

Computed Tomography–Based Thrombus Imaging for the Prediction of Recanalization after Reperfusion Therapy in Stroke

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The prediction of successful recanalization following thrombolytic or endovascular treatment may be helpful to determine the strategy of recanalization treatment in acute stroke. Thrombus can be detected using noncontrast computed tomography (CT) as a hyperdense artery sign or blooming artifact on a T2*-weighted gradient-recalled image. The detection of thrombus using CT depends on slice thickness. Thrombus burden can be determined in terms of the length, volume, and clot burden score. The thrombus size can be quantitatively measured on thin-section CT or CT angiography/magnetic resonance angiography. The determination of thrombus size may be predictive of successful recanalization/non-recanalization after intravenous thrombolysis and endovascular treatment. However, cut-offs of thrombus size for predicting recanalization/non-recanalization are different among studies, due to different methods of measurements. Thus, a standardized method to measure the thrombus is necessary for thrombus imaging to be useful and reliable in clinical practice. Software-based measurements may provide a reliable and accurate assessment. The measurement should be easy and rapid to be more widely used in practice, which could be achieved by improvement of the user interface. In addition to prediction of recanalization, sequential measurements of thrombus volume before and after the treatment may also be useful to determine the efficacy of new thrombolytic drugs. This manuscript reviews the diagnosis of thrombus, prediction of recanalization using thrombus imaging, and practical considerations for the measurement of thrombus burden and density on CT.

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Introduction

Imaging studies, including computed tomography (CT) and magnetic resonance imaging (MRI), are essential for the diagnosis and treatment of patients with acute stroke. Imaging methods in stroke have been developed and evolved for the accurate diagnosis of infarction/hemorrhage and arterial occlusion and the assessment of perfusion and collateral circulation. Since the successful introduction of reperfusion therapy in stroke, one of the key issues has been the selection of patients who would

benefit from the recanalization therapy.^{1,2} Thus, the development and use of imaging techniques in acute stroke have been focused on identifying the presence and extent of potentially salvageable areas upon recanalization and the durability of ischemic areas until recanalization. This imaging strategy has also been used for patient selection in several major clinical trials.³⁻⁶ However, to rescue the salvageable areas, the occluded artery should be opened after recanalization treatment. Meanwhile, favorable clinical outcomes are not achieved in many patients treated with intravenous (IV) tissue plasminogen activator (tPA)

or endovascular treatment.⁷⁻⁹ Therefore, the prediction of successful recanalization following thrombolytic or endovascular treatment is important. This prediction may also be helpful in determining the recanalization treatment strategy.

Imaging methods for the diagnosis of stroke and salvageable areas target the brain tissues and arteries. However, the thrombus is the ultimate target of recanalization treatment. In this regard, thrombus imaging evaluation is essential for predicting the response to IV tPA or endovascular treatment.¹⁰ Various preclinical and clinical studies on direct thrombus imaging have been introduced in a recent review.¹¹ While the thrombus can be detected using noncontrast CT (NCCT), gradient-recalled echo (GRE), and susceptibility-weighted imaging (SWI) in humans (Supplementary Figure 1), most studies that investigated the prediction of thrombus imaging for recanalization have been performed using CT. Compared to MRI, CT is more easily and widely used, and CT-based thrombus imaging provides more precise information on thrombus burden. Furthermore, the density (Hounsfield unit [HU]) may represent the characteristics/composition of the thrombus to some extent. Recently, as endovascular thrombectomy has been more widely used for acute stroke, we can obtain the thrombi occluding the intracranial arteries and know more about their histological characteristics and relationship with thrombus densities on CT.

This manuscript reviews the imaging diagnosis of thrombus on CT, prediction of recanalization using CT-based thrombus imaging, methods for the quantitation of thrombus burden and density on CT, and histological and imaging characteristics of thrombus in acute stroke.

Detection of the thrombus

Thrombus is detected on NCCT as a hyperdense artery sign. The diagnosis of thrombus on NCCT depends on the slice thick-

ness. Conventional CT using 5- or 10-mm slice thickness has a limitation in displaying thrombi in the intracranial arteries, including the MCA, which has a diameter < 3 mm.¹² In 51 patients with infarction in the middle cerebral artery (MCA) or anterior cerebral artery (ACA) territory, thrombi were identified in 45 patients (88%) on thin-section (1.25- or 1-mm thickness) NCCT, but only in 16 patients (31%) on standard 5-mm NCCT.¹³ This finding was replicated by another study that compared the detection of clot between 5-mm NCCT and 0.625-mm NCCT in 54 patients with MCA occlusion.¹⁴ The thin-section NCCT is sensitive, reliable, and accurate for the detection of thrombi.¹⁵

Prediction of recanalization based on thrombus size

Prediction in intravenous tPA thrombolysis

Recanalization rates after IV tPA in stroke depend on the location of the occluded cerebral arteries. IV tPA-induced recanalization is achieved more frequently in the MCA M2 occlusion than in the proximal MCA or the internal carotid artery occlusion.^{16,17} Thrombus volume differs according to the location of occluded arteries. For example, the average thrombus volume is largest in the internal carotid artery occlusion, followed by MCA M1 and MCA M2 occlusion.¹⁸ Thus, thrombus volume may be a critical factor for successful recanalization in patients with acute stroke treated with IV tPA.

Several studies investigated whether the determination of thrombus size can predict successful recanalization/non-recanalization after IV tPA treatment in patients with stroke (Table 1). Kim and colleagues first investigated the association between successful recanalization and thrombus volume, which was measured automatically using a 3-dimensional imaging software, in 34 patients with MCA occlusion.¹⁹ This study included patients who were treated with IV tPA or IV tPA plus intra-arte-

Table 1. Thrombus burden and recanalization (IV thrombolysis)

Author (year)	Patient No.	Artery	Imaging (CT thickness, mm)	Method	Association with recanalization
Kim, 2006 ¹⁹	8	MCA	NCCT (1.25)	Volume	No (58.8 ± 52.7 vs. 44.36 ± 66.5, <i>P</i> = 0.564)*
Riedel, 2011 ²⁰	138	Not specified	NCCT (2.5)	Length	Yes (cut-off 8 mm, <i>P</i> < 0.001)
Shobha, 2013 ²¹	41	M1	NCCT (5.0)	Length	Yes (86% vs. 37% vs. 0%, <i>P</i> < 0.001) [†]
Behrens, 2014 ²²	96	Any intracranial	CTA, MRA	Length	Yes (OR 0.78, 95% CI 0.65-0.95, <i>P</i> = 0.014) [‡] No recanalization in thrombus > 16 mm
Rohan, 2014 ²³	80	M1	CTA	Length	Yes (cut-off 12 mm, sensitivity 0.67, specificity 0.71, OR 4.81, 95% CI 1.86-12.40)
Strbian, 2014 ²⁴	103	BA	CTA, MRA	Length	Yes (15 [6-25] vs. 5.5 [3.6-15.4], <i>P</i> < 0.001)

CT, computed tomography; MCA, middle cerebral artery; NCCT, noncontrast computed tomography; CTA, computed tomography angiography; MRA, magnetic resonance angiography; OR, odds ratio; CI, confidence interval; BA, basilar artery.

*Recanalization vs. nonrecanalization, mm³; [†]thrombus length < 10 mm vs. 10-19 mm vs. 20 mm, percent for the disappearance of hyperdense artery sign on follow-up scan; [‡]decreased probability of recanalization per mm.

rial (IA) urokinase, and no association was found between the thrombus volume and recanalization. Negative association in this study might be ascribed to the small sample size and the use of heterogeneous recanalization treatment modalities. In the subsequent studies, thrombus length was determined on NCCT or maximum intensity projection images using CT angiography (CTA)/MR angiography (MRA), and the length of thrombus was significantly associated with successful recanalization after IV tPA treatment.²⁰⁻²⁴ They attempted to determine the optimal cut-off for predicting non-recanalization. However, the optical cut-off was different among studies varying from 8–16 mm (Table 1). Furthermore, they evaluated recanalization at different time points after IV tPA infusion.¹⁹

Prediction in endovascular treatment

The association between thrombus size and successful recanalization after endovascular treatment has also been investigated. The results of the studies were inconsistent (Table 2). It might be because of the different mechanical devices used, different methods used to determine thrombus size, and small number of cases included.^{21,25-30} However, in a recent study of a relatively large number of patients who were treated with a stent retriever, higher clot burden scores were associated with increased likelihood of recanalization.² Smaller thrombi may be more easily retrieved with fewer attempts using a Solitaire device. However,

the predictability of thrombus size for successful recanalization seems less remarkable in endovascular treatment than in IV tPA treatment.

Practical considerations for the measurement of thrombus size

Thrombus volume

Thrombus size can be determined in terms of volume, length, or burden score (Table 3). The thrombus volume is measured using imaging analysis software.^{18,31} This software-based measurement of thrombus volume provides the most accurate and reliable information on thrombus burden, irrespective of the angio-architecture. Rapid and easy measurements of thrombus volume and density are now feasible using a 3-dimensional software. Briefly, after the detection of thrombus on NCCT via the process of pixel pigmentation, a region of interest (ROI) is defined within any portion of thrombus using a brush tool. Then, automatic region growing is performed in the range of HU 40-100, and the volume and mean HU are automatically calculated and shown. This software may be used in emergent situations.³²

Thrombus length on noncontrast CT

Thrombus length can also be used to estimate the thrombus size. The accurate determination of thrombus length on standard

Table 2. Thrombus burden and recanalization (endovascular treatment)

Author (year)	Patient No.	Artery	Primary treatment modality	Imaging (CT thickness, mm)	Method	Association with recanalization*
Kim, 2006 ¹⁹	12	MCA	IAT	NCCT (1.25)	Volume	No (39.2 ± 37.4 vs. 123.5 ± 169.1, <i>P</i> = 0.2)*
	14		IVT+IAT			No (106.1 ± 94.5 vs. 79.2 ± 61.8, <i>P</i> = 0.482) *
Spiotta, 2014 ²⁵	122	MCA	Penumbra,	CTA	Length	No (13.3 ± 10.0 vs. 13.5 ± 7.6, <i>P</i> = 0.92)*
Shobha, 2013 ²¹	35	M1	Not specified	NCCT (5.0)	Length	Yes (60% vs. 33% vs. 50%, <i>P</i> < 0.002) [†]
Mokin, 2014 ²⁶	41	ICA, M1, M2	Solitaire	NCCT (5.0)		No
					CBS	6.6 ± 1.1 vs. 6.6 ± 1.8, <i>P</i> = 0.87
					Volume, Length	101.0 ± 81.0 vs. 89.8 ± 65.0, <i>P</i> = 0.43 12.2 ± 4.7 vs. 14.0 ± 6.0, <i>P</i> = 0.44
Jindal, 2014 ²⁷	28	M1, ICA	Penumbra, Solitaire, Trevo	SWI, CTA, NCCT	length	No, <i>P</i> = 0.378
Soize, 2015 ²⁸	153	Any intracranial	Solitaire	GRE	Length	15.4 ± 8.4 vs. 20.1 ± 9.0, <i>P</i> = 0.00003, cut-off 18 (sensitivity 0.70, specificity 0.57, OR 3.09)
Angermler, 2016	63	MCA, ICA	Stent retriever	CTA	CBS	No (7 [6-8] vs. 6 [4.5-7.0], <i>P</i> = 0.08)
Mokin, 2016	69	MCA, ICA	Solitaire	CTA	CBS	No (6.5 ± 1.7 vs. 7.3 ± 1.3, <i>P</i> = 0.25)
Treurniet, 2016	499	MCA, ICA	Solitaire	CTA	CBS	Yes (model A: OR, 1.25, 95% CI, 1.13-1.81, model B: OR 1.27, 95% CI, 1.14-1.41) [‡]

Values are mean ± standard deviation, median [interquartile range], or odds ratio (OR) with 95% confidence interval (CI).

The volume is presented as mm³, and the length is presented as mm.

CT, computed tomography; MCA, middle cerebral artery; IAT, intra-arterial thrombolysis; NCCT, noncontrast computed tomography; IVT, intravenous thrombolysis; ICA, internal carotid artery; M1, M1 segment of MCA; CTA, computed tomography angiography; SWI, susceptibility-weighted imaging; GRE, gradient-recalled echo; CBS, clot burden score.

*Recanalization (TICI ≥ 2) vs. nonrecanalization (TICI < 2); [†]thrombus length < 10 mm vs. 10–19 mm vs. 20 mm, percent for the disappearance of hyperdense artery sign on follow-up scan; [‡]odds ratio (OR) and 95% confidence interval (CI) based on two different statistical models.

Table 3. Methods to measure the thrombus size and burden

	Volume	Length		Clot burden score
		On NCCT	On angiography	
Imaging tool	Thin-section NCCT	Thin-section NCCT	CTA, MRA	CTA, MRA
Thrombus measurement	Direct	Direct	Indirect based on absence of contrast opacification	Indirect based on absence of contrast opacification
Measurement method	Pixel segmentation, region growing, and automatic calculation using 3-dimensional imaging software	Pixel segmentation and Euclidean length measurement after reducing to skeleton using software	Measurement using free-hand curve function on MIP image after post processing procedure	Visual scoring based on determining the absence of contrast opacification in the predefined locations
Measurable artery	Any intracranial artery	Usually proximal segment of intracranial artery	Any intracranial artery	Anterior circulation
Accuracy	Close to actual thrombus burden (volume)	Close to actual thrombus length	Can be overestimated	Approximate burden Can be overestimated
Practical use	Requires software	Requires software	Requires postprocessing	Easy and rapid by visual assessment

NCCT, noncontrast computed tomography; CTA, computed tomography angiography; MRA, magnetic resonance angiography; MIP, multiple projection images.

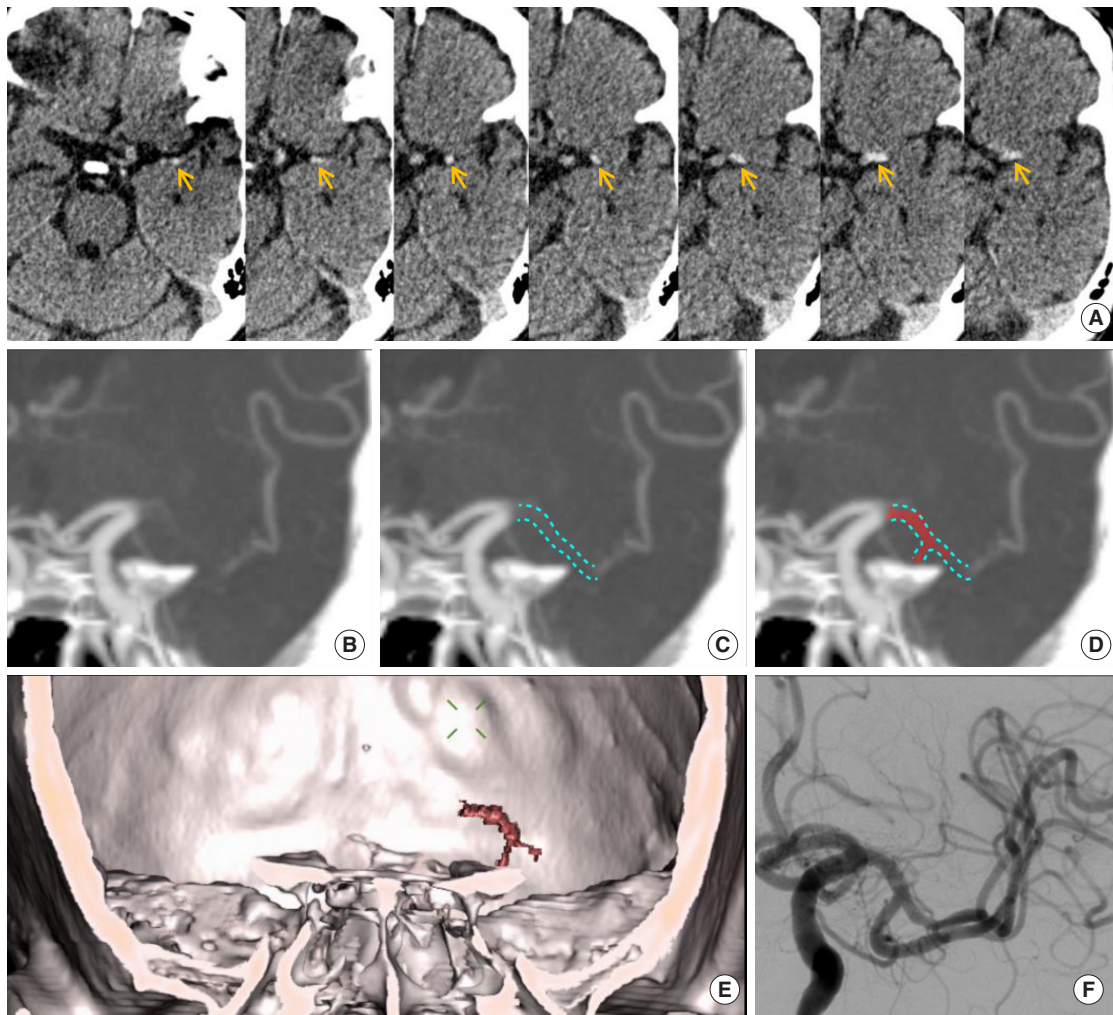


Figure 1. A representative case for the measurement of thrombus length. Hyperdense artery sign is seen on thin-section noncontrast computed angiography (CT) scan (arrows) (A). Measurement of thrombus length on this plain CT is almost impossible (A). An imaginary line (green dotted line) is drawn to measure the length on CT angiography (B, C). The actual location of the thrombus (D), which was visualized using 3-dimensional software (E), was superimposed on the imaginary lines of the actual angioarchitecture based on the angiographic findings after successful retrieval of thrombi using Solitaire stent (F). The thrombus length is overestimated on CT angiography, and thrombus in the bifurcated branch cannot be measured (D).

NCCT is very difficult (Figure 1A), and depends on the slice thickness of the CT scan. Accordingly, the length is first determined on thin-section NCCT via image processing procedures: pixel segmentation, region growing, reducing to a skeleton by applying a topography-preserving morphological thinning operation, and calculation of the maximum Euclidean length of the resulting skeleton.¹² Based on this method, a thrombus length of 8 mm on 2.5-mm NCCT was suggested as a cut-off of predicting non-recanalization after IV tPA treatment.²⁰ In fact, the THERAPY trial (The Randomized, Concurrent Controlled Trial to Assess the Penumbra System's Safety and Effectiveness in the Treatment of Acute Stroke), which tested the effect of aspiration thrombectomy, included a thrombus length of 8 mm or longer as inclusion criteria.³³

Thrombus length on CT angiography

Thrombus length may be measured on CTA, MRA, delayed gadolinium-enhanced T1 image, or SWI.^{34,35} The freehand curve function is used to measure thrombus length on maximum intensity projection (MIP) images.²³ The measurements on CTA or MRA are based on an arbitrarily drawn line in the absence of information on the actual angioarchitecture. Determination of the distal end of thrombus is dependent on the backflow from collateral circulation. Thus, the length on CTA or MRA cannot be adequately measured in cases that lack the backflow and is therefore frequently overestimated. Obtaining delayed images using multiphase CTA or dynamic CTA may be helpful in reducing overestimation due to the backflow issue.³⁴ In addition, accurate measurements of length either on NCCT or CTA/MRA are limited in curved or branched arteries. In cases with different arterial diameters, thrombus length may not precisely represent the actual burden of thrombus (Figure 1). Due to these limitations, the determination of thrombus length is usually limited to the MCA M1 segment in most cases.

Clot burden score

The clot burden score is a 10-point scoring system to quantify the thrombus burden for anterior circulation. For scoring, major arteries are allotted for the presence of contrast opacification on CTA. One or two points are subtracted for the absence of contrast opacification in the infraclinoid internal carotid artery (ICA) (2), supraclinoid ICA (2), proximal M1 (2), distal M1 (2), M2 branches (one each), and A1 (1).³⁶ This scoring system provides easy and rapid, yet only approximate, information on thrombus burden and can be used for the occlusion in anterior circulation only. The clot burden score is also influenced by the backflow from collateral circulation; hence, clot burden may be overestimated in cases with insufficient collaterals.² However, overestimated clot burden because of the lack of contrast filling due to

poor collaterals may strengthen the prognostic value of this clot burden score because poor collaterals are known to be associated with poor outcomes.²

Prediction of recanalization based on the thrombus density

Thrombus density on CT may reflect the constituents of the thrombus to some extent. Red blood cells (RBCs) in the thrombus increase attenuation on CT. A hyperdense artery sign is seen more commonly in RBC-dominant or mixed thrombi than in fibrin-rich thrombi.^{37,38} RBC-rich thrombi are also seen on MRI. The RBC components in thrombi induce ferromagnetic field distortion, which results in a blooming artifact on GRE and SWI.

Thrombi are traditionally differentiated into "red thrombi" or RBC-fibrin-rich thrombi and "white thrombi" or platelet-fibrin-rich thrombi. It is assumed that the constituents of thrombi differ in large artery atherosclerosis and in cardioembolism because they have different mechanisms of thrombus formation. The introduction of mechanical thrombectomy has allowed the comparison of the histological features of retrieved thrombi from patients with acute stroke. Earlier studies compared thrombi using hematoxylin-eosin staining and found no histological difference between arterial and cardiac thrombi.^{38,39} Subsequent studies used hematoxylin-eosin and special or immunohistochemical staining to define the constituents of thrombi more distinctly. However, findings were inconsistent among studies on RBC dominance in arterial thrombi⁴⁰⁻⁴² or cardiac thrombi^{43,44} (Supplementary Table 1).

The microscopic distribution of platelets and fibrin within the thrombus may be different between arterial and cardiac thrombi. In arterial thrombi, RBC masses are located in the center with a thin outer covering of fibrin-platelet and platelet aggregates in the edge of the thrombi. However, in cardiac thrombi, platelet aggregates are scattered throughout the thrombi with large amounts of fibrin.⁴¹ Although the simple average of thrombus HU does not provide consistent information on the prediction of thrombus histology and the origin of thrombi (cardiac or arterial), higher HU on CT may suggest a higher proportion of RBC in the thrombus. However, a blooming artifact on MRI can provide information on the presence of thrombus only.

Different thrombus characteristics may affect the response to IV tPA. Previous studies showed that thrombus density (HU) is predictive of recanalization (Table 4). Successful recanalization was achieved more frequently in patients with thrombi of higher HU than those of lower HU after IV tPA or endovascular treatment.^{19,26,45-47} However, in studies that assessed the degree of thrombus resolution on thin-section NCCT taken before and af-

Table 4. Thrombus density on CT and recanalization

	Thickness (mm)	Method of ROI drawing	Recanalization assessment	Treatment modality	Patient No.	Recanalization mean \pm SD HU (relative HU*)		
						Yes	No	P-value (cut-off [†])
Kim, 2006 ¹⁹	1.25	Automatic	Within 1 day	IVT	8	55 \pm 3.2	48.4 \pm 3.2	0.043
				IAT	12	53.8 \pm 2.9	49.5 \pm 2.4	0.025
				IVT+IAT	14	53.2 \pm 2.7	47.3 \pm 2.9	0.009 (< 49.5)
Puig, 2011 ⁴⁵	3.0	Manually outlined the margin	1 hour	IVT	45	49.3 (1.57 \pm 0.23)	42.1 (1.11 \pm 0.15)	< 0.001 (< 1.382)
Moftakhar, 2012 ⁴⁶	2.5	Manually drawn within thrombus	Not specified	IVT	45	1.58	1.39	0.01
				IAT	43	1.66	1.4	0.006
				IVT+EVT	77	1.7	1.3	< 0.0001
Mokin, 2014 ²⁶	5.0	Manually outlined the margin	at EVT	IVT+stent	41	49.9 \pm 7.6 (1.2 \pm 0.2)	43.8 \pm 6.6 (1.0 \pm 0.1)	0.01 0.03
Nielsten, 2014 ⁴⁷	1.0	Manually drawn small circles	1-5 days	IVT	88	63.1 \pm 10.7 (1.54 \pm 0.23)	52.2 \pm 9.5 (1.29 \pm 0.20)	< 0.0001 (< 56.5, < 1.38)
Spiotta, 2014 ²⁵	4.8	Manually drawn small circles	at EVT	IVT/IAT IVT+Penumbra	137	57.1 \pm 16.3	68.7 \pm 43.2	0.22

CT, computed tomography; SD, standard deviation; ROI, region of interest; HU, hounsfield unit; IVT, intravenous thrombolysis; IAT, intra-arterial thrombolysis; EVT, endovascular treatment.

*Relative HU is calculated as HU of symptomatic side/HU of asymptomatic side; [†]Cut-off for persistent occlusion.

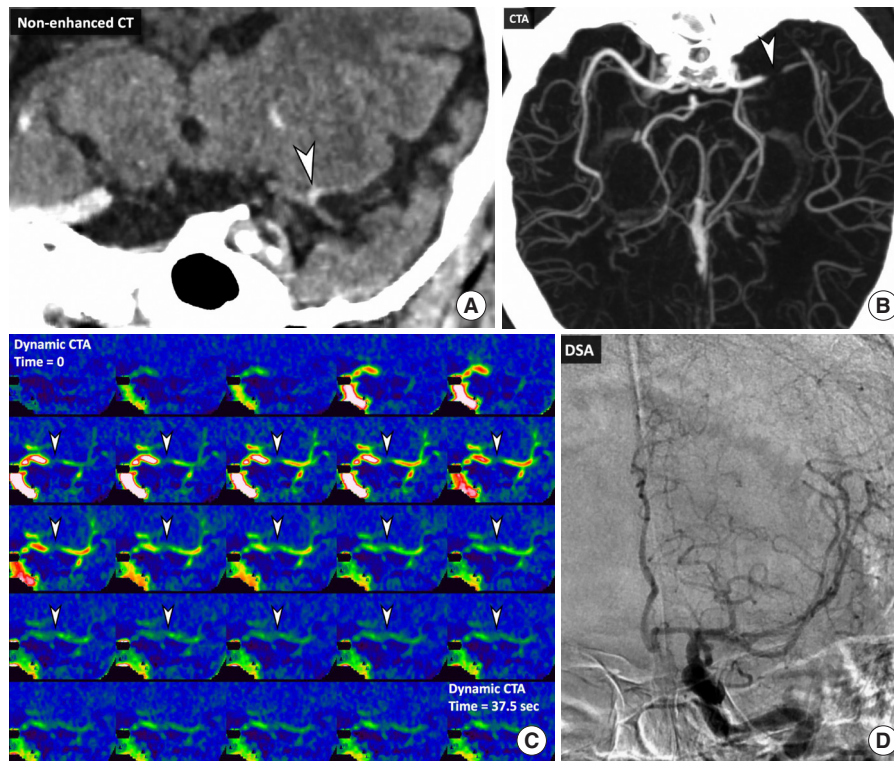


Figure 2. A representative case with perviousness. A 78-year-old man who presented with right-side weakness and sensory aphasia. Non-enhanced CT shows a "hyperdense" thrombus (arrowhead) in the bifurcation of the left middle cerebral artery (MCA), which corresponds to the occlusion on computed tomography angiography (CTA) (arrowhead) (A, B). Dynamic CTA shows gradual enhancement in the thrombus (arrowheads). This gradual enhancement indicates the perviousness of a contrast agent into the thrombus (C). Intravenous tissue plasminogen activator (tPA) was administered after obtaining dynamic CTA. Digital subtraction angiography taken 2 hours after tPA demonstrates complete recanalization of left MCA (D).

ter IV tPA infusion, the thrombus density was not associated with the degree of thrombus resolution.^{32,48} As mentioned earlier, the proportion and distribution of each component in thrombus

are quite heterogeneous. In addition, recanalization is influenced by other factors including thrombus volume and the degree of collaterals. Therefore, further studies are necessary to ascertain

the role of averaged density of thrombus on NCCT in predicting recanalization.

In a recent study, thrombus density was simultaneously measured on thin-section NCCT and CTA.⁴⁹ Then, the perviousness of thrombus was determined by calculating the increase in HU on CTA compared with NCCT. The increase in HU ≥ 23 was associated with recanalization after IV tPA treatment.⁴⁹ Perviousness to the contrast agent may reflect less compact thrombi that are more pervious to tPA, which could enhance the action of tPA within the thrombi (Figure 2). Thus, the comparison of simultaneously measured densities of thrombi on NCCT and CTA may be helpful in predicting the response to tPA.

Practical considerations for the measurement of thrombus density

Thrombus density on NCCT has been measured using different methods. To calculate density, the ROI should be defined. The thrombus margin was defined by manually outlining the margin of thrombus in each section. Then, the values of HU in each section were summed and divided by the total number of sections.⁴⁵ This method is difficult to perform in a clinical setting and may underestimate the density since low attenuated areas in the peripheral area of the thrombus might be included when manually outlining the thrombus. In another study, small circles were manually drawn three times within the thrombus, and their mean values were calculated.⁴⁷ This method is easy but may overestimate the density.

The prediction of recanalization using the average value of thrombus density should rely on how the density is measured. The distribution of RBCs, fibrin, and platelets within the thrombus are quite heterogeneous among patients and stroke subtypes.⁴¹ In fact, thrombi of arterial origin show a thin outer covering of platelet-fibrin and a zone of platelet aggregation at the edge or periphery of the thrombus.⁴¹ While responses to recanalization treatment in platelet-rich areas may be different from RBC-fibrin rich areas, platelet-fibrin area, or zone within the thrombus may be missed by manually defining the area. Therefore, the entire area of thrombus should be included for averaging HU. While defining the ROI is critical for the accurate calculation of mean HU, it is not easy to manually outline the margin of thrombi precisely. Thus, the prediction of recanalization based on thrombus density has some practical limitations for accurate measurements, which needs careful attention for the interpretation of findings in previous studies. These limitations can be overcome substantially by using 3-dimensional software, which automatically defines the ROI based on the HU of pixels so that the entire area of thrombus can be included and averaged.

Thrombus imaging to determine the efficacy of thrombolytic drugs

The degree of thrombus resolution is a direct indicator of the efficacy of thrombolytic drugs. The effect of IV tPA has been determined by quantitatively assessing the changes in thrombus volume using 3-dimensional software on NCCT before and after IV tPA infusion.^{32,48} The median volume decreased by 20%, and thrombus was completely resolved in 8% of patients after tPA infusion. The thrombus resolution increased by 9% per 10 mg increment of tPA, indicating that the degree of thrombus resolution was associated with the total dose of tPA.⁴⁸ The effect of tPA is also time-dependent. The probability of thrombus resolution was inversely correlated with the time from symptom onset to tPA treatment. These findings shed light on the importance of time course in IV tPA treatment. Earlier treatment is important not only for the rescue of tissues but also for better thrombus resolution. Hence, "Time is clot as well as brain."

Of note, thrombus volume paradoxically increased in about 20% of patients.⁴⁸ The reason for this paradoxical increase in thrombus volume after tPA treatment is still speculative. However, reocclusion after initially successful recanalization occurs in about 14–34% of patients treated with IV thrombolysis.^{50–54} The mechanism of reocclusion is associated with paradoxical activation of platelets and thrombin by tPA.⁵⁵ Reocclusion is more common in cases with residual thrombus.⁵¹ Some thrombi, including platelet-rich thrombi, may be resistant to tPA, which is fibrin-specific. The increase in thrombus volume after tPA treatment may be associated with tPA-induced paradoxical activation of platelets and generation of thrombin in patients with tPA-resistant thrombi.

Conclusions and perspectives

Imaging of thrombus has evolved from a mere diagnostic technique for the presence of clots in intracranial arteries to a quantitative and qualitative assessment tool. In addition, further understanding of the clot histology and comparison of thrombus imaging are now possible as we can get actual thrombi using clot-retrieval devices. Several methods have been suggested to assess the thrombus. However, measured thrombus volume and density differ with the methods used. Thus, it is necessary to understand the pitfalls of each measurement method. Quantitative and qualitative information on thrombi can help predict recanalization after IV tPA and endovascular treatment. Direct endovascular treatment without IV tPA treatment can be considered in cases with large thrombi that are predicted not to be recanalized by IV tPA. Sequential measurements of thrombus volume

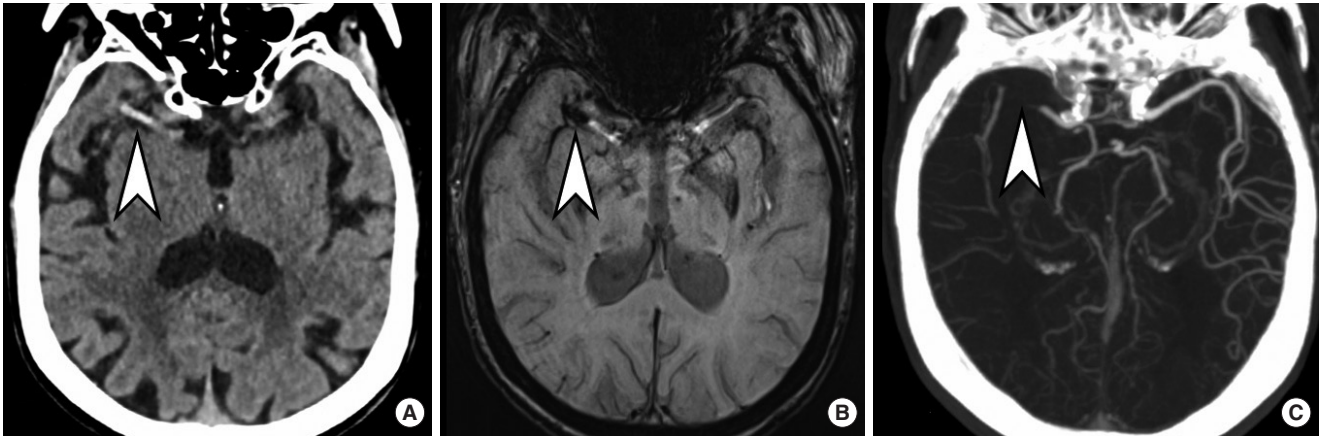
before and after thrombolytic treatment are also useful to test the efficacy of new drugs. However, a standardized method to measure the thrombus is necessary for thrombus imaging to be used more widely and reliably. Furthermore, if thrombus imaging is to be used in clinical practice for predicting recanalization after the reperfusion therapy, physicians should be able to measure thrombus volume and density easily and rapidly. Since quantitative measurements of thrombus size and density require software, the user interface and availability of software should be improved.

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Supplementary Figure 1. Diagnosis of thrombus in imaging studies. (A) Hyperdense artery sign on CT scan (arrowhead), (B) Blooming artifact on the susceptibility-weighted image (arrowhead), and (C) Occlusion on CT angiography (arrowhead). CT-Computed Tomography.

Supplementary Table 1. Thrombus histology according to the stroke subtypes

Author, year	Patient No.	Device	Staining	Analysis	RBC-dominance	Fibrin/fibrin-platelet-dominance
Marder, 2006 ¹	25	Merci	H&E	Feature detection analysis	No difference	No difference
Liebeskind, 2011 ²	50	Merci	H&E	Semi-automated quantitation using ImageJ	No difference	No difference
Sato, 2012 ³	17	Autopsy	FibII, GPIIb/IIIa, glycophorin A	Semi-automated quantitation using ImageJ	Cardiac	No difference
Niessen, 2014 ⁴	22	Merci, Trevo, Solitaire	H&E, Mallory's phosphotungstic acid-hematoxylin, glycophorin A, CD31	Quantitation by consensus	Arterial	No differences
Kim, 2015 ⁵	37	Solitaire, Aspiration	platelet glycoprotein IIIa, CD61	Semi-automated quantitation using ImageJ	Cardiac	Arterial (fibrin)
Ahn, 2016 ⁶	32	Aspiration	H&E, Martius scarlet blue, CD42b	Quantitation by software	Arterial	Cardiac (fibrin)*

H&E, hematoxylin and eosin; RBC, Red blood cell.

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