, 159.4, 159.0, 148.96, 148.85, 148.29, 148.21, 146.8, 146.56, 146.54, 145.7, 135.5, 134.7, 134.3, 133.5, 133.2, 132.9, 132.3, 131.0, 129.9, 127.5, 127.2, 122.9, 120.5, 113.0, 112.9, 112.8, 112.7, 112.6, 112.3, 110.0, 55.8, 55.6, 55.5, 55.4 ppm; UV-vis (CH<sub>2</sub>Cl<sub>2</sub>) λ<sub>max</sub> (log ε) 418 (5.0), 490 (4.23), 529 (4.23), 701 (sh), 762 (4.12) nm; FT-IR (neat, diamond ATR): 1716 (n<sub>C=O</sub>) cm<sup>-1</sup>; HR-MS (ESI<sup>+</sup>, 100% CH<sub>3</sub>CN, TOF) *m/z* calcd for C<sub>48</sub>H<sub>36</sub>N<sub>5</sub>O<sub>5</sub> ([M-H]<sup>+</sup>) 762.2716, found 762.2738.

**meso-Tris(*p*-hydroxyphenyl)(*p*-hydroxy)quinoline-annulated porphyrin (4c)—**

Quinoline *N*-oxide **5b** (26 mg, 3.3 × 10<sup>-5</sup> mol) was dissolved in dry CH<sub>2</sub>Cl<sub>2</sub> (5.5 mL) in a round bottom flask equipped with a magnetic stir bar and N<sub>2</sub> inlet. A 1.0 M solution of BBr<sub>3</sub> in CH<sub>2</sub>Cl<sub>2</sub> (1.35 mL, ~40 equiv) was added drop-wise to the flask and the reaction mixture was stirred. When the starting material was consumed (after 24-48 h; reaction control by TLC), the excess BBr<sub>3</sub> was quenched by the careful addition of the reaction mixture to distilled water (10 mL). The resulting mixture was extracted with EtOAc (3 × 20 mL), washed with sat'd sodium bicarbonate solution and water (2 × 20 mL). The organic layer was then dried over anhydrous Na<sub>2</sub>SO<sub>4</sub>. The resulting residue was adsorbed onto silica gel and dry-loaded onto a silica gel column and purified by chromatography (silica-CH<sub>2</sub>Cl<sub>2</sub>/10% MeOH) to afford **4c** in 65% yield (18 mg): *R*<sub>f</sub> (silica-CH<sub>2</sub>Cl<sub>2</sub>/10% MeOH) = 0.45; <sup>1</sup>H NMR (400 MHz, DMSO-*d*<sub>6</sub>): δ 10.37 (s, 1H, exchangeable with D<sub>2</sub>O), 10.09 (s, 1H, exchangeable with D<sub>2</sub>O), 9.97 (s, 1H, exchangeable with D<sub>2</sub>O), 9.71 (s, 1H, exchangeable with D<sub>2</sub>O), 8.81 (s, 1H), 8.61 (s, 1H), 8.34 (s, 1H), 8.20 (s, 1H), 8.12 (d, <sup>3</sup>*J* = 4.4 Hz, 1H), 8.03 (d, <sup>3</sup>*J* = 5.8 Hz, 1H), 7.75 (d, <sup>3</sup>*J* = 7.5, 3H), 7.58 (d, <sup>3</sup>*J* = 7.8 Hz, 2H), 7.34 (d, <sup>3</sup>*J* = 3.9 Hz, 1H), 7.16 (d, <sup>3</sup>*J* = 7.9 Hz, 2H), 7.11 (d, <sup>3</sup>*J* = 8.2 Hz, 2H), 7.04 (d, <sup>3</sup>*J* = 8.4 Hz, 2H) ppm; <sup>13</sup>C NMR (100 MHz, DMSO-*d*<sub>6</sub>): δ 194.6, 158.6, 158.1, 157.5, 157.4, 150.51, 150.49, 150.47, 146.12, 146.10, 142.03, 141.96, 138.92, 138.89, 136.1, 135.8, 135.43, 135.39, 135.2, 134.7, 134.6, 134.03, 133.94, 133.4, 132.5, 131.4, 131.1, 130.6, 130.3, 130.10, 130.09, 129.4, 127.86, 127.83, 127.80, 127.32, 127.30, 127.27, 127.26, 124.59, 124.57, 123.29, 123.26, 123.20, 123.19, 120.98, 120.96, 120.95, 120.26, 120.25, 115.44, 115.41, 114.95, 114.92, 114.82, 114.76, 114.68, 111.9, 109.4, 100.0 ppm; UV-vis (MeOH) λ<sub>max</sub> (log ε) 417 (5.15), 487 (sh), 531 (4.31), 748 (4.24) nm; FT-IR (neat, diamond ATR): 1705 (n<sub>C=O</sub>) cm<sup>-1</sup>; HR-MS (ESI<sup>+</sup>, 100% CH<sub>3</sub>CN, TOF) *m/z* calcd for C<sub>44</sub>H<sub>28</sub>N<sub>5</sub>O<sub>5</sub> ([M-H]<sup>+</sup>) 706.2090, found 706.2061.

**meso-Tris(*p*-MeOPEG<sub>4</sub>Ophenyl)(*p*-MeOPEG<sub>4</sub>O)quinoline-annulated porphyrin (4d)—**

Following a literature protocol for the PEGylation of a *meso*-(*p*-OH-phenyl)porphyrin,<sup>29</sup> quinoline-annulated porphyrin **4c** (10 mg, 1.4 × 10<sup>-5</sup> mol) was dissolved in dry DMF (4.0 mL) in a two-neck round bottom flask equipped with a magnetic stir bar. MeO-PEG<sub>4</sub>-OMs (25.0 mg, 8.9 × 10<sup>-5</sup> mol, 6 equiv.) and Cs<sub>2</sub>CO<sub>3</sub> (24.2 mg, 7.4 × 10<sup>-5</sup> mol, 5.2 equiv.) were added and the reaction mixture was immersed in a preheated oil bath at ~100 °C. After consumption of the starting material after ~3 h (reaction control by TLC) the solvent was evaporated and the residue was partitioned between EtOAc (10 mL) and H<sub>2</sub>O (10 mL). The organic layer was washed with H<sub>2</sub>O (3 × 10 mL) and dried over Na<sub>2</sub>SO<sub>4</sub>. The brown residue was purified by column chromatography (silica-CH<sub>2</sub>Cl<sub>2</sub>/5% MeOH) to afford the tetra-PEGylated product **4d** as a yellow-brown oil in 56% yield (12 mg): *R*<sub>f</sub> (silica-CH<sub>2</sub>Cl<sub>2</sub>/10% MeOH) = 0.56; <sup>1</sup>H NMR (500 MHz, CD<sub>2</sub>Cl<sub>2</sub>): δ 9.06-9.04 (m,

2H), 8.40 (d,  $^3J = 4.5$  Hz, 1H), 8.36 (d,  $^3J = 5.0$  Hz, 1H), 8.23 (d,  $^3J = 4.5$  Hz, 1H), 8.16 (d,  $^3J = 4.5$  Hz, 2H), 7.99 (d,  $^3J = 8.5$  Hz, 3H), 7.89 (d,  $^3J = 8.5$  Hz, 2H), 7.71 (d,  $^3J = 8.5$  Hz, 2H), 7.63 (dd,  $^3J = 9.1$ ,  $^4J = 2.5$  Hz, 1H), 7.30 (d,  $^3J = 8.6$  Hz, 2H), 7.23 (dd,  $^3J = 8.5$ ,  $^4J = 1.8$  Hz, 4H), 4.44 (t,  $^3J = 4.5$  Hz, 2H), 4.38 (two overlapping t,  $^3J = 4.7$  Hz, 4H), 4.35 (t,  $^3J = 4.6$  Hz, 2H), 3.99 (dd,  $^3J = 8.8$ ,  $^4J = 4.7$  Hz, 6H), 3.82-3.77, (m, 8H), 3.72-3.57 (m, 34H), 3.55-3.50 (m, 8H), 3.35 (s, 3H), 3.34 (s, 3H), 3.33 (s, 3H), 3.31 (s, 3H) ppm; UV-vis ( $\text{CH}_2\text{Cl}_2$ )  $\lambda_{\text{max}}$  (log  $\epsilon$ ) 419 (5.2), 491 (4.5), 531 (4.4), 764 (4.3) nm; HR-MS (ESI<sup>+</sup>, 100%  $\text{CH}_3\text{CN}$ , TOF)  $m/z$  calcd for  $\text{C}_{80}\text{H}_{100}\text{N}_5\text{O}_{21}$  ( $[\text{M}\cdot\text{H}]^+$ ), 1466.6911, found 1466.6891.

**meso-Tris(*p*-MeOPEG<sub>12</sub>Ophenyl)(*p*-MeOPEG<sub>12</sub>O)quinoline-annulated porphyrin (4e)**—Prepared from **4c** (22 mg,  $3.1 \times 10^{-5}$  mol) in dry DMF (10.0 mL),  $\text{Cs}_2\text{CO}_3$  (80 mg,  $1.6 \times 10^{-4}$  mol, 5.2 equiv.), and MeO-PEG<sub>12</sub>-OMs (80 mg,  $1.2 \times 10^{-4}$  mol, 4 equiv.) as described for the preparation of **4d**. Reaction time at 90 °C ~3 h. Purified by column chromatography (silica- $\text{CH}_2\text{Cl}_2$ /10% MeOH) to afford the tetra-PEGylated porphyrin **4e** as a brown oil in 90-99 % yield (81 mg–89 mg):  $^1\text{H}$  NMR (400 MHz,  $\text{CD}_2\text{Cl}_2$ ):  $\delta$  9.04 (s, 1H), 8.38 (two overlapping d, 2H), 8.19 (d, 3H), 7.98 (t,  $^3J = 6.6$  Hz, 3H), 7.89 (d,  $^3J = 8.3$  Hz, 3H), 7.72 (d,  $^3J = 8.4$  Hz, 2H), 7.63 (d,  $^3J = 8.3$  Hz, 1H), 7.31 (d,  $^3J = 8.5$  Hz, 3H), 7.24 (dd,  $^3J = 8.6$ ,  $^4J = 2.2$  Hz, 4H), 3.34 (four overlapping s, 12H) ppm; UV-vis ( $\text{CH}_2\text{Cl}_2$ )  $\lambda_{\text{max}}$  (rel I.) 422 (1.0) 529 (0.20) 763 (0.09) nm; HR-MS (ESI<sup>+</sup>, 100%  $\text{CH}_3\text{CN}$ , TOF) cluster of peaks corresponding to addition of four PEG groups, see ESI.

**[meso-Tris(*p*-hydroxyphenyl)(*p*-hydroxy)quinoline-annulated porphyrinato]Zinc(II) (4cZn)**—Quinoline-annulated porphyrin **4c** (19 mg,  $2.7 \times 10^{-5}$  mol) was dissolved in  $\text{CH}_2\text{Cl}_2$ /10% MeOH (7.0 mL) in a round bottom flask equipped with a magnetic stir bar.  $\text{Zn}(\text{OAc})_2 \cdot 2\text{H}_2\text{O}$  (18 mg,  $8.1 \times 10^{-5}$  mol, 3 equiv.) was added and the reaction was gently warmed. When the starting material was consumed (after 10 min; reaction control by TLC and UV-vis), the solvents were evaporated, and the residue was taken up in EtOAc and washed with water ( $3 \times 20$  mL). The organic layer was dried over anhydrous  $\text{Na}_2\text{SO}_4$  and evaporated to dryness by rotary evaporation to afford **4cZn** as an orange solid in near-quantitative yield (21 mg):  $R_f$  (silica- $\text{CH}_2\text{Cl}_2$ /10% MeOH) = 0.39;  $^1\text{H}$  NMR (400 MHz,  $\text{DMSO}-d_6$ ):  $\delta$  10.23 (s, 1H, exchangeable with  $\text{D}_2\text{O}$ ), 9.94 (s, 1H, exchangeable with  $\text{D}_2\text{O}$ ), 9.85 (s, 1H, exchangeable with  $\text{D}_2\text{O}$ ), 9.57 (s, 1H, exchangeable with  $\text{D}_2\text{O}$ ), 8.90 (t,  $^3J = 7.9$  Hz, 2H), 8.19 (d,  $^3J = 4.5$  Hz, 1H), 8.05 (d,  $^3J = 4.6$  Hz, 1H), 7.99 (dd,  $^3J = 12.1$ ,  $^4J = 4.4$  Hz, 2H), 7.76 (t,  $^3J = 6.4$  Hz, 4H), 7.70 (d,  $^3J = 8.2$  Hz, 2H), 7.56 (dd,  $^3J = 9.0$ ,  $^4J = 2.4$  Hz, 1H), 7.47 (d,  $^3J = 8.2$  Hz, 2H), 7.13 (d,  $^3J = 8.3$  Hz, 2H), 7.07 (d,  $^3J = 8.3$  Hz, 2H), 7.00 (d,  $^3J = 8.2$  Hz, 2H) ppm;  $^{13}\text{C}$  NMR (100 MHz  $\text{CD}_2\text{Cl}_2$ /10% MeOH):  $\delta$  195.7, 159.8, 158.1, 157.8, 157.0, 156.6, 152.7, 152.1, 150.9, 150.5, 150.1, 148.0, 146.3, 143.3, 142.7, 135.6, 135.4, 134.8, 134.6, 133.8, 133.7, 133.6, 133.52, 133.47, 133.2, 132.0, 131.2, 131.06, 130.13, 130.0, 126.7, 123.7, 121.0, 115.6, 115.0, 114.7, 114.5, 111.9 ppm; UV-vis (MeOH)  $\lambda_{\text{max}}$  (log  $\epsilon$ ) 420 (5.13), 484 (sh), 518 (sh), 737 (sh), 816 (4.25) nm; FT-IR (neat, diamond ATR): ~1750 ( $\nu_{\text{C=O}}$ )  $\text{cm}^{-1}$ ; HR-MS (ESI<sup>+</sup>, 100%  $\text{CH}_3\text{CN}$ , TOF)  $m/z$  calcd for  $\text{C}_{44}\text{H}_{26}\text{N}_5\text{O}_5\text{Zn}$  ( $[\text{M}\cdot\text{H}]^+$ ) 768.1225, found 768.1222.

***p*-(BODIPY)-tris-*p*-(OH)-quinoline-annulated porphyrin, mixture of regioisomers (4f)**—*meso*-thiomethyl-4,4,-difluoro-4-bora-3a,4a-diaza-s-indacene **10** (6 mg,  $2.7 \times 10^{-5}$  mol) was dissolved in dry CH<sub>3</sub>CN (3.0 mL) in a round bottom flask equipped with a magnetic stir bar under N<sub>2</sub> atmosphere. Tetraol **4cZn** (21 mg,  $2.7 \times 10^{-5}$  mol, 1 equiv) was added and the mixture was stirred for 5 min under N<sub>2</sub>. Copper(I) thiophene-2-carboxylate (CuTC) (5 mg,  $2.7 \times 10^{-5}$  mol, 1 equiv.) and Na<sub>2</sub>CO<sub>3</sub> (3 mg,  $2.7 \times 10^{-5}$  mol, 1 equiv.) were added and the reaction mixture was immersed in a pre-heated oil bath at 50 °C and stirred.<sup>27</sup> After 48 h, a saturated aqueous NH<sub>4</sub>Cl solution was added and the reaction mixture was stirred for several hours. The resulting biphasic mixture was extracted with EtOAc (3 × 10 mL), washed with H<sub>2</sub>O (2 × 10 mL), and dried over Na<sub>2</sub>SO<sub>4</sub>. The remaining residue was purified by column chromatography (silica-CH<sub>2</sub>Cl<sub>2</sub>/10% MeOH) to afford recovered **4cZn** (6 mg) and the mono-BODIPY-tagged product **4f** as a series of closely running yellow fractions. The combined yellow fractions were dissolved in EtOAc (5.0 mL) and treated with 3 M HCl (5.0 mL) until the UV-vis spectrum of a neutralized aliquot indicated full demetallation. The organic layer was then washed with a sat'd aq NaHCO<sub>3</sub> solution and H<sub>2</sub>O, and was dried over anhyd. Na<sub>2</sub>SO<sub>4</sub> to provide **4f** as a yellow film in 30% yield (7 mg): *R*<sub>f</sub> (silica-CH<sub>2</sub>Cl<sub>2</sub>/10% MeOH) = 0.21; <sup>1</sup>H-NMR (500 MHz, DMSO-*d*<sub>6</sub>): δ 10.09-10.07 (m, 1H, exchangeable with D<sub>2</sub>O), 9.95-9.93 (m, 1H, exchangeable with D<sub>2</sub>O), 9.69-9.64 (m, 1H, exchangeable with D<sub>2</sub>O), 9.10 (br s, 1H), 8.45 (d, <sup>3</sup>*J* = 4.4 Hz, 1H), 8.4-8.37 (m, 1H), 8.18 (d, <sup>3</sup>*J* = 5.2 Hz, 2H), 8.13-8.10 (m, 2H) 8.08-7.95 (m, 3H), 7.92-7.88 (m, 3H), 7.80-7.77 (m, 4H), 7.60-7.59 (m, 1H), 7.31 (s, 1H), 7.19 (d, *J* = 6.0 Hz, 2H), 7.12 (two overlapping d, <sup>3</sup>*J* = 7.8 Hz, 2H), 7.05-7.03 (m, 2H), 6.81 (d, *J* = 6.1 Hz, 2H), 6.76-6.72 (m, 1H) ppm; <sup>19</sup>F NMR (470 MHz, DMSO-*d*<sub>6</sub>): δ -142.1 to -142.2, (m) ppm; UV-vis (MeOH) λ<sub>max</sub> (rel I.) 400 (1.0), 443 (0.56), 510 (sh), 784 (0.1) nm; Fl (MeOH, λ<sub>excitation</sub> = 441 nm) λ<sub>max</sub> 488 nm, φ (EtOAc) = 0.01; HR-MS (ESI<sup>+</sup>, 100% CH<sub>3</sub>CN, TOF) *m/z* calcd for C<sub>53</sub>H<sub>33</sub>BF<sub>2</sub>N<sub>7</sub>O<sub>5</sub> ([M·H]<sup>+</sup>) 896.2613, found 896.2613.

***p*-(BODIPY)-tris-*p*-(OPEG<sub>12</sub>)-quinoline-annulated porphyrin, mixture of regioisomers (4g)**—Prepared according to the procedure for **4e** from **4d** (10 mg,  $1.1 \times 10^{-5}$  mol), MeO-PEG<sub>550</sub>-OMs (22 mg,  $3.4 \times 10^{-5}$  mol, 3 equiv.), 14 mg of Cs<sub>2</sub>CO<sub>3</sub> ( $4.4 \times 10^{-5}$  mol, 3.9 equiv.) in DMF (2.0 mL) to afford **4g** as a yellow oil in 56% yield (16 mg): <sup>1</sup>H NMR (400 MHz, CD<sub>2</sub>Cl<sub>2</sub>): δ 9.14 (s, 1H), 8.45 (s, 1H), 8.38 (d, <sup>3</sup>*J* = 4.6 Hz, 1H), 8.21 (d, 4H), 8.01 (d, <sup>3</sup>*J* = 6.8 Hz, 3H), 7.91 (d, <sup>3</sup>*J* = 7.6 Hz, 2H), 7.73 (d, <sup>3</sup>*J* = 7.2 Hz, 3H), 7.52 (s, 1H), 7.31 (d, <sup>3</sup>*J* = 8.0 Hz, 4H), 7.25 (d, <sup>3</sup>*J* = 5.0 Hz, 5H), 7.13-7.11 (m, 2H), 6.82 (d, <sup>3</sup>*J* = 5.7 Hz, 1H), 6.46 (s, 1H), 3.35-3.3 (three overlapping s, 9H) ppm; <sup>19</sup>F NMR (470 MHz, CD<sub>2</sub>Cl<sub>2</sub>): δ -142.1 to -142.2, (m) ppm; UV-vis (MeOH) λ<sub>max</sub> (rel I.) 402 (1.0), 473 (sh), 510, (sh), 769 (0.12) nm; Fl (MeOH, λ<sub>excitation</sub> = 441 nm) λ<sub>max</sub> 485 nm, φ (EtOAc) < 0.003; HR-MS (MALDI, 100% DHBA) cluster of peaks corresponding to addition of three PEG groups, see ESI.

### Co-registered pulse-echo-photoacoustic tomography

The details to the 64 channel co-registered ultrasound pulse echo-photoacoustic tomography (PE-PAT) system is described elsewhere.<sup>30</sup> Briefly, the system utilizes a unique field-programmable gate array (FPGA) technology that allows for real-time acquisition of ultrasound and photoacoustic signals. The photoacoustic signal is generated by a 15 Hz, 12



ns pulse width light of a tunable Ti-Sapphire laser (LT-2211, Symphotics TII Corp, Camarillo, CA) pumped by a second harmonic Nd:YAG laser (LS-2134, Symphotics TII Corp). Free space illumination is used for light delivery. The laser light is expanded by a combination of concave and convex lenses and shone on the sample using mirrors. A small portion of the beam is separated by a beam splitter (BSN11, Thorlabs) and is focused on a single element ultrasound transducer for monitoring the fluctuations in laser energy during the experiment.<sup>31</sup> The pulse-echo (PE) ultrasound signal is generated and received by the system in synchrony with the laser pulses. The PE and PAT images are formed by a beamforming algorithm. The data sampling is performed at 40 MHz. A 64 channel ultrasound transducer with a center frequency of 3.5 MHz, a bandwidth of 80%, and a sector scan type is utilized for acquiring the co-registered PE-PAT images. Ultrasound and PAT images are overlapped to form the co-registered images. The effects of laser energy fluctuations are compensated for in the data analysis.

The setup was also used for the phantom photoacoustic signal generation efficiency evaluation of the dyes, as described previously.<sup>17</sup>

### Animal protocols

All experiments involving mice were performed as approved by the Institutional Animal Care and Use Committee (IACUC) of the University of Connecticut under license #A15-047. The purity of contrast agents **4e** and **4g** was assessed by HPLC (see ESI). Solutions of **4e** and **4g** were also filtered through a syringe filter (nylon membrane, pore size 0.22  $\mu\text{m}$ ) prior to injection.

**Toxicity test**—100  $\mu\text{L}$  of PBS based solution of **4e** with 33.3 mM concentration was injected into anesthetized 6 week old BALB/c mice ( $n = 2$ ). The heart rates of the mice were monitored by a pulse oximeter (MouseStat, Kent Scientific) before injection and during a 3 h period after injection.

**Tumor model**—Tumor cell preparation was adopted from the literature.<sup>32</sup> Briefly, 4T1 Luc cells were cultured at 37  $^{\circ}\text{C}$  with 5%  $\text{CO}_2$  in a T75 flask (BD Biosciences, Bedford, MA); DMEM (Dulbecco's Modified Eagle's medium, Gibco, USA) medium supplemented with 10% FBS and 50 U/mL penicillin/streptomycin. After 3 passes, the cells were suspended in the DMEM and  $1 \times 10^5$  cells were injected subcutaneously on top of the right leg of female BALB/c mice (6–8 weeks old, body weight  $\sim 20$  g). The mice were monitored for approximately two weeks post-inoculation until the tumor size was between 7–10 mm.

**In vivo PAT of murine tumor**—Prior to the *in vivo* imaging, the mice were anaesthetized (1.5 L/min oxygen with 1.5% isoflurane) and the tumor area depilated. The position of the mouse was fixed. Ultrasound gel was applied on the tumor area and a bag of water was placed on top of the tumor for acoustic wave coupling. The pulsed laser at 790 nm of the pulse-echo-photoacoustic tomography (PE-PAT) setup described above (780 nm for ICG) was shone on the tumor through the water bag; surface optical fluence on the tissue was always maintained below the maximum permissible exposure according to the ANSI safety standard.<sup>33</sup> The transducer position was adjusted by a three-dimensional mechanical stage to



reach a suitable imaging condition. The pre-injection PAT image of the tumor was acquired. Then 100  $\mu$ L of the PBS based solution of the dye **4e** (~33.3 mM concentration) or ICG was injected via retro-orbital injection.<sup>24</sup> Care was taken to avoid any changes in the position of the mouse, transducer, and light beam as a result of the injection. The PAT images of the tumor were acquired during the 45 min period following injection. The PAT images and the maximum PA signal levels were compared before and after the injection. The p-values in a student t-test between the results obtained for the dye and ICG are less than 0.005 for all instances, indicating statistical significance. The schematic of the *in vivo* experiment setup is illustrated in Figure 7.

**Ex vivo fluorescent imaging**—100  $\mu$ L of **4g** (3 mM in PBS) was injected to three BALB/c mice of similar weight and similar tumor size. The mice were sacrificed 15 and 120 min after the injection. Tumor, liver, kidneys, heart, lung, and spleen were harvested, washed twice in PBS, and imaged using an IVIS® Lumina II fluorescent imaging system (Caliper Life Sciences, Hopkinton, MA);  $\lambda_{\text{excitation}} = 465$  nm, GFP emission filter.

**Photophysical measurements**—The photophysical measurements were performed as described previously.<sup>17</sup>

## Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

## Acknowledgments

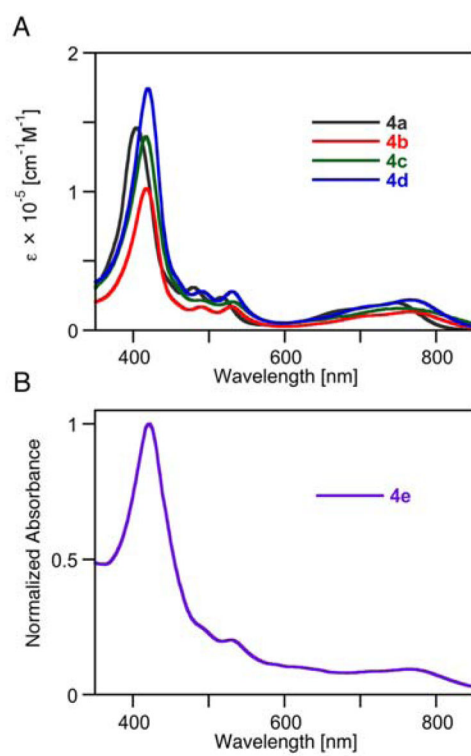
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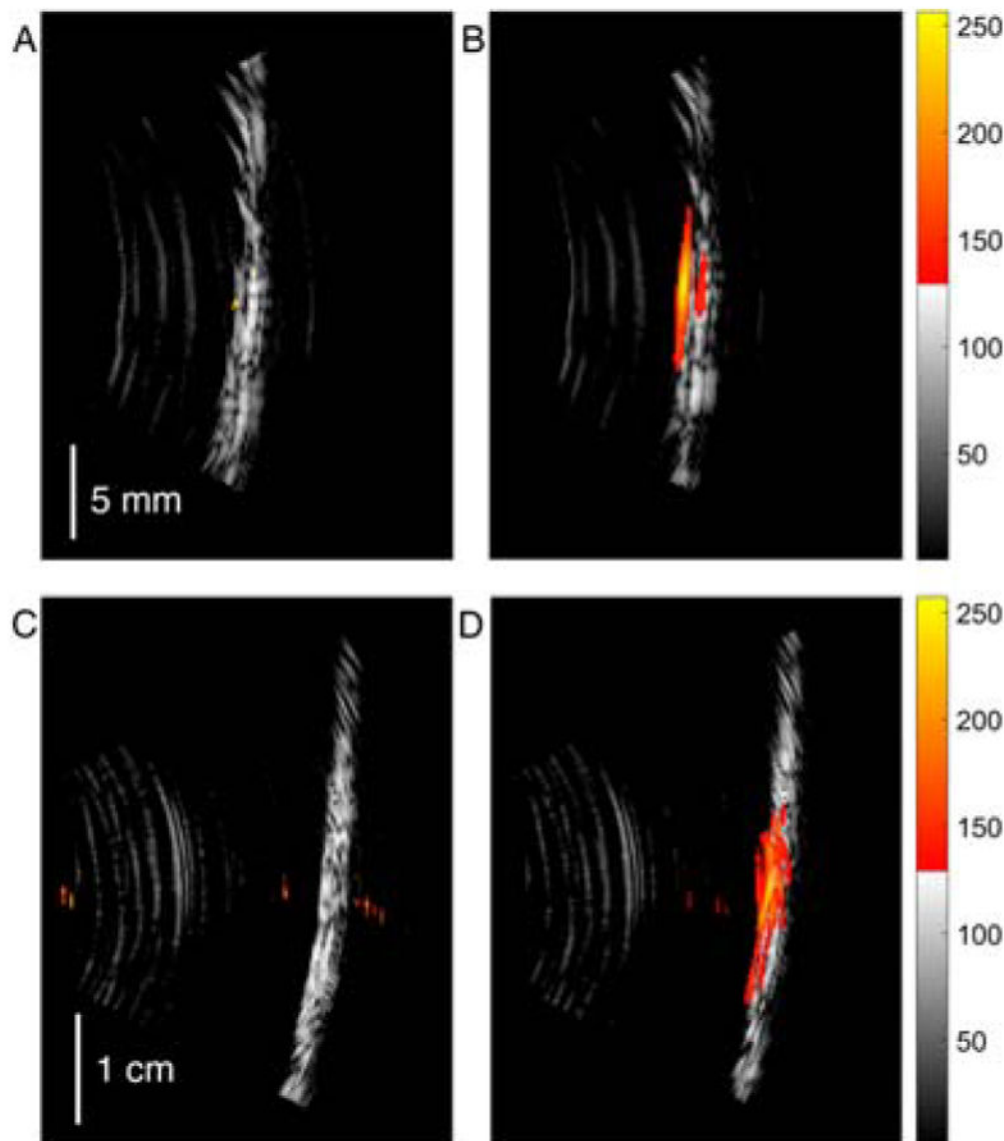
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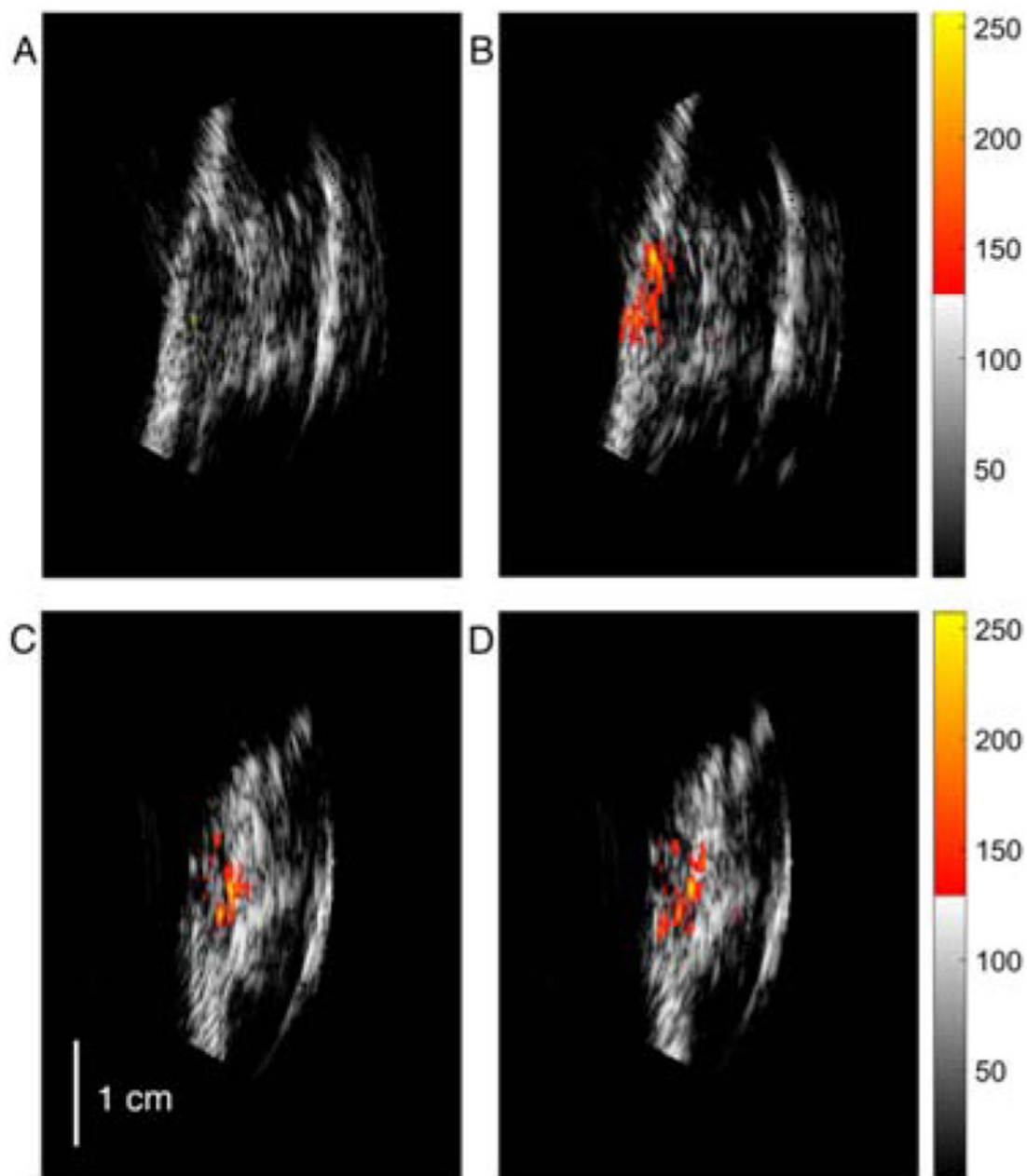


**Figure 1.**  
UV-vis spectra (A:  $\text{CH}_2\text{Cl}_2$ , B:  $\text{H}_2\text{O}$ ) of the compounds indicated.



**Figure 2.**

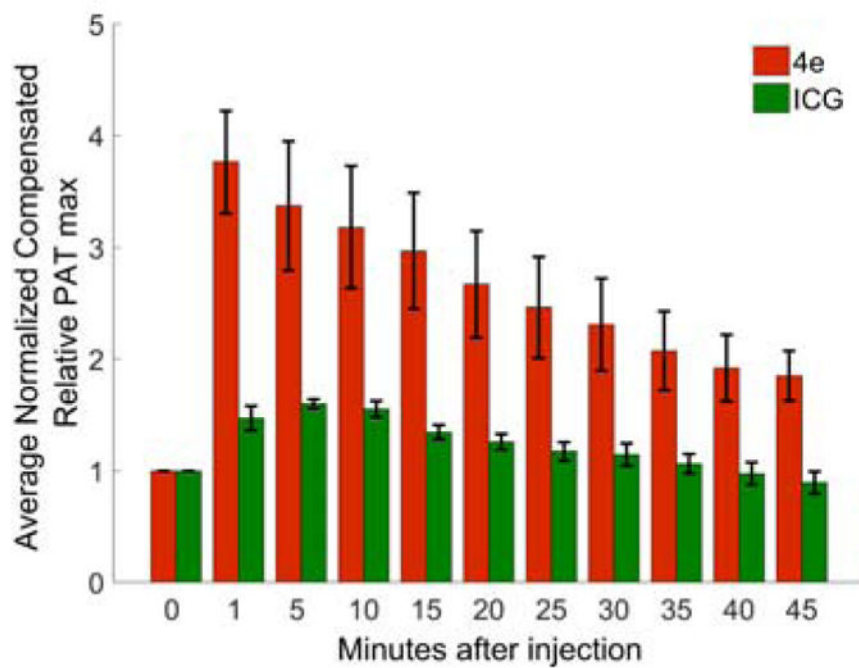
Co-registered PE-PAT images of polyethylene tubes (inner/outer  $\varnothing = 0.58/0.96$  mm) filled with (A and C) one-day-old rat blood and (B and D) with a solution of PEG-ylated quinoline-annulated porphyrin **4e** at a concentration in which the sample possessed the identical absolute absorbance value at 790 nm as the undiluted blood (see ESI). In each image pair (A-B and C-D) the PAT signal was normalized to the maximum value recorded from the tube filled with **4e**. Samples immersed in water (A and B, PA signal dynamic range of  $-12$  dB, the threshold is 25% of maximum) and Intralipid® (C and D, dynamic range of  $-15$  dB, the threshold is 18% of maximum) at 1 cm (A and B) and 2.5 cm (C and D) scan depths, respectively. Vertical image axis is approximately parallel to the tube length and horizontal axis represents imaging depth.



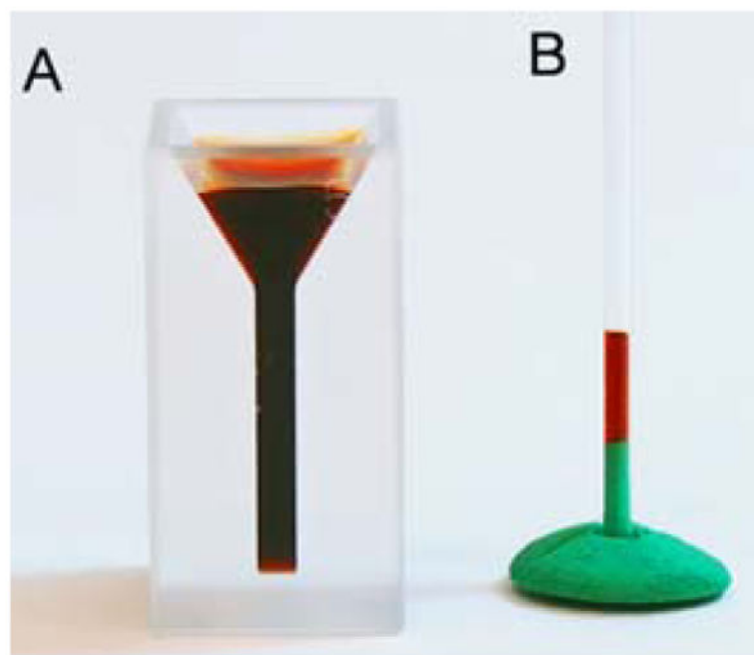
**Figure 3.**

Co-registered PE-PAT images before injection of the contrast agent (A) and ICG (C) and after the systemic injection of **4e** (B) and ICG (D). In each image pair (A-B and C-D) the PAT signals were normalized to the same maximum value recorded after the injection; a similar dynamic range of  $-12$  dB is applied to all images (the threshold is 25% of the maximum value). The vertical axis is approximately parallel to the surface of the mouse body and the horizontal axis represents the depth inside the body.





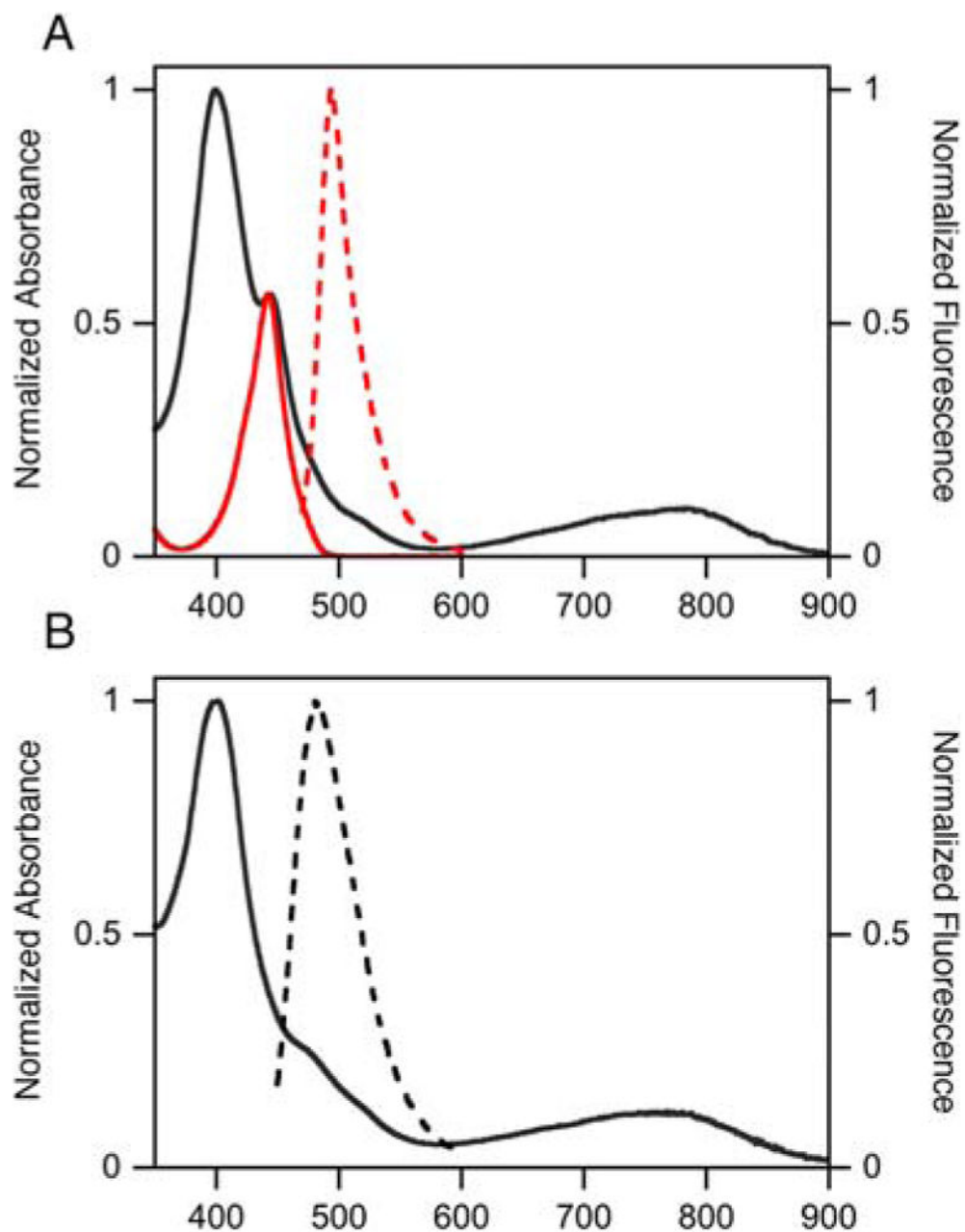
**Figure 4.** Time-dependence of the relative enhancement of the PAT max value following the injection of 100  $\mu\text{L}$  of the dye **4e** ( $\sim 33.3$  mM,  $\lambda_{\text{excitation}} = 790$  nm) and ICG (1.33 mM,  $\lambda_{\text{excitation}} = 780$  nm) at identical absorbance value.



**Figure 5.**

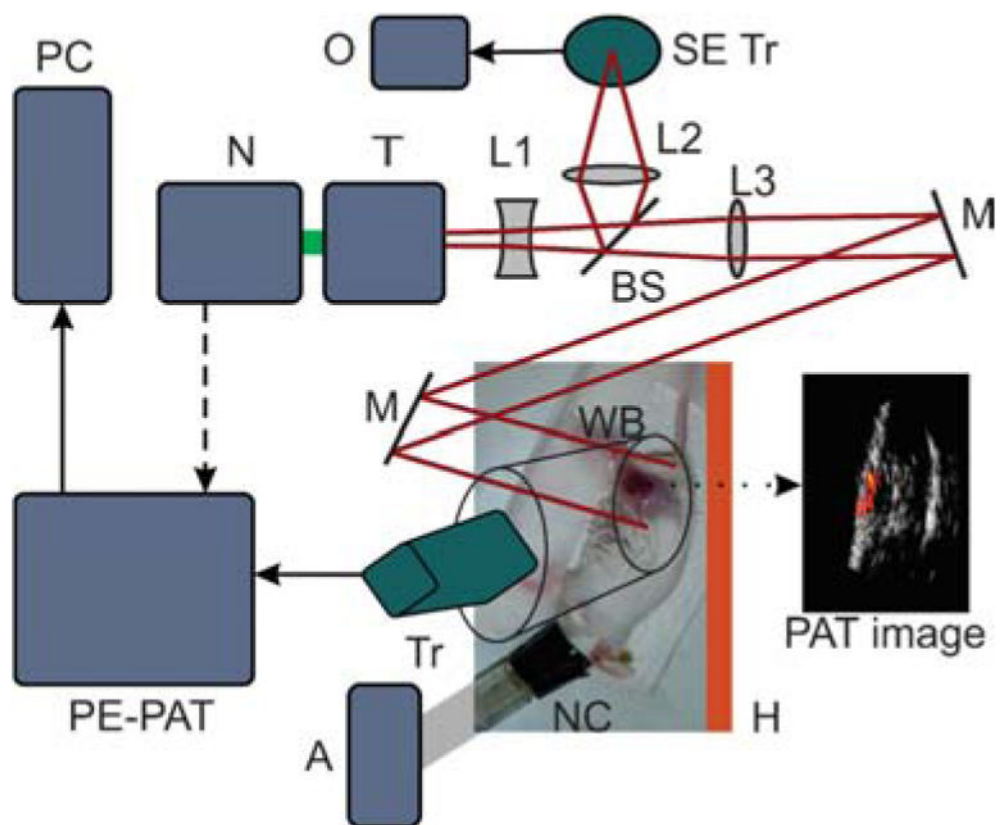
A. PEG-ylated quinoline-annulated dye **4e** dissolved in PBS (~33.3 mM) in a microcuvette.

B. Mouse urine collected after ~45 min after injection of **4e** in a capillary tube.



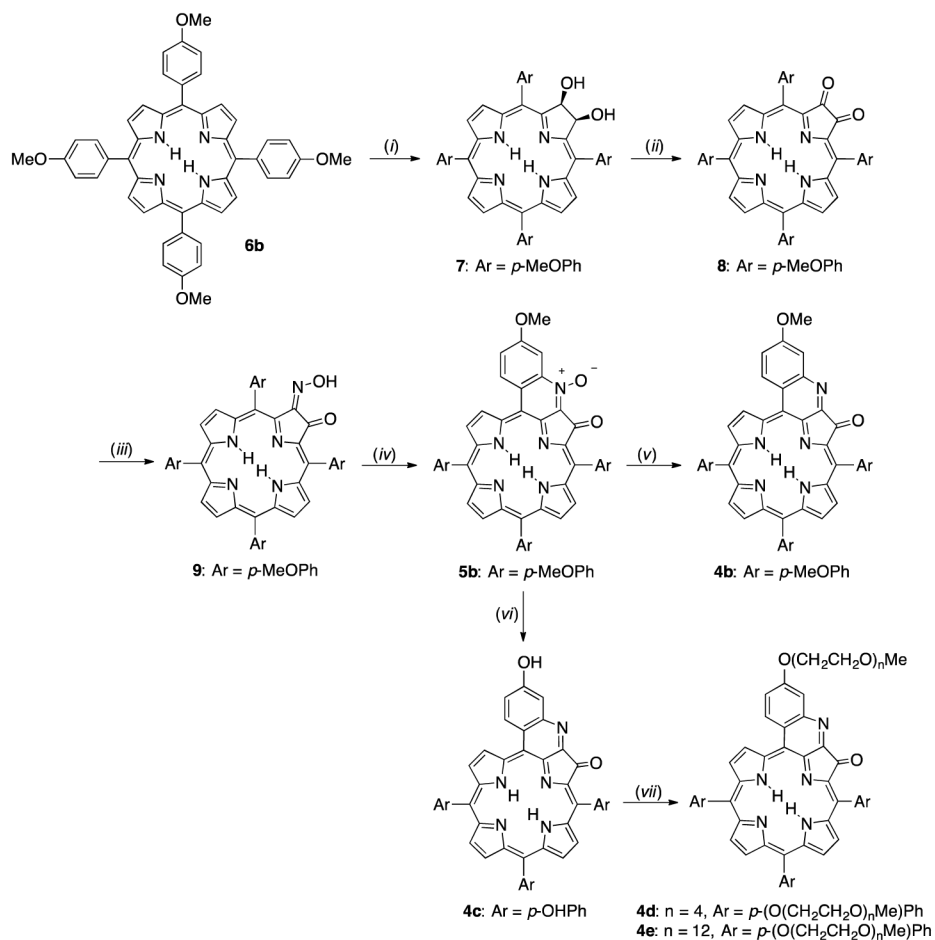
**Figure 6.**

A. UV-vis spectra of **4f** (black) and **11** (red) (solid lines), and fluorescence emission (red broken line;  $\lambda_{\text{excitation}} = 441$  nm) for phenoxy-BODIPY **11** (all MeOH). B. UV-vis (solid line) and fluorescence emission (broken line;  $\lambda_{\text{excitation}} = 441$  nm) spectra of quinoline-annulated porphyrin-BODIPY dyad **4g** (MeOH).

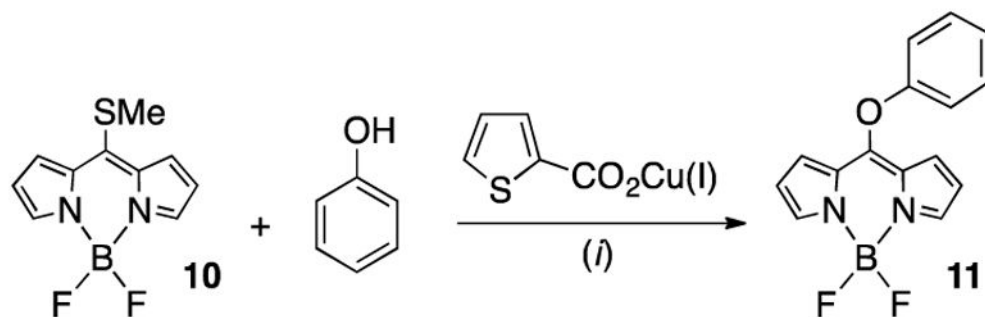


**Figure 7.**

*In vivo* PAT experiment setup. N: Nd:YAG second harmonic laser, T: tunable Ti:sapphire laser, L1, L2, L3: lenses, BS: beam splitter, SE Tr: single element transducer for monitoring laser fluctuations, O: oscilloscope, M: mirror, WB: water bag, Tr: transducer, H: heater, NC: nose cone, A: anesthesia compound (1.5 L/min oxygen with 1.5 % isoflurane), PE-PAT: the co-registered PE-PAT system, PC: computer.

**Scheme 1.**

Reaction conditions: (i) 1. 1 equiv. OsO<sub>4</sub>, 30% pyridine/CHCl<sub>3</sub>, r.t.; 2. H<sub>2</sub>S (ii) 4 equiv. DMP, CH<sub>2</sub>Cl<sub>2</sub>, r.t. (iii) 100 equiv. NH<sub>2</sub>OH·HCl, pyridine, N<sub>2</sub> atmosphere, r.t. (iv) DDQ, CH<sub>2</sub>Cl<sub>2</sub>, r.t. (v) pyridine, (vi) 1. BBr<sub>3</sub>, CH<sub>2</sub>Cl<sub>2</sub> (vii) Me(OCH<sub>2</sub>CH<sub>2</sub>)<sub>*n*</sub>OMs, Cs<sub>2</sub>CO<sub>3</sub>, DMF, 90 °C.

**Scheme 2.**

*Reaction Conditions:* (i) Na<sub>2</sub>CO<sub>3</sub>, MeCN, 55 °C.



