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Tolerogenic Nanoparticles to Treat Islet Autoimmunity

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Abstract

Purpose of Review—The current standard therapy for type 1 diabetes (T1D) is insulin replacement. Autoimmune diseases are typically treated with broad immunosuppression, but this has multiple disadvantages. Induction of antigen-specific tolerance is preferable. The application of nanomedicine to the problem of T1D can take different forms, but one promising way is the development of tolerogenic nanoparticles, the aim of which is to mitigate the islet-destroying autoimmunity. We review the topic and highlight recent strategies to produce tolerogenic nanoparticles for the purpose of treating T1D.

Recent Findings—Several groups are making progress in applying tolerogenic nanoparticles to rodent models of T1D, while others are using nanotechnology to aid other potential T1D treatments such as islet transplant and islet encapsulation.

Summary—The strategies behind how nanoparticles achieve tolerance are varied. It is likely the future will see even greater diversity in tolerance induction strategies as well as a greater focus on how to translate this technology from preclinical use in mice to treatment of T1D in humans.

Keywords

Tolerance; Type 1 diabetes; PLG nanoparticles; Diabetogenic antigens; Regulatory T cells

Introduction

Type 1 diabetes (T1D) is an autoimmune disease in which cells of the immune system destroy the insulin-producing β cells located in the pancreatic islets of Langerhans. Disease onset can occur at any time, but most often happens at 5–7 years of age or puberty, and there are about 280 million cases worldwide today [1, 2]. Currently, the most common therapy for T1D is insulin replacement [1–3]. Unfortunately, insulin replacement is not without its drawbacks. The discomfort of subcutaneous injection and imperfect knowledge of patient

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Compliance with Ethical Standards

Human and Animal Rights and Informed Consent This article does not contain any studies with human or animal subjects performed by any of the authors. All procedures performed in studies involving animals were in accordance with the ethical standards of the institution or practice at which the studies were conducted.

Conflict of Interest Tobias Neef declares that he has no conflict of interest.

glucose levels make managing T1D difficult and suboptimal [2], with significant risk of severe hypoglycemia, so that there is a need for better and more efficient therapies.

Nanotechnology as a concept has been in existence for approximately 60 years, but its application to medical therapy dates back about half that time [4, 5•]. While nanomedicine may have a multitude of incarnations ranging from diagnostic devices to tissue regeneration, much of it has focused on the reformulation and delivery of small molecules or biologic drugs such as proteins or nucleic acids [2, 4, 5•]. More recently, researchers have turned to nanoparticles for immunomodulation and as potential therapeutics for immune-related diseases [4, 5•, 6]. The end goal of many of these new approaches is to reestablish immune tolerance. Tolerance can be defined in many ways [6] but may generally be thought of as a restoration of the balance between the different components of the immune system resulting in inability of the immune system to respond to self-antigens, a process that breaks down when autoimmunity arises.

In this review, we will discuss the application of tolerogenic nanoparticles to islet autoimmunity. We will review the latest views of T1D and some of its treatments, both broad-based immunosuppression and specific tolerogenic therapies, discuss the influence of nanoparticle properties on their ability to induce immunomodulation, and present recent approaches to producing tolerogenic nanoparticles, with a specific focus on those studies that are aimed at developing new treatments for T1D.

Islet Autoimmunity and T1D Treatment

Though it has been difficult to characterize islet autoimmunity in humans and many details of it remain unknown, several features are well accepted. Post-mortem examination of the pancreases of patients at various stages of T1D shows heterogeneous infiltration of CD8⁺ and CD4⁺ T cells, macrophages, and B cells [7–11]. Additionally, antibodies with specificities for the β cell antigens insulin, glutamic acid decarboxylase 65 (GAD65), insulinoma-associated protein 2 (IA-2), and zinc transporter 8 (ZnT8) are found in the serum of people with T1D and at risk for T1D [12–17]. In fact, detection of islet-reactive antibodies has become a technique for predicting development of T1D in at-risk subjects [18–20]. However, the islet-reactive antibodies appear to be neither cytotoxic nor pathogenic [21, 22].

An important requirement for the development of tolerance therapies is precise identification of the antigenic targets of autoreactive T cells. $CD4^+$ cells specific for the C-peptide of proinsulin, the precursor to insulin, have been found in the pancreas of a patient with T1D [23]. $CD8^+$ cells specific for the beta cell antigens insulin, islet-glucose-6-phosphatase catalytic subunit-related protein (IGRP), IA-2, GAD65, and prepro islet amyloid protein (ppIAP) have also been found [10]. It has also been found that $CD8^+$ T cells specific for β cell antigens, isolated from the blood of patients with T1D, can kill beta cells [24–26]. Thus far, however, no epitope has been found to be solely responsible for T1D pathogenesis [27] and it is likely that multiple autoantigens are targeted. A recent study of 50 T cell lines from human donors found reactivity to "a broad range of studied native islet antigens and to posttranslationally modified peptides" [28••].

Safety issues prevent obtaining pancreas biopsies from living patients, and fewer people dying of ketoacidosis results in fewer pancreases available post-mortem [1]. The establishment of the Network for Pancreatic Organ Donors with Diabetes (nPOD) in 2007 has increased research access to human pancreas from patients with active disease, which prior to that was a very rare event. Therefore, the vast majority of research on the pathogenesis of T1D has relied on a number of mouse models. Since its development in the 1980s, the non-obese diabetic (NOD) mouse has become a favored model for studying T1D, with spontaneous disease incidence of up to 80–90% in females [1, 29, 30]. Many different T cell autoantigens have been discovered in NOD mice, though insulin, and particularly the Ins B9–23 peptide, seems to be the dominant and initial target [29, 30, 31••, 32••, 33]. While many of these antigens overlap with those found in humans, it is important to note that there are many significant differences between T1D in humans and NOD mice, including disease onset time and amount and morphology of islet infiltration [1, 20]. The utility of the NOD mouse can be seen by the many potential T1D therapies developed using it that have been tested in clinical trials, as has been reviewed elsewhere [29, 34•]. However, it has also been noted that many treatments that were successful in NOD mice have shown little efficacy in humans [1, 29, 34•]. Several groups have also made use of models involving the adoptive transfer of diabetogenic cells into either young NOD or immunocompromised mouse strains, i.e., NOD.Scid, in certain cases leading to a more time-efficient, accelerated model of T1D [35–38]. In these studies, cells with the BDC2.5 T cell receptor (TCR), specific for the beta cell protein chromogranin A (CHrA), are often used [39-41].

Many studies suggest that patients with T1D may retain a significant number of β cells at the time of diagnosis [1], a time when a substantial amount of insulin is still produced [3]. This represents a "window of opportunity" for therapeutic intervention [1]. Clinical trials with immunosuppressants such as cyclosporine, prednisone, and azathioprine near time of T1D onset led to remission, although all have associated adverse effects [27]. Safer methods are being explored, among them monoclonal antibodies against CD3 (teplizumab and otelixizumab) and CD20 (rituximab), and a fusion protein of portions of CTLA-4 and IgG1 (abatacept) [27]. Another potential approach is targeting microbiota and the related interaction with the innate immune system [30], including, for example, administration of the antibiotic vancomycin [42]. It has been noted that general immunosuppression does not cure underlying autoimmunity [43–45]. Therefore, antigen-specific tolerance that does not affect the rest of the immune system and would avoid side effects is a preferable alternative [46].

Several tolerance approaches used for the treatment of T1D are summarized in Table 1. One involves the administration of soluble antigens, as has been done with GAD, insulin, and proinsulin, delivered through a variety of routes, including intraperitoneal (i.p.), intravenous (i.v.), intranasal (i.n.), oral, and subcutaneous (s.c.) [43]. Preclinical and clinical trials using tolerance approaches have proven largely ineffective [47–58]. Significantly, s.c. or i.v. infusion of BDC2.5 mimotopes to either NOD mice or BDC2.5 transgenic mice was able to protect against T1D development [60, 61]. Another approach is DNA vaccination, using either plasmid DNA or viral vectors. Thus far, their clinical progress has been limited, though at least plasmid vaccination is noted for its economy and safety [43]. Finally, cell-based therapies have shown potential as T1D therapies. Regulatory T cells (Tregs) have been

shown to be effective in NOD mice [62–64] and recent clinical trials show they are well tolerated in humans [65•], but there is still concern with the plasticity of Tregs and their possible reversion to effector cell phenotypes. Another cell-based technique is to use diabetogenic antigens linked to apoptotic cells targeting the body's natural tolerogenic clearance pathways. These have proven protective in NOD [32••, 59, 66], transgenic NOD [67], and adoptive transfer T1D mouse models [66].

Nanoparticles and the Immune System

An examination of tolerogenic nanoparticles requires understanding of their inherent properties which determine how they interact with the immune system. Notable ones include size, charge, and shape, as well as composition of the resulting protein corona. An additional consideration concerns the route of nanoparticle administration.

The biodistribution of administered particles in the "nano-" range (1–1500 nm) [5•] depends largely on a convolution of particle size and route of administration. Subcutaneous, intramuscular, intradermal, and mucosal injection leads to interaction with the lymphatic system and, ultimately, transport to the draining lymph nodes. Smaller particles (< 100–200 nm) drain there freely. Larger particles (> 100–200 nm) must be transported there by APCs [4, 5•, 68, 69]. Particles less than 30 nm seem to be able to escape the lymph node once there [70].

Systemic administration of nanoparticles (Fig. 1) favors accumulation in the organs and tissues such as the spleen, bone marrow, liver, lungs, and kidneys [6, 71]. The site of accumulation is also dependent on particle size as particles < 100 nm can evade clearance by the reticuloendothelial system (RES), a.k.a. the mononuclear phagocyte system [72]. Particles < 5.5 nm undergo renal filtration and may be excreted via the urine [73]. Nanoparticle size also impacts which cells nanoparticles interact with. Dendritic cells preferentially internalize smaller-sized particles, while macrophages tend to take up larger ones [72].

Nanoparticle charge can be influenced by surfactants and other coating materials, thereby allowing manipulation of their interaction with the immune system [4]. Cationic particles are more likely to elicit a Th1 response, be taken up by dendritic cells, and engage the MHC class I loading pathway following phagocytosis [4, 74–78], but they have also potentially toxic properties [79, 80]. Conversely, anionic particles exhibit low toxicity in a number of studies [81–86] and associate with the macrophage scavenger receptor MARCO favoring tolerance induction [4, 87].

Various studies have shown that nanoparticle shape and structure are also important in determining the favorability and nature of nanoparticle uptake by cells [88, 89]. Furthermore, the shape/structure of a nanoparticle can also be important for interaction with the immune system, especially in terms of proper conformational display of an antigen in vaccine particles [90–94].

Lastly, the interaction of nanoparticles with biomolecules following administrations is important to consider. For instance, it is thought that the corona can have an effect on

important characteristics such as cellular uptake and biodistribution [95]. Though multiple models of the protein corona have been proposed, one recent study suggests that it forms early and is mostly stable in composition 2 min following formation [96]. Another study stressed the influence of nanoparticle size and charge on the corona's protein composition [97]. Additionally, nanoparticles decorated with antigen may attract antibodies in presensitized individuals, leading to anaphylaxis in certain cases [98•].

Tolerogenic Nanoparticles

The tolerogenic nanoparticles we review here can be broadly separated into two categories: (1) carrier particles that target or reformulate immunomodulatory agents and (2) antigen or disease-specific nanoparticles. Many of the former have been reviewed elsewhere [6, 71, 99], but certain examples merit repeating here. Phillips et al. were able to incorporate antisense oligonucleotides for the costimulatory molecules CD40, CD80, and CD86 within PEG/PVP nano/microparticles, in order to convert DCs uptaking them to a suppressive phenotype [100]. Leuschner et al. used small lipid nanoparticles to deliver small interfering ribonucleic acid (siRNA) to inflammatory monocytes, in order to silence expression of the chemokine receptor CCR2, thus limiting their recruitment to tissues [101]. Wang et al. synthesized nanoparticles consisting of a dextran-coated iron oxide core labeled with Cy5.5 and conjugated to siRNA targeting β_2 microglobulin to downregulate MHC class I expression as well as acting as a fluorescent and magnetic detection probe [102]. Lastly, Shah et al. loaded diblock polymer-based nanoparticles with the soluble immunosuppressant molecule rapamycin in order to limit its exposure to the kidneys and provide slow release, thereby reducing its toxicity [103]. Although not directly related to T1D, the rapamycinloaded nanoparticles showed signs of being as or more effective than free rapamycin as a therapeutic for Sjogren syndrome, another autoimmune disease that uses the NOD mouse as a spontaneous model, with the additional effect of reduced toxicity.

Other studies have made use of nanoparticle strategies that are specific or related to particular autoantigens (Table 2 and Fig. 2). One approach made use of iron oxide nanoparticles coated with major histocompatibility complex (MHC) class I or II molecules loaded with peptides related to autoimmune disease [104, 105••, 106]. This resulted in the expansion of cognate cells with regulatory potential present as part of a negative feedback loop in response to the autoantigen [104] or conversion of effector/memory T cells into regulatory T_R1-like cells [105••]. An advantage of this technique is that, while it requires the presence of cells specific for and experienced with the antigen/peptide loaded onto the MHC molecule, it is not antigen specific. Instead, the authors classify it as "disease specific." This can be seen as a benefit because it requires no knowledge of the antigen's role in disease pathogenesis or progression. When the particles were coated with MHC II molecules, they showed efficacy in multiple disease models, including experimental autoimmune encephalomyelitis (EAE) and collagen-induced arthritis (CIA) [105••]. Both the MHC I and MHC II approach were also tested in models of T1D [104, 105••], as will be described in the next section. An added benefit is that the degradation of the iron oxide particles will fold into natural iron metabolism pathways and, indeed, initial tests show that the particles have low potential for dangerous side effects [106] and do not suppress the ability of the immune system to clear a pathogen [105••].

Another approach used gold particles surrounded by polyethylene glycol (PEG) and loaded with both the EAE T cell epitope myelin oligodendrocyte glycoprotein residues 35 to 55 (MOG_{35-55}) and a small molecule aryl hydrocarbon receptor (AhR) ligand [111]. DCs were shown to take up the nanoparticles and subsequently expanded Foxp3⁺ Tregs in vitro. This approach was shown to reduce severity in EAE and the mechanism of action was shown to be related to the presence of Foxp3⁺ Tregs. It was later extended to tolerance induction in the NOD model of T1D [112••], also described in the next section.

Other studies employing antigen-specific tolerogenic nanoparticles have made use of such diverse strategies as co-encapsulation of autoantigens with rapamycin in poly(lactide-*co*-glycolide) (PLG) nanoparticles [109, 110], decoration of liposomal nanoparticles with antigen and inhibitory co-receptor ligands [113, 114], coating PLG nanoparticles with red blood cell membranes [115], and coupling both peptide-loaded HLA and apoptosis-inducing IgM to epoxy beads [107, 108].

Lastly, our group and collaborators have used highly negatively charged biodegradable PLG nanoparticles to treat a variety of mouse models of immune-related diseases. Both antigenconjugated and antigen-encapsulating particles have been used in Th1/Th17-mediated EAE [116••, 117••, 118••], Th2-mediated allergic airway inflammation [98•], and minor antigen mismatched bone marrow transplant [119•]. The exact mechanisms behind the tolerance induction in this model are still under investigation, but it is thought that intravenous administration leads to uptake of the carboxylated PLG nanoparticles by splenic marginal zone macrophages via the MARCO scavenger receptor, thereafter triggering various tolerogenic pathways including cell-intrinsic anergy and the activation of Foxp3⁺ Tregs and IL-10-producing Tr1 cells. A recent study, however, has highlighted the importance of liver macrophages in addition to those in the spleen [118••].

Application of Tolerogenic Nanoparticles to T1D

Several strategies to reformulate immunomodulatory agents using nanoparticles have shown efficacy in T1D models. For example, the nano/microparticles described by Phillips et al. [100] prevented or reversed disease in NOD mice and prevented it when T cells from treated mice were co-transferred with NOD diabetogenic cells into NOD.Scid mice.

Antigen-specific therapies have also been applied to the treatment of T1D. The nanoparticles used by Tsai et al. [104] were able to protect against development of T1D in young NOD mice, reverse recent-onset NOD T1D, and restore normal glucose levels in a humanized mouse model. The particles interacted directly with low-avidity $CD8^+$ T cells and expanded them into a population of regulatory $CD8^+$ T cells that prevented or reversed disease. Building on these results, Clemente-Casares et al. [105••] expanded T_R1-like cells out of antigen-experienced CD4⁺ T cells and eventually created a "regulatory network" that also included regulatory B cells and was able to reverse hyperglycemia in NOD mice and prevent its onset in adoptive transfer models involving NOD.Scid mice.

Yeste et al. [112••] used gold nanoparticles coated with PEG, proinsulin, and the tolerogenic AhR ligand ITE to target dendritic cells. The induced tolerogenic phenotype of the DCs in

turn led to induction of CD4⁺ Treg cells which were able to suppress T1D onset when administered to NOD mice at 8 weeks of age in both spontaneous and cyclophosphamideaccelerated models. Additionally, bone marrow-derived dendritic cells (BMDC) that had been incubated in vitro with the nanoparticles were able to reduce T1D development in the spontaneous NOD model. Perhaps most interestingly, the nanoparticles used in this study were also incubated in vitro with human dendritic cells (hDCs), swapping out insulin for the human T1D antigen GAD_{555–567}. Measurements of gene expression and costimulatory cell surface markers suggested that a tolerogenic phenotype was induced in hDCs as well. Subsequently, the treated hDCs were able to decrease IFN- γ secretion in a human GADspecific CD4⁺ T cell.

Our group has used insulin and the P31 CHrA mimetope of transgenic BDC2.5 CD4⁺ T cells in various formulations to treat T1D in two different mouse models [120••]. P31 coupled to apoptotic splenocytes was able to delay and significantly reduce spontaneous T1D onset in NOD mice and a single intravenous infusion was enough to protect NOD.Scid mice from hyperglycemia for 90 days following adoptive transfer of BDC2.5 cells. Envisioning clinical translation of this tolerance induction pathway, we began to focus instead on biodegradable PLG nanoparticles as antigen-carriers. P31-coupled or P31-encapsulating nanoparticles were able to protect against adoptive transfer mediated T1D by sequestering autoreactive T cells in the spleen and decreasing inflammation in the pancreas. Tolerization was shown to be mediated by PD-L1 and CTLA-4 signaling and long-term maintenance of tolerance was found to depend on the induction of Tregs. We have been further able to show similar efficacy using the same approach with a mimotope of CD8⁺ NY8.3 transgenic T cells.

The approach of Yeste [112••], as well as our group's research, indicates the need for loading a tolerogenic nanoparticle with insulin when used in the NOD spontaneous onset model. Indeed, when apoptotic splenocytes were used as the antigen carrier, only insulin and InsB₉₋₂₃ proved effective in preventing disease [32••]. Furthermore, only full-length insulin was fully tolerogenic when the particles were administered later in life (19–21 weeks of age). Data from our group has shown that nanoparticles which encapsulate antigen may be preferable to ones in which the antigen is displayed on the particle surface in terms of patient safety [98•]. Taken together, this means a nanoparticle that encapsulates full-length insulin or proinsulin is a promising therapeutic for testing in the NOD mouse model. While encapsulating insulin remains challenging, efforts are underway to optimize its loading while still controlling nanoparticle size [123].

Finally, nanoparticles may be used in tolerance induction in conjunction with pancreatic islet cell transplantation. Transplant of either stem cell or deceased donor origin islet cells is a promising technique for curing T1D, especially for those suffering from severe hypoglycemia. Sadly, however, recipients of allogeneic islet grafts require lifelong immunosuppression to avoid host rejection of the transplanted cells [3, 46]. Our group and collaborators have explored the use of negatively charged antigen-coupled or encapsulating nanoparticles to induce tolerance in transplant models [122] and have used ECDI-treated donor splenocytes to tolerize recipients of islet transplants [124•]. A recent study investigated the feasibility of using donor antigen-coupled PLG nanoparticles in place of

apoptotic cells. The treatment was successful in producing tolerance in about 20% of recipient mice. Adding a small dose of rapamycin to the nanoparticle treatment increased that number to approximately 60% [121•]. Wang et al. [102] used the previously described magnetic nanoparticles conjugated to siRNA to inhibit rejection in a kind of xenograft of human islet to NOD.Scid mice reconstituted with NOD splenocytes. Another potential application of nanotechnology to islet transplant is the encapsulation of islets using engineered capsules to protect the islet from an immune response. A comprehensive discussion of this approach can be found elsewhere [125], but two key points can be addressed. Firstly, one of the most pressing concerns is the need for precise control of pore size in the capsule material to protect from immune components but also to allow for proper β cell function and viability. Additionally, materials need to be engineered to promote vascularization and prevent fibrosis at the site of the transplant.

Conclusions and Future Directions

The uptake of nanoparticles by phagocytic cells makes them a natural choice for testing as tolerogenic agents. The properties of nanoparticles, including size, charge, and shape, as well as their route of administration, may be altered to specifically target their effect to one or several populations of immune cells. Here, we have reviewed approaches using nanoparticles that aim to induce antigen- or disease-specific tolerance, particularly in regards to treatment of T1D. For many of the remaining studies referenced in this manuscript that have not been tested in models of T1D, there is no reason why they cannot be modified to blunt, prevent, or delay islet cell-directed autoimmunity.

Given the increasing uses in which nanotechnology is being employed in the medical arena, it is likely that future development of tolerogenic nanoparticles will not be limited to simply abrogating islet autoimmunity. Innovative applications, such as the induction of donor-specific tolerance in order to allow pancreas or islet transplant, may be used either alone or in concert with autoantigen-specific tolerance. Future work in this area is also likely to focus on considerations not discussed in this review, such as the safety versus toxicity of nanoparticles, their cost benefit, and the ability of their manufacture to be scaled up to industry levels. The very fact that these concerns are being addressed demonstrates the translational potential of this promising new technology.

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Fig. 1.

Effect of nanoparticle size on biodistribution following systemic administration. *MPS* mononuclear phagocyte system, *RES* reticuloendothelial system

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Fig. 2.

Proposed mechanisms of tolerance induction of selected tolerogenic nanoparticle treatments. **a** Nanoparticles targeting APCs. *Top*: MARCO receptor dependent uptake of antigencoupled and antigen-encapsulating PLG [98•, 116••, 117••, 118••, 119•, 120••, 121•, 122]. *Middle*: PLG encapsulating both antigen and rapamycin [109, 110]. *Bottom*: gold nanoparticles decorated with both antigen and AhR ligand [111, 112••]. **b** Iron oxide nanoparticles coated with peptide-MHC that interact directly with T cells to expand autoregulatory cell populations [104, 105••, 106]. *APC* antigen presenting cell, *PLG*

poly(lactide-co-glycolide), *AhR* aryl hydrocarbon receptor, *MHC* major histocompatibility complex

Table 1

Summary of non-nanoparticle antigen-specific therapies tested for treatment of T1D

Antigen	Treatment method	References
GAD	Soluble Ag	[43, 47–53]
Insulin and proinsulin	DNA vaccination	[43]
	Soluble Ag	[43, 54–58]
	DNA vaccination	[43]
BDC2.5 mimotopes	Cell-based	[32••, 43, 59]
	Soluble Ag	[43, 60, 61]
	Cell-based/Treg	[43, 62]
Other cell-based	Cell-based/Treg	[43, 63, 64, 65•, 66, 67]

Table 2

Summary of antigen- or disease-specific tolerogenic nanoparticle strategies

Approach	Disease models	References
Iron oxide-pMHC	EAE, <i>T1D</i> , CIA	[104, 105••, 106]
Peptide-HLA/IgM-epoxy	N/A	[107, 108]
PLG nanoparticles encapsulating antigen and rapamycin	EAE, allergy/hypersensitivity, factor VIII tolerance	[109, 110]
Gold PEG-Ag-ITE	EAE, <i>T1D</i>	[111, 112••]
Lipid Ag-Siglec C or CD22	Factor VIII tolerance	[113, 114]
PLG coated with RBC membrane	Pathogenic antibodies	[115]
Carboxylated PLG nanoparticles coupled with or encapsulating antigen	Allergy, EAE, <i>T1D</i> , bone marrow transplantation, islet transplantation	[98•, 116••, 117••, 118••, 119•, 120••, 121•]

Italicized text indicates studies relevant to T1D