

Predicting Treatment Response of Breast Cancer to Neoadjuvant Chemotherapy Using Ultrasound-Guided Diffuse Optical Tomography



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Abstract

PURPOSE: To prospectively investigate ultrasound-guided diffuse optical tomography (US-guided DOT) in predicting breast cancer response to neoadjuvant chemotherapy (NAC). **MATERIALS AND METHODS:** Eighty-eight breast cancer patients, with a total of 93 lesions, were included in our study. Pre- and post-last chemotherapy, size and total hemoglobin concentration (THC) of each lesion were measured by conventional US and US-guided DOT 1 day before biopsy (time point t0, THC THC0, SIZE S0) and 1 to 2 days before surgery (time point tL, THCL, SL). The relative changes in THC and SIZE of lesions after the first and last NAC cycles were considered as the variables Δ THC and Δ SIZE. Receiver operating characteristic curve was performed to calculate Δ THC and Δ SIZE cutoff values to evaluate pathologic response of 93 breast cancers to NAC, which were then prospectively used to predicate response of 61 breast cancers to NAC. **RESULTS:** The cutoff values of Δ THC and Δ SIZE for evaluation of breast cancers NAC treatment response were 23.9% and 42.6%. At Δ THC 23.9%, the predicted treatment response in 61 breast lesions for the time points t1 to t3 was calculated by area under the curve (AUC), which were AUC_1 0.534 ($P = .6668$), AUC_2 0.604 ($P = .1893$), and AUC_3 0.674 ($P = .0027$), respectively; for Δ SIZE 42.6%, at time points t1 to t3, AUC_1 0.505 ($P = .9121$), AUC_2 0.645 ($P = .0115$), and AUC_3 0.719 ($P = .0018$). **CONCLUSION:** US-guided DOT Δ THC 23.9% and US Δ SIZE 42.6% can be used for the response evaluation and earlier prediction of the pathological response after three rounds of chemotherapy.

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Introduction

In females, breast cancer is the most common cancer that causes major cancer mortality [1]. Neoadjuvant chemotherapy (NAC) has become the standard treatment for locally advanced breast cancer. NAC can downstage breast cancer, inhibit micrometastases, improve breast-conserving therapeutic strategy during surgery, and assess preoperative lesion sensitivity to medication [2]. Complete eradica-

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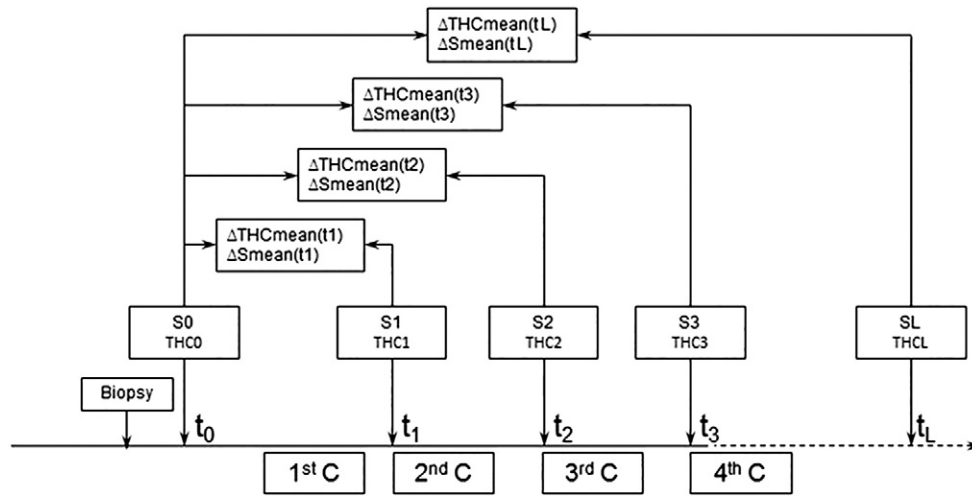


Figure 1. The flowchart of the study design with the THC and SIZE parameters derived from US and US-guided DOT images at four time points of the NAC rounds. C, cycle.

tion of invasive tumor cells in primary tumor bed following NAC renders longer disease-free survival [3,4]. Preoperative assessment of breast cancer NAC response is crucial since it helps physicians to decide the deadline of chemotherapy regimens. Conventional mammography, ultrasound [5], and magnetic resonance imaging (MRI) [6], which are based on tumor size changes, have been reported to assess response. Functional imaging techniques, such as dynamic contrast-enhanced (CE-MRI), MR spectroscopy, and positron emission tomography (PET) [7–9], have been used to monitor cancer response to NAC and demonstrated promising initial results. But mammography with radiation, PET, and CE-MRI, involving costly facilities and inserting drugs invasively, are not very desirable imaging modalities.

Diffuse optical tomography (DOT) is an optical imaging technique that uses near-infrared light to probe the absorption and scattering properties of biologic tissues and to acquire information of tumor physiology, biochemistry, angiogenesis, and hypoxia [10–13]. Because of the poor spatial resolution caused by intense light scattering in soft tissue, DOT alone has not been widely used in clinical studies. DOT combined with other imaging techniques such as x-ray mammography, MRI, or ultrasonography (US) for lesion locating has been explored for breast cancer diagnosis and monitoring NAC responses for locally advanced breast cancers [14–16]. Presurgical evaluation of NAC efficacy in solid tumors has been solely reliant on anatomical tumor burden and its alteration [17]. Given the long duration of NAC and poor patient compliance, so far, all the studies on US-guided DOT evaluation of breast cancer NAC efficacy had been limited to very small sample pools (10–34 patients) [10,18–26], without referring to ΔTHC best cutoff values to assess pathologic response. Therefore, our current study assembled a much larger cohort to investigate the best cutoff values to differentiate NAC responder group from nonresponder group and time points to get maximum diagnostic performance, as well as early predictive value of US-guided DOT ΔTHC in evaluating breast cancer pathologic response to NAC.

Materials and Methods

Study Design and Population

Patients were recruited from Fudan University Shanghai Cancer Center (FUSCC) from September 2014 to May 2016. The study protocol was approved by the institutional review board of the Human

Subjects Protection Office of FUSCC. Written informed consent was obtained from all patients. FUSCC is one of the largest cancer centers in China with approximately 4500 breast cancer patients receiving surgical resection treatment in the past 2 years.

All study subjects were pathologically diagnosed before receiving neoadjuvant treatment. Patients received four to eight rounds of NAC according to their molecular subtypes.

One hundred and seventy-eight lesions in 170 female patients were included in presurgical NAC, 85 lesions later were excluded: 79 did not have the last US-guided DOT evaluation at the end of presurgery NAC; 4 lesions were located too shallow, only 1 to 2 mm away from the skin; 2 lesions were located close to nipples, showing nipple artifacts. In all, 93 lesions with pre- and post-last chemotherapy (mean size, 41 mm; range, 14 to 93 mm) in 88 patients (mean age, 50 years; range, 32 to 82 years) were included in the final data analysis. Because, according to RECIST guidelines [27], all baseline evaluations should be performed as close as possible to the beginning of treatment, US-guided DOT evaluation was done within a week of starting NAC.

Pre- (time point t_0) and post-last (time point t_L) chemotherapy, the size and total hemoglobin concentration (THC) of each lesion were measured by conventional US and US-guided DOT 1 day before biopsy (time point t_0 , THC0, S0) and 1 to 2 days before surgery (time point t_L , THCL, SL). The relative changes in THC and SIZE of lesions after the first and last NAC rounds were considered as the variables ΔTHC and ΔSIZE . The area under the ROC curve (AUC) was used to calculate the cutoff values of ΔTHC and ΔSIZE in predicting pathologic responses and was prospectively tested in 61 breast lesions which were measured using both US and US-guided DOT (time point t_0 - t_3 , t_L , THC0-THC3, THCL, S0-S3, SL). THC and SIZE of 61 breast lesions were measured by conventional US and US-guided DOT 1 day before biopsy (time point t_0 , THC0, S0), 1 day before next NAC cycle (time point t_1 - t_3 , THC1-THC3, S1-S3), and 1 day before surgery (time point t_L , THCL,SL) (Figure 1).The NAC clinical efficacy was determined with surgical pathologic examination results as the verification standard.

Ultrasonography and US-Guided DOT Acquisition and Evaluation Criterion of 93 Target Lesions Response

The US examinations were performed using the Aixplorer US system (SuperSonic Imagine, Aix-en-Provence, France) with a SL15-4 multifrequency linear probe operating at 4 to 15 MHz. The breast

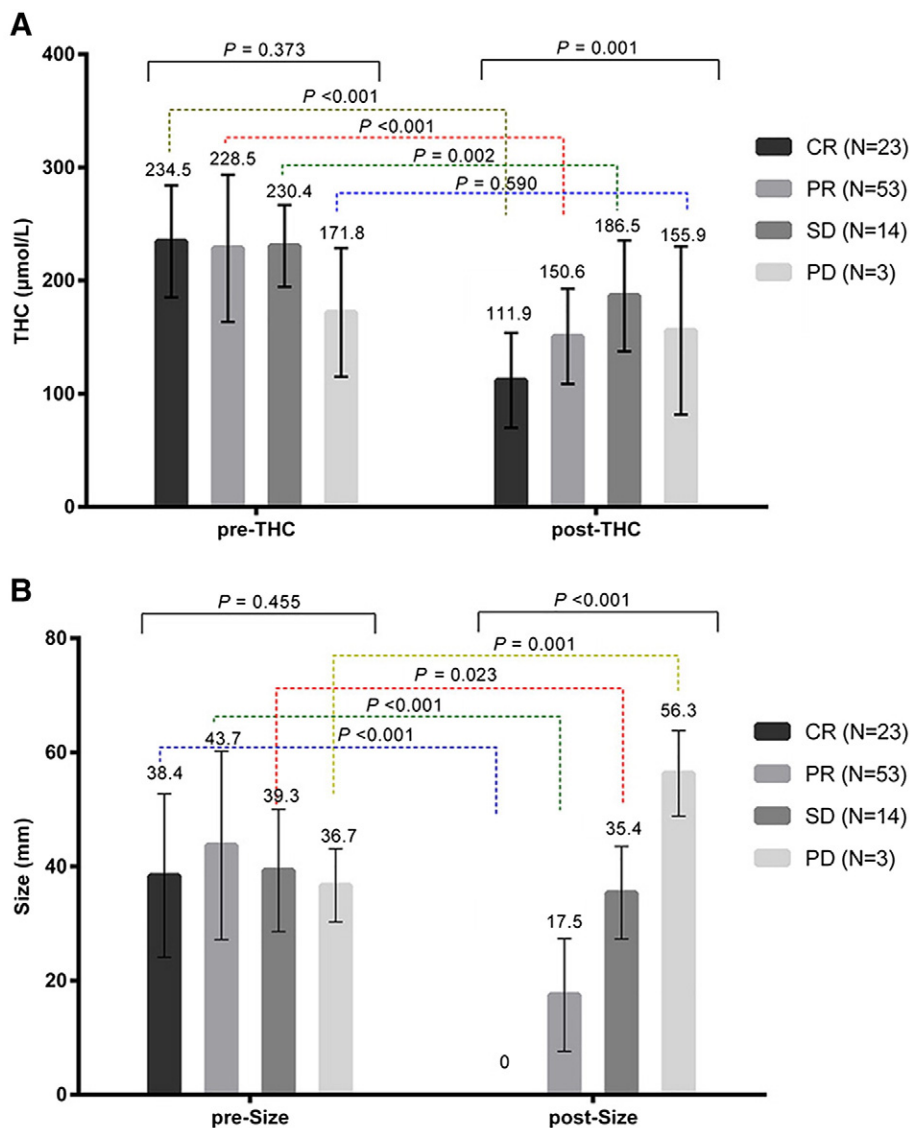


Figure 2. Pre- and post-NAC parameters changes of CR, PR, SD, and PD groups. (A) Pre- and post-NAC THC of CR, PR, SD, and PD groups. (B) Pre- and post-NAC tumor size of CR, PR, SD, and PD groups.

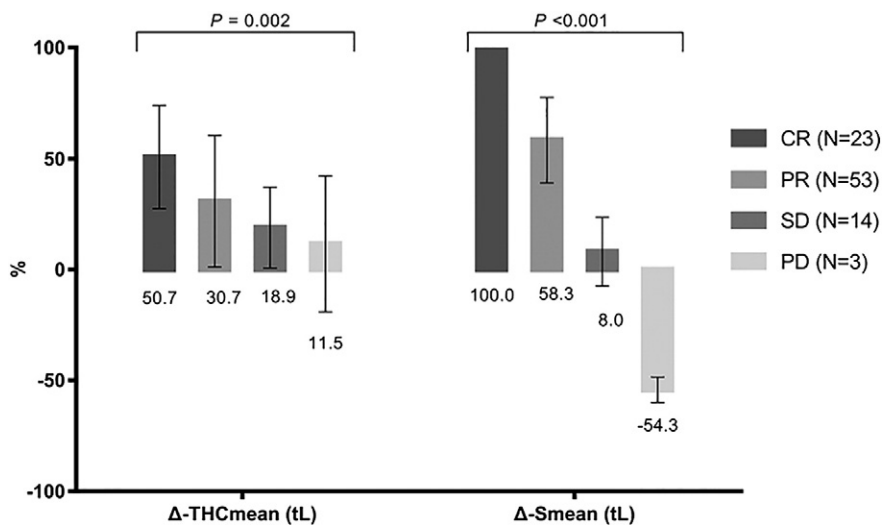


Figure 3. Pre- and post-NAC ΔSmean (tL) and ΔTHCmean (tL) of CR, PR, SD, and PD groups.

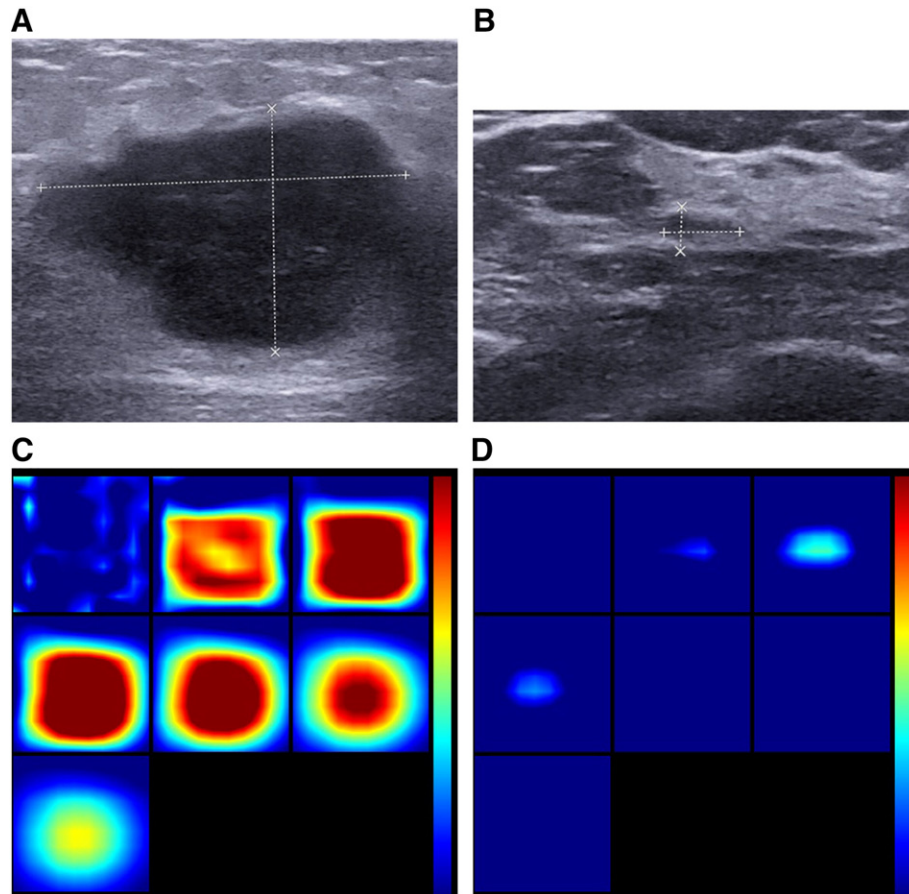


Figure 4. One responder case: invasive ductal carcinoma in a 48-year-old woman. (A, B) US images show a pre- and posttreatment lesion with hypoechoic, irregular shape and indistinct margins, with US measuring pre-size of 3.6 cm and post-size 0.7 cm in diameter. It was a pathologically complete response with Miller-Payne grade 5; therefore, $\Delta S_{\text{mean}}(\text{tL})$ was 100%. (C, D) Pre- and posttreatment reconstructed optical absorption maps show that the lesion was resolved in slices from 1 (top left, left to right) to 7 (bottom left, left to right) and from 2 to 4 (top row, left to right). Pre- and posttreatment THCs were $279.0 \mu\text{mol/L}$ and $128.0 \mu\text{mol/L}$, respectively. $\Delta \text{THC}_{\text{mean}}(\text{tL})$ of the lesion was 54.1%. The first section (slice 1, top left) is a 6×6 -cm spatial x - y image (coronal plane of the body) obtained at a depth of 0.5 cm, as measured from the skin surface. The last section (slice 7, bottom left) is a 6×6 -cm spatial x - y image (coronal plane of the body) obtained at a depth of 3.5 cm towards the chest wall. Spacing between sections is 0.5 cm in the direction of propagation. The vertical color scale from blue to red is the THC in micromoles per liter from low to high.

US examinations were performed by the same radiologists (W.X.Z. and A.Y.M. with more than 9 years of experience in breast US) according to the American Institute of Ultrasound in Medicine practice guidelines for performing breast US [28], with the patient in the supine position. The US respectively measured pre- and post-NAC lesion sizes (t_1 and t_L , S_0 and S_L) (maximal diameters) of 93 lesions. The relative change in size after the first and last NAC cycles was considered as the variable $\Delta \text{Size}(\text{tL})$. $\Delta \text{Size}(\text{tL}) = (S_0 - S_L)/S_0 \times 100\%$. Based on the Guidelines to Evaluate the Response to Treatment in Solid Tumors [27], the responses to NAC were classified into complete response (CR), partial response (PR), static disease (SD), progressive disease (PD) groups. Patients with CR and PR were assigned as responders, and patients with SD and PD as nonresponders on conventional US [7].

US-guided DOT, using Optimus-01HWS breast diagnostic system (XinAo-MDT Technology, Hebei, China), which is a dual imaging modality combining conventional ultrasound (Terason T3000 ultrasound, Teratech, USA) and near-infrared (NIR) optical tomography, was used to measure functional tissue properties with optical spectroscopic analysis. The main functional parameter was the

total hemoglobin concentration (THC) calculated from absorption coefficients measured by using two optical wavelengths (785 nm and 830 nm). The technical details of this imaging system, including system configurations, imaging acquisition methods, and the data processing algorithms, have been previously described by us [15]. Tumors were located by conventional US, and optical imaging was then performed using a handheld probe. After freezing the frame at the maximal section, raw optic data acquisition was performed five times for each breast lesion and the corresponding normal area in the contralateral breast. The final data were obtained by automatically or manually defining the region of interest (ROI), imaging and data computing, a process that takes about 3 to 5 minutes. The data were input into Excel files, and mean values of THC (THC_{mean}) were established.

Therefore, each optical parameter value reported is a mean of approximately 5 values of the ROI, and the SD is a reflection of the physiologic variation for that patient. ROI was drawn to include the maximal dimension of the lesion based on the US images, which encompassed the whole area of the identified lesion and a small

Table 1. Diagnostic Performance of Δ THCmean 23.9% and Δ Smean 42.6% in Assessing Treatment Response of 93 Breast Cancers to NAC

Variables	Sen (%)	Spe (%)	PPV (%)	NPV (%)	Accuracy (%)	AUC (95% CI)	P Value
Δ THC 23.9%	73.7	76.5	93.3	76.5	74.2	0.751 (0.650-0.835)	<.0001
Δ SIZE 42.6%	80.3	52.9	88.4	37.5	77.4	0.690 (0.586-0.782)	.0125

Sen, sensitivity; Spe, specificity.

portion of the surrounding normal tissues. The optical imaging-measured normal site in the symmetrical region of the contralateral breast was used as references in the reconstruction. The only one optical characteristic parameter THC used in our study was related to tissue microstructure and biochemical composition such as oxygenated hemoglobin (HbO₂), deoxygenated hemoglobin (Hb), and total hemoglobin concentration ([THC] = [Hb] + [HbO₂]), which were obtained by calculating the difference between the lesion and the symmetric normal site. The relative change in THC after the first and last NAC cycles was considered as the variable Δ THC. Δ THCmean (tL) = (THCmeant0 - THCmeantL)/THCmeant0 \times 100%. All examinations were performed by the same radiologist who also participated in the acquisition of conventional US images. According to RECIST1.1 guidelines [17], CR or PR is needed to deem either one the best overall response. Overall response rate (ORR) = (CR + PR)/(CR + PR + SD + PD) \times 100%. Receiver operating curve (ROC) analysis was performed to analyze the diagnostic performance of Δ THC(tL) and Δ SIZE(tL) to predict the pathological response. The best cutoff values of Δ THC and Δ SIZE were then used to calculate the sensitivity, specificity, positive predictive value (PPV), negative predictive value (NPV), and accuracy for predicting pathological responsiveness. The NAC clinical efficacy was determined with surgical pathologic examination results as the verification standard.

Ultrasonography and US-Guided DOT Acquisition and Evaluation Criterion of 61 Target Lesions Response

We applied the predictive cutoff values of Δ THC and Δ SIZE to 61 NAC breast lesions. In order to assess the early predictive values of Δ THC and Δ SIZE, we analyzed breast lesions which went through top three rounds of chemotherapy. THC and SIZE of 61 breast lesions were measured by conventional US and US-guided DOT 1 day before biopsy (time point t0, THC0, S0), 1 day before next NAC cycle (time point t1-t3, THC1-THC3, S1-S3), and 1 day before surgery (time point tL, THCL, SL) (Figure 1). The relative changes in SIZE and THC of the primary tumor from baseline were calculated at four different time points (S1, THC1 at t1, S2, THC2 at t2, S3, THC3 at t3, SL, THCL at tL) using the following equations:

$$\begin{aligned} \Delta\text{THCmean}(t1) &= (\text{THC0mean} - \text{THC1mean}) / \text{THC0mean} \times 100\% \\ \Delta\text{THCmean}(t2) &= (\text{THC0mean} - \text{THC2mean}) / \text{THC0mean} \times 100\% \\ \Delta\text{THCmean}(t3) &= (\text{THC0mean} - \text{THC3mean}) / \text{THC0mean} \times 100\% \\ \Delta\text{THCmean}(tL) &= (\text{THC0mean} - \text{THCLmean}) / \text{THC0mean} \times 100\% \end{aligned}$$

$$\begin{aligned} \Delta\text{Smean}(t1) &= (\text{S0mean} - \text{S1mean}) / \text{S0mean} \times 100\% \\ \Delta\text{Smean}(t2) &= (\text{S0mean} - \text{S2mean}) / \text{S0mean} \times 100\% \\ \Delta\text{Smean}(t3) &= (\text{S0mean} - \text{S3mean}) / \text{S0mean} \times 100\% \\ \Delta\text{Smean}(tL) &= (\text{S0mean} - \text{SLmean}) / \text{S0mean} \times 100\% \end{aligned}$$

Figure 1 illustrates the flowchart of the study design with the THC and SIZE parameters derived from US and US-guided DOT images at four time points of the NAC rounds.

Pathological Evaluation of NAC Efficacy

The final pathologic response was assessed using the Miller-Payne grading system [29], in which pathologic response is divided into five grades based on comparison of tumor cellularity between pre-NAC core biopsy and postoperative surgical specimen. For this study, two pathologists performed final diagnosis, and discrepancies were resolved by consensus. Responders were categorized as having a Miller-Payne grades 3 or 4 or 5, while nonresponders had grades 1 or 2.

Statistical Analysis

Statistical analyses were performed with MedCalc software (version 15.2.2; Med-Calc, Mariakerke, Belgium). The one-way ANOVA and paired-sample *t* test were used to estimate group differences for SIZE and THC parameters of different time points, with *P* < .05 considered a statistically significant difference. With postsurgical Miller-Payne grading as the gold standard, ROC curves were used to analyze the best cutoff values of Δ THC and Δ Size to differentiate NAC responder group from nonresponder and to predict the clinical efficacy of breast cancer NAC.

Results

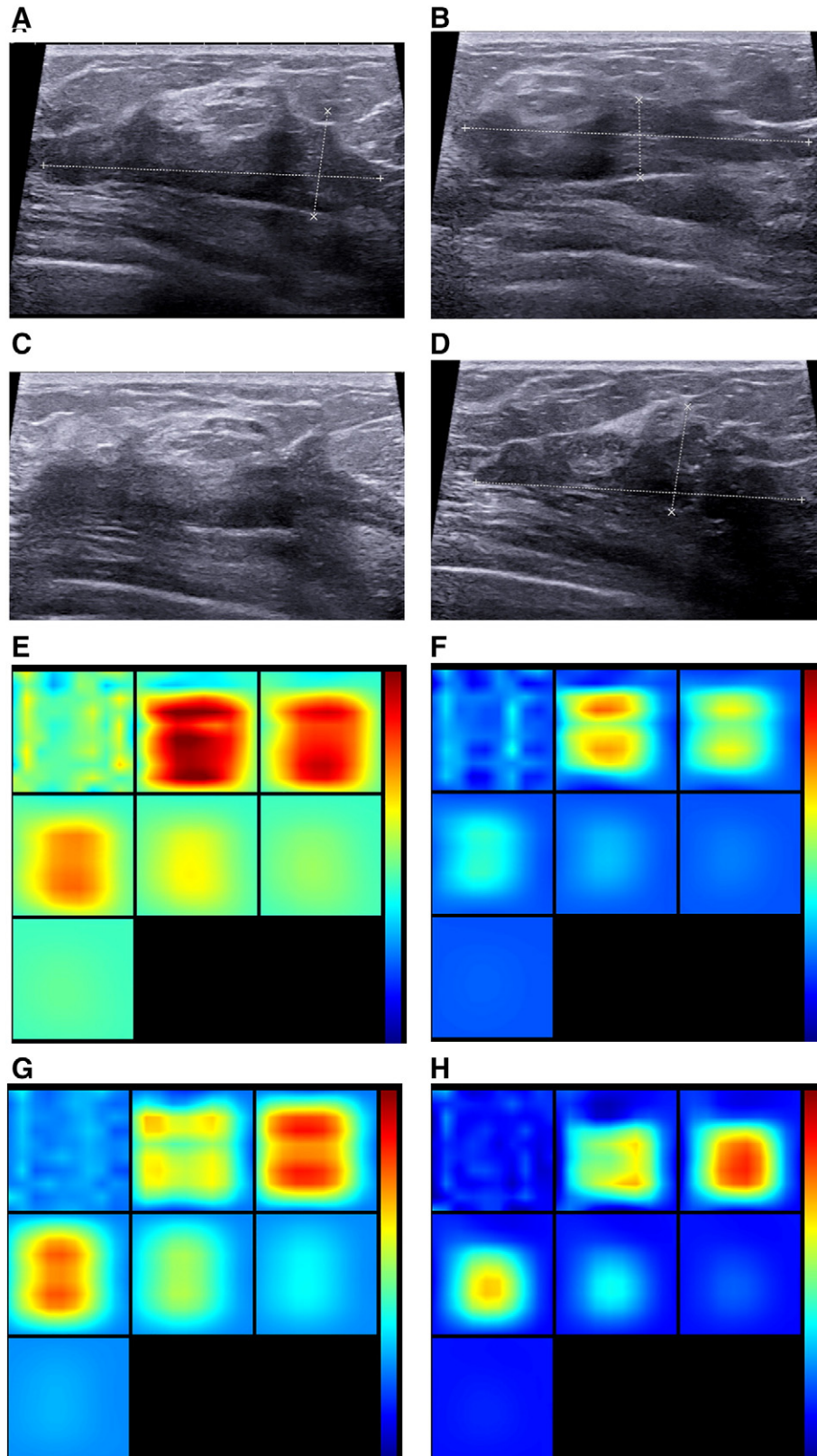
Out of 93 lesions, 23 had CR, 53 PR, 14 SD, and 3 PD. Figure 2 indicated US-guided DOT monitoring pre-NAC and post-NAC parameters of different groups. As shown in Figure 2A, although before NAC THC had no difference among the groups (*F* = 1.053, *P* = .373), after NAC treatment, THC varied significantly (*F* = 5.80, *P* = .001), with the lowest THC reading in CR group, higher in PD and SD groups. Within each group, except for group PD (*P* = .590), THC changed significantly: CR (*P* < .001), PR (*P* < .001), SD (*P* = .002). As demonstrated in Figure 2B, pretreatment tumor sizes were similar among the groups (*F* = 2.617, *P* = .455); post-NAC tumor sizes were significantly different (*F* = 69.77, *P* < .001); tumors size of CR was 0 and gradually increased in PR, SD, and PD groups. Not surprisingly, pre- and post-NAC tumor sizes were significantly different in all groups: CR (*P* < .001), PR (*P* < .001), SD (*P* = .023), PD (*P* = .001). Figure 3 illustrated that Δ Smean (tL) (*F* = 150.9, *P* < .001) and Δ THCmean (tL) (*F* = 5.43, *P* = .002) differed significantly among the groups: Δ Smean (tL) was highest in group CR (100%) (Figure 4): PR 58.3 \pm 19.2%, SD 8.0 \pm 015.6%, PD -54.3 \pm 5.7%; Δ THCmean (tL) was also highest in CR group (Figure 4): 50.7 \pm 23.2%, PR 30.7 \pm 29.6%, SD 18.9 \pm 18.3%, PD -11.5 \pm 30.7%.

Table 2. Diagnostic Performance of Δ THC 23.9% and Δ SIZE 42.6% in Predicting 61 Breast Cancers Lesions' Response to NAC at Different Cycles

Parameters at Different Time Points	Sen	Spe	PPV	NPV	Accuracy	AUC (95% CI)	P Value
Δ THCmean (t1)	0.34	0.727	0.850	0.195	0.410	0.534(0.401-0.663)	.6668
Δ THCmean (t2)	0.48	0.727	0.889	0.235	0.525	0.604(0.470-0.727)	.1893
Δ THCmean (t3)	0.62	0.727	0.912	0.296	0.639	0.674(0.542-0.788)	.0270
Δ THCmean (tL)	0.70	0.727	0.921	0.348	0.705	0.714(0.584-0.822)	.0059
Δ SIZEmean (t1)	0.08	0.909	0.800	0.179	0.230	0.505(0.374-0.636)	.9121
Δ SIZEmean (t2)	0.38	0.909	0.950	0.244	0.475	0.645(0.512-0.763)	.0115
Δ SIZEmean (t3)	0.62	0.818	0.939	0.321	0.656	0.719(0.589-0.827)	.0018
Δ SIZEmean (tL)	0.86	0.455	0.878	0.417	0.787	0.657(0.525-0.774)	.0567

Of the 93 breast cancer lesions, according to the RECIST 1.1 criteria, 76 breast cancers were responders, and 17 breast cancers were non-responders, ORR 为81.7%. ROC curve analysis was used to identify maximum value sum of sensitivity and specificity, while $\Delta\text{THC}_{\text{mean}}$ 23.9% and $\Delta\text{S}_{\text{mean}}$ 42.6% were used as the threshold value to differentiate NAC responder group from nonresponder

group. The sensitivity, specificity, PPV, NPV, and accuracy of US-guided DOT were 73.7%, 76.5%, 93.3%, 76.5%, and 74.2%, respectively. The AUC was 0.751 (95% CI: 0.650-0.835). The sensitivity, specificity, PPV, NPV, and accuracy of conventional US were 80.3%, 52.9%, 88.4%, 37.5%, and 77.4%, respectively. The AUC was 0.690 (0.586-0.782) (Table 1). We then applied the cutoff



values of $\Delta\text{THC}_{\text{mean}}$ 23.9% and $\Delta\text{S}_{\text{mean}}$ 42.6% to the breast lesions that went through various NAC rounds to predict pathologic responses (Table 2) (Figures 5-6). Our results showed that, at $\Delta\text{S}_{\text{mean}}$ 42.6%, the AUCs of NAC responder group after chemotherapy rounds were: $\text{AUC}_1 = 0.505$ (95% CI: 0.374-0.636), $P = .9121$, $\text{AUC}_2 = 0.645$ (95% CI: 0.512-0.763), $P = .0115$, $\text{AUC}_3 = 0.719$ (95% CI: 0.589-0.827), $P = .0018$, and $\text{AUC}_L = 0.657$ (95% CI: 0.525-0.774), $P = .0567$. The sensitivity and accuracy were climbing higher from t1 to t3. As early as after the second round of NAC, $\Delta\text{S}_{\text{mean}}$ 42.6% was able to differentiate responder group from nonresponder group ($P = .0115$), with AUC reaching the highest value at t3. For ΔTHC 23.9%, the AUCs were $\text{AUC}_1 = 0.534$ (95% CI: 0.401-0.663), $P = .6668$, $\text{AUC}_2 = 0.604$ (95% CI: 0.470-0.727), $P = .1893$, $\text{AUC}_3 = 0.674$ (95% CI: 0.542-0.788), $P = .027$, and $\text{AUC}_L = 0.714$ (95% CI: 0.584-0.822), $P = .0059$. The sensitivity and accuracy showed a similar trend as the $\Delta\text{S}_{\text{mean}}$ 42.6%. As early as after the third round of NAC, ΔTHC 23.9% could differentiate responder group from nonresponder group ($P = .027$).

Discussion

US-guided DOT, as functional imaging technique without use of exogenous contrast agents, is relatively inexpensive and short-timed compared to with MRI and PET [30]. This technique also provides functional information as a potential complement to traditional structural imaging techniques of MRI and conventional US. Previous studies with small sample pools have demonstrated the feasibility of using DOT for monitoring treatment in patients with locally advanced breast cancer, with diffuse optical parameters of THC to indicate angiogenesis and oxygen saturation of tumor tissue, i.e., cancer cell growth [18,20].

In our current study with more lesion samples, we found no difference of THC reading among the groups before the NAC, indicating that pretreatment THC measurements may not predict therapy efficacy. This finding is apparently different from what Zhu et al. [25] discovered in their cohort of 32 lesions. The possible reason for this discrepancy could be due to the pre-DOT needle biopsy procedures in that study, as a bruise or hematoma caused by prior biopsy may have some effect on THC measurements.

For posttreatment data, THC measurements and ΔTHC all showed significant variations among groups, with the lowest THC reading and highest $\Delta\text{THC}\%$ found in the CR group and with the SD group having the opposite; these results of ours demonstrate the potential use of ΔTHC in evaluating breast cancer efficacy. Pakalniskis et al. [31] uncovered that, for women with CR, pretreatment MVD of CD105-expressing blood vessels correlated with high THC. Comparing prechemo with postsurgery tumor vascularity, previous studies [32] concluded that decreased tumor

vascularity indicates good response and increased or unchanged vascularity indicates no response at all. Hence, in agreement with previous studies, we reiterate that THC correlates with blood vessels inside tumor lesion: the more THC decreases, the less tumor blood vessel grows, and the better the therapy efficacy achieves [33]. On the other hand, as elevated levels of THC indicating efficient blood supply to tumor, this allows for better drug and nutrients delivery to cancer cells [34]. Our data revealed a significantly higher THC in almost all pretreatment groups comparing to the posttreatment ones, suggesting NAC inhibited tumor angiogenesis.

Tumor sizes and ΔSize differed significantly among different groups, which were consistent with other research reports, confirming the value of US for evaluation of NAC efficacy in treating breast cancer [5,6]. Along with shrinking tumor size and lowered THC, ΔSize and ΔTHC also bore a signature among the groups, with highest value in CR followed by PR and SD groups.

In CR and PR groups (total 93 breast cancer lesions), facilitated by pathology reports, we further used ROC curves to analyze the efficacy of $\Delta\text{S}_{\text{mean}}$ and $\Delta\text{THC}_{\text{mean}}$ in predicting pathologic response to NAC. Our results indicated that the $\Delta\text{S}_{\text{mean}}$ 42.6% (AUC 0.751) and ΔTHC 23.9% (AUC 0.690) had moderate value in determining NAC response. This finding of ours suggests that the NAC response evaluation power of US-guided DOT is similar to DCE-MRI and PET/CT, as An et al. [7] reported that the AUCs for DCE-MRI using MR-CAD analysis and PET/CT were 0.77 and 0.76. Our results from 61 lesions also pointed out that for early prediction of NAC response (after only two rounds), ΔTHC 23.9% achieved higher sensitivity and accuracy than $\Delta\text{S}_{\text{mean}}$ 42.6%. This finding is consistent with the previous report by Cerussi et al. [21] probably due to the fact that, in the lesions, changes of functional metabolism are always earlier than those of morphology. Overall, we found that for the first three NAC rounds, in predicting pathologic response, ΔTHC 23.9% and $\Delta\text{S}_{\text{mean}}$ 42.6% had low sensitivity and high specificity. But the sensitivity and accuracy of these tests increased with more rounds of treatment: as early as the end of the second NAC round, $\Delta\text{S}_{\text{mean}}$ 42.6% could differentiate responder and nonresponder groups; for ΔTHC 23.9%, it was the third round. Interestingly, the sensitivity of prediction power of $\Delta\text{S}_{\text{mean}}$ 42.6% at the end of the second round was only 38%, lower than 62% of the third round. This finding, combined with the AUC result (AUC_2 0.645 vs AUC_3 0.719), made us conclude that the best time point for $\Delta\text{S}_{\text{mean}}$ 42.6% to predict NAC efficacy is after the third round of treatment. Another point to add is that ΔTHC 23.9% and $\Delta\text{S}_{\text{mean}}$ 42.6% all achieved highest NPV for prediction at the third round. In conclusion, $\Delta\text{S}_{\text{mean}}$ 42.6% and ΔTHC 23.9% can effectively predict NAC efficacy early in treatments, around the end of the third round. Rousseau et al. [35,36] described that pathologic response to breast cancer NAC could be predicted accurately by FDG PET after two

Figure 5. One nonresponder case: invasive ductal carcinoma in a 43-year-old woman. (A, B, C, D) US images show at different time points lesion with hypoechoic, irregular shape and indistinct margins, with US measuring S0 5.0 cm (A), S1 5.1 cm (B), S2 4.8 cm (C), and S3 4.8 cm (D) in diameter. The final pathological size was 4.0 cm with Miller-Payne grade 2; therefore, $\Delta\text{S}_{\text{mean}}$ (t1) was -2% , $\Delta\text{S}_{\text{mean}}$ (t2) 4% , and $\Delta\text{S}_{\text{mean}}$ (t3) 4% . (E, F, G, H) Reconstructed optical absorption maps showed that the lesion was resolved in slices from 1 (top left, left to right) to 7 (bottom left, left to right). $\text{THC}_{0\text{mean}}$ was $206.0 \mu\text{mol/L}$ (E), $\text{THC}_{1\text{mean}}$ $173.3 \mu\text{mol/L}$ (F), $\text{THC}_{2\text{mean}}$ $185.0 \mu\text{mol/L}$ (G), and $\text{THC}_{3\text{mean}}$ $189.3 \mu\text{mol/L}$ (H). Therefore, $\Delta\text{THC}_{\text{mean}}$ (t1) was 15.9% , $\Delta\text{THC}_{\text{mean}}$ (t2) 10.2% , and $\Delta\text{THC}_{\text{mean}}$ (t3) 8.1% . The first section (slice 1, top left) is a 6×6 -cm spatial x - y image (coronal plane of the body) obtained at a depth of 0.5 cm, as measured from the skin surface. The last section (slice 7, bottom left) is a 6×6 -cm spatial x - y image (coronal plane of the body) obtained at a depth of 3.5 cm towards the chest wall. Spacing between sections is 0.5 cm in the direction of propagation. The vertical color scale from blue to red is the THC in micromoles per liter from low to high.

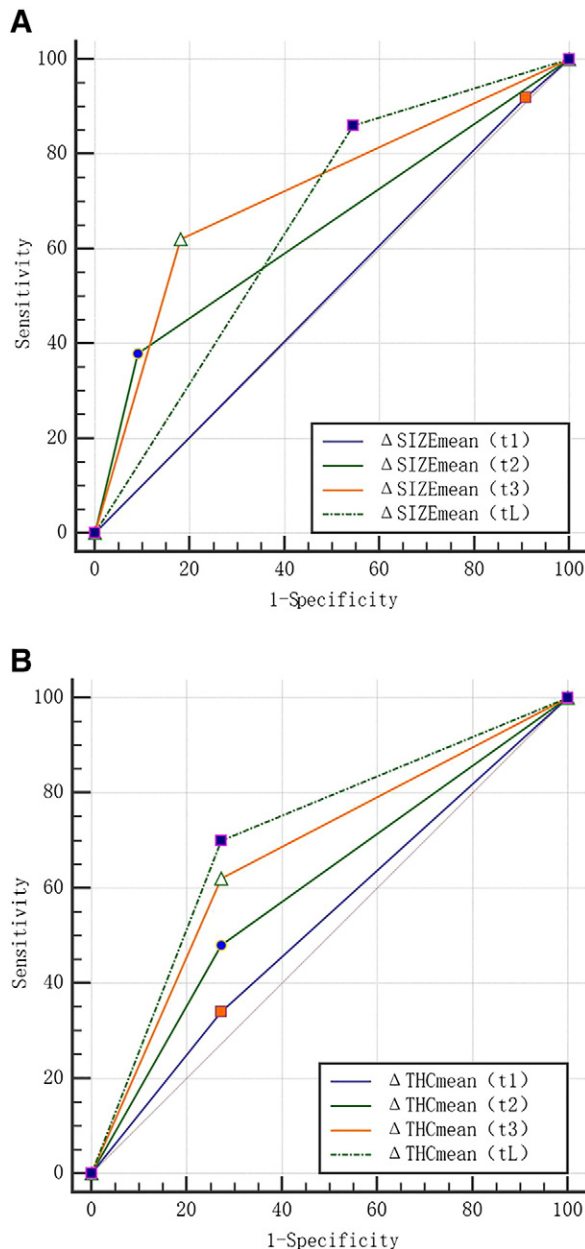


Figure 6. (A) Comparison of Δ SIZE ROC curves from the lesions treated with different chemotherapy cycles. (B) Comparison of Δ THC ROC curves from the lesions treated with different chemotherapy cycles.

rounds of chemotherapy. Falou et al. [37] reported that Deoxygenated hemoglobin concentration and water percentage were found to be the best predictors of response at 1 week of treatment using Diffuse Optical Spectroscopy. These different optimal time points for response prediction might be a result of different imaging technologies and parameters.

Of course our study has limitations. First, the shallow lesions cannot be fully covered by the optical field due to the inherent distance between light emitter and detector in the US probe. In addition, areolar and periareolar skin has different optic absorbance, which can cause data inaccuracy. Therefore, we had to exclude all the shallow lesions (within 3 mm to the skin) as well as subareolar lesions. Secondly, we used contralateral healthy breast as normal control; lesions from one-breast patients who lost the other breast due to cancer were also excluded.

Conclusion

In summary, US-guided DOT Δ THC 23.9% and US Δ SIZE 42.6% can be used for the response evaluation and earlier prediction of the pathological response after three rounds of chemotherapy.

Conflicts of Interest

None.

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