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Mechanosensing in the immune response

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Abstract

Cells have a remarkable ability to sense and respond to the mechanical properties of their environment. Mechanosensing is essential for many phenomena from cell movements and tissue rearrangements to cell differentiation and the immune response. Cells of the immune system get activated when membrane receptors bind to cognate antigen on the surface of antigen presenting cells. Both T and B lymphocyte signaling has been shown to be responsive to physical forces and mechanical cues. Cytoskeletal forces exerted by cells likely mediate this mechanical modulation. Here we discuss recent advances in the field of immune cell mechanobiology at the molecular and cellular scale.

Keywords

immune cells; mechanosensing; cytoskeleton; forces; T cell receptor; actin

1. Introduction

The mechanical environment of cells, such as the extracellular matrix (ECM) or other cells, plays a critical role in regulating many aspects of cell function [1, 2]. Examples of mechanical stimuli include forces due to muscle contraction, shear stresses induced by flow in blood vessels or strains induced by collective movements of tissues. Similarly, cells also encounter environments with varying physical properties, such as tissue or stiffness of the ECM, topography and fluidity. Studies have revealed that in addition to soluble chemical cues, the physical environment plays a key role in controlling cell proliferation, cell fate determination, cell migration and global organization of tissues by regulating genetic and biochemical signaling pathways [1]. Mechanical regulation of cell function appears to result from a conserved set of physical mechanisms [3]. Forces arising from the actin cytoskeleton and myosin motors generate active tension that is applied to adhesions (both cell-cell and cell-matrix), initiating biochemical signaling [4]. Given the importance of dynamic force transmission for cell and tissue physiology, the underlying mechanisms that translate forces into an appropriate cellular response need to be understood. The regulation of receptor-

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mediated cell signaling by cytoskeletal and external forces and the mechanical properties of the environment is important in many aspects of physiology including the immune system.

The adaptive immune system forms a strong line of defense against infections, through its ability to recognize foreign molecules (antigens), develop an appropriate response, and rapidly recall this action on subsequent re-exposure [5]. Naïve lymphocytes (T and B cells) in search for their cognate antigens encounter a variety of mechanical stimuli as they circulate through blood, lymphoid tissues, and sites of inflammation. T and B cell activation requires physical interaction with professional antigen presenting cells (APC) – dendritic cells and follicular dendritic cells respectively [6–8]. APCs display protein fragments derived from infecting pathogens on their surface. A membrane protein complex, called the T or B cell receptor (TCR/BCR), recognizes these fragments and assembles into microclusters [9–11]. Signaling proteins and adaptors accumulate at developing microclusters [11] which trigger signal transduction pathways and ultimately lead to the initiation of transcription and cell fate determination (cell activation) [12] (Fig. 1a).

Several lines of evidence have converged upon the view that physical forces can trigger signaling during lymphocyte activation [13–15]. Activation also critically depends upon rearrangements of the actin cytoskeleton [16, 17]. Lymphocyte signaling is also sensitive to the mechanical properties of antigen-bearing surfaces including stiffness [18–20], mobility and topography. In this review, we explore what is currently known about mechanosensing in the immune response at different length scales ranging from the molecular scale of how mechanical forces play a role in activating immune and adhesion receptors to the cellular scale of how a cell responds functionally to mechanical forces. We then briefly review cytoskeletal dynamics in immune cells and the different ways in which cellular forces have been measured. We further discuss the potential role of cytoskeletal forces in establishing and modulating mechanotransduction. In this review, we largely focus on mechanical responses in T cells with some insights into B cells.

2. Mechanosensing at the molecular scale

2.1 Immune (antigen) receptors

The T Cell Receptor (TCR) is a multi-subunit complex expressed on the T cell membrane, which binds antigenic peptides embedded within major histocompatibility complex molecules (pMHC) on APCs during antigen recognition [21]. This heteromeric complex consists of the ligand binding TCR (α and β subunits) non-covalently associated with CD3 $\gamma\epsilon$, CD3 $\delta\epsilon$, and CD3 $\zeta\zeta$ polypeptide chains. Structural and biophysical analyses have revealed extensive conformational changes within the TCR complex upon binding to antigenic peptides, implying the conversion of biochemical interactions into mechanical information [22].

Any proposed mechanism for antigen recognition by TCR must explain certain distinct features of TCR/pMHC interactions. A single pMHC complex can lead to TCR triggering and T cell activation (sensitivity) [23]. Further, T cells can discriminate between small numbers of agonist pMHC molecules from a large number of very similar, non-agonist pMHC molecules (specificity). How the TCR achieves this level of sensitivity and

specificity is not completely understood. The TCR/pMHC bond is weak [24], suggesting that the free energy changes underlying conformational transitions likely require applied forces. Recent work has hinted that forces exerted on the TCR-pMHC bond may be critical in optimizing TCR triggering, suggesting that the TCR is a mechanosensor as it can transduce mechanical stimuli into biochemical signals through structural and conformational changes [25].

In one of the first such studies, Kim et al. [14] used optical tweezers to apply forces on beads coated with non-activating antibody or pMHC and quantified Ca^{2+} levels as a measure of T cell activation. They found that tangential but not normally applied forces to pMHC-coated beads induced Ca^{2+} signaling, indicating that TCR is mechanically triggered. A force threshold of 50 pN was required for activation. Li et al. used fibroblasts as artificial APCs to show that application of force to T cells by magnetic beads resulted in robust Ca^{2+} influx for ligands specific to TCR but not for integrins or non-TCR receptors [26].

In a tour-de-force study, Zhu and colleagues used a micropipette-RBC based force probe apparatus, capable of detecting <2 pN forces to examine how applied forces regulate TCR-pMHC interaction [27, 28]. If the affinity of protein-protein interaction increases with applied force up to a threshold, the interaction is called a catch-bond. Liu et al. showed that the lifetime of the bond between TCR and its cognate ligand was prolonged with application of 10 pN force, indicative of catch-bond behavior [28]. For non-specific TCR-pMHC interactions however, the affinity peaked at zero force, indicative of slip-bond behavior (weakening under applied force). At a cellular scale, high Ca^{2+} levels were induced with the application of force. These studies emphasize that load-induced structural transitions tune TCR-pMHC bond lifetime with high specificity. Using optical tweezers and DNA tethers, Das et al. have shown that the domains in the β -subunit of the TCR undergo force-dependent conformational transition [29]. This allosteric transition prolonged the TCR-pMHC bond lifetime, providing a possible molecular basis for the observed catch-bond behavior.

While the role of forces on the specificity and sensitivity of antigen recognition by TCR is coming to light, how information about TCR-antigen binding is transmitted into the cell is unclear. As TCRs lack large intracellular domains or intrinsic kinase activity, signal propagation across the membrane involves the CD3 intracellular domains [21] containing immunoreceptor tyrosine-based activation motifs (ITAMs) [30]. ITAM chains, buried in the hydrophobic interior of the membrane are inaccessible to Src kinases, preventing spontaneous phosphorylation [31]. Ligand binding to TCR must induce conformational transitions that propagate to CD3, extending its cytoplasmic tails for ITAM phosphorylation. Several considerations suggest that this propagation must involve forces. Soluble monomeric pMHC are poor activators of TCR triggering, while surface-bound pMHC efficiently activate TCRs, suggesting that TCR triggering requires additional steps beyond pMHC binding [25, 32]. Structural studies indicate that electrostatic interactions between the TCR- α and CD3 transmembrane regions create a pivot which can mechanically couple antigen binding and force application to conformational changes within the CD3 $\zeta\zeta$ cytosolic regions [33] (Fig. 1a, inset).

One unresolved question is the directionality of the applied force necessary for TCR triggering. While forces tangential to the cell membrane can engage the TCR-CD3 pivot driving the conformational changes leading to triggering [33], forces normal to the cell membrane along the TCR axis are required to engage the catch-bond and induce signaling [28]. Overall, these observations raise the following questions: what is the magnitude and direction of forces *in situ*? How do internal forces link to the TCR complex? What are the contributions of the various force-generating cytoskeletal elements to TCR activation?

Finally, we note that much less is known about whether mechanical induction is required for BCR activation and whether applied forces allow antigen discrimination and internalization. Soluble antigens are potent activators of B cell signaling but work stemming from the studies of Batista and colleagues [34, 35] have shown that surface-anchored antigens are more efficiently gathered [34, 36, 37]. Moreover, monovalent antigens are able to induce BCR clustering, potentially as a result of conformational changes induced by forces generated upon cell-substrate contact [38]. The most compelling evidence for mechanical regulation of B cell signaling comes from an elegant study combining DNA-based molecular force sensors and engineered substrates showed that B cells apply tension to the BCR-antigen bond and extract antigen from surfaces in an affinity-dependent manner [39, 40]. AFM-based force-probes showed the rupture forces of antigen/BCR bonds to be in the pN range. However, there are no direct demonstrations of force-dependent structural rearrangements in BCRs in a manner analogous to the TCR.

2.2 Integrin receptors

In addition to TCRs, integrin-dependent interaction between T cells and APC are important for signaling activation, immune synapse (IS) formation, and T cell trafficking [41, 42]. The integrin α L β 2 LFA-1, which is expressed exclusively in leukocytes and its binding to ligand, ICAM-1 is important for T cell adhesion to APC and co-stimulatory signaling enabling lymphocyte activation. In resting T cells, LFA-1 integrins are in a bent conformation, leading to low affinity binding with ICAM-1. TCR stimulation induces conformational change in LFA-1 to relieve the inhibitory conformation into an extended state, which binds ligands with intermediate affinity (inside-out signaling) [42]. Forces applied to the integrin-ligand bond induce further conformational change into an open state, which enables highest affinity binding (~100 fold increase) [43] (Fig. 1a inset). This force-induced change in affinity allows integrins to behave as mechano-sensors. LFA-1 binding with ICAM-1 behaves like a catch bond [44], similar to other integrins [45]. During IS formation, ligand-engaged LFA-1 undergoes spatiotemporal reorganization driven by actin flows. Different activated forms of LFA-1 partition to different regions of the IS in an actin flow dependent manner, suggesting that cytoskeletal forces are important in patterning protein distributions during early T cell activation [46]. Recent work from the Burkhardt group has revealed that actin-dependent constrained mobility of ICAM-1 on the APC surface promotes integrin (LFA-1) activation [47], further supporting the notion of force mediated mechanotransduction in T cells. T cells also express the α 4 β 1 integrin VLA-4, which influences T cell activation. Interestingly, VLA-4 ligation to its ligand, VCAM-1, leads to a dramatic arrest of actin retrograde flow [48, 49] but its effect on cellular forces and microcluster dynamics remain to be tested.

3. Cytoskeletal dynamics during immune cell activation

Cellular mechanotransduction largely involves cell-generated forces, which result from cytoskeletal rearrangements. Below, we briefly review studies of cytoskeletal dynamics in immune cells that accompany signaling events.

3.1 Actomyosin dynamics in T cells

Among the first events after TCR engagement with antigen is the onset of actin polymerization at the contact zone between T cells and APC [50, 51] (Fig. 1a), which drives membrane deformation and cell spreading facilitating further receptor-antigen binding [10, 11, 52–54]. The cell edge is highly dynamic with extensive protrusions/retractions [55], which may allow efficient antigen sampling. Actin polymerization and myosin contraction induced by TCR engagement results in retrograde flow of actomyosin at the cell periphery which serves as a primary force-generating element at the cell-substrate interface. The advent of super-resolution imaging and novel fluorescent probes has revealed a diversity of actin structures at the T cell/substrate interface [56]. On planar substrates (and conjugates), within 2–3 minutes of stimulation, the actin network forms an annular ring at the lamellipodium and is composed of the characteristic Arp2/3 mediated branched networks as well as formin-mediated linear bundles. At the rear of the lamellipodium, the linear bundles condense into arc-like structures under the action of myosin II motors. Interestingly, unlike adherent cells, myosin activity is not required for maintenance of retrograde flow [48, 49], raising questions about the role of myosin contractility in force generation and T cell activation.

3.2 Microtubule dynamics in T cells

The initial contact of T cells and APC is also characterized by reorientation of the microtubule (MT) cytoskeleton and the centrosome towards the contact zone [57]. It is believed that the MT cytoskeleton acts as a scaffold, holding lytic granules and guiding centrosomal reorientation towards the APC for directional secretion [58] as well as reorganization of signaling microclusters [59] and other signaling pathways. However, the contribution of the MT to force generation at the synapse has been relatively unknown, despite the fact that organelle movement as well as MT deformation clearly indicates the existence of forces. We recently found that MT tip dynamics at the lamellipodial/lamellar region modulate NMII filament assembly and lamellipodial actin flow through the RhoGTPase pathway and modulates the traction forces exerted by T cells [60]. These studies suggest that centrosomal movement and microtubule deformations result from forces generated by MT motors and the actomyosin cytoskeleton [61–64], and point to the importance of interactions between the actin and MT cytoskeleton [65] in force generation and force balance at the immune synapse, but its role in TCR signaling remains to be explored.

3.3 Actin dynamics in B cells

In resting B cells, the ezrin/radixin/moesin (ERM) family proteins couple cortical actin to the plasma membrane [66], impeding BCR diffusion. Signaling cascades downstream of BCR antigen interaction cause detachment of cortical actin from the plasma membrane,

increased BCR mobility and enhanced signaling [67]. Subsequently, as the B cell spreads, actin undergoes dramatic reassembly, establishing lamellipodial retrograde flow, which drives the centripetal movement of microclusters [37, 68, 69]. Additionally, *de novo* actin polymerization is detected at locations of BCR microcluster formation [70]. After maximal spreading, the cell undergoes contraction and BCR clusters merge into a central cluster [70, 71] leading to signaling inhibition and subsequently antigen internalization. The mechanisms underlying B cell contraction and associated actin remodeling remain elusive, but likely involve myosin contractility, signaling inhibitors [72], and actin regulatory proteins WASP and NWASP [73]. These findings implicate feedback loops coupling actin dynamics/regulation and cellular forces with signaling to drive the transition from activation to inhibition.

4. Measuring cellular force generation during immune cell activation

Recent advances in imaging and force measurements in live cells have begun to reveal the biophysics of force generation by immune cells during activation, elucidating the regulation of immune cell signaling by mechanical events. These techniques typically measure the displacement of a calibrated force sensor in response to a cellular force.

Husson et al. developed a force probe to measure forces exerted by the T cell on an antibody-coated microbead [74]. Activation resulted in a pushing response, as the T cell spread on the microbead, followed by a pulling response, accompanied by Ca^{2+} influx and early signaling. The typical force generated during the pushing phase was ~20–30 pN. The median loading rate during the pulling phase was ~2–3 pN/sec and increased linearly with probe stiffness, suggesting a form of mechanosensitivity. However, Ca^{2+} dependence on stiffness was not measured. Li and Butte used an atomic force microscope (AFM) tip coated with anti-CD3 or pMHC to stimulate primary and Jurkat T cells and measured pushing and pulling forces ~1nN [75]. Interestingly, they did not find correlations between the total Ca^{2+} flux and the magnitude of the applied force. but these were temporally correlated. Actin dynamics and myosin contractility were required for force generation. However, neither of these studies determined the spatiotemporal organization of forces in the plane of the T-cell/APC surrogate interface.

Two recent studies have adapted traction force microscopy (TFM) using ligand-coated elastic substrates to mimic an APC to measure forces during T cell activation. Bashour et al. [76] microfabricated polydimethylsiloxane (PDMS) pillars in a dense array (2 μm spacing) coated with stimulatory ligands (Fig. 1b). T cells spreading on the array deflected the pillars, first radially outward (similar to the pushing phase) and then radially inwards (pulling phase). Individual pillars were subject to peak forces of ~50 pN, with a total force of ~1nN. Force development required Src kinase signaling and was specific to TCR activation. Conventional TFM employs polyacrylamide (PA) substrates with embedded fluorescent marker beads and uses elasticity theory to calculate traction forces from the displacement of the beads [77–79] (Fig. 1c). We used PA gels coated with anti-CD3 antibodies to measure traction forces while simultaneously monitoring actin dynamics [19]. We found that cells exerted median average traction stresses in the range of 5–10 Pa, peak traction stresses of 10–30 Pa corresponding to ~1–2nN of total force. These forces were specific to TCR-ligand

binding, and both actin dynamics (polymerization and depolymerization) and myosin activity were required for force generation. We have recently shown that microtubule tip dynamics modulate force generation in T cells [60].

While polyacrylamide substrates offer a relatively easy method to measure cell-exerted forces, they are limited in spatial resolution to about $1\text{--}2\ \mu\text{m}^2$. Recently, several groups have developed DNA-based tension sensors that can measure pN forces with near-single-molecule resolution [80] (Fig. 1d). Salaita's group has used this approach to demonstrate that individual TCR-pMHC complexes experience $10\text{--}20$ pN forces exerted by cytoskeletal dynamics [81]. The magnitude of these forces modulates the sensitivity of TCRs to specific antigens, as reducing the forces reduced the response to agonist antigens. The various force measurement techniques and results are summarized in Table 1.

Overall, these studies indicate that forces exerted by T cells are relatively weak and correspond to $\sim 10\ \text{pN}/\mu\text{m}^2$ of stress, consistent with the measured value of external force needed for TCR triggering. Based on the observed stiffness of Jurkat cells, Young's modulus $E \sim 50\text{--}100\ \text{Pa}$ [82], the expected value of maximum force, $F \sim E \times \text{area} \sim 2\text{--}5\ \text{nN}$, suggesting that T cells which are softer than adherent cells ($1\text{--}5\ \text{kPa}$ [83]), generate weaker tractions, but these are sufficient to activate individual TCRs.

5. Mechanosensing at the cellular scale

5.1 Microcluster formation and transport in T cells

Upon receptor engagement, TCR assemble into signaling microclusters at sites of close adhesion [54, 84]. Signaling microclusters are the sites of early signaling. Activated TCR recruit a host of downstream signaling molecules into these microclusters as well as several actin regulatory proteins [52]. Signaling proteins in microclusters recruit and activate RhoGTPases, which in turn activate actin regulatory proteins. Such dense localization of actin regulators at microclusters primes them to being "hotspots" of actin dynamics. Indeed we have observed 'actin waves' or bursts of actin polymerization originating from signaling microclusters [49].

Initially clusters form at the periphery as the cell edge is forced outwards by actin dynamics and allows the cell to sample the antigen-presenting surface [6]. Over a time-scale of several minutes, receptor microclusters and signaling molecules organize into the ordered spatially symmetric structure of the immune synapse. Microclusters are rapidly transported centripetally towards the cell center by acto-myosin retrograde flows [10, 53, 85] and potentially MT based motors [59], forming the cSMAC (central supramolecular activation cluster) surrounded by a ring of integrins (LFA-1/ICAM bonds) in the pSMAC (peripheral supramolecular activation cluster). Importantly, TCR-MHC bonds are much smaller ($10\text{--}15\ \text{nm}$) than LFA-ICAM bonds ($45\text{--}50\ \text{nm}$) or other surface molecules such as phosphatases and glycoproteins. This difference in size creates energetic barriers that must be overcome for size-dependent spatial segregation to occur [86, 87]. The role of cytoskeletal forces for kinetic segregation, along with associated kinetic proofreading models for TCR signaling have been exhaustively reviewed in Comrie et al. [88]. Further evidence for active formation of microclusters comes from a recent study which used high-resolution light sheet

microscopy to show that dynamic microvilli on T cells drive the formation of close contacts on the APC surface, which are colocalized with TCR microclusters [89]. This is consistent with earlier work showing the correlation between microclusters and regions of reduced membrane fluctuations [84]. These findings suggest that active forces, potentially generated by the cytoskeleton, may enhance the efficacy of TCR triggering by enabling and stabilizing contacts between the T cell membrane and APC.

5.2 Sensing substrate stiffness

The functional consequences of mechanosensitivity are best highlighted by the findings that mesenchymal stem cells differentiate into specific cell lineages depending on substrate stiffness [90]. Similar experiments in which stimulatory ligands were presented to T cells on PA substrates of varying stiffness showed that stiffer surfaces (100–200 kPa) elicited greater cytokine production in mouse CD4⁺ T cells than softer ones [20]. Conversely, human CD4⁺ cells were more strongly stimulated on 100–200 kPa PDMS substrates than stiffer ones (2 MPa), suggesting a biphasic response pattern of stiffness sensitivity [91]. In all cases, myosin inhibition led to loss of sensitivity to substrate stiffness. However, these results must be viewed against the fact that T cells are significantly softer (~1 kPa) and most models of force generation posit that cellular forces rapidly saturate at substrate stiffness values that are ~5–10x of the cell's stiffness [92]. Using PA substrates, we showed that traction forces exerted by T cells exhibited sigmoidal behavior as a function of substrate stiffness [19], with the total exerted forces saturating on surfaces of ~5kPa stiffness. Recent studies have found that the stiffness of many immune cells varies in the range of a few kPa, suggesting that T cells need to interact with (or discriminate between) relatively soft surfaces *in vivo* [82]. Intriguingly, Jurkat cells showed distinct differences in the dynamics of signaling and cell morphology as a function of substrate stiffness [19]. On stiff PA substrates (~5kPa), phosphotyrosine (pY) signaling rapidly peaked at ~3 min after stimulation and declined to baseline levels, with monotonic expansion of the cell edge. On soft substrates (<1 kPa), pY signaling remained sustained even at 15 min but at lower levels, with the cell edge undergoing repeated rounds of protrusions and retractions.

The response of T cells to substrate stiffness [19] appears to obey predictions from a simple model derived from active matter theory [92]. The cell exerts an active stress (σ_a) resulting from actin polymerization and myosin contractility, which consumes energy by ATP

hydrolysis. Force balance leads to a simple expression for the force, $F_{ss} = F_{sat} \frac{k_{subs}}{k_{subs} + k_{cell}}$, where F_{ss} is the steady state force and F_{sat} is the saturating force. $F_{sat} = \frac{\sigma_a A}{A}$, where A is the cell area, k_{subs} is the effective spring constant for the substrate (0.1 – 10 nN/ μ m) and k_{cell} is the stiffness of the cell (~1 nN/ μ m). Thus, on compliant substrates, the steady state force exerted by the cell is predicted to linearly increase with stiffness and saturates when $k_{subs} \gg k_{cell}$. Assuming a linear force-velocity relationship, the loading rate can be estimated as

$\frac{dF}{dt} \sim \frac{A \sigma_{sat}}{\eta} k_{subs}$, where $\eta = \tau(k_{subs} + k_{cell})$ is the viscous dissipation in the actin gel and A is the area over which the stress is exerted. Using the estimated values for these parameters ($\tau \sim 10$ s, $k_{subs} \sim k_{cell}$), a μ m² patch of TCRs would experience loading rates of ~2–3 pN/sec, which is similar to the force probe experiments [74].

While immune cells encounter substrates (e.g. APCs) whose stiffness is in the low kPa range [82], conventional strategies to expand clonal populations of T cells for adoptive immunotherapies use protein-coated microbeads [93], which are significantly more rigid. Alternate strategies that mimic APCs *in vivo* may be better in stimulating T cells. Exploiting this, the Kam group used PDMS microbeads to stimulate CD4⁺ and CD8⁺ T cells and observed a stronger proliferative response [94]. However, it is unclear whether the enhanced proliferative response was due to the nanoscale structure of the polymer or changes in substrate rigidity. Nevertheless, exploiting the mechanosensitivity of T cells may enhance strategies for T cell based immunotherapies.

B cells also appear to be mechanosensitive, exhibiting strong early BCR signaling and Ca²⁺ responses on stiffer antigen-coated elastic substrates, whereas cell proliferation is higher on softer substrates [95, 96]. An elegant study from the Tolar group showed that follicular dendritic cells are stiff and promote strong B cell pulling forces and stringent affinity discrimination [40]. In contrast, dendritic cells are soft and promote acquisition of low-affinity antigens through low forces. Thus, the mechanical properties of B cell synapses regulate antigen extraction, suggesting that distinct properties of presenting cells support different stages of B cell responses.

Finally, Huse and colleagues have shown that the killing responses of cytotoxic T lymphocytes are mechanosensitive and enhanced by forces [97]. Upon formation of an immune synapse like structure, CTLs secrete pore-forming proteins called perforins to lyse the target cell. Altering the membrane tension of the target cells using pharmacological means or osmotic shock and showed that perforin-induced pore formation was strongly affected. Similarly, altering the membrane tension of the target cells by changing substrate stiffness again altered cell killing, with cells on stiffer substrates being more sensitive to perforin-induced pore formation.

5.3 Sensing ligand mobility

Lymphocyte engagement with APCs also results in extensive changes in cytoskeletal and lipid membrane composition of the APC [98–100]. Consequently, the mobility of pMHC complexes, integrin and other co-receptor ligands at the APC membrane may be modulated as they partition into lipid microdomains or associate with tetraspanin (family of small proteins with four transmembrane domains) complexes [101]. Disruption of lipid raft integrity reduces antigen presentation by class-II MHC complexes in B cells cholesterol, which modulates the diffusion of transmembrane receptors [102], affects lymphocyte signaling; tetraspanins accumulate at the immune synapse, where they form enriched membrane microdomains and cluster MHCs [101]. These studies suggest that the plasma membrane environment undergoes fluctuations in its lipid and protein composition, which may serve to modulate signaling, in part by altering ligand mobility [103].

Despite this evidence, few studies have explicitly addressed how the biophysics of ligand (or receptor) mobility influences lymphocyte signaling. Groves and colleagues used nanofabricated 10–20 nm high chromium barriers on stimulatory supported bilayer surfaces, which allow for free lipid diffusion in the bilayers but block movement of proteins with larger cytoplasmic domains. Blocking the movement of TCR microclusters from the

periphery to the center prolonged pY signaling levels [104], suggesting location-dependence of TCR signaling. Intriguingly, actin dynamics in the vicinity of stalled clusters was altered compared to the regions between barriers [105]. In a complementary approach, altering the mobility of lipids and proteins by modifying the lipid composition of stimulatory bilayers showed that increased diffusivity resulted in higher Ca^{2+} influx, greater microcluster mobility and enhanced pY signaling as well as altered actin dynamics [106]. It is interesting to note that these two studies suggest opposite effects of mobility on signaling, however the mechanisms behind these differences remain to be explored. It is possible that the sensitivity to ligand mobility may be dependent in a non-trivial manner on spatial location in the immune synapse and this would require higher resolution studies (super resolution and single molecule imaging) to decipher.

Studies from the Batista lab have highlighted the importance of BCR diffusion in early B cell signaling [37, 67, 107], implying that ligand mobility may control signaling by modulating BCR diffusion and clustering. We examined BCR clustering, mobility and signaling when activated by mobile (on lipid bilayers) and immobile (on glass) ligands [108]. B cells interacting with mobile ligands displayed significantly greater signaling. Moreover, microcluster movement required actin polymerization, suggesting that the static actin network acts as a diffusion barrier, corralling BCRs in the initial phases of B cell activation while active polymerization is required for BCR microcluster coalescence and centralization. These studies suggest the existence of an intricate feedback loop between actin polymerization and receptor movement, which leads to global organization of membrane proteins and signaling components at the lymphocyte/APC interface.

6. Summary and future perspectives

Recent advances in the field have made it abundantly clear that the physical environment is a strong modulator of immune cell responses. The biophysical basis of mechanosensitivity remains unclear, but likely involves forces generated by actin polymerization and myosin-based contraction, interacting with the membrane, receptor-ligand bonds and microclusters. While the signaling function of microclusters is well studied, the mechanism of their formation and spatial organization is not completely understood. In adherent cells, integrin-ECM linkages lead to focal adhesions whose growth and signaling depend on locally applied cytoskeletal forces. Thus focal adhesions act as mechanosensors which couple integrin binding and actin flow with signaling. Whether TCR-associated signaling microclusters serve a similar role in T cells is not known, but it is interesting to speculate that they might do so given the similarities in the molecular players. Force transmission must involve coupling between microclusters and actin [49, 53, 104, 105, 109, 110], but what mediates this coupling is not known. Resolving this question requires measurement of forces with high spatial resolution while simultaneously monitoring actin dynamics and microcluster assembly with genetic manipulation of candidate molecules. While traction forces give a measure of the magnitude of cell-generated forces, the intracellular forces experienced by the immune receptors are expected to be stronger. It is possible to directly measure intracellular forces by measuring the displacements of small (~200 nm) beads inside cells [111] or by calibrated fluorescence resonance energy transfer (FRET) based force probes [112]. Another possibility is to measure actin flows and use computational analysis and

assumptions about the viscoelasticity of actin networks to infer forces [113, 114]. Such measurements remain to be made for immune cells, but would likely yield a more accurate estimate of the forces experienced by TCRs.

In addition to stiffness and mobility, discussed here, the topography of the environment may be important in dictating immune cell function. T and B cells navigate complex topography in the lymph nodes and thymus with extensive membrane folds on APC surfaces or fibrillar structures on follicular dendritic networks. These structures present regions of high curvature, which might recruit curvature-sensing signaling proteins and actin regulators, thereby modulating cytoskeletal dynamics. The role of topography on immune cell signaling activation is an open question for future studies.

Future work must also consider the crosstalk between different receptors (e.g. TCR and integrins) and co-stimulatory or inhibitory receptors in determining the global cellular response to physical cues. Finally, while we have a better knowledge of how cellular forces, proximal signaling and certain functional responses depend on the physical environment; mechanical modulation of gene expression in immune cells is completely unstudied and is open for future research. A recent study showed that the nucleus undergoes dramatic deformation by actin-based forces upon T cell activation [115], suggesting possible changes in gene expression that may be mechanically modulated.

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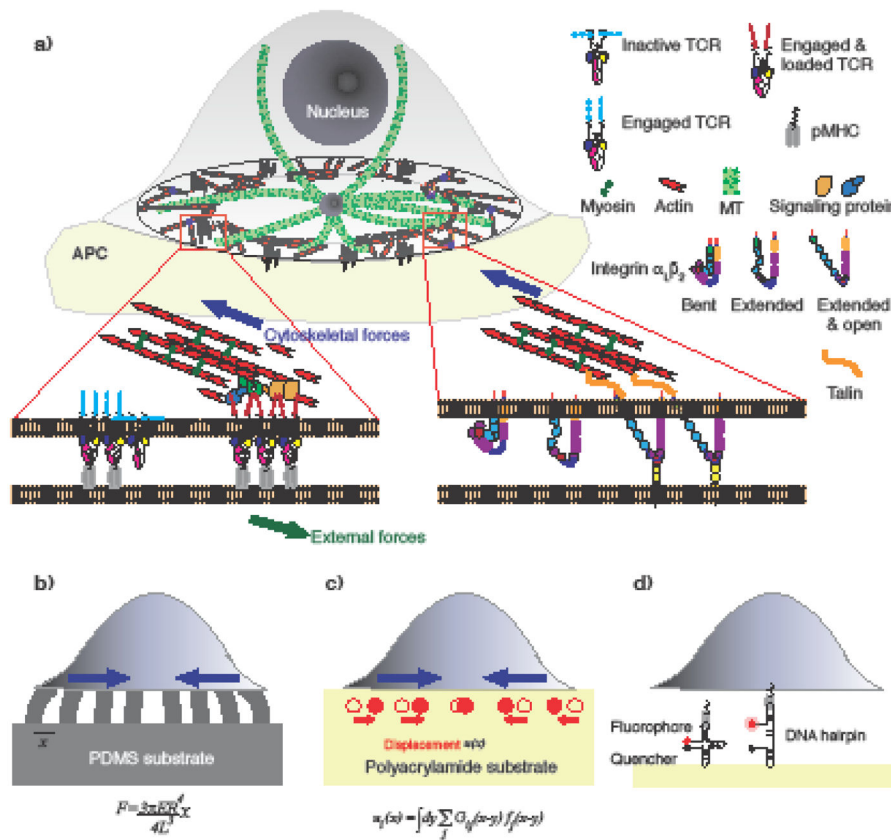


Figure 1. Cytoskeletal forces during immune cell activation

(a) Schematic diagram of a T cell spreading on the surface of an APC. The contact zone shows spatiotemporal organization of actin into Arp2/3 mediated branched networks and formin-mediated actin arcs. MT emanate from the centrosome. The insets depict conformational changes resulting from the application of actomyosin forces on TCR microclusters (left) and integrin receptors (right). One of many possible conformational changes in the TCR is shown. Cartoons of (b) a cell on PDMS microposts showing deflection of posts resulting from cellular forces, (c) a cell on a PA gel depicting movement of embedded beads as the cell exerts traction forces. The measured displacement field $u(x)$ and the traction stress field, $f(x)$ are related by the integral equation in the figure, with $G(x-y)$ is the Boussinesq Green function, (d) a cell on a glass substrate with DNA-hairpin based tension sensors. The fluorophore (red sphere) is near the quencher (black sphere) when the ligand attached to the hairpin is free. Ligand binding and subsequent force application moves fluorophore away from the quencher.

Table 1

Comparison of different force measurement techniques.

Study	Measurement technique	Force Magnitude	Signaling response	Significance
Husson et al.	Calibrated force probe	20–30 pN	Ca ²⁺ influx	Established the role of forces in T cell activation.
Bashour et al.	Nanopillar array	~1 nN	Syk/ZAP70/SFK phosphorylation, IL2 secretion	First study to measure forces exerted during T cell activation.
Hui et al.	Polyacrylamide gel	~1 nN	ZAP70/LAT phosphorylation	Mapped the spatiotemporal characteristics of T cell forces and showed that T cell signaling was mechanosensitive. Showed that actomyosin contractility was necessary for force generation.
Hu and Butte	Atomic force probe	~ 1nN	Ca ²⁺ influx;	An AFM based study to show that T cells are triggered by external forces and generate actin dependent forces upon stimulation. Showed temporal correlation between Ca ²⁺ flux and force
Liu et al.	DNA-based tension sensors	~ 1nN	Ca ²⁺ influx, Lck/ZAP70 phosphorylation	Performed a high-resolution (near single-molecule resolution) mapping of forces exerted during T cell activation. Showed that forces modulate sensitivity to antigen.

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