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## Challenges of Integrating Stochastic Dynamics and Cryoelectron Tomograms in Whole-cell Simulations

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## Abstract

Cryo-electron tomography (cryo-ET) has rapidly emerged as a powerful tool to investigate the internal, three-dimensional spatial organization of the cell. In parallel, the GPU-based technology to perform spatially resolved stochastic simulations of whole cells has arisen, allowing the simulation of complex biochemical networks over cell cycle timescales using data taken from - omics, single molecule experiments, and in vitro kinetics. By using real cell geometry derived from cryo-ET data, we have the opportunity to imbue these highly detailed structural data—frozen in time—with realistic biochemical dynamics and investigate how cell structure affects the behavior of the embedded chemical reaction network. Here we present two examples to illustrate the challenges and techniques involved in integrating structural data into stochastic simulations. First, a tomographic reconstruction of *Saccharomyces cerevisiae* is used to construct the geometry of an entire cell through which a simple stochastic model of an inducible genetic switch is studied. Second, a tomogram of the nuclear periphery in a HeLa cell is converted directly to the simulation geometry through which we study the effects of cellular substructure on the stochastic dynamics of gene repression. These simple chemical models allow us to illustrate how to build whole-cell simulations using cryo-ET derived geometry and the challenges involved in such a process.

## **TOC** image

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## Introduction

Over the last three decades, computational biologists have developed the ability to model the structure and function of biological systems at the molecular-and more recently-cellular levels. Key approaches in this pursuit are bioinformatics, molecular visualization, molecular simulation, and most recently, stochastic cell simulations. Computing complements experimentation, transforming static atomic force microscopy maps, structures derived from X-ray crystallography, super-resolution microscopy data, cryo-electron microscopy (cryo-EM) maps, and cryo-electron tomography (cryo-ET) 3-D reconstructions into dynamic systems through simulations which integrate single molecule fluorescence data, -omics, and kinetic data. Increasingly often, computing correctly predicts missing structural information and interactions at both the molecular and cellular levels. The work by Klaus Schulten and his co-workers to create a model of a photosynthetic chromatophore and analyze its overall energy conversion efficiency is perhaps one of the best examples of the power of molecular modeling.<sup>1–5</sup> This undertaking involved the modeling of vesicles measuring hundreds of nanometers, and required many methodological and algorithmic improvements to molecular dynamics flexible fitting (MDFF), the molecular dynamics simulation program NAMD, and the visualization and analysis program VMD.

During its early phase, computational biology was considered a valuable, but limited tool, the limits being mainly due to restrictions in size and timescales. Computational cell biology has now matured such that its descriptions of subcellular systems and whole-cell processes compare favorably with observations for both bacterial and eukaryotic organisms. A revolution in structural biology has taken place with the combination of cryo-EM and cryo-ET with cryo-focused-ion-beam (cryo-FIB) milling, allowing for the collection of three-dimensional, high resolution snapshots of complex molecular landscapes in individual cells.<sup>6–8</sup> To keep pace with this revolution, the development of simulation software that extends to the timescales of a cell cycle (measured in minutes) and the length scales of entire cells (measured in microns) will be required. While current efforts to build an atomic scale model of a minimal cell measuring 0.4  $\mu$ m in diameter<sup>9</sup> are expected to be fruitful within the next five to ten years, the dynamical timescales will continue to be a bottleneck.

Whole-cell simulations performed with the Lattice Microbes (LM)<sup>10,11</sup> stochastic simulation package provide a bridge to describe dynamical processes over several cell cycles and generate snapshots of complex cellular states that result in clear, testable predictions for further experiments. LM is a GPU-based simulation code that was designed from the ground up to be highly computationally efficient<sup>10</sup> in order to reach the length and time scales necessary to study biological systems across entire cells. Reaction processes within the cell

are modeled within the framework of reaction–diffusion master equations (RDME), whose specification requires kinetic parameters obtained from many disparate sources including super-resolution imaging, fluorescence, and biochemical experiments as well as other computational techniques such as molecular dynamics and Brownian dynamics. To date, LM has been used to study the *lac* genetic switch,<sup>8</sup> ribosome biogenesis,<sup>12,13</sup> and the effect of DNA replication on gene expression networks.<sup>13,14</sup> The probabilistic description of ribosome biogenesis in a replicating cell, requiring 251 species and over 1000 reactions, was one of the largest systems modeled with LM. Using a NVIDIA TITAN X graphics card, a full 90-minute cell cycle of an *Escherichia coli* cell could be simulated in approximately 24 hours.<sup>13</sup>

The importance of environmental fluctuations and the discrete nature of chemical reactions on the fate of individual cells are now well known. While the stochastic dynamics of the genetic switches in bacteria have been well studied, the determination of how transcription factors find specific DNA binding sites in eukaryotes is a challenging problem. These studies are complicated by the increased size of the system, the sequestration of the DNA in a spatial compartment separate from the cytoplasm, and the variation in chromatin states.<sup>15,16</sup> Using 3-D chromatin density inferred from structured illumination imaging of a DAPI-stained mammalian nucleus<sup>15</sup> and soft X-ray tomography,<sup>16</sup> Isaacson et al. performed lattice-based simulations of the diffusive search of a hypothetical transcription factor to its DNA binding site. These simulations model the search as the 3-D diffusion of a single particle with an assumed diffusivity of 10  $\mu$ m<sup>2</sup> s<sup>-1</sup> through an external potential,  $U(\mathbf{r}) =$  $C\rho(\mathbf{r})$ , where  $\rho(\mathbf{r})$  is the density of chromatin, and *C* is a free parameter of their model. They revealed that the search times are exponentially distributed and that there exists a proportionality constant C > 0 where the search time is minimized, implying that the chromatin structure helps to direct the transcription factor to its binding site.

The implication is that there can be features of the spatial environment which affect the reaction-diffusion dynamics in unexpected ways. Attempts to construct generic, ideal geometry in whole-cell simulations can overlook these details. For instance, it would be difficult to construct an idealized endoplasmic reticulum due to its convoluted structure. Getting the details wrong means that the search times of mRNA to find ER-bound ribosomes and export times of their products, such as membrane-bound proteins, would be inaccurate. Thus, it is prudent to construct the simulation volume using experimental data when available.

Here, we present two examples illustrating the integration of cryo-ET data into whole-cell simulations. First, using a tomographic reconstruction of a ~1  $\mu$ m<sup>3</sup> volume of an individual *Saccharomyces cerevisiae* cell, we extrapolate the remaining geometry to build the simulation environment. Second, we translated the pre-segmented EM density acquired about the nuclear periphery of a HeLa cell<sup>6</sup> directly to the simulation lattice, leading to non-idealized cellular geometries. In both cases, we investigate how the geometry affects the behavior of idealized genetic switch models. We are able to break down the induction of these genetic switches into several steps: (i) diffusion of an inducer molecule from its transporter in the plasma membrane through the cytoplasm and into the nucleus through a nuclear pore complex (NPC) and its binding to a specific gene triggering transcription; (ii)

diffusion of the mRNA through the nucleus into the cytoplasm where it is translated by one of the ribosomes surrounding the nucleus; and (iii) transport of the resulting permease into the cell membrane. Since there was insufficient information available in the tomogram to reconstruct a realistic ER, only transport of the permease through cytoplasm is considered. In the case of the HeLa cell, since our simulation volume is restricted to the nuclear periphery, we study the local dynamics of a repressor protein and its mRNA in the nucleus and cytoplasm (ii). The simple form of these reaction networks allows us to demonstrate the challenges and possible simplifications that can be made in modeling chemical reactions in eukaryotic cells. The results should be viewed as a basis for introducing further complexity into the dynamics as more structural details become available from the analysis of the cryoelectron tomography data.

## Methods

#### Cryo-electron tomography

Haploid *Saccharomyces cerevisiae* cells (W303a) were cultured in YPD (20 g/L peptone, 10 g/L yeast extract, 20 g/L glucose) at 30 °C to a density of 10<sup>7</sup> cells/ml. 7 µl of this culture were deposited onto glow-discharged holey carbon grids (QUANTIFOIL R 2/1 200 mesh, copper; Electron Microscopy Sciences), blotted and rapidly vitrified in a liquid ethane and propane mixture (50:50) using a custom-built plunger (Max Planck Institute of Biochemistry, Germany). The lamellas (250 to 300 nm thickness) containing several sliced yeast cells were prepared using cryo-FIB milling as previously described.<sup>6</sup> Cryo-electron tomography was obtained using a Titan Krios transmission electron microscope (FEI) equipped with a Quantum energy filter (Gatan) and a K2 Summit direct detection device (Gatan). Imaging was performed at 300 kV under low-dose conditions with 5.31 Å sampling. Tilt series ( $\pm$ 62°) for tomography were collected around a single axis with a 2° sampling increment using SerialEM software<sup>17</sup> (~100 e/Å<sup>2</sup> cumulative dose). Tomographic reconstructions were calculated using the IMOD tomography package.<sup>18</sup>

Subtomograms containing ribosomes are picked using EMAN2<sup>19</sup> and subsequently averaged, classified, and placed in their location in the original tomogram using Dynamo.<sup>20</sup> In order to segment individual organelles, the tomogram data was filtered using nonlinear anisotropic diffusion using the IMOD tomography package.<sup>18</sup> The membranes (cell wall, plasma membrane, nuclear envelope, mitochondrial and ER membranes) were automatically segmented using TomoSegMemTV.<sup>21</sup> Segmentation of tomography volumes for the representation of various organelles and nuclear density were performed with Amira software (FEI Visualization Sciences Group).

The HeLa tomography data were previously reported.<sup>6</sup>

#### Simulations

Spatially resolved stochastic chemical reaction trajectories were simulated using Lattice Microbes v2.3.0.<sup>10,22,23</sup> Lattice Microbes (LM) efficiently samples particle number trajectories from the solution to the underlying RDME describing the chemical system embedded in a lattice-based representation of the system geometry. The RDME is

$$\frac{\mathrm{d}P(\boldsymbol{x},t)}{\mathrm{d}t} = \sum_{v}^{V} \sum_{r}^{R} [-a_{r}(\boldsymbol{x}_{v})P(\boldsymbol{x}_{v},t) + a_{r}(\boldsymbol{x}_{v} - \boldsymbol{S}_{r})P(\boldsymbol{x}_{v} - \boldsymbol{S}_{r},t)] \\
+ \sum_{v}^{V} \sum_{\xi}^{\hat{i},\hat{j},\hat{k}} \sum_{\alpha}^{N} [-d_{v}^{\alpha}x_{v}^{\alpha}P(\boldsymbol{x},t) + d_{v+\xi}^{\alpha}(x_{v+\xi}^{\alpha}+1)P(\boldsymbol{x}+\mathbf{1}_{v+\xi}^{\alpha}-\mathbf{1}_{v}^{\alpha},t)], \quad (1)$$

where  $P(\mathbf{x}, t)$  is the probability distribution to find a configuration  $\mathbf{x}$  at time t, and the configuration vector  $\mathbf{x}$  contains the number of species present of each type at each subvolume. The first term in Equation 1 describes the flow of probability between different copy number states at each lattice site. The reaction propensities  $a_t(\mathbf{x}, \mathbf{v})$  give the transition probabilities due to reaction r firing at site  $\mathbf{v}$ . The r row of the stoichiometry matrix  $\mathbf{S}$  is the change in species counts when reaction r occurs. The second term describes the flow of probability due to diffusion between neighboring lattice sites, indexed by  $\boldsymbol{\xi}$ . The diffusive propensity  $d_v^{\alpha}$  for a particle of species  $\mathbf{a}$  to leave subvolume  $\mathbf{v}$  is computed from the diffusion constant  $D_v^{\alpha}$  and lattice spacing  $\lambda$  as  $d_v^{\alpha} = D_v^{\alpha}/\lambda^2$ . The notation  $\mathbf{1}_v^{\alpha}$  represents a single molecule of species  $\mathbf{a}$  in volume  $\mathbf{v}$ , i.e.  $(\mathbf{1}_v^{\alpha})_{\mu}^{\beta} = \delta_{\alpha\beta} \delta_{\mu v}$ . All simulations were performed on a local cluster consisting of three Cirrascale GB5600 Multi-GPU nodes, two equipped with eight NVIDIA GeForce GTX TITAN X GPUs, and one equipped with four NVIDIA Tesla K80 GPUs. The multi-GPU capabilities of LM were used to share the simulation workload for the *S. cerevisiae* simulation over eight GPUs, and for the HeLa simulation over four GPUs.

Simulation design, visualization, and analysis of simulation results were performed using Python 3.5.3 in the Jupyter environment<sup>24</sup> with the SciPy Stack.<sup>25</sup> EM data was injected into the Python workflow by converting density files from the MRC format to NumPy<sup>26</sup> native data files using EMAN2,<sup>19</sup> which currently does not support Python 3.

Visual Molecular Dynamics (VMD)<sup>27</sup> was used for interactive visualization of experimental tomography volumes and LM simulation trajectories, enabling several different data modalities to be inspected and superimposed for comparison. The VMD MRC plugin was extended to support several IMOD-specific variants of the MRC file format, allowing it to read the experimental tomogram volumes produced as described above. The volume visualization and ray tracing capabilities of VMD were enhanced to permit visualization of volumes containing more than 2 billion voxels. The large size and geometric complexity of the graphical representations for the experimental tomograms and the LM simulation trajectories presented a significant performance challenge for interactive display in VMD using conventional OpenGL rasterization. The GPU-accelerated interactive ray tracing capabilities of VMD were used to overcome the performance challenge posed by complex scenes.<sup>4</sup> For the complex structures studied herein, ray tracing acceleration algorithms avoid consideration of occluded geometry, and the use of progressive refinement ray tracing permits very high interactivity, even for visualizations using rendering techniques such as

ambient occlusion lighting or depth-of-field focal blur that require large numbers of stochastic lighting samples to be computed.<sup>28</sup>

## **Results and Discussion**

#### Inferring the architecture of a yeast cell from cryo-ET

Using cryo-FIB with cryo-ET, we have acquired the 3-D structure of a  $2.04 \times 1.91 \times 0.242 \ \mu m^3$  volume of an individual *S. cerevisiae* cell with a sampling rate (pixel size) of 0.53 nm (Figure 1). The structure clearly shows a portion of the nuclear envelope with 12 nuclear pores, 750 ribosomes in the cytoplasm, a section of the plasma membrane, and portions of the ER and a mitochondrion. Using the data available to us through this tomogram, we have constructed the internal geometry of an entire cell, filling in any missing data using measurements published in the literature as well as numerical optimization.

The simulation geometry consists of ten distinct spatial regions: extracellular, cell wall, plasma membrane, cytoplasm, vacuole, mitochondria, ribosomes, nuclear pores, nuclear envelope, and nucleoplasm (Figure 2). Each region can have its own set of species-specific diffusion constants and set of reactions allowing for spatially heterogeneous reaction–diffusion behavior. The starting point to reconstruct a realistic yeast cell from the tomography data is the 3-D binary mask resulting from the segmentation of the nuclear envelope and plasma membrane surfaces (Figure 1a), which we resample to the dimensions of the simulation lattice. A 3–D representation of this mask is shown in Figure 1b–c. The original tomogram data was resampled from a sampling rate of 0.53 nm to a simulation lattice spacing of 28.7 nm—a 54-fold reduction.

To extrapolate the geometry of the nucleus and cell volume outside of the tomographic volume, we fit ellipsoids to the mask coordinates using local optimization. To ensure that the result is both biologically reasonable and faithfully reflects the data, we augment the squared error with terms penalizing deviations from an expected volume and aspect ratio.<sup>29,30</sup> These penalizing terms are small compared to the squared error, ensuring that only perturbations to the parameters which do not affect the fit to the mask coordinates significantly are allowed.

To construct the nucleus, we started with initial ellipsoid parameters computed from the mask coordinates: the center from the mean of the mask coordinates and the ellipsoid axes from the maximum distance between two mask coordinates. Assuming that the volume of the cell in the tomogram is ~40  $\mu$ m<sup>3</sup><sup>29</sup> and that the volume percentage of the nucleus is 7%,<sup>30</sup> we use an expected volume of 2.8  $\mu$ m<sup>3</sup> and an aspect ratio of 1.0 in our fitness function. This results in a nucleus of volume 3.17  $\mu$ m<sup>3</sup> and aspect ratio 1.2. For the cell volume, we used an expected volume of 33.6  $\mu$ m<sup>3</sup>, which is assuming that the cell wall occupies 15.9% of the cell volume,<sup>30</sup> and an expected aspect ratio of 1.5. Since only a small portion of the plasma membrane is present in the tomogram, we used the center of the nucleus as the initial position and the radius of a sphere of volume 33.6  $\mu$ m<sup>3</sup> as the initial ellipsoid axes. The resulting ellipsoid spanned a volume of 33.9  $\mu$ m<sup>3</sup> and had an aspect ratio of 1.50. Figure 2a compares the cryo-ET-derived masks to the extrapolated geometry.

A natural way to work with the RDME site-type lattice is in terms of set operations. We define the set of lattice sites to be

$$= \left\{ \boldsymbol{n} \in \mathbb{Z}^3 : 0 \le n_x < N_x \text{ and } 0 \le n_y < N_y \text{ and } 0 \le n_z < N_z \right\}.$$
(2)

Then an ellipsoid embedded in the lattice is the set,

Ellipsoid= 
$$\left\{ \boldsymbol{n} \in : \left| \mathbf{A} \cdot \mathbf{R} \cdot (\boldsymbol{n} - \boldsymbol{n}_0) \right|^2 < 1 \right\}$$
, (3)

where  $\mathbf{A} = \text{diag}(1/a, 1/b, 1/c)$ , a matrix with the inverse of the ellipsoidal semi-axes on the diagonal,  $\mathbf{R} = \mathbf{R}_{\hat{z}}(\alpha) \cdot \mathbf{R}_{\hat{x}}(\beta) \cdot \mathbf{R}_{\hat{z}}(\gamma)$  is an Euler rotation matrix, and  $\mathbf{n}_0$  is the centroid of the ellipse. By representing the site type lattice in this way, we can easily describe the construction of more complicated structures in the language of set operations and binary morphology.

These ellipsoids are used to form the nucleoplasm and cytoplasm, as well as the nuclear envelope, plasma membrane, and cell wall. The membrane regions are constructed as,

$$Membrane = (Ellipsoid \oplus S_{mem}) \setminus Ellipsoid$$
(4)

where  $\texttt{Ellipsoid} \oplus S_{mem}$  denotes the dilation of Ellipsoid with a structuring element  $S_{\rm mem}$ . The resulting mask, Membrane is a shell one subvolume thick surrounding Membrane. The structuring element,  $S_{\text{mem}}$ , is a cube with edge length 3 with all elements set to 1, which matches all 26 neighbors. This choice ensures that all subvolumes within Membrane have at least one neighbor along the principal axes. This is critical for membranebound particles since diffusion in Lattice Microbes is modeled as transitions between the 6 nearest neighbor subvolumes. Otherwise, there would be regions of the membrane compartment which would be topologically separated to diffusing particles. The resulting membranes are 28.7 nm thick which is reasonable for the nuclear envelope (typically ~30 nm thick in S. cerevisiae<sup>31</sup>). However, this is considerably larger than the thickness of the plasma membrane (9.2 nm<sup>32</sup>). Lattice-based simulations such as this limit the smallest features to the lattice spacing, however we must choose a coarser lattice resolution in order to accelerate the simulation. Fortunately, the plasma membrane thickness does not affect the outcome of the simulation since the chemical species which pass through the membrane are represented by separate external and internal species types, allowing for particles to be on different sides of the membrane within a single lattice site. The cell wall is formed from an ellipsoid with the same shape, orientation, and location as the cell volume ellipsoid. The axes are scaled such that the resulting ellipsoid has the expected volume of the cell ( $40 \,\mu m^3$ ). From this ellipsoid region, we subtract the union of the cell volume and plasma membrane regions to arrive at the cell wall. The resulting shell is 129 nm thick, which compares well with measurements performed with single-molecule AFM.<sup>33</sup>

By observing the number of pores in the nuclear envelope (12) and its surface area (0.91  $\mu$ m<sup>2</sup>) from the tomogram, we computed the expected number of pores on the full nucleus to be 139. This quantity is consistent with the value of 119 ± 39 pores per nucleus reported in the literature<sup>34</sup> for haploid yeast cells grown in similar conditions. Since the pores visible in the tomogram do not include the full nuclear pore complex, we used a pore diameter of 40 nm,<sup>35</sup> instead of measuring the diameter from the segmentation. The pores are initially represented as the union of 139 cylinders i.e.,

PoreCylinders=
$$\bigcup_{i=1}^{139} \left\{ n \in : \boldsymbol{m} = \mathbf{R}_i \cdot (\boldsymbol{n} - \boldsymbol{n}_{0,i}) \text{ and } - \frac{l}{2} < m \cdot \hat{z} < \frac{l}{2} \text{ and } |\boldsymbol{m} - m \cdot \hat{z}\hat{z}|^2 < r^2 \right\}.$$

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where r is the nuclear pore radius,  $\Lambda$  is one half the nuclear radius, and the transformation parameters  $\mathbf{R}_i$  and  $\mathbf{n}_{0,i}$  are chosen as follows. Each cylinder is placed at the center of the nucleus, rotated to a random polar and azimuthal angle, and translated to place the centroid of the cylinder in the nuclear envelope. The random position is checked against all previous placements to ensure that the new pore does not merge with the remaining pores. The nuclear pore lattice is then the intersection, Membrane<sub>nuc</sub>  $\cap$  PoreCylinders, and the the nuclear envelope is the difference, Membrane<sub>nuc</sub>  $\setminus$  PoreCylinders.

Using volume percentages measured from cryo-FIB-milled scanning electron microscopy data of entire budding yeast cells,<sup>30</sup> we add ellipsoids representing the mitochondria and vacuole. The ER, which can occupy 2.2% of the cell volume,<sup>30</sup> is not included. The presence of the ER would affect diffusion throughout the cell due to its folded morphology, however there is not enough information from the tomogram to infer the geometry outside of the imaged volume. Finally, 180,000 ribosome sites<sup>36</sup> are placed uniformly throughout the cytoplasm. The resulting geometry requires a lattice size of  $192 \times 192 \times 192$ , which represents a cube of edge length 5.5 µm.

To explore the effects of the cell geometry on a behavior of a biochemical network, we simulated a model of a simple inducible genetic switch (introduced in Table 1) in the extrapolated yeast lattice. A concentration of 4  $\mu$ M of inducer is placed in the extracellular space, where it may enter the cell via passive diffusion across the plasma membrane. Inducer molecules diffuse through the cytoplasm into the nucleus through a nuclear pore, where it may interact with a gene species located in a single subvolume of the nucleus, activating the transcription of mRNA coding for a transporter protein. The mRNA diffuses out of the nucleus through the nuclear pores into the cytoplasm. Since dwell times of exported molecules in the pore are reported to be on the order of milliseconds,<sup>37</sup> we approximated the mRNA export process as simple diffusion out of the nucleus. The actual process is certainly more complicated than this,<sup>37,38</sup> however it is an appropriate approximation for the level of detail in this model. After leaving the nucleus, the mRNA binds to a ribosome in the cytoplasm to begin translation The translated protein, being a membrane-bound transporter, normally would be translated by ribosomes associated with the ER and exported to the

plasma membrane through the Golgi apparatus. However without a large volume of tomographic structures of these organelles, it is difficult to incorporate their geometry in our model realistically. Furthermore, the development of a plausible RDME-based protein targeting model is beyond the scope of this work. Instead, we allow the transporter protein to diffuse through the cytoplasm and into the plasma membrane. Once installed in the membrane, the protein transports more inducer into the cell through active transport.

The transcription and translation rates were estimated from steady-state mRNA and protein abundance, protein lifetime,<sup>36</sup> and mRNA lifetime<sup>39</sup> using the gene expression model

 $D \xrightarrow{k_{ts}} D+m$  (6a)

$$m \xrightarrow{k_{tl}} P + m$$
 (6b)

$$m \xrightarrow{k_{dm}} \emptyset$$
 (6c)

$$P \xrightarrow{k_{dp}} \emptyset$$
 (6d)

where the mean number of mRNA, m, is given by the ratio of transcription to mRNA decay rates,

$$\overline{n}_m = \frac{k_{\rm ts}}{k_{\rm dm}}$$
 (7)

and the mean number of protein, P, is given by the ratio of the total translation rate  $\overline{n}_m k_{tl}$  to the protein decay rate,

$$\overline{n}_{\rm p} = \frac{k_{\rm tl} \overline{n}_{\rm m}}{k_{\rm dp}} = \frac{k_{\rm ts} k_{\rm tl}}{k_{\rm dm} k_{\rm dp}}.$$
(8)

To represent this hypothetical transporter, we chose values describing the high-affinity glucose transporter HXT6. These parameters result in a steady state mRNA abundance of 7.86 and protein abundance of 42,600 per cell. In the interest of computational efficiency, the passive and active transport parameters as well as the rate of gene activation were adapted from a previous model of the *lac* genetic switch in *E. coli*.<sup>8</sup> Since competitive binding to ribosomes between different mRNA species can have a significant effect on the copy number statistics,<sup>13</sup> we added a second series of transcription, translation, and mRNA degradation reactions. The rates were chosen to yield 12,200 mRNA<sup>36</sup> and  $5 \times 10^7$  protein<sup>40</sup>

at steady state. Through we do not track these "background" proteins in our simulation, their translation rate impacts the simulation through their effect on the average ribosome occupancy.

We ensured the proper localization of molecules to their respective compartments by choosing the transition rates between the ten different regions explicitly. In Lattice Microbes, the diffusion rate between two subvolumes is specified by the type of chemical species, the type of the site the particle currently occupies, and the type of the site that the particle may diffuse to. This allows for the specification of one-way transitions between compartments by setting the reverse diffusion rate to zero. We will use this technique extensively in both models presented in this work. The gene species is fixed in place in the nucleus by setting its diffusion constant to zero. mRNA can diffuse freely in the nucleoplasm, cytoplasm, nuclear pores, and ribosome regions with a diffusion rate of 0.5  $\mu$ m<sup>2</sup> s<sup>-1</sup>. To prevent mRNA from reentering the nucleus, we define the site-dependent diffusion rate for mRNA from cytoplasm to nuclear pores to be zero. Transporter proteins diffuse through the cytoplasm in three dimensions  $(1 \ \mu m^2 \ s^{-1})$  and in the plasma membrane in two dimensions. (0.01  $\mu$ m<sup>2</sup> s<sup>-1</sup>). To allow for the proper progression of transporter diffusion from the ribosome, through the cytoplasm, to the membrane, we set all transitions into the nuclear pore and ribosome regions to zero. Since transporters are created at ribosome site types, they are allowed to diffuse in these regions. However their reentry is forbidden, in order to allow for the ribosome sites to act as crowding agents in the cytoplasm. Finally, the transporters can diffuse from the cytoplasm to the membrane, however the reverse rate is set to zero to prevent their detachment.

The inducer is represented by two separate species types: internal and external. External inducer can diffuse freely through the extracellular, cell wall, and plasma membrane regions with a diffusion constant of  $2 \mu m^2 s^{-1}$ . This rate is significantly lower than what would be expected for a small molecule (100–1000  $\mu$ m<sup>2</sup> s<sup>-1</sup>), however in this model it is necessary to slow the diffusion of inducer since the maximum acceptable time step in an RDME simulation scales with 1/D. It has been shown previously that this approximation has a limited effect on the outcome of the simulation,<sup>8</sup> so long as the correct ordering of diffusion constants,  $D_{mRNA} < D_{prot}$ .  $< D_{ind.}$ , is maintained. However, validity of the approximation notwithstanding, it is not necessary to treat a species found in such a high concentration (2  $\mu$ M) using a stochastic representation. The solution to this problem is to use multiple coupled simulation methods each for different concentration and diffusivity regimes, e.g. a deterministic, well-mixed representation using ODEs for small molecules in large concentrations or a deterministic, spatially resolved representation using PDEs for slowly diffusing molecules in high concentrations. Work on Lattice Microbes is underway to enable this ability. The external inducer species is transformed to internal through passive diffusion, represented as the first order reactions

$$I_{\text{in}} \stackrel{k_{\text{txDif}}}{\underset{k_{\text{txDif}}}{\rightleftharpoons}} I_{\text{out}}$$
(9)

which occurs only in the plasma membrane site type, and active transport, represented by the Michaelis-Menten scheme

$$T+I_{out} \underset{k_{txOff}}{\overset{k_{txOn}}{\rightleftharpoons}} T: I \xrightarrow{k_{tx}} T+I_{in}.$$
(10)

The internal species is free to diffuse through the plasma membrane, cytoplasm, and nucleoplasm regions. By dividing the inducer into internal and external species, we are able to model transport into the cell simply by using the plasma membrane compartment as a staging area.

Using the multi-GPU capabilities of Lattice Microbes,<sup>10</sup> we complete a 60-minute simulation in 28 hours using eight NVIDIA TITAN X GPUs, taking 67-µs time steps. A summary of the simulation parameters and diffusion rates is provided in Table 2. Representative particle abundance time series are presented in Figure 3a–c. The concentration of inducer in the nucleus rises slowly, leading to the gene switching on at 4.2 minutes. The first transporter protein reaches the membrane 9.3 minutes after the gene is activated (Figure 3d). At about 21.7 minutes, the nuclear inducer concentration dynamics becomes dominated by active transport with the appearance of 1900 transporter proteins in the membrane. Due to the finite size of the simulation volume and closed boundary conditions, the extracellular inducer is depleted to 1% of its original concentration after 46.7 minutes of simulated time.

#### Exploring the nuclear periphery in a HeLa cell

Starting from an EM map of the periphery of a HeLa cell nucleus obtained through cryo-ET/ cryo-FIB,<sup>6</sup> we constructed a discrete environment to explore a simple gene expression system. The density has been pre-segmented into six regions corresponding to actin filaments, microtubules, ER, large and small ribosomal subunits, and the nuclear pore complexes (Figure 4). Instead of using measurements derived from the EM density, the problem one is now posed with is how to directly map a 3D density represented on a grid sampled at 0.35 nm to a coarse-grained lattice which is faithful to the dimensions of the original tomogram. Solving this problem entails choosing a suitable threshold to discriminate cellular substructures from the background density, and determining an optimal lattice spacing for the RDME simulations.

To minimize the computational time necessary to perform the simulations, the lattice spacing must be large as possible while accurately reproducing the cellular substructure. In order to resolve the actin filaments we have chosen a lattice spacing of 8 nm, larger than their actual diameter (~6 nm), to ensure that the voxelized actin filaments remain contiguous while not excessively overestimating their impact on the excluded volume. To begin constructing the system geometry, the EM map was resampled to the dimensions of the RDME lattice using trilinear interpolation. A unique threshold is determined for each of the six segmented maps, which is used to compute a binary lattice such that lattice elements for which their density is below the threshold are interpreted as background. These thresholds were chosen such that the dimensions of the identified cellular substructures are correctly

recovered. Figure 4 shows a comparison between the segmented tomogram and the derived site type lattice.

Our simulation domain consists of four active regions, cytoplasm, nuclear pore, nucleoplasm, and ribosomal small subunit. The nuclear pore region allows the transport of particles between the cytoplasm and nucleus to be monitored, and the small subunit region contains the reaction sites for translation. The obstructions include the NPC, actin, microtubules, large subunit, and ER, as well as the nuclear envelope. Due to the orientation of the sample, the nuclear envelope was not resolved in the tomogram. To include this region, we will approximate its position and shape from the context of the tomogram.

To begin the construction of the RDME geometry, first two auxiliary binary lattices are constructed to aid in the construction of the simulation volume: the convex hull of all of the cryo-ET derived site type lattices,

$$Hull = convex\_hull (NPC \cup Actin \cup Microtubules \cup LSU \cup SSU \cup ER), \quad (11)$$

and the neighborhood around the nuclear pores, NpcDomain, which is constructed by thresholding a Gaussian-filtered version of the NPC density. The nuclear envelope is constructed starting with a spherical shell,

EnvShell = {
$$n \in :r_{n} - r_{ne} < |n - x_{n}| \le r_{n}$$
}, (12)

where  $r_n$  and  $r_{ne}$  are the radius of the nucleus and thickness of the nuclear envelope respectively, and  $x_n$  is the position of the center of the nucleus, necessarily outside of the lattice space. The nuclear envelope region is then,

Envelope = (EnvSphere (NPC • 
$$S_{npc}$$
))  $\cap$  (Hull  $\cup$  NpcDomain) (13)

where • denotes the morphological closing operation and  $S_{npc}$  is a structuring element sufficient to fill the interior of the pores without joining adjacent NPCs. This allows us to construct the obstruction lattice as the union,

 $Obstructions = Envelope \cup NPC \cup Actin \cup Microtubules \cup LSU \cup ER.$  (14)

The nucleoplasm is constructed starting with the sphere,

NucSphere = 
$$\{ \boldsymbol{n} \in : |\boldsymbol{n} - \boldsymbol{x}_{n}| \leq r_{n} - r_{ne} \}, \quad (15)$$

then cropping to fit the simulation volume and subtracting the NPCs,

$$Nucleoplasm = (NucSphere \cap (Hull \cup NpcDomain)) \setminus (NPC \bullet S_{npc})$$
(16)

The interior of the nuclear pores is simply,

PoreInterior = (NPC • 
$$S_{npc}$$
)\NPC. (17)

Finally, the cytoplasm is the convex hull excluding all other regions,

 $Cytoplasm = Hull \setminus (Nucleoplasm \cap PoreInterior \cap Obstructions).$ (18)

The resulting simulation volume (Figure 5) is  $1.554 \times 0.296 \times 1.496 \ \mu m^3$  ( $194 \times 37 \times 187$  lattice sites).

To explore this lattice geometry, we will use a simple model of gene expression (Table 3). mRNA diffuses from gene sites in the nucleoplasm, through the nuclear pores, to find ribosome species positioned in the small subunit site type. The mRNA and ribosome species react to form a translating ribosome, which then decays yielding the original mRNA and ribosome species as well as a transcription factor. Finally, the protein is able to diffuse back through the nuclear pores and repress its originating gene. The same diffusion constants were used for mRNA (0.5  $\mu$ m<sup>2</sup> s<sup>-1</sup>) and protein (1.0  $\mu$ m<sup>2</sup> s<sup>-1</sup>) in the HeLa model as in yeast, and the same deterministic rate constants were used as well. The numerical difference between the values in Table 1 and Table 3 arises from a factor of  $(\lambda_{veast}/\lambda_{HeLa})^3$  converting between lattice site volumes. We would not expect either the reaction rates or the diffusion constants to be identical between the two organisms, however going to slower, more realistic values will require tens of hours of simulated time to observe the same repression behavior. Since only the broad effects of the cell geometry on the reaction model are of interest, this is an acceptable approximation. We use a similar scheme as the *S. cerevisiae* model to keep particles in their proper compartments. The gene has a diffusion rate of zero in order to fix it in place inside the nucleus. The protein and mRNA species are forbidden from entering the obstruction regions. mRNA is prevented from reentering the nucleus by setting its transition from the cytoplasm into the nuclear pore to zero, however protein is not restricted from the nucleus. A summary of the simulation parameters and diffusion rates is provided in Table 2 in comparison to the S. cerevisiae model.

As shown in Figure 6a the dynamics begins with the formation of mRNA from a gene located in the nucleoplasm. Within 0.85 seconds, it escapes through the nuclear pore into the cytoplasm and diffuses to one of the ribosome sites where it is translated into a repressor protein. The repressor protein appears on average 0.60 seconds after formation of the translating complex. Finally the newly translated protein diffuses back through the nuclear pore and represses the originating gene, taking an average time of 75.6 seconds measured from the birth of the mRNA. Since the mean translation time is 0.498 seconds and the gene/ repressor and ribosome/mRNA binding rates are fast, the first passage time (FPT)

distribution of gene repression events is dominated by the return of protein into the nucleus —a consequence of the geometry of the simulation domain. There are many ribosome sites near the nuclear pores, allowing a newly exported mRNA to immediately begin translation, however a newly translated protein has no preferred direction to diffuse, so it will typically diffuse far from the pore before returning.

To study how obstructions such as the nuclear membrane and microtubules affect the time for a particle to diffuse between compartments and reaction sites, a second set of simulations were performed where all reactions were instantaneous, using both the previously defined geometry (Figure 5) and a version where the obstacles were removed. By requiring that the ribosome make a single protein, only a single particle is present at any time in the simulation. This allows the FPTs to be measured without ambiguity (Figure 6b–e).

We find that the transition times between gene to nuclear pore, nuclear pore to ribosome, and ribosome to nuclear pore are greater in the presence of obstacles. The transition from the gene site to the nuclear pore is 9.7 times greater, simply due to the fact that the particle must find one of the four nuclear pores to exit. The transition from nuclear pore to ribosome is only 2.2 times greater with obstacles. Here, the structures impeding the search are the large subunits, microtubules, actin filaments, and ER. With little opportunity to become trapped away from the ribosomes, it is not surprising that the difference in transition time is not as profound. The transition from the ribosome to a pore is 20.5 times greater with obstacles, which arises for the same reason as the gene to pore transition. However the mean time between encounters with the nuclear envelope or nuclear pores must be smaller for a particle in the nucleus versus a particle in the cytoplasm due to the fact that the volume of the cytoplasm is 3.5 times that of the nucleus. Interestingly, the time for the repressor to find the gene site after entering the nucleus is 1.18 times faster when obstacles are present. This is because the repressor is less likely to escape the nucleoplasm with the nuclear envelope intact.

## Conclusions

Acquiring the capacity to simulate stochastic biochemistry in whole cells at a spatially resolved level over cell-cycle-long timescales, is a crucial step in the development of the field of computational biology. Through the availability of massively parallel computational hardware, such as GPUs, and the development of methods to measure the 3-D structure of cells in their native environment at high resolution, such as cryo-ET, it is now possible to build integrative computational models of whole cells. We have presented two vignettes of the integration of structural data into RDME models of gene expression. Though limited in realism, they provide an illustration of the techniques necessary for this sort of data integration and hint at the challenges faced in undertaking such a task.

Using the 3-D structure of a fraction of a yeast cell, we have shown a way to infer the remaining cell geometry from the tomogram supplemented with data from the literature, and simulated a multi-compartment model of an inducible genetic switch in this environment. From a previously published cryo-ET structure of the HeLa nuclear periphery, we have shown how to use the EM map data directly to construct a spatial model and simulate a gene

repression model, which was used to study the effect of the cellular substructure on the molecular search times. Models built using these techniques, compiling experimental data from many disparate sources into a single cohesive whole, will form a computational framework capable of making testable predictions of the effects of perturbations to both the underlying biochemical network and the architecture of the cell.

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#### Figure 1.

(a) Tomographic slice of a *S. cerevisiae* cell (16 nm thickness). The nucleus (1), separated by the nuclear envelope (2) from the cytoplasm (3), occupies the majority of the tomogram. Ribosomes are visible in the cytoplasm (3) as dark spots (arrow). A portion of the cell wall (4) appears in the upper right corner. Nuclear pores (5) are present in the nuclear envelope. A mitochondrion (6) is present on the right edge of the tomogram, as well as a portion of the ER (7). (b, c) Annotated view of the tomographic data (240 nm thickness). Nuclear envelope, yellow; ribosome, cyan; cell wall, magenta; mitochondrion, green; ER, orange.

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#### Figure 2.

(a) Construction of the simulation geometry of a *S. cerevisiae* cell derived from cryo-ET data and other literature sources. Regions marked "CET" are the segmentation surfaces from the tomogram, regions marked "fit" are derived from fitting ellipsoids to the cryo-ET segmentation data, and the regions marked "ext" are simulation compartments which were not derived from tomography. The nuclear envelope from the tomogram volume (cyan) is used to fit an ellipsoid (blue). A small segment of plasma membrane identified in the tomogram (magenta) is used to fit an ellipsoid (orange) along with constraints on its centroid and volume. Ribosomes (yellow) are distributed uniformly throughout the cytoplasm and act as molecular crowders to cytoplasmic protein and inducer. The mitochondria (green) and ER (gray) surfaces are included from the tomogram for context, however are not incorporated into the simulation. (b) Another view of the model yeast cell showing the placement of mitochondria (green), the vacuole (pink), the 129 nm thick cell wall (gold), and nuclear pores (silver).



## Figure 3.

Species abundance time series for (a) inducer, (b) transporter protein, and (c) transporter mRNA for a single replicate. The vertical dotted line denotes the time at which the gene is activated. The extracellular inducer concentration decreases slowly due to passive transport into the cell until 21.7 minutes, after which transporter proteins begin to appear in the membrane and active transport of inducer begins. The distribution of transporter arrival times at the membrane (d) shows that the first membrane transporters appear at 10 minutes (5 minutes after gene induction).



#### Figure 4.

Adaptation of a segmented cryo-electron tomogram of the nuclear periphery of a HeLa cell<sup>6</sup> to RDME simulations using an 8-nm lattice spacing. The upper panel shows both the processed tomography data (upper left) and the discretized RDME lattice (lower right). The inset shows detail of the vicinity of a nuclear pore for both the original data (top), and the RDME lattice (bottom).



#### Figure 5.

RDME simulation volume for the HeLa nucleus periphery. The nucleoplasm and cytoplasm are shown in light blue and tan respectively. The cytoplasm is created from the convex hull of the cryo-ET derived site type lattices, where as the nucleoplasm is created from the neighborhood surrounding the nuclear pore complexes. The total accessible simulation volume is  $0.329 \ \mu m^3$ . The nucleoplasm and cytoplasm are connected by channels through the nuclear pore complexes.

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#### Figure 6.

Abundance and escape dynamics for a simple genetic switch simulated in the intracellular environment of a HeLa cell. (a) Mean particle abundance (solid line) and standard deviation (shaded area) were computed over 37 simulation replicates. The time for a mRNA to diffuse out of the nucleus and find a ribosome is two orders of magnitude larger than the time for a newly translated protein to return and bind to its originating gene. The mRNA abundance in the cytoplasm is the sum of free mRNA and mRNA bound to ribosomes. (b–e) First passage time distributions of diffusion between compartments and reaction sites for the complete HeLa cell geometry (blue) and with all obstructions removed (green). These simulations were performed with instantaneous reaction rates in order to measure the time for diffusion alone over 222 simulation replicates. mRNA diffuses from the gene site into the cytoplasm (b), from the cytoplasm to the ribosome (c), the protein diffuses back into the nucleus (d), and the protein binds to the gene (e).

#### Table 1

Reactions and rate parameters used in the S. cerevisiae gene expression model.

Description	Reaction	Stochastic rate [s <sup>-1</sup> ]	Defined regions
Inducer/TF binding	$\mathrm{I_{in}+D_{off}} \xrightarrow{k_{\mathrm{gnOn}}} \mathrm{D_{on}}$	1.599	Nucleoplasm
Transcription	$D_{on} \xrightarrow{k_{ts}} D_{on} + m$	$6.202 \times 10^{-3}$	Nucleoplasm
SSU/mRNA association	$\mathbf{R}{+}\mathbf{m}\xrightarrow{k_{\mathrm{tIInit}}}\mathbf{R}{:}\mathbf{m}$	$7.043\times10^3$	Ribosome
Translation elongation	$\mathbf{R:m} \xrightarrow{k_{\mathrm{tlTerm}}} \mathbf{R+m+T}$	1.393 Ribosome	
mRNA degradation	$\mathbf{m} \xrightarrow{k_{\mathbf{mDcy}}} \emptyset$	$7.889\times 10^{-4}$	Nucleoplasm, Ribosome, NPC, Cytoplasm
mRNA degradation	$\mathbf{R}{:}\mathbf{m} \xrightarrow{k_{\mathbf{mDcy}}} \mathbf{R}$	$7.889 \times 10^{-4}$	Ribosome
Transcription (other)	$\emptyset \xrightarrow{k_{\mathrm{ts}'}} \mathbf{m}'$	$5.895\times10^{-5}$	Nucleoplasm
SSU/mRNA association (other)	$\mathbf{R+m}^{'} \xrightarrow{k_{\mathrm{tlInit}}} \mathbf{R:m}^{'}$	$7.043\times10^3$	Ribosome
Translation elongation (other)	$\mathbf{R:m}^{'} \xrightarrow{k_{\mathrm{tlTerm}^{'}}} \mathbf{R+m}^{'}$	1.101	Ribosome
mRNA degradation (other)	$\mathbf{m'} \xrightarrow{k_{\mathbf{mDcy'}}} \emptyset$	$5.776  imes 10^{-4}$	Nucleoplasm, Ribosome, NPC, Cytoplasm
mRNA degradation (other)	$\mathbf{R:m'} \xrightarrow{k_{\mathbf{mDcy'}}} \mathbf{R}$	$5.776 \times 10^{-4}$	Ribosome
Passive diffusional transport	$\mathbf{I_{in}} \xrightarrow{k_{\mathrm{txDif}}} \mathbf{I_{out}}$	$2.33  imes 10^{-3}$	Membrane
Passive diffusional transport	$\mathbf{I}_{\mathrm{out}} \xrightarrow{k_{\mathrm{txDif}}} \mathbf{I}_{\mathrm{in}}$	$2.33\times10^{-3}$	Membrane
Transporter/inducer association	$\mathbf{T}{+}\mathbf{I}_{\text{out}} \xrightarrow{k_{\text{txOn}}} \mathbf{T}{:}\mathbf{I}$	2.134	Membrane
Active inducer transport	$\mathrm{T:}\mathrm{I} \xrightarrow{k_{\mathrm{tx}}} \mathrm{T+}\mathrm{I_{\mathrm{in}}}$	12.000	Membrane
Transporter/inducer dissociation	$T{:}I \xrightarrow{k_{txOff}} T{+}I_{out}$	0.120	Membrane
Transporter degradation	$T \xrightarrow{k_{tDcy}} \emptyset$	$2.567\times 10^{-4}$	Cytoplasm, Membrane
Transporter degradation	$\text{T:I} \xrightarrow{k_{\text{tDcy}}} \emptyset$	$2.567\times 10^{-4}$	Cytoplasm, Membrane

## Table 2

Model parameters and diffusion rates used in the S. cerevisiae and HeLa models.

	Model		
Parameter	S. cerevisiae	HeLa	
Time step [µs]	67.0	10.7	
Lattice dimensions	$192\times192\times192$	$224 \times 128 \times 224$	
Lattice spacing [nm]	28.7	8.0	
Inducer diffusion rate $[\mu m^2 s^{-1}]$	2.045	_	
mRNA diffusion rate $[\mu m^2 s^{-1}]$	0.5	0.5	
Protein diffusion rate [µm <sup>2</sup> s <sup>-1</sup> ]	1.0	1.0	
Protein diffusion rate (membrane) $[\mu m^2 \ s^{-1}]$	0.01	_	
Maximum diffusion rate $[\mu m^2 s^{-1}]$	2.045	1.0	

## Table 3

Simple model of a self repressing gene used in the HeLa model.

Description	Reaction	Stochastic rate [s <sup>-1</sup> ]	Defined regions
Repressor/gene association	$D_{on} + P \xrightarrow{k_{gnOff}} D_{off}$	73.622	Nucleoplasm
Translation initiation	$\mathbf{R}{+}\mathbf{m}\xrightarrow{k_{\mathrm{tlInit}}}\mathbf{R}{:}\mathbf{m}$	$3.243  imes 10^5$	SSU
Translation termination	$\mathbf{R:m} \xrightarrow{k_{\mathrm{tiTerm}}} \mathbf{R+m+P}$	1.393	SSU