

Recapitulation of physiological spatiotemporal signals promotes in vitro formation of phenotypically stable human articular cartilage

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Standard isotropic culture fails to recapitulate the spatiotemporal gradients present during native development. Cartilage grown from human mesenchymal stem cells (hMSCs) is poorly organized and unstable in vivo. We report that human cartilage with physiologic organization and in vivo stability can be grown in vitro from self-assembling hMSCs by implementing spatiotemporal regulation during induction. Self-assembling hMSCs formed cartilage discs in Transwell inserts following isotropic chondrogenic induction with transforming growth factor β to set up a dual-compartment culture. Following a switch in the basal compartment to a hypertrophic regimen with thyroxine, the cartilage discs underwent progressive deep-zone hypertrophy and mineralization. Concurrent chondrogenic induction in the apical compartment enabled the maintenance of functional and hyaline cartilage. Cartilage homeostasis, chondrocyte maturation, and terminal differentiation markers were all up-regulated versus isotropic control groups. We assessed the in vivo stability of the cartilage formed under different induction regimens. Cartilage formed under spatiotemporal regulation in vitro resisted endochondral ossification, retained the expression of cartilage markers, and remained organized following s.c. implantation in immunocompromised mice. In contrast, the isotropic control groups underwent endochondral ossification. Cartilage formed from hMSCs remained stable and organized in vivo. Spatiotemporal regulation during induction in vitro recapitulated some aspects of native cartilage development, and potentiated the maturation of self-assembling hMSCs into stable and organized cartilage resembling the native articular cartilage.

tissue engineering | biomimetic | regenerative medicine | cartilage development | cartilage repair

Functional tissues generated in vitro from a patient's own cells could provide biological substitutes for tissues lost or damaged due to old age or injury (1). Our growing understanding of developmental biology has guided tissue-engineering approaches to better regulate stem cell differentiation and tissue formation (2–4). The articular cartilage has a limited regenerative ability due to its avascular nature (5). Current approaches to repair focal cartilage lesions include autograft, mosaicplasty, and autologous chondrocyte implantation (6–8). However, these methods are limited by donor site morbidity. Thus, there is an ongoing effort toward developing stem cell-based therapies, particularly with mesenchymal stem cells (MSCs)—the most attractive cell source for clinical application (9). Our group and others have shown that self-assembly methods recapitulated mesenchymal condensation and enhanced chondrogenesis of MSCs in vitro (10–12). Still, standard isotropic culture fails to recapitulate the spatiotemporal gradients present during native development (3, 9, 13, 14). Cartilage formed by MSCs is poorly organized and prone to endochondral ossification in vivo (4, 15). Instead, the native articular cartilage is organized and comprises the superficial zone, which develops into permanent cartilage, and the deep zone, which mineralizes to form calcified cartilage (16). We hypothesized that the

implementation of spatiotemporal regulation during induction of self-assembling human (h)MSCs in vitro can potentiate the formation of functional cartilage with physiologic organization and in vivo stability. Specifically, we investigated whether a spatiotemporally regulated induction regimen can (i) generate hyaline cartilage discs with physiologic organization from self-assembling hMSCs, (ii) induce deep-zone hypertrophy and mineralization to guide cartilage maturation, and (iii) enable the cartilage discs to remain stable and organized in vivo.

To this end, we compacted hMSCs on coated Transwell membranes by centrifugation and allowed the cells to differentiate under chondrogenic induction. At 3 wk, we switched induction in the basal compartment to a hypertrophic regimen in the experimental group, and maintained isotropic chondrogenic or hypertrophic regimens in the control groups. After 10 wk, all groups were implanted ectopically in immunocompromised mice to evaluate their stability in vivo. Through extensive analyses, we showed that the implementation of spatiotemporal regulation during induction of self-assembling hMSCs in vitro resulted in the formation of cartilage discs with physiologic stratification and deep-zone mineralization. Human MSCs formed deep-zone mineralized cartilage discs that did not undergo endochondral ossification in vivo. Instead, the cartilage discs retained zonal organization and exhibited columnar chondrocytes and nascent tidemark formation. We thus propose that the mimicry of native spatiotemporal gradients can be achieved in vitro

Significance

Despite significant efforts, stable and organized human cartilage has not been grown from human mesenchymal stem cells in vitro. We report the formation of organized cartilage discs that resemble the articular cartilage from self-assembling human mesenchymal stem cells by implementing spatiotemporal regulation in vitro that mimics native development. Selective application of chondrogenic and hypertrophic induction regimens enabled the maintenance of functional hyaline cartilage and progressive deep-zone mineralization. We demonstrate that this simple biomimetic approach helped mature the cartilage discs and enabled them to remain stable and organized following implantation. These findings highlight the limitations of current isotropic culture, and could greatly accelerate the development of new therapeutic modalities for cartilage repair from a patient's own cells.

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to enhance the organization and stability of cartilage tissues formed by self-assembling MSCs. We expect that this simple and effective approach can also be applied toward engineering other tissue types originating from self-assembling progenitor cells patterned with spatiotemporal gradients during native development.

Results

We hypothesized that the recapitulation of physiological spatiotemporal signals present during native cartilage development would promote the *in vitro* formation of phenotypically stable human articular cartilage. To test this hypothesis, we formed cartilage discs by self-assembly of hMSCs following isotropic chondrogenic induction with transforming growth factor β (TGF- β) in a dual-compartment culture (CH). The basal compartment of cartilage discs was changed to a hypertrophic regimen with thyroxine, to induce progressive deep-zone hypertrophy and mineralization, whereas the apical compartment was subjected to chondrogenic induction to maintain functional hyaline cartilage. Cartilage discs cultured under spatially isotropic chondrogenic conditions (IC) served as controls. The effects of spatiotemporal signals were investigated with respect to the formation and mineralization of cartilage, gene expression, biochemical composition, and mechanical properties of the engineered tissue.

Biochemical and Mechanical Analysis. The DNA content of the CH group was lower at 6 wk (Fig. 1C), correlating with deep-zone cleaved caspase-3 expression (Fig. S1). This suggests the onset of apoptosis with cartilage mineralization. The lower GAG content of the CH group correlated with the DNA content (Fig. S2). Collagen (COL) contents and GAG and COL productivities (contents normalized to DNA) were similar between the groups (Fig. 1C). Correspondingly, the CH group exhibited a slightly lower Young's modulus and thickness (Fig. 1D). Instead, GAG and COL contents of the IH group deteriorated significantly (Fig. S3B).

Hyaline Cartilage Formation and Deep-Zone Mineralization. Both the IC and CH groups formed hyaline cartilage rich in sulfated

glycosaminoglycan (GAG). Depthwise cross-sections of the CH group exhibited deep-zone mineralization starting at 6 wk (Fig. 1B). Histological analysis confirmed maintenance of hyaline cartilage and progressive deep-zone mineralization. Whole-tissue transverse bright-field images revealed deep-zone mineralization reaching completion by 10 wk (Fig. 1E). In contrast, the isotropic hypertrophic (IH) control group exhibited near-complete loss of cartilage, and mineralized everywhere at the edge after 10 wk (Fig. S3A and D).

Changes in Gene Expression. We assessed the gene expression of both the IC and CH groups at different time points. Correlating with the biochemical compositions, the expression of aggrecan (*ACAN*) and type II collagen (*COL2A1*) was similar between the groups. Instead, the expression of trophic factors (*BMP2*, *DKK1*, *IHH*) and markers associated with chondrogenesis (*SOX9*, *S100A*), chondrocyte maturation (*COL9A1*, *COL11A1*), and terminal differentiation (*COL10A1*, *RUNX2*, *SPPI*) was significantly up-regulated in the CH group from 6 to 10 wk (Fig. 2A). In contrast, the expression of chondrogenic markers was abolished and terminal maturation markers were up-regulated in the IH group at 10 wk (Fig. S3C).

Deep-Zone Hypertrophy. We stained for type X collagen expression and found enhanced deep-zone hypertrophy in the CH group, which correlated with deep-zone mineralization (Fig. 2C). Profiling the expression, we observed a sharp-intensity peak in the deep zone of the CH group, which increased without a change in relative position from 6 to 10 wk. Instead, the expression in the IC group was more diffuse (Fig. 2D). Thus, the implementation of spatiotemporal regulation potentiated deep-zone chondrocyte terminal differentiation.

Cartilage Maintenance and Stability *in Vivo*. We implanted all groups *s.c.* in immunocompromised mice to assess cartilage maintenance *in vivo*. After 4 wk, the IC group underwent endochondral ossification as marrow cells, and nascent bone lined the bottom of the discs. Remarkably, the CH group resisted endochondral ossification

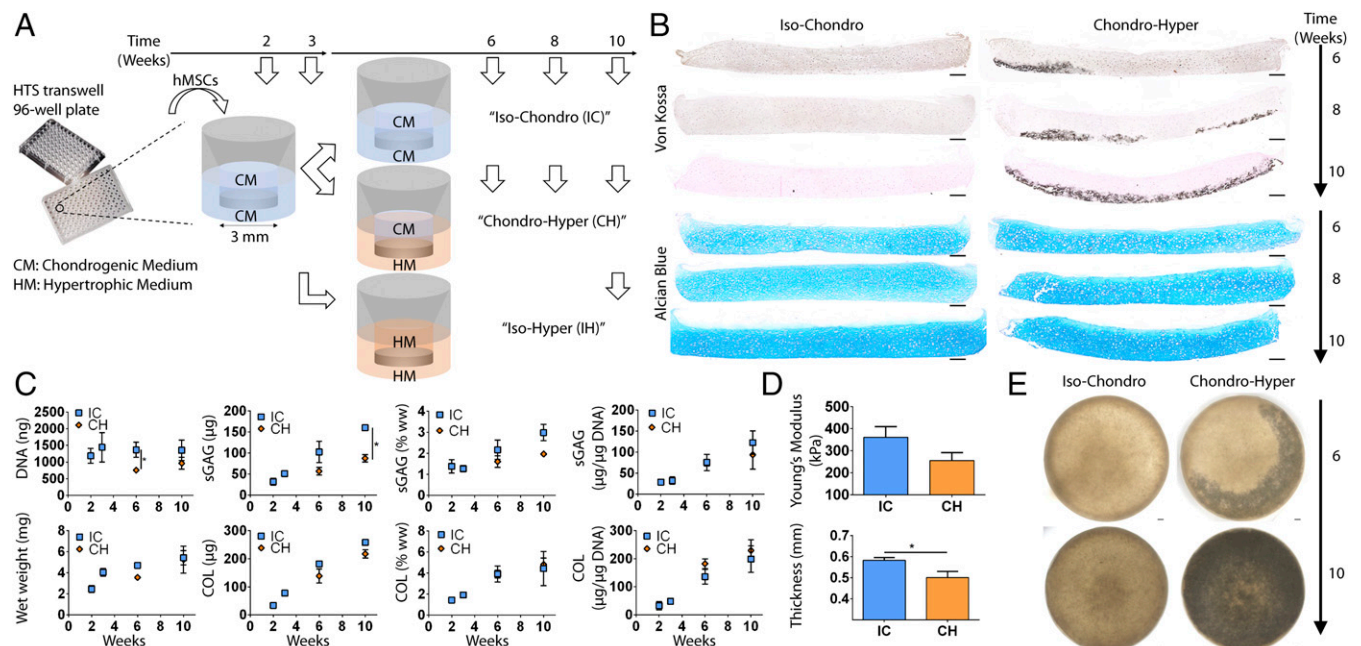


Fig. 1. Experimental design and tissue morphogenesis. (A) Schematic of the induction regimens. (B) Progressive deep mineralization in the CH group but not the IC group (Von Kossa), and maintenance of hyaline cartilage in both groups (Alcian blue). (C) Biochemical analyses revealed a lower DNA content (6 wk) and a lower GAG content (10 wk) in the CH group. COL content and GAG and COL productivities (normalized to DNA) were similar. sGAG, sulfated GAG; ww, wet weight. (D) Mechanical testing showed similar compressive Young's modulus between the groups. The IC group was slightly thicker. (E) Whole-tissue bright-field images showed near-complete mineralization by 10 wk. Mean \pm SEM; * $P < 0.05$. (Scale bars, 200 μ m.)

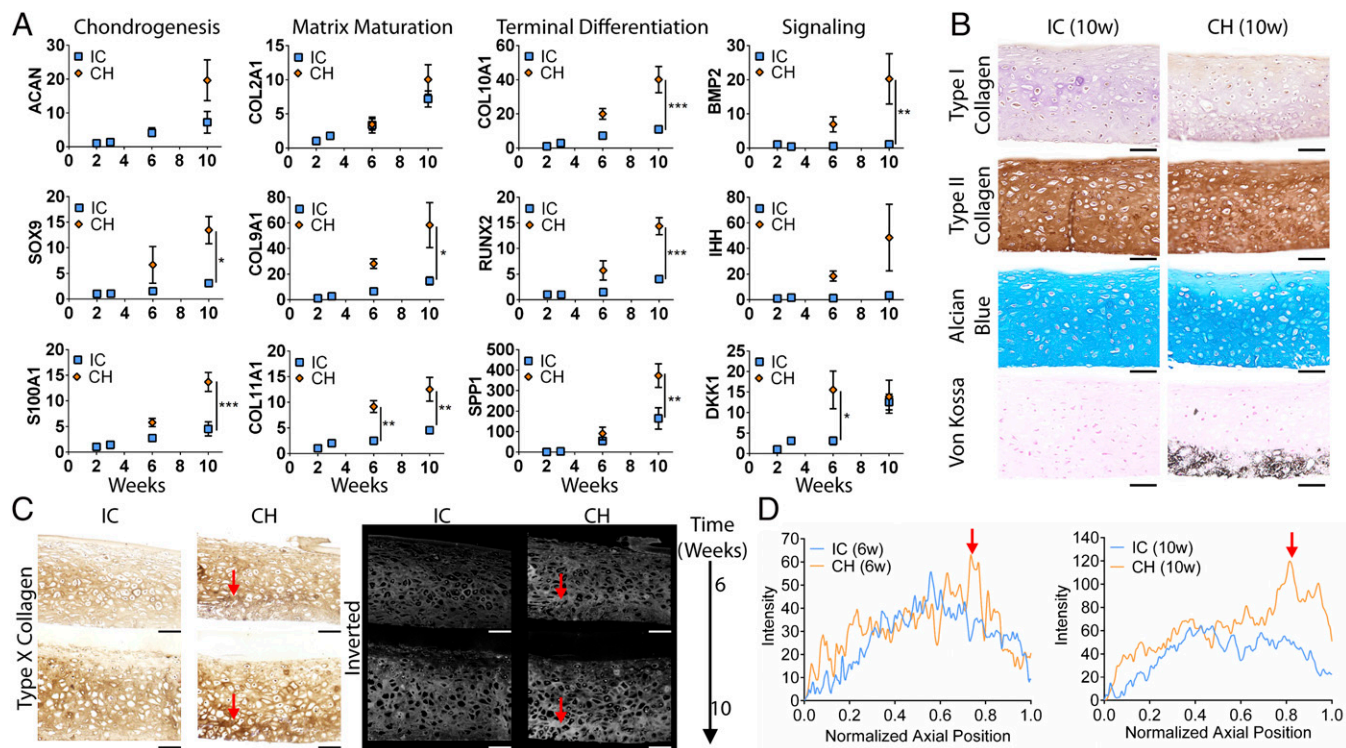


Fig. 2. Cartilage maturation and organization. (A) The CH group showed increased expression of cartilage homeostasis (SOX9, S100A1), chondrocyte maturation (COL9A1, COL11A1), terminal differentiation (COL10A1, RUNX2, SPP), and trophic markers (DKK1, BMP2, IHH) (for primers please see Table S1). ACAN and COL2A1 expression was similar between groups. All gene expression ($2^{-\Delta\Delta Ct}$) is normalized to GAPDH and 2-wk controls. (B) Hyaline cartilage at 10 wk with homogeneous type II collagen and GAG deposition. The CH group was mineralized in the deep zone. (C) Type X collagen immunohistochemical stains and inverted images. Red arrows indicate bands of hypertrophy. (D) Intensity profile of stains showed distinct deep-zone peaks in the CH group. Mean \pm SEM; * $P < 0.05$, ** $P < 0.01$, and *** $P < 0.001$. (Scale bars, 200 μ m).

and exhibited columnar chondrocytes and tidemark formation (Fig. 3). Microcomputed tomography (μ CT) analysis revealed greater mineral deposition in the IC group than in the CH group (Fig. 3B and C). Movat's pentachrome stains confirmed significant bone and marrow fractions in the IC group not seen in the CH group (Fig. 3D and E). Von Kossa stains revealed more extensive mineralization in the IC group (Fig. 3F). The IH group was also extensively mineralized, with bone formation and marrow infiltration all around the discs (Fig. S4). Thus, the implementation of spatiotemporal regulation during induction of self-assembling hMSCs in vitro resulted in the formation of organized cartilage discs that are stable in vivo.

Retention of Cartilage Markers and Zonal Organization. The CH group remained type II collagen-rich, and distinctly expressed lubricin in the superficial zone and osteopontin in the deep zone. In contrast, the IC group exhibited loss of type II collagen in the cartilage layer and deposition of type I collagen in the bone layer. The IC group exhibited faint lubricin expression and extensively expressed osteopontin. Platelet-derived growth factor-BB (PDGF-BB) staining revealed infiltration of preosteoclasts and multinuclear osteoclasts into the bottom of the IC but not the CH discs (Fig. 4A). SOX9, RUNX2, alkaline phosphatase, and type X collagen expression was zonally delineated in the CH discs but not the IC discs (Figs. S5 and S6). Compositionally, GAG content recovered in the CH group but decreased in the IC group (Fig. 4B). Correspondingly, the expression of genes associated with cartilage maintenance (SOX9, ACAN, COL2A1, COL9A1, COL11A1) and chondrocyte terminal differentiation (COL10A1, RUNX2) persisted in the CH group following implantation. In contrast, all cartilage maintenance markers were significantly down-regulated in the IC group (Figs. S6 and S7).

Standard isotropic culture conditions fail to recapitulate native spatiotemporal gradients, and tend to form poorly organized cartilage tissues that are prone to endochondral ossification in vivo (4, 15). Here we implemented spatiotemporal regulation during the induction of self-assembling hMSCs in vitro, and showed that it potentiated the formation of physiologic cartilage discs with deep-zone mineralization and in vivo stability.

Discussion

Tissue-engineering approaches are increasingly guided by biological principles. Mesenchymal condensation has been adapted into self-assembly methods to enhance cartilage formation in vitro (10, 11). TGF- β and thyroxine, potent effectors of cartilage maintenance and chondrocyte terminal differentiation, have been used in chondrogenic and hypertrophic induction regimens to guide MSC differentiation (4, 14, 17–22). Thus, we chose these two factors as culture supplements. Chondrogenesis of MSCs in vitro is defined by a temporal sequence of cellular events (3). We recently showed that isotropic chondrogenic induction of hMSCs in hydrogel formed cartilage with a deficient core (23). In other studies, isotropic hypertrophic induction of chondrogenically differentiated hMSCs resulted in uncontrolled mineralization (4, 12). As such, spatiotemporal regulation poses a significant challenge that we seek to overcome.

To enable compartmentalization and stepwise maturation, we switched deep-zone induction to a hypertrophic regimen at 3 wk. The formation of cartilage discs isolated the apical compartment from the basal compartment to set up a dual-compartment culture. This process recapitulates some aspects of the spatiotemporal gradient present during native cartilage development. Following the switch, hyaline cartilage was maintained and deep-zone mineralization progressed through 10 wk of culture.

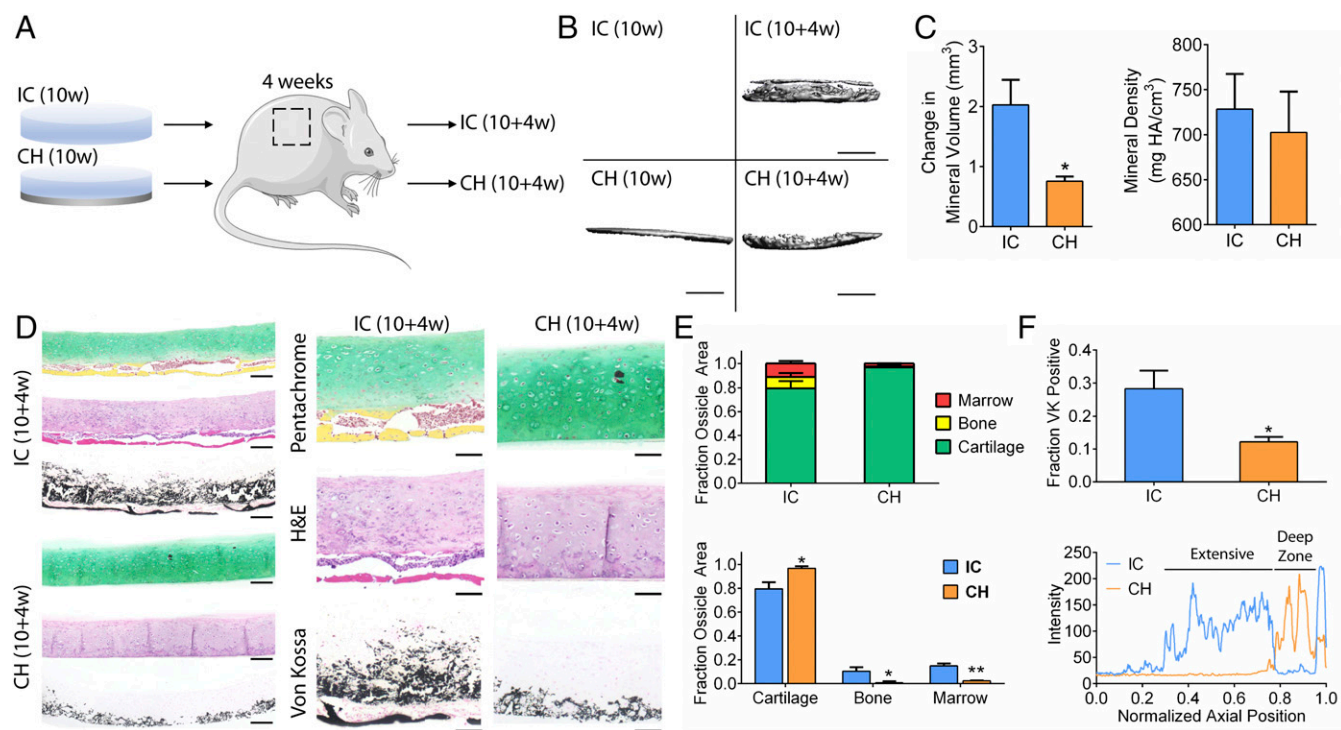


Fig. 3. Cartilage maintenance and stability in vivo. (A) Discs cultured for 10 wk under different regimens were implanted s.c. in the back of immunocompromised mice for 4 wk and explanted for analysis. (B) μ CT images showed extensive mineral deposition in the IC group following implantation but not the CH group. (Scale bar, 1 mm.) (C) The increase in mineral volume was significantly greater in the IC group than the CH group postimplantation, with similar mineral density. HA, hydroxyapatite. (D) Whole-tissue (Left) and detailed (Right) histological comparisons of IH and CH discs postimplantation. Movat's pentachrome and H&E stains of tissue cross-sections showed mature bone (yellow) with marrow cells (red) lining the bottom of the IC discs but not the CH discs. Instead, the CH discs displayed columnar chondrocytes and tidemark formation. Von Kossa stain showed extensive mineralization in the IC discs but local deep-zone mineralization in the CH discs (for antibodies please see Table S2). [Scale bars, 200 μ m (Left); 100 μ m (Right).] (E) Segmentation and quantitation of Movat's pentachrome stains showed significant fractions of bone and marrow present in the IC group but not the CH group. (F) Quantitation and profiling of Von Kossa (VK) staining showed greater and more extensive mineralization in the IC group. Mean \pm SEM; * $P < 0.05$ and ** $P < 0.01$.

Cartilage maintenance and maturation are governed by complex signaling cross-talk involving multiple pathways and transcription factors (24, 25). SOX9 and its target S100A1 are required for chondrogenesis during limb development and postnatal cartilage homeostasis (26, 27). DKK1 is a canonical Wnt inhibitor that prevents terminal differentiation (28). On the contrary, BMP2 and IHH promote terminal differentiation and the up-regulation of RUNX2 (29). Types II, IX, and XI collagen are indicative of mature articular chondrocytes, whereas type X collagen and mineral-binding proteins such as osteopontin are indicative of hypertrophic chondrocytes (25). In the present study, spatiotemporal regulation in vitro potentiated the up-regulation of these genes associated with cartilage maintenance, matrix maturation, and terminal differentiation. Along with the increased type X collagen expression in the deep zone, these data suggest that the increase in local terminal differentiation was concurrent with overall cartilage maturation.

Interestingly, gene expression at 6 wk was not significantly different between groups. This could be attributed to the heterogeneous differentiation states of the cells during induction. At 6 wk, the discs were mineralized at the rim, which suggests that deep-zone cells at the rim underwent terminal differentiation before cells in the middle. At 10 wk, the mineralization was complete and differences in gene expression of relevant markers reached significance.

Notably, we showed that the cartilage discs formed under spatiotemporal regulation in vitro were stable and remained organized during ectopic implantation in mice. Instead, discs formed in isotropic cultures underwent uncontrolled mineralization and endochondral ossification in vivo, in agreement with previous

studies (4, 15, 30). The stratification was evidenced by superficial-zone expression of lubricin and deep-zone expression of osteopontin. We previously showed that self-assembling MSCs formed cartilage with a superficial lubricin lining after 5 wk of chondrogenic induction (10). In the present study, zonal lubricin expression was observed after implantation. Despite the heterogeneous differentiation states indicated by patchy expression, SOX9 was generally expressed in the upper zone and RUNX2 in the deep zone. These indicated zonal delineation of cartilage homeostasis and chondrocyte terminal differentiation. Persistent expression of cartilage maintenance and maturation markers, and a recovery in GAG content, further confirmed the in vivo stability of the discs.

The native calcified cartilage bridges the articular cartilage and subchondral bone, and protects the articular cartilage by blocking vascular invasion and selectively permitting the passage of small molecules from the subchondral bone (31). A recent study showed that engineered mineralized cartilage increases the interfacial shear strength of osteochondral composites (12). We determined that the mineral found in the calcified cartilage formed from hMSCs is apatite, similar to that of the native cartilage, and established that the mineral density increased during implantation before endochondral ossification. In the present study, deep-zone mineralized cartilage discs formed from hMSCs remained stable and organized in vivo. Interestingly, the mineralized cartilage bore a tidemark following implantation and resembled the native calcified cartilage. The lack of endochondral ossification in vivo could be attributed in part to the chondroprotective effects of the engineered calcified cartilage.

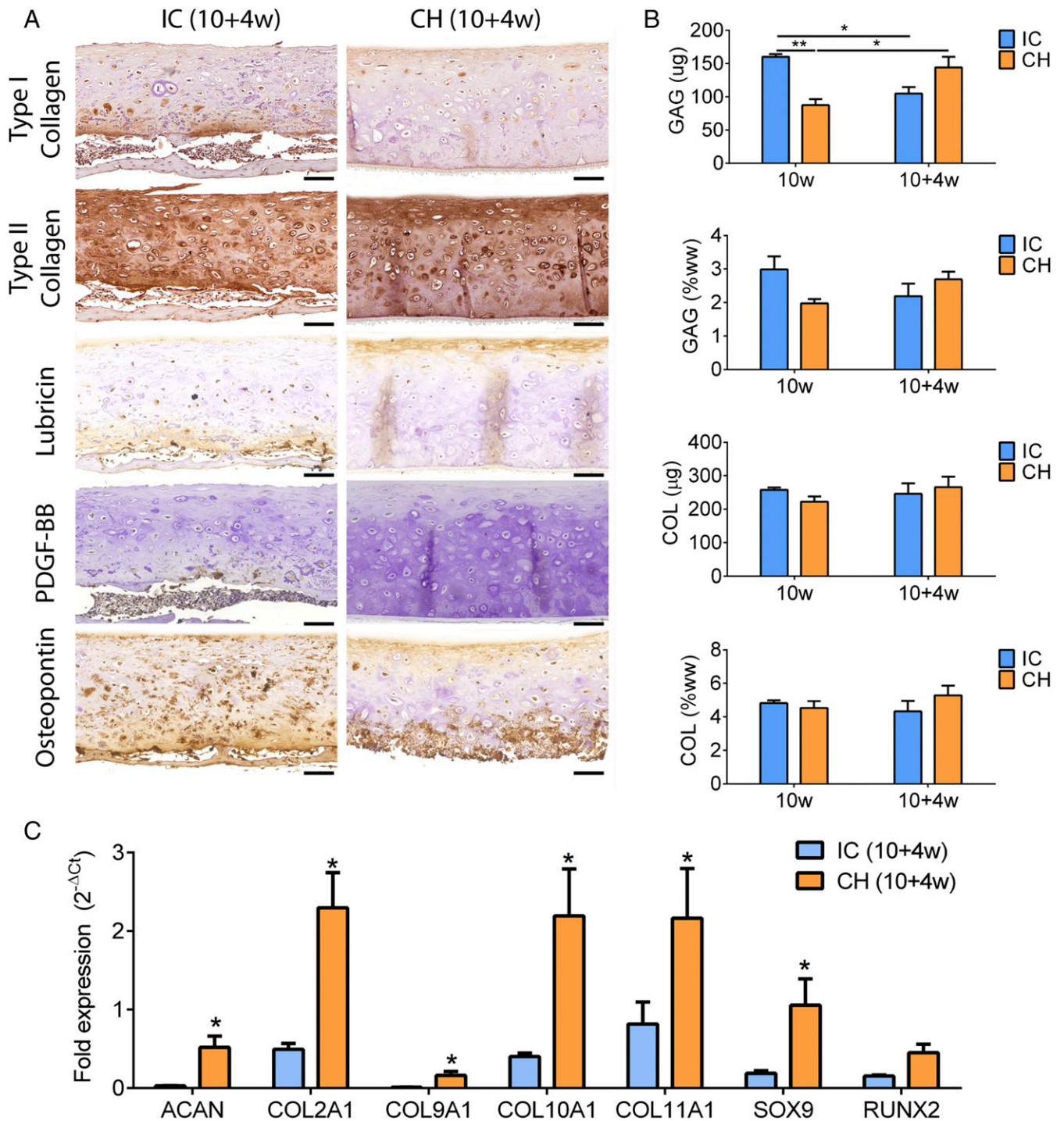


Fig. 4. Retention of cartilage phenotype. (A) The IC group showed type I collagen deposition, loss of type II collagen, faint lubricin expression in upper and lower aspects, and extensive osteopontin expression. The CH group showed homogeneous type II collagen deposition, superficial-zone lubricin expression, and deep-zone osteopontin expression. PDGF-BB staining revealed preosteoclasts/osteoclasts invading IC discs but not CH discs. (Scale bar, 100 μm .) (B) The GAG content of the CH group recovered whereas that of the IC group deteriorated postimplantation. COL contents were similar. (C) Expression of cartilage maintenance (SOX9, ACAN, COL2A1, COL9A1, COL11A1) and chondrocyte terminal differentiation (COL10A1, RUNX2) markers persisted in the CH group but not the IC group postimplantation. All gene expression ($2^{-\Delta\text{Ct}}$) is normalized to GAPDH. Mean \pm SEM; * $P < 0.05$ and ** $P < 0.01$.

There are several ways to further improve the current study. Despite showing that similarities in the organization and maturation profiles exist between the engineered cartilage and the native articular cartilage, we could not clearly define underlying mechanisms. RNA in situ hybridization would further clarify expression patterns. To increase the cartilage thickness, we could

integrate our novel approach with a method we developed to engineer large cartilage by fusing condensed mesenchymal bodies on bone scaffolds (10). Importantly, this approach locally regulated but did not inhibit type X collagen expression. The incorporation of other factors such as hypoxia and compressive loading could inhibit spontaneous hypertrophy and improve functional properties

of the engineered cartilage (30, 32). Whether bona fide articular cartilage can be formed from MSCs requires validation with well-defined markers that distinguish between mature chondrocytes and MSCs (33). Developmentally, the articular cartilage is formed by outer interzone cells originating from the chondrogenic mesoderm (16). The use of pluripotent stem cells would also enable unprecedented control, as they can generate chondrocytes with distinct articular and growth plate phenotypes (34).

In summary, we report that organized and stable articular cartilage with physiologic likeness can be grown in vitro from self-assembling hMSCs by implementing spatiotemporal regulation during induction that recapitulates some aspects of native cartilage development. We showed that this simple and effective method potentiated the formation of physiologic cartilage with deep-zone mineralization and up-regulation of markers associated with cartilage homeostasis and maturation. We demonstrated that the stratified cartilage resisted endochondral ossification and retained zonal organization without loss of cartilage marker expression in vivo. Conceivably, this method could be applied toward engineering other tissues from self-assembling progenitor cells also patterned with spatiotemporal gradients during native development.

Materials and Methods

Please see *SI Materials and Methods* for hMSC preparation, s.c. implantation, and gene expression, histological, μ CT, biochemical, mechanical, and statistical analyses. All animal experiments followed federal guidelines and were conducted under a protocol approved by the Columbia University Animal Care and Use Committee.

Disc Formation. Type I collagen (Corning) was diluted to 1.5 mg/mL in ethanol and used to coat the polycarbonate membrane (0.4- μ m pore size) of 96-well HTS Transwell inserts (Corning). The inserts were air-dried overnight and rinsed with PBS. Multiple layers of hMSCs (250,000 per well) were seeded into the inserts and compacted by centrifugation (200 \times g, 5 min). Seeded inserts were assembled with reservoir plates, each filled with 20 mL chondrogenic media. Media in the inserts were carefully topped up 3 h postcentrifugation (200 μ L per well). Tissues were incubated in a controlled humidified chamber [37 $^{\circ}$ C, 5% (vol/vol) CO₂], and media were replaced every other day. Samples were fixed in 10% (vol/vol) formalin or snap-frozen and stored at -80° C.

Induction Regimens. Chondrogenic medium comprises high-glucose DMEM supplemented with 10 ng/mL TGF- β 3, 100 nM dexamethasone, 50 μ M ascorbic acid-2 phosphate, 100 μ M sodium pyruvate, 5 μ g/mL proline, 1% insulin, transferrin, and sodium selenite mix (ITS+), and 1% penicillin-streptomycin (P/S). Hypertrophic medium comprises high-glucose DMEM supplemented with 50 nM T4, 5 mM β -glycerophosphate, 1 nM dexamethasone, 50 μ M ascorbic acid-2 phosphate, 100 μ M sodium pyruvate, 5 μ g/mL proline, 1% ITS+, and 1% P/S. After 3 wk of chondrogenic induction in both compartments, 400- μ m-thick discs formed and isolated the compartments from each other. Induction in the basal compartment (reservoir) was switched to a hypertrophic regimen in the experimental (CH) group. Chondrogenic induction was maintained in both compartments for the isotropic chondrogenic control group. Inductions in both compartments were switched to hypertrophic regimens and maintained for the isotropic hypertrophic control group. All groups were kept in culture for up to 10 wk. Samples were taken at different time points for analysis ($n = 4$).

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