



Articular cartilage tissue engineering: the role of signaling molecules

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Abstract Effective early disease modifying options for osteoarthritis remain lacking. Tissue engineering approach to generate cartilage in vitro has emerged as a promising option for articular cartilage repair and regeneration. Signaling molecules and matrix modifying agents, derived from knowledge of cartilage development and homeostasis, have been used as biochemical stimuli toward cartilage tissue engineering and have led to improvements in the functionality of engineered cartilage. Clinical translation of neocartilage faces challenges, such as phenotypic instability of the engineered cartilage, poor integration, inflammation, and catabolic factors in the arthritic environment; these can all contribute to failure of implanted neocartilage. A comprehensive understanding of signaling molecules involved in osteoarthritis pathogenesis and their actions on engineered cartilage will be crucial. Thus, while it is important to continue deriving inspiration from cartilage development and homeostasis, it has become increasingly necessary to incorporate knowledge from osteoarthritis pathogenesis into cartilage tissue engineering.

Keywords Articular cartilage · Tissue engineering · Osteoarthritis · Signaling molecules · Cartilage development

Introduction

Arthritis is a debilitating disease that currently affects more than 50 million of US adults; this number is projected to rise to ~67 million by 2030 [1–3]. Characterized by the destruction of joint cartilage, osteoarthritis is the most common type of arthritis. Changes in biomechanical characteristics of articular cartilage and chondrocyte metabolism, which are often associated with aging or injury, lead to matrix degradation, causing severe pain and disability. Due to the limited intrinsic regenerative capacity of articular cartilage, surgical and conservative therapies have been employed in attempts at tissue restoration and to relieve pain [4–6]. However, current treatment modalities are insufficient to modify the disease as they give poor long-term outcomes. Effective therapeutic options for osteoarthritis remain lacking despite its prevalence.

Tissue engineering has emerged as a promising treatment option for articular cartilage repair. Engineering cartilage tissue often involves the fabrication of three-dimensional (3D) tissues in vitro by seeding cells into scaffolds in the presence of biochemical and biomechanical stimuli. Scaffold-free cultures have also been investigated in tissue engineering to minimize the adverse effects of scaffold degradation and alternations in cell phenotype [7–9]. The goal is to replace articular cartilage defects in the patient with neocartilage formed in vitro to restore function. A variety of cell sources, including stem cells and primary cells, natural or synthetic scaffold materials, signaling molecules, and mechanical stimuli have been explored to improve biological and biomechanical functions of engineered cartilage.

Signaling molecules play major roles in modulating cell to cell signaling and cellular activities within developing and mature articular cartilage. Several growth and

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transcription factors that are involved in cartilage development and homeostasis have been examined in the application of cartilage tissue engineering. Transforming growth factor- β (TGF β) subfamily members, bone morphogenetic proteins (BMPs), insulin-like growth factors (IGFs), fibroblast growth factors (FGFs), and sex determining region Y (SRY)-box (SOXs) are common molecules used to induce chondrogenesis *in vitro*. The role of these signaling molecules in engineering cartilage as biochemical stimuli and the signal transduction pathways involved have been well characterized in past years, signifying the importance of repurposing cues seen in cartilage development toward cartilage tissue engineering.

Successful cartilage tissue engineering relies not only on the functionality of the engineered articular cartilage to mimic properties of native tissue, but also on the clinical applicability of such tissue. Using soluble signals derived from our knowledge of cartilage development has led to significant strides in engineering cartilage, resulting in the maintenance of the cartilage phenotype *in vitro* and the production of cartilaginous matrices (Fig. 1). Despite this, the clinical translation of engineered cartilage continues to face challenges. Engineered tissues with insufficient mechanical properties that do not replicate the properties of native tissue, phenotypic instability after implantation, and poor integration into surrounding native tissue remain major challenges. In addition, inflammation in the degenerative joint is another barrier to overcome for successful cartilage repair in the clinical setting. To resolve these challenges, it has become increasingly important for clinicians and researchers to derive insight not only from cartilage development, but also from cartilage homeostasis, repair, and degenerative processes, and to apply such new-found knowledge toward the clinical translation of engineered cartilage (Fig. 1). In short, a continuum of states can be observed for articular cartilage *in vivo*, ranging from a

mostly anabolic development phase to a mostly catabolic disease phase. Inspiration can be drawn from each state toward implementing engineering replacements.

This review discusses the significant role of signaling molecules in engineering articular cartilage while placing them in the context of chondrogenesis during development. Special focus is placed on signaling molecules involved in differentiation and cartilaginous matrix production, such as TGF- β s, BMPs, IGFs, FGFs, and SOXs. Additionally, the role of biophysical agents, such as chondroitinase, that break down articular cartilage, is discussed to note how these, too, can have a role in engineering cartilage. Molecules that have shown potential for improving stability and integration of engineered cartilage, and for resisting inflammation, are also discussed.

Signaling molecules in chondrogenesis during cartilage development

Chondrogenesis, the process by which cartilage is formed, involves a plethora of different signaling pathways. Through a process termed condensation, undifferentiated mesenchymal stem cells (MSCs) derived from the lateral plate mesoderm migrate to the limb field region and aggregate [10] (Fig. 2). The process of condensation, regulated by cell–cell and cell–matrix interactions, is critical for chondrocyte differentiation [11]. Stem cells in the condensation differentiate into chondrocytes that produce an abundance of extracellular matrix (ECM) (e.g., proteoglycans and collagen types II, IX, and XI) [12], forming the cartilaginous anlage. During the process known as endochondral ossification, chondrocytes in the center of the condensation zone become hypertrophic, producing type X collagen [10, 12]. This is followed by interzone initiation and formation of the epiphyseal ossification center, which defines the developing joint. Subsequently, the cells at the edge of the cartilaginous anlage form the articular cartilage. For a more detailed description, please see Ref. [13].

Various signals are involved in regulating the processes of chondrogenesis and hypertrophy. The roles of growth and transcription factors range from modulating the chondrocytic phenotype to stimulating cartilage matrix production. As discussed below, knowledge of signaling molecules ubiquitous in cartilage development has been the inspiration for many advances in cartilage tissue engineering. In order to provide a background of how signaling molecules are used in tissue engineering, their roles during chondrogenesis and chondrocyte hypertrophy are described below. Further details on signaling pathways involved in development and maintenance of articular cartilage can be found elsewhere [13].

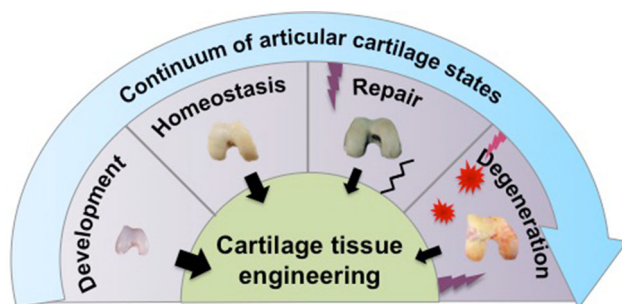


Fig. 1 Cartilage tissue engineering inspired by the states of articular cartilage *in vivo*. From cartilage development, a mostly anabolic phase, to degeneration, a mostly catabolic phase, inspiration drawn from each state has led to many advances in cartilage tissue engineering

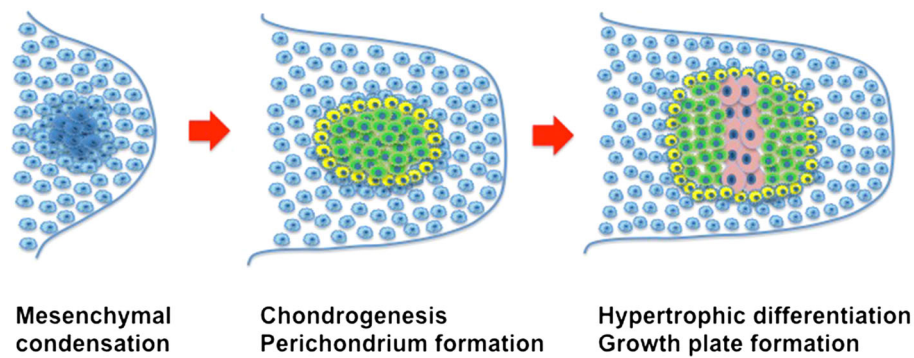


Fig. 2 Formation of the cartilage anlage during development. During the mesenchymal condensation phase, mesenchymal cells (*blue*) condense. Subsequently, during the chondrogenesis phase the cells differentiate into chondrocytes (*green*). Perichondrium cells are also

formed (*yellow*). During the hypertrophic differentiation phase, chondrocytes in the central zone undergo hypertrophy (*pink*) to initiate the formation of the growth plate

Transforming growth factor-beta (TGF- β) superfamily

The members of the TGF- β superfamily consist of various ligands including activin/inhibin, TGF- β s, BMPs, and growth and differentiation factors (GDFs). Members of the TGF- β superfamily bind to type I and II receptors to activate downstream signaling pathways that are involved in development and homeostasis of a variety of tissues [14]. They are widely expressed in chondrocytes and play a crucial role in the process of chondrogenesis as well as maintenance of cartilage homeostasis.

TGF- β

TGF- β s are representative proteins involved in cartilage development. TGF- β signals are transduced through type II receptors, which recruit and phosphorylate type I receptors, resulting in activation of Smad proteins, Smad2 and 3. The phosphorylated Smad proteins interact with co-Smad (Smad4) to translocate to the nucleus, activating target gene expression [15]. Studies have shown that TGF- β signaling during chondrogenesis and chondrocyte maturation is mediated predominantly by Smad3 rather than Smad2 [16, 17]. TGF- β can also activate mitogen-activated protein (MAP) kinase pathways, extracellular signal-regulated kinase (ERK) and p38 to regulate chondrogenesis [18]. TGF- β isoforms, TGF- β 1, TGF- β 2, and TGF- β 3, are found in the perichondrium and periosteum, a fibrous cell layer derived from cells at the periphery of the mesenchymal condensation, as well as in the hypertrophic cartilage in the growth plate. TGF- β 1 and TGF- β 2 expression persists in adult articular cartilage, suggesting their involvement not only in the development but also in the maintenance of articular cartilage [19].

TGF- β s are important in all stages of chondrogenesis, including mesenchymal condensation, chondrocyte proliferation, ECM production, and terminal differentiation. During the first phase of condensation, MSCs express adhesion molecules to promote cell interactions. TGF- β s 1–3 are involved in the synthesis of adhesion molecules including N-cadherin and N-CAM, as well as ECM proteins such as fibronectin and tenascin to which the cells bind [20]. MAP kinases, ERK, p38, and c-Jun N-terminal kinase (JNK), as well as Wingless-Int (Wnt) signaling are involved in the modulation of N-cadherin expression mediated by TGF- β in mesenchymal progenitor cells [21]. Blocking of the adhesion molecules and ECM proteins disrupts cartilage differentiation both in vitro and in vivo by inhibiting condensation [22–24]. In addition to the role in condensation, TGF- β stimulates cell proliferation and synthesis of cartilage matrix such as glycosaminoglycans (GAG) as well as expression of cartilage-specific genes such as aggrecan and type II collagen [25, 26]. TGF- β -activated Smad3/4 has been shown to stimulate SOX-9-mediated transcription; this involves the association of SOX-9 with the activated Smad3 and p300, a transcriptional co-activator, and their binding to the enhancer region of type II collagen gene [27]. Thus, TGF- β s contribute as stimulators in chondrogenesis, and their interaction with other signaling molecules modulates the chondrogenesis.

While TGF- β s have stimulatory effects in the early stages of chondrogenesis, they act as inhibitors in the later stages of chondrocyte differentiation. TGF- β inhibits differentiation into hypertrophic chondrocytes by inhibiting expression of type X collagen, matrix metalloproteinase 13 (MMP-13), vascular endothelial growth factor (VEGF), and osteocalcin [28]. Smad2/3 signaling mediates the inhibitory effect of TGF- β and is essential in inhibiting further progression into hypertrophy [16]. A study using homozygous mice with a targeted disruption of Smad3 has

shown abnormally increased numbers of hypertrophic chondrocytes, suggesting the essential role of Smad signaling in suppressing chondrocyte terminal differentiation by TGF- β [29]. Furthermore, Smad3 activated by TGF- β interacts with runt-related transcription factor-2 (RUNX-2), a transcription factor involved in chondrocyte maturation and osteoblast differentiation [30], to inhibit RUNX-2 function [31]. The dual role of TGF- β signaling pathways in regulating chondrogenesis and hypertrophic differentiation, as well as controlling their levels at certain stages of development, may largely affect cartilage formation.

Bone morphogenetic protein (BMP)

Bone morphogenetic proteins are heavily involved in multiple stages of skeletal development. They play crucial roles in chondrogenesis and osteogenesis *in vivo*, including the commitment of mesenchymal cells to the chondrogenic lineage, induction of cell proliferation and maturation in the growth plates, and formation of joints and bones [19]. TGF- β s and BMPs are modulated by distinctly different signaling pathways to influence chondrogenesis, although these two categories of growth factors are members of the TGF- β superfamily. TGF- β signaling is mediated by Smad2/3, whereas Smad1/5/8 are responsible for transducing BMP signaling [15]. BMP-induced chondrogenesis has been shown to involve the p38 MAP kinase pathway [32].

The function of BMP signaling during chondrogenesis is mediated by the SOX family. Among the SOX family, SOX-9, L-SOX-5, and SOX-6 are well studied transcription factors involved in chondrogenesis. BMP induces expression of SOX-9, which acts downstream of BMP signaling to stimulate expression of cartilage markers [33]. Similarly, SOX-6 has been shown to be induced by BMP in a time-dependent manner; the binding of the SOX-6 to the type II collagen gene enhancer was increased with BMP treatment, indicating an important role of SOX-6 in mediating BMP signaling in chondrogenesis [34]. In addition, BMP signaling is essential for maintenance of SOX protein expression as demonstrated by a study where expressions of SOX-9, L-SOX-5, and SOX-6 were abolished during condensation in mice carrying double mutants of BMP receptor type 1A (BMPRI1A) and 1B, where BMPs bind to transduce their signals [35]. Enhanced BMP-induced chondrogenic differentiation by overexpression of SOX-9, and synergistic effects on chondrocyte condensation and proliferation by both SOX-9 and BMP *in ex vivo* limb culture were reported [36]. Taken together, the relationship between BMP signaling and SOX expression is a key regulator of chondrogenesis.

In addition to the role in the early stages of chondrogenesis, BMPs reveal their roles in later stages in the

growth plates by promoting chondrocyte proliferation and hypertrophy [19]. Addition of BMP increased longitudinal growth of metatarsal bone and stimulated chondrocyte proliferation and hypertrophy in the growth plate, while addition of noggin, an antagonist for BMP signaling, resulted in blocking these effects [37]. Transgenic mice expressing BMP under the control of the $\alpha 2$ (XI) collagen gene promoter/enhancer had an enlarged area of hypertrophic zone; this was possibly due to enhanced hypertrophic differentiation of chondrocytes [38]. Instead of mature hypertrophic chondrocytes, immature chondrocytes were observed in noggin over-expressing mice [38]. As noggin is also expressed during cartilage development, the level and function of BMP may be regulated by the action of its antagonist during the development of the growth plate cartilage.

Multiple BMP ligands including BMP-2, -4, -7, and GDF-5 have been shown to play roles during chondrogenesis and in the growth plate. BMP-2 is essential in the condensation process of MSCs and stimulates the synthesis of cartilage matrix proteins [19]. It also induces hypertrophic differentiation of proliferating chondrocytes in the growth plate by stimulating type X collagen. BMP-2-stimulated Smad1/5 in association with RUNX-2 has been shown to stimulate transcription of type X collagen expression gene to regulate chondrocyte hypertrophy [39]. Similarly, BMP-4 promotes cartilage matrix production by increasing type II collagen and aggrecan expression. However, BMP-4 suppresses expression of type X collagen, thus preventing chondrocyte hypertrophy [40]. BMP-7 is synthesized by proliferating chondrocytes present near the perichondrium [19]. In the presence of BMP-7, MSCs decrease their proliferative ability but increase the synthesis of cartilage matrix proteins [41]. BMP-7 exhibits not only anabolic activity, but also anti-catabolic activity such as expression inhibition of matrix proteases and cytokines [42]. GDF-5, also known as BMP-14, is expressed in the early condensation phase, while it is also involved in stimulating joint formation [43]. GDF-5 has been shown to stimulate survival of mesenchymal cells and maturation of chondrocytes [44, 45]. Different BMP isoforms display similar as well as distinct roles, and thus their involvement during cartilage development in terms of levels and phases is different.

SRY (sex determining region Y)-box (SOX)

Among many transcription factors involved in cartilage development, SOX-9 is a key molecule that regulates chondrocyte differentiation and cartilage formation. It encodes a high mobility group DNA binding domain and associates with the SOX-9 binding sites on promoters/enhancers of cartilage specific genes such as type II, IX, and XI collagens, and aggrecan [46]. SOX-9 is necessary in the

condensation phase of MSCs during chondrogenesis. Cells that express SOX-9 undergo aggregation and start differentiating into the chondrocyte lineage [12]. Loss of SOX-9 in limb buds resulted in disruption of the mesenchyme condensation and no cartilage and bone formation [47]. The essential roles of SOX-9 after mesenchymal condensation on chondrocyte differentiation have also been demonstrated; inactivation of SOX-9 after condensation phase led to severe chondrodysplasia, inhibited chondrocyte proliferation, and induced defects in joint formation [47].

SOX-9 induces and is necessary for the expression of SOX-5 and SOX-6. SOX-5 and 6 are also known transcription factors that guide MSCs into the chondrogenic lineage. These stimulate type II, IX, and XI collagens and aggrecan by cooperating with SOX-9 [48, 49]. The activation of SOX-5 and 6 is needed for chondroprogenitor cells expressing SOX-9 to undergo appropriate chondrogenic differentiation. In the absence of SOX-5 and 6, chondroprogenitors shift their fate toward tendon and ligament lineage by expressing scleraxis (SCX), a tendon and ligament transcription factor [50]. Mutation of either or both genes results in mild skeletal defects and chondrodysplasia, respectively [49]. Thus, the interplay between SOX-5/6 and SOX-9 plays a key role in chondrogenesis.

In addition to its role in promoting chondrogenesis, SOX-9 is also involved in the process of endochondral ossification. Loss of SOX-9 resulted in the maturation of immature chondrocytes into hypertrophic cells while overexpression of SOX-9 decelerates the processes of chondrocyte hypertrophy in immature chondrocytes [51, 52]. SOX-9 has been shown to block the activity of RUNX-2 and to suppress genes such as type X collagen and VEGF-A, expressed by hypertrophic chondrocytes [53–55], suggesting the multiple roles of SOX-9 not only during chondrogenesis but also in the growth plate.

SOX-9 expression is modulated by several transcription and growth factors [46]. Sonic hedgehog, a molecule involved in patterning of the anterior–posterior limb axis, as well as hypoxia-inducible factor 1 α , a positive regulator of chondrogenesis, have been shown to enhance the promoter activity of SOX-9 and increase its expression [46]. TGF- β and BMP-2 signals, and FGF-1/2 and IGF-1 are also involved in upregulating the expression of SOX-9 [46]. Thus, SOX-9 can be controlled by or interact with signaling pathways activated by other molecules to regulate cartilage development.

Insulin-like growth factor (IGF)

As with the factors discussed above, IGF also plays multiple roles in cartilage development. IGF is a key

component for mesenchymal differentiation toward chondrocytes and also in the subsequent stages of development, such as the synthesis of cartilaginous matrix. In addition, IGF is involved in the chondrogenesis of mesenchymal cells as well as the maintenance and survival of differentiated articular chondrocytes via a phosphoinositide 3-kinase (PI3K) pathway, involving ERK, p38 kinase, and protein kinase C (PKC) signaling [56]. Further, it was demonstrated that IGF has a pivotal role in the relationship between chondrogenesis and osteogenesis.

IGF-1 is a regulatory factor in the process of chondrogenesis from MSCs. Both IGF isoforms, IGF-1 and IGF-2, have been shown to promote clonal growth of human adult and fetal chondrocytes, respectively [57, 58]. Specifically, IGF-1 was shown to induce cell proliferation in MSC pellets and promoted the expression of chondrogenic markers, such as type II collagen and SOX-9 [59]. IGF appears to act independently during chondrogenic differentiation of MSCs, but its actions can be enhanced when acting in conjunction with TGF- β or BMP-2 [12, 59]. IGF has proven to be a critical factor for chondrocyte proliferation during the early phases of chondrogenesis [12]. IGF-1 mediates type II collagen synthesis mainly via the increased binding of SOX-9 and specificity protein (Sp1)/Sp3 to their *cis* elements in the intron-specific enhancer region of type II collagen gene, and this involves a physical interaction with p300 [60].

Apart from chondrogenesis, IGF was proven to play a key role in hypertrophic maturation of chondrocytes. Recently, the dogma that considers chondrocytes and osteoblasts as entirely independent lineages derived from a common progenitor [61] came into question when hypertrophic chondrocytes were observed to have the ability to become osteoblasts and osteocytes during endochondral bone formation and during bone repair [62]. The strategic role of IGF as a regulator of the above processes was confirmed by the presence of specific cellular patterns of gene expression for the IGF system during both chondro- and osteogenesis [63]. Furthermore, mRNAs of IGF receptors (IGF-1R and IGF-2R) are expressed in great amounts in hypertrophic chondrocytes. The role of IGF in both mature chondrocytes and osteoblasts has been confirmed by similar actions of IGF and IGF receptors to growth plate chondrocytes. Specifically, IGF is a critical component of chondrocyte proliferation in growth plate [12]. In an *in vitro* study using embryonic and postnatal growth plate chondrocytes isolated from a IGF-1R gene knockout mice, the absence of IGF-1R was associated with suppressed cell proliferation and promoted apoptosis via increased PTHrP expression [64]. Thus, IGF has manifold functions not only during the early phases of chondrogenesis but also in hypertrophy and matrix synthesis.

Fibroblastic growth factor (FGF)

Fibroblastic growth factors represent a family of 22 structurally related proteins that share common biochemical and functional properties [65]. The role of FGF signaling in skeletal development has been revealed from the discovery that a point mutation in the transmembrane domain of FGF receptor (FGFR) 3 is responsible for achondroplasia, the most common genetic form of dwarfism in humans. Subsequently, it was discovered that two major groups of skeletal developmental disorders were associated etiologically with specific mutations in the genes encoding FGFRs 1, 2, and 3: (1) the dwarfing chondrodysplasia syndromes, such as hypochondroplasia [66] and achondroplasia [67, 68] and (2) the craniosynostosis syndromes, such as Apert syndrome [69], Crouzon syndrome [70–72], and Pfeiffer syndrome [72, 73].

For the early chondrogenesis stages, FGFR expression is critical for further limb development. Signaling from mesenchymally expressed FGF-10 to FGFR2b is important for the formation of the apical ectodermal ridge. Afterwards, FGF-8 is expressed in the apical ectodermal ridge and initiates a type of reciprocal signaling to FGFR1c in the limb mesoderm [74]. During the mesenchymal condensation phase, FGFR2 is expressed in the ectoderm of the condensing mesenchyme, and FGFR1 is expressed in the periphery of the mesenchymal condensation [74]. Despite the fact that FGF-2 is the most common growth factor used in cartilage tissue engineering, its exact role during chondrogenesis remains unclear. This may be due to its indirect regulatory action during chondrogenesis, as it has been shown that FGF-2 inactivates signaling pathways involving IGF-1 and TGF- β [75].

During chondrogenesis, FGFR3 expression begins as chondrocytes differentiate and proliferate. Other FGF family members also contribute to chondrogenesis. [76, 77]. Specifically, FGF-1, FGF-2, and FGF-7 have been shown to enhance SOX-9 expression via a MAP kinase, ERK1/2 pathway in mouse primary costal chondrocytes [78]. Further, in C3H10T1/2 cells, which are murine mesenchymal progenitor cells, members of the FGF family were able to induce their differentiation toward chondrocytes [78]. FGFR3/FGF-18 interaction suppressed cellular proliferation and promoted limb mesenchymal cell differentiation [79]. In later stages of chondrogenesis, different members of the FGF family are expressed, such as FGF-9, -10, -18, together with FGF-1, -2 and -3 as stated above [74]. FGF-8's central role in chondrogenesis was confirmed by the central regulatory effect of FGF-8 in heterotopic ossification, a type of endochondral ossification [80]. FGF family acts via tyrosine kinase receptors, and their activations leads to mitogenic response in various cell types including chondrocytes [81].

During chondrocyte hypertrophy, both FGF and FGFRs play major roles. Specifically, in both pre-hypertrophic and hypertrophic chondrocytes, FGFR1 is expressed, and it may contribute to the maintenance of hypertrophy and survival of hypertrophic chondrocytes [74, 76, 82]. FGFR3 was also expressed in hypertrophic chondrocytes [65, 74, 83]. Interestingly, FGFR1 and 3 seem to be expressed in different subpopulations of hypertrophic chondrocytes with minimum overlap [74, 83]. FGFR1 was expressed initially in chondrocytes originating from mesenchymal condensation, but, subsequently, it is expressed mainly in chondrocytes in the peripheral mineralized zones and in the adjacent osteoblasts, suggesting a potential role in hypertrophy and in osteoblastic differentiation [74, 83]. In contrast, FGFR3 is mainly expressed in proliferating chondrocytes, which implies a regulatory role in chondrocyte proliferation [83]. FGF-18 has been found to regulate early chondrocyte proliferation and differentiation through FGFR3 signaling [84]. Interestingly, FGF-9 also has a potential role in chondrocyte proliferation and hypertrophy. As demonstrated in mice that lack FGF-9 expression, the dearth of an adequate number of chondrocytes undergoing hypertrophy was responsible for a delay in type X collagen expression and simultaneous maintenance of type II collagen [85]. Despite the fact that several FGF ligands are involved in all stages of chondrogenesis, only FGF-9 and FGF-18 have been recognized so far as active molecules during the cartilage hypertrophy stage.

Several signaling pathways involving FGF have been shown to interact during chondrogenesis. Recently, it was demonstrated that FGF, TGF- β , and Wnt protein families control different differentiation stages during chondrogenesis via the presence of a signaling crosstalk [86]. FGFs increase the level of SOX-9 expression and enhance the activity of SOX-9-dependent-chondrocyte-specific enhancer elements in the gene for type II collagen [78]. From all these examples, it becomes obvious that multiple signaling factors interact in a well-balanced manner to promote chondrogenesis; better understanding of the processes that occur during cartilage development would further enrich applicable knowledge in tissue engineering.

Signaling molecules for cartilage tissue engineering

Cell sources and biochemical/biomechanical stimuli represent two of the main elements of cartilage tissue engineering. Articular chondrocytes, adult stem cells, embryonic stem cells (ESCs), and induced pluripotent stem cells (iPSCs) are all promising cell sources for articular cartilage repair and regeneration. The ability for the cells to differentiate into and maintain the chondrogenic phenotype

is largely affected by biochemical and biomechanical stimuli (Fig. 3). A variety of signaling molecules have been applied in cartilage tissue engineering to trigger chondrogenic differentiation and to stimulate synthesis of cartilage-specific matrix. To address the role of signaling molecules in a variety of cell types used in cartilage tissue engineering, the following sub-sections review (1) signaling factors used in expansion and differentiation of each cell type, and (2) biochemical molecules and biophysical agents employed for the improvement of biomechanical properties of engineered articular cartilage, including corresponding ECM components.

Signaling molecules for expansion and differentiation of different cell types

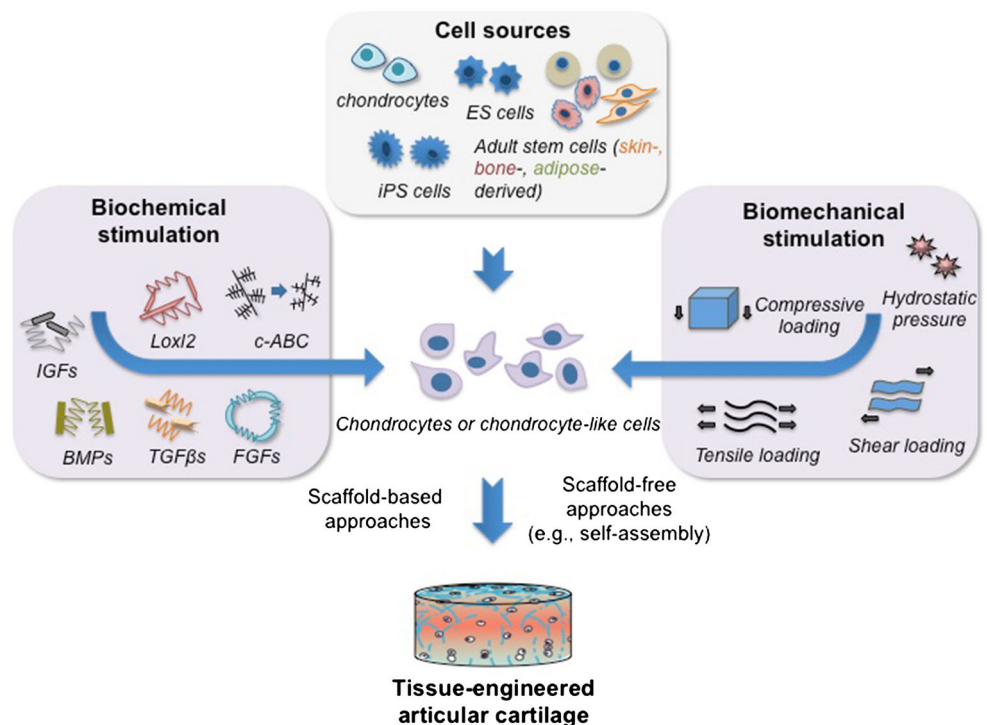
Chondrocytes

Articular chondrocytes (e.g., autologous articular chondrocytes) are already used clinically to repair cartilage defects. However, due to the limited availability of donor tissue, obtaining a sufficient amount of cells for clinical application is challenging. Expansion of articular chondrocytes in monolayer causes dedifferentiation with increased type I collagen expression and potential loss of ability to revert to a chondrogenic phenotype.

The use of growth factors and their effects on 2D and 3D cultures (e.g., alginate beads, micromass, pellet, and scaffolds) have been investigated to improve the proliferative

capacity and to restore the chondrogenic potential of articular chondrocytes. FGF-2 has shown to increase cell proliferation and to reduce apoptosis in human articular chondrocytes in monolayer, while it decreased the amount of type II collagen and aggrecan [87]. A combination of IGF-1 and BMP-7 has been shown to promote cell viability, cell proliferation, and matrix synthesis in both normal and osteoarthritic human articular chondrocytes in alginate beads in vitro [88]. When combined with IGF-1 and BMP-7, FGF-2 significantly stimulated cell proliferation in human articular chondrocytes cultured in alginate beads. However, a high dose, 100 ng/ml of FGF-2 as compared to 1 ng/ml, decreased proteoglycan levels and inhibited the ability of IGF-1 and BMP-7 to stimulate proteoglycan production [89]. A synergistic effect on the expression of type II collagen and aggrecan was also observed for TGF- β 2 and IGF-1 when human articular chondrocytes were cultured in alginate beads [90]. BMP-2 sustained expression of type II collagen and increased aggrecan in chondrocytes cultured in monolayer [91, 92], though no distinct changes in matrix production occurred when BMP-2 was applied in aggregate and pellet cultures [93]. Dedifferentiated rabbit articular chondrocytes, transduced with adenovirus expressing BMP-4, recovered their chondrogenic phenotype both in monolayer and in pellet cultures [94]. In vitro expansion of human articular chondrocytes in monolayer with a combination of TGF- β 1 and FGF-2 has been shown to promote cell proliferation and express abundant cartilage matrix protein when

Fig. 3 Articular cartilage tissue engineering. Engineering cartilage tissue often involves the formation of three-dimensional (3D) tissues in vitro by seeding chondrocytes or chondrocyte-like cells into scaffolds or through scaffold-free approaches in the presence of biochemical and biomechanical stimuli. A variety of cell sources, signaling molecules, and mechanical stimuli has been explored for cartilage tissue engineering



redifferentiated in pellets [95]. Cell expansion with TGF- β 1, FGF-2, and platelet-derived growth factor (PDGF)-bb, followed by a combination of TGF- β 1, GDF-5, and BMP-2 during post expansion in human articular chondrocytes, resulted in heightened expression of chondrogenic genes and cartilage-specific matrix synthesis [96]. Culturing human articular chondrocytes with TGF- β 2 in hypoxic conditions prominently elevated expression of type II collagen when compared to a condition without TGF- β 2 [97]. Interestingly, hypoxic conditions and 3D environment, provided by methoxypolyethyleneglycol-block-co-poly (50:50 lactide-co-glycolide) (MPEG-PLGA) scaffold, resulted in higher expression of cartilage-specific genes, including SOX-9, aggrecan, and type II collagen in human articular chondrocytes when compared to hypoxic conditions in monolayer culture [98].

Taken together, the effects of growth factors known to play key roles in cartilage development, either alone or in combination, have been investigated for maintenance of the chondrogenic phenotype and for promoting cartilage formation *in vitro*. The effects of these growth factors on chondrocytes are dependent on both concentration and the presence of other growth factors. In addition, the effect of hypoxia on chondrogenic phenotype is also to be considered. Importantly, 2D versus 3D culture greatly influences cellular response. It is still unclear if the activity of growth factors used *in vitro* will persist after orthotopic implantation *in vivo*. Comprehensive understanding of the function of growth factors with respect to time, dose, and dosing regimen is critical for the clinical application of chondrocytes.

Adult mesenchymal stem cells

Mesenchymal stem cells constitute an alternative cell source in cartilage tissue engineering. A variety of adult tissues such as bone marrow, fat tissue, skeletal muscle, and skin are sources of MSCs. Due to their abundant proliferative capacity and multiple lineage differentiation potential, much attention has been paid to MSCs as an effective source of chondrocytes for cartilage repair. The most commonly used adult stem cells for cartilage tissue engineering are MSCs derived from bone marrow, adipose, and synovium.

TGF- β 1 and TGF- β 3 are the main chondrogenic inducers used for MSCs. In addition, BMPs, FGF-2, and IGF-1 have been studied on promoting chondrogenic differentiation of MSCs *in vitro*. FGF-2 treatment during *in vitro* expansion enhanced cell proliferation in monolayer and promoted chondrogenesis in both synovium and bone marrow-derived MSCs [99, 100]. Adipose-derived MSCs treated with FGF-2 followed by chondrogenesis in the presence of TGF- β 1 significantly increased cartilage-

specific matrix gene expression and decreased type X collagen gene expression compared to cells expanded without FGF-2, suggesting possible crosstalk between FGF-2 and TGF- β 1 for chondrogenesis [101]. The effects of combining growth factors have also been investigated for chondrogenic induction. A combination of TGF- β 3 and BMP-6, or TGF- β 3 and IGF-1 enhanced chondrogenesis in bone marrow MSCs when compared to treatment with TGF- β 3, BMP-6, and IGF-1 alone [102]. BMP-2 was more effective than BMP-4 and -6 for the synthesis of proteoglycans and type II collagen in cartilage formation from bone marrow MSCs in the presence of TGF- β 3 [103]. Chondrogenesis of adipose MSCs was most effectively induced by treatment with a combination of TGF- β 2 and BMP-7 when compared to a combination of TGF- β 2 and BMP-2 or TGF- β 2 and BMP-6 [104]. Synovium MSCs synthesized more cartilage matrix in the presence of TGF- β 3 and BMP-2, as compared to combinations of TGF- β 3 and IGF-1, and TGF- β 3 and FGF-2 [105]. Exposure of synovium MSCs to a combination of TGF- β 1, IGF-1, and FGF-2 for the first 3 days of culture in pellets stimulated cell growth and enhanced chondrogenic differentiation by TGF- β 1 [106]. Further, FGF-2 treatment for the first 3 days, followed by the continuous treatment with TGF- β 1 and IGF-1, supported chondrogenesis using synovium MSCs [106]. Although the growth factors described above tend to exhibit similar effects, it is important to note that different combinations of growth factors, including variance in isoforms and timing of exposure, can influence chondrogenic differentiation of stem cells and the effects may vary depending on stem cell sources.

In addition to the use of various growth factors to induce chondrogenic differentiation, the effects of hypoxia toward chondrogenesis have also been investigated in MSCs. Hypoxia was shown to induce chondrogenesis in bone marrow MSCs in the absence of exogenous growth factors [107]. When compared to normoxia, hypoxia in the presence of GDF-5 increased expression of type II collagen and aggrecan, and decreased expression of type X collagen in self-assembled cartilage from bone marrow MSCs [108]. Thus, performance of various growth factors in terms of chondrogenic efficacy of adult stem cells, as a function of oxygen tension, continues to require additional evaluation.

While MSCs can be coaxed to progress toward the chondrogenic lineage by growth factors, this process is frequently accompanied by hypertrophic differentiation, as evident by the production of type X collagen, MMP13, and alkaline phosphatase (ALP). The subsequent potential for tissue mineralization remains an unsolved problem for tissue engineering articular cartilage. Parathyroid hormone related peptide (PTHrP) is a molecule present in the growth plate and acts as an inhibitor of chondrocyte hypertrophy. For marrow MSCs and adipose MSCs in pellet culture,

expression of type X collagen and RUNX-2 were reduced significantly by PTHrP [109]. Parathyroid hormone (PTH) inhibited expression of type X collagen and increased expression of type II collagen in marrow-derived MSCs from patients with osteoarthritis [110]. Further, PTHrP/PTH's ability to regulate hypertrophic differentiation may be useful for controlling MSC-chondrogenesis *in vitro*.

Embryonic stem cells

Embryonic stem cells (ESCs) provide infinite proliferative capacity and pluripotency [111]. However, complex ethical and political issues are associated with the derivation of these cells. For cartilage tissue engineering, ESCs are often first cultured as 3D embryoid bodies to differentiate them toward the chondrogenic phenotype. During this time, TGF- β s, BMPs, and IGF-1 to ESCs are often used. For example, ESCs treated with TGF- β 3, followed by a combination of TGF- β 1 and IGF-1, while being cultured as embryoid bodies yielded cells that, when used for engineering articular cartilage, produced no type I collagen [112]. In the same study, exposure to BMP-2 during the embryoid body phase produced a fibrocartilage-like phenotype [112]. In another study, embryoid bodies were plated and differentiated with TGF- β 3 and BMP-2, resulting in positive staining for type II collagen and SOX-9 [113]. Instead of embryoid body formation, ESCs seeded in pellet culture showed the highest gene expression of aggrecan and type II collagen when treated with BMP-7 alone, as compared to TGF- β 1 alone or a combination of TGF- β 1 and BMP-7 [114].

The effect of hypoxia in chondrogenic differentiation of ESCs has also been reported. Exposure of ESCs to hypoxic conditions during embryonic body culture was shown to significantly enhance cartilage protein synthesis and mechanical properties of self-assembled neocartilage [115]. Similarly, pellets, derived from ESCs cultured in conditioned medium by primary chondrocytes in the presence of transient hypoxia during embryonic body culture, produced enhanced type II collagen and GAG when compared to pellets derived from ESCs in normoxia [116].

These findings indicate the ability of growth factors to induce chondrogenesis in ESCs and potentiate the application of ESCs in cartilage repair and regeneration. However, as compared to differentiated cells, ESCs are more sensitive to culture conditions. The studies discussed above applied tissue engineering techniques to cells dissociated from embryoid bodies, cells still in the embryoid body form, cells that migrated out of embryoid bodies, and cells that were not placed in embryoid bodies at all. The effects of growth factors on chondro-differentiation and on chondrogenesis can, thus, be different from one condition to the next. Systematic examinations comparing growth

factor effects across different culture conditions are, therefore, needed for optimizing the use of signaling molecules in ESC culture.

Induced pluripotent stem cells

Induced pluripotent stem cells (iPSCs) do not face the same ethical issues as ESCs. iPSCs can be autologous, providing less risk of immune rejection and disease transmission. By introducing defined factors, Oct-3/4, SOX-2, KLF-4, and c-Myc, adult fibroblasts can be reprogrammed to iPSCs with pluripotent and self-renewal capacities [117]. To avoid the risk of tumor formation by transduction of the reprogramming factors, methods to generate iPSCs without genomic integration of transgenes have been reported [118–121]. For engineering articular cartilage, strategies using an adult's own cells can start with the generation of iPSCs that are subsequently differentiated into chondrocytes, for example, using TGF- β 3 and BMP-2, singly or in combination, as seen for iPSCs from various cell sources [122–125]. For the chondrogenic induction of iPSCs, the duration of the growth factor application is important. iPSCs treated with a combination of TGF- β 1, BMP-2, and GDF-5 resulted in chondrogenesis, but removing the stimulus followed by another 4 weeks of culture significantly reduced type I collagen expression compared to continuous exposure [126]. Studies on the effects of growth factor stimulation on iPSC chondrogenesis are yet limited, and it is unclear if inducing pluripotency is necessary for engineering articular cartilage.

Other cell sources

Skin and costal cartilage may be viable cell sources for cartilage tissue engineering without induced pluripotency. While dermal fibroblasts have been recognized as a resource for iPSC applications, their capability for chondrogenesis through other means has also been investigated. Direct chondrogenic induction has been demonstrated using human dermal fibroblasts without going through a pluripotent state by transducing c-Myc, KLF-4, and SOX-9 to generate chondrogenic cells [127, 128]. Whether these cells will respond similarly as iPSCs do to growth factors remains to be seen, and further comprehensive approaches using growth factors for chondrogenic differentiation of iPSCs are necessary. Without genetic manipulation, it has been shown that dermal fibroblasts pre-treated with IGF-1 can be chondro-induced through exposure to an aggrecan substrate, as seen by type II collagen and GAG expression [129]. Human dermal fibroblasts stimulated with GDF-5 expressed cartilage-specific markers including type II collagen, aggrecan, and SOX-9 both in monolayer and in micromass culture [130].

Various subpopulations of stem cells likely exist within skin [131]. Dermis includes multipotent adult stem cell populations that have the potential to differentiate into multiple cell types. Skin-derived precursors isolated from the whole dermis population by culturing them in suspension using FGF-2, epidermal growth factor (EGF), and B27TM showed differentiation potentials toward both neural and mesodermal cell types [132]. Chondrogenic differentiation of the skin-derived precursors was demonstrated in the presence of BMP-2 in micromass culture [133]. Clonally derived dermal fibroblasts can differentiate into multiple lineages including the chondrogenic lineage. Studies have shown chondrogenic differentiation of the clonally derived dermal fibroblasts in the presence of TGF- β 1 or TGF- β 1 plus IGF-1 in pellet cultures [134, 135]. Stem cells isolated from dermis obtained by rapid adherence to tissue culture plates, termed dermis isolated adult stem (DIAS) cells, showed multiple lineage differentiation potentials; the chondrogenic potential, when cultured with TGF- β 1 or BMP-2, was observed with increased GAG contents in self-assembled constructs [136]. Chondrogenesis of DIAS cells was enhanced with hypoxia in the presence of TGF- β 1 and IGF-1 in micromass culture [137]. Studies are still needed to enhance the chondrogenic capacity of cells derived from the skin to reach the biochemical and biomechanical characteristics of native articular cartilage, and it remains to be seen whether tissues engineered from these cells possess lubricious properties.

Despite the promise of using the stem cell sources described above, there remain concerns that still need to be addressed. For example, human ESCs expanded in vitro have a tendency to undergo karyotypic aberrations, while undifferentiated ESCs have the capacity to form teratomas in vivo [138, 139]. Furthermore, malignant transformation in bone marrow MSCs cultured for long-term ex vivo has also been reported [140]. Immunogenicity and biodistribution of stem cells are additional concerns [141]. The development of specific assays to identify and remove these concerns, toward evaluating safety and efficacy, is thus of paramount importance [141].

Costal cartilage, located at the anterior ends of the ribs, is not an articular cartilage. However, chondrocytes derived from costal cartilage have been used to engineer tissues that express lubricin, a protein that helps articular cartilage achieve low frictional properties. In this case, TGF- β 1, FGF-2, and PDGF were applied to costochondral cells during monolayer expansion [142]. Not much research has been reported for the use of costochondral cells to tissue engineer articular cartilage, and further studies comparing various growth factors to improve the quality of the engineered tissue are necessary. Nonetheless, the potential of using costal cartilage opens up another autologous cell source for cartilage repair and regeneration.

Signaling molecules for improving biomechanical properties

Articular cartilage withstands compressive, tensile, and shear loads as part of its function, and it is also lubricious, resulting in a tissue with very low coefficient of friction. Compressive, tensile, and shear moduli have been measured or estimated to range from 0.08 to 2, 5 to 25, and 0.05 to 0.25 MPa, respectively [13] and the coefficient of friction ranges from 0.03 to 0.06 [143]. Cartilage's biochemical content, primarily water, collagen, and proteoglycans, and the organization of these molecules allow for appropriate load distribution and transmission. Therefore, one of the major design criteria in cartilage tissue engineering is the creation of neocartilage with biomechanical properties that will withstand the demanding mechanical environment in vivo. Proper organization of the neocartilage is anticipated to allow for long-term functionality and durability.

Compressive properties and corresponding ECM components

Through their effects on matrix metabolism, growth factors influence GAG and collagen synthesis. Specifically, addition of IGF-1 in chondrocytes seeded onto biodegradable polyglycolic acid (PGA) scaffolds resulted in an increase in the total GAG content of the tissue 5-fold [144]. In contrast, a supplement of PDGF decreased GAG production by 43 %, with no effect on collagen content [144]. There is universal acceptance that TGF- β 1 enhances collagen synthesis (e.g., up to 34-fold increase in monolayer culture [25, 144], though its effects on GAG synthesis appears varied and dependent on 3D versus 2D culture and cell origin. In chondrocytes seeded in PGA scaffolds a decrease in GAG was recorded, while in monolayer culture an increase in total GAG content was demonstrated [25, 144]. Compared to cells from other zones, superficial zone chondrocytes responded to TGF- β 1 with the highest increase (220 % compared to control) in GAG production [25]. Regarding BMPs, BMP-2, BMP-12, and BMP-13 were shown to increase GAG synthesis in chondrocytes, but only BMP-2 use was not associated with chondrocyte hypertrophy [145]. Growth factor-induced alterations in biochemical content not only provide insight to phenotype but are also important due to their direct linkage to biomechanical properties.

In a study comparing combinations of BMP-2, IGF-1, and TGF- β 1 at various dosing regimens, all were shown to increase compressive properties (71, 75, and 73 %, respectively) with increases in GAG content (39, 41, and 31 %, respectively) [146]. In terms of dosing regimen, it was found that IGF-1 and BMP-2 were efficacious when

applied either continuously or intermittently toward improving compressive properties by ~ 90 and over 70 %, respectively, although TGF- $\beta 1$ was only effective with continuous administration (89 % increase in compressive properties compared to control). The combination of BMP-2 and IGF-1 was the most successful in improving the GAG content of the engineered tissue by 54 %, which was translated to the highest improvement in compressive properties, a 119 % increase [146]. Finally, it was shown that a lag time after TGF- β administration was required for the observed effect [146].

Signaling molecules have been successfully combined with compressive loading to improve the biomechanical properties of engineered cartilage. Moderate dynamic compressive loading between 0–12 % strain of articular cartilage has been demonstrated to play an anabolic role on chondrocytes by promoting collagen and proteoglycan synthesis by 31–34 and 17–38 %, respectively [147]. IGF-1 stimulation with dynamic compression at 3 % and 0.1 Hz showed a synergistic effect on collagen and proteoglycan synthetic activity, as demonstrated by an increase in H-proline incorporation by 180 % and in S-sulfate incorporation by 290 % compared to 30 and 120 % increase, respectively, with dynamic compression only, and 90 and 160 % increase with IGF-1 stimulation alone [148]. This difference was potentially due to changes in the transport of IGF-1 by different loading regimens, as demonstrated by the analysis of diffusivity of IGF-1 in cartilage [148]. Dynamic compression of chondrocyte-seeded agarose hydrogels at 10 % strain and 1 Hz combined with either TGF- $\beta 1$ or IGF-1 resulted in a three- to fourfold increase in aggregate modulus for both growth factors, as well as in collagen (~ 7 - and ~ 5 -fold increases for TGF- $\beta 1$ and IGF-1, respectively) and GAG synthesis (~ 2 - and ~ 2.5 -fold increases for TGF- $\beta 1$ and IGF-1, respectively) [149]. It is noteworthy that, in general, changes in biomechanical properties do not scale linearly with changes in biochemical components, suggesting important roles for interaction among matrix components and matrix organization in determining biomechanical properties.

Similar to direct compression, hydrostatic pressure is a stimulus that improves the compressive and biochemical properties of engineered cartilage [150]. Combined with TGF- $\beta 3$ in a chondrogenesis model using mesenchymal stem cells, intermittent hydrostatic pressure of 10 MPa at 1 Hz stimulated mRNA expression of SOX-9, type II collagen, and aggrecan by 1.9-fold, 3.3- and 1.6-fold, respectively, compared to TGF- $\beta 3$ application alone [151]. Combined with BMP-2 and IGF-1, 10 MPa static hydrostatic pressure in neocartilage, engineered with articular chondrocytes, increased aggregate and tensile modulus values by 17 and 30 %, respectively [152]. The same hydrostatic pressure regimen improved aggregate and

tensile modulus values by 41 and 40 %, respectively, when applied with TGF- $\beta 1$ [152]. Since hydrostatic pressure can be applied before engineered cartilage develops robust mechanical characteristics, hydrostatic pressure can be applied earlier than direct compression during tissue engineering of articular cartilage.

Better understanding of the exact mode of action and how synergism occurs among the different stimulatory signals above is the next step towards optimization of their potential. In a study where TGF- $\beta 3$ was released from a poly(lactide-co-caprolactone) PLCL scaffold over a 12-week period, the compressive properties of the engineered cartilage gradually increased from ~ 300 kPa at 4 weeks, to ~ 400 kPa at 8 weeks, and to ~ 550 kPa at 12 weeks [153]. In cartilage tissue engineering, the development and use of different anabolic stimuli, in combination with mechanical loading signals, is emerging as a promising approach to enhance the compressive properties of neocartilage.

Tensile properties and corresponding ECM components

Improving the tensile properties of neocartilage has been one of the major challenges in cartilage tissue engineering [154]. Among the different growth factors used in articular cartilage engineering, TGF- β is the one that has most prominently been shown to improve tensile properties. Application of 30 ng/ml TGF- $\beta 1$ has been shown to increase tensile properties by twofold over controls when applied continuously as a result of increased collagen synthesis [146, 149]. The stimulatory effect of the application of dynamic, unconfined, compressive loading on chondrocyte-seeded agarose hydrogels at 0–10 % strain and 1 Hz was further enhanced by TGF- $\beta 1$ leading to increased collagen production by approximately twofold [149]. Despite these advancements, improvements in tensile properties due to stimulation by growth factors are still substantially lower than native tissue values. This is true even when combining growth factors with compressive loading and hydrostatic pressure [149, 152]. As a result, biophysical agents, such as chondroitinase-ABC (c-ABC), and enzymes, such as lysyl oxidase-like 2 (LOXL2), and ECM proteins, such as superficial zone protein (SZP), have been investigated to further improve the tensile properties of neocartilage.

Application of c-ABC to native tissue and to tissue-engineered cartilage results in cleavage of chondroitin and dermatan sulfate and immediate depletion of GAGs [155, 156]. The depleted GAGs recover upon culture, bringing the compressive mechanical properties back to levels of untreated samples [155, 157]. Counterintuitively, however, persistent effects of c-ABC treatment were observed; collagen production was enhanced by approximately 300 %,

and an increase of $\sim 180\%$ in tensile properties was observed [157]. Multiple c-ABC applications result in improvement over a single application [157–159]. It has been hypothesized that this effect may be due to matrix-bound growth factors that are released upon c-ABC's loosening of the cartilage matrix [160]. Another reason may be that c-ABC treatment induces cell proliferation [155]. Genetic microarrays, however, showed that c-ABC's effects are mostly biophysical [161]. Trimethylamine N-oxide (TMNO), an osmolyte that is found in sharks, has been used in combination with c-ABC to improve tensile properties by $\sim 100\%$ [159]. Cell proliferation, osmotic-loading, and protein stabilization due to TMNO have been hypothesized as potential routes of action. Additional studies that elucidate how, for instance, protein stabilization may work in concert with c-ABC to result in improved tensile properties may help to identify other protein stabilizing molecules to be used in cartilage tissue engineering.

Collagen cross-links represent a fundamental component of collagen organization and contribute significantly to the tensile properties of cartilaginous tissues [154, 162, 163]. In a novel application of exogenous LOXL2 in neocartilage, it was shown that the tensile properties were significantly improved by fivefold through pyridinoline (PYR) cross-linking (16-fold increase in PYR cross-linking compared to control) [154]. This improvement in tensile properties was both time- and dose-dependent. High dose LOXL2 application improved the tensile modulus by ~ 2 -fold compared to low dose application, and early LOXL2 application led to a ~ 3 -fold increase compared to late application [154]. The improved properties persisted in vivo, with LOXL2 increasing collagen fibril density that also helped improve tensile properties [154]. Interestingly, hypoxia induced upregulation of LOX gene expression, resulting in increases in PYR crosslinks and tensile properties in engineered cartilage [164].

SZP is a glycoprotein that is produced mainly by synovocytes and chondrocytes of the superficial cartilaginous zone [165]. A recent study that used chondrocytes from middle and superficial zones in different ratios demonstrated that chondrocytes in the superficial zone were able to improve tensile properties of the neocartilage. By increasing the ratio of superficial zone cells from 0 to 100%, the tensile modulus increased from 1.1 to 4.5 MPa [166]. This increase was hypothesized to be due to increased synthesis of SZP, as it was demonstrated that SZP media accumulation increased from approximately 0.5 to 3.5 $\mu\text{g/ml}$, respectively [167].

A few soluble molecules have been identified to increase tensile properties of engineered cartilage, but these are not as numerous when compared with molecules identified to improve cartilage compressive properties. Further, it appears that mechanical stimuli used to improve

compressive properties do not have the same magnitude of effect on tensile properties. Combinations of growth factors, biophysical agents, ECM components, and even new classes of mechanical stimuli need to be explored with respect to engineering robust tensile properties in articular cartilage.

Mechanotransduction of signals

Cells convert physical forces into biochemical signals through mechanotransduction. Mechanotransduction can occur through various mechanisms, linked by cellular components such as tyrosine kinase receptors, ion channels, and various cytoskeletal filaments; these are termed mechanosensors [168]. These mechanosensors have been investigated with regard to their roles in mechanotransducing signals in chondrocytes, as described below.

As noted previously, mechanical stimuli, such as direct compression and hydrostatic pressure, can lead to changes in cell proliferation and matrix synthesis that, in turn, manifest as changes in mechanical properties of the engineered cartilage. Understanding how mechanical stimuli can alter proliferation and matrix synthesis is, thus, of importance for obtaining finer control of mechanical stimuli. An example is studying the role of ERK in mechanotransduction. In cartilage explants compressive static loading at 40% strain induced phosphorylation of ERK, a MAP kinase, leading to increased cell proliferation [169]. Application of 10 MPa of static hydrostatic pressure in tissue-engineered cartilage activated the ERK signaling pathway and led to increases in tensile properties by 70% [169, 170]. Inhibition of the ERK pathway during hydrostatic pressure loading abolished this enhancement [170]. The ERK signaling pathway has been recognized as a major component of mechanotransduction; understanding of its exact role, as well as recognition of other signaling pathways involved, can serve as an important addition to the tissue engineering of articular cartilage.

Ion channels are important mechanosensors. Hydrostatic pressure application of 10 MPa inhibited Na^+/K^+ ion channels and activated Na^+/H^+ channels in chondrocytes, as shown by the effect on the Na^+ and H^+ exchange activity [171, 172]. Modulation of Na^+/K^+ and calcium ion channels using inhibitors of Na^+ ion transporters, such as ouabain and bumetanide, and stimulators of intracellular Ca^{2+} , such as histamine and ionomycin, have been shown to result in increases in the mechanical properties of neocartilage [173]. Tensile properties reached 185 and 130% as stimulated by ouabain and ionomycin, respectively [173]. Mechanical stress in a form of fluid flow shear was also shown to enhance chondrocyte proliferation via activation of ion channels through Indian hedgehog and BMP-dependent pathways [174]. The exact roles that ion channel

signaling play in mechanical transduction remain to be determined toward improvement of engineered cartilage functional properties.

Mechanotransduction through the cytoskeleton can begin with integrin-mediated adhesions that transmits forces from the ECM to cytoskeletal filaments [168]. Cadherins may also have a role in mechanotransduction due to their close interaction with both integrins and kinase receptors [168]. Disturbances of microtubule organization prevented the stimulatory effect of hydrostatic pressure loading on proteoglycan synthesis [175]. Specifically, microtubule de-polymerization induced by nocodazole, an anti-polymerization agent that is used as an anti-neoplastic agent, inhibited the increase of ~20 % in proteoglycan synthesis that would normally be exhibited from application of 5 MP cyclic hydrostatic pressure at 0.5 Hz [175]. Despite the fact that the mechanotransduction pathways involved in articular cartilage and the exact role of mechanosensors is yet to be determined, current knowledge indicates the beginning of an exciting era where modulation of these signaling pathways would potentially result in significant improvement of engineered tissue.

Current challenges in cartilage tissue engineering and future perspectives

Despite the progress in engineering biologically functional cartilage tissue *in vitro* with the aid of signaling molecules, challenges remain for its successful clinical translation. Issues often arise after the transplantation of engineered tissue *in vivo*, and these include phenotypic instability and poor integration (Fig. 4). Inflammatory responses against implanted engineered tissue are also problematic. In the following section, reviewed are the major challenges in the current cartilage tissue engineering and the bioactive agents that exhibit potential toward resolving these challenges.

Phenotypic instability

The phenotypic instability of engineered cartilage is a common problem. Implanted cells often contain undesired phenotypes that potentially lead to the formation of tissues that exhibit deficient biological and biomechanical functions. Frequently, cells with inferior chondrogenic ability form fibrous cartilage with properties that are not reminiscent of the physiological function of hyaline cartilage. Dedifferentiation of implanted cells with increased production of type I collagen leads to inferior cartilage matrix and mechanical function. Additionally, the appearance of hypertrophic phenotype in engineered tissue can also be problematic as it may promote mineralization. In stem cell-

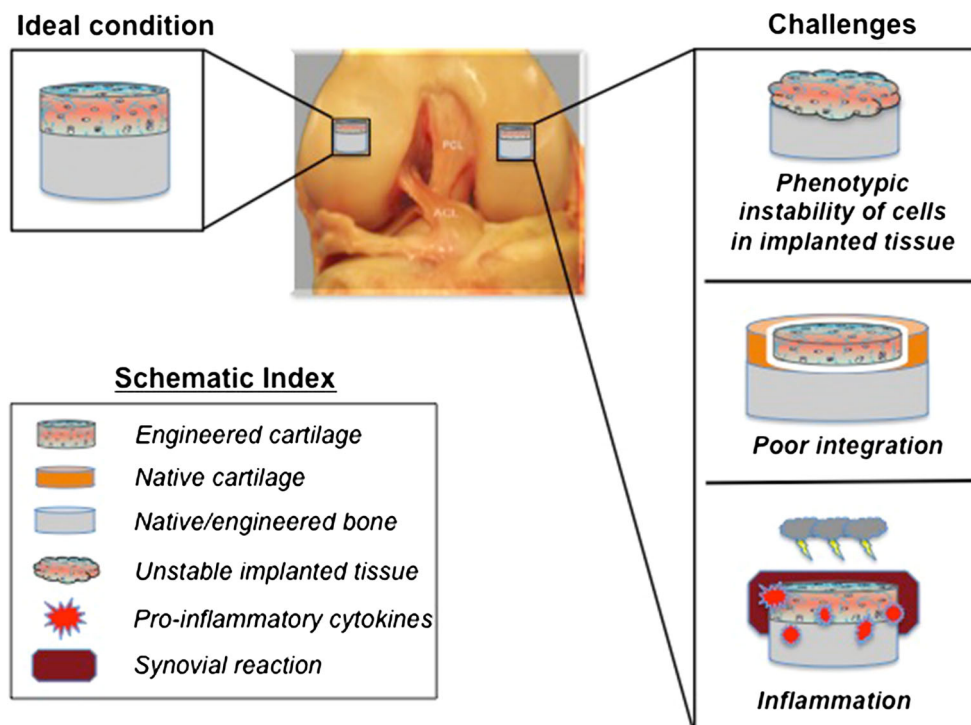
based treatments, *in vitro* chondrogenesis using adult stem cells is often accompanied by hypertrophic differentiation with increased expression of type X collagen. As an example, stem cells from different sources were shown to result in fibrous or hypertrophic phenotypes, when transplanted subcutaneously *in vivo* [176]. To suppress hypertrophic differentiation, several molecules have been explored. In addition to PTH and PTHrP described above, BMP-7 has been shown to inhibit type X collagen in human MSCs while also inducing chondrogenic differentiation [177]. A combination of SOX-5/-6/-9 was able to suppress hypertrophic markers and osteogenic markers in human MSCs [178]. Nkx3.2, a transcription factor involved in cartilage development, also inhibits RUNX-2 function [179], suggesting a potential use for preventing hypertrophy. With the increased desire of identifying and using stem cells for cartilage tissue engineering, retaining cells in a state of differentiated mature chondrocytes becomes of paramount importance and remains a main challenge for translation. Further improvement of current methodologies, as well as studies on potential bioactive agents to prevent these challenges, will be necessary.

Chondrocyte hypertrophy is commonly detected in osteoarthritis pathogenesis. Chondrocytes in osteoarthritis cartilage exhibit hypertrophic phenotypes by expressing type X collagen [180]. Although the characteristics of chondrocytes in osteoarthritis resemble those of chondrocytes in the growth plate, their pathways for controlling hypertrophy may be different [181]. The hypertrophic phenotype of chondrocytes in osteoarthritis is induced by many cytokines, growth factors, and ECM degradation products [181]. Thus, it is possible that the osteoarthritic environment can also contribute to hypertrophic differentiation of implanted cells for tissue engineering applications. Understanding hypertrophy processes in osteoarthritis, including signaling molecules and corresponding pathways, will be pivotal toward overcoming the challenge of phenotypic instability of engineered tissue.

Integration

Failure of integration between engineered tissue and surrounding native cartilage continues to be a fundamental problem in the field of cartilage tissue engineering. Cartilage lesions can also extend into the subchondral bone, making cartilage to cartilage, cartilage to bone, and bone to bone integration processes relevant for the clinical translation of cartilage implants. Several factors that influence the ability of the repair tissue to integrate with the native cartilage have been proposed, such as cell death at the wound edge, the phenotype of the cells in the implanted tissue, and donor age [182]. In addition, the degree of maturation of engineered constructs can affect integration [183].

Fig. 4 Challenges in cartilage tissue engineering. Phenotypic instability of engineered cartilage tissue, poor integration, and the inflammatory environment are disadvantages that need to be addressed toward successful cartilage tissue engineering for future clinical use



Traditionally, cartilage tissue engineering has sought to stimulate the production of collagen and GAGs at levels similar to native tissue. Ironically, it has been shown that these matrix components can interfere with integration. The matrix of the native tissue can prevent adhesion and diffusion of cells and matrix proteins [184, 185], which can impede the engineered tissue from integrating [185]. Strategies have, thus, been developed to disrupt the mature matrix in order to effect integration. Disruption of certain matrix molecules via enzymatic treatment has been shown to enhance integration. For example, collagenase and hyaluronidase applied to the wound site increased cell density as well as improved integration with implanted cartilage [186]. β -Aminopropionitrile (BAPN), a blocker of lysyl oxidase, was used on tissue-engineered constructs to prevent crosslinks from forming in the engineered tissue, allowing for the presence of more crosslink sites on the sides of implanted tissue for enhanced integration [187]. Similarly, considering that the PYR crosslink in collagen can take weeks to complete forming, strategies have also included “priming” the implant with exogenous LOXL2 to accumulate collagen precursors. The concept is that, upon implantation, these crosslink precursors in the engineered cartilage will form mature crosslinks with the native cartilage [188].

Temporal depletion of GAG at cartilage surface by c-ABC or trypsin has also been shown to improve coverage by repair cells and integration of repair tissue, respectively [183, 184]. These enzymes can be combined with the

anabolic factors described previously to counteract their catabolic effects [161] or with factors and molecules that disrupt cartilage matrix formation, such as IGF-1, BAPN, and para-nitrophenyl- β -D-xyloside, which disrupts proteoglycan formation, to promote integration [189]. Although the presence of matrix components, such as GAG and collagen, in engineered cartilage is necessary to withstand stresses *in vivo*, their temporal absence may allow for robust integration. The dual roles that bioactive agents c-ABC and LOXL2 play in improving integration, as well as enhancing collagen production and tensile properties, signify that these agents should be part of the tissue engineering armamentarium toward resolving the as-of-yet intractable challenge of integration.

Inflammation

Inflammation is well recognized as a main contributor in osteoarthritis development and progression, but the exact mechanisms of action of pro-inflammatory cytokines requires further clarification. Elevated levels of these cytokines in the osteoarthritic joint impair cartilage homeostasis by disrupting the balance between chondrocyte anabolic and catabolic activities. Inflammation mediated by interaction between the joint cartilage and surrounding tissues such as bone, muscle, adipose tissues, and synovium has also been suggested to contribute to the development and progression of osteoarthritis [190]. Notably, interleukin-1 β (IL-1 β) and tumor necrosis factor-

α (TNF- α) are pro-inflammatory cytokines present in the arthritic joint and involved in the progression of cartilage destruction. Pro-inflammatory cytokine signals are transduced through the nuclear factor kappa B (NF- κ B) pathway, resulting in the induction of nitric oxide (NO), cyclooxygenase2 (COX2), and prostaglandin E2 (PGE2) [191]. Several *in vitro* studies suggest the destructive effects of an inflammatory environment can influence implanted engineered cartilage tissue *in vivo*. Application of both IL-1 β and TNF- α inhibited chondrogenesis of human MSCs in a dose-dependent manner through activation of the NF- κ B pathway [192]. Osteoarthritic synovium-derived, conditioned medium has also shown to inhibit chondrogenesis of human MSCs [193]. Inflammation in the arthritic joint can potentially impede with neotissue growth and integration into the joint while also diminishing its functional properties. Thus, providing an environment controlling inflammation to reduce damage of the implanted tissue, as well as to maintain its functionality, may be necessary for successful cartilage repair.

In an attempt to prevent cartilage damage from inflammation, growth factors, GAG compounds, and platelet-rich plasma (PRP) have been investigated. Growth factors such as IGF-1 and PDGF-bb have shown to suppress IL-1 β induced NF- κ B activation and apoptosis in chondrocytes [194]. BMP-2 and BMP-9 recovered IL-1 β -induced damage and partially blocked the suppressive effect of IL-1 β on cartilage-specific matrix expression in human MSCs [195]. In addition to growth factors, some GAG compounds such as chondroitin sulfate, glucosamine, and hyaluronic acid have shown to have anti-inflammatory effects [196]. A synergistic action between hyaluronic acid and PRP has been observed in recovering the chondrogenic phenotype of osteoarthritic articular chondrocytes through activation of CD44 and TGF- β receptor II, and inhibiting expression of inflammation-related chemokines and cytokines [197].

PRP contains various growth factors, chemokines/cytokines, and adhesive proteins [198], and its use has been associated with reducing pain and restoring function in osteoarthritic joints [198, 199]. Several reports demonstrated the potential use of PRP on cell proliferation and differentiation of cartilage cells and MSCs *in vitro* [199]. However, discrepancies within studies, possibly due to preparation methods and donor variance [199], means more studies should be performed to understand how PRP may influence engineered cartilage. Although anti-inflammatory products have been introduced to inhibit inflammation-induced damage, their exact roles and mechanisms are not clear. To effect successful cartilage regeneration, the role of degenerative changes on this process needs to be elucidated. Thus, comprehensive studies need to be conducted to establish the role of inflammation leading to

osteoarthritis, as well as the role of anti-inflammatory agents as potential protectors of the implanted neotissue.

Conclusion

Current research in articular cartilage tissue engineering derives most of its inspiration from phenomena observed during cartilage development as well as homeostasis. Advances in bio-functionality of engineered cartilage, especially in terms of neotissue biochemical and biomechanical properties, in response to signaling molecules or matrix-modifying agents, have emanated from knowledge in development and normophysiology (Fig. 5). However, we are still away from engineering neocartilage with biochemical and biomechanical properties on par with those of native articular cartilage. This continues to be a major challenge in cartilage tissue engineering, especially when one considers that the engineered tissue is frequently intended to operate in an inflammatory environment. Indeed, implanted engineered tissues face a complex plethora of stimuli in the arthritic joint, in addition to the highly strenuous environment. Furthermore, engineered tissues exhibit phenotypic instability and suffer from lack of integration as well in the recipient site.

To address these challenges, it is informative to understand pathogenesis of osteoarthritis for two major reasons: (1) to identify catabolic agents or other pathological factors

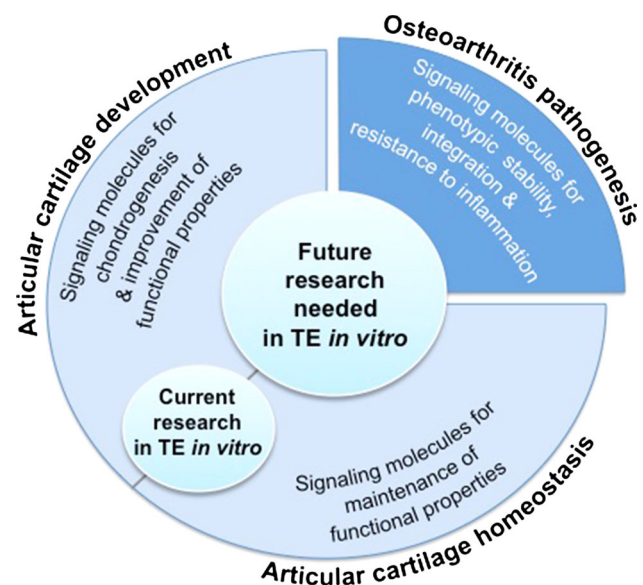


Fig. 5 Future research in tissue engineering *in vitro*. Current research is often informed by knowledge pertaining to articular cartilage development and homeostasis to tissue-engineer articular cartilage. Future research needs to continue to derive inspiration from these phases but also needs to incorporate information from OA pathogenesis to resolve the challenges in cartilage tissue engineering

that can have a positive effect in the tissue engineering process, such as for example chondroitinase-ABC, and (2) to help us design an engineered tissue that, when implanted in vivo, can function in an inflammatory environment. Thus, for future research, it will be important not only to continue to derive inspiration from cartilage development and homeostasis but also to incorporate information from osteoarthritis pathogenesis.

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