MAJOR PAPER

Juxtacortical Lesions in Multiple Sclerosis: Assessment of Gray Matter Involvement Using Phase Difference-enhanced Imaging (PADRE)

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Purpose: In multiple sclerosis (MS), a juxtacortical lesion at the border between the gray matter (GM) and subcortical white matter (WM) may often involve the GM. A recently developed, phase-weighted magnetic resonance imaging (MRI) technique "phase difference enhanced imaging (PADRE)" can delineate the GM and WM clearly due to the difference in myelin concentration. We evaluated whether PADRE is useful for the detection of GM involvement in the juxtacortical MS lesions.

Methods: One neuroradiologist reviewed the conventional MRI in 13 MS patients and selected 48 juxtacortical lesions. At the first reading session with the conventional MRI alone (T₂-weighted imaging, and two-dimensional and three-dimensional fluid-attenuated inversion recovery), two other neuroradiologists classified the lesions into three patterns according to their anatomical locations: (a) subcortical WM lesions involving the subcortical WM alone; (b) intracortical (IC) lesions involving the GM alone; (c) mixed GM/subcortical WM (mixed) lesions involving the both subcortical WM and GM. We defined the subcortical WM as a WM within a distance of 10 mm from inner edge of the GM. For the analyses, we excluded the white matter lesions further than 10 mm from inner edge of the GM. At the second reading session MRI and PADRE were available and the radiologists re-evaluated their prior classification.

Results: At the first reading session, 27 lesions were classified as (a), 1 as (b), and 20 as (c). Therefore, a total of 21 lesions (44%) were judged to involve the GM. At the second reading session, the classification of 15 (31%) lesions changed; all 15 lesions were judged to involve the GM on the PADRE. Interobserver agreement (kappa value) was 0.84 for the first- and 0.95 for the second reading session.

Conclusion: PADRE is useful for detecting GM involvement of the juxtacortical MS lesions.

Keywords: multiple sclerosis, phase difference enhanced imaging, juxtacortical lesion, gray matter involvement

Introduction

Multiple sclerosis (MS), an inflammatory demyelinating disease of the central nervous system, usually

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such as T₂-weighted imaging (T₂WI), fluid-attenuated inversion recovery (FLAIR) imaging, and T₁-weighted imaging (T₁WI) with and without gadolinium-based

and for assessing the efficacy of treatment.

affects young adults and leads to chronic invalidism.

The high sensitivity of magnetic resonance imaging

(MRI) facilitates the detection of macroscopic tissue

abnormalities in MS patients. Conventional MRI studies

contrast enhancement yield information important for

diagnosing MS, for understanding its natural history,

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Histopathologically, in patients with MS, a juxtacortical lesion at the border between the gray- and subcortical white matter (GM, WM) often involves the GM. 1-3 Although the plaque burden within the GM seems to be correlated with neurologic impairment in MS patients, on conventional MRI scans it can be difficult to identify GM involvement. Double inversion recovery (DIR) MRI 4-6 and phase imaging using high-field MRI^{7,8} are superior to conventional MRI for depicting MS lesions close to or in the GM. However, the signal-to-noise ratio (SNR) on DIR MRI scans is low, although the patient-specific optimization of three-dimensional (3D)-DIR is now feasible and further improves GM-WM contrast.9 Moreover, 7T MRI can only be used in research studies. A new phaseweighted MRI technique, phase difference-enhanced imaging (PADRE), uses the phase difference between the target and surrounding tissue to enhance the contrast of the target tissue. 10,11 Choosing the appropriate phase differences allows the variation in tissue contrast using single imaged magnetic resonance (MR) data. Some PADRE images yield a level of contrast that could not be realized with earlier phase techniques. Kakeda et al.10 and Ide et al.¹² who reported that various fibre tracts were delineated on PADRE images, speculated that PADRE enhanced the identification of differences in myelin density. Under the hypothesis that the PADRE technique is highly sensitive to the myelin concentration and that it presents MS lesions in terms of myelin loss (demyelination), we evaluated its usefulness for the detection of GM involvement of the juxtacortical lesions of MS patients.

Materials and Methods

Patient selection

Our institutional review board (The Hospital Ethics Committee of Medicine and Medical Care, University of Occupational and Environmental Health, Japan) approved this retrospective study and waived informed consent. The patient records/information was anonymized and de-identified prior to analysis.

Thirteen patients (4 men, 9 women, mean age 35.6 years, range 23–52 years) with clinically definite MS¹³ were included. Their median expanded disability status scale score (EDSS) was 4.0 and the mean disease duration was 75.0 months. MS was diagnosed by two neurologists (K.O. with 24 years of experience and H.A. with 25 years of experience in neurology). All patients were clinically evaluated between June 2012 and April 2013 and underwent PADRE in addition to routine brain MRI including T₂WI, 2D and 3D FLAIR imaging.

MR imaging

All studies were performed on a 3T MRI system Signa EXCITE 3.0T (GE Healthcare Waukesha, Wisconsin,

USA) using a dedicated eight-channel phased-array coil (USA Instruments Aurora, Ohio, USA). PADRE images were obtained with a 3D multi-echo spoiled gradient echo (GRE) sequence. ¹⁴ The imaging parameters were: axial planes covering the brain; number of echo times, 11; first echo time, 4.5 msec; uniform echo time spacing, 5 msec; repetition time, 58.4 msec; flip angle, 15°; band width per pixel, \pm 62.5 Hz; field of view, 22 × 16.5 cm; acquisition matrices, 320 × 416; slice thickness, 1.5 mm; imaging time, 7 min 1 sec. A parallel imaging method, the array spatial sensitivity encoding technique, was used with a reduction factor of 2.

All patients were also scanned using our standard brain MRI protocol for MS patients including axial T₂WI, and 2D and 3D FLAIR imaging. The imaging parameters were $4500/85/1/10.9/512 \times 512/2 \text{ min } 10 \text{ sec (repeti$ tion time msec/echo time msec/number of excitation/ echo-spacing/matrix/imaging time) for T₂-weighted fast spin-echo (FSE) imaging, and 12,000/140/2600/2/9.1/ $224 \times 256/3 \, \text{min} \, 20 \, \text{sec}$ (repetition time msec/echo time msec/inversion time/number of excitation (NEX)/echospacing/ matrix/imaging time) for 2D FLAIR imaging. T₂WI and 2D FLAIR images were acquired with a section thickness of 4 mm, an intersection gap of 1 mm, and a field of view of 22 cm. The parallel imaging technique (reduction factor, 2) was used only for T₂WI. For 3D FLAIR imaging, the parameters were 10,000/141/2478/1/62.5/ $224 \times 224/22$ cm/1.2 mm/2.86/5 min 30 sec (repetition time msec/echo time msec/inversion time/NEX/echo train length/matrix/field of view/section thickness/reduction factor/imaging time).

PADRE technique

PADRE was as described by Kakeda et al. ¹⁰ Its power lies in its phase-difference selection which enhances the magnetic properties of the target tissue. While susceptibility-weighted imaging (SWI) identifies only phase differences related to vessels, especially veins, the PADRE technique classifies and selects various phase differences, $\Delta\theta$, to enhance different tissues. It enhances all tissues on the magnitude image $|\rho|$ with the enhancing function w ($\Delta\theta$). Finally, the PADRE image ρ_{PADRE} is reconstructed as:

$$\rho_{PADRE} = w \left(\Delta \theta \right) |\rho|$$

We optimized the reconstitution parameters of PADRE based on Kakeda et al. ¹⁰ and we reconstructed SWI-like images from the MR data.

Image interpretation

Evaluation of artifacts on PADRE images: To determine the possible rate of artifacts misinterpreted as lesions in the juxtacortical area, PADRE images of five healthy subjects with normal findings on conventional MRI scans were read by two experienced neuroradiologists (J.M. and

S.K., with 11 and 16 years of experience in neuroradiology, respectively). Five healthy control subjects (1 man and 4 women) had a mean age of 35.4 ± 8.96 years (range 26–49).

Lesion identification: We defined MS lesions as hyperintense lesions on conventional MR images (T₂WI, 2D and 3D FLAIR images). On PADRE images, MS lesions were defined as sharply demarcated areas of high signal intensity compared to the adjacent normal-appearing brain parenchyma. One radiologist (K.F. with 6 years of experience in neuroradiology) reviewed the conventional MR images of the 13 MS patients and selected 48 juxtacortical lesions in 6 patients (6 women; mean age, 36 years; range, 23–48 years). The other seven patients had no juxtacortical lesions.

Observer study: Two radiologists (J.M. and S.K.) participated in the observer performance study of 48 juxtacortical lesions. At the first reading session they were shown only the conventional MR images. They classified the lesions into three patterns according to their anatomical locations: (a) subcortical WM lesions involving the subcortical WM alone; (b) intracortical (IC) lesions involving the GM alone; (c) mixed GM/ subcortical WM (Mixed) lesions involving the both subcortical WM and GM.15 We defined the subcortical WM as a WM within a distance of 10 mm from inner edge of the GM. For the analyses, we excluded the white matter lesions further than 10 mm from inner edge of the GM (Fig. 1). At the second reading session MRI and PADRE images were available and the radiologists re-evaluated their prior classification of the juxtacortical lesions. We then compared the number of lesions assigned to each category in the two sessions.

Statistical analysis

Inter-observer agreement for quantitative and qualitative assessments was calculated as a weighted κ value. The strength of the agreement was considered fair for $\kappa=0.21\text{--}0.40,$ as moderate for $\kappa=0.41\text{--}0.60,$ as good for $\kappa=0.61\text{--}0.80,$ and as excellent for $\kappa=0.81$ or greater.

Results

Evaluation of artifacts on PADRE images

Both radiologists agreed that the signal intensity of the GM was homogeneously slightly hyperintense, and that the signal intensity of the subcortical WM was homogeneously hypointense vis-à-vis the GM in all healthy volunteers (Fig. 2). They detected no abnormalities in the juxtacortical area of the volunteers.

Observer study

Table 1 shows the results of the observer study for each reading session. Of the 48 juxtacortical lesions,

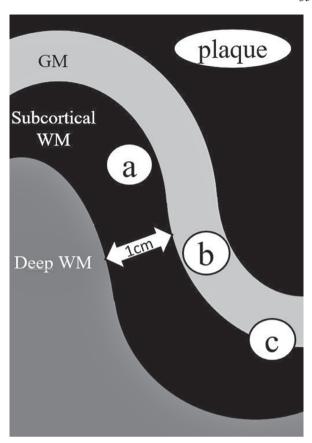


Fig. 1. Classification of the 48 juxtacortical MS lesions. Involvement is of (a) subcortical WM alone, (b) GM alone, (c) subcortical WM and GM. We defined the subcortical WM as a WM within a distance of 10 mm from inner edge of the GM. GM, gray matter; MS, multiple sclerosis; WM, white matter.

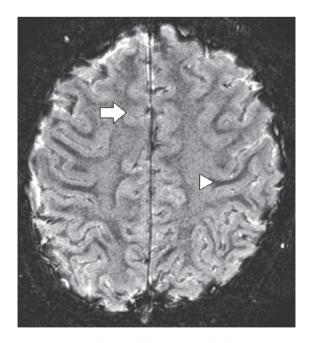


Fig. 2. PADRE image of a 35-year-old healthy woman. The signal intensity of the GM is homogeneously slightly hyperintese (arrow). The subcortical WM is homogeneously hypointense vis-à-vis the GM (arrowhead). GM, gray matter; WM, white matter.

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21 (44%) were judged to involve the GM in the first session. The classification of 15 lesions changed in the second session; all had been judged not to involve the GM. Consequently, a total of 36 lesions (75%) were found to involve the GM on PADRE images (Fig. 3). Interobserver agreement was moderate (kappa = 0.84) for the first- and excellent (kappa = 0.95) for the second reading session.

Discussion

As our study assessed the potential additional diagnostic value of PADRE for the detection of juxtacortical lesions with GM involvement in MS patients, we evaluated only the lesions that could be detected on conventional MRI images. We found that on PADRE images the number of juxtacortical lesions with GM involvement was greater than on conventional MRI scans and that interobserver agreement was better for PADRE images.

Phase images from GRE sequences depict brain structures at much greater detail than do the corresponding conventional MRI scans. While the origin of the susceptibility contrast on the phase images is not fully understood, differences in the myelin level, ¹⁶ the relative

volume and oxygenation state of blood, ^{17,18} iron deposition, ^{16,19,20} the chemical exchange between water and macromolecular protons, ²¹ and the orientation of underlying WM fiber with respect to the main magnetic field ²² have been suggested. Kakeda et al. ²³ identified nerve fiber as low signal intensity bands on PADRE images; they speculated that the myelin concentration was the main factor that determined the low signal intensity on PADRE images. Based on an earlier study, we attempted to optimize the reconstitution parameters of PADRE to enhance the myelin density. ¹²

The subcortical WM fills the space between the deep WM and the GM; it contains a larger amount of nerve fibers, not only the large axonal bundles but also the U-fiber. Our observation that PADRE delineated the subcortical WM as a low signal intensity area suggests a higher myelin content. In contrast, the GM was slightly hyperintense. Although the precise mechanisms underlying the signal intensity of the GM are unclear, the myelin content, ¹⁷ cellular composition, vascularization, and the iron content might affect the signal intensity of the GM on PADRE images. Consequently, the GM and WM are clearly delineated on PADRE images due to differences in the myelin concentration.

Table 1. The results of the observer study for each reading session

Classification	The first reading session	The second reading session
	(– PADRE)	(+ PADRE)
(a) Subcortical WM lesions	27 (56.3%)	12 (25%)
(b) Intracortical lesions	1 (2.0%)	1 (2.0%)
(c) Mixed GM/subcortical WM lesions	20 (41.7%)	35 (72.9%)

GM, gray matter; PADRE, phase difference enhanced imaging; WM, white matter.

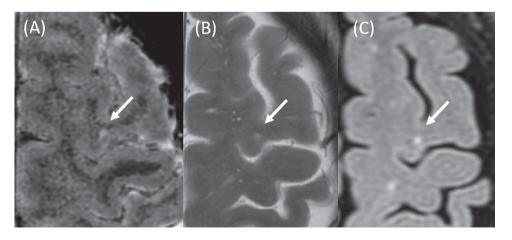


Fig. 3. A juxtacortical multiple sclerosis lesion visualized on a PADRE (**A**), a T₂-weighted imaging (**B**), and a 3D FLAIR image (**C**). The PADRE image shows a lesion involving both the gray matter and U-fiber. On the other images, involvement of the U-fiber only was recognized (arrows). 3D FLAIR, three-dimensional fluid-attenuated inversion recovery; PADRE, phase difference enhanced imaging.

The good results we obtained with the PADRE technique may be attributable to spatial resolution differences and to well-defined contrast differences between MS lesions and the surrounding gray and white matter. The spatial resolution for the PADRE sequence is 0.69 \times 0.40 \times 1.5 mm; for T₂WI, 2D FLAIR-, and 3D FLAIR imaging it is approximately $0.43 \times 0.43 \times 4.0$ mm, 0.98 \times 0.86 \times 4.0 mm, and 0.98 \times 0.98 \times 1.2 mm, respectively. The higher spatial resolution of the PADRE technique may also explain the excellent interobserver agreement we recorded for the depiction of juxtacortical lesions with GM involvement. On PADRE images almost all MS lesions exhibited high signal intensity due to myelin loss within the MS lesions. Therefore, the signal intensity of the juxtacortical lesions, the subcortical WM, and the GM was high-, low-, and slightly high, respectively, yielding well-defined contrast differences between the MS lesions and the subcortical WM and GM.

Involvement of the GM by the juxtacortical lesions is typically not seen on conventional MR images because the lesions are relatively small, manifest poor contrast against the surrounding normal GM, and can be obscured by partial volume effects from cerebral spinal fluid.²⁴ It has been reported that the SNR was improved on 3D FLAIR images and that the contrast-to-noise ratio was better than on 2D FLAIR images, 25 however, it remained difficult to distinguish between juxtacortical lesions with- and without GM involvement. With respect to infratentorial lesions with slightly prolonged T₂ relaxation times, the DIR technique has advantages over FLAIR imaging.^{26–28} As, besides demyelination, the pathologic features of MS lesions include perivascular cellular infiltration, DIR images are particularly sensitive to these water-rich conditions. PADRE may be less sensitive for depicting these conditions. Consequently, DIR and PADRE images yield different and complementary information for the assessment of MS lesions.

Our study has some limitations. As we have no histologic confirmation (reference standard) for the diagnosis of all MS lesions we evaluated, the juxtacortical lesions we studied may include artifacts. However, since no juxtacortical lesions were found on PADRE images of our healthy subjects, is unlikely that artifacts were misinterpreted as MS lesions. We also did not evaluate intracortical lesions depicted only on PADRE images because there is no consensus reference standard for establishing the diagnosis of MS lesions on such images. We did not specifically focus on correlating our lesion count with clinical and neuropsychologic parameters. Future studies must focus on correlating a well-defined load of GM- and subcortical WM lesions with specific degrees of disability and neuropsychologic function in a large MS patient cohort. Finally, in this study we did not directly compare 3D DIR- and PADRE images.

Conclusion

Our preliminary results suggest that PADRE and conventional MRI provide complementary information that may be useful for a better understanding of the pathologic processes underlying the manifestation of MS lesions. Our findings suggest that PADRE is useful for detecting GM involvement of the juxtacortical lesions of MS patients.

References

- 1. Brownell B, Hughes JT. The distribution of plaques in the cerebrum in multiple sclerosis. J Neurol Neurosurg Psychiatry 1962; 25:315–320.
- 2. Kidd D, Barkhof F, McConnell R, Algra PR, Allen IV, Revesz T. Cortical lesions in multiple sclerosis. Brain 1999; 122(Part 1):17–26.
- Peterson JW, Bö L, Mörk S, Chang A, Trapp BD. Transected neurites, apoptotic neurons, and reduced inflammation in cortical multiple sclerosis lesions. Ann Neurol 2001; 50:389–400.
- Geurts JJ, Pouwels PJ, Uitdehaag BM, Polman CH, Barkhof F, Castelijins JA. Intracortical lesions in multiple sclerosis: improved detection with 3D double inversion-recovery MR imaging. Radiology 2005; 236:254–260.
- Hammond KE, Metcalf M, Carvajal L, et al. Quantitative in vivo magnetic resonance imaging of multiple sclerosis at 7 Tesla with sensitivity to iron. Ann Neurol 2008; 64:707–713.
- Nelson F, Poonawalla A, Hou P, Wolinsky JS, Narayana PA. 3D MPRAGE improves classification of cortical lesions in multiple sclerosis. Mult Scler 2008; 14:1214–1219.
- Kangarlu A, Bourekas EC, Ray-Chaudhury A, Rammohan KW. Cerebral cortical lesions in multiple sclerosis detected by MR imaging at 8 Tesla. AJNR Am J Neuroradiol 2007; 28:262–266.
- 8. Mainero C, Benner T, Radding A, et al. In vivo imaging of cortical pathology in multiple sclerosis using ultra-high field MRI. Neurology 2009; 73:941–948.
- Gabr RE, Sun X, Pednekar AS, Narayana PA. Automated patient-specific optimization of three-dimensional double-inversion recovery magnetic resonance imaging. Magn Reson Med 2015 Mar 11. [Epub ahead of print]
- Kakeda S, Korogi Y, Yoneda T, et al. A novel tract imaging technique of the brainstem using phase difference enhanced imaging: normal anatomy and initial experience in multiple system atrophy. Eur Radiol 2011; 21:2202–2210.
- 11. Yang L, Wang S, Yao B, et al. Characterizing the contrast of white matter and grey matter in high-resolution phase difference enhanced imaging of human brain at 3.0 T. Eur Radiol 2015; 25:1068–1076.
- Ide S, Kakeda S, Korogi Y, et al. Delineation of optic radiation and stria of Gennari on high-resolution phase difference enhanced imaging. Acad Radiol 2012; 19:1283–1289.

- 13. Polman CH, Reingold SC, Banwell B, et al. Diagnostic criteria for multiple sclerosis: 2010 revisions to the McDonald criteria. Ann Neurol 2011; 69:292–302.
- 14. Liu T, Surapaneni K, Lou M, Cheng L, Spincemaille P, Wang Y. Cerebral microbleeds: burden assessment by using quantitative susceptibility mapping. Radiology 2012; 262:269–278.
- de Graaf WL, Zwanenburg JJ, Visser F, et al. Lesion detection at seven Tesla in multiple sclerosis using magnetization prepared 3D-FLAIR and 3D-DIR. Eur Radiol 2012; 22:221–231.
- Fukunaga M, Li TQ, van Gelderen P, et al. Layerspecific variation of iron content in cerebral cortex as a source of MRI contrast. Proc Natl Acad Sci U S A 2010; 107:3834–3839.
- 17. Marques JP, Maddage R, Mlynarik V, Gruetter R. On the origin of the MR image phase contrast: an in vivo MR microscopy study of the rat brain at 14.1 T. Neuroimage 2009; 46:345–352.
- Sedlacik J, Kutschbach C, Rauscher A, Deistung A, Reichenbach JR. Investigation of the influence of carbon dioxide concentrations on cerebral physiology by susceptibility-weighted magnetic resonance imaging (SWI). Neuroimage 2008; 43:36–43.
- Kakeda S, Korogi Y, Kamada K, et al. Signal intensity of the motor cortex on phase-weighted imaging at 3T. AJNR Am J Neuroradiol 2008; 29:1171–1175.
- Ogg RJ, Langston JW, Haacke EM, Steen RG, Taylor JS. The correlation between phase shifts in gradient-echo MR images and regional brain iron concentration. Magn Reson Imaging 1999; 17:1141–1148.

- 21. Shmueli K, Dodd SJ, Li TQ, Duyn JH. The contribution of chemical exchange to MRI frequency shifts in brain tissue. Magn Reson Med 2011; 65:35–43.
- 22. Denk C, Hernandez Torres E, MacKay A, Rauscher A. The influence of white matter fibre orientation on MR signal phase and decay. NMR Biomed 2011; 24:246–252.
- 23. Kakeda S, Korogi Y, Yoneda T, et al. Parkinson's disease: diagnostic potential of high-resolution phase difference enhanced MR imaging at 3 T. Eur Radiol 2013; 23:1102–1111.
- 24. Filippi M, Rocca MA, De Stefano N, et al. Magnetic resonance techniques in multiple sclerosis: the present and the future. Arch Neurol 2011; 68:1514–1520.
- 25. Tan IL, Pouwels PJ, van Schijndel RA, Adèr HJ, Manoliu RA, Barkhof F. Isotropic 3D fast FLAIR imaging of the brain in multiple sclerosis patients: initial experience. Eur Radiol 2002; 12:559–567.
- Bedell BJ, Narayana PA. Implementation and evaluation of a new pulse sequence for rapid acquisition of double inversion recovery images for simultaneous suppression of white matter and CSF. J Magn Reson Imaging 1998; 8:544–547.
- Turetschek K, Wunderbaldinger P, Bankier AA, et al. Double inversion recovery imaging of the brain: initial experience and comparison with fluid attenuated inversion recovery imaging. Magn Reson Imaging 1998; 16:127–135.
- 28. Redpath TW, Smith FW. Technical note: use of a double inversion recovery pulse sequence to image selectively grey or white brain matter. Br J Radiol 1994; 67:1258–1263.