

Gamma-Hydroxybutyrate Increases Resting-State Limbic Perfusion and Body and Emotion Awareness in Humans

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Gamma-hydroxybutyrate (GHB) is a GHB-/GABA-B receptor agonist inducing a broad spectrum of subjective effects including euphoria, disinhibition, and enhanced vitality. It is used as treatment for neuropsychiatric disorders including narcolepsy and alcohol withdrawal, but is also a drug of abuse. Non-medical users report enhancement of body and emotion awareness during intoxication. However, the neuronal underpinnings of such awareness alterations under GHB are unknown so far. The assessment of regional cerebral blood flow (rCBF) by pharmacological magnetic resonance imaging (phMRI) enables the elucidation of drug-induced functional brain alterations. Thus, we assessed the effects of GHB (35 mg/kg p.o.) in 17 healthy males on rCBF and subjective drug effects, using a placebo-controlled, double-blind, randomized, cross-over design employing arterial spin labeling phMRI. Compared to placebo, GHB increased subjective ratings for body and emotion awareness, and for dizziness ($p < 0.01$ – 0.001 , Bonferroni-corrected). A whole-brain analysis showed increased rCBF in the bilateral anterior cingulate cortex (ACC) and the right anterior insula under GHB ($p < 0.05$, cluster-corrected). ACC and insula rCBF are correlated with relaxation, and body and emotion awareness ($p < 0.05$ – 0.001 , uncorrected). Interaction analyses revealed that GHB-induced increase of body awareness was accompanied by increased rCBF in ACC, whereas relaxation under GHB was accompanied by elevated rCBF in right anterior insula ($p < 0.05$, uncorrected). In conclusion, enhancement of emotion and body awareness, and increased perfusion of insula and ACC bears implications both for the properties of GHB as a drug of abuse as well as for its putative personalized potential for specific therapeutic indications in affective disorders.

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INTRODUCTION

Gamma-hydroxybutyrate (GHB) is an endogenous short-chain fatty acid that is biosynthetically derived from gamma-aminobutyric acid (GABA). GHB acts as an agonist on GABA-B receptors (Engberg and Nissbrandt, 1993) and GHB receptors (Benavides *et al*, 1982). Because of the presence of specific G-protein-coupled high and low affinity binding sites and the specificity of the GHB antagonist NCS-382, GHB was postulated to be a neurotransmitter (Benavides *et al*, 1982; Snead, 2000). Although physiological concentrations of GHB seem to be insufficient to stimulate GABA-B receptors, this mechanism is discussed to be mainly

responsible for its psychotropic effects when administered orally in humans (Carter *et al*, 2009). Apart from its direct effects on GHB and GABA-B receptors, GHB has neuromodulator properties on glutamate, dopamine, serotonin, norepinephrine, and acetylcholine transmission (Andresen *et al*, 2011).

In humans, GHB strongly influences behaviors related to core human autonomic functions such as control of food intake, sexual behavior, and sleep-wake regulation (Bosch and Seifritz, 2016). Some of these behavioral effects are clinically utilized in neuropsychiatric disorders such as narcolepsy, fibromyalgia, and binge-eating syndrome. Moreover, the drug was shown to exert prosocial and prosexual effects and to induce a mixed stimulant-sedative pattern, including euphoria, disinhibition, and enhanced vitality (Abanades *et al*, 2006; Bosch *et al*, 2015, 2017), which are instrumentalized by illicit users (Barker *et al*, 2007; Kapitany-Foveny *et al*, 2015; Lee and Levounis, 2008; Sumnall *et al*, 2008; Teltzrow and Bosch, 2012). Specifically, non-medical users of the drug reported relaxation, and enhancement of body and emotion awareness, defined as the ability to

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perceive one's own feelings (eg, feeling amazed, satisfied, joyous, or irritated, annoyed, dissatisfied, etc) and physical sensations (eg, experiencing the body schema, heartbeat, breathing, skin, and intestinal sensations etc) (Boden and Thompson, 2015; Cioffi, 1991), often related to the above mentioned prosocial and prosexual effects (Barker *et al*, 2007; Sumnall *et al*, 2008; Teltzrow and Bosch, 2012). However, the neuronal underpinnings of such awareness alterations under GHB are unknown so far.

Interoception and emotional self-referential states have crucial roles in healthy functioning and, when impaired, in neuropsychiatric disorders (Paulus and Stein, 2010). Although intensified body and emotion awareness frequently occur in disorders, such as chronic pain in fibromyalgia and dysphoria in depression, also reduction of interoception can be seen in these patients, resulting in feelings of numbness, emptiness, as well as physical and emotional self-alienation (Harshaw, 2015). The anterior cingulate cortex (ACC) and the insula have been suggested as key brain regions in the processing of attentional control, interoceptive, and emotional representations (Lee and Siegle, 2012; Wiebking *et al*, 2015). Although body awareness seems to be processed in the insula, emotional self-reference and emotional values of interoceptive signals are assumed to be processed in the ACC (Smith and Lane, 2015).

A valid method to measure drug-induced functional brain alterations is pharmacological magnetic resonance imaging (phMRI). Specifically, regional cerebral blood flow (rCBF) changes after drug challenge assessed by arterial spin labeling (ASL) can reveal brain signatures of pharmacological compounds and relationships between brain activity patterns and subjective phenomena (Chen *et al*, 2011; Detre *et al*, 2009; Salmeron and Stein, 2002). Two drugs with neuropharmacological resemblances to GHB have been studied using ASL-phMRI: amisulpride and baclofen. Amisulpride is an atypical antipsychotic with antidepressant properties (Racagni *et al*, 2004), which primarily acts as an antagonist on dopamine D2/D3 receptors, but also as an agonist on GHB receptors (Maitre *et al*, 1994). Interestingly, amisulpride and GHB are able to both block and to enhance dopaminergic neurotransmission (Maitre, 1997; Perrault *et al*, 1997), have antidepressant-like effects in animal models (Papp and Wieronska, 2000; Zerbib *et al*, 1992) and prosocial effects in humans (Bosch *et al*, 2015; Saleem *et al*, 2002). In healthy male adults, 7 days with 200 mg per day led to increased rCBF in the basal ganglia and decreased rCBF in the frontal cortex including prefrontal areas, supplementary motor cortex, and bilateral ACC (Viviani *et al*, 2013). The muscle relaxant baclofen is, like GHB, a GABA derivate and GABA-B receptor agonist that is currently investigated as a treatment of substance use disorders (Agabio *et al*, 2013; Leone *et al*, 2010). Both drugs have substantial neurobiological overlaps regarding their metabolomic footprint (Nasrallah *et al*, 2010), astrocyte activation in the ventral tegmental area (VTA) (Gould *et al*, 2014), and bi-directional effects on dopaminergic VTA activity (Cruz *et al*, 2004), most likely due to their shared agonist effect on GABA-B receptors. However, baclofen is selective to GABA-B receptors, whereas GHB also stimulates GHB receptors, and in contrast to baclofen GHB has mood enhancing and prosocial properties (Bosch *et al*, 2015). Acute (Franklin *et al*, 2012) and continuous (Franklin *et al*, 2011)

application of 20 and 80 mg per day baclofen in smokers diminished rCBF in limbic areas, highly overlapping with the amisulpride effects in the medial orbitofrontal cortex (OFC), ACC, and ventral anterior insula. However, subjective psychotropic effects have not been assessed in these studies.

To identify GHB-specific rCBF patterns and their relationships to subjective drug effects, we employed ASL imaging at baseline and 40, 65, and 85 min post challenge with 35 mg/kg p.o. vs placebo in 19 healthy male subjects. Computerized visual analog scales (VAS) were used to measure subjective appraisals of relaxation, and emotion and body awareness. In addition, dizziness served as marker for side effects. We hypothesized that GHB increases body and emotion awareness, and that these changes are correlated with rCBF alterations in functionally associated limbic regions such as the ACC and the insula (Smith and Lane, 2015), also identified in previous phMRI studies using amisulpride and baclofen (Franklin *et al*, 2012; 2011; Viviani *et al*, 2013).

MATERIALS AND METHODS

Design and Participants

A randomized, double-blind, placebo-controlled, balanced, crossed within-subject design was used (Figure 1). Nineteen

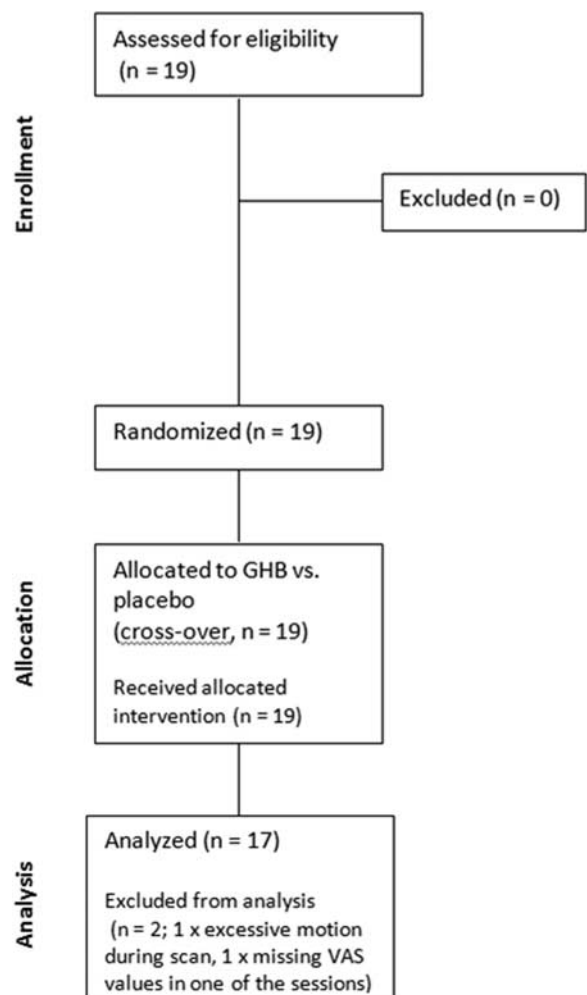


Figure 1 Randomization flow chart.

participants took part in the study. They had a mean age of 23.5 years (SD: ± 3.6 , 20–36), a mean verbal intelligence quotient (IQ) of 113.4 (± 18.4 , 88–145), and a mean weight of 72.2 kg (± 7.4 , 59–85). All participants were non-smoking, healthy males. They were recruited by online advertising and underwent a medical and psychiatric examination. Exclusion criteria were any DSM-IV psychiatric disorder, neurological disorder, severe medical disease, left-handedness, and illegal drug use (lifetime use < 5 occasions, with exception of recreational cannabis use < 1 time per week), latter assessed using the Interview for Psychotropic Drug Consumption (Quednow *et al*, 2004). Five subjects reported regular but very low cannabis consumption < 1 time/week (mean 2 times per month) and one subject showed traces of $\Delta 9$ -tetrahydrocannabinol in one of two urine tests but was not excluded. A German vocabulary test—the Mehrfachwahl-Wortschatz-Intelligenztest (Lehrl, 2005)—was used to estimate the verbal IQ. Participants had to abstain from drinking alcohol 24 h before the study days and from drinking caffeinated beverages during the course of the study days. Abstinence from illegal drugs was ensured by semi-quantitative drug urine tests (Dimension RXL Max, Siemens, Erlangen, Germany). The study was approved by the Cantonal Ethics Committee of Zurich and by Swissmedic, registered at ClinicalTrials.gov (NCT02342366), and took place at the Psychiatric Hospital of the University of Zurich. All participants provided written informed consent and were financially compensated.

Procedure

GHB and placebo were applied in two sessions separated by 7 days. On both test days, participants completed an fMRI paradigm (Bosch *et al*, 2017) on a Philips Achieva 3T whole-body MR-unit equipped with a 32-channel head coil (Philips Medical Systems, Best, The Netherlands) according to a phMRI experimental design as illustrated in Supplementary Figure 1. The experiment started with a T1-weighted anatomical brain scan, a baseline resting-state functional MRI (rsfMRI), and an ASL scan. Subsequently, participants were taken out of the scanner and were orally administered with a single dose of GHB (35 mg/kg) or placebo ($t = 0$ min). A dose of 35 mg/kg was considered to induce moderate subjective effects in illicit and medical use (Bosch and Seifritz, 2016). As maximal plasma concentration of GHB can be expected after about 40 min (Liechti *et al*, 2016), the fMRI paradigm began at $t + 30$ min. Next, a post-challenge rsfMRI and an ASL scan were acquired at the pharmacologic and subjective peak drug effect ($t = +40$ min). Then, participants underwent the first run of the fMRI paradigm (a visual stimulation task, $t = +48$ min). After that, another rsfMRI and an ASL scan were performed followed by the second run of the fMRI paradigm ($t = +70$ min). At the end of the experiment, final rsfMRI and ASL scans were acquired again ($t = +85$ min) after which participants were taken out of the scanner and debriefed. Subjective drug effects using VAS (100 mm scale, with item name and according statement, eg, 'I am aware of my body', with 'not at all' and 'strongly' on the poles of the scale) assessing general drug effect, sedation, relaxation, stimulation, euphoria, body awareness, emotion awareness, sexual arousal, dizziness, and nausea were applied at $t = -28$, $+45$, $+55$, $+68$, $+77$, and

$+93$ min (Abanades *et al*, 2006; Bosch *et al*, 2015; Thai *et al*, 2007). Experimental sessions lasted for 200 min. Here, the GHB effects on VAS for relaxation, body and emotion awareness, and ASL data are presented, whereas the rsfMRI and fMRI data are published elsewhere (Bosch *et al*, unpublished; Bosch *et al*, 2017).

MRI Data Acquisition

fMRI/rsfMRI time series were acquired with a sensitivity-encoded single-shot echo-planar imaging sequence (SENSE-sshEPI) (Schmidt *et al*, 2005). The fMRI protocol used the following acquisition parameters: TE = 35 ms, TR = 2500 ms ($= 82^\circ$), FOV = 24 cm, acquisition matrix = 80×80 interpolated to 128×128 , voxel size = $3 \times 3 \times 3$ mm³, 40 contiguous axial slices (placed along the anterior-posterior commissure plane), and SENSE factor $R = 2.0$.

ASL data were acquired with the pseudo-continuous ASL sequence (Dai *et al*, 2008) with additional background suppression pulses. Imaging parameters were as follows: TR/TE = 4120/14 ms, flip angle = 90° , FOV = 240×240 mm², matrix size = 80×80 , 23 slices with 7 mm thickness and no gap, gradient-echo single-shot EPI, SENSE factor $R = 2.5$; labeling duration = 1650 ms, post-labeling delay = 1525 ms, number of dynamics (control/tag pairs) = 35, labeling gap between imaging volumes and labeling slabs = 20 mm. Background suppression was achieved by applying a saturation pulse preceding labeling and by applying two inversion pulses (1680 and 2830 ms) after the saturation pulse. For subsequent ASL calibration (see below for absolute rCBF quantification), a proton density (PD) weighted image (TR/TE = 10 000/14 ms) was also acquired with the same position and geometric parameters. Total ASL (+PD) scan duration was 336 s. For structural reference, a 3-dimensional (3D) T1-weighted anatomical scan with the following fast field echo (FFE) sequence was obtained: TR/TE = 9.3/4.6 ms, flip angle = 8° , 160 sagittal slices, FOV = 240×240 mm², voxel size = $1 \times 1 \times 1$ mm³.

MRI Data Preprocessing

2D ASL+PD and 3D T1-weighted data sets were analyzed in BrainVoyager QX version 2.8 (Brain Innovation B. V., Maastricht, The Netherlands). Auxiliary custom scripts were prepared in Matlab version 8.3.0.532 release R2014b (The Mathworks, Natick, MA) to automatically calculate rCBF maps from each preprocessed ASL scan and prepare all rCBF maps for the group-level statistical analyses. The 2D-ASL data preprocessing included 3D rigid body motion correction and spatial smoothing (Gaussian kernel of 6 mm full width half maximum). After motion correction, the estimated motion parameters were inspected and one subject had to be excluded from subsequent steps due to excessive motion (> 2 mm). For the other 18 subjects, ASL and equilibrium magnetization (M0) images from each individual scan were registered to the corresponding same-session 3D T1-weighted images and then spatially normalized to the Talairach standard space using a 12 parameters affine transformation. The ASL images were resampled to an isometric 3 mm grid covering the entire Talairach box. To ensure that all ASL scans were normalized to exactly the same locations, the 3D T1-weighted scan of the second

session was registered to the 3D T1-weighted of the first session and the same transformation parameters (which were determined from the first 3D T1 scan) were used for normalization of all ASL scans. After registration and normalization, all dynamics were separately averaged over control and label time points. For rCBF quantification at each voxel (absolute rCBF) the following model (Alsop *et al*, 2015; Buxton *et al*, 1998) was used:

$$\text{CBF} = \frac{6000\lambda (S_{I_{\text{control}}} - S_{I_{\text{label}}}) \times e^{\frac{\text{PLD}}{T_{1,\text{blood}}}}}{2\alpha T_{1,\text{blood}} \times S_{I_{\text{PD}}} \left(1 - e^{-\frac{\tau}{T_{1,\text{blood}}}}\right)} \text{ (ml/100 g/min)},$$

where $S_{I_{\text{control}}}$ and $S_{I_{\text{label}}}$ are the time-averaged signal intensities in the control and labeled images, $S_{I_{\text{PD}}}$ is the signal intensity of the PD-weighted image, PLD is the post-labeling delay, τ is the label duration, $T_{1,\text{blood}}$ is the T_1 of arterial blood (1664 ms), α is the labeling efficiency (0.95) and λ is brain/blood partition coefficient (0.98 ml/g).

Statistical Analysis

For the analyses of VAS scales, repeated measures ANOVA with drug (GHB, placebo) and six time points as within-subject factors were applied using SPSS22.0 for Windows (Armonk, NY: IBM). Greenhouse–Geisser correction and adjusted p -values were used in models with more than one degree of freedom in the numerator. Bonferroni-corrected paired t -tests were applied for *post hoc* placebo vs GHB comparisons (six tests). All confirmatory statistical tests were carried out at a significance level of $p < 0.05$ (two-tailed, corrected).

For the whole-brain voxel-based analysis of ASL data, all Talairach-normalized rCBF maps from the preprocessed 144 ASL/M0 data sets (18 subjects, 2 sessions, 4 repeated scans) were combined and entered into the analysis of (co)variance (AN(C)OVA) module of BrainVoyager QX. Here, a three-way ($4 \times 2 \times 2$) mixed-effects ANOVA design was specified with two within-subject factors (scan, treatment), and one between-subject factor (session). Following the experimental design, the factor scan was assigned with four levels (baseline, $t = +40$ min, $t = +70$ min, $t = +85$ min), the factor treatment with two levels (GHB, placebo) and the factor session had two levels (GHB first, placebo first). All interactions between and among all three factors were also added to the model.

After least square model fitting, to detect any effects of systematic rCBF changes in relation to time, treatment, and session, the F-statistics for the three-way interaction (scan \times treatment \times session) was computed at each voxel, yielding a whole-brain F-map, which was overlaid in pseudo-color onto the average normalized T1 image. To protect against false positives and correct for multiple comparisons, only statistically significant regional effects were displayed for compact clusters surviving the joint application of a voxel- and a cluster-level threshold, which were chosen using a non-parametric randomization approach based on Monte Carlo simulations. In detail, an arbitrary (uncorrected) threshold ($p < 0.005$) was initially applied to all voxels; then, a minimum cluster size was set in such a way that an average of 5% false positive clusters were counted in 1000 randomly generated images to which the same thresholds were applied.

To match the level of ‘smoothness’ between the calculated F-map and the simulated images, after random number generation at each voxel, the resulting images were spatially filtered with a Gaussian kernel at the full width at half maximum initially estimated from the original ASL images according to (Forman *et al*, 1995). Apart from interaction effects, no further neuroimaging analyses were performed. In fact, given the experimental design, the main effects of each single ANOVA factor (ie, scan, treatment, or session effects taken independently from each other) were considered as confounds for the ‘pure’ effect of GHB on CBF coded in the three-way interaction term.

For regions identified in the above analysis, mean regional absolute CBF values were extracted for each scan, session and subject, and used for region-of-interest (ROI)-based correlation analyses with subjective VAS measures body awareness, emotion awareness, relaxation, and dizziness. One additional subject was excluded from these analyses due to missing VAS values in one of the sessions.

The correlation analyses entailed with a (one-factor) regression analysis and a (two-factor) analysis of covariance analysis (ANCOVA). In the regression analysis, the correlation between rCBF and VAS changes was assessed after either GHB or placebo challenge across time points. In the ANCOVA analysis, the correlation between rCBF and VAS changes was assessed independently of the treatment (main effect) and the possible interaction between the different treatment and the observed ‘brain-behavior’ correlation was also addressed (uncorrected).

All ROI-based analyses were performed in Matlab (The Mathworks, www.matlab.com) using the regression analysis (function: ‘regress’) and the ANCOVA tools (function: ‘aocool’), which are both part of the built-in statistical toolbox of the Matlab software package. For each post-challenge time point ($t = 40$ min, $t = 65$ min or $t = 85$ min), rCBF and VAS differences from the corresponding baseline time point (Δ_{rCBF} and Δ_{VAS}) were calculated and given as input to the regression and ANCOVA functions. In the regression analyses, Δ_{VAS} values were separately regressed against Δ_{rCBF} values for each treatment (GHB or placebo) producing separate coefficients of determination (R^2) for each time point and treatment. The R^2 values were displayed on scatter plots to illustrate the possible modulation of these correlations in different time points and treatments. To further assess the rCBF vs VAS correlations independently of the treatment as well as the effect of treatment on these correlations, all Δ_{VAS} and Δ_{rCBF} values from corresponding post-challenge time points in the GHB and placebo sessions were pooled together and entered into the same ANCOVA model in which the treatment was added as the categorical factor. In this way, besides the correlation, the statistical significance of the change in the slope of the regression line between GHB and placebo sessions was also estimated and reported as an interaction between rCBF and VAS correlation and treatment (uncorrected).

RESULTS

Subjective Measures

In drug \times time (2×6) ANOVAs, significant time effects were found for dizziness ($F_{1,15} = 5.98$, $p < 0.01$), drug effects

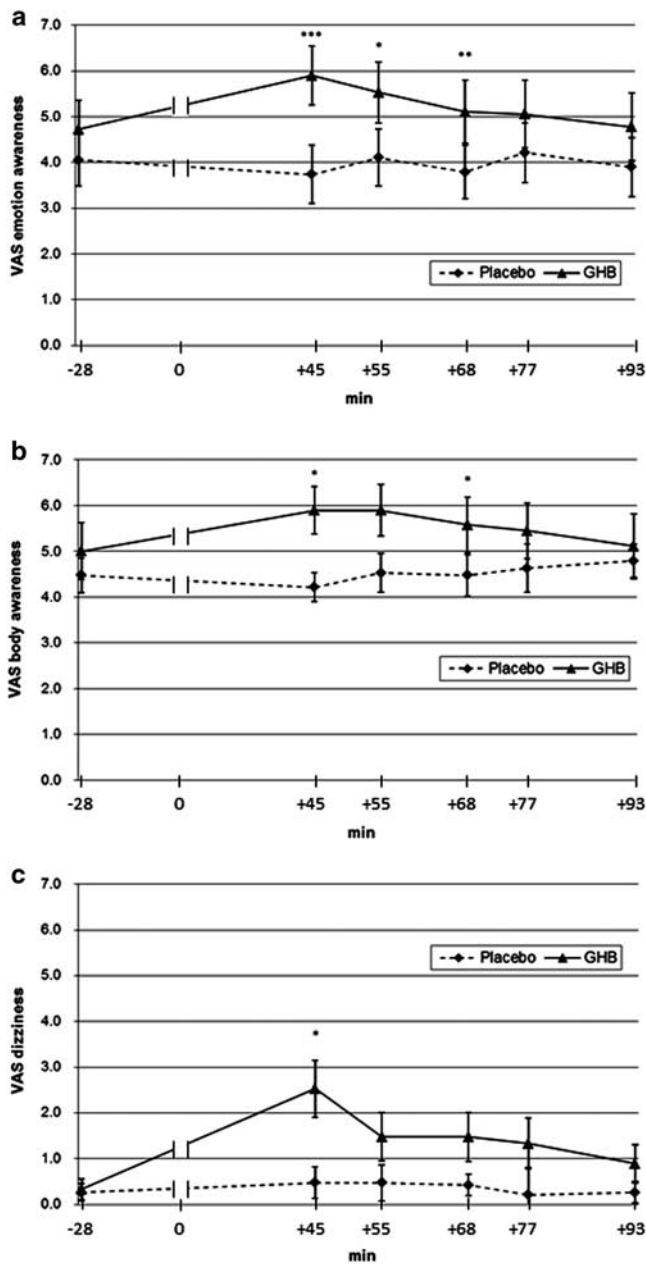


Figure 2 Effects on visual analog scale scores of gamma-hydroxybutyrate (GHB) vs placebo for (a) body awareness, (b) emotion awareness, and (c) dizziness. *** $p < 0.001$, ** $p < 0.01$, * $p < 0.05$ (Bonferroni-corrected).

for emotion awareness and dizziness ($F_{5,11} = 8.69-9.46$, $p < 0.01-0.001$) and drug \times time interactions for body and emotion awareness and dizziness ($F_{5,11} = 2.76-4.79$, $p < 0.05-0.01$). Regarding relaxation, the drug \times time ANOVA showed no significant interaction. Paired t -tests revealed significant GHB effects for body and emotion awareness and dizziness VAS measures, compared with the placebo (body awareness +45, +68 min, $p < 0.01$; emotion awareness +45, +55, +68 min; $p < 0.01-0.001$; dizziness +45, $p < 0.01$) (Figure 2).

Neuroimaging

Cerebral perfusion. We performed a whole-brain analysis for possible three-way interaction effects in a voxel-based

three-way ANOVA analysis with factors scan (baseline, +40, +65, +85 min), treatment (GHB, placebo), session (GHB first, placebo first), which resulted in three regions of statistically significant changes in the bilateral ACC and the right anterior insula (Figure 3). Significant changes were also found in the right caudate nucleus (rCN) and the right superior temporal gyrus (rSTG). However, this has to be considered with caution given that baseline rCBF values were significantly different in the placebo vs GHB condition in these two regions (Supplementary Figure 2).

Correlation of cerebral perfusion and subjective parameters. In the ACC and the insula, changes in the subjective effects ($\Delta_VAS = VAS1$ vs $VAS2$) were correlated with the corresponding change in the regional rCBF values (Δ_CBF) after GHB challenge. The ANCOVA model highlighted a statistically significant ($p < 0.05$) correlation between Δ_CBF and Δ_VAS for relaxation (ACC +40, +85 min; insula +85 min; rSTG +85 min), as well as body (ACC +40, +85 min; insula +85 min) and emotion (ACC +40, +85 min; insula +85 min) awareness, whereas the slope effect (ie, the interaction) was significant ($p < 0.05$) for the dimension body awareness with the ACC at +40 min (Figure 4) and relaxation with the insula at +85 min. No significant correlations or interactions were found with regard to the dizziness VAS score.

DISCUSSION

Here, we investigated the neural effects of GHB using absolute changes in rCBF. We found that 35 mg/kg (p.o.) GHB increased ratings for body and emotion awareness, conceptualized as the ability to perceive one's own feelings and physical sensations (Boden and Thompson, 2015; Cioffi, 1991), which indicated a modulation of subjective interoception and self-referential processing in healthy males. Moreover, GHB increased rCBF in the bilateral ACC and the right anterior insula compared with the placebo, with body and emotion awareness and relaxation but not dizziness being positively correlated with ACC and right anterior insula rCBF. In addition, positive interactions between subjective body awareness and ACC rCBF and between relaxation and insula rCBF were found. Finally, GHB compared with the placebo increased rCBF in the right caudate nucleus and superior temporal gyrus. However, as baseline rCBFs at both drug conditions were already significantly different in these regions, these effects should be interpreted with caution.

The exact physiological basis for neurovascular coupling, which is supposedly depicted by rCBF alterations, is incompletely understood (Wang *et al*, 2011). However, evidences point to an involvement of coordinated activities of neurons, astrocytes, and the microvasculature (Iadecola and Nedergaard, 2007). Synaptic activity due to binding to target region or downstream stimulation, triggers increases in intracellular calcium concentration in adjacent astrocytes, which lead to secretion of vasodilatory substances that increase local blood flow (Jakovcovic and Harder, 2007). GHB mainly acts via GABA-B and partly via GHB receptors. In our participants, GHB increased rCBF in the insula and the ACC. Exclusive binding to these target regions is implausible, as both GABA-B (Billinton *et al*, 2000) and

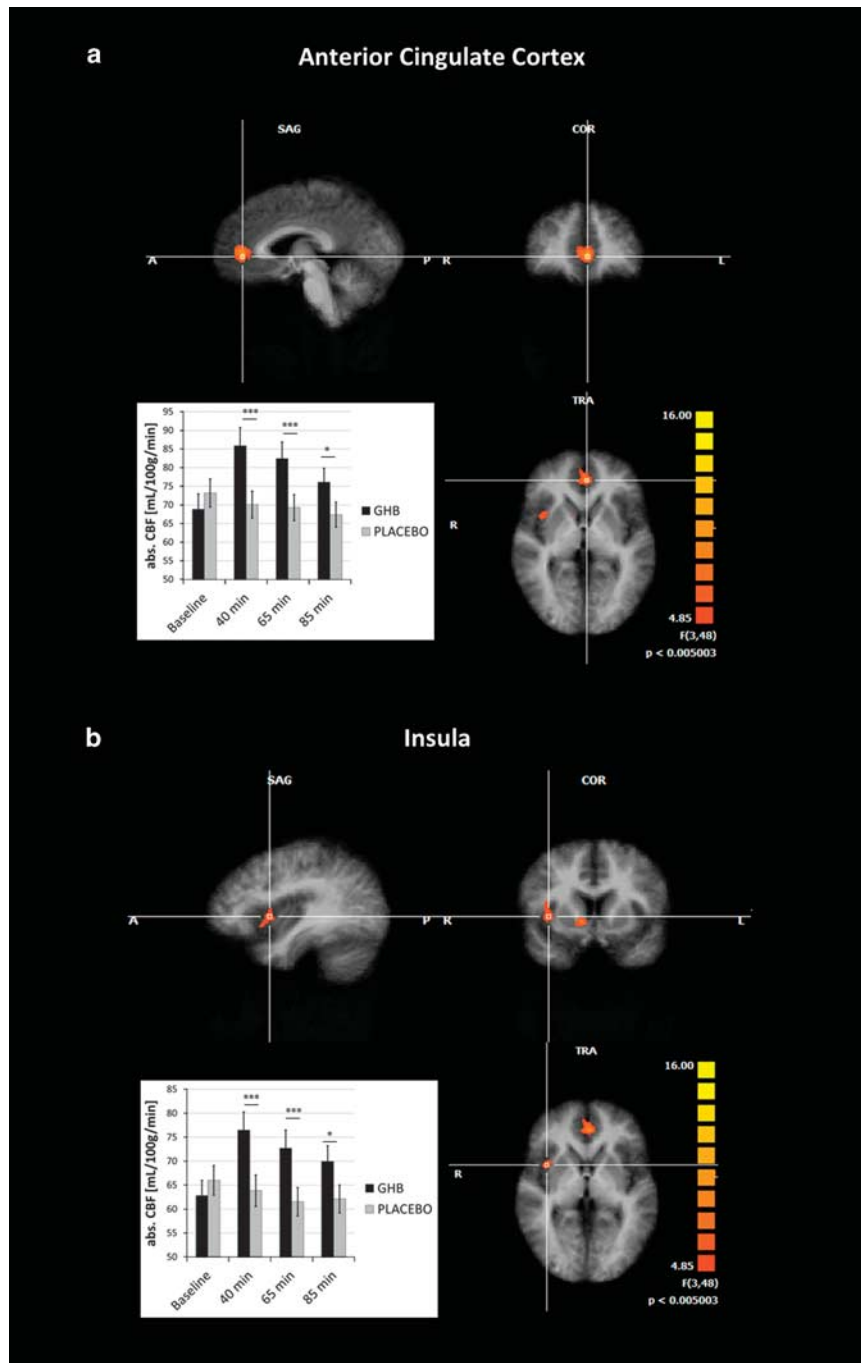


Figure 3 Whole-brain map for cerebral blood flow changes gamma-hydroxybutyrate (GHB) vs placebo with significant clusters in the (a) anterior cingulate cortex (ACC) and (b) insula, threshold $p < 0.05$ (cluster-corrected) including time course of regional cerebral blood flow changes, *** $p < 0.001$, * $p < 0.05$.

GHB (Benavides *et al*, 1982; Gould *et al*, 2003) receptors have a widespread distribution throughout the brain including cortex, basal ganglia, and hippocampus. By contrast, GHB has well-documented effects on GABAergic interneurons disinhibiting mesolimbic dopamine (Cruz *et al*, 2004; Labouebe *et al*, 2007; Maitre, 1997; Pistis *et al*, 2005) release. These indirect dopaminergic effects lead to coordinated downstream increases in cortical activity (Crunelli *et al*, 2006). Hence, increased ACC and insula activity after GHB intake, which is reflected by increased rCBF in these regions, is most likely due to mesolimbic disinhibition via GABA-B

autoreceptor-regulated interneurons. Consequently, the opposing effects of baclofen and GHB on the activity in the ACC and the insula are thus, most likely, due to their differential effects on mesolimbic dopamine release.

The so-called limbic system comprises several functional networks or subsystems dedicated to linking somatosensory and emotional states with cognition, emotion, and behavior (Mesulam, 2000). Derived from data in healthy subjects, a resting-state connectivity system for the integration of interoceptive information with emotional salience that forms a subjective representation of the body was located

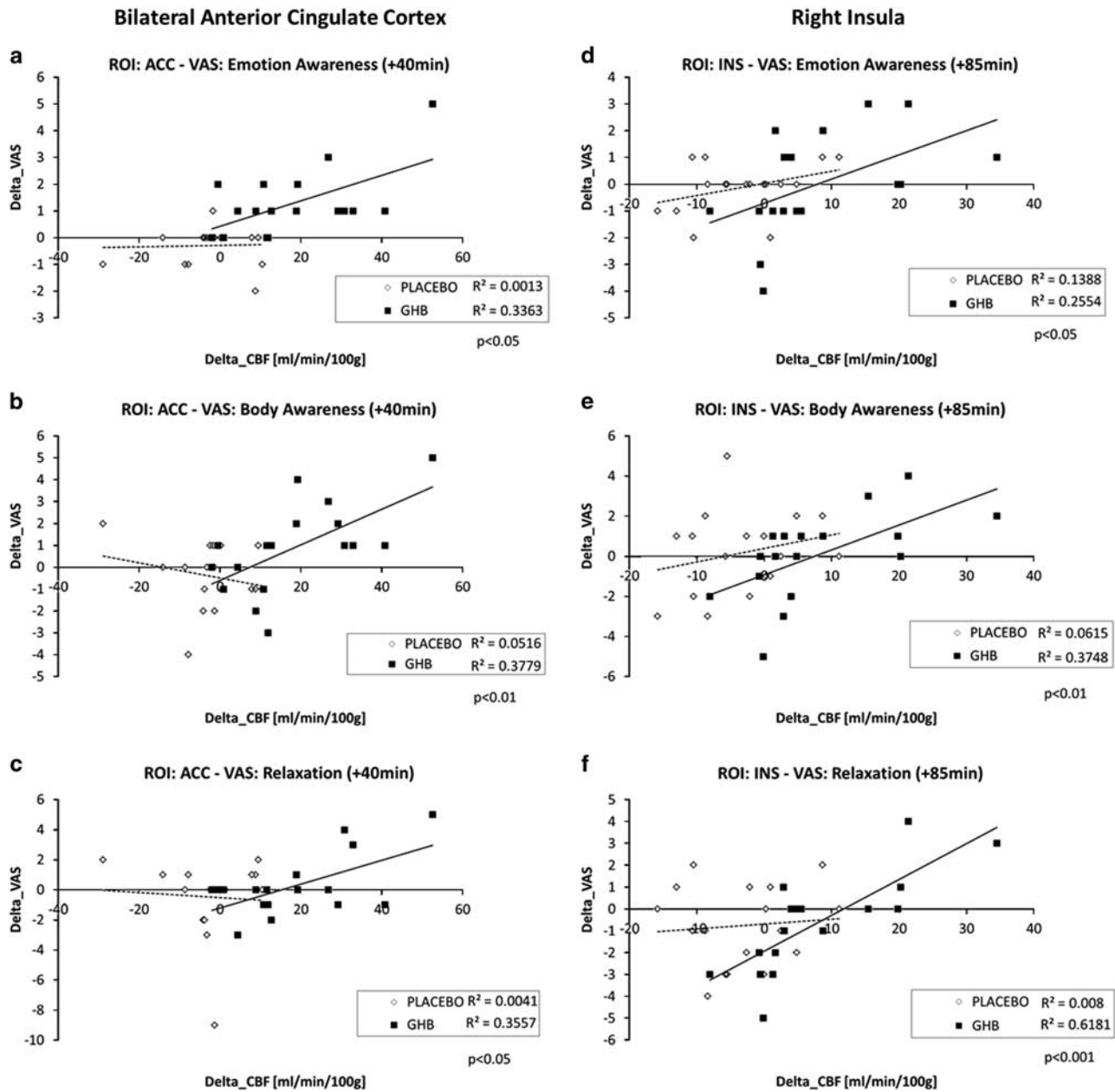


Figure 4 Correlations of subjective ratings and regional cerebral blood flow, gamma-hydroxybutyrate (GHB) vs placebo (fitted lines: regression lines; all uncorrected): (a) anterior cingulate cortex (ACC) and emotion awareness ($p < 0.05$), (b) ACC and body awareness ($p < 0.01$), (c) ACC and relaxation ($p < 0.05$), (d) insula and emotion awareness ($p < 0.05$), (e) insula and body awareness ($p < 0.01$), (f) insula and relaxation ($p < 0.001$).

between the anterior insula and parts of the anterior and mid-cingulate cortex, which are part of the limbic system (Taylor *et al*, 2009). A recent meta-analysis of studies assessing explicit emotion evaluation showed that the two core areas for the processing of the recognition of one's own emotional state are the ACC and the insula (Lee and Siegle, 2012). There is growing evidence that the emotional meaning of one's perceived body state is processed within the ACC, whereas non-emotional body-states are processed within the anterior insula (Smith and Lane, 2015). In our study, we found that GHB increases rCBF in the insula and ACC and that GHB enhances subjective body awareness by increasing cerebral perfusion in latter area. Following the argumentation of Smith and Lane (2015), this seems counterintuitive, as

positive interactions of body awareness with insula rCBF, and emotion awareness with ACC rCBF would have been expected. However, as overlapping processing of both qualities were demonstrated for the insula (Zaki *et al*, 2012), this might also occur in the ACC. Moreover, pleasant touch was shown to be associated with increased connectivity between the insula and the cingulate gyrus (Sailer *et al*, 2016) and increased activity of the ACC (Lindgren *et al*, 2012; Rolls *et al*, 2003). Interestingly, correlations of subjective parameters first occurred at 40 min in the ACC and only became significant in the insula at 85 min after GHB administration. One reason might be that the sample was underpowered, leaving the insula correlation at 40 min on a trend level, or that the described subjective effects

are triggered by ACC hyperperfusion, which then lead to a top-down increase of insula susceptibility towards external stimuli.

Interestingly, GHB is illicitly used to achieve euphoria, recreation/relaxation, increased sociability, and increased sexual arousal (First *et al*, 2002; Luby *et al*, 1992; Miotto *et al*, 2001; Sumnall *et al*, 2008), which are subjective qualities that are related to above mentioned networks. In fact, we found GHB-associated increased body and emotion awareness in our healthy subjects, which were previously reported by illicit users (Barker *et al*, 2007; Kapitany-Foveny *et al*, 2015; Lee and Levounis, 2008; Sumnall *et al*, 2008). Intensified sensitivity towards touch and pleasure of being touched is frequently reported in this population and is probably closely linked to the prosocial and prosexual effects of the drug (Bosch *et al*, 2015; Bosch *et al*, 2017; Palamar *et al*, 2014; Teltzrow and Bosch, 2012). GHB effects generally peak at about 45 min after intake, including seemingly paradoxical effects such as sedation and stimulation (Bosch *et al*, 2015, 2017; Bosch and Seifritz, 2016; Liechti *et al*, 2016). Particularly, body awareness, emotion awareness, and dizziness also peak at the same time (Figure 2), although the co-occurrence of these effects does not necessarily imply they are strictly coupled with (or causally related between) each other. In fact, as it was evident from Figure 2, VAS score for dizziness increases steeper than VAS scores for emotion and body awareness from baseline to 45 min after intake and then falls back to being not significantly different from placebo at the next time point (55 min), whereas VAS scores for emotion and body awareness remain significantly increased compared with the placebo over several time points. Interestingly, insula-associated hyperactivation of pleasant interoceptive stimuli is a candidate biomarker for the transition to drug abuse (Migliorini *et al*, 2013; Stewart *et al*, 2015). Regarding the argumentation of Franklin *et al* (2011, 2012), stating that the selective GABA-B receptor agonist baclofen exerts its putative anti-craving effects via down-regulation of reward- and hedonia-associated limbic areas, such as ACC, orbitofrontal cortex, and insula, it might be assumed that the here shown ACC and insula rCBF increases could represent an abuse-promoting mechanism. However, on the one hand, GHB was also shown to have withdrawal- and craving-reducing effects in alcohol- (Leone *et al*, 2010) and opiate- (Gallimberti *et al*, 1994) dependent individuals. On the other hand, acute i.v. heroin application led to diminished rCBF in highly overlapping areas like acute baclofen (ACC, medial prefrontal cortex, and insula) (Denier *et al*, 2013), which challenges the dichotomy of abuse and anti-craving drugs and the assumption that these might be discernible by their effects on cerebral perfusion. As baclofen diminished rCBF in the medial orbitofrontal cortex, ACC, and ventral anterior insula (Franklin *et al*, 2012; Franklin *et al*, 2011), and the (dopamine D2/D3 receptor antagonist and) GHB receptor agonist amisulpride also reduced rCBF in prefrontal areas including ACC, the here found rCBF increase in these areas was unexpected. Such differences are most likely due to differential effects of these drugs on mesolimbic dopamine (Cruz *et al*, 2004; Di Giovanni *et al*, 1998; Labouebe *et al*, 2007; Pistis *et al*, 2005) release and/or might be related to different pharmacokinetic and other pharmacodynamic properties, such as the rapid distribution or short elimination half-life of GHB as well as the strong

D2/D3 antagonism of amisulpride or the low to moderate affinity of baclofen to voltage-dependent calcium channels (Zvejniece *et al*, 2015).

Because of the above mentioned findings, impairments of interoception and self-referential processing are supposed to be related to pathological rCBF changes in limbic areas such as the ACC and insula, occurring in depression and other neuropsychiatric disorders. Assessment of cerebral perfusion via ASL has yielded conflicting results in depression, and no studies exist where direct associations with self-referential processing were measured. In a study, where ASL was assessed in depressed patients without measuring attentional processes, depression was associated with increased rCBF in ACC, left dorsomedial prefrontal cortex, and left subcortical areas (Duhamel *et al*, 2010). However, hypoperfusion of the ACC was shown in adolescent (Ho *et al*, 2013), adult (Ota *et al*, 2014) and elderly (Ishizaki *et al*, 2008) patients with depression, and depression severity was correlated with reduced perfusion in the default mode network (Orosz *et al*, 2012). Moreover, a mixed pattern with limbic hyperperfusion and prefrontal hypoperfusion was also described (Lui *et al*, 2009), fitting to Mayberg *et al*, 1999 depression model of frontocingular dysfunction based on previous positron emission tomography (PET) studies. Interestingly, a recent PET study showed differential prognostic effects of right anterior insula metabolism for the treatment response towards pharmaco- or psychotherapy in depression (McGrath *et al*, 2013), strengthening earlier evidences for a central role of the anterior insula in depression (Fu *et al*, 2013; Takahashi *et al*, 2010). Contrary to the heterogeneous ASL findings in depression, perception of pain is consistently associated with increased rCBF in the insula and other limbic areas in healthy volunteers (Maleki *et al*, 2013; Owen *et al*, 2008; Segerdahl *et al*, 2015) and patients, eg, with fibromyalgia (Cottam *et al*, 2016; Howard *et al*, 2012; Liu *et al*, 2013; Shokouhi *et al*, 2016). However, it seems that an increase of insula activity is not specific for pain, but rather reflects enhancement of body awareness, as it is also associated with the perception of pleasant touch (Rolls, 2015; Sailer *et al*, 2016). As GHB intake increases pleasure of physical contact (Teltzrow and Bosch, 2012) and enhanced emotion and body awareness in our participants, increased insular rCBF found in our study rather seems to reflect an affirmative mode of self-reference. GHB was demonstrated to be an effective treatment for binge-eating disorder (McElroy *et al*, 2011) and fibromyalgia (Spaeth *et al*, 2012), and was proposed as an experimental therapeutic in depression (Bosch *et al*, 2012; Mamelak, 2009). Enhancement of interoception and emotional self-referential processes via ACC and right anterior insula rCBF increase might be a useful diagnostic and/or therapeutic biomarker in these conditions.

Our study bears a number of limitations: GHB plasma levels were not assessed and therefore individual differences, eg, due to individual metabolic patterns or not permitted food intake cannot be ruled out completely. Moreover, effectivity of blinding was not systematically assessed, and questionable due to recognizable subjective drug effects. Finally, body and emotion awareness was assessed using VAS, which means these effects reflect the subjective impression of one's own awareness. In future studies, GHB plasma levels should be assessed, the use of an active placebo

should be considered to reduce probability of unblinding, and additional experimental paradigms should be employed to investigate in more detail body and emotion awareness.

In summary, our main finding is that GHB enhanced body and emotion awareness, defined as the ability to perceive one's own feelings and physical sensations, and increased rCBF in the ACC and right anterior insula in healthy male volunteers. These effects were positively correlated with each other. In terms of interaction, GHB-induced body awareness was accompanied by increased ACC rCBF, whereas relaxation under GHB was accompanied by increased insular rCBF. The time course of the effects suggests a possible initiation of the subjective effects via rCBF increase in the ACC and a consecutive top-down enhancement of insular susceptibility for external stimuli. It is likely that this interaction reflects a primary high-level enhancement of the emotional meaning of the subjects' perceived body state, which has implications for the understanding of motivations of drug use, as well as for the modulation of interoception and self-referential processes in patients with affective disorders. As such, we suggest GHB to be a candidate medication for personalized treatment of depression for selected patients and with specific indications.

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