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REVIEW ARTICLE

Fiducial marker guided prostate radiotherapy: a review

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ABSTRACT

Image-guided radiotherapy (IGRT) is an essential tool in the accurate delivery of modern radiotherapy techniques. Prostate radiotherapy positioned using skin marks or bony anatomy may be adequate for delivering a relatively homogeneous whole-pelvic radiotherapy dose, but these surrogates are not reliable when using reduced margins, dose escalation or hypofractionated stereotactic radiotherapy. Fiducial markers (FMs) for prostate IGRT have been in use since the 1990s. They require surgical implantation and provide a surrogate for the position of the prostate gland. A variety of FMs are available and they can be used in a number of ways. This review aimed to establish the evidence for using prostate FMs in terms of feasibility, implantation procedures, types of FMs used, FM migration, imaging modalities used and the clinical impact of FMs. A search strategy was defined and a literature search was carried out in Medline. Inclusion and exclusion criteria were applied, which resulted in 50 articles being included in this review. The evidence demonstrates that FMs provide a more accurate surrogate for the position of the prostate than either external skin marks or bony anatomy. A combination of FM alignment and soft-tissue analysis is currently the most effective and widely available approach to ensuring accuracy in prostate IGRT. FM implantation is safe and well tolerated. FM migration is possible but minimal. Standardization of all techniques and procedures in relation to the use of prostate FMs is required. Finally, a clinical trial investigating a non-surgical alternative to prostate FMs is introduced.

INTRODUCTION

Prostate cancer (PCa) is the most commonly diagnosed cancer in males and is often treated with radical external beam radiotherapy. Advances in linear accelerator technology and treatment planning software have made it possible to deliver highly conformal radiation dose distributions using techniques such as intensity-modulated radiotherapy (IMRT). Dose escalation studies have demonstrated improved outcomes for patients with PCa increasingly using hypofractionated stereotactic radiotherapy to exploit the sensitivity of PCa to large doses per fraction. $1-4$ $1-4$ $1-4$ Imageguided radiotherapy (IGRT) is considered an essential tool in ensuring the safe clinical application of these techniques.

Prostate radiotherapy positioned with reference skin marks and/or aligned to bony anatomy is dependent on stability and reproducibility. This may be adequate for delivering a relatively homogeneous dose to large pelvic fields. However, it is not a reliable approach for IMRT, volumetric arc therapy, dose-escalated or hypofractionated stereotactic treatment. Collectively, these advanced techniques require a greater degree of precision, given the decreased margin for error and the potential for radiation injury from overdosing critical structures or treatment failure due to underdosing the target. With the exception of MRI-guided treatment, technological advances which enable complex planning and delivery have surpassed that which aims to verify target position or dose delivery in patients. Two-dimensional (2D) megavoltage (MV) or kilovoltage (kV) prostate IGRT is reliant on pelvic bone alignment and while cone-beam CT (CBCT) enables three-dimensional (3D) imaging, prostate gland visualization remains challenging owing to inadequate soft-tissue contrast. Internal organ motion adds to the challenge of accurately targeting the prostate and is a limiting factor in margin reduction and dose escalation.

Fiducial markers (FMs) surgically implanted within the prostate gland prior to radiotherapy planning have been developed to improve contrast and therefore treatment setup and prostate targeting. Where employed in clinical practice, there are a variety of approaches in relation to how prostate FMs are utilized. This article aimed to review the evidence for the use of FMs in prostate IGRT in relation to feasibility and efficacy, implantation, number and type of FMs, migration, imaging modalities used and clinical impact. Furthermore, it outlines current evidence

on a natural alternative to FMs and introduces a recently opened clinical trial investigating this.

METHODS AND MATERIALS

A literature search was carried out in Medline using the search strategy outlined in Figure 1.

Results of the initial literature search were subject to the following selection criteria:

- Inclusion criteria: studies on humans, specifically investigating the technical aspects or clinical efficacy of FMs for prostate IGRT; studies of prostate motion based on FMs
- Exclusion criteria: review articles, studies of \leq 20 patients (where treatment setup data are reported), phantom studies, post-prostatectomy treatments.

Limiting articles to those reporting setup data on at least 20 patients resulted in a significant number of articles being automatically excluded from this review. This is justified on the basis that published guidance states that at least 20 patients and preferably 25 patients should be included in such studies to be representative of a given patient population and technique.^{[5](#page-14-0)}

Figure 1. Medline search strategy.

FIDUCIAL MARKERS FOR PROSTATE IMAGE-GUIDED RADIOTHERAPY

Feasibility and efficacy

The feasibility and efficacy of using FMs for prostate IGRT has been documented in the literature. $6-1$ $6-1$

Before in-room imaging was widely available, Crook et al^{[6](#page-14-0)} demonstrated significant prostate gland motion based on FM positions relative to bony landmarks on repeat CT scans in a study of 55 patients. They found the average prostate displacement in the posterior and inferior directions to be 6 mm and that 30% had displacements >10 mm posteriorly, which standard treatment planning margins would not have encompassed. They strongly recommended the use of implanted FMs for treatment setup verification as opposed to alignment using bony landmarks.

Crook et al findings^{[6](#page-14-0)} from 1995 were supported by Schallenkamp et al^{[9](#page-15-0)} in 2005 using MV electronic portal imaging (MV EPI) and digitally reconstructed radiographs, and then reconfirmed in 2013 by Paluska et al¹¹ using modern planning and imaging techniques. Paluska et al acquired weekly CBCT scans following setup to retrospectively reconstruct and verify dose delivered to patients receiving IMRT to the prostate with a simultaneous integrated boost to the proximal seminal vesicles (SVs). For bone setup using a 10-mm clinical target volume (CTV)–planning target volume (PTV) margin, inadequate prostate coverage was observed in 5 out of 29 patients, resulting in underdosing of the target. Despite a reduced CTV–PTV margin, the prostate coverage for FM-based setup was better. Schallenkamp et al and Paluska et al both proposed that prostate FMs, when used with a daily online imaging correction protocol, facilitate CTV–PTV margin reduction.

The largest study on the reliability of FMs was reported in a retrospective analysis of daily treatment setup data from 453 patients treated with IMRT using an offline correction protocol by van der Heide et al. 12 They reported minimal marker migration, accurate marker detection and time trends in relation to prostate motion but recommended caution when considering reducing planning margins owing to other sources of uncertainty such as target delineation and SV motion.

Much of the evidence in relation to prostate motion is based on setup data acquired using FM position measured using a range of imaging modalities. Nine studies investigating prostate motion and otherwise satisfying the search criteria were included.

In a study of 427 patients undergoing prostate IMRT treated using FM IGRT, Kotte et al 13 observed intrafraction motion >2 mm in a time frame of 5–7 min in 66% of patients. No correlation was found between fraction number and degree of motion. Motion was more frequent in the anteroposterior (AP) and superior–inferior directions. They recommended the use of FMs for prostate treatment setup and at least a 2-mm margin to account for intrafraction motion, not including other sources of

3D, three-dimensional; ADT, androgen deprivation therapy; CBCT, cone-beam CT; CTV, clinical target volume; EBRT, external beam radiotherapy; EPI, electronic portal imaging; EPID, electronic portal imaging device; FM, fiducial marker; GI, gastrointestinal; GU, genitourinary; IG, image-guided; IG-IMRT, image-guided intensity-modulated radiotherapy; IGRT, image-guided radiotherapy; IMD, intermarker distance; IMRT, intensity-modulated radiotherapy; INB, intraprostatic nerve block; kV, kilovoltage; MV, megavoltage; PCa, prostate cancer; PNB, periprostatic nerve block; PTV, planning target volume; RCT, randomized controlled trial; SABR, stereotactic ablative radiotherapy; SV, seminal vesicle; TAUS, transabdominal ultrasound; TP, transperineal; TR, transrectal; TRUS, transrectal ultrasound; TURP, transurethral resection of the prostate.

uncertainty. These findings are supported by data from other studies of prostate motion also based on FMs.^{[14,15](#page-15-0)}

FMs have been employed in assessing the increased precision required for stereotactic ablative radiotherapy. Quon et al, 16 using preand post-treatment 2D kV imaging of prostate FMs, concluded that intrafraction motion is small and that the degree of motion observed indicates that the time taken for delivery of step-and-shoot IMRT did not significantly increase prostate motion. However, it is possible that transient prostate displacements may have gone undetected. This idea is supported by Xie et al, 17 who described another approach to monitoring FM position using stereoscopic (SC) X-ray imaging during treatment and pausing treatment if outside a predefined threshold. They found significant motion with an image sampling rate of every 40 s and suggest a higher sampling rate may be appropriate for some patients. These findings would indicate that prostate motion is more significant than observed by Quon et $al¹⁶$ $al¹⁶$ $al¹⁶$ and also that pre- and post-treatment images may not be adequate to assess intrafraction motion.

FMs combined with online correction can minimize the uncertainty associated with aligning the prostate for IGRT and act as an aid to assessing the impact of prostate intrafraction motion. However, the evidence suggests that the method used to assess motion using FMs can produce varying results and therefore, changes to dose, planning margins and correction protocols should allow for this.

Online correction based on prostate FM position will not necessarily ensure coverage of other critical structures, for example SVs, if included in the PTV. Van der Wielen et al^{[18](#page-15-0)} used FMs to investigate prostate and SV deformation. In their study of 21 patients, analyzing prostate contours relative to FM position on repeat CT scans, they found prostate deformation to be small

[standard deviation $(SD) \le 1$ mm] and SV deformation, relative to FMs, significant (SD \leq 3 mm). De Boer et al^{[19](#page-15-0)} also report significant differences in the position of the prostate and SVs and describe a method in which SVs are included to ensure registration of both based on CBCT imaging. FM corrections are generally translational corrections only. Despite the differences reported in prostate and SV deformation, the addition of a rotational correction has been shown to allow only a modest re-duction in planning margins.^{[18,20](#page-15-0)}

Nichol et $al²¹$ $al²¹$ $al²¹$ used repeat MRI scans to assess prostate deformation relative to FMs in 25 patients and suggest that FMs are a good surrogate in the left–right direction but not as good in the AP or craniocaudal directions. They identified isolated cases of large changes in prostate volume and shape and suggest that increases in prostate volume may result in a geographic miss if using reduced margins.

The evidence spanning almost 20 years would indicate that alignment to FMs is feasible and more effective at localizing the prostate for radiotherapy than alignment to external skin marks or bony anatomy on planar imaging.

FIDUCIAL MARKER IMPLANTATION

Implantation of FMs into the prostate involves a surgical procedure which carries associated risks including pain, bleeding, inflammation and infection, but on balance, it is safe and well tolerated.

There are two main approaches: transrectal (TR) or transperineal (TP), both usually under TR ultrasound (TRUS) guidance. A TR technique is proposed by Shinohara and Roach^{[22](#page-15-0)} as suitable for insertion of gold markers and electromagnetic transponders. The technique, developed over 10 years with 705 patients, is similar to a TRUS-guided biopsy procedure. They reported one case of urinary tract infection and no cases of bleeding or haematuria. Linden et al^{[23](#page-15-0)} also report no complications using a similar technique in a retrospective review of 98 males.

Both studies describe preparation including prophylactic antibiotics, rectal enemas, cessation of anticoagulant/antiplatelet medication, local anaesthesia and preparation of markers and both employed a triangular arrangement of markers, i.e. right base, left mid-gland or base and right apex. Shinohara and Roach highlight the importance of avoiding of the urethra to ensure markers are not subsequently lost to voiding. They also refer to "tenting" of the prostate by the needle, which on TRUS may give the appearance of being in the prostate when in fact the needle has not penetrated the capsule. This, as well as placing within the urethra, may explain the "loss" of some markers reported by other investigators.^{[6](#page-14-0)[,24](#page-15-0)}

Igdem et $al²⁴$ prospectively quantified patient-reported morbidity with 135 out of 177 patients completing a questionnaire relating to side effects from TRUS-guided TR implantation of 3 gold FMs. No anaesthesia was used. 5 patients reported rectal bleeding and haematuria was experienced by 20 patients, although none required additional medication or intervention. Three patients experienced urinary infection requiring additional antibiotics. Using the Wong Baker pain scale, 25 36% of patients indicated 2 (mild) on a 0–5 scale and the mean pain score was 1.7. Gill et al^{[26](#page-15-0)} reported on 234 patients undergoing the same TRUS TR procedure with the addition of a periprostatic nerve block, which is considered the gold standard for TRUS-guided prostate biopsy.^{[27](#page-15-0)} Of those patients who gave a pain score, only 21.9% of patients in total scored pain at 2 or higher and 75% patients scored pain as 1 or 0 (very mild or no pain), and the mean pain score was lower than that observed by Igdem et al at 1.1.

Langenhuijsen et al 28 reported on 209 patients who underwent TRUS TR implantation of 4 gold markers without a preceding enema or local anaesthesia. Using a different pain scale, 50% of patients thought pain was less than that of biopsy, 40% patients thought it was comparable and 10% patients thought it was worse.

Many authors report low or moderate rates of complications following FM implantation and conclude that TRUS-guided implantation of FMs is safe and well tolerated in the majority of patients.[23,24](#page-15-0),[28](#page-15-0)–[30](#page-15-0) One might expect a higher proportion of complication rates with such an invasive procedure. In general, these studies are based on retrospective voluntary patient reporting and therefore, less serious side effects may have been underreported. Another study by Loh et $al³¹$ $al³¹$ $al³¹$ suggests that the risk from FM implantation is underestimated. They report an infective complication rate of 5.6% minimum from 297 patients who underwent TR FM implantation, which is similar to that reported for prostate biopsy complication rates.³

Moman et $al³³$ $al³³$ $al³³$ compared TR and TP routes of implantation in 402 and 512 patients, respectively. Toxicity and subsequent marker migration were similar. They have since continued to use

the TP route and have omitted the use of antibiotic therapy since reporting their findings and report no infections several months following. It would be reasonable to suppose that TR implantation would result in a higher incidence of infection, particularly when no rectal evacuation is employed. However, the evidence does not seem to suggest this. This may be due to the use of prophylactic antibiotic therapy. A significant saving and benefit to the patient could be realized if TP implanting removed the need for antibiotics, as suggested by Moman et al. 33 Indeed, the benefits of reducing the need for antibiotics may be more far reaching. Recent studies have demonstrated increasing rates of antibiotic-resistant infection following TR intraprostatic procedures, suggesting TP techniques may become more frequent in the future.^{32,[34](#page-15-0)}

Assuming the use of antibiotics is standard, there is no evidence to recommend one technique over the other. Based on the evidence presented, both approaches are safe and well tolerated. In clinical practice, the choice may be pragmatic and predetermined by the facilities and expertise available. Those with prostate brachytherapy expertise and capacity may choose the TP route, while those employing the skills of a biopsy clinic may rely on the TR route. Factors common to both should be standardized for the purpose of FM implantation, such as use of enemas, anaesthesia, patient follow-up, placement of markers and timing of implant prior to CT planning.

NUMBER AND TYPES OF FIDUCIAL MARKERS

FMs exist in a variety of shapes, sizes and materials and are commercially available from a variety of vendors. Gold markers are by far most frequently used for prostate IGRT. This is due to the fact that they are widely available and are visible using MV or kV image guidance. The basic specification for an FM includes radio-opacity for a given imaging modality (or preferably a number of imaging modalities), that they are readily available and that they are not prohibitively expensive.

This review elicited only one study specifically comparing types of markers. Fonteyne et $al³⁵$ $al³⁵$ $al³⁵$ investigated five different gold FMs. They observed a better correlation between automatic CBCT image-matching results and manual match results for the largest FM, which was $20 \text{ mm} \times 0.75 \text{ mm}$, than for smaller FMs, suggesting that larger markers may result in more consistent setup data when comparing automatic and manual alignment. However, they also state the largest FM resulted in increased image artefact. Artefact created by FMs on CT and CBCT is one of the main disadvantages of using gold or entirely metallic markers and may add to the degree of uncertainty associated with con-touring and matching the prostate^{[36](#page-16-0)} and may also result in in-accurate treatment planning.^{[37](#page-16-0)} One study suggests that platinum is superior to gold in terms of its visibility on MRI and therefore preferable as an aid for CT/MRI registration.^{[38](#page-16-0)} This would have the disadvantage of being more expensive than gold.

Non-metallic FMs have been around for a number of years and claim to overcome the problem of metal-induced image artefacts. Despite this, in the evidence presented in this review, little attention has been given to what effect FMs may have on the dose distribution within the prostate. Dose and effects on dose

distribution require modelling and measurement using geometrically appropriate phantoms and techniques and therefore, a full discussion is beyond the scope of this review. However, there is a growing body of evidence on the dosimetric consequences of various types of prostatic FMs. The effect may be minimal, but some reports suggest that using gold FM dose may be reduced by as much as 20% using photons^{[39](#page-16-0)} and reduced by up to 85% in proton therapy in the area immediately around the FM.[40](#page-16-0)

Many authors have reported studies based on the use of three or four implanted gold markers. $6,7,9,12,14,41$ $6,7,9,12,14,41$ $6,7,9,12,14,41$ $6,7,9,12,14,41$ $6,7,9,12,14,41$ $6,7,9,12,14,41$ Most studies employ three FMs placed in a 3D triangular arrangement to facilitate assessment in the three cardinal directions (Figure 2).

Using gold FM coils, de Boer et $al⁴²$ $al⁴²$ $al⁴²$ evaluated the impact of the number of markers on matching and concluded that two accurately locate the prostate if adequately spaced. Other investigators favour three or more markers in the event that one or more migrate or are somehow lost.^{[43](#page-16-0)}

Nickel–titanium stents based on those used in the management of urinary obstruction have been adapted and tested for feasibility in prostate IGRT. They are visible on kV and MV images, create no artefact on CT and are suitable for MRI.^{[44](#page-16-0)} Further evidence is needed to justify the complex surgical procedure and associated risks required to implant these.

OTHER TYPES OF MARKER

Real-time target tracking has been developed and used clinically using electromagnetic transponders.^{[45,46](#page-16-0)} Radiofrequencyemitting transponders are implanted into the prostate similar to FMs. They are detected and monitored by an external magnetic array linked to the treatment room and located in relation to the isocentre and couch corrections applied. This system addresses intrafraction motion and theoretically eliminates operator subjectivity associated with image analysis. No ionizing radiation is received by the patient; however, this also means

Figure 2. Three gold fiducial markers detected on anteroposterior megavoltage electronic portal imaging.

there is no radiographic record of treatment and no assessment of bladder, rectum or SV position is possible. Routine use of this technology is expensive.

An alternative type of surrogate first described by Shchory et $al⁴⁷$ was clinically evaluated by de Kruijf et al, 48 who used radioactive iridium-192 as an implanted tracer in 20 patients. They report this approach as feasible and safe. With the exception of reduced image artefact, no particular advantages are apparent over inert FMs. Given the additional radiation dose received by the patient, and the additional precautionary measures required during implantation, this method is not widely used.

Three gold markers as per Figure 2 are most commonly used. Whatever type and arrangement is used, each institution should be consistent, use standardized procedures and develop expertise in their chosen approach. Non-metallic markers offer an attractive alternative in terms of reduced cost, reduced image artefact and potentially reduced dosimetric consequences and should be further investigated.

PROSTATE FIDUCIAL MARKER MIGRATION

The efficacy of FMs for prostate IGRT is based on the assumption that each marker will remain fixed in position between planning and treatment and for the duration of radiotherapy. True migration of FMs is likely rare and when it does occur, the effect is minimal or negligible. Prostate gland distortion before or during radiotherapy can occur owing to: (1) post-implant oedema or bleeding, (2) changes in surrounding organs at risk (OARs) and (3) shrinkage due to androgen deprivation therapy.

A number of reports focused on this issue $29,49-52$ $29,49-52$ $29,49-52$ $29,49-52$ and collectively evaluated a combined total of 144 patients with between 3 and 5 gold FMs. Each group recorded intermarker distance (IMD) as a measure of FM migration, with the exception of Delouya et al, 51 who compared the 3D position of the FMs from planar imaging with that at planning. Mean migration observed was between 0.8 mm $(=/-0.3 \text{ mm SD})^{52}$ $(=/-0.3 \text{ mm SD})^{52}$ $(=/-0.3 \text{ mm SD})^{52}$ and 1.2 mm $(±0.2 \text{ mm})$ SD),^{[49](#page-16-0)} (\pm 0.6 mm SD).^{[51](#page-16-0)} Pouliot et al^{[29](#page-15-0)} report a mean SD of 1.3 mm (range 0.44–3.04 mm).

From their study of 453 patients, van der Heide et $al¹²$ report minimal changes in IMD, demonstrating that markers are stable in relation to each other and can be detected accurately.

In general, the evidence suggests that FM migration is not significant but raises a number of issues to consider when using FMs.

Kupelian et al⁵⁰ highlight one such issue when they observed two patients demonstrating IMD variation where the SD was >4 mm (maximum 4.2 mm). In each case, one particular IMD varied owing to variations in rectal filling. The proportion of IMD variation contributed by actual migration in such cases is difficult to establish. Migration may not reliably be measured unless all other surrounding physical conditions remain constant. Such cases, as observed by Kupelian et al,^{[50](#page-16-0)} demonstrate that if the prostate has changed shape, the inconvenient reality is this cannot be corrected by standard IGRT conventions with or without the use of FMs. Deformable image registration and adaptive planning strategies are required to address this problem, a detailed discussion of which is beyond the scope of this review, but an overview of these topics is given by Maintz and Viergever,^{[53](#page-16-0)} Kashani et al⁵⁴ and Kupelian and Meyer.^{[55](#page-16-0)}

Pouliot et al²⁹ measured IMDs of 3 gold implanted markers in 11 patients using orthogonal MV image pairs. They observed a time trend in three patients where the distance between all three markers decreased over the course of radiotherapy, suggesting overall shrinkage of the prostate. Volume reduction was subsequently confirmed on CT for one of the patients. They suggest that all three patients received neoadjuvant hormones, which may have caused prostate shrinkage. However, shrinkage was not observed in all patients who received hormone therapy, indicating there are other influencing factors. Details of the timing of fiducial implantation were not given. Anatomical or physiological changes have the potential to cause or mimic marker migration and therefore, approaches minimizing this should be considered. Oedema and inflammatory responses initiated during implantation may still be present during CT planning. These may then resolve before or during treatment, resulting in volume changes or deformation. This could potentially alter the position of the FMs and introduce systematic positioning error. This is supported by the findings of Delouya et al.[51](#page-16-0) Of 31 patients, 7% of patients demonstrated "significant shrinkage". The maximum reduction was 95% of the volume at planning. They observed that of 31 patients included in their study, 23 patients had their CT planning scan the same day as FM implantation and had larger migrations than those whose CT planning was later than the day of implantation. The actual differences in migration are not reported, but this group subsequently changed their local practice to allow a minimum of at least 3 days between implantation and CT planning.

FM migration can occur, but prostate gland deformation is more commonly observed. However, in clinical practice, it is unlikely that migration or deformations are significant limitations to the utilization of FMs for prostate radiotherapy, but standardized approaches to minimize known causes should be incorporated.

IMAGING MODALITIES

Evidence supporting the use of prostate FM IGRT is largely based on the use of 2D imaging (MV or kV). There is significantly less evidence available on the use of FMs with 3D imaging such as CBCT or ultrasound.

In a study of 36 patients, Barney et $al⁵⁶$ $al⁵⁶$ $al⁵⁶$ compared their standard technique of kV imaging of FMs with CBCT soft-tissue alignment to ascertain the degree of correlation. They reported mean and absolute differences in setup data between the two modalities and observed a mean difference of 3 mm in two of three dimensions, which affected target coverage in 25% of all shifts observed. In a larger study, Gill et al investigated interfraction prostate displacement in 333 patients and compared MV EPI and FMs with KV imaging of FMs. They found a statistically significant smaller setup error with MV imaging in all directions, but particularly so in the AP direction. 41 It is possible that setup

error was underestimated owing to the inferior image quality of MV *vs* kV images. This would be more apparent on lateral images (used to assess the AP position) owing to increased X-ray attenuation. Regardless of the reasons, the differences reported by these investigators may result in different planning margins being derived depending on which imaging modality is used to generate treatment setup data. According to Gill et al, 41 this may be most likely in the AP direction which will impact clinically at the prostate–rectal interface. This is where the CTV–PTV margin is often reduced to avoid rectal toxicity, thus increasing this risk of missing the posterior aspect of the prostate or overdosing the rectal wall.

Soft-tissue contrast is not optimal on CT or CBCT; therefore, it can be reasoned that accurately identifying the position of the prostate based on CBCT is a subjective process and there is evidence to support this.^{[57,58,36](#page-16-0)} A key issue when using CBCT without FM is interobserver variability due to poor soft-tissue contrast, which can introduce a source of systematic error in the application of treatment setup corrections, which by definition contribute to the error in margin calculations. FMs serve to eliminate a degree of the uncertainty associated with soft-tissue alignment, but cannot overcome other contributory factors in-cluding the variations associated with imaging modality.^{[56](#page-16-0),[41](#page-16-0)}

When used with 2D imaging alone, FMs do not enable visualization of the target or assessment of organ motion or deformation. It has been reported that a large rectal volume is predictive of poorer treatment outcome^{[59](#page-16-0)} and therefore requires assessment in conjunction with accurate prostate alignment to ensure treatment efficacy. In this regard, CBCT may be preferable to 2D imaging, or it could be reasoned, should be used as an adjunct to planar imaging with FMs. While the accuracy of a CBCT prostate match may be inherently variable, it will nevertheless reveal gross anatomical differences in rectal and also bladder volumes that may significantly alter the planned dose distribution to the target and/or OARs. This information alerts therapists to take action to improve this, thereby optimizing treatment delivery. This review found no studies directly comparing ultrasound detection of FM with detection using another imaging modality. This may be because FMs are not easily vi-sualized on transabdominal ultrasound (TAUS).^{[35](#page-15-0)} Further research into the use of in-room ultrasound techniques for FM IGRT is warranted.

There are limited studies on the use of FMs with SC imaging and six degrees of freedom capability. Using the ExacTrac® 6D IGRT system (Brainlab AG, Feldkirchen, Germany), Shi et al^{[60](#page-16-0)} report mean shifts of 0.2, -1.09 and -0.93 mm in the lateral, longitudinal and vertical directions, respectively, with corresponding rotational errors of 0.25, 0.1 and 0.02° for all fractions in 43 patients with PCa with FMs. Rotational corrections were not applied. Those exceeding 2° were investigated and repositioned.

In a series of 40 patients, Fuller et $al⁶¹$ $al⁶¹$ $al⁶¹$ compared treatment setup errors derived from in-room TAUS imaging of the prostate with those from kV SC images of prostate FMs for radiotherapy verification. As in Barney et al, the purpose of this comparison study was not to establish which modality was superior, although

treatment was corrected and treated according to SC FM position. They concluded that concordance of resulting TAUS prostate and SC FM measurements was "poor" or "unacceptable" with 95% of measures within 15 mm.^{[61](#page-16-0)} Numerous other groups have found significant differences in treatment setup data derived from TAUS soft-tissue assessment compared with FM data from other modalities, greater variation within ultrasound data and ultrasoundderived PTV margins may be up to 3–4 times smaller than those reported in the literature.^{[43,62,63](#page-16-0)} Fuller et al⁶¹ also provide a useful narrative on the inherent difficulties of comparing IGRT modalities which briefly include the lack of an established ground truth and the statistical inaccuracies of comparing data generated by incomparable methods or devices.

The evidence presented here would suggest that treatment setup error data, with or without the use of FMs, are not interchangeable between imaging modalities and may generate different planning margins for the same treatment site and technique. Larger multicentre studies comparing standardized IGRT methods are needed to establish a gold standard IGRT approach that will enhance the benefits of FMs.

With currently available IGRT solutions, it is likely that a combined IGRT approach employing CBCT with FMs or CBCT in addition to FMs and planar imaging will provide the best possible assessment of prostate position and changes in OARs.

CLINICAL IMPACT OF PROSTATE FIDUCIAL MARKER IMAGE-GUIDED RADIOTHERAPY

Many studies demonstrate that the use of FMs improves prostate targeting during image-guided (IG) external beam radiotherapy. It is less clear what clinical impact this has in terms of patientreported toxicity and overall survival and no prospective randomized controlled trials have been performed.

Paluska et al,^{[11](#page-15-0)} Cheung et al^{[64](#page-16-0)} and Skarsgard et al⁶⁵ have all demonstrated the feasibility of reducing PTV margins with the use of FMs. Paluska et al proposed that a 10-mm CTV–PTV margin used with daily bone setup could be reduced to 7 mm using FMs and daily imaging. Furthermore, they observed better CTV coverage using FMs and reduced margins compared with bony setup plus a 10-mm margin. Toxicity was not reported in this study. However, by further limiting dose to normal surrounding structures, the PTV margin reduction theoretically reduces toxicity, since reducing the volume of rectum receiving 60 Gy or more has been shown to be associated with a reduction in rectal toxicity.^{[66](#page-17-0)} In addition, reducing the PTV facilitates dose escalation and may improve progression-free survival.

Cheung et al^{64} al^{64} al^{64} prospectively assessed acute toxicity. They delivered a hypofractionated IMRT boost using patient-specific margins, the average of which was 3, 3 and 4 mm in the lateral, superior–inferior and AP directions, respectively. These margins were based on their assessment of intrafraction prostate motion using daily FM IGRT. They reported acceptable acute toxicity; however, Grade 3 genitourinary toxicity (National Cancer Institute Common Toxicity Criteria v. 2.0) was reported in 3 out of the 33 patients included in the study. In a more recent retrospective study, Takeda et al^{67} analyzed the outcome data for 141 patients treated using high-dose

FM IG-IMRT and reported that treatment is well tolerated based on 5-year outcomes. Cheung et al and Takeda et al report findings which are reassuring in terms of demonstrating acceptable toxicity using reduced margins, but neither had a non-FM IGRT control group; therefore, it is unclear what contribution the use of FMs made to the outcome data.

The impact of IG-IMRT with FMs and reduced margins was compared with IMRT without FM IGRT by Chung et al^{68} al^{68} al^{68} in a prospective non-randomized study of 25 patients. Radiation Therapy Oncology Group and Common Terminology for Adverse Events scores for rectal and bladder toxicity were consistently lower in the FM IG-IMRT group. These findings are partially supported by Singh et $al⁶⁹$ in relation to rectal toxicity in a large patient cohort, where 154 patients had FM IGRT and 128 patients had non-IGRT. There was no difference in reported urinary symptoms in each group.

Zelefsky et al,^{[70](#page-17-0)} Kok et al⁷¹ and Sveistrup et al^{[72](#page-17-0)} compared large cohorts of patients retrospectively, where the main difference was the use or not of FMs for image guidance. All report improvements in urinary and gastrointestinal toxicity for the FM groups. Kok et al observed a reduced incidence of gastrointestinal toxicity despite a higher dose of 78 Gy in the FM group compared with 74 Gy in the non-FM group, but no difference in biochemical failure-free survival was observed. Sveistrup et al observed a biochemical progression-free advantage for the FM group, but this was not statistically significant.

There is convincing evidence that FM IGRT improves the accuracy of prostate targeting and some evidence that using FM IGRT reduces treatment-related toxicity without compromising treatment outcomes; therefore, it is unlikely a prospective randomized control trial comparing FM IGRT with non-FM IGRT will ever be performed.

PROSTATE CALCIFICATIONS AS FIDUCIAL MARKERS

The risks of prostate FM implantation described earlier are justified, provided a similar non-invasive approach does not exist. Alternatives that remove the need for artificial FMs would also eliminate the use of anaesthesia and antibiotics and save significant health service time and resources. For example, MRIbased radiotherapy using MRI linear accelerators may in the future offer a non-invasive and also non-ionizing approach to prostate IGRT which may not require FMs.

Prostate calcifications (PCs) are small ovoid or round bodies impregnated with calcium phosphate and calcium carbonate and are reported to be present in almost 90% of prostatectomy specimens.[73](#page-17-0) It has been reported that up to 35% of patients undergoing prostate radiotherapy have calcifications visible on CBCT.^{[74](#page-17-0)} PCs may be detected coincidentally from histological or radiological findings, and patients are often asymptomatic. The significance of PCs is not well understood, but there is some evidence to suggest an association of PCs and prostatic in-flammation, lower urinary tract symptoms and PCa.^{[75](#page-17-0)-[77](#page-17-0)} Their relevance here is that PCs visible on radiographic images may present a natural alternative to surgically implanted markers.

Zeng et al⁷⁴ investigated the stability of PCs with a view to using them as a surrogate for prostate position during IGRT and found that they were stable. A subsequent study recommended the use of central intraprostatic PCs for IGRT.^{[78](#page-17-0)} More encouraging is the work by Kim et al,^{[79](#page-17-0)} who used PC mismatch as the end point in assessing similarity metrics on CBCT. They found the presence of PCs increased the success of CT/CBCT image registrations. These findings are based on 4, 10 and 14 patients, respectively, and therefore, investigation using larger patient numbers is warranted.

Given the potential for reducing risk and inconvenience to patients of surgically implanted FMs and the potential cost savings, PCs as a natural FM justifies more in-depth research. A prospective feasibility study investigating this is under way at our centre. The study Calcifications as an Alternative to Surgically Implanted Fiducial Markers for Prostate IGRT will directly compare FMs and PCs for the purpose of online image matching and correction. This study will also prospectively collect patient feedback regarding their experience of FM implant.

CONCLUSION

FMs present a good surrogate for the position of the prostate and may reflect prostate gland motion or deformation. Changes in rectal and bladder volume, prostate deformation and SV motion are not detected by FM imaging alone.

A combination of FM alignment and soft-tissue analysis is currently the most effective and widely available approach to ensuring accuracy in prostate IGRT. Standardized clinical protocols are needed to enable comparison of treatment accuracy data, toxicity and treatment outcomes. Further research into the use of TAUS with FMs and the dosimetric implications of FMs is warranted.

There is a lack of randomized studies on the benefits of FM IGRT that control for other parameters such as the effect of hormone therapy and pre-existing urinary symptoms.

Marker migration is minimal. Anatomical or physiological changes such as rectal and bladder filling may cause deformation or distortion of the prostate gland and result in the apparent migration of FMs. Other factors such as the timing of CT planning following implantation and the use of androgen deprivation therapy may influence the apparent stability of markers.

Implantation of FMs is well tolerated, but surgical techniques and toxicity data require standardization. Development of FM implantation techniques that facilitate a reduction in the use of prophylactic antibiotic therapy should be considered in light of the global problem of multiresistant bacteria.

Organ deformation and conflicting alignment of multiple targets requires 3D verification, deformable image registration and adaptive planning techniques and cannot be addressed by conventional IGRT with or without the use of FMs.

Despite the advent of MR-guided radiotherapy, such technology is unlikely to become the standard of care in most centres for some time. Also, while superior in terms soft-tissue contrast, MRI is contraindicated for some patients and since dose escalation, hypofractionation and stereotaxy are already here, the authors suggest that the future of FMs in prostate IGRT is secure for the foreseeable.

It is clear from the evidence that FMs are a useful aid to enhancing the accuracy of prostate IGRT. However, given the issues in relation to FM implantation including cost, risk of infection and antibiotic resistance, there is merit, perhaps also a duty, to investigate a natural alternative to FMs that has the potential to benefit a significant proportion of the PCa population.

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