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Stage 2 Sleep EEG Sigma Activity and Motor Learning in Childhood ADHD: A Pilot Study

Jared M. Saletin, PhD^{1,2}, William G. Coon^{2,3}, and Mary A. Carskadon, PhD^{1,2,4}

¹Department of Psychiatry and Human Behavior, Alpert Medical School of Brown University, Providence, RI, USA

²Sleep for Science Research Laboratory, E.P. Bradley Hospital, Providence, RI, USA

³National Center for Adaptive Neurotechnologies, New York State Department of Health, Albany, NY, USA

⁴Centre for Sleep Research, University of South Australia, Adelaide, South Australia, Australia

Abstract

Objective—Attention deficit hyperactivity disorder (ADHD) is associated with deficits in motor learning and sleep. In healthy adults, overnight motor skill learning improvement is associated with sleep spindle activity in the sleep EEG. This association is poorly characterized in children, particularly in pediatric ADHD.

Method—Polysomnographic sleep was monitored in seven children with ADHD and fourteen typically developing controls. All children trained on a validated motor sequence task (MST) in the evening with retesting the following morning. Analyses focused on MST precision (speed-accuracy trade-off). NREM Stage 2 sleep EEG power spectral analyses focused on spindle-frequency EEG activity in the sigma (12–15 Hz) band.

Results—The ADHD group demonstrated a selective decrease in power within the sigma band. Evening MST precision was lower in ADHD, yet no difference in performance was observed following sleep. Moreover, ADHD-status moderated the association between slow sleep spindle activity (12–13.5 Hz) and overnight improvement; spindle-frequency EEG activity was positively associated with performance improvements in children with ADHD but not in controls.

Conclusions—These data highlight the importance of sleep in supporting next day behavior in ADHD, while indicating that differences in sleep neurophysiology may, in part, underlie cognitive deficits in this population.

Keywords

Sleep; ADHD; Motor learning; Adolescence; Sleep spindles

Corresponding Author: Jared M. Saletin, PhD, Sleep for Science Research Laboratory, 300 Duncan Drive, Providence, RI 02906, jared_saletin, brown.edu, P: (401) 421 - 9440, F: (401) 453 - 3578.

Introduction

Attention deficit hyperactivity disorder (ADHD) is associated with simultaneous deficits in daytime learning (Adi-Japha, Fox, & Karni, 2011) and nocturnal sleep (Owens et al., 2013). Whereas sleep supports learning in adults, particularly for motor skills (Walker, Brakefield, Morgan, Hobson, & Stickgold, 2002), this association is less well understood in adolescents, those with ADHD in particular. This pilot study examines whether distinct profiles of sleep-dependent learning are observed in ADHD and typically developing children.

The current study focused on a procedural memory paradigm known to demonstrate sleepdependent improvement in adults. Whereas sleep deprivation impairs overnight improvement in motor skill learning (Fischer, Hallschmid, Elsner, & Born, 2002), both nocturnal sleep (Walker et al., 2002) and daytime naps (Nishida & Walker, 2007) consolidate and stabilize performance. A neural marker of sleep-related overnight improvement is found in the non-rapid eye movement Stage 2 Sleep EEG: the thalamocortical sleep spindle (a synchronous burst in the 12–15 Hz range (Nishida & Walker, 2007)). Sleep-spindle-frequency EEG activity in the sigma band (12–15 Hz) over motor cortex predicts overnight gains in motor learning in healthy adults, and indexes the degree of motor skill learning deficits in circumstances such as schizophrenia (Wamsley et al., 2013).

While one recent study examined sleep-dependent procedural motor skill learning in pediatric ADHD (Prehn-Kristensen et al., 2011), the authors did not perform spectral analysis of the sleep EEG. Indeed, whether sleep spindles are atypical in children with ADHD is unclear. When compared to traditional polysomnography, relatively little is known about the micro-features of the sleep EEG in this population. Whereas one recent study identified lower slow wave activity and higher spindle-frequency sigma activity in ADHD (Prehn-Kristensen et al., 2013), another group demonstrated a converse increase in slow wave activity over central cortices (Ringli et al., 2013). Neither of these latter studies involved a motor-learning paradigm. Thus, the current pilot study therefore aimed to add to this growing literature while testing the hypothesis that overnight motor learning ability in ADHD may be sensitive to spindle-frequency EEG activity expressed during sleep.

Materials and Methods

The local institutional review board approved the study. Informed consent was obtained from all parents, with assent from all children. Each child received monetary compensation for participating in the study.

Participants

26 children (aged 10–12.9 years) entered the study. Five children were excluded from analysis for technical issues (n=2) or attrition (n=3), yielding a final sample of 7 children with ADHD and 14 typically developing controls (TDC). The sample was primarily male, yet was balanced for gender, with 2 girls in the ADHD group, and 4 girls in the TDC group. Complete demographics are reported in Table 1.

A brief parental telephone interview screened for current past medical/psychiatric conditions, family history of medical/psychiatric conditions, current use of psychoactive agents, and abnormal sleep habits. Diagnosis of ADHD was confirmed using the "ADHD" and "other DSM-IV Diagnostic Categories" of the Diagnostic Interview Schedule for Children, Fourth Edition (DISC-IV) (Shaffer, Fisher, Lucas, Dulcan, & Schwab-Stone, 2000) (Table 1). Exclusion criteria included: parental or child report of irregular sleep patterns (e.g., self-reported sleep schedules that vary by greater than 3 hours across a week, self-reported excessive daytime sleepiness, frequent napping (3 times/week), a morningness/eveningness score (Smith, Reilly, & Midkiff, 1989) of greater than 2 standard deviations above or below the mean values of subjects in the same grade (age) and of the same sex, based on our laboratory normative data pool); travel beyond two time zones within 2 months of the study; diagnosis of a learning disability, mental retardation, dyslexia, pervasive developmental disorder; a personal and/or family history of narcolepsy.

Neuropsychological assessment characterized children on intelligence/achievement, attention/impulse control, learning/memory, response speed/productivity, and problem solving/cognitive control. Trained staff administered the Kaufman Brief Intelligence Test, Second Edition (KBIT-2) (Kaufman & Kaufman, 2004), the Wide Range Assessment of Memory and Learning, Second Edition (WRAML-2) (Sheslow & Adams, 2003), and the Wide Range Achievement Test, Fourth Edition (WRAT4) (Wilkinson & Robertson, 2006). Both groups were in normative ranges (Table 1), while TDC children had higher math computation scores compared to ADHD peers (*p*=.018).

Procedures

At-Home Protocol

Participants were monitored by wrist actigraphy (Sadeh, Sharkey, & Carskadon, 1994) and completed a sleep-wake diary for one week before and throughout the study. During this time participants were asked to maintain a 10-hour sleep schedule set to habitual rise time (call-ins to a laboratory answering machine ensured compliance) to ensure stable sleep patterns prior to the start of the study for all children. Participants abstained from caffeine 12 hours before bedtime for the entire course of the study. Those in the ADHD group were withdrawn from psychostimulants for two weeks before and throughout the in-lab study.

In-Lab Protocol

Participants spent two consecutive nights in the laboratory on the same schedule as above: (i) an adaptation night to acclimate to the laboratory and screen for sleep-disordered breathing; (ii) the primary experimental night. On the adaptation night participants arrived approximately 3.5 hours before scheduled bedtime and were monitored overnight using polysomnography (see below). Participants returned the next evening, were provided dinner, and were again prepared for polysomnography. Approximately 80 minutes before bedtime, each participant began a cognitive test battery including a declarative memory assessment (Ellenbogen, Hulbert, Stickgold, Dinges, & Thompson-Schill, 2006) (not reported here), followed by the Motor Sequence Task (MST) (Nishida & Walker, 2007; Walker et al., 2002; Walker et al., 2003), described in detail below. MST training occurred approximately 60

minutes before bed; morning testing on the MST began after breakfast, approximately 75 minutes after waking.

Motor Sequence Task

To assess procedural skill learning, participants completed a Motor Sequence Task (Figure 2, upper-panel; MST), well documented as sleep-dependent in adults (Nishida & Walker, 2007; Walker et al., 2002). The MST required participants to tap a 5-element sequence (4-1-3-2-4) on the numeric keys of a computer keyboard with the fingers of their nondominant hand "as quickly and accurately as possible" for 30 seconds. Participants could see the sequence on the screen; however, no feedback was given with respect to accuracy. Evening training consisted of 12, 30-second trials interspersed with 30-second periods of rest. Morning testing consisted of 4, 30-second trials, with equivalent intervening rest. "MST Precision" was calculated as the proportion of total keystrokes that were not errors. This metric represents a trade-off between speed (number of correct 5-digit sequences typed) and accuracy (number of errors made). As in prior studies, evening performance was defined as the average of the final two evening trials; morning performance was defined as the average of the first two trials (Nishida & Walker, 2007; Walker et al., 2002; Walker et al., 2003; Walker & Stickgold, 2005; Walker, Stickgold, Alsop, Gaab, & Schlaug, 2005; Walker, Stickgold, Jolesz, & Yoo, 2005). A within-subject measure of overnight improvement was derived as the absolute difference between morning and evening scores.

Polysomnographic Recording

Sleep on both nights was monitored by polysomnography (PSG) using a Grass Comet XL system (Astro-Med, Inc., West Warwick, RI) measuring the electroencephalogram (EEG) at central and occipital derivations (C3/A2, C4/A1, O1/A2, and O2/A1), right and left electrooculogram (EOG), electromyogram (EMG), and electrocardiogram (ECG). Sleep stages were visually scored by trained technicians (blind to ADHD condition; inter-rater reliability 85%) in 30-second epochs from C3/A2 according to standard criteria (Rechtschaffen & Kales, 1968). Respiratory measures were applied on the adaptation night to screen to sleep-disordered breathing. An Apnea-Hypopnea Index (the number of apnea or hypopnea events per hour of sleep) was derived according to standard criteria (Iber, Ancoli-Israel, Chesson, & Quan, 2007).

Power Spectral Analysis of Sleep EEG

The current analyses focus upon sleep spindle frequencies in Stage 2 sleep due to their documented role in supporting overnight MST improvement (Nishida & Walker, 2007; Walker et al., 2002). A power spectral analysis of the Stage 2 NREM sleep EEG was performed following established procedures (Kurth et al., 2010; Mander, Santhanam, Saletin, & Walker, 2011; Ringli et al., 2013; van der Helm et al., 2011). In short, following semi-automated artifact detection fast fourier transforms on hamming-windowed 5-second segments yielded power spectral densities with 0.2 Hz resolutions. To normalize amplitude differences among individuals, the power spectrum of each channel was divided by the total integrated power (0.6–32 Hz), yielding relative power spectral densities, which were matched with corresponding sleep stages.

Relative power was assessed for the average of the C3/A2 and C4/A1 derivations, reflecting activity over primary motor cortex, motivated by prior associations with overnight MST improvement (Nishida & Walker, 2007). Group differences in sleep EEG spectra were first examined across the entire frequency range (0.6–32 Hz), and subsequently using *a priori* defined bands of interest in the sigma band: slow sleep spindle activity (12–13.5 Hz) and fast sleep spindle activity (13.5–15 Hz). While the primary focus of this analysis was placed on sleep spindle frequency activity, slow wave activity SWA (1–4.6 Hz) was also derived as a comparison and to test prior reports of SWA changes in ADHD (Ringli et al., 2013).

Statistical Analysis

Group differences in the EEG power density spectra were examined using bootstrapped independent-sample t-tests. This method makes no assumptions regarding the distributional qualities of the EEG frequency spectrum and is described in detail elsewhere (Tarokh & Carskadon, 2010a, 2010b). In short, for each 0.2 Hz frequency bin, 5000 random group assignments were sampled with replacement from the data, yielding a bootstrapped distribution for each group. A difference distribution, S_2 - S_1 was used to test statistical significance of the actual difference between groups. If the true difference exceeded the 97.5th percentile of the bootstrapped distribution, it was considered statistically significant (equivalent to a two-tailed alpha level of .05). To limit erroneous Type-1 errors from testing many frequencies, significant frequencies not surrounded by at least 2 other significant frequencies were discarded.

Performance data were analyzed in StataSE 13.0 (StataCorp LP, College Station, TX) using mixed-effects models including a within-subjects factor condition (Evening/Morning) and a between-subjects factor group (ADHD/TDC). Primary focus was placed upon the interaction of group and condition; that is, whether ADHD-status moderates the impact of sleep. Exploratory simple main-effects decomposed the interaction to examine (i) whether the groups differed statistically in the morning or evening conditions and (ii) whether overnight changes occurred within-each group independently. Effect sizes are reported as appropriate.

Multiple regression analyses were used to test whether the relationship between prior night sleep EEG activity and overnight behavioral change differed between the ADHD and TDC groups. Each model included three parameters: (i) Relative EEG power, (ii) Group (ADHD/TDC), and (iii) the interaction of group and EEG power; that is, did ADHD status moderate the relationship between sleep EEG activity and overnight learning. Simple-slopes decomposed the interaction. Robust standard errors accommodated potential effects of outliers in a heterogeneous and small sample.

Results

Group Sleep Variables

Polysomnographic sleep variables are reported in Table 2. The ADHD group spent less time in bed as evident by a lower Total Dark Time (p=.025). Despite this difference, both groups demonstrated total sleep time of nearly 10 hours thus suggesting no major differences in sleep opportunity. A non-significant trend suggested fewer minutes in REM sleep in the

ADHD group (p=.069); however, this trend was eliminated when expressed as a percentage of total sleep time (p=.10). No other differences in sleep were observed. No evidence for sleep-disordered breathing was observed in these participants; AHI was low for both the TDC (1.21±0.22) and ADHD (1.41±0.16) groups; further, AHI did not distinguish the groups (p=.54).

Sleep Power Spectra by Group

Stage 2 EEG analyses revealed a suppression of power in the spindle-related sigma band (12.4–16.4 Hz) in ADHD relative to TDC (Figure 1, bootstrapped p's<.05). While theta activity (~4–8 Hz) was marginally higher in ADHD, this difference was not statistically significant. No other significant differences in the power spectra between ADHD and TDCs occurred. These results were confirmed by examining *a priori* bands of interest. Slow wave activity did not differentiate groups (t(19)=-0.01, p=.99, d=-0.0048) while the ADHD group expressed lower power in the slow (t(19)=-2.48, p=.023, d=-1.15) and fast (t(19)=-2.11, p=. 049, d=-0.98) spindle bands, with the greatest deficit observed for slow spindle activity.

MST Behavioral Performance

MST precision—representing the trade-off between speed and accuracy—improved following sleep (Figure 2), as indicated by a main-effect of condition (Wald- χ^2 =17.56, *p*<. 0001, *d*=.67). The magnitude of this overnight improvement in precision differed by ADHD status, as shown by an interaction of group and condition (Wald- χ^2 =6.08, *p*=.014, *d*=1.14). Specifically, MST precision improved overnight for the ADHD group (Wald- χ^2 =16.61, *p*<. 0001, *d*=1.33), but not for TDCs (Wald- χ^2 =2.23, *p*=.14, *d*=.079). As a result, while the ADHD group had impaired MST precision in the evening vis-à-vis TDC (Wald- χ^2 =3.90, *p*=.048, *d*=1.33), this effect was ameliorated in the morning (Simple effect: Wald- χ^2 =0.02, *p*=.88, *d*=.34).

Sleep–Behavior Relationships

We next examined whether the group differences in slow and fast spindle-frequency activity accounted for differential overnight improvement in MST precision in ADHD; these results are illustrated in Figure 3. ADHD status significantly moderated the association between slow spindle EEG frequency activity and overnight improvement in MST precision (β =-8.22, *p*=.023). Specifically, MST precision was positively associated with slow spindle activity for the ADHD group (β =8.71, *p*=.003), but not for TDCs (β =.50, *p*=.82). That is, despite having lower slow spindle activity, children with ADHD appear more sensitive than TDCs to the cognitive benefits it supports. These associations were not mirrored for fast spindle activity (*p*'s>.05). In light of the potential (albeit not statistically significant) group difference in IQ (ADHD group: 110.3±14.1; TDCs: 120.07±9.4), we repeated this analysis with IQ included as a covariate in the model. Despite controlling for IQ, we confirmed the moderating effect of ADHD-status on the association between slow sleep spindle activity and overnight gains in MST precision (β =-8.72, *p*=.026); thus, a significant effect remained in the ADHD group with no effect for the TDC group (β =.435, *p*=.85).

Discussion

These initial findings provide a series of novel insights. First, despite no differences in sleep structure, sleep spindle EEG activity appears attenuated in 10–13 year old children with ADHD. Second, despite deficits in motor skill precision present in children with ADHD prior to sleep (Adi-Japha et al., 2011), no group difference was observed in the morning. Third, the degree of successful overnight improvement in ADHD children is associated with the magnitude of sleep spindle EEG frequency activity retained. Together these data underscore a necessity to ensure healthy sleep in this population, while indicating a need for future research examining mechanisms underlying these associations.

Traditional polysomnography has yet to reveal a consistent sleep signature of ADHD (Gruber, 2009; Owens et al., 2013). Our finding of reduced spindle-frequency EEG activity adds to recent quantitative spectral analyses (Prehn-Kristensen et al., 2013; Ringli et al., 2013) in demonstrating that micro-features of the sleep EEG may aid in distinguishing children with ADHD. One limitation of early, inconsistent reports of fewer spindles in ADHD (Khan & Rechtschaffen, 1978; Kiesow & Surwillo, 1987) is that sleep EEG sigma frequencies shift during development (Jenni & Carskadon, 2004; Kurdziel, Duclos, & Spencer, 2013) making automated spindle detection in this age-range challenging. The current study examined the entire range of EEG frequencies, circumventing this limitation. Further studies will continue to elucidate how sleep EEG may differentiate children with and without ADHD.

It is intriguing that no association emerged between overnight gains in MST precision and spindle-frequency EEG activity for the typically developing children, despite spindledependent effects in healthy adults (Nishida & Walker, 2007; Wamsley et al., 2013), consistent with other sleep-dependent memory studies in children (Wilhelm, Diekelmann, & Born, 2008). Despite this null finding in typically developing children, those with ADHD demonstrated an adult-like relationship despite an overall decrease in sleep spindle activity. Thus, the success of spindle production may be functionally protective in children with ADHD, as those with higher (more TDC-like) spindle activity benefited by exhibiting a concomitantly higher improvement in MST precision the next day. Conversely, those with a greater spindle deficit demonstrated lower overnight improvement in MST precision. The magnitude of the spindle activity deficit in a child with ADHD may therefore provide an index of their behavioral deficits, while also providing a mechanistic target within sleep for intervention. For example, non-invasive stimulation of the brain using techniques such as transcranial direct current stimulation (tDCS) (Prehn-Kristensen et al., 2014) or sensorimotor rhythm (SMR) neurofeedback (Hoedlmoser et al., 2008) can manipulate sleep EEG in a non-pharmacological manner, potentiating slow wave as well as sleep spindle frequency activity above baseline levels. These studies have demonstrated benefits in declarative memory from this modulation of the sleep EEG; however, they have not yet been extended to the motor learning domain described here.

This study is not without limitations. First, as the adaptation night may include EEG-altering first-night effects (Agnew, Webb, & Williams, 1966), the current study cannot preclude the possibility that the differences in sleep EEG reported reflect not a stable difference in

ADHD but rather a difference in learning-dependent changes in EEG (Huber, Ghilardi, Massimini, & Tononi, 2004). Second, the current sample was unable to dissociate between symptom presentations of ADHD. To do so will require sample sizes greater than here or other sleep studies (Prehn-Kristensen et al., 2011; Prehn-Kristensen et al., 2014). In the context of the small sample size of the current study, we note that the strength of the effects reported (e.g., d=1.14 with respect to the group difference in overnight performance gains) indicate a potentially powerful difference in sleep-dependent cognition in ADHD, meriting a more robust sample. Specifically, a large within-group effect of sleep was observed in the ADHD group (d=1.33) yet a small effect was observed for TDCs (d=0.079). Third, our subjects were recruited to be free of disordered sleep. Thus, the current study cannot address how sleep disorders in ADHD (e.g., sleep disordered breathing (Sedky, Bennett, & Carvalho, 2014) or atypical Cyclic Alternating Pattern (Akinci et al., 2015)) may impact overnight improvements in motor learning. Fourth, the current study does not replicate a groupdifference in slow wave activity (Ringli et al., 2013). The lack of frontal EEG derivations limits our present ability to address whether a stable slow wave activity difference is present in ADHD. Slow wave activity transitions from posterior- to anterior-dominance during adolescence (Kurth et al., 2012); thus, future studies employing denser EEG montages will be necessary to more adequately address this issue. Finally, the current participants were withdrawn from psychostimulants throughout the protocol, limiting the ecological validity of our participants' sleep. Stimulants prescribed for ADHD (e.g., dextroamphetamine) may disrupt sleep (Andersen et al., 2009), although the nature of this disruption, particularly with respect to the frequencies described here, is unclear (Surman & Roth, 2011). More generally, the potential interaction of ADHD medications and sleep in mitigating behavioral deficits in ADHD warrants further examination.

In conclusion, while sleep disturbance is a common complaint in childhood ADHD, traditional polysomnography has been inconclusive in identifying a neurophysiological signature in sleep that indexes cognitive and behavioral deficits. These data join with other recent reports to indicate that microstructural properties of the sleep EEG not commonly examined in a clinical study —here sleep spindle frequency activity—may, in part, regulate next-day behavioral function in ADHD. Future clinical and basic studies will elucidate the extent to which these sleep EEG oscillations relate to the broader spectrum of symptoms common to ADHD, and whether interventions targeting such sleep neurophysiology may therapeutically aid in the treatment of this and other neurodevelopmental disorders.

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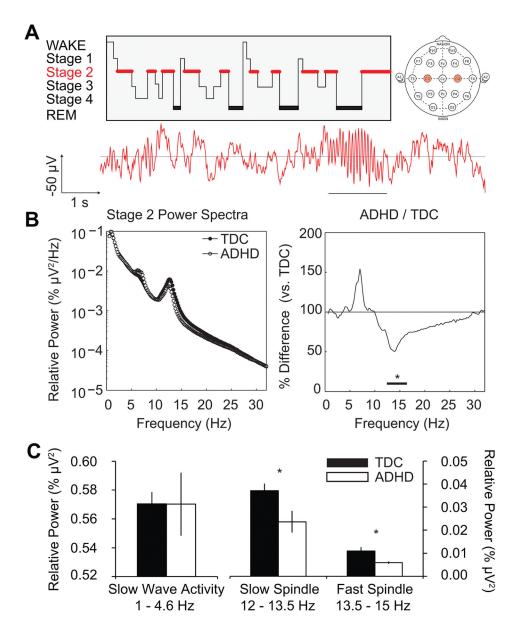


Figure 1. All-night NREM Stage 2 Power Spectra

(A) Top-Left: A schematic "hypnogram" (redrawn and adapted from (Abel, Havekes, Saletin, & Walker, 2013)) demonstrating a prototypical night of sleep, as staged by polysomnography. Red highlights NREM Stage 2 sleep, from which all EEG analyses derive. Top-Right: A pictorial depiction of the standard electrode placements for EEG. Power spectra are averaged for the left and right central derivations (C3 and C4, labeled in red), respectively, corresponding to primary motor cortex. Bottom: Representative 10-seconds of Stage 2 NREM EEG. Time and amplitude scale as indicated. Underlined portion highlights a prototypical sleep spindle frequency event. (B) Left: Relative EEG power during Stage 2 sleep for the typically developing controls (black circles) and ADHD group (white circles), respectively from 0.6 Hz to 32 Hz at 0.2 Hz resolution (frequency on abscissa). Each participant's power spectrum is normalized to his or her total power across this range

yielding relative (%) values, plotted here on a base-10 logarithmic scale. Right: Stage 2 power in the ADHD group plotted as a percentage of the typically developing group; frequency axis as before. Black bar indicates frequencies of significant difference between groups. (C) Integrated Stage 2 power extracted for the slow wave, slow spindle, and fast spindle bands, respectively, using *a priori* frequency definitions. Significance values are derived from appropriate statistics reported in the text and are indicated as: + = p < 0.10, * = p < 0.05.

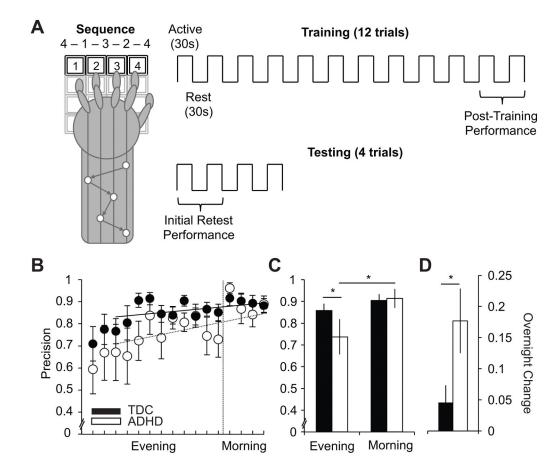


Figure 2. Motor Sequence Task (MST) Behavior

Motor learning was measured using the Motor Sequence Task (MST). (A) MST protocol: Evening training (right-top panel) consisted of 12 rounds of 30-second trials of repeatedly tapping the motor sequence "4 - 1 - 3 - 2 - 4" on the numeric keys of the keyboard with the non-dominant hand (schematic shown in left panel) alternated with 30-second bouts of rest. Morning testing consisted of 4 rounds of tapping and rest, as before. Evening performance was quantified as the average of the final two training trials, and morning performance as the average of the first two testing trials. MST schematic adapted and redrawn from Walker, et al., 2003 (Walker et al., 2003). (B) MST precision is reported trial-by-trial (left panel) and using evening and morning summary scores (right panel) for the TDC (black-fill) and ADHD (white-fill) groups, respectively. Lines of best fit for ADHD (dotted) and TDC (solid) are fit to the final 10 trials of training, and project forward to morning, to predict precision gains based on practice alone. (C–D) Histograms plotting evening and morning summary scores for each group (C), and within-subject overnight change scores (D). All error bars indicate standard error of the mean. Significance values are derived from appropriate statistics reported in the text and are indicated as: + = p < 0.10, * = p < 0.05.

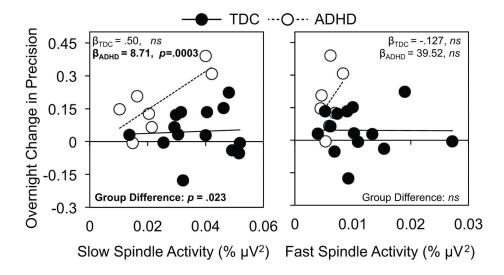


Figure 3. Association between EEG spindle activity and overnight precision gains

Scatterplots of the association between individual levels of slow (12–13.5 Hz; left) and fast (13.5–15 Hz; right) spindle activity during NREM Stage 2 sleep and overnight change in MST precision (proportion of keystrokes not associated with errors). Lines of best fit for the TDC group (black circles) are plotted as solid lines with those for the ADHD group (white circles) plotted as dotted lines. Group-wise simple slopes and the difference between these slopes are extracted from the regression models reported in the text. ns = p > 0.05.

Table 1

Demographic Variables

	ADHD $n = 7$	Controls $n = 14$	р
Gender (# Girls)	2	2	1.000
Age (years)	11.9 ± 0.9	11.7 ± 0.9	.62
DISC-IV			
ADHD Symptoms	11.3 ± 3.4	0.86 ± 1.2	< .001
Behavioral Impairments	6.6 ± 1.9	0.00 ± 0.0	< .001
Symptoms + Impairments Impairments	17.9 ± 4.1	0.86 ± 1.2	< .001
BDI			
Raw Score	5.1 ± 4.0	5.00 ± 4.0	.94
T-Score	39.2 ± 4.3	39.15 ± 4.2	.95
WRAML-2			
Verbal Memory	112.3 ± 9.8	116.21 ± 10.5	.42
Visual	98.7 ± 15.1	97.64 ± 11.5	.86
Screening Memory	106.9 ± 11.3	108.86 ± 11.3	.71
KBIT-2			
Verbal	111.6 ± 13.3	119.21 ± 10.6	.17
Nonverbal	105.9 ± 13.3	115.05 ± 9.3	.079
IQ	110.3 ± 14.1	120.07 ± 9.4	.072
WRAT4			
Word Reading	99.2 ± 15.2	115.21 ± 15.9	.067
Spelling	107.0 ± 12.7	116.29 ± 16.3	.31
Math Computation	101.8 ± 18.4	120.20 ± 11.6	.018

Note: Data reported as mean \pm sd. Significance from 2-tailed X² tests, or independent samples t-tests as appropriate. Definitions: DISC-IV: *Diagnostic Interview Schedule for Children Version IV.* WRAML-2: *Wide Range Assessment of Memory and Learning, Second Edition.* KBIT-2: *Kaufman Brief Intelligence Test, Second Edition.* WRAT4: *Wide Range Achievement Test 4.*

Table 2

Polysomnographic Sleep Statistics

	ADHD $n = 7$	Controls $n = 14$	p
Total Dark Time (min.)	590 ± 15	602 ± 9	.025
Sleep Period Time (min.)	563 ± 11	579 ± 19	.051
Total Sleep Time (min.)	541 ± 21	561 ± 23	.064
Sleep Efficiency (%)	96.0 ± 3.0	96.8 ± 1.7	.44
Latency to Sleep Onset (min.)	18 ± 15	17 ± 10	.76
Latency to REM Sleep (min.)	144 ± 64	124 ± 55	.48
Wake After Sleep Onset (min.)	16 ± 16	10 ± 9	.28
Wake After Final Awakening (min.)	8 ± 17	6 ± 16	.76
Wake (min.)	42 ± 28	32 ± 18	.33
NREM Stage 1 (min.)	35 ± 19	30 ± 9	.38
NREM Stage 2 (min.)	205 ± 29	222 ± 41	.36
NREM Stage 3 (min.)	74 ± 28	66 ± 22	.56
NREM Stage 4 (min.)	125 ± 21	124 ± 30	.95
REM Sleep (min.)	108 ± 22	119 ± 18	.069
Slow Wave Sleep (min.)	199 ± 41	190 ± 40	.66
Wake (% TST)	9.0 ± 5.7	5.9 ± 3.6	.31
NREM Stage 1 (% TST)	6.5 ± 3.5	5.3 ± 1.5	.28
NREM Stage 2 (% TST)	38.1 ± 6.4	39.5 ± 6.9	.65
NREM Stage 3 (% TST)	13.5 ± 6.8	11.7 ± 3.6	.43
NREM Stage 4 (% TST)	23.2 ± 4.3	22.3 ± 5.9	.72
REM Sleep (% TST)	17.3 ± 3.7	19.8 ± 2.9	.10
Slow Wave Sleep (% TST)	36.7 ± 7.0	34.0 ± 7.3	.43
Stage 2 EEG Spectral Power			
Slow Wave Activity (% µV ²)	$.57 \pm .058$	$.57 \pm .031$.99
Slow Sleep Spindle Activity (% μV^2)	$.024\pm.012$	$.037\pm.011$.023
Fast Sleep Spindle Activity (% μV^2)	$.0059\pm.0014$	$.011 \pm .0062$.049

Note: Data reported as mean ± sd. Definitions: Time in Bed: *elapsed time from lights out to lights on*. Sleep Period Time (SPT): *elapsed time from sleep onset to final awakening*. Total sleep time (TST): *total time scored sleep within SPT*. Sleep Efficiency: *(TST/SPT)*100. Slow Wave Sleep: Stages 3+4 collapsed*. Significance from 2-tailed independent-samples *t*-tests.