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## Simulated Online Adaptive MR-Guided SBRT for the Treatment of Oligometastatic Disease of the Abdomen and Central Thorax: Characterization of Potential Advantages

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## Abstract

**Purpose/Objectives**—Stereotactic body radiotherapy (SBRT) is increasingly used to treat oligometastatic or unresectable primary malignancy, although proximity of organs-at-risk (OAR) may limit delivery of sufficiently ablative dose. Magnetic resonance (MR)-based online-adaptive radiotherapy (ART) has potential to improve SBRT's therapeutic ratio. This study characterizes potential advantages of online-adaptive MR-guided SBRT to treat oligometastatic disease of the non-liver abdomen and central thorax.

**Materials/Methods**—Ten patients treated with RT for unresectable primary or oligometastatic disease of the non-liver abdomen (n=5) or central thorax (n=5) underwent imaging throughout treatment on a clinical MR-IGRT system. SBRT plans were created based on tumor/OAR anatomy at initial CT simulation ( $P_I$ ) and simulated adaptive plans were created based on observed MR-image set tumor/OAR "anatomy-of-the-day" ( $P_A$ ). Each  $P_A$  was planned under workflow

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constraints to simulate online-ART. Prescribed dose was 50Gy/5fractions with goal coverage of 95% PTV by 95% of the prescription, subject to hard OAR constraints.  $P_I$  was applied to each MR dataset and compared to  $P_A$  to evaluate changes in dose delivered to tumor/OARs, with dose escalation when possible.

**Results**—Hard OAR constraints were met for all  $P_I$  based on anatomy from initial CT simulation, and all  $P_A$  based on anatomy from each daily MR-image set. Application of the  $P_I$  to anatomy-of-the-day caused OAR constraint violation in 19/30 cases. Adaptive planning increased PTV coverage in 21/30 cases, including 14 cases where hard OAR constraints were violated by the non-adaptive plan. For 9  $P_A$  cases, decreased PTV coverage was required to meet hard OAR constraints that would have been violated in a non-adaptive setting.

**Conclusions**—Online-adaptive MRI-guided SBRT may allow PTV dose escalation and/or simultaneous OAR sparing compared to non-adaptive SBRT. A prospective clinical trial is underway at our institution to evaluate clinical outcomes of this technique.

#### Keywords

Online-adaptive radiation therapy; ART; MRI-guided radiation therapy; MR-IGRT; SBRT; Oligometastases; Adaptive Planning

#### INTRODUCTION

Stereotactic body radiotherapy (SBRT) has emerged as a highly attractive, conformal, and non-invasive means to focally ablate oligometastatic or unresectable primary malignancy (1–3). In-field control rates of metastases treated with SBRT of 80% up to four years after therapy have been reported, including series examining heterogeneous histologies, sites, and dose (4–6). Although many patients who undergo SBRT for oligometastases will experience relapse with distant metastases (DM), approximately 20% of patients with in-field control remain disease-free at 2–4 years follow-up (4, 5, 7). Achievement of disease-free survival (DFS) is contingent upon complete local ablation of metastases (8). For SBRT, improved local control correlates with increased dose, as demonstrated by several dose escalation trials, with reported rates up to 100% at 12 months follow-up (5, 9–11).

Nevertheless, high-dose treatment of oligometastatic/unresectable primary disease with SBRT has been historically limited by normal tissue toxicity. This narrow therapeutic ratio is most evident in the central thorax, where attempted dose-escalated treatment of tumors proximal to critical structures of the mediastinum has caused pronounced increase in unacceptable toxicity, and in the abdomen, where proximity to radiosensitive organs including bowel and attempts to account for respiratory motion may increase toxicity and limit dose (12, 13).

The safe ablation of oligometastatic or unresectable primary disease with SBRT depends on accurate target delineation and localization. Until recently, technology to define and track targets during treatment has been limited to either internal tumor surrogates such as fiducial markers, or external tumor surrogates including patient surface anatomy for correlation with internal motion. These modalities may inadequately account for intrafractional organ motion and do not address interfractional motion or variability in the position of organs-at-risk

(OARs), which remain significant sources of positional uncertainty (14–18). In contrast to CT-based imaging for daily setup, onboard low-field MRI may improve soft tissue visualization for accurate definition of target volumes (19).

Recently, the necessary technology and treatment planning system (TPS) for implementation of online-ART was developed in the form of a dedicated MR-image-guided radiotherapy (MR-IGRT) system (20–23). With respect to SBRT, daily reoptimization of treatment plans based on observed daily anatomy could provide the accurate real-time target delineation that is essential for OAR sparing and dose escalation. However, potential improvements in the therapeutic ratio of SBRT using online-ART have yet to be evaluated in the context of clinical implementation of new MR-IGRT technology.

To evaluate potential applications of ART for SBRT, we compare CT-based, non-adaptive SBRT plans with simulated MR-IGRT-based adaptive plans. In this study, we characterize the potential advantages of online-adaptive MR-guided SBRT to treat oligometastatic or unresectable primary disease of the abdomen and central thorax. We hypothesized that compared with CT-based non-adaptive SBRT, simulated online-adaptive MR-guided SBRT planning may reduce OAR dose and potential toxicity while allowing dose escalation.

## METHODS AND MATERIALS

#### Patient and tumor characteristics

Ten patients treated at our institution from 2014–2015 with CT-simulated, non-adaptive radiation therapy for unresectable primary/oligometastatic disease of the central thorax or abdomen were identified for inclusion in this study. Patient and tumor characteristics are listed in Table 1. Initial clinical treatment, consisting of fractionated therapy (n=3) or SBRT (n=7), occurred either on a linear accelerator-based system (n=3) or an MR-IGRT-Co-60-based system (n=7). All patients, including those not clinically treated with SBRT, had disease limited to 1–2 oligometastatic/unresectable primary lesions that were retrospectively deemed appropriate for online-adaptive SBRT, had such technology been available at time of treatment. For patients treated on the MR-IGRT system, localization images were used for adaptive stereotactic replanning in this study. Patients not treated with MR-IGRT were selected based on prior inclusion on a separate, MR imaging study, in which they underwent additional daily imaging throughout treatment on a clinical MR-IGRT system.

#### Treatment system; time and workflow constraints

All initial and adaptive planning was performed using a dedicated MR-IGRT TPS (ViewRay Inc. Oakwood Village, OH) under time/workflow constraints to simulate online-ART. This clinical workflow has been previously described (24). In brief, the clinically-deployed, MR-IGRT unit comprises a split-solenoid 0.35 Tesla MR scanner mounted on a ring gantry with three MLC-equipped <sup>60</sup>Co heads. On each treatment day, a high-resolution volumetric MR-image (1.5x1.5x3.0mm isotropic for all patients included in this study) is acquired for each patient at time of setup. Deformable registration is performed using the planning CT dataset, followed by transfer of contours and electron density map to the daily MR. All contours were confirmed by a physician and edited manually when needed. The deformed electron

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density map is then used to recalculate dose of the original plan on the daily MR for physician evaluation. The supporting Monte Carlo-based TPS is accessible from the delivery workflow, permitting real-time adaptive planning while the patient is on the table. TPS details have been previously described (22). For this study, all imaging data was prospectively collected, but dose recalculation and adaptive planning were retrospectively performed.

#### Initial, non-adaptive planning

Traditional, non-adaptive SBRT plans were retrospectively simulated for all patients, regardless of prior treatment modality, based on tumor/OAR anatomy at initial CT-simulation (P<sub>I</sub>). Clinical simulation for thoracic patients included a free-breathing helical CT scan used for planning for this study. For abdominal patients, CT simulation was at exhale-breath hold. The hypothetically prescribed dose was 50Gy/5 fractions with goal coverage of 95% of the planned target volume (PTV) by 95% of prescription dose. PTV coverage was subject to hard OAR constraints (Table 2). Constraints were selected based on current SBRT institutional practice for thoracic and abdominal treatment sites. When necessary, dose deescalation to the PTV was performed in order to meet hard constraints with the goal of toxicity avoidance, in accordance with a strict isotoxicity approach.

#### Simulated adaptive planning

Additional daily, simulated adaptive plans (PA) were then created based on variable tumor/OAR anatomy observed on each of three subsequent MR-image sets. These MRimage sets were obtained on each patient's actual SBRT treatment days to accurately capture daily anatomic variation. All daily MR-images were prospectively obtained at free-breathing for thoracic patients and exhale-breath hold for abdominal patients. Virtual dosimetric replanning was then performed to simulate adaptive planning, using a single breath-hold MRimage for formation of  $P_A$ . If target coverage or OAR dose exceeded constraints (Table 2), re-optimization was performed using original beam angles and optimization objectives. Additionally, in cases where hard OAR constraints required dose de-escalation at expense of PTV coverage in P<sub>I</sub>, PTV dose escalation to a maximum of 60Gy was performed in P<sub>A</sub> if more favorable daily OAR anatomy was observed. Dose escalation was based on this maximum prescription dose, applied on a fraction-by-fraction basis (maximum of 12Gy per fraction) to avoid excess dose to an OAR in any individual treatment fraction. Each adaptive fraction was planned and evaluated using a target dose and OAR constraints that were scaled to 5 fractions, without dose accumulation. An adaptive plan was deemed acceptable when OAR constraint compliance was met, with a secondary objective of maximized PTV coverage/dose. For all patients, three P<sub>A</sub> were constructed for comparison to P<sub>I</sub>.

We then evaluated changes in dose delivered to tumors and OARs between traditional, nonadaptive  $P_I$  and all subsequent  $P_A$ . To do so,  $P_I$  was applied to each daily MR contour and dataset. Specifically, virtual couch correction was used for virtual patient set up to the PTV itself, with subsequent  $P_I$  application by study physicians to achieve maximal threedimensional overlap between the PTV from time of the simulation and the actual observed daily MR target anatomy. Dose for  $P_I$  was recalculated on the observed "anatomy of the day" via transfer of the electron density map from the initial CT simulation dataset to the

daily MR with deformable registration. Recalculated  $P_I$  dose was then compared to the corresponding daily  $P_A$  using side-by-side comparison of isodose distributions and dose volume histograms (DVH). Any changes in dose delivered to tumors/OARs between  $P_I$  and  $P_A$  were recorded.

#### **Evaluation parameters**

Specific changes in dose recorded included 95% PTV coverage, increase or decrease in PTV coverage with adaptive plans relative to the initial plan, violation of mean dose constraints for OARs, and the frequency and extent of violation of maximum dose to OARs according to predetermined constraints (Table 2). Frequency and extent of dose constraint violations and 95% PTV coverage were compared between  $P_I$  and  $P_A$ .

### RESULTS

#### Organ-at-risk constraints

A total of 30  $P_A$  were constructed. Hard OAR constraints were met for all  $P_I$  based on anatomy from initial CT simulation. Similarly, all  $P_A$  met hard OAR constraints based on anatomy-of-the-day from each daily MR-image set. Significant interfractional variation was observed in relationships between tumor and OAR anatomy. Figure 1 demonstrates the observed degree of interfractional shifts in the position of OARs relative to target volumes when simulation anatomy was compared to daily treatment anatomy (Fig. 1a versus 1b), and when daily treatment anatomy was compared to subsequent daily treatment anatomy (Fig. 1b versus 1c). Although all initial plans based on simulation anatomy adhered to the OAR constraints (represented by Figure 2a), when these  $P_I$  were subsequently applied to the treatment day anatomy captured by each MR-image set, violation of hard OAR constraints occurred in 19/30 cases (represented by Fig 2b). All patients had 1 fraction with 1 OAR constraint violation when  $P_I$  was applied to daily MR anatomy. By contrast, potential OAR violations were resolved by adaptive planning (representative example, Fig 2c), resulting in  $0/30 P_A$  OAR violations.

For thoracic cases, common OAR violations for application of P<sub>I</sub> to daily anatomy included the trachea (n=6) and esophagus (n=5). For abdominal cases, the most common OARs to receive excess dose via traditional non-adaptive planning were the duodenum (n=7) and stomach (n=6). Figure 2 illustrates a representative duodenal dose violation and subsequent resolution with adaptive planning. OAR violations were variable, both in terms of volume of OARs that received excess dose (Table 2) and magnitude by which constraints were exceeded (Figure 3). For example, when the duodenal dose constraint of 0.5cc 35Gy was exceeded, the range of duodenal volume treated to 35Gy was 0.9cc-12.85cc (mean 8.3cc, median 5.8cc), with maximum dose to the 0.5cc constraint volume ranging from 35.7Gy-46.6Gy. A complete summary of OAR violation type and magnitude is represented in Table 2 and Figure 3.

#### Target volume coverage

Increased PTV coverage was achieved by adaptive planning in 21/30 fractions. Dose was increased in 10/15 (66.7%) of abdominal and 11/15 (73.3%) of thoracic fractions. PTV dose

escalation relative to the initial plan occurred concurrently with reversal of 1 OAR violation in 14/21 (66%) of cases where hard OAR constraints were initially violated by application of P<sub>1</sub> to the anatomy-of-the-day. Specifically, improved PTV dose coverage was possible despite increased OAR protection in 7/11 (63%) dose-escalated thorax fractions and 8/10 (80%) dose-escalated abdominal fractions (example DVH, Figure 4a). For nine P<sub>A</sub> cases, decreased PTV coverage relative to PI was required to meet hard OAR constraints that would have otherwise been violated in a non-adaptive setting (example DVH, Figure 4b). When no OAR violation occurred by application of PI to the anatomy-of-the-day, PTV dose was increased in 9/9 (100%) of fractions. Goal 95% PTV coverage by 47.5Gy (95% prescription dose) was met in  $7/30 P_I$  and  $13/30 P_A$ . Average PTV coverage (all fractions included) for thorax cases was 88.1% at the 95% isodose line for  $P_I$  and 92.4% at the 95% isodose line for  $P_A$ . For non-liver abdomen cases planned to 50Gy, only 70.7% of the PTV was covered at the 95% isodose line by P<sub>I</sub>, with improvement to 83.4% PTV coverage, on average, by  $P_A$ . Overall, when PTV dose escalation was achievable, median dose increase (relative percentages of the initial dose covering 95% of the PTV) was 11.2% (range 2.2-52.9%).

#### DISCUSSION

We present a dosimetric analysis of potential benefits of online-adaptive MRI-guided SBRT for treatment of oligometastatic/unresectable primary disease in the central thorax and abdomen. Application of SBRT as an ablative therapy may be limited in these sites by positional uncertainty and toxicity risk. We hypothesized that online-adaptive MRI-guided SBRT might allow PTV dose escalation and/or simultaneous OAR sparing when compared to non-adaptive SBRT, and confirmed this using simulated online-adaptive planning for 10 patients under workflow and time constraints similar to our clinical MR-IGRT implementation.

Application of traditional SBRT plans to the observed daily MR anatomy resulted in numerous unplanned, potentially toxic violations of dose constraints for organs-at-risk (Figure 2b). Notably, every patient in this study had at least one normal tissue constraint violation in at least one non-adaptive fraction. Although constraint violation magnitude was variable and it is possible that low-level violations would not have resulted in clinically meaningful normal tissue toxicity, several patients' OAR doses markedly exceeded the permitted limit (Table 2, Fig. 3). It is plausible that cases with substantial variability in OAR position and delivered dose may represent the subset of patients who experienced high-grade toxicity in prior SBRT dose escalation trials—such as those observed by Timmerman et al. in the central thorax (12).

Despite high frequency of OAR constraint violations in non-adaptive fractions (61%), we demonstrated successful resolution of violations in all cases by online-adaptive planning. Resolution of normal tissue constraint violation was equally achievable in the abdomen and central thorax. Online-adaptive planning may allow daily identification of this variability, and provide opportunity to eliminate unanticipated toxicity and safely deliver dose-escalated therapy. Further data regarding clinical outcomes is required.

We also observed that adaptive planning allowed PTV dose increase relative to initial plans in a majority of patients and treatment fractions, including those where OAR violations were present following application of the initial plan. Given that our goal of coverage of 95% of the PTV at 47.5Gy (95% of prescription) is typically higher than OAR constraints that would be used in treatment sites such as the abdomen, sacrifice of PTV coverage was often necessary in initial planning due to prioritization of OAR protection. Of note, our median simulated hotspot was 120% of 50Gy (range 109–130%); we chose to limit excessive hotspots because of concerns regarding potential toxicity risk, in the context of doseescalated treatment. However, our findings suggest that online-ART may permit improved PTV dose coverage on a fraction-by-fraction basis for patients whose simulation anatomy requires a conservative plan. In fact, for most (66%) simulated fractions where adaptive planning was required for OAR protection, simultaneous dose escalation toward/beyond goal prescription of 50Gy was achievable. Dose escalation was also achieved by PA in 100% of patients whose daily anatomy was favorable and did not result in OAR violation by P<sub>I</sub>. The clinical benefits achieved by such dose escalation using this technique require future study. However, for oligometastases, disease control has been demonstrated to increase with increasing dose, approaching 100% with appropriate dose escalation (5, 9–11). Our findings indicate that MR-guided online-adaptive planning could improve local control of oligometastatic disease without increasing toxicity.

Our findings are encouraging to inform potential clinical applications of online-adaptive, MR-guided SBRT. Although the prospective dosimetric and clinical feasibility of MRguided SBRT planning and treatment have recently been demonstrated, feasibility and clinical applicability of online-adaptive planning has yet to be confirmed (25, 26). While online-adaptive planning was retrospectively simulated in this study, the process used was similar to that implemented as part of our clinical workflow, with MR imaging data that was prospectively collected. This allowed us to represent interfractional target volume motion and potential advantages of online-ART with maximum accuracy. It is possible that the impact and limitations of five-fraction OAR constraints would be partially ameliorated with use of a less-hypofractionated treatment regimen. Similarly, use of greater hotspots potentially can result in steeper dose fall-off in immediate proximity to the target. However, the principle of variable daily OAR anatomy still applies, as does the challenge of treating tumors adjacent to critical OARs (27). Similarly, calculation of true dose accumulation to organs-at-risk is not presently available with our treatment planning process. We recognize that the absence of dose accumulation in the context of an isotoxicity dose escalation approach may cause overestimation of the impact of observed changes in anatomy on OAR dose. Although dose deformation and accumulation is of future research interest at our institution, we have clinically implemented the isotoxicity approach presented here, recognizing it as a conservative approach in order to minimize complication risk. Additionally, we recognize as a limitation that some observed differences in anatomy from simulation to time of treatment in this study may be attributable to differences in CT versus MR-image set data. However, given that very high-dose fractions of radiation are delivered with SBRT, even small changes in daily anatomy risk significant underdosage of portions of the tumor by up to 20% and inadvertent overdose of OARs, creating risk of patient injury. Importantly, significant interfractional motion was also demonstrated between sequential

MR datasets (Fig 1). These findings are consistent with previous reports of interfractional organ motion and deformation where imaging modality remained consistent both from time of simulation to time of treatment delivery and between fractions(20). Given limitations of comparison across image modalities, MR-only planning is of future interest to minimize this potential bias. Finally, although ART may require additional time for physicians, physicists, therapists, and patients, our institution has implemented online-adaptive IMRT planning within an acceptable clinical time frame (median institutional time of 26 minutes for recontouring, reoptimization, and QA) (24). Our online-adaptive workflow for IMRT is identical to that used for online-adaptive SBRT, and thus online-adaptive SBRT should be similarly feasible. Overall, we demonstrate here that online-adaptive SBRT is likely to achieve significant dosimetric gains. However, prospective evaluation of online-ART is needed for dosimetric validation, to evaluate time required to deliver online-ART in real-time, and to evaluate if dosimetric gains translate into clinical benefit.

Future directions include the ongoing clinical implementation of real-time, online-adaptive MR-guided SBRT at our institution (28) and MR-only treatment planning. Based on this encouraging dosimetric study, we opened a prospective study evaluating use of this technique to treat oligometastatic or unresectable primary disease of the abdomen and central thorax. Data collected will be used to evaluate a primary endpoint of clinical feasibility/timing, with secondary endpoints including tumor response rate, survival, and quality of life metrics.

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#### Summary

In this study, potential dosimetric gains from daily online adaptive SBRT for central thoracic and abdominal applications were characterized. Initial CT-simulation plans were applied to MR localization images, with evaluation and reoptimization based on variable anatomy. We found a significant incidence of OAR constraint violation by application of the initial plan to localization images. Online adaptive planning resolved all potential OAR violations, and allowed dose escalation in a majority of patients and fractions. Our findings suggest that this method could improve the therapeutic ratio for SBRT of central thoracic and abdominal malignancies.



#### Figure 1.

Patient anatomy at simulation (1a, 1d) compared with "anatomy-of-the-day" revealed by the MR-image set at fraction one (1b, 1e) versus "anatomy-of-the-day" revealed by MR imaging at fraction two (1c, 1f). In frames 1a–1c, large interfractional shifts occur in the position of the stomach (S) relative to the adrenal tumor (T). Similarly, in a separate patient (frames 1d to 1f), interfractional variability in esophageal position (E) relative to a paraaortic lymph node tumor (T) was observed.



#### Figure 2.

Computed tomography (CT)-based, non-adaptive  $P_I$  met all organ-at-risk (OAR) constraints based on anatomy from initial CT simulation (2a). Application of  $P_I$  to the daily MR-image set of a patient with a pancreatic tumor (blue colorwash) resulted in violation of hard duodenal constraints (2b). Daily adaptive planning achieved resolution of the OAR constraint violation to the duodenum (marked with arrows) while preserving target volume coverage (2c).



#### Figure 3.

Maximum point dose delivered to constraint volumes of organs-at risk (OARs) when initial non-adaptive plans were applied to daily anatomy.



#### Figure 4.

Dose-volume histograms (DVH) comparing esophageal (4a), stomach (4b), and planning target volume (PTV, 4a and 4b) dose for initial simulation plans based on simulation anatomy, non-adaptive plans applied to daily anatomy, and daily adaptive plans. In 4a, esophageal protection occurred concurrently with PTV dose escalation. In 4b, dose de-escalation to the PTV was required to meet hard stomach constraints.

#### Table 1

#### Patient and tumor characteristics

Disease site		
Central thorax	5	
Inoperable hilar non-small cell lung cancer	2	
Mediastinal lymph node	2	
Peri-hilar lymph node	1	
Abdomen	5	
Adrenal mass	1	
Extra-hepatic cholangiocarcinoma	1	
Internal iliac lymph node	1	
Inoperable pancreas adenocarcinoma	2	
Median age (range)	70 (48–81)	
Median tumor size in cm (range)	3.4 (0.8-8.0)	

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Hard Dose Constraints for Initial and Adaptive Plans, with Recorded Organ-at-risk Violation Metrics for Application of Non-adaptive Plans (P1) to MR Localization Images

Henke et al.

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			Degree	e of Violatic	u				Degre	e of Violati	u
Abdominal OAR	Constraint	# of PI constraint violations	Mean (Std Dev)	Median	Range	Thorax OAR	Constraint	# of PI constraint violations	Mean (Std Dev)	Median	Range
Uninvolved liver (liver - GTV)	700cc < 20 Gy	1	NA	NA	NA	Lungs (combined)	V12.5Gy 1500 cc	0	ΥN	ΥN	NA
	V25Gy < 33%	0	NA	NA	NA		V13.5Gy 1000 cc	0	ΥN	ΝA	NA
	$Mean < 20 \; Gy$	1	1 Gy	1 Gy	1 Gy	Esophagus max	V32Gy 0.5 cc	5	$1.5\pm0.9cc$	1.6 cc	0.3–2.8 cc
Duodenum max	V35Gy < 0.5 cc	7	$5.7 \pm 4.6 \text{ cc}$	5.3 сс	0.4–12.4 cc	Heart/Pericardium	V32Gy 15 cc	1	0.4 cc	0.4 cc	0.4 cc
Stomach max	V33Gy < 0.5 cc	9	$8.7 \pm 14.9 \text{ cc}$	3.7 сс	0.5-38.9 сс	Great vessels, non- adjacent wall	V47Gy < 10 cc	0	ΥN	ΥN	NA
Small bowel max	V30Gy 0.5 cc	2	$1.6\pm0.4$ cc	1.57 cc	1.26–1.88 cc						
Large bowel max	V35Gy 0.5 cc	2	$0.2 \pm 0.3 \text{ cc}$	0.24 cc	0.04-0.44cc	Trachea and ipsilateral	V10Gy < 0.2 cc	9	$0.5\pm0.4cc$	0.4 cc	0.08–1.05 cc
Cord	V25Gy < 0.5cc	0	NA	NA	NA	broncnus, non- adjacent wall					
Kidney (combined)	$Mean < 18 \; Gy$	0	NA	NA	NA	Cord	V8Gy < 1 cc	0	NA	NA	NA

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