

The effect of age and speed on foot and ankle kinematics assessed using a 4-segment foot model

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Abstract

Background: The effects of age and speed on foot and ankle kinematics in gait studies using foot models are not fully understood, whereas this can have significant influence. We analyzed these variables with the 4-segment Oxford foot model.

Methods: Twenty-one healthy subjects (aged 20–65 years) were recruited for gait analysis. The effect of speed on foot and ankle kinematics was assessed by comparing results during slow walking and fast walking. To assess the effect of age, a group of 13 healthy young adults (aged 20–24 years) were compared with a group of 8 older adults (aged 53–65 years). Also, the interaction between age and speed was analyzed.

Results: Regarding speed, there was a significant difference between forefoot/hindfoot motion in the sagittal plane (flexion/extension) during both loading- and push-off phase ($P = .004$, $P < .001$). Between hindfoot/tibia, there was a significant difference for all parameters except for motion in the sagittal plane (flexion/extension) during push-off phase ($P = .5$). Age did not significantly influence kinematics. There was no interaction between age and speed.

Conclusion: Our analysis found that speed significantly influenced the kinematic outcome parameters. This was more pronounced in the ankle joint. In contrast, no significant differences were found between younger and older healthy subjects.

Abbreviations: MSFM = multi-segment foot model, OFM = Oxford foot model, ROM = range of motion.

Keywords: age, clinical biomechanics, gait, multi-segment foot model, speed

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1. Introduction

Kinematic models are increasingly used for biomechanical evaluation of the foot and ankle in healthy subjects and patients after injury.^[1–9] However, the effect of age and speed on foot and ankle kinematics are not fully understood.^[4,10–12]

A number of studies on age-related differences in foot kinematics have been performed, with inconclusive results. Kerrigan et al^[4] found reduced peak plantar flexion in the ankle joint of older adults (65–84 years) compared with young adults (18–36 years) using a single-segment foot model. In contrast, a study using a 4-segment foot model by Legault-Moore et al^[13] found no significant differences in gait parameters between 11 healthy young subjects (18–30 years) and 11 healthy elderly subjects (>55 years). A more recent study with a 5-segment foot model found that older adults (average 73.2 years) had different foot kinematics than younger adults (average 23.2 years) during walking, with reduced mobility of the calcaneus, midfoot, metatarsus, and changes in the angular position of the hindfoot.^[14]

Studies analyzing the effect of speed on foot kinematics have found that speed significantly influences foot and ankle kinematics.^[15–21] Dubbeldam et al^[22] used a multi-segment foot model (MSFM) to study foot and ankle kinematics in 14 healthy young subjects, and found that walking speed significantly affected foot and ankle kinematics, leading to higher range of motion (ROM) with higher speed. However, speed alone does not fully explain the changes in foot and ankle kinematics and it is unknown whether speed influences foot kinematics differently in different age groups.^[23] To our knowledge, no previous studies reported results on both age and speed and their interaction on foot and ankle kinematics using a MSFM.

The aim of the present prospective study was, therefore, to investigate the role of age and speed on foot and ankle kinematics, using the 4-segment Oxford foot model (OFM). In addition, the interaction between age and speed was analyzed. Our hypothesis was that age (negatively, less ROM) and speed (positively, more ROM) significantly influence foot and ankle kinematics and that speed has less impact on foot and ankle kinematics in older adults. A better understanding of the effects of age and speed and the interaction between age and speed in normal subjects would allow foot and ankle kinematics in pathologic feet to be interpreted more accurately.

2. Methods

2.1. Study population

In this prospective study, healthy subjects were randomly recruited around the Maastricht University for gait analysis of the foot and ankle at the movement laboratory. Only healthy subjects of working age (18–65 years old), while most clinical studies focus on this group, with no previous injury to the lower extremity or neurological diseases, with no limitations in daily life and sport exercise every week were included.^[8,24] Based on previous studies a minimum of 15 subjects were needed to investigate speed on foot and ankle kinematics.^[4,12,13,22]

To analyze the effect of age, the same group of subjects was used and was divided in 2 groups. Based on previous age-related studies, an age gap of at least 30 years was chosen between a younger adults group and an older adults group.^[4,12,13] This was achieved by including only persons aged 18 to 25 years and those aged 55 to 65 years. Exclusion criteria were a history of ankle, foot or leg injuries or operations, arthritis, anatomical abnormalities (e.g., pes planus, pes cavus, or congenital abnormalities), diabetes, peripheral neuropathy, and spinal or neurological injuries.

Finally 21 subjects, who met the inclusion criteria, were willing to participate in this study. Those 21 were used to analyze the effect of speed. Of them 13 patients were included in the younger adults group and 8 in the older adults group to analyze the effect of age. All measurements were performed by 1 independent researcher who was experienced in examining the foot and using the OFM. All subjects signed an informed consent form. This study was approved by the medical ethics committee of the Maastricht University Medical Centre (MEC azM/UM).

2.2. Equipment

Motion capture was conducted using the VICON system (Vicon Motion Systems Ltd., Oxford, UK), which comprises 8 cameras (6 MX3 and 2 T20 running at 200Hz). Markers were placed according to the OFM guidelines.^[25–28] Subjects were asked to walk on a 10 m platform with a force platform (Kistler 9282E) in the middle to identify the foot contact with the floor. Vicon NEXUS 1.8 was used to visualize and process the 3D motions. The OFM gait analysis data (8 trials) were generated with Matlab (version 7.12, 2011) and processed in Excel (Microsoft, 2010). Results beyond 2 standard deviations were removed. Randomly 6 trials were used to calculate means. Means were further analyzed with SPSS (IBM Statistics, version 20).

2.3. Protocol

Twenty-one subjects were invited to the movement laboratory and underwent a physical examination assessing body mass, height, leg length, knee width, and ankle width. After placing of

all 42 (14mm) reflective markers, 1 static trial was performed.^[25–28] Subsequently, dynamic trials were conducted with subjects walking barefoot on 10m catwalk at self-selected “normal,” “slow,” and “fast” speed. Eight proper recordings for each condition were made during walking, in which the subjects hit the center of the force plate. With a stopwatch time and speed was controlled by the researcher. To correct for foot dominance, in the first 50% of the group (10 subjects) both feet were analyzed.^[29,30] This were 4 persons from the younger adults group and 6 from the older adults group.

The effect of speed on foot and ankle kinematics was evaluated by analyzing data of all 21 subjects (31 feet). Outcome parameters during slow walking were compared with those during fast walking. To test the effect of age on foot and ankle kinematics results of 13 younger adults (17 feet) were compared with the results of 8 older adults (14 feet). One step per trial was evaluated, from heel strike to toe-off, and each step was divided into 2 parts, a loading phase (from heel strike to midstance or 0–50%) and a push-off phase (from midstance to toe-off or 50–100%). The force plate was used to determine the heel-strike and toe-off phases during walking. Intersegment angles during locomotion were analyzed for the forefoot and hindfoot and for the hindfoot and tibia, in all planes (sagittal, frontal and transverse, representing flexion/extension, abduction/adduction, and inversion/eversion, respectively).^[31,32]

2.4. Statistical analysis

Characteristics (age, body mass, height) of the healthy subjects are presented with descriptive statistics. The ROM results are presented as mean ± standard deviation (SD) (minimum–maximum) and calculated with descriptive statistics. Wilcoxon signed rank test was used to compare the mean values of the parameters for slow versus fast walking speed. The Mann–Whitney *U* test was used to compare the kinematic parameters between younger and older healthy subjects. For these results, a *P* value below .05 was considered to be statistically significant. Repeated measures Anova test was used to analyze the interaction between age and speed.

3. Results

3.1. Healthy subject characteristics

Table 1 lists the participants' characteristics. The analysis included 21 healthy subjects (31 feet; aged 20–65 years) with 13 (17 feet) younger adults (20–24 years) and 8 (14 feet) older adults (53–65 years). There was a significant difference in age ($P < .001$) between the younger adult group and the older adult group. Other significant differences between the younger and older adults groups were found for body mass index (BMI), weight, and ankle width, which were higher in the older adults group ($P = .005$, $P = .035$, and $P = .045$, respectively). No significant differences in walking speed were found between the 2 groups as regards slow, normal, or fast walking ($P = .719$, $P = .645$, and $P = .479$, respectively).

3.2. Effect of speed

Table 2 presents the foot and ankle kinematics between the forefoot and hindfoot and between the hindfoot and tibia during slow and fast walking (0.94 ± 0.20 vs 1.60 ± 0.24 , $P < .001$) in 21 healthy subjects. There was a significant difference between the slow and fast speeds as regards ROM between forefoot and hindfoot in the sagittal plane (flexion/extension), during both the

Table 1

Patient characteristics.

	Young group (n=13)	Old group (n=8)	P	Total (n=21)
Number of feet	17	14		31
Demographics				
Gender (m/f)	12/1	6/2		
Age, y	22.4 ± 1.3 (20–24)	57.5 ± 3.9 (53–65)	<.001	35.8 ± 17.6 (20–65)
Height, cm	179.4 ± 6.2 (169–188)	178.7 ± 5.1 (168.5–184)	.796	179 ± 56.9 (168.5–188)
Weight, kg	71.4 ± 8.7 (62–90)	80.8 ± 9.8 (63–91)	.035	75.0 ± 10.0 (62–91)
BMI, kg/L ²	22.1 ± 2.0 (19.4–26.6)	25.3 ± 2.5 (20.2–29.1)	.005	23.3 ± 2.7 (19.4–29.1)
OFM measurements				
Leg length, cm	90.1 ± 5.0 (78.0–96.0)	94.0 ± 2.4 (90.0–97.0)	.055	92.3 ± 4.4 (78.0–97.0)
Knee width, cm	10.3 ± 7.6 (9.3–12.0)	10.6 ± 5.2 (9.9–11.4)	.119	10.4 ± 6.8 (9.3–12.0)
Ankle width, cm	6.8 ± 4.6 (6.2–8.0)	7.1 ± 4.6 (6.3–7.7)	.045	7.0 ± 4.9 (6.2–8.0)
Walking speed				
Slow, m/s	0.93 ± 0.19	0.95 ± 0.22	.719	0.94 ± 0.20 (0.54–1.23)
Normal, m/s	1.21 ± 0.19	1.24 ± 0.20	.645	1.22 ± 0.19 (0.89–1.59)
Fast, m/s	1.57 ± 0.25	1.63 ± 0.23	.479	1.60 ± 0.24 (1.16–2.11)

BMI=body mass index, OFM=Oxford foot model.

loading phase and the push-off phase ($P=.004$ and $P<.001$). See, Fig. 1.

There was also a significant difference between slow and fast speed as regards the ROM between the hindfoot and tibia in the sagittal plane (flexion/extension) during the loading phase ($P=.001$), in the frontal plane (abduction/adduction) during the loading and push-off phases ($P<.001$ and $P<.001$), and in the transverse plane (inversion/eversion) during the loading and push-off phases ($P=.014$ and $P=.027$). There was no significant difference between the slow and fast speeds as regards the ROM in the sagittal plane (flexion/extension) during the push-off phase ($P=.518$). During fast walking, ROM increased most in the ankle. See, Fig. 2.

3.3. Effect of age

The foot and ankle kinematics between forefoot/hindfoot and hindfoot/tibia are listed in Table 3 for the younger and older adults groups during normal speed. There was no significant difference in speed between the 2 groups during normal speed

(1.21 vs 1.24 $P=.645$). There were no significant differences between the younger and older adults groups regarding the ROM between the forefoot and hindfoot in the sagittal, frontal, and transverse planes, neither during the loading phase nor during the push-off phase. Nor were there significant differences between the 2 groups in ROM between the hindfoot and tibia in the sagittal, frontal, and transverse planes, neither during the loading phase nor during the push-off phase Figs. 3 and 4.

3.4. Interaction between age and speed on gait parameters

Table 4 presents the results for the foot and ankle kinematics for slow and fast speeds in the younger and older adults groups, as well as the interaction of age on speed differences. There were no significant interactions found between speed and age for the ROM between the forefoot and hindfoot in the sagittal, frontal, and transverse planes, neither during the loading phase nor during the push-off phase. Nor were there significant interactions found between speed and age for the ROM between the hindfoot

Table 2

Effect of speed.

	Slow speed 31 feet	Fast speed 31 feet	P
Speed, m/s	0.94 ± 0.20	1.60 ± 0.24	<.001
Forefoot–hindfoot loading phase			
Sagittal plane (flexion/extension)	7.80 ± 2.33 (4.27–12.88)	8.88 ± 2.80 (4.86–14.98)	.004
Frontal plane (abduction/adduction)	4.61 ± 1.40 (2.19–7.83)	4.50 ± 1.42 (2.11–7.55)	.845
Transverse plane (inversion/eversion)	7.66 ± 1.87 (3.49–11.61)	8.10 ± 3.44 (3.17–16.49)	.875
Forefoot–hindfoot push-off phase			
Sagittal plane (flexion/extension)	16.61 ± 3.52 (8.15–23.72)	18.32 ± 3.30 (10.70–26.71)	<.001
Frontal plane (abduction/adduction)	9.81 ± 2.96 (3.95–17.31)	9.92 ± 2.76 (3.89–15.56)	.337
Transverse plane (inversion/eversion)	8.93 ± 1.82 (5.36–12.63)	8.59 ± 2.48 (4.28–16.72)	.112
Hindfoot–tibia loading phase			
Sagittal plane (flexion/extension)	10.08 ± 2.65 (3.86–14.78)	11.47 ± 2.86 (6.18–18.06)	.001
Frontal plane (abduction/adduction)	12.07 ± 3.11 (6.85–18.09)	16.03 ± 3.82 (9.97–26.38)	<.001
Transverse plane (inversion/eversion)	6.29 ± 1.93 (2.95–11.21)	7.11 ± 2.74 (3.03–14.83)	.014
Hindfoot–tibia push-off phase			
Sagittal plane (flexion/extension)	12.09 ± 3.42 (5.32–18.35)	12.02 ± 2.85 (7.57–20.81)	.518
Frontal plane (abduction/adduction)	10.48 ± 4.07 (5.68–27.25)	12.85 ± 3.37 (7.14–22.64)	<.001
Transverse plane (inversion/eversion)	9.75 ± 3.49 (4.94–17.89)	10.67 ± 3.30 (4.48–18.76)	.027

Range of motion in degrees presented as mean ± standard deviation (range).

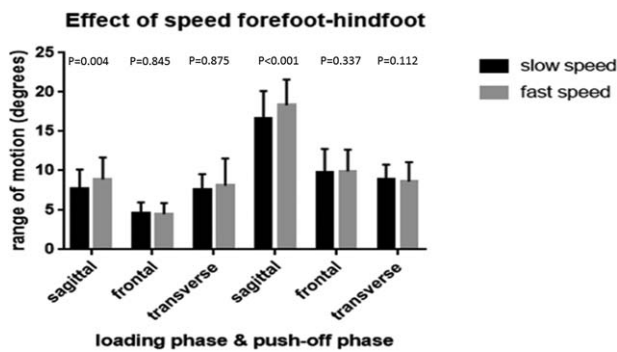


Figure 1. Range of motion between forefoot and hindfoot in subjects during slow (black) and fast (grey) walking during loading phase and push-off phase in sagittal (flexion/extension), frontal (abduction/adduction), and transverse (inversion/eversion) plane.

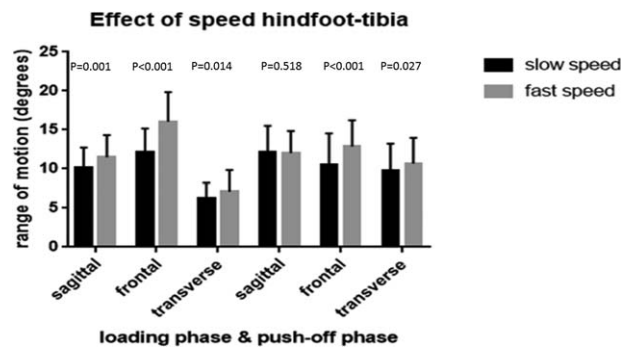


Figure 2. Range of motion between hindfoot and tibia in subjects during slow (black) and fast (grey) walking during loading phase and push-off phase in sagittal (flexion/extension), frontal (abduction/adduction), and transverse (inversion/eversion) plane.

and tibia in the sagittal, frontal, and transverse planes, neither during the loading phase nor during the push-off phase.

4. Discussion

The present study examined the effects of age and speed on foot and ankle kinematics in people of working age using the 4-segment OFM. In addition, this study was the first to analyze the interaction between age and speed. The findings showed that speed had a significant influence on several kinematic parameters leading to higher ROM, especially on the ankle joint (ROM between hindfoot and tibia). In contrast, there was no significant effect of age on foot and ankle kinematics. There was no interaction between age and speed.

As regards the influence of speed on the ROM between the forefoot and hindfoot, the influence was limited to the ROM in the sagittal plane (flexion/extension) during both phases. For both parameters differences between slow and fast walking was more than 1° (respectively, 1.08° and 1.71°). For all other parameters differences were less than 0.50°. As regards the ROM between the hindfoot and tibia, almost all parameters were

significantly higher at higher speed. Highest differences were found for the ROM in the frontal plane during loading phase (3.96°). These results are comparable with the study of Dubbeldam et al,^[22] who found that speed significantly influenced ROM in a multi-segment model. They included 14 healthy subjects and found several significant differences leading to higher ROM with higher speed. They found significant differences between normal and lower speed for ROM between different segments with difference of 1° or more as in our study. In our study, the most significant differences were found in the ankle joint, as was also found by Dubbeldam et al. They also found significant differences in the hallux, which was not analyzed in our present study.

As regards the influence of age on ROM, differences between both groups for all parameters were small, <1°. The highest difference between both groups was found in the ankle. The ROM between hindfoot and tibia in the frontal plane during push-off phase revealed 2.16° difference between both groups. This difference, however, was not significant.

Comparing with other studies, Kerrigan et al^[4] found significant differences in walking patterns between a group of

Table 3

Effect of age.

	Young group 17 feet	Old group 14 feet	P
Speed, m/s	1.21 ± 0.19	1.24 ± 0.20	.610
Forefoot–hindfoot loading phase			
Sagittal plane (flexion/extension)	8.26 ± 2.11 (5.87–12.82)	7.70 ± 2.99 (4.14–14.18)	.297
Frontal plane (abduction/adduction)	4.07 ± 1.36 (1.85–6.69)	4.37 ± 1.22 (2.69–6.46)	.597
Transverse plane (inversion/eversion)	7.42 ± 2.04 (4.41–11.52)	7.01 ± 2.71 (3.65–13.79)	.356
Forefoot–hindfoot push-off phase			
Sagittal plane (flexion/extension)	16.80 ± 3.96 (10.36–24.02)	17.15 ± 2.94 (12.27–20.95)	.653
Frontal plane (abduction/adduction)	9.95 ± 2.83 (5.33–15.46)	9.17 ± 3.24 (3.65–15.04)	.336
Transverse plane (inversion/eversion)	8.90 ± 1.88 (5.70–12.79)	7.38 ± 1.87 (4.58–10.14)	.053
Hindfoot–tibia loading phase			
Sagittal plane (flexion/extension)	11.15 ± 2.19 (8.24–15.98)	10.25 ± 2.97 (6.57–15.52)	.336
Frontal plane (abduction/adduction)	13.05 ± 2.58 (9.25–17.99)	12.84 ± 4.24 (5.41–20.91)	1.000
Transverse plane (inversion/eversion)	5.68 ± 1.83 (2.39–8.07)	7.01 ± 2.33 (3.62–13.22)	.161
Hindfoot–tibia push-off phase			
Sagittal plane (flexion/extension)	11.84 ± 2.74 (7.21–17.25)	12.34 ± 3.50 (6.23–17.37)	.468
Frontal plane (abduction/adduction)	10.74 ± 3.16 (6.36–16.96)	12.90 ± 5.00 (6.54–27.53)	.200
Transverse plane (inversion/eversion)	9.01 ± 3.04 (4.60–16.37)	11.16 ± 3.33 (6.04–17.44)	.064

Range of motion in degrees presented as mean ± standard deviation (range).

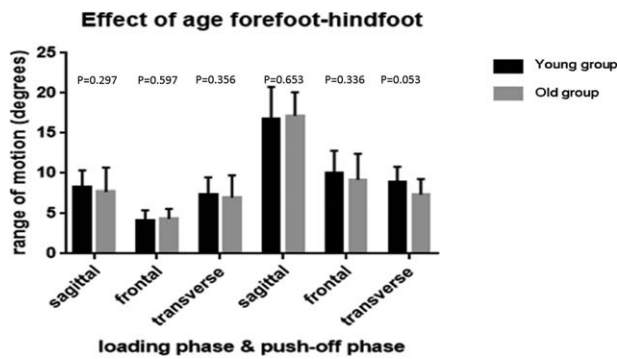


Figure 3. Range of motion between forefoot and hindfoot in younger adults (black) and older adults (grey) during loading phase and push-off phase in sagittal (flexion/extension), frontal (abduction/adduction), and transverse (inversion/eversion) plane.

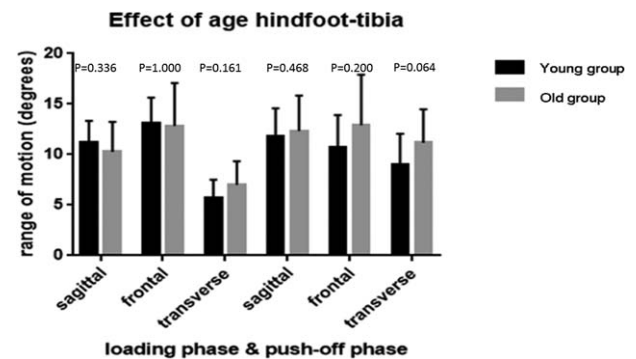


Figure 4. Range of motion between hindfoot and tibia in younger adults (black) and older adults (grey) during loading phase and push-off phase in sagittal (flexion/extension), frontal (abduction/adduction), and transverse (inversion/eversion) plane.

healthy younger subjects (ages 18–36 years) and a group of healthy older subjects (aged 65–84 years), as regards hip extension, anterior pelvic tilt, and ankle plantar flexion using a 1-segment model. Their study, however, reported peak kinematics, and not ROM, as ours does. Another major difference between their study and ours is the much older age of their older group.

Two studies investigating the influence of age on foot and ankle kinematics using a MSFM presented mixed findings. Legault-Moore et al^[13] compared 11 healthy young male subjects aged 18 to 30 years with 11 healthy adults aged 55 years and over. They used a 4-segment foot model to analyze differences in ROM and peak joint angles between the 2 groups. Just as our study, they found no significant differences ($P > .05$) between the 2 age groups. They found highest differences (around 2°) in the ankle,

who were not significant, comparable with our study.^[13] They did not investigate the effect of speed and the interaction of age and speed on foot and ankle kinematics.

In contrast, Arnold et al^[14] found significant differences between 2 groups of different ages in a 5-segment foot model. They included 20 healthy young subjects (mean age 23.2 years) and compared them with 20 healthy older adults (mean age 73.2 years). They found that the older group showed reduced mobility of the calcaneus, midfoot, and metatarsus, and changes in the angular position of the hindfoot, suggesting a less propulsive gait pattern. Significant differences in ROM between both groups were found to differ for most parameters with $>5^\circ$. However, some of these changes were influenced by walking speed. These results are difficult to compare with our present study, as we used a 4-segment foot model and eliminated the effect of speed by

Table 4

Effect of speed in the young and old group.

	Young group 17 feet		Old group 14 feet		Interaction speed and age
	Slow speed	Fast speed	Slow speed	Fast speed	P
Speed, m/s	0.93 ± 0.19	1.57 ± 0.25	0.95 ± 0.22	1.63 ± 0.24	–
Forefoot–hindfoot loading phase					
Sagittal plane (flexion/extension)	7.80 ± 2.33 (4.27–12.88)	9.32 ± 2.43 (5.59–14.26)	7.81 ± 2.53 (4.27–12.04)	8.35 ± 3.21 (4.06–14.98)	.127
Frontal plane (abduction/adduction)	4.19 ± 1.25 (2.19–6.12)	4.54 ± 1.36 (2.11–7.13)	5.11 ± 1.45 (2.66–7.83)	4.45 ± 1.54 (2.80–7.55)	.179
Transverse plane (inversion/eversion)	7.99 ± 1.78 (5.42–11.61)	7.77 ± 2.20 (3.33–12.07)	7.25 ± 1.96 (3.49–10.07)	8.51 ± 4.58 (3.17–16.49)	.204
Forefoot–hindfoot push-off phase					
Sagittal plane (flexion/extension)	16.33 ± 4.09 (8.15–23.72)	17.82 ± 3.46 (10.70–23.49)	16.94 ± 2.80 (12.59–22.05)	18.93 ± 3.11 (14.00–26.71)	.532
Frontal plane (abduction/adduction)	10.01 ± 2.62 (6.50–15.10)	10.15 ± 2.89 (5.19–15.56)	9.57 ± 3.43 (3.95–17.31)	9.63 ± 2.68 (3.89–13.15)	.900
Transverse plane (inversion/eversion)	9.17 ± 1.71 (6.43–12.63)	8.92 ± 1.90 (6.35–12.11)	8.65 ± 1.98 (5.36–11.45)	8.19 ± 3.08 (4.28–16.72)	.791
Hindfoot–tibia loading phase					
Sagittal plane (flexion/extension)	10.16 ± 1.99 (6.44–13.44)	11.52 ± 2.16 (7.94–15.68)	9.99 ± 3.36 (3.86–14.78)	11.41 ± 3.63 (6.18–18.06)	.941
Frontal plane (abduction/adduction)	11.63 ± 2.85 (6.85–17.73)	14.79 ± 2.74 (9.97–20.21)	12.61 ± 3.44 (7.22–18.09)	17.53 ± 4.47 (11.54–26.38)	.144
Transverse plane (inversion/eversion)	5.90 ± 1.87 (2.95–9.52)	6.57 ± 1.93 (4.07–9.99)	6.76 ± 1.96 (3.73–11.21)	7.78 ± 3.45 (3.03–14.83)	.614
Hindfoot–tibia push-off phase					
Sagittal plane (flexion/extension)	11.34 ± 2.65 (7.60–16.44)	11.37 ± 2.17 (7.57–15.62)	13.00 ± 4.09 (5.32–18.35)	12.82 ± 3.43 (8.28–20.81)	.812
Frontal plane (abduction/adduction)	9.56 ± 2.80 (5.68–13.93)	11.62 ± 3.13 (7.13–19.44)	11.59 ± 5.12 (6.46–27.25)	14.34 ± 3.13 (11.06–22.64)	.460
Transverse plane (inversion/eversion)	8.53 ± 2.87 (4.94–13.97)	9.21 ± 2.89 (4.48–14.80)	11.22 ± 3.69 (6.13–17.89)	12.44 ± 2.94 (7.93–18.76)	.503

Range of motion in degrees presented as mean ± standard deviation (range).

using equal walking speeds for both groups. Furthermore, their older adults group was older compared with our older adults group.

The primary focus of our study was to investigate the effect of age in healthy people at working age, so we did not include any persons aged 65 years or over.

Hence, this manuscript does not provide information about foot and ankle kinematics in 80-year-old adults compared with those of 25-year-olds.

Some limitations have to be addressed in this manuscript. Foot dominance was found to have influence on walking patterns and ground reaction forces during walking in literature.^[29,30] We, therefore, cannot rule out that this also affects foot and ankle kinematics during walking. To reduce this influence the first 50% of all subjects had both feet analyzed. These were 4 persons from the younger adults group and 6 from the older adults group. In the remaining group 1 single foot was analyzed (50% dominant and 50% nondominant). Consequently, this led to a higher number of subjects in the older age group who had both feet analyzed.

A total number of 21 subjects was included for this study. This number of patients is in line with previous studies reporting on foot and ankle kinematics, using a MSFM.^[7,13,14,22,24–28] When patients were divided by age, 13 subjects (17 feet) were included in the younger adults group and 8 subjects (14 feet) in the older adults group. These groups were smaller. We found no significant difference between both groups, regarding ROM. Differences between both groups were small ($<2.5^\circ$) and range between both groups were comparable. In contrast, speed significantly influenced ROM leading to higher differences ($>2.5^\circ$ for some parameters) and higher absolute range between both groups.

Besides age significant differences between the younger and older adults groups were found for BMI, body mass, and ankle width ($P=.005$, $P=.035$, and $P=.045$, respectively). When corrected for the parameters no other results were found. In literature no data were found that linked BMI, body mass, and ankle width with different foot and ankle kinematics.

5. Conclusion

This study found a significant influence of speed on foot and ankle kinematics, which was more pronounced in the ankle joint. No significant differences in foot and ankle kinematics between healthy young subjects (aged 18–25 years) and healthy older adult subjects (aged 55–65 years) were found, when measured with the 4-segment OFM. No interaction was found between age and speed. When comparing results of different subjects using the OFM, special attention should be given to walking speed.

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