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REVEALING THE ACTIVATION PATHWAY FOR TMEM16A CHLORIDE CHANNELS FROM MACROSCOPIC CURRENTS AND KINETIC MODELS

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Abstract

TMEM16A (ANO1), the pore-forming subunit of calcium-activated chloride channels, regulates several physiological and pathophysiological processes such as smooth muscle contraction, cardiac and neuronal excitability, salivary secretion, tumour growth, and cancer progression. Gating of TMEM16A is complex because it involves the interplay between increases in intracellular calcium concentration ($[Ca^{2+}]_i$), membrane depolarization, extracellular Cl^- or permeant anions, and intracellular protons. Our goal here was to understand how these variables regulate TMEM16A gating and to explain four observations. a) TMEM16A is activated by voltage in the absence of intracellular Ca^{2+} . b) The Cl^- conductance is decreased after reducing extracellular Cl^- concentration ($[Cl^-]_o$). c) I_{Cl} is regulated by physiological concentrations of $[Cl^-]_o$. d) In cells dialyzed with $0.2 \mu M [Ca^{2+}]_i$, Cl^- has a bimodal effect: at $[Cl^-]_o < 30 \text{ mM}$ TMEM16A current activates with a monoexponential time course, but above 30 mM $[Cl^-]_o$ I_{Cl} activation displays fast and slow kinetics. To explain the contribution of V_m , Ca^{2+} and Cl^- to gating, we developed a 12-state Markov chain model. This model explains TMEM16A activation as a sequential, direct, and V_m -dependent binding of two Ca^{2+} ions coupled to a V_m -dependent binding of an external Cl^- ion, with V_m -dependent transitions between states. Our model predicts that extracellular Cl^- does not alter the apparent Ca^{2+} affinity of TMEM16A, which we corroborated experimentally. Rather, extracellular Cl^- acts by stabilizing the open configuration induced by Ca^{2+} and by contributing to the V_m dependence of activation.

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Keywords

Chloride channel; kinetics; patch clamp; permeation; gating; mathematical modelling

INTRODUCTION

Cl⁻ movements through Ca²⁺ activated chloride (Cl⁻) channels (CaCCs) play important roles in many cellular functions such as regulation of smooth muscle contraction, regulation of cardiac and neuronal excitability, salivary secretion, and tumour growth and progression in many types of cancer [13, 21, 29, 40]. TMEM16A (ANO1) and TMEM16B (ANO2) are the pore-forming subunits of CaCCs [6, 45, 50]. The gating mechanism of these channels is quite complex. Gating requires increases in intracellular calcium concentration ([Ca²⁺]_i), but also involves membrane depolarization, extracellular Cl⁻ or permeant anions, and intracellular protons. Ca²⁺-dependent activation is coupled to V_m [27, 35, 49] and is regulated by intracellular protons that compete for Ca²⁺ binding [1, 8]. When [Ca²⁺]_i is in the range of 0.1 – 0.8 μM, channel gating is strongly V_m-dependent, and the I–V_m relationships show outward rectification. Such V_m-dependence is lost when [Ca²⁺]_i > 5 μM. Hence, the dose-response curve to [Ca²⁺]_i displays weak V_m-dependence [2, 49, 52]. This V_m-dependence is explained by a voltage-dependent Ca²⁺ dissociation [49]. We have shown that TMEM16A and TMEM16B exhibit fast and slow gating modes [11]. Both modes depend on intracellular Ca²⁺, membrane voltage (V_m) and the extracellular Cl⁻ concentration ([Cl⁻]_o). Apart from the Ca²⁺-dependent activation, TMEM16A can also be activated by strong depolarizations in the absence of intracellular Ca²⁺ [49].

We assume that direct binding of Ca²⁺ activates TMEM16A [2, 3, 27]. This idea is supported by the following observations: a) injection of Ca²⁺, Ba²⁺ or Sr²⁺ into *Xenopus* oocytes activates CaCC [32]; b) TMEM16A in excised patches or liposomes can be activated by Ca²⁺, Ba²⁺ or Sr²⁺ [34, 46, 49]; c) mutating residues E702, E705, E730 and D734 located in the Ca²⁺ binding pocket of TMEM16A decrease the Ca²⁺ sensitivity 100 – 1000-fold [47, 52]; d) the x-ray structure of the *Nectria haematococca* TMEM16 homolog (*nh*TMEM16) shows the presence of two Ca²⁺ ions bound to a site located within the membrane [5]; e) changing the *nh*TMEM16 Ca²⁺-coordinating residues significantly reduces the functional Ca²⁺ sensitivity, which strongly indicates these residues are part of a high-affinity Ca²⁺ binding site [5, 34, 47]; and f) vertebrate TMEM16A is activated in a cooperative manner by Ca²⁺ [49]. Also, other regions of TMEM16A including the N-terminus and the first intracellular loop have been shown to contribute to Ca²⁺ sensitivity [17, 49]. Thus, the existing evidence strongly suggests that TMEM16A is directly activated by binding at least two Ca²⁺ ions.

The role of permeant ions in channel gating has increasingly been recognized. Gating of Cl⁻ channels such as CIC-2, volume-sensitive channels, and CFTR are reported to be dependent on permeant anion [23, 25, 41, 51]. CaCCs are not the exception. Anions with a higher permeability than Cl⁻ such as SCN⁻, I⁻, and NO₃⁻ when applied from the extracellular side promote opening and accelerate the opening rate while slowing down the closing rate in CaCCs [4, 36, 38, 49]. In addition, these anions decrease the EC₅₀ for Ca²⁺ both in *Xenopus*

oocyte CaCCs as well as heterologous-expressed TMEM16A and TMEM16B [4, 38, 39]. These observations suggest gating and ion permeation are coupled in TMEM16A channels.

The rather complex gating of TMEM16 channels cannot be understood without the help of a model. In this work, we developed a 12-state Markov chain model to explain the TMEM16A gating mechanism. The model reproduces the complex TMEM16A activation in response to V_m , Ca^{2+} and different $[Cl^-]_o$. The model also predicts that extracellular Cl^- does not alter the channel's affinity for Ca^{2+} . Further experiments corroborated this prediction. We propose that TMEM16A is activated by sequential, direct, V_m -dependent binding of two Ca^{2+} ions coupled by a V_m -dependent binding of one external Cl^- ion.

MATERIALS AND METHODS

Culture of HEK 293 cells and expression of TMEM16A

Human embryonic kidney 293 cells (HEK293) were cultured in Dulbecco's modified Eagle medium (DMEM, Gibco BRL, Carlsbad, CA, USA) supplemented with 10% heat-inactivated fetal bovine serum, 1% gentamicin and 1% L-glutamine at 37 °C in a 95% O_2 /5% CO_2 atmosphere. Stable cell lines were developed by transfecting a cDNA encoding the mouse TMEM16A (ac variant) sub-cloned into the bi-cistronic expression vector pIRES2-EGFP (Clontech, Mountain View, CA, USA.). The PolyFect transfection reagent (Qiagen, Valencia, CA, USA) was used according to the manufacturer's specification. After 24 h, the cells were transferred to 24-well plates at low density in DMEM medium supplemented with 1 mg/ml G418 (Sigma- Aldrich Co. St. Louis, MO, USA.). G418-resistant transformants were identified by EGFP fluorescence and expanded. Stable cell lines were maintained in medium supplemented with G418 at 500 μ g/ml. Cells were seeded at low density on 5 mm circular coverslips before electrophysiological recordings.

Recording solutions

Table 1 lists the composition of external solutions (ES) and internal solutions (IS) used to record the Cl^- current activated by intracellular Ca^{2+} or V_m (I_{Cl}). IS with buffered Ca^{2+} was prepared using EGTA and Ca^{2+} ; the free $[Ca^{2+}]_i$ was estimated using MAXCHELATOR (maxchelator.stanford.edu). ES-140Cl and IS-40Cl/0.2Ca are control solutions. An IS with 5 μ M $[Ca^{2+}]_i$ (IS-40Cl/5Ca) was used to activate fully TMEM16A and record I_{Cl} with long depolarizations in cells bathed with ES-140Cl. To analyse the activation of TMEM16A in zero $[Ca^{2+}]_i$ we used IS-40Cl/0Ca containing 25.2 mM EGTA and 50 mM HEPES. The Cl^- dependence of activation was studied using ES containing 140, 109, 70.5, 30, 10 or 1.5 mM $[Cl^-]_o$. The pH of each solution was adjusted to 7.3 with TEA-OH or NaOH. ES was made hypertonic relative to the internal solutions to avoid activation of volume-sensitive Cl^- channels present in HEK293 cells [23]. Osmolarity was adjusted by adding D-mannitol and measured using the vapour pressure point method (VAPRO, Wescor Inc., South Logan, UT, USA). All chemicals were purchased from Sigma-Aldrich (Co. St. Louis, MO, USA.).

Electrophysiological recordings

We record I_{Cl} at room temperature using the whole cell configuration of the patch clamp technique. Cells were held at -60 mV and the V_m was changed stepwise from -100 mV to

+160 mV or +180 mV in 20 mV increments, and then returned to -60 mV or -100 mV. Pulse duration varied between 0.5 to 20 s. I_{Cl} was recorded with an Axopatch 200B amplifier (Molecular Devices, Sunnyvale, CA, USA); currents were filtered at 5 kHz and digitized at 10 kHz for 0.5 s pulses. For 20 s pulses, the currents were filtered at 1 kHz and digitized at 2 kHz using pClamp software. Errors due to liquid junction potentials (-4.8 to -6.6 mV for our recording solutions) were minimized by using a 0.5 M KCl agar-bridge to ground the recording chamber and not corrected.

The effects of $[Cl^-]_o$ on TMEM16A activation were determined by measuring the magnitude of tail currents (I_{tail}) at -100 mV after a depolarising test pulse to +120 mV whose duration was varied from 0 to 3 s. The initial magnitude of I_{tail} after each pulse and each $[Cl^-]_o$ was used to calculate the tail conductance (G_{tail}) as a function of time and $[Cl^-]_o$ using Equation 1.

$$G_{tail} = \frac{I_{tail}}{V_m - V_{rev}} \quad \text{Equation 1}$$

where V_{rev} is the reversal potential of I_{Cl} . $G(t, [Cl^-]_o)$ was then normalized to the conductance obtained at the end of a 3 s test pulse with 140 mM Cl^- . The resulting normalized G vs time curve represented the time course of TMEM16A activation at +120 mV at each $[Cl^-]_o$. Dose-response curves were constructed using recordings obtained from patches excised from cells stably expressing TMEM16A. Patches were held at the desired V_m and exposed to increasing $[Ca^{2+}]_i$ ranging from 0 to 12 μ M (Table 1) using a Fast-Step Perfusion System (VC-77SP Warner Instruments, Hamden, CT, USA). In between each $[Ca^{2+}]_i$ test solution, a control solution containing 0 Ca^{2+} and 25.2 mM EGTA was applied to check for changes in seal resistance. I_{Cl} was recorded with an Axopatch 200B amplifier, filtered at 1 kHz and digitized at 10 kHz.

Analysis and modelling

The magnitude of I_{Cl} at each V_m was converted to conductance using Equation 1. Normalization was carried out using either G_{+120mV} or G_{max} to obtain G_{Norm} (G/G_{max} or G/G_{+120mV}), which is proportional to the apparent open probability of the channel. We extracted the time constants by fitting the data to a mono or bi-exponential function of the form:

$$y_0 + a^{-t/\tau} \quad \text{or} \quad y_0 + a^{-t/\tau_f} + b^{-t/\tau_s} \quad \text{Equation 2}$$

where y_0 is the value of y when $t \rightarrow \infty$, t is the time, τ is a time constant, a and b are the contribution of fast and slow processes, and τ_f and τ_s are the fast and slow time constants [11], respectively. The dose-response curves were constructed using normalized currents; only patches with stable basal current obtained with 0 $[Ca^{2+}]_i$ were used. In each case the basal current was subtracted to obtain the magnitude of the current activated by a given $[Ca^{2+}]_i$. The currents obtained from a particular patch were normalized to the maximum current estimated using equation:

$$\frac{I_{Cl}}{I_{max}} = \left[\frac{1}{1 + \frac{EC_{50}}{[Ca^{2+}]_i}} \right]^{n_H} \quad \text{Equation 3}$$

where I_{max} is the estimated maximum current, EC_{50} is the $[Ca^{2+}]_i$ needed to obtain $I_{max}=0.5$, and n_H is the Hill coefficient. To search for a kinetic scheme able to describe the time- and V_m -dependencies of I_{Cl} collected under a variety of experimental conditions we used Markov chain kinetic models [9] because they provide a good description of gating properties for different channels [24, 26, 28, 43, 48]. Different models with various discrete closed (C) and open (O) states were built using IChMASCOT software [10, 42]. Experimental and model I_{Cl} vs V_m , G_{Norm} vs $[Ca^{2+}]_i$, and EC_{50} were compared. Finally, by computing the probability of occupation of each of the kinetic states as a function of time we aimed to find the activation route(s) of TMEM16A. In the model, a given transition was controlled by forward and backward rate constants, which were V_m -dependent in most cases:

$$k_f = k_{f,0} * e^{\frac{z_f F V_m}{RT}} \quad \text{and} \quad k_r = k_{r,0} * e^{-\frac{z_r F V_m}{RT}} \quad \text{Equation 4}$$

where k_f and k_r are forward and backward rate constants, respectively, $k_{f,0}$ and $k_{r,0}$ are the values of k_f and k_r at $V_m=0$, z_f , z_r are the apparent gating charges associated with a given transition, F is the Faraday constant, R is gas constant, and T is the temperature. The most likely values of the rate constant parameters at $V_m = 0$ mV for a given model were obtained by best-fits as described in [12]. For that purpose, the squared differences between experimental and modelled values were minimized as follows:

$$\sum_{i=1}^N W_i \sum_{j=1}^{M_i} (E_{ij} - S_{ij})^2 \quad \text{Equation 5}$$

and

$$W_i = \frac{w_i}{M_i W E_{imax}^2} \quad \text{Equation 6}$$

where N = number of different data sets included in the global fitting procedure; M_i = number of independent experimental observations in the dataset i ; E_{ij} = experimental values of a given observation, S_{ij} = modelled values of a given observation; W_i = normalized weight factor for specific dataset; w_i = arbitrary weight factor for the measurement i ; and E_{imax} = maximal experimental value for the dataset i . The global fit was repeated 15 times. The resulting values were averaged and then used for the final fit to obtain the values reported in Table 2. Subsequently, we simulated the steady-state activation properties of TMEM16A using the IonChannelLab software [44] along with the rate constants previously determined with IChMASCOT. The experimental conditions to be tested such as $[Ca^{2+}]_i$,

$[Cl^-]_o$, $[Cl^-]_i$, and V_m were included. To determine the most likely activation pathway, we calculated the probability (P) that TMEM16A stayed in a given state of a chosen gating kinetic model. For that purpose, the differential equations describing the time dependence of P (Equations 1 – 12 in Supplemental material) were numerically integrated using the Gear's BDF method. P was calculated for 20 s depolarizations with 0.2 μM $[Ca^{2+}]_i$, 140 mM and 30 mM $[Cl^-]_o$ and 40 mM $[Cl^-]_i$ and for 1 s depolarizations with 0 μM $[Ca^{2+}]_i$, 140 mM and 30 mM $[Cl^-]_o$ and 40 mM $[Cl^-]_i$ using the rate constants listed in Table 2.

Figures and fits were constructed using Origin (Origin Lab, Northampton, MA). Data were plotted as mean \pm SEM of n (number of independent experiments). Dashed black lines and arrows in each Figure indicate $I_{Cl}=0$. Where necessary, a Student t-test was used to evaluate statistically significant differences between data sets at $P<0.05$; as indicated by the * symbol.

RESULTS

Here we characterized the effects of V_m and $[Cl^-]_o$ on TMEM16A gating. We used these data to build a kinetic model to explain the contribution of V_m , Ca^{2+} , and Cl^- to TMEM16A gating. Finally, using the model we predict the most likely pathway taken by the channel during activation.

Activation of TMEM16A in the absence of intracellular Ca^{2+}

Under physiological conditions, CaCCs are activated by depolarization and increases in $[Ca^{2+}]_i$ [2, 27, 31, 35]. However, TMEM16A can be activated even when no Ca^{2+} is present on the cytosolic side [49]. Here we recorded whole cell Cl^- currents (I_{Cl}) in the absence of intracellular Ca^{2+} (with 25.2 mM EGTA). I_{Cl} displays fast onset kinetics and lacks an inward tail (I_{tail}) current upon repolarization to -100 mV (Figure 1A, black traces). The current is inhibited with 100 μM tannic acid, a TMEM16A blocker (Figure 1A, bottom panel). To strengthen the assertion that the current was carried through TMEM16A in the absence of intracellular Ca^{2+} , we replaced external Cl^- with SCN^- , a more permeable anion that accelerates opening and retards channel closing [36, 49]. Figure 1B shows representative current traces recorded at $+160$ mV from a cell bathed first with 140 mM Cl^- then 140 mM SCN^- . This manoeuvre increased the current (Figures 1B and 1C, triangles), consistent with SCN^- permeating through TMEM16A. However, we could not determine a definite reversal potential of the current in zero $[Ca^{2+}]_i$ to calculate the permeability ratio P_{SCN}/P_{Cl} . In contrast, I_{Cl} was negligible at every V_m in cells transfected with an empty vector (Figure 1D). These results indicate that the I_{Cl} recorded in zero Ca^{2+} is flowing through TMEM16A activated by V_m and not through some other endogenous conductance.

Cl^- -dependence of TMEM16A gating

To analyse the effect of extracellular Cl^- we recorded I_{Cl} at different $[Cl^-]_o$. Figure 2A shows examples of I_{Cl} recorded from the same cell dialyzed with an IS containing 0.2 μM $[Ca^{2+}]_i$, 40 mM $[Cl^-]_i$, that was sequentially exposed to 140 mM, 70 mM and 10 mM $[Cl^-]_o$. The I_{Cl} magnitude decreased when $[Cl^-]_o$ was reduced. This is summarized in the I_{Cl} vs V_m curves in Figure 2B. Since reduction of $[Cl^-]_o$ from 140 mM to 10 mM increased the driving

force ($V_m - V_{rev}$) from -92.6 ± 2.5 mV to -146.2 ± 4.6 mV, we expected a 1.6-fold increase in I_{tail} amplitude at -100 mV. However, I_{tail} in 10 mM Cl^- did not increase; instead it fell drastically; the mean $I_{tail_10mM}/I_{tail_140mM}$ ratio was 0.78 ± 0.05 ($n=7$). The time constant values of I_{tail} at -100 mV after the pre-pulse to $+160$ mV were 47 ± 4 ms and 43.7 ± 3.1 ms with 140 mM and 10 mM $[Cl^-]_o$, respectively, indicating no change in kinetics. When the conductance was calculated using the current magnitude at the end of each pulse and normalized using the value at $+120$ mV (G_{Norm}), we observed a 5-fold conductance drop at each V_m (Figure 2C) when $[Cl^-]_o$ was reduced from 140 mM to 10 mM. Thus, at low external $[Cl^-]_o$ the apparent open probability of TMEM16A declines.

To determine the effects of $[Cl^-]_o$ on time-dependent activation we recorded I_{tail} from the same cell sequentially exposed to 140, 109, 70, 30, 10 and 1.5 mM. The cells were dialyzed with an IS containing $0.2 \mu M Ca^{2+}$ and 40 mM Cl^- . Figure 3A shows representative recordings. Tail currents were obtained at -100 mV after a $+120$ mV depolarization as shown in the voltage protocol. In this case, we lengthened the depolarization from 0.5 s to 3 s in 0.5 s increments. At 140 mM $[Cl^-]_o$ the I_{tail} amplitude (indicated by arrows) increased with longer pulses. In contrast, with 10 mM $[Cl^-]_o$ the I_{tail} magnitude was smaller. This finding could be explained if gating is dependent on $[Cl^-]_o$. In Figure 3B, G_{Norm} at the indicated $[Cl^-]_o$ is plotted as a function of pulse duration. The graph shows that decreasing the $[Cl^-]_o$ from 140 mM to 10 mM produces a 3-fold reduction in G_{Norm} . A 5-fold decrease in G_{Norm} is observed when comparing 140 mM with 1.5 mM $[Cl^-]_o$. At $[Cl^-]_o = 30$ mM, G_{Norm} levelled off and the G_{Norm} vs time curves were described by a single exponential function (solid lines) with $\tau = 293.7 \pm 17$ ms and 334 ± 19.6 ms for 1.5 mM and 10 mM $[Cl^-]_o$, respectively. However, with $[Cl^-]_o > 30$ mM, only the initial part (time < 0.5 s) of the curves was described by a single exponential because as pulse duration increased G_{Norm} rose in an almost linear fashion. $\tau = 368.2 \pm 23$ ms and 353.4 ± 23.1 ms for 109 mM and 140 mM $[Cl^-]_o$, respectively.

In cells bathed with a solution containing 140 mM or 30 mM $[Cl^-]_o$ we extended the duration of the V_m pulses to 20 s and found that I_{Cl} displayed a second mode of gating, something we previously reported [11]. Figure 3C shows that the conductance was reduced nearly 22-fold upon switching from 140 mM to 30 mM $[Cl^-]_o$ (note the scale bar is 10-times smaller for 30 mM $[Cl^-]_o$). At 140 mM $[Cl^-]_o$ (left) the $G_{Norm}(t)$ at $+140$ mV continuously increased for the entire 20 s pulse duration. The time course had a fast ($\tau_f = 448.1 \pm 26.3$ ms) onset followed by a slower rise ($\tau_s = 19.1 \pm 3.8$ s). The contributions of the fast and slow components were 0.17 ± 0.04 and 0.83 ± 0.04 , respectively. With 30 mM $[Cl^-]_o$, $G_{Norm}(t)$ was described by a τ_f of 368.6 ± 55.5 ms and τ_s of 6.2 ± 1.5 s; however, the fractional contribution of the fast and slow phases were reversed: 0.92 ± 0.1 and 0.08 ± 0.1 , respectively. These observations reinforce the conclusion that TMEM16A gating depends on $[Cl^-]_o$. We next asked if the Cl^- effect on gating would also occur in the presence of high $[Ca^{2+}]_i$, a condition that maximally activates TMEM16A [49]. To test this, we recorded I_{Cl} from cells dialyzed with $5 \mu M [Ca^{2+}]_i$. Figure 3D shows a trace obtained by averaging the current from 8 cells that were bathed in 140 mM $[Cl^-]_o$ and depolarized to $+100$ mV for 20 s and then repolarized to -60 mV. Under these conditions, I_{Cl} did not display dual gating, instead the current had a monoexponential time course with τ of 3.7 ± 0.36 s. Taken

together, our data demonstrate that TMEM16A gating is dependent on external Cl^- but the Cl^- effects are attenuated when high $[\text{Ca}^{2+}]_i$ activates the channel.

Kinetic analysis of TMEM16A gating

The data in Figures 1, 2 and 3 as well as evidence cited in the Introduction highlight the complexity of TMEM16A activation. In an effort to have an integrated view of the activation mechanism we constructed a kinetic model that takes into account the V_m , Ca^{2+} , and $[\text{Cl}^-]_o$ dependencies of TMEM16A. Scheme IV in Figure 4 presents a 12-state model with 26 free parameters that satisfactorily reproduce the V_m , Ca^{2+} and Cl^- dependencies of channel activation. The model was built based on the following experimental data and assumptions:

1. TMEM16A can be activated by V_m in the absence of intracellular Ca^{2+} and the presence of extracellular Cl^- as shown in Figure 1 (see also [49]).
2. Intracellular Cl^- plays no role in TMEM16A activation. This observation is based on experiments where the V_m -dependence of TMEM16A was nearly identical in the presence of 40 and 88 mM $[\text{Cl}^-]_i$ (data not shown).
3. TMEM16A can be activated in a cooperative way by V_m , intracellular Ca^{2+} , and Cl^- (Figures 2 and 3).
4. The interaction between intracellular Ca^{2+} and TMEM16A is a V_m -dependent process [49].
5. Binding of at least 2 Ca^{2+} ions activates TMEM16A as suggested by dose-response curves and structural data [5, 17, 35, 49, 52].
6. Binding of the two Ca^{2+} ions occurs in a sequential manner with the same single site-affinity.

Activation of TMEM16A by V_m in cells dialyzed with 0 μM $[\text{Ca}^{2+}]_i$ (Figure 1) was described as a simple closed-open ($\text{C} \rightleftharpoons \text{O}$) transition. This condition is represented by Scheme I in Figure 4 where α_1 and β_1 are forward and backward rate constants (Equation 4) that change exponentially with V_m [15, 16].

In the presence of Cl^- , a channel dwelling in C or O states can bind Cl^- and move into C_{Cl} and $\text{C}_{\text{Cl}}\text{O}$ states (see Scheme II(A) in Figure 4). The rate constants $[\text{Cl}^-]_o k_{\text{CCl1}}$, k_{CCl2} , $[\text{Cl}^-]_o k_{\text{OCl1}}$, and k_{OCl2} control the $\text{C} \rightleftharpoons \text{C}_{\text{Cl}}$ and $\text{O} \rightleftharpoons \text{C}_{\text{Cl}}\text{O}$ transitions in the presence of external Cl^- , while α_{Cl1} and β_{Cl1} control the $\text{C}_{\text{Cl}} \rightleftharpoons \text{C}_{\text{Cl}}\text{O}$ transitions. A subsequent increase in intracellular Ca^{2+} will drive the channel into one of the following states: $\text{C} \rightleftharpoons \text{C}_{\text{Ca}}$, $\text{O} \rightleftharpoons \text{C}_{\text{Ca}}\text{O}$, $\text{C}_{\text{Cl}} \rightleftharpoons \text{C}_{\text{Cl}}\text{C}_{\text{Ca}}$ and $\text{C}_{\text{Cl}}\text{O} \rightleftharpoons \text{C}_{\text{Cl}}\text{O}_{\text{Ca}}$ (see Scheme III(A), Figure 4). These transitions are controlled by forward rate constants $[\text{Ca}^{2+}]_i k_{\text{C1}}$, $[\text{Ca}^{2+}]_i k_{\text{C1Cl}}$, $[\text{Ca}^{2+}]_i k_{\text{O1Cl}}$ and $[\text{Ca}^{2+}]_i k_{\text{O1}}$ and backward rate constants k_{C2} , k_{C2Cl} , k_{O2Cl} and k_{O2} (described by Equation 4). Previous fast perfusion experiments show that upon Ca^{2+} removal the current deactivates in a V_m -dependent manner [49]. Therefore, only the rate constants controlling unbinding of Ca^{2+} , k_{O2} , k_{C2} , k_{C2Cl} and k_{O2Cl} are V_m -dependent. The rate constants controlling Ca^{2+} -binding are V_m -independent. Depending on their permeability anions can facilitate channel activation [36] and decrease the amount of Ca^{2+} needed to produce half-maximum activation [4, 39]. Based on this we introduced an effect of Ca^{2+} on the rate constants (k_{CCl} and k_{OCl})

controlling the $C \rightleftharpoons C_{Cl}$ and $O \rightleftharpoons C_{Cl}O$ transitions. This effect of Ca^{2+} is represented in the model by weight parameters I, L, h, H, m and M . Table 2B lists the relationship between rate constants and weight factors. Finally, the Ca^{2+} dose-response curves suggest that at least two Ca^{2+} are needed to activate TMEM16A [2, 27, 35, 47, 49, 52]. The binding of an additional Ca^{2+} to the channels leads to Scheme IV. In this new scheme we presuppose that: 1) the open and closed state can bind Ca^{2+} with different affinity, and 2) within each state both Ca^{2+} ions bind with the same single site affinity.

Alternatively, when both intracellular Ca^{2+} and Cl^- are present, a channel dwelling between C and O states (Scheme I) can bind two Ca^{2+} ions to move into Schemes II(B) and III(B), respectively. The transitions between C and O states are controlled by rate constants $[Ca^{2+}]_i k_{Cl}, k_{C2}, [Ca^{2+}]_i k_{O1}$ and k_{O2} . Next binding of one external Cl^- to channels in Scheme III(B) leads to Scheme IV. Note that binding of just one Cl^- by channels represented in Scheme II(B) leads to Scheme III(A). Since Cl^- permeates through the channel, then we do not expect that all cycles of Scheme IV will satisfy microscopic reversibility. Cycles represented with states connected by wider arrows did not satisfy the reversibility principle.

The models depicted by Schemes III(A) and IV take into account the contribution of V_m , Ca^{2+} , and Cl^- to gating and hence can be used to describe the properties of TMEM16A. To test them we performed a global fit of data describing the V_m , Ca^{2+} , and Cl^- dependence of gating. The experimental data used in the global fits included:

1. I_{Cl} vs V_m curves obtained from cells dialyzed with 0 Ca^{2+} and 40 mM Cl^- and bathed in 140 mM or 30 mM Cl^- .
2. Mean I_{Cl} traces obtained from cell dialyzed with $[Ca^{2+}]_i = 0, 0.2$ and 1 μM and stepped to V_m ranging from -100 mV to 160 mV.
3. Representative I_{Cl} traces obtained by fast perfusion of 20 μM $[Ca^{2+}]_i$ to excised patches held at V_m from -100 mV to 100 mV in 20 mV increments.
4. Mean I_{Cl} recordings obtained from cells sequentially exposed to 1 mM, 10 mM and 140mM $[Cl^-]_o$.
5. Mean I_{Cl} recordings obtained from cells dialyzed with 0.2 μM $[Ca^{2+}]_i$ and 40 mM $[Cl^-]_i$ while bathed in 140 mM or 30 mM $[Cl^-]_o$ and depolarized to -20 mV to $+120$ mV for 20 s.

The inclusion of such a wide range of data in the global fit constrained the value for the rate constants and ensured the robustness of our model. The model depicted in Scheme III(A), which included only one Ca^{2+} bound, partially reproduced TMEM16A activation. It was not able to describe activation at very high $[Ca^{2+}]_i$, the kinetics of tail currents in cells dialyzed with 1 μM Ca^{2+} , or I_{Cl} generated with 20 s pulses from cells exposed to 30 mM Cl^- (Supplemental Figures 1 and 2). In contrast, Scheme IV, which included two Ca^{2+} ions bound, described the data reasonably well. The results are shown in Figures 5 and 6 as solid black traces (fits) superimposed on the experimental data (grey lines). Figures 5 A, B and C show fits of Scheme IV to I_{Cl} recorded from different cells dialyzed with 0, 0.2 and 1 μM $[Ca^{2+}]_i$. Figure 5D displays the fits of I_{Cl} generated by rapid perfusion with 20 μM $[Ca^{2+}]_i$ to inside-out patches held from -100 mV to $+100$ mV. The model fit the entire traces nicely.

The model was able to fit the fast onset of the currents recorded at 0 $[Ca^{2+}]_i$ (inset in A), the fast tail currents recorded with 0.2 μM Ca^{2+} (inset in B) and the fast on and off time courses of the current activated with 20 μM Ca^{2+} . However, the model did not describe well the tail current recorded with 1 μM Ca^{2+} (inset in C). Similarly, Scheme IV was able to fit the $I_{Cl}-V_m$ relationships obtained from cells exposed to 30 and then 140 mM $[Cl^-]_o$ in the absence of intracellular Ca^{2+} (Figure 6A, grey and black circles) and the I_{tail} recorded from different cells exposed to 10 and 1 mM $[Cl^-]_o$, dialyzed with 0.2 μM $[Ca^{2+}]_i$ and 40 mM $[Cl^-]_i$ (Figure 6B). Scheme IV also fitted the mean I_{Cl} recorded with 20 s depolarizations from cells exposed to 30 mM and 140 mM $[Cl^-]_o$ and dialyzed with 0.2 μM $[Ca^{2+}]_i$ and 40 mM $[Cl^-]_i$ (Figure 6C). Here we can see that the model described quite well I_{Cl} recorded in the presence of 140 mM Cl^- but not 30 mM Cl^- . Fast components, such as the tail currents (right insets in B and C) at both $[Cl^-]$ were well described. The overall global fit goodness of the model with the binding of Ca^{2+} to two sites with the same affinity (k_{O2}/k_{O1}), given by the regression coefficient (R^2) associated with the minimization process had a value of 0.98 (Equation 5). We also tested the alternative model that considers different Ca^{2+} affinities for the two Ca^{2+} binding sites: k_{O2}/k_{O1} for the first site and $c^* k_{O2}/k_{O1}$, for the second site, where c is a constant parameter. This model fits the data with the same $R^2=0.98$ as that obtained with Scheme IV with two sites with the same affinity. However, the binding affinities only varied by a factor of 0.61 and the V_m -dependence of EC_{50} was indistinguishable from that obtained assuming the same affinity. Therefore, we consider that Scheme IV with two Ca^{2+} binding sites with the same affinity was a reasonable model of TMEM16A and can be used to obtain the rate constant parameters and the apparent charge (z) values for Scheme IV. Table 2 lists these values. The z values indicate that most of the V_m -dependence is conferred by: a) the charge transferred during the Ca^{2+} unbinding steps controlled by k_{O2} ($z=0.168$), b) the transition $C_{Cl} \rightleftharpoons O_{Cl}$ controlled by α_{C11} ($z=0.11$) and β_{C11} ($z=0.32$), and c) the Cl^- binding steps to C or O conformations controlled by k_{CC11} ($z=0.2$) and k_{OC1} ($z=0.65$), respectively.

If these global fits are a realistic representation of TMEM16A gating, then Scheme IV plus the set of parameter values listed in Table 2 should be able to predict the quasi-steady-state properties of TMEM16A. These properties include $I_{Cl}-V_m$ curves, Ca^{2+} dose-response curves, and the V_m -dependence of EC_{50} and the Hill coefficient. We chose these fingerprint properties because they have been well characterized by different laboratories [2, 19, 27, 31, 32, 35]. Our approach consisted of simulating TMEM16A currents under different $[Ca^{2+}]_i$ and V_m using IonChannelLab software [44] as described in Methods. Then we used the simulated I_{Cl} to construct $I_{Cl}-V_m$ curves and Ca^{2+} dose-response curves. To make a stringent comparison, we compared the simulated properties to previously published data [49]. Data was from cells dialyzed with $[Ca^{2+}]_i$ ranging from 0 to 6.5 μM , and stimulated with 0.7 s pulses from -100 mV to $+100$ mV. Figure 7 shows superimposed experimental data (black symbols) and model predictions (solid lines) for I_{Cl} vs V_m relationships at the indicated $[Ca^{2+}]_i$ (Figure 7A), dose-response curves to $[Ca^{2+}]_i$ at different V_m (Figure 7B), and V_m -dependence of EC_{50} and the Hill coefficient n_H (Figure 7C). These properties of TMEM16A, except the EC_{50} , were adequately predicted by Scheme IV and its associated rate constants. Nevertheless, the EC_{50} value predicted by the model at $+60$ mV/140 mM

$[Cl^-]_o$ was 0.85 μM , which is within the range of values determined experimentally [2, 17, 22, 35, 49].

Finally, it has been shown that anions more permeable than Cl^- modify CaCC and TMEM16A gating [36, 49]. Importantly, anions more permeable than Cl^- increase the apparent Ca^{2+} sensitivity of TMEM16A and TMEM16B [4, 39]. In this work, we show that increasing $[Cl^-]_o$ facilitates gating, but whether or not this effect is due to an increased Ca^{2+} sensitivity is unknown. Therefore, we used the model to predict whether extracellular Cl^- regulates TMEM16A gating by altering its Ca^{2+} or voltage sensitivity. Dose-response curves to Ca^{2+} were calculated using Scheme IV with 140 mM or 30 mM $[Cl^-]_o$ and $V_m = +60/-60$ mV. The model predicts that neither the apparent Ca^{2+} sensitivity nor the V_m -dependence of EC_{50} are altered by decreasing $[Cl^-]_o$. To determine whether this prediction is true, we determined the dose-response curves to Ca^{2+} for TMEM16A using inside-out patches held at ± 60 and ± 80 mV in 140 mM or 30 mM $[Cl^-]_o$. Figures 8A and 8B show typical raw I_{Cl} traces obtained from two different patches bathed in 140 mM (A) and 30 mM (B) Cl^- while the $[Ca^{2+}]_i$ was changed between zero and the concentrations indicated by the small letters. Upward deflections are records obtained at +60 mV while downward deflections are records obtained at -60 mV. Clearly I_{Cl} at +60 mV saturated when $[Ca^{2+}]_i$ was around 5–12 μM regardless of the $[Cl^-]_o$ present. At -60 mV, I_{Cl} nearly saturated with 12 μM $[Ca^{2+}]_i$. Figure 8C shows the resulting dose-response curves at +60 mV (left) and at -60 mV (right). The data (black and grey circles) nicely matched the values predicted by Scheme IV (solid lines). Furthermore, the predicted V_m -dependence of EC_{50} was also matched by the experimental data (continuous lines and symbols in Figure 8D). The EC_{50} value of 0.85 μM predicted by the model at +60 mV and 140 mM $[Cl^-]_o$ was similar to those experimentally reported: 1.5, 1.3, 0.4, 1.5, and 0.79 ± 0.05 μM [27, 46, 48, 49, this work]. Taken together these results demonstrate that external Cl^- does not alter Ca^{2+} -sensitivity in TMEM16A. The fact that our kinetic model predicted this result is a good indication of the model robustness and that the model includes critical information about the mechanism of TMEM16A gating.

Activation pathways

Since Scheme IV was able to reproduce the activation properties of TMEM16A, we decided to apply the model to determine what would be the most likely pathway(s) followed by TMEM16A during the activation process. For this purpose, we calculated the probability (P) that TMEM16A visited each of the 12 states when intracellular Ca^{2+} , external Cl^- , and V_m were varied (Supplemental material). To obtain a gating pathway we determined the most likely state to be occupied once the channel visited a given state. For example, when the channel visits state C, it can go to O, C_{Cl} or C_{Ca} states. Our P value calculations indicated that state C_{Ca} was the most likely state to be occupied. We repeated this strategy to find the next most probable state to be visited until the channel reached ClO_2Ca . First, we consider activation of TMEM16A by a 0.5 s depolarization to +120 mV followed by repolarization to -60 mV when $[Ca^{2+}]_i = 0$, $[Cl^-]_i = 40$ mM and $[Cl^-]_o$ changed between 140 mM and 30 mM. This condition is represented by the pink kinetic scheme box in Figure 9C. The time-dependent P values for states C, O, C_{Cl} , and ClO are shown in Figure 9A. P_C , P_O , $P_{C_{Cl}}$ and P_{ClO} values were 0.782, 0, 0.217 and 0.0008, when $[Cl^-]_o$ was 140 mM. After external Cl^- was decreased to 30 mM P_C increased to 0.941, while $P_{C_{Cl}}$ and P_{ClO} fell to 0.057 and

0.0002, respectively. Thus, in the absence of intracellular Ca^{2+} the most likely gating route is $\text{C} \rightarrow \text{C}_{\text{Cl}} \rightarrow \text{C}_{\text{ClO}}$ (Figure 9C, blue and pink arrows).

Subsequently, P values were calculated when $[\text{Ca}^{2+}]_i$ was 0.2 μM , $[\text{Cl}^-]_o$ was either 140 or 30 mM, $[\text{Cl}^-]_i = 40$ mM, and V_m was +120 mV during 20 s followed by repolarization to -60 mV. These experimental conditions are the same as the ones used for collecting data shown in Figure 3C (right) and data collected using short depolarizations. Figure 9B shows P values for states in the inner circle (pink), middle circle (white), and outer circle (grey), respectively. When $[\text{Cl}^-]_o$ was 140 mM (left column), the depolarization induced an abrupt decrease of P_{C} , followed by a further exponential decrease. Such decrease was mirrored by an abrupt increase and then exponential decrease in P_{CCa} . At the same time, $P_{\text{C}_{\text{ClO}}\text{Ca}}$ and $P_{\text{C}_{2\text{Ca}}}$ increased little, and $P_{\text{O}_{2\text{Ca}}}$ increased transiently. Notably, $P_{\text{C}_{\text{ClO}}\text{O}_{2\text{Ca}}}$ increased steadily reaching 0.4 by the end of the 20 s depolarization. The same trend was observed when $[\text{Cl}^-]_o$ was 30 mM, albeit the magnitude of P for each state declined. Interestingly, during the first 2 s into the depolarization $P_{\text{C}_{\text{Cl}}\text{C}}$ decreased but then increased in a time-dependent manner. In summary, in the presence of 0.2 μM $[\text{Ca}^{2+}]_i$ and 140 mM or 30 mM $[\text{Cl}^-]_o$, TMEM16A activation proceeded following two pathways. At early times (<2 s), the route $\text{C} \rightarrow \text{C}_{\text{Ca}} \rightarrow \text{C}_{2\text{Ca}} \rightarrow \text{O}_{2\text{Ca}} \rightarrow \text{C}_{\text{ClO}}\text{O}_{2\text{Ca}}$ (black arrow) was preferred. However, as depolarization continued, the route $\text{C} \rightarrow \text{C}_{\text{Cl}}\text{C} \rightarrow \text{C}_{\text{Cl}}\text{C}_{\text{Ca}} \rightarrow \text{C}_{\text{Cl}}\text{O}_{\text{Ca}} \rightarrow \text{C}_{\text{Cl}}\text{O}_{2\text{Ca}}$ (green arrow) also contributed to the total current. The effect of lowering $[\text{Cl}^-]_o$ to 30 mM was to decrease the contribution of both routes to the total current (grey and light green arrows). From these calculations, we observed that the greatest contribution to the total current is given by the active states $_{\text{Ca}}\text{O}_{\text{Cl}}$, $_{2\text{Ca}}\text{O}$ and $_{2\text{Ca}}\text{O}_{\text{Cl}}$. Therefore the net effect of increasing chloride from 30 to 140 mM was to increase $P_{_{\text{Ca}}\text{O}_{\text{Cl}}}$ and $P_{_{2\text{Ca}}\text{O}_{\text{Cl}}}$.

DISCUSSION

CaCC gating is a complex process; it involves the combined action of V_m , Ca^{2+} and Cl^- . Several kinetic models have been previously proposed to explain the V_m and Ca^{2+} -dependence of CaCC gating [2, 20, 27]. However, these early models assumed an initial Ca^{2+} -dependent $\text{C} \rightleftharpoons \text{C}_{\text{Ca}}$ transition and did not consider a $\text{C} \rightleftharpoons \text{O}$ transition in the absence of Ca^{2+} or the role of external Cl^- in gating. These models predict an open probability of zero at any V_m if $[\text{Ca}^{2+}]_i = 0$, which is not the case for TMEM16A [49]. In this work, we present an alternative kinetic model that satisfactorily accounts for the V_m , Ca^{2+} , and Cl^- -dependent gating of TMEM16A channel. We propose that the gating of the TMEM16A Cl^- channel is caused by consecutive direct V_m -dependent binding of two intracellular Ca^{2+} ions, coupled to a V_m -dependent binding of external Cl^- . External Cl^- facilitates gating by binding to a Ca^{2+} -free closed state and favouring the transition to Ca^{2+} -bound open states. By means of facilitating the $_{2\text{Ca}}\text{O} \rightleftharpoons _{2\text{Ca}}\text{O}_{\text{Cl}}$ transition, external Cl^- induces the slow gating [11]. In our model (Scheme IV) the direct Ca^{2+} -binding is controlled by forward rate constants that are independent of voltage and V_m -dependent backward rate constants. The off-rate constant measured from simulations with the model predicted that Ca^{2+} remains attached to the channel at depolarized voltages. This coincides with experimental data showing that at depolarized V_m the rate of current decay—due to Ca^{2+} washout—is very slow compared to that observed at negative V_m . Also, increasing the $[\text{Ca}^{2+}]_i$ decreases the off rate of whole cell currents at negative potentials [2, 27, 52]. Such data show that Ca^{2+}

unbinding is a V_m -dependent phenomenon [19, 27, 35, 49, 52]. Thus, the open state is stabilized when Ca^{2+} is high, and/or V_m is depolarized.

The model is not perfect. It cannot describe well I_{tail} recorded with $1 \mu M Ca^{2+}$ and I_{Cl} recorded in the presence of $30 mM Cl^-$ using $20 s$ depolarizations. Also, the EC_{50} is not adequately predicted by Scheme IV. There are different possibilities to explain these discrepancies. The rate constants are relatively simple; they are exponential functions of V_m and depended linearly on $[Cl^-]_o$. However, such dependence could be state dependent and/or be more complicated. The weight factors (l , L , h , H , m , and M) are assumed to be constant and we considered that only one Cl^- ion is needed affect channel gating without affecting the single channel conductance. These assumptions may not hold under all experimental conditions. Finally, for simplicity, we assumed that Ca^{2+} binds to two sites with a single binding affinity which we call single-site affinity. This may not be the case as suggested by mutagenesis experiments which show that mutations located in different parts of the protein alter Ca^{2+} sensitivity [17, 47, 49, 52]. Inadequacies of one or all these variables would hinder the ability of the model to reproduce the data. Refining the model to include the exact number of Ca^{2+} binding sites, their binding affinity and allosteric interactions with Cl^- would be more realistic as more structural data becomes available. In addition, our model ignores the permeation process. Including this property would be necessary to understand the effects of pore occupancy by permeant anions on channel gating [4, 36, 39]. Despite these limitations, Scheme IV predicted no change in the apparent Ca^{2+} affinity of TMEM16A when $[Cl^-]_o$ was lowered from $140 mM$ to $30 mM$, and this prediction was successfully corroborated experimentally. The model also predicts that a small fraction of the charge ($z_2 = 0.17$) is transferred during the Ca^{2+} unbinding steps. This number agrees with the small V_m -dependence of the dose-response curves to $[Ca^{2+}]_i$ [2, 22, 35, 49]. We consider that Scheme IV was effective because a large data set was used to extract the rate constant parameters. This tactic largely constrained the possible values of the rate constant parameters and contributed to enhance the robustness of the model.

The effect of external Cl^- on CaCCs is maybe more complex than previously anticipated since our data show that varying external Cl^- alters both the fast and slow gating modes of TMEM16A and TMEM16B [11]. In addition, our model-dependent calculations using the rate constants listed in Table 2 revealed that external Cl^- ion plays a significant role on V_m -dependent activation in the absence of Ca^{2+} . Under this condition, there is a substantial amount of charge transferred during the Cl^- binding steps to either C or O conformations as indicated by $z_{+Cl} = 0.2$ and $z_{+O} = 0.65$ (Table 2A). The binding of one Cl^- to the C conformation of the channel prompts its conversion into C_1C and subsequently the C_1O state. The later transition is also accompanied by charge transferred as indicated by $z_{11} = 0.11$ and $z_{12} = 0.33$ (Table 2). The C_1O state would enable Cl^- conductance in the absence of intracellular Ca^{2+} . Furthermore, when Ca^{2+} is bound to the channel the external Cl^- favours the ${}_{2Ca}O \rightleftharpoons {}_{2Ca}OCl$ transition and so the slow component of channel gating arises. In fact, by increasing $[Cl^-]_o$ from $30 mM$ to $140 mM$ in the presence of $0.2 \mu M [Ca^{2+}]_i$ we observed an increase in $P_{{}_{2Ca}OCl} + P_{{}_{Ca}OCl}$ from 0.08 to 0.22 , suggesting that Ca^{2+} remains bound to the channel for a longer time. Also, an increased occupation of the ${}_{2Ca}OCl$ state implies a longer dwell time of the channel in this state. High $[Cl^-]_o$ shifted to negative values the V_m -dependence of occupation for the ${}_{2Ca}OCl$ state such that at a given V_m the probability of

occupation is increased with high $[Cl^-]_o$. Despite these changes, the overall apparent affinity of TMEM16A for Ca^{2+} was not altered. However, previous experimental observations suggest a coupling of the permeation and gating mechanisms. For example, highly permeant anions alter the kinetics and EC_{50} as described for CaCC from mouse parotid acinar cells, *Xenopus* oocytes and TMEM16B [4, 36, 38, 39]. These data can be reconciled considering that TMEM16A may have two anion binding sites as previously suggested [38] and the external anions might alter TMEM16A gating by at least two mechanisms. One mechanism may involve permeation and gating, while another mechanism may affect only gating, similar to what we describe here. Our idea describes the effect of external Cl^- on TMEM16A based on what has been proposed for other Cl^- channels. For example, in CLC-0 and CLC-1 external anions have a profound facilitating effect on gating [7, 14, 37] and in CLC-2 V_m -dependence is conferred by permeant anions that occupy and then exit the pore [25, 41]. Thus, the role of permeant anions in gating the Cl^- channels may be more important than thought in the past. More research is needed to establish the connection between permeation and gating.

TMEM16A gating shares some similarities with BK channel gating. For example, both channels display coupling between V_m and Ca^{2+} binding, both channels are activated by V_m alone, and increments in $[Ca^{2+}]_i$ lead to a leftward shift of the $G_{Norm}(V_m)$ curve. However, there are also differences: BK has an intrinsic V_m sensor and TMEM16A does not, Ba^{2+} activates BK channels by interacting with the Ca^{2+} binding site but Ba^{2+} also binds and blocks the conduction pathway of BK channels while Ba^{2+} only activates TMEM16A [24, 33, 34, 49, 52, 53]. Allosteric models have been successful in explaining the interaction between V_m and Ca^{2+} in the gating of BK channels [24]. Although TMEM16A gating is not exactly like the gating of BK channels, an allosteric model should be considered for TMEM16A channel.

Our findings could be relevant to TMEM16A function under physiological conditions. For example, the model could be helpful to understand the behaviour of TMEM16A during agonist-stimulated Ca^{2+} -dependent fluid secretion. Secretory epithelial cells response to agonist include an oscillatory membrane potential accompanied by oscillations in the intracellular $[Ca^{2+}]_i$ [30]. Furthermore, during fluid and electrolyte secretion by acinar cells, $[Cl^-]_i$ decreases from about 61 to 29 mM [18] due to Cl^- exit through TMEM16A channels [40]. Under these conditions, Cl^- would transiently increase on the extracellular side which would favour activation of TMEM16A to sustain secretion. Although the TMEM16A activation pattern may very complex under physiological conditions, it can be understood using Scheme IV.

In summary, we propose a TMEM16A gating mechanism caused by consecutive direct V_m -dependent binding of two intracellular Ca^{2+} ions, coupled to a V_m -dependent binding of one external Cl^- .

Supplementary Material

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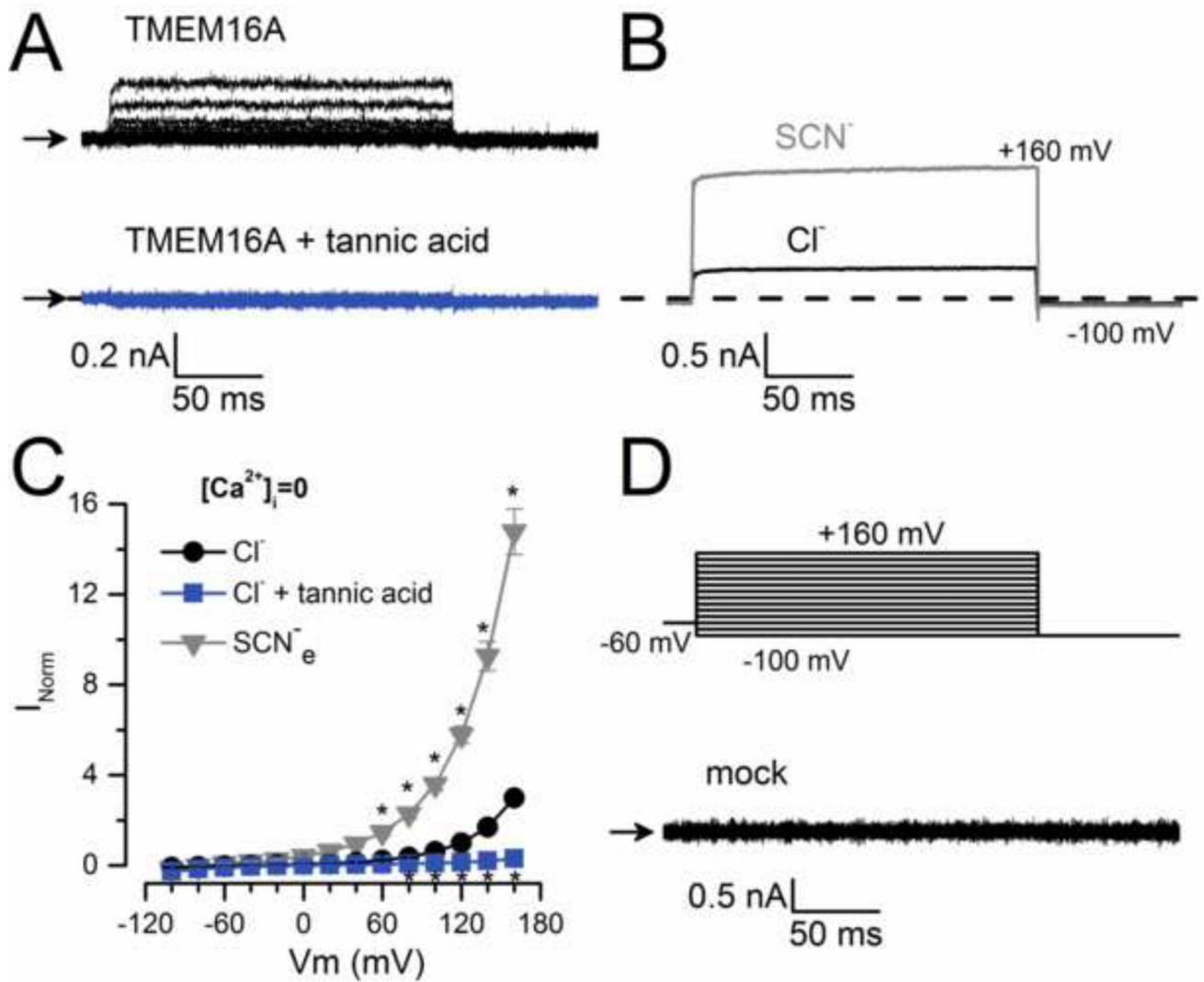


Fig. 1. Activation of TMEM16A in zero intracellular Ca²⁺

(A) Representative I_{Cl} recordings (n=5) obtained from HEK293 cells expressing TMEM16A, bathed in a solution containing 0 (black traces) or 100 μM tannic acid (grey traces). (B) Representative current traces (n=5) obtained from the same cell bathed in 140 mM Cl⁻ (black) or 140 mM SCN⁻ (grey). Currents evoked by pulses to +160 mV followed by repolarization to -100 mV. (C) I_{Cl}-V_m relationships from cells bathed in [Cl⁻]_o=140 mM (circles), [Cl⁻]_o=140 mM + 100 μM of tannic acid (squares), or 140 mM SCN⁻ (triangles). For each cell, whole cell currents were normalized to the current magnitude recorded at +120 mV from control cells bathed in [Cl⁻]_o=140 mM. Normalized currents from different cells were averaged and plotted. (D) Lack of I_{Cl} (n=6) in mock transfected cells dialyzed with a solution containing 40 mM [Cl⁻]_i. In A and D the [Cl⁻]_o was 140 mM and the I_{Cl} were generated using the protocol shown in D. In all experiments, cells were dialyzed with 0 μM [Ca²⁺]_i + 40 mM [Cl⁻]_i (IS-40Cl/0Ca).

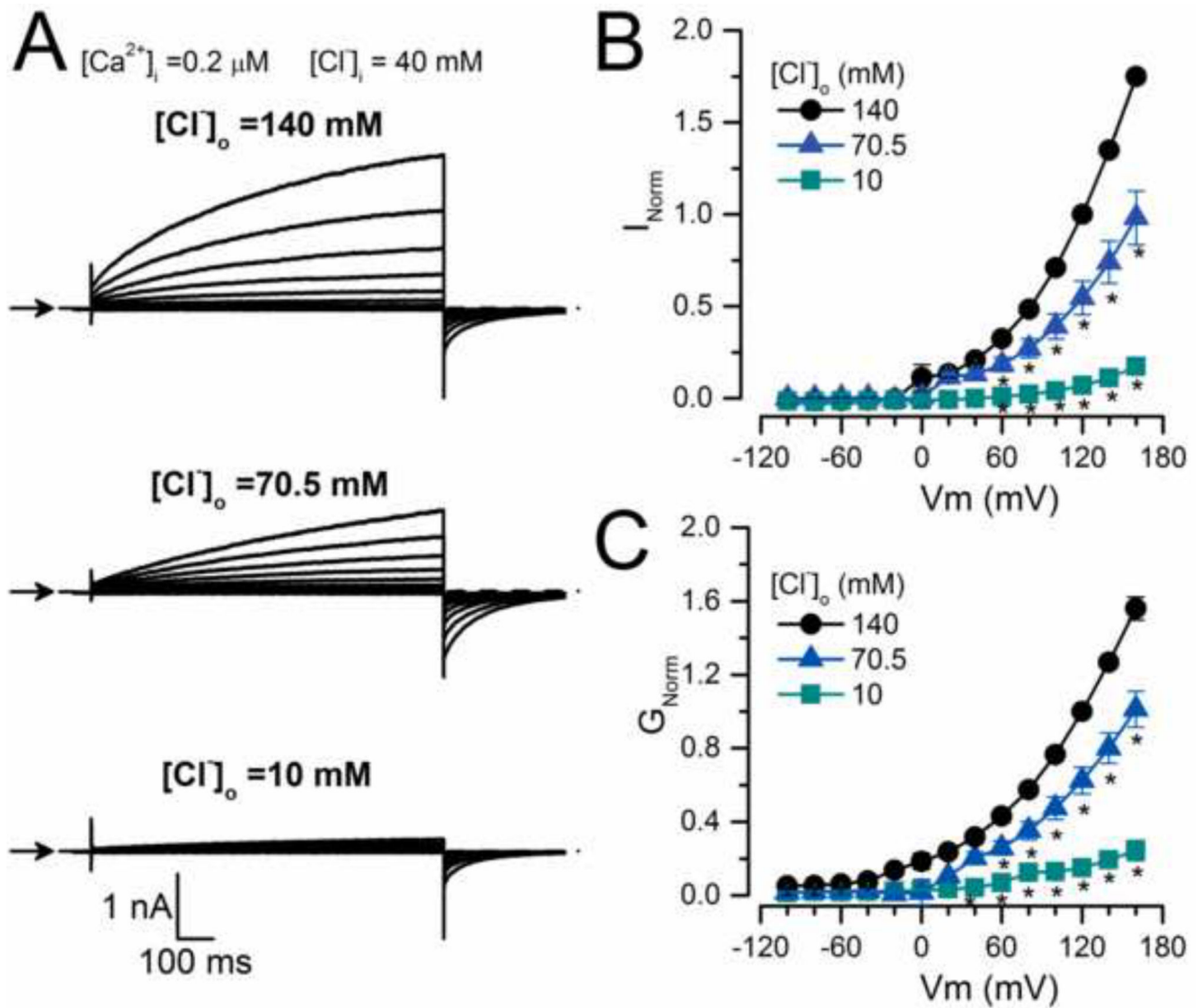


Fig. 2. TMEM16A chloride conductance depends on $[Cl^-]_o$

(A) Representative I_{Cl} recordings ($n=7$) obtained from the same cell sequentially bathed in ES containing 140, 70.5 and 10 mM $[Cl^-]_o$ and dialyzed with an IS containing $0.2 \mu M$ $[Ca^{2+}]_i$ + 40 mM $[Cl^-]_i$ (IS-40.5Cl/0.2Ca). Cells were held at -60 mV, then stepped for 0.5 s to voltages ranging from -100 mV to $+160$ mV in 20 mV increments and repolarised to -100 mV. Note that I_{tail} at -100 mV did not increase despite the increased driving force for Cl^- (i.e. driving force = -92.6 ± 2.5 mV with $[Cl^-]_o$ 140 mM and -146.2 ± 4.6 mV with 10 mM $[Cl^-]_o$). (B) I_{Cl} vs V_m relationships at the indicated $[Cl^-]_o$. (C) G_{Norm} vs V_m curves at the indicated $[Cl^-]_o$. I_{Cl} and G were normalized to either I_{Cl} or G obtained at $+120$ mV with $[Cl^-]_o=140$ mM. External solutions with different $[Cl^-]_o$ were prepared by mixing ES-136Cl and ES-1.5Cl.

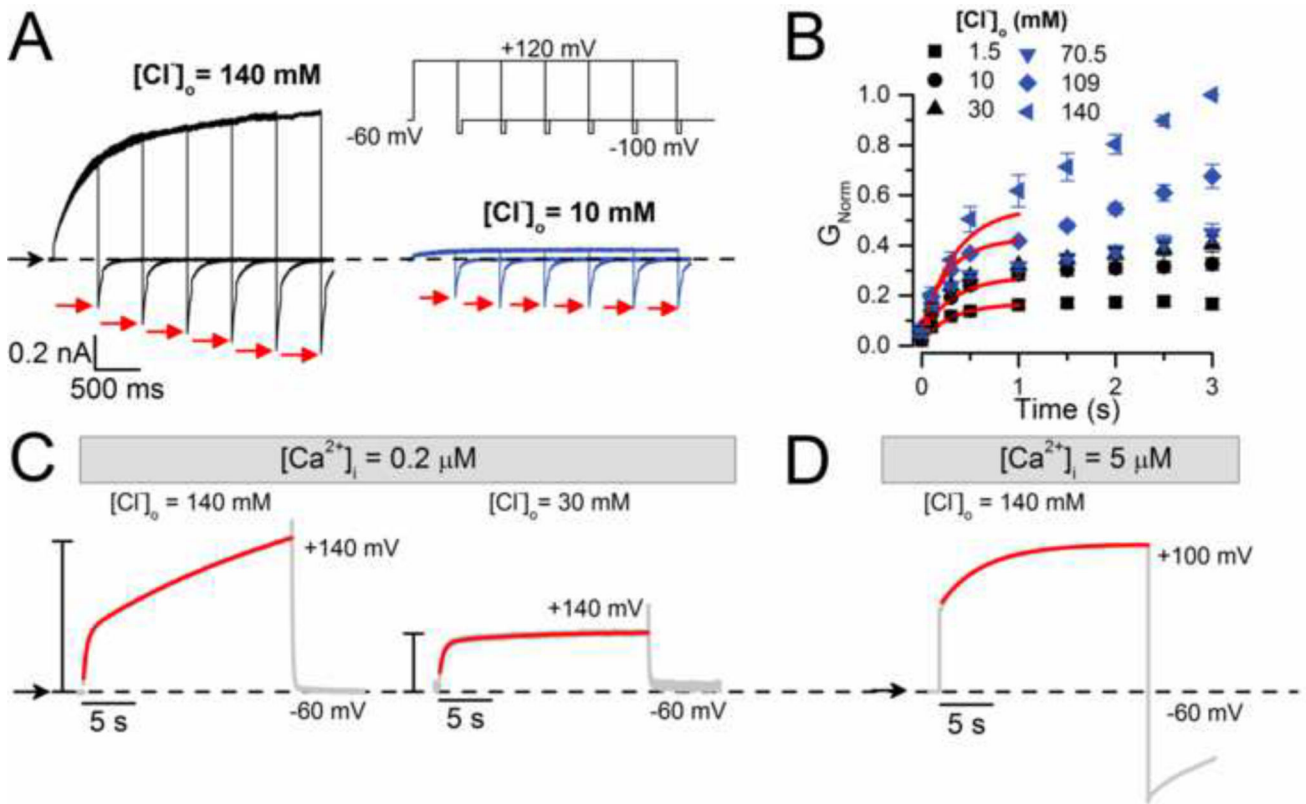


Fig 3. Extracellular Cl^- regulates TMEM16A gating

(A) I_{Cl} recordings from the same cell bathed in 140 mM (left) or 10 mM $[Cl^-]_o$ (right). I_{Cl} was recorded using the V_m protocol shown in the inset. The duration of the test pulse increased from 0 to 3 s in 0.5 s steps. Arrows indicate the peak current amplitudes at -100 mV. (B) The magnitude of I_{tail} recorded as in A was used to determine the conductance at each time and $[Cl^-]_o$ ($n=5$). G_{Norm} was calculated using the G obtained with $[Cl^-]_o=140$ mM and a 3s depolarization. Note that a single exponential can not describe the entire time course (continuous lines) when $[Cl^-]_o = 30$ mM. (C) $G_{Norm}(t)$ plots obtained from a cell stimulated with a 20 s depolarization to +140 mV and dialyzed with 0.2 μM Ca^{2+}_i (IS-40.5Cl/0.2Ca). The cell was exposed to 140 mM (left, ES-140Cl) and then to 30 mM (right, ES-30Cl) $[Cl^-]_o$. I_{Cl} was converted to $G(t)$ and then normalized using the G value at +140 mV to determine $G_{Norm}(t)$ at each $[Cl^-]_o$ ($n=4-8$). $G_{Norm}(t)$ plots were fit with a bi-exponential function (continuous lines) to obtain τ_s , τ_f and fractional contribution of each component. Note that the y-scale bar is 1 and 0.1 for 140 and 30 mM Cl^- , respectively. (D) TMEM16A- I_{Cl} recorded from cells dialyzed with 5 μM $[Ca^{2+}]_i$ (IS-40Cl/5Ca) and depolarized to +100 mV. I_{Cl} from each cell was normalized to I_{Cl} obtained with a 20 s depolarization and then normalized values were averaged ($n=8$). The continuous line is the fit to a mono-exponential function.

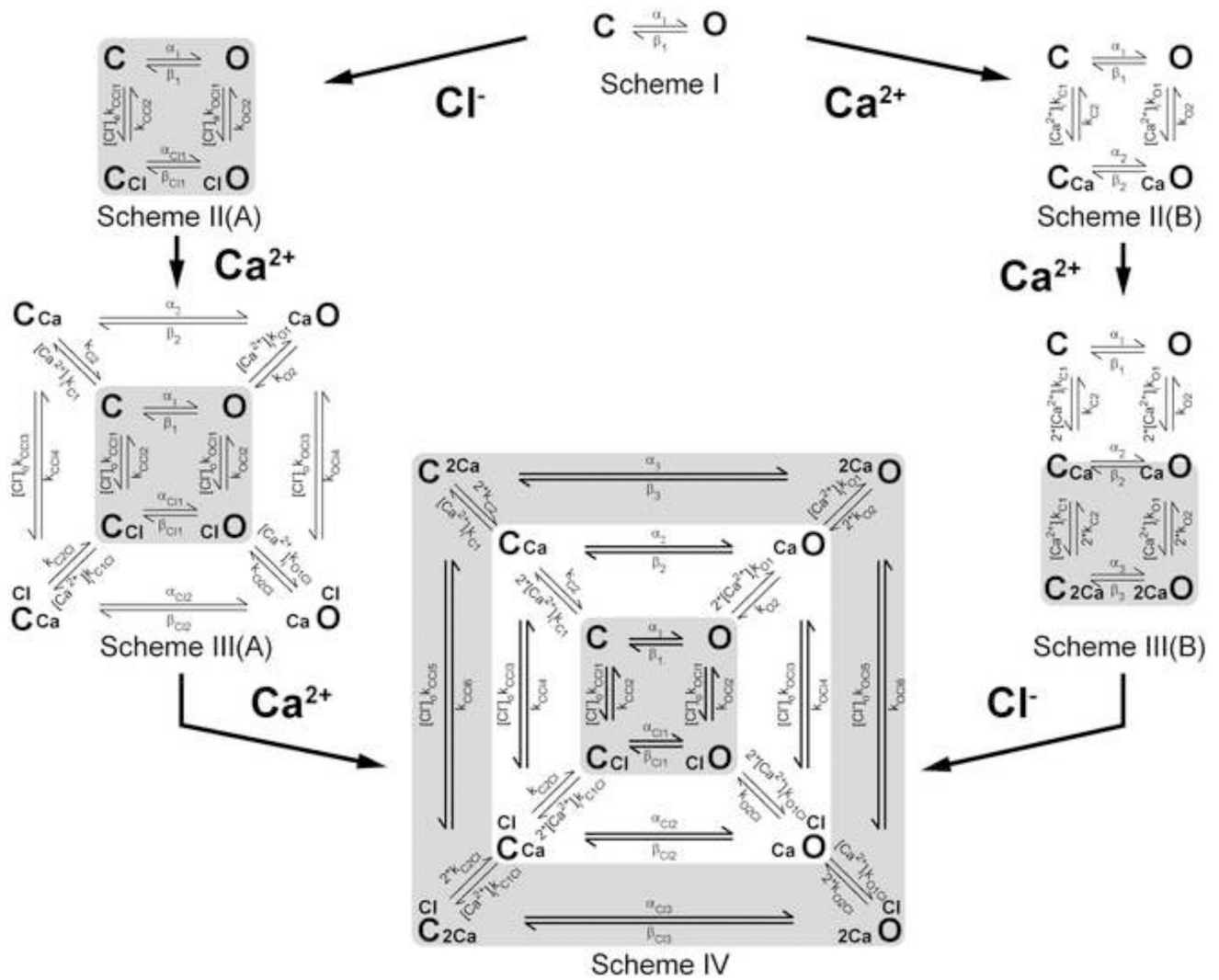


Fig 4. Kinetic model employed to explain the V_m , Ca^{2+} , and Cl^- contributions to TMEM16A gating

Scheme I represents V_m -dependent transitions in the absence of intracellular Ca^{2+} and external Cl^- . C and O are closed and open states, and α_1 and β_1 are V_m -dependent rate constants. **Scheme II(A)** represents the transitions in the presence of one external Cl^- when $[Ca^{2+}]_i = 0$. $[Cl^-]_o k_{CCl1}$ and $[Cl^-]_o k_{OC1}$ are rate constants controlling Cl^- association to C and O configurations, while k_{CCl2} , k_{OC12} rate constants control Cl^- dissociation. **Scheme III(A)** results after binding of one Ca^{2+} to states represented in **Scheme II(A)**. The $[Ca^{2+}]_i k_{O1}$, $[Ca^{2+}]_i k_{O1Cl}$, $[Ca^{2+}]_i k_{C1Cl}$ and $[Ca^{2+}]_i k_{C1}$ are Ca^{2+} association rate constants while k_{O2} , k_{O2Cl} , k_{C2Cl} and k_{C1} are Ca^{2+} dissociation rate constants. The subscript Cl indicates rate constants associated with Cl^- -occupied transitions. **Scheme II(B)** represents transitions resulting after binding of one intracellular Ca^{2+} to C and O states depicted in **Scheme I**. $[Ca^{2+}]_i k_{C1}$, $[Ca^{2+}]_i k_{O1}$ are rate constants controlling Ca^{2+} association to C and O configurations, while k_{C2} , k_{O2} rate constants control Ca^{2+} dissociation. **Scheme III(B)** represents the transitions resulting after binding of an additional Ca^{2+} to states shown in **Scheme II(B)**. Association and dissociation of the second Ca^{2+} was assumed to be same as

for the first Ca^{2+} binding reaction. **Scheme IV** results after binding of an additional Ca^{2+} to states shown in **Scheme III(A)**. The association and dissociation rate constants were the same as that for the first Ca^{2+} binding (left pathway). Alternatively, **Scheme IV** could be achieved after binding of one external Cl^- to states shown in **Scheme III(B)** with forward rate constants $[\text{Cl}^-]_o k_{\text{CC15}}$, $[\text{Cl}^-]_o k_{\text{CC13}}$, $[\text{Cl}^-]_o k_{\text{CC11}}$, $[\text{Cl}^-]_o k_{\text{OC11}}$, $[\text{Cl}^-]_o k_{\text{OC13}}$ and $[\text{Cl}^-]_o k_{\text{OC15}}$ and backward rate constants k_{CC16} , k_{CC14} , k_{CC12} , k_{OC12} , k_{OC14} and k_{OC16} . Concentric kinetic cycles with states connected by wider arrows indicate cycles that did not satisfy microscopic reversibility. Table 2A shows the Equations for each rate constant.

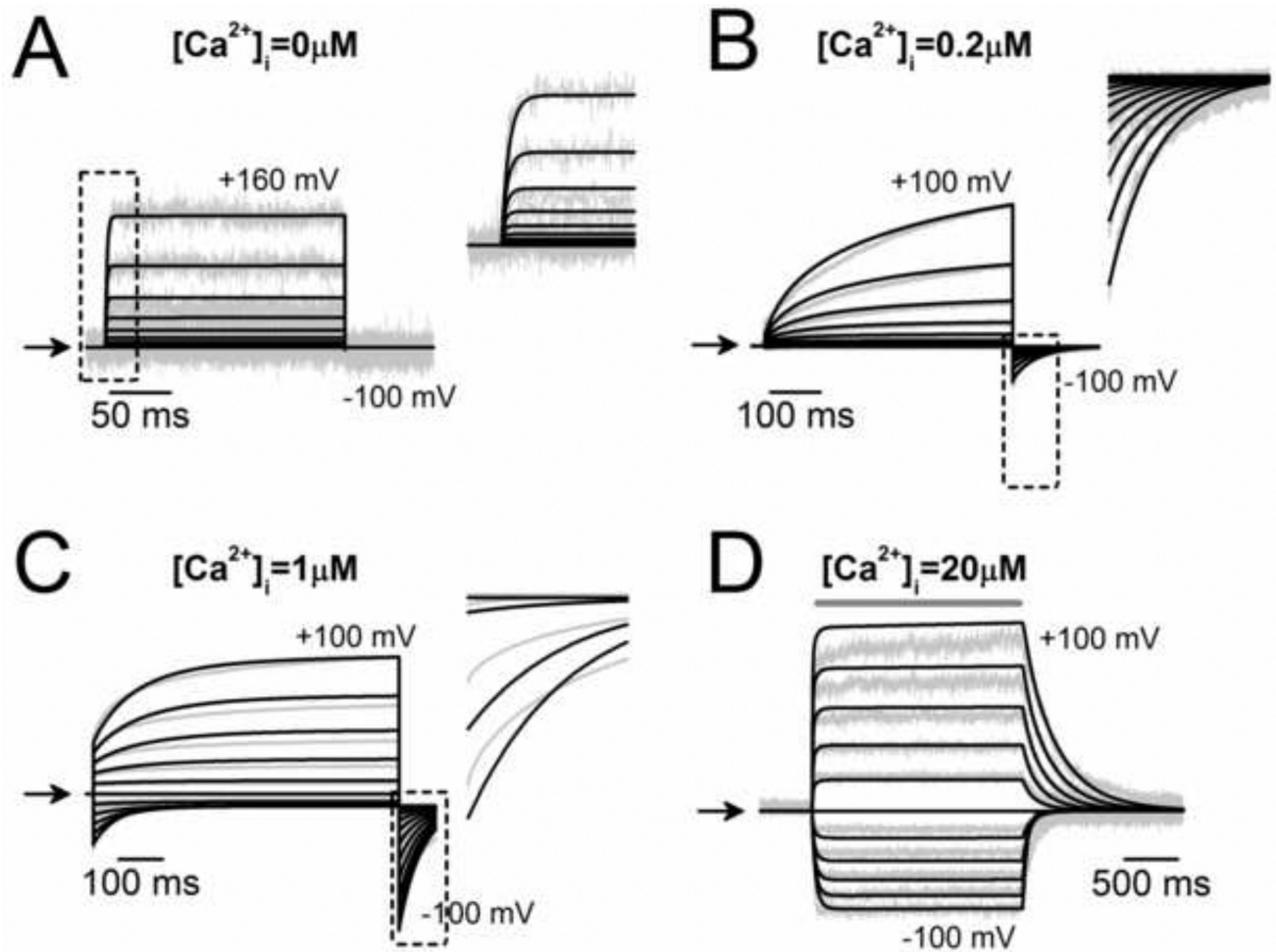


Fig 5. Global fit using Scheme IV to TMEM16A recordings obtained at different V_m and $[Ca^{2+}]_i$. Best fits were performed with the IChMASCOT software; solid lines are fits and grey lines are data. **(A–C)** Fits to I_{Cl} recordings obtained between -100 mV to $+100$ mV (20 mV increments) from cells dialyzed with 0 (A), 0.2 (B), or 1 (C) μM $[Ca^{2+}]_i$. **D** Best fits to data obtained by fast perfusion with 20 μM $[Ca^{2+}]_i$ to an inside-out patch held at V_m between -100 mV to $+100$ mV. The insets in A, B and C show magnified fits to fast phases of I_{Cl} enclosed in black squares. I_{Cl} shown in **A** and **B** were recorded from cells dialyzed with $[Cl^-]_i = 40$ mM; **C** and **D** were from cells exposed to symmetrical 140 mM Cl^- .

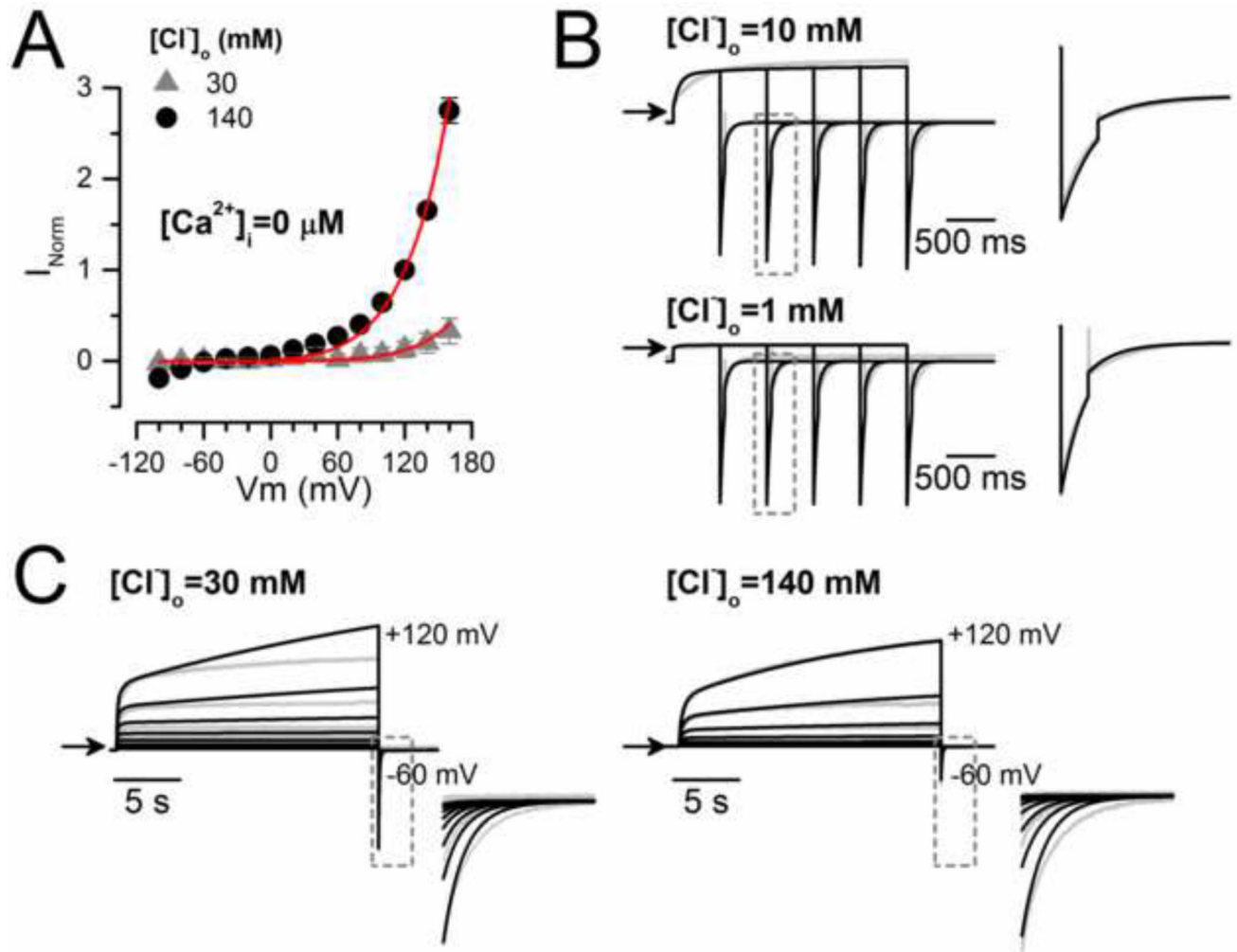


Fig 6. Global fit using Scheme IV to TMEM16A recordings obtained at different $[Cl^-]_o$
 Grey lines are data and solid lines are best fits to: (A) $I-V_m$ relationships obtained with 30 mM and 140 mM $[Cl^-]_o$ from cells dialyzed with a zero Ca^{2+} solution; (B) I_{Cl} recorded from the same cell exposed to 10 mM and 1 mM $[Cl^-]_o$, dialyzed with 0.2 μM $[Ca^{2+}]_i$ and stimulated with the V_m protocol shown in Figure 3A; (C) I_{Cl} recorded from cells exposed to 30 mM and 140 mM $[Cl^-]_o$, dialyzed with 0.2 μM $[Ca^{2+}]_i$ and stimulated with 20 s pulses from -20 mV to $+120$ mV. Data in B and C were obtained from cells dialyzed with $[Cl^-]_i = 40$ mM. The right insets in B and C show magnified fits to fast phases of I_{tail} enclosed in grey squares. The R^2 value for the global fits shown in Figures 5 and 6 was 0.98.

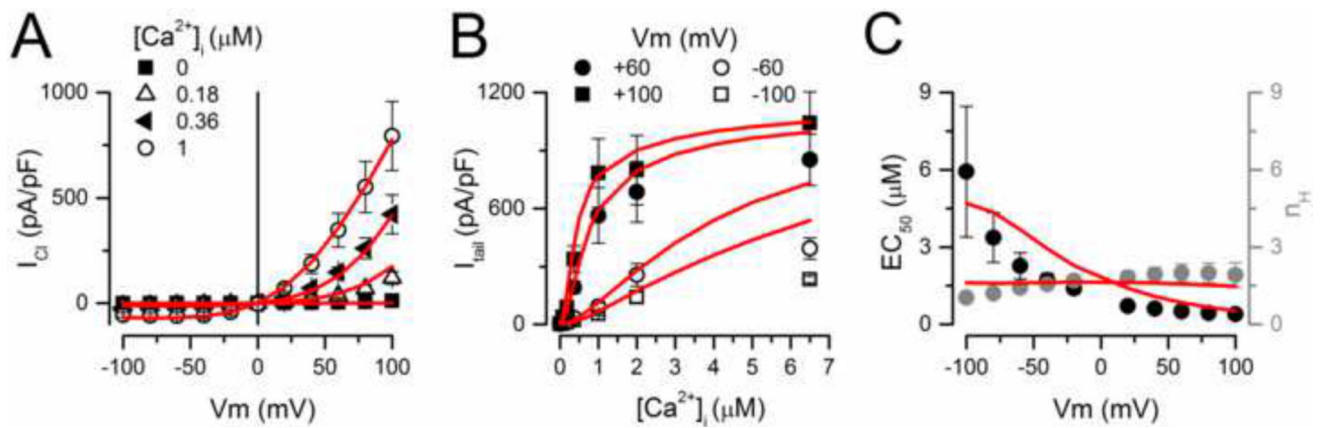


Fig 7. Scheme IV mimics the I_{Cl} vs V_m , dose-response curve to $[Ca^{2+}]_i$ and the EC_{50}/n_H vs V_m relationships for TMEM16A channels

Black symbols correspond to experimental data. Solid lines are simulations using Scheme IV. (A) Current Density vs V_m relationships. (B) Current Density as a function of $[Ca^{2+}]_i$ at the indicated V_m . (C) EC_{50} for TMEM16A Ca^{2+} activation and the Hill coefficient n_H vs V_m . EC_{50} and n_H values were obtained from B. The experimental data was collected using $[Cl^-]_i=[Cl^-]_o=140$ mM and 0.7 s depolarizations. The same conditions were used in the simulations. All simulations were carried out using the IonChannelLab software and the rate constants listed in Table 2. $R^2 = 0.95$.

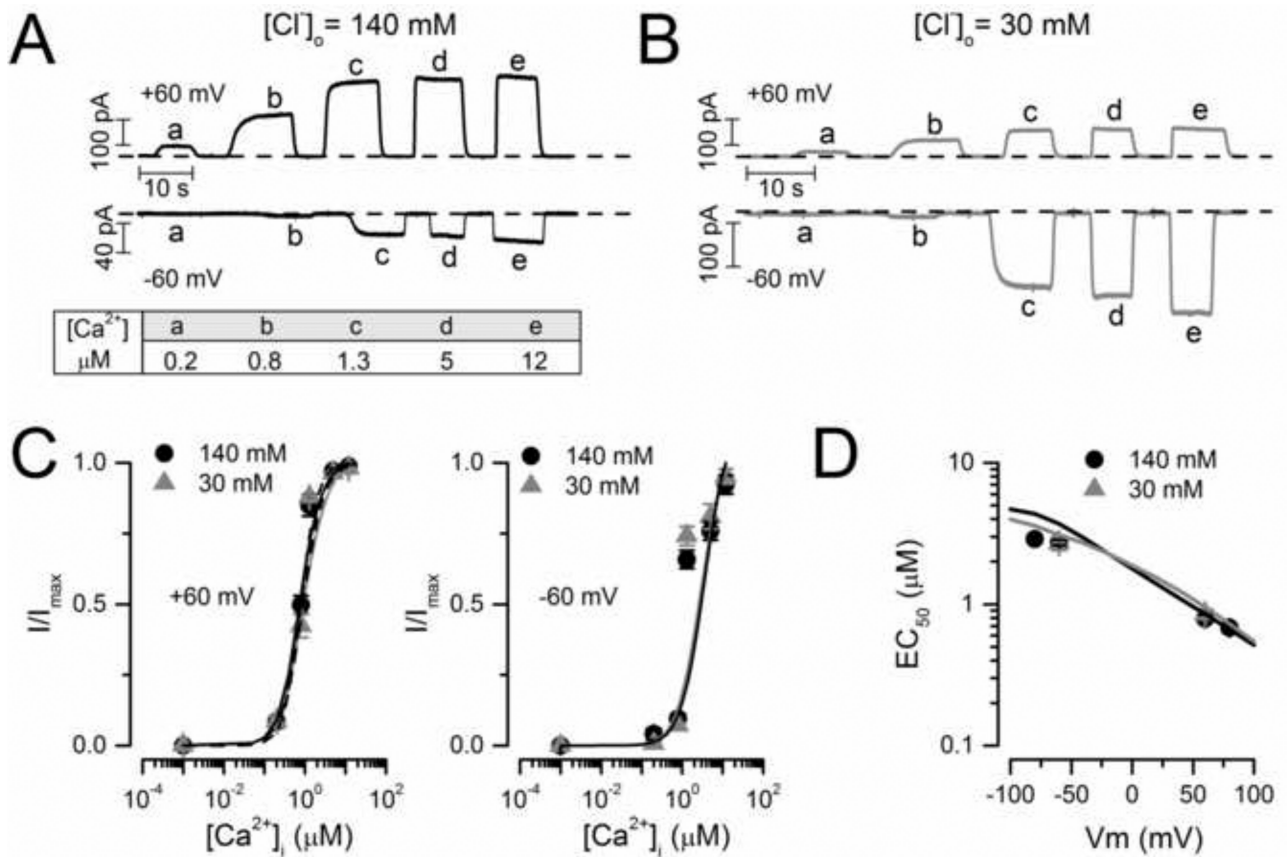


Fig 8. The apparent Ca^{2+} sensitivity of TMEM16A was not altered by lowering the $[Cl^-]_o$
A–B Typical I_{Cl} recordings from inside-out patches held at ± 60 mV and exposed to 140 mM **(A)** or 30 mM $[Cl^-]_o$ **(B)**. I_{Cl} were activated by applying 0, 0.2 **(a)**, 0.8 **(b)**, 1.3 **(c)**, 5 **(d)** and 12 μM $[Ca^{2+}]_i$ **(e)**. Dashed lines indicate I_{Cl} obtained with 0 $[Ca^{2+}]_i$ and 25.2 mM EGTA. **(C–D)** Dose-response and EC_{50} vs V_m curves (symbols) obtained from experimental data like that shown in **A and B** were identical to the predictions made with Scheme IV at 30 (grey lines) and 140 (black lines) mM $[Cl^-]_o$.

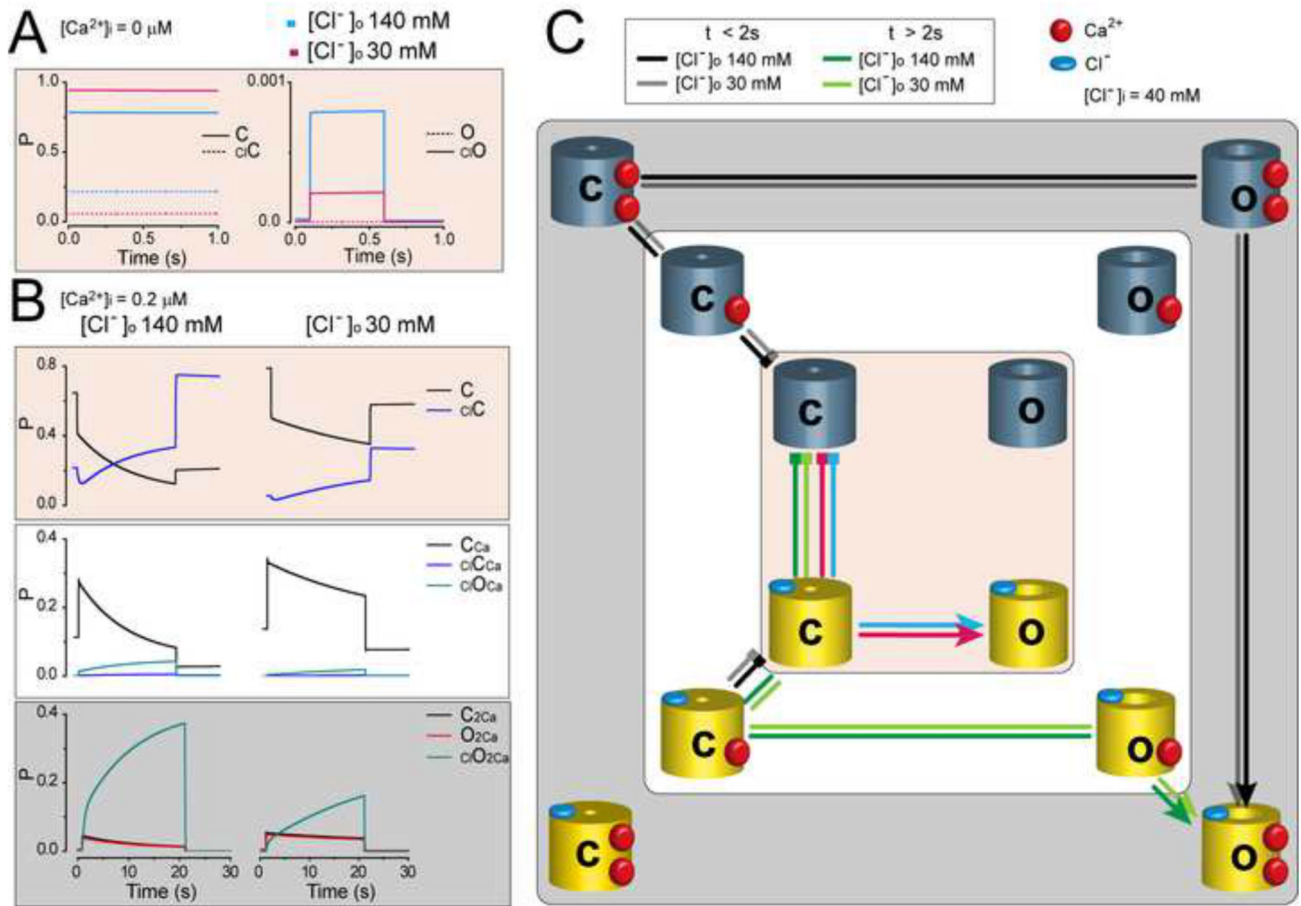


Fig 9. TMEM16A activation pathways predicted by Scheme IV

(A) Time dependent P_C , P_O , P_{cCl} and P_{cO} when $[Cl^-]_o$ was 140 mM (blue lines) or 30 mM (red lines) while $[Ca^{2+}]_i$ and $[Cl^-]_i$ were 0 M and 40 mM, respectively. Note that P_O was ≈ 0 at both $[Cl^-]$. (B) Time dependent P_C , P_{cCl} , P_{cCa} , P_{cClcCa} , $P_{cClOcCa}$, P_{cC_2Ca} , P_{O_2Ca} , and P_{cClO_2Ca} are shown in rectangles coloured according to the colours of the layers of Scheme IV presented in panel C. Left column: $[Ca^{2+}]_i = 0.2 \mu M$, $[Cl^-]_o/[Cl^-]_i = 140/40 mM$. Right column: $[Ca^{2+}]_i = 0.2 \mu M$, $[Cl^-]_o/[Cl^-]_i = 30/40 mM$. P_O , P_{cO} , P_{OcCa} , and P_{cClc_2Ca} are not shown for clarity, their values were ≈ 0 . P values were calculated by numerically integrating the differential equations (supplemental material) under the following conditions: $[Cl^-]_o = 140 mM$ or $30 mM$, $[Cl^-]_i = 40 mM$, $[Ca^{2+}]_i = 0$ (A), 0.2 (B) μM , and $20 s$ pulse to $+140 mV$ followed by repolarization to $-60 mV$. The set of rate constants listed in Table 2 was used to obtain the time dependence of occupation probability. (C) TMEM16A activation pathways according to probability of occupation. Blue and pink arrows indicate the pathway in the absence of intracellular Ca^{2+} while $[Cl^-]_o$ was 140 mM or 30 mM, respectively. Black, grey, green and light green arrows indicate the activation pathways when intracellular Ca^{2+} was $0.2 \mu M$ while $[Cl^-]_o$ was 140 mM (black and green lines) or 30 mM (grey and light green lines). $[Cl^-]_i$ was set at 40 mM. Red button = Ca^{2+} , blue donut = Cl^- .

Recording solutions

Table 1

External solutions with different $[Cl^-]$ were prepared by mixing solutions ES-136 Cl^- , ES-10 Cl^- and ES-1.5 Cl^- to obtain the required Cl^- concentration.

Compound	External solutions (mM)				
	ES-140Cl	ES-140Na	ES-10Cl	ES-1.5Cl	ES-30Cl
TEA-Cl	139	-	9	0.5	29
NaCl		139	-	-	
CaCl ₂	0.5	0.5	0.5	0.5	0.5
HEPES	20	20	20	20	20
D-Mannitol	100	100	300	320	330
Osmolarity (mosm/kg)	390	390	340	340	390
Total $[Cl^-]$	140	140	10	1.5	30

Compound	Internal solutions (mM)						
	IS-40Cl/0Ca	IS-40Cl/0.2Ca	IS-40Cl/0.8Ca	IS-40Cl/1.3Ca	IS-40Cl/5Ca	IS-40Cl/12Ca	IS-83Cl/0.2Ca
TEA-Cl	40	30	17	27.4	11.8	2	72.5
CaCl ₂	-	5.2	11.5	6.3	14.1	19	5.2
HEPES	50	50	50	50	50	50	50
D-Mannitol	90.2	85	150	154	85	85	-
EGTA-TEA	25.2	25.2	25	-	-	-	25.2
HEDTA	-	-	-	25	25	25	-
Osmolarity (mosm/kg)	290	290	290	290	290	290	288
Free $[Ca^{2+}]$ (μ M)	0	0.2	0.8	1.3	5	12	0.2
Total $[Cl^-]$	40	40	40	40	40	40	83

Table 2
Parameter values associated with the rate constants of Scheme IV

(A) Figures listed were obtained from the global fit of TMEM16A data shown in Figures 5 and 6. z values are the apparent charge. (B) The relationship between forward and backward rate constants and weight factors l , L , h , H , m and M —which take into account the presence of Ca^{2+} in a given state. Grey boxes include weight factor values obtained from the global fit. Values shown in *Italics and parenthesis (A and B)* are averaged values obtained during the first 15 fit trials and were used as a seed for the final global fit. All listed parameter values were used for simulations of Scheme IV shown in Figures 7, 8 and 9.

A			
Rate Constant	Expression	Parameter	Parameter Values At 0 mV
α_1	$\alpha_{1,0} e^{\frac{z_{\alpha} F V_m}{RT}}$	$\alpha_{1,0} (s^{-1})$	0.0077 (0.00803±0.00064)
		z_{α}	0 (0±0)
β_1	$\beta_{1,0} e^{\frac{-z_{\beta} F V_m}{RT}}$	$\beta_{1,0} (s^{-1})$	917.1288 (875.07±51.77)
		z_{β}	0.0064 (0.01133±0.0021)
k_{O1}	$k_{O1,0} e^{\frac{z_1 F V_m}{RT}}$	$k_{O1,0} (s^{-1} \mu M^{-1})$	597.9439 (583.58±14.41)
		z_1	0 (0±0)
k_{O2}	$k_{O2,0} e^{\frac{-z_2 F V_m}{RT}}$	$k_{O2,0} (s^{-1})$	2.8530 (2.8547±0.0189)
		z_2	0.1684 (0.166±0.00118)
α_{CI}	$k_{1,0} e^{\frac{z_{11} F V_m}{RT}}$	$k_{1,0} (s^{-1})$	1.8872 (1.9349±0.0708)
		z_{11}	0.1111 (0.1141±0.00403)
β_{CI}	$k_{2,0} e^{\frac{-z_{12} F V_m}{RT}}$	$k_{2,0} (s^{-1})$	5955.783 (5769.96±207.83)
		z_{12}	0.3291 (0.3272±0.00346)
k_{CCU}	$k_{+Cl,0} e^{\frac{z_{+Cl} F V_m}{RT}}$	$k_{+Cl,0} (s^{-1} mM^{-1})$	1.143×10 ⁻⁶ (1.14×10 ⁻⁶ ±9.17×10 ⁻⁸)
		z_{+Cl}	0.1986 (0.2112±0.0238)
k_{CC2}	$k_{-Cl,0} e^{\frac{-z_{-Cl} F V_m}{RT}}$	$k_{-Cl,0} (s^{-1})$	0.0009 (8.52×10 ⁻⁴ ±1.28×10 ⁻⁵)
		$z_{-Cl,0}$	0.0427 (0.04847±0.0098)
k_{OCI}	$k_{+OI,0} e^{\frac{z_{+OI} F V_m}{RT}}$	$k_{+OI,0} (s^{-1} mM^{-1})$	1.1947 (1.1495±0.0459)
		z_{+OI}	0.6485 (0.65±0.0026)
k_{OC2}	$k_{-OI,0} e^{\frac{-z_{-OI} F V_m}{RT}}$	$k_{-OI,0}$	3.4987 (3.443±0.1096)
		z_{-OI}	0.0300 (0.0308±0.00054)
B			
$\alpha_2 = l\alpha_1$	$\alpha_3 = l^2\alpha_1$	$\beta_2 = L\beta_1$	$\beta_3 = L^2\beta_1$
$k_{CCB} = hk_{CC1}$	$k_{CCB} = h^2k_{CC1}$	$k_{CC4} = Hk_{CC2}$	$k_{CC6} = H^2k_{CC2}$
$k_{OCB} = mk_{OC1}$	$k_{OCB} = m^2k_{OC1}$	$k_{OC4} = Mk_{OC2}$	$k_{OC6} = M^2k_{OC2}$
$k_{C1Cl} = \frac{h}{H}k_{O1}$	$k_{C2Cl} = \frac{l}{L}k_{O2}$	$k_{O1Cl} = \frac{m}{M}k_{O1}$	$k_{O2Cl} = k_{O2}$

$\alpha_{C12} = \frac{Hml}{M} \alpha_{C11}$	$\alpha_{C13} = \frac{Hml^2}{M^2} \alpha_{C11}$	$\beta_{C2} = hL\beta_{C1}$		$\beta_{C3} = (hL)^2\beta_{C1}$
$k_{C1} = k_{O1}$	$k_{C2} = \frac{l}{L} k_{O2}$	$l = 41.6411 (42.04 \pm 1.7)$	$m = 0.0102 (0.010 \pm 0.00023)$	$h = 0.3367 (0.342 \pm 0.018)$
		$L = 0.1284 (0.134 \pm 0.004)$	$M = 0.0632 (0.064 \pm 0.001)$	$H = 14.2956 (14.2 \pm 0.70)$

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