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Bone-induced expression of integrin $\beta 3$ enables targeted nanotherapy of breast cancer metastases

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Abstract

Bone metastases occur in ~70% of metastatic breast cancer patients often leading to skeletal injuries. Current treatments are mainly palliative and underscore the unmet clinical need for improved therapies. In this study, we provide preclinical evidence for an antimetastatic therapy based on targeting integrin $\beta 3$ ($\beta 3$) which is selectively induced on breast cancer cells in bone by the local bone microenvironment. In a preclinical model of breast cancer, $\beta 3$ was strongly expressed on bone metastatic cancer cells but not primary mammary tumors or visceral

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metastases. In tumor tissue from breast cancer patients, $\beta 3$ was significantly elevated on bone metastases relative to primary tumors from the same patient (n=42). Mechanistic investigations revealed that TGF- β signaling through SMAD2/SMAD3 was necessary for breast cancer induction of $\beta 3$ within the bone. Using a micelle-based nanoparticle therapy that recognizes integrin $\alpha v\beta 3$ ($\alpha v\beta 3$ -MPs of ~12.5nm), we demonstrated specific localization to breast cancer bone metastases in mice. Using this system for targeted delivery of the chemotherapeutic docetaxel, we showed that bone tumor burden could be reduced significantly with less bone destruction and less hepatotoxicity compared to equimolar doses of free docetaxel. Furthermore, mice treated with $\alpha v\beta 3$ -MP-docetaxel exhibited a significant decrease in bone-residing tumor cell proliferation compared to free docetaxel. Taken together, our results offer preclinical proof of concept for a method to enhance delivery of chemotherapeutics to breast cancer cells within the bone by exploiting their selective expression of integrin $\alpha v\beta 3$ at that metastatic site.

Keywords

Breast Cancer; Bone Metastases; Integrins; Nanoparticles; Drug Therapy

Introduction

Bone metastases occur in approximately 70% of metastatic breast cancer patients (1), often leading to the development of significant skeletal complications, such as pathological fracture, spinal cord compression, or bone pain (2). Current treatments – radiation, surgery, chemotherapy, and antiresorptive drugs – can improve quality of life but are rarely curative, with limited effect on overall survival (3-5). Treating breast cancer bone metastases has proven difficult due to frequent dissemination of metastases throughout the skeleton, a lack of tumor-specific targets expressed across breast cancer subtypes, and the chemo-protective nature of the bone microenvironment (2,6,7).

One approach to overcome these problems has been to enhance drug delivery to bone, most commonly by using bone matrix-targeted hydroxyapatite-avid bisphosphonates (8-10). Bisphosphonates are standard of care in patients with bone metastases or osteoporosis for their ability to inhibit osteoclast function and formation (1,2,10). While osteoclast inhibition can attenuate tumor-associated bone destruction with secondary effects on bone tumor growth, it does not improve overall survival in metastatic breast cancer patients (11,12). In line with this, bisphosphonate-targeted chemotherapy delivery can reduce mouse models of breast cancer-associated bone loss more effectively than free-drug chemotherapy (13,14). However, bisphosphonate-targeted drug delivery indiscriminately accumulates on all skeletal bone matrix and primarily targets osteoclasts and neighboring marrow cells near the bone matrix (8,15). To improve drug uptake by bone metastases, we sought to target tumor cells in the bone microenvironment more directly.

One targeting candidate of interest was the integrin $\alpha v\beta 3$. Integrins are heterodimeric cell surface receptors, composed of an α and β subunit from a large family of subunits, that bind to components of the extracellular matrix or to other cells (16). Integrin are expressed in a cell-specific and context-dependent manner, and are critical to all aspects of cancer

progression and metastasis through effects on migration, invasion, and cell survival (16-18). Specifically, integrin $\alpha v\beta 3$ is composed of the tightly regulated integrin subunit $\beta 3$ and the more widely expressed αv subunit. Expression of $\alpha v\beta 3$ on most cells in the body is typically low, but is elevated on several cancer types (17), as well as a variety of cell types that are important within the tumor microenvironment, such as osteoclasts (11,12), neo-angiogenic endothelium (19), and tumor-promoting macrophages (20). The expression of $\alpha v\beta 3$ on these cells led to the investigation of $\alpha v\beta 3$ as a therapeutic target for cancer treatment (21). In several clinical trials, pharmacological inhibition with $\alpha v\beta 3$ antagonists as a single-agent cancer therapy did not demonstrate a significant clinical effect (22,23). We, and others, have demonstrated that the inefficiency of $\alpha v\beta 3$ inhibitors in advanced cancer may be due to the inherent complexities of integrin signaling and off-target effects of $\alpha v\beta 3$ antagonism (20,24).

Rather than aiming to antagonize $\alpha v\beta 3$ function, we sought to utilize $\alpha v\beta 3$ as a molecular target for enhancing drug delivery to cells of interest within the bone. Integrin $\beta 3$ and $\alpha v\beta 3$ expression has been observed on human breast cancer bone metastases (25-27), and ectopic overexpression of tumoral $\beta 3$ on breast cancer has been demonstrated to enhance tumor establishment in bone (26,28). However, for the purpose of targeting $\alpha v\beta 3$, physiological expression on breast cancer during tumor growth and metastasis has not been defined. Here, we report that the bone microenvironment preferentially induces integrin $\beta 3$ on breast cancer metastases, as compared to the primary tumor or visceral metastases, and we identify TGF- β to be responsible for this induction. Utilizing this information, we evaluated nanoparticle-mediated drug delivery targeted against integrin $\alpha v\beta 3$. We recently developed phospholipid/polysorbate-80 micelle nanoparticles (MPs, ~12.5 nm) for their small size and unique mechanism of “contact-facilitated drug delivery” (29); in the present study, we demonstrate that integrin $\alpha v\beta 3$ -targeted micelle nanoparticles ($\alpha v\beta 3$ -MPs) carrying the chemotherapeutic docetaxel reduce bone metastases and tumor-associated bone destruction more effectively than free-docetaxel. Collectively, we demonstrate that $\alpha v\beta 3$ is a tumor target on breast cancer bone metastases and provide support for safer, more effective therapies against this often incurable disease by targeting integrin $\alpha v\beta 3$.

Materials and Methods

Animals

Animal studies were performed according to the guidelines established by the Washington University Institutional Animal Care and Use Committee (IACUC). PyMT-Bo1 tumor cells were implanted into female C57BL/6 mice, or 4T1 tumor cells were implanted into female BALB/c mice. All mice were obtained from The Jackson Laboratory, and injected at 6 to 7 weeks of age. All rodents were housed according to the guidelines of the Division of Comparative Medicine, Washington University School of Medicine. In collaboration with Dr. Theresa Guise, histological bone sections from female athymic nude mice injected with MDA-MB-231 human breast cancer cells were obtained from an experiment previously described (30).

Cell lines

The murine C57BL/6 PyMT-Bo1 luminal B breast cancer cell line (stably expressing GFP and firefly luciferase genes) was originally isolated from a transgenic MMTV-PyMT breast tumor, as previously validated and described (20). The murine BALB/c 4T1 triple-negative breast cancer cell line was purchased from ATCC, as previously described (31). Human MDA-MB-231 breast cancer cells (HTB-26) were purchased from ATCC (30). All cells were maintained at sub-confluence in DMEM with 10% FBS and 0.5% penicillin–streptomycin, in a humidified chamber at standard culture conditions. Low-passage stocks were used and regularly tested for *Mycoplasma* and maintenance of growth characteristics.

Murine cancer models

To establish orthotopic mammary fat pad (MFP) tumors, 0.1×10^6 tumor cells in 50 μ L PBS were injected into MFP tissue of 7-week-old female mice. To establish experimental secondary metastases, 0.05×10^6 tumor cells in 50 μ L PBS were intracardiac injected into the left ventricular chamber of 6-week-old female, with one exception; in collaboration with Dr. Theresa Guise, human MDA-MB-231 tumor cells were intracardiac injected (0.1×10^6 tumor cells in 100 μ L PBS) into 4-week-old female athymic nude mice, as previously described (30).

Synthesis of $\alpha v \beta 3$ -targeted micelle nanoparticles

Phospholipid/polysorbate 80 micelle nanoparticles (MPs) were prepared as a microfluidized suspension of 20% (v/v), combining polysorbate tween 80 (Sigma Aldrich, Inc.) with a 2.0% (w/v) of a surfactant comixture, and 1.7% (w/v) glycerin in pH 6.5 carbonate buffer, as previously described (29). Optionally, the surfactant comixture included 2.28 mol% of docetaxel-prodrug (DTX-PD), and/or 0.15 mol% of $\alpha v \beta 3$ -targeted quinolone nonpeptide coupled to phosphatidylethanolamine-PEG2000, with the remaining mol% lecithin. Docetaxel was modified into an Sn2 lipase-labile phosphatidylcholine DTX-PD as previously described (32). For fluorescent labeling, rhodamine-conjugated to phosphatidylethanolamine (0.1 mol%) was incorporated into the lipid surfactant. The surfactant components for each formulation were combined with the polysorbate, buffer, and glycerin mixtures and were homogenized at 20,000 psi for 4 minutes at 4C with a microfluidics (M110s; Microfluidics, Inc). The nanoparticles were preserved under inert gas in sterile sealed vials until use. Dynamic light scattering showed a nominal particle size of 12.5 ± 0.8 nm, with polydispersities 0.290 ± 0.03 , and an average electrophoretic zeta potential of -3.82 ± 1.23 mV.

The nanoparticle-targeting quinolone nonpeptide specific for integrin $\alpha v \beta 3$ was originally developed by Bristol-Myers Squibb Medical Imaging (US patent 6,511,648 and related patents) and coupled to phosphatidylethanolamine-PEG2000, as previously described (29). The quinolone nonpeptide was initially characterized as the ^{111}In -DOTA conjugate RP478 and cyan 5.5 homologue TA145 (33). This $\alpha v \beta 3$ -targeting ligand is selective for cells expressing $\alpha v \beta 3$ ($\text{IC}_{50} = 12$ nM), as compared to $\text{IC}_{50} > 10$ μM for $\alpha v \beta 5$, $\alpha 5 \beta 1$, or $\alpha \text{II} \beta 3$ (34). Furthermore, the affinity of the $\alpha v \beta 3$ -targeting ligand increases 15-fold for activated integrin $\alpha v \beta 3$ receptor in the presence of Mn^{2+} (33). *In vitro*, pretreating human endothelial with the human-specific integrin $\alpha v \beta 3$ antibody (LM609) competitively inhibited binding of

this $\alpha v\beta 3$ -targeting ligand (33). This $\alpha v\beta 3$ -targeted ligand has been applied to the surface of large, vascular-constrained perfluorocarbon nanoparticles (~250nm), which displayed a specific affinity for $\alpha v\beta 3$ -expressing angiogenic blood vessels and $\alpha v\beta 3$ -expressing melanoma cells, in contrast to nanoparticle controls (32,35,36). The *in vivo* specificity of this $\alpha v\beta 3$ -targeting ligand has been further demonstrated through competitive pretreatment with unlabeled $\alpha v\beta 3$ -targeting ligand, which inhibited $\alpha v\beta 3$ -targeted nanoparticle binding (35).

Bioluminescence imaging (BLI)

In vivo and *ex vivo* BLI was performed on IVIS50 (PerkinElmer, Waltham, MA) as previously described (20). Total photon flux (photons/sec) was measured from fixed regions of interest (ROIs) over entire mouse or manually around *ex vivo* organs using Living Image 2.6, as indicated. Mice with outstanding chest BLI intensity indicative of a failed intracardiac injection or with ineffective D-luciferin administration were excluded from all analyses. Investigators were blinded to treatment groups during all BLI analyses.

Rhodamine-labeled MP colocalization with breast cancer bone metastases

Tumor-bearing mice day 8 post-intracardiac injected with PyMT-Bo1 cells, or age-matched tumor-free mice, were treated with a single dose of rhodamine-labeled MPs (either non-targeted or $\alpha v\beta 3$ -targeted) at a nanoparticle dose of 2nmol/g mouse weight. Investigators were blinded to treatment groups during intravenous MP and $\alpha v\beta 3$ -MP injections. MPs were allowed to circulate for 3 hours *in vivo*, before sacrifice and tissue collection. Unbound MPs were cleared from circulation via cardiac perfusion with 30mL of PBS.

For fluorescent analysis of nanoparticle colocalization within bone, fresh-frozen long bones in optimum cutting temperature embedding medium (Tissue-Tek) were sectioned 5 μ m thick onto cryofilm tape (Section Lab Co., Ltd, Hiroshima, Japan) at the histology core of the Washington University Musculoskeletal Research Center. Cryofilm tape sections were fixed in -20°C acetone for 5 minutes and air-dried for 10 minutes. Slides were briefly rehydrated with PBS, and then mounted with ProLong Gold with DAPI (Invitrogen).

Fluorescent imaging and analysis

Fluorescent images were captured on a Photometrics CoolSNAP MYO camera connected to a Nikon Eclipse Ti-E microscope, acquired with the 4x Plan Fluor PhL DL objective through a TxRED HYQ filter cube and DAPI filter cube. The TxRED fluorescent channel was equally set using fluorescent look-up-table (LUT) to the same minimum and maximum values, gamma=1. Fluorescent colocalization analysis was performed using NIS-Elements AR (Nikon Canada, Inc., Richmond, BC, Canada). Bone metastatic region of interest (ROI) was drawn at the tumor/marrow boundary, as defined by DAPI visualization of nuclei density. Using the object count function in NIS-Elements AR, fluorescent nanoparticle colocalization was calculated via the ratio of rhodamine-positive pixel area by the total tumor ROI pixel area [(number of pixels of positively labeled objects within the fixed tumor area) / (total number of pixels within the fixed tumor area) \times 100].

Treatment of murine breast cancer metastases

Using the experimental metastasis model, PyMT-Bo1 metastases were established within female C57BL/6 mice. BLI analysis confirmed the establishment of bone metastases on day 3 post-intracardiac injection, and metastatic-bearing mice were randomly sorted and treatment started. Docetaxel (LC Laboratories, Woburn, MA) was prepared at 10 mg/mL in a tween80/ethanol/saline (20:13:67, v/v/v) solution for drug solubility, and diluted to 0.5 mg/mL DTX or 1.0 mg/mL in saline for intravenous administration. For nanoparticle treatment, mice received either a cumulative dose of 5.55 mg/kg docetaxel, an equimolar dose of nanoparticle-encapsulated docetaxel-prodrug (2.2 $\mu\text{mol/kg}$), or an equal amount of saline or cargo-free $\alpha\text{v}\beta\text{3-MP}$, fractionally administered intravenously every three days. *A priori* comparisons of interest were between saline-treated mice as compared to DTX or $\alpha\text{v}\beta\text{3-MP/DTX-PD}$, or between saline-treated mice compared to the nanoparticle control treatments.

In collaboration with Dr. Theresa Guise, histological bone sections were obtained from female athymic nude mice bearing MDA-MB-231 bone metastases, treated daily with the TGF- β Receptor I kinase inhibitor, 60 mg/kg/d SD-208 (Epichem Pty Ltd, Murdoch University, Australia) or vehicle (1% methylcellulose), from an experiment previously published (30).

Serum chemistry and hematologic analysis

Blood was collected by submandibular vein puncture into Microtainer EDTA tubes (BD Biosciences) for hematologic analysis (Hemavet 950 FS; Drew Scientific, Inc., Dallas, TX) or Microtainer serum separator tubes (BD Biosciences) for serum chemistry analysis on a Liasys 330 AMS Diagnostic liquid chemistry analyzer (Weston, FL). Investigators were blinded to treatment groups during analysis.

MTT assay

The MTT assay was performed as described previously (31). Signal intensity normalized to 0% for the viability of cells at time of drug addition, and 100% for the viability of vehicle control treated cells at 72 hr.

Radiography

Osteolytic lesions were imaged by X-Ray imaging system (Faxitron, Buffalo Grove, IL), and lesion area within the tibiofemoral joint was quantified using ImageJ (NIH, Bethesda, Maryland).

Immunohistological staining

Freshly removed tissue was fixed in 10% neutral buffered formalin for 24 hours. Bone was decalcified in 14% EDTA for 10 days. Tissue was paraffin embedded and sectioned 5 μm thick at the histology core of the Washington University Musculoskeletal Research Center. Standard tartrate-resistant acidic phosphatase (TRAP) staining or hematoxylin and eosin (H&E) staining was performed by the musculoskeletal histology core of the Washington University Musculoskeletal Research Center.

For immunohistochemistry, all slides were stained in parallel, using identical staining conditions. Paraffin tissue slides were prepared by immersing slides in xylene and rehydrating tissue in 100% ethanol, 95% ethanol, 70% ethanol, 50% ethanol, and deionized water washing steps. Slides were immersed in EDTA antigen retrieval buffer (1mM EDTA, 0.05% Tween 20, PH 8.0) at 50 °C overnight. Slides were treated with dual endogenous enzyme block (Dako), TBS/0.1% Tween-20 (TBST) wash buffer, and 10 minutes of serum-free protein block (Dako). Slides were stained with the following primary antibodies: anti-integrin $\beta 3$ antibody (D7X3P, 1:200, Cell Signaling), anti-integrin αv (ab179475, 1:500, Abcam), isotype control rabbit IgG (ab27472, Abcam) antibody, or biotinylated anti-PCNA antibody (PC10, 1:100, eBioscience). Following primary antibody incubation, slides were extensively washed in TBST. Either Anti-Rabbit EnVision+ System-HRP (Dako) or Vectastain Elite ABC HRP kit (Vector Laboratories, Burlingame, California) was used as the secondary antibody, followed by Liquid DAB+ (3,3'-Diaminobenzidine) Substrate system (Dako), according to the manufacturer's protocol. Nuclear hematoxylin counterstain was applied, followed by dehydration through 70% ethanol, 95% ethanol, 100% ethanol, and xylene. Slides were mounted with Cytoseal XYL (Thermo Scientific).

Histological imaging and analysis

Histological slides were imaged on either an Olympus NanoZoomer 2.0-HT System or on a Zeiss AxioScan.Z1. In each experiment, post-image analysis was limited to changes in brightness or contrast, gamma = 1, which were applied equally to all images. Sections stained with integrin $\beta 3$ or proliferating cell nuclear antigen (PCNA) were quantified using Visiopharm software (Hørsholm, Denmark), which allows for recognition and quantification of DAB-stained tissue areas. A supervised bayesian pixel classifier was used to classify an image based on three distinct categories: DAB staining, hematoxylin staining (nuclei), and unstained tissue and other background structures. Integrin $\beta 3$ expression from each sample was calculated within 5 to 10 random high-powered fields (hpf) of 100-200 cells within the tumors. Values expressed as the percentage of integrin $\beta 3$ expression (area of total DAB-positive staining) divided by the tumor area in the hpf. PCNA proliferation index was quantified by calculating the number of PCNA-positive cells divided by the total number of cells within the entire bone metastatic region. ImageJ software (NIH, Bethesda, Maryland) was used to measure tumor area, and to quantitate osteoclasts (OCs) (defined as a TRAP positive, multinucleated cell on a bone surface) per millimeter of bone surface (mmB.S.) at the tumor/bone interface (N.OC/mmB.S.). Histological analysis of bone metastatic tumor burden (tumor area / total bone marrow area) was calculated by measuring the tumor area within the metaphysis of the tibiofemoral joint, divided by the total marrow area of the metaphysis.

Flow cytometry and fluorescence activated cell sorting (FACS)

In vitro tumor cells were lifted with 1x Versene (Invitrogen). *Ex vivo* tumor cells were collected from the MFP or the bone, and prepared into single-cell suspensions for flow cytometry analysis as previously described (20). *Ex vivo* cells were stained with PE-conjugated anti-mouse integrin $\beta 3$ (1:200, clone: 2C9.G2, BD Pharmingen), fixed and permeabilized using the Cytotfix/Cytoperm kit (BD Biosciences) according to the manufacturer's protocol, and then with AlexaFluor488-conjugated anti-human/mouse

cytokeratin 18 (1:100, clone LDK18, eBioscience). Data acquisition was performed on the LSRFortessa (BD Biosciences) and FlowJo software version 10.1 (Tree Star) was used for analysis, and fluorescent compensation using UltraComp eBeads (eBioscience) according to the manufacturer's protocol. All flow cytometry data presented as median fluorescent intensity (MFI). *Ex vivo* flow cytometry analysis of bone samples with insufficient number of tumor cells (<500 events) were excluded.

For fluorescence activated cell sorting (FACS), *in vitro* tumor cells were lifted with 1x Versene (Invitrogen) and stained for surface expression of integrin $\beta 3$ as described above. Tumor cells were sorted into two populations using a BD FACS Aria-II cell sorter (BD Biosciences): integrin $\beta 3$ negative ($\beta 3^-$) cells (based on the fluorescent intensity of unstained cells) and integrin $\beta 3$ -expressing ($\beta 3^+$) cells. In addition, control cells sorted without $\beta 3$ discrimination were also collected ($\beta 3$ -all). After sorting, each population was counted for live/dead cells, and 0.05×10^6 live tumor cells in 50 μ L PBS were intracardiac injected into the 6-week-old female mice.

Pharmacological inhibition of signaling pathways

Tumor cells were pretreated for 1 hour with pharmacological inhibitors: cells were pretreated for 1 hour with the following pharmacological inhibitors: TGF β -receptor I kinase inhibitor, specific for the site necessary for SMAD2/SMAD3 phosphorylation (SMAD2/3i, SB431542, 20 μ M, Sigma-Aldrich); p38 MAP kinase (MAPK) inhibitor (p38i, SB203580, 20 μ M, Cell Signaling); MEK1/2 (MAPK/ERK Kinase) inhibitor (MEK1/2i, U0126, 20 μ M, Cell Signaling); c-Jun N-terminal kinase (JNK) inhibitor (JNKi, SP600125, 50 μ M, Sigma-Aldrich). After 1 hour of pretreatment, cells were treated with 2 ng/mL of murine TGF- $\beta 1$ (R&D systems) or vehicle treatment. Cells were all cultured in 0.1% DMSO.

Western blot analysis

Whole cell lysates from tumor cells were collected in RIPA buffer (Cell signaling) in the presence of Halt phosphatase inhibitor cocktail (Thermo Scientific) at 4°C. Protein samples were separated on 10% Mini-PROTEAN TGX polyacrylamide gels (Bio-Rad) and transferred onto an Immobilon-P polyvinylidene difluoride membrane (EMD Millipore). Membranes were incubated with phosphorylated-SMAD2/phosphorylated-SMAD3 (pSMAD2/pSMAD3, D27F4), total SMAD2/SMAD3 (D7G7), integrin $\beta 3$ (D7X3P), or β -actin (13E5), followed by horseradish peroxidase-conjugated anti-rabbit secondary antibody (all from Cell Signaling). All antibodies were diluted and used according to the manufacturer's protocol. Bands were developed by enhanced chemiluminescence.

Real-time quantitative PCR (qPCR) analysis

Total RNA from cells was isolated with the RNeasy Mini Plus kit (Qiagen). Complementary DNA was made using the SuperScript II first-strand synthesis system for qPCR (Invitrogen). qPCR was performed using SYBR Advantage mix (Bio-Rad) as previously described (20), with mouse-specific primers for mRNA genes of interest: *Itgb1* forward: 5'-GCAGGTGTCGTGTTTGTGAATGCT-3', *Itgb1* reverse: 5'-ACAAGTTGGCCCTTGAACTTGGG-3', *Itgb3* forward: 5'-TTCAATGCCACCTGCCTCAACAAC-3', *Itgb3* reverse: 5'-

ACGCACCTTGGCCTCGATACTAAA-3', *Itgb5* forward: 5'-TGTTTCAGCTACACAGAACTGCCCA-3', *Itgb5* reverse: 5'-TTTGGAACCTGGCAAACCTCTCGGC-3', *Itgb6* forward: 5'-TCAAACCTCCTTCACTCCTGCCAT-3', *Itgb6* reverse: 5'-TGAATCTGCTGGTTGCTCCAGACT-3', *Itgb8* forward: 5'-CAACTGCATCCAGGAGCTGA-3', *Itgb8* reverse: 5'-AACCAAGACGGAAGTCACGG-3', *Itga2* forward: 5'-AGCCCGTGATCTTTCCTAAAC-3', *Itga2* reverse: 5'-GCAGCCACAGAGTAACCTAAA-3', *Itga2b* forward: 5'-ACATTGAGGGCTTTGAGAGGCT-3', *Itga2b* reverse: 5'-TTGCCACAGGCAACATCACG-3', *Itga3* forward: 5'-GCGGAAGGACTGGGATTTAT-3', *Itga3* reverse: 5'-GATGATGTCCGTGGGATGTAG-3', *Itgav* forward: 5'-AGAAGACGTTGGGCCTATTG-3', *Itgav* reverse: 5'-TGTAAGGCCACTGGAGATTTAG-3', *Gapdh* forward: 5'-AGGTCGGTGTGAACGGATTTG-3', *Gapdh* reverse: 5'-TGTAGACCATGTAGTTGAGGTCA-3'. Target gene expression was normalized against the housekeeping gene GAPDH (*Gapdh*), and data were analyzed using the Ct method.

Panel of cytokines and growth factors

Tumor cells were cultured for 24 hours with the following murine factors: 2 ng/mL TGF- β 1 (R&D Systems), 2 ng/mL TGF- β 2 (R&D Systems), 50 ng/mL Sonic Hedgehog (Shh) (PeproTech, #315-22), 50 ng/mL WNT-3A (PeproTech, #315-20), 100 ng/mL Insulin-Like Growth Factor 1 (IGF-1) (PeproTech, #250-19), 50 ng/mL Epidermal growth factor (EGF) (PeproTech, #315-09), 50 ng/mL Fibroblast Growth Factor 2 (FGF2 or bFGF) (PeproTech, #450-33), 100 ng/mL Osteopontin (OPN) (Leinco, #O121), 10 ng/mL Interleukin 4 (IL-4) (R&D systems), 200 ng/mL Stromal Cell-derived Factor 1 α (SDF-1 α or CXCL12) (Biolegend), 10 ng/mL Interleukin 6 (IL-6) (R&D systems).

Patient breast cancer and matching bone metastatic biopsies

Matching primary breast and bone metastatic biopsies were both taken at the time of metastatic diagnosis, from patients without detectable bone metastases at diagnosis but detectable bone metastases at least 6 months after diagnosis. Data was obtained in accordance with the guidelines established by the Washington University Institutional Review Board (IRB #201102394) and WAIVER of Elements of Consent per 45 CFR 46.116 (d). All patient information was de-identified prior to sharing with investigators. All of the human research activities and all activities of the IRBs designated in the Washington University (WU) Federal Wide Assurance (FWA), regardless of sponsorship, are guided by the ethical principles in "The Belmont Report: Ethical Principles and Guidelines for the Protection of Human Subjects Research of the National Commission for the Protection of Human Subjects of Biomedical and Behavioral Research."

Tissue samples all displayed detectable tumor cells, as previously determined by examination of cellular morphology by a board-certified pathologist. Immunohistochemistry for integrin β 3 was performed as described in the previous section. Tumor-associated β 3 expression was semi-quantitatively scored in a blinded manner, in which the scorer did not

have access to disease classification or clinical annotation, using the histoscore (H-score) system: $H\text{-score} = \sum (i \times \%)$, where 'i' is the staining intensity (0 to 3 scale), and '%' is the percentage of tumor cells stained at each intensity, ranging 0% to 100%. We observed an expression pattern of tumoral $\beta 3$ consistent with a previous literature description of $\beta 3$ expression in human breast cancer: primarily localized along the cell plasma membrane at sites of tumor-tumor and tumor-stroma contact (37). In addition to the $\beta 3$ expression on bone metastases, we also observed $\beta 3$ staining on some host cells within the primary and bone tumor microenvironments, including tumor-infiltrating immune cells ($\beta 3$ expression colocalized with CD68-stained cells, predominately expressed on monocytes and macrophages), tumor-associated blood vessels, and osteoclasts, consistent with previous observations (11,12,19,20).

Breast cancer subtyping was based on ER,PR,HER2 status, where luminal A was ER+,PR+,HER2- (n=18), luminal B was ER+,PR+,HER2+ (n=7), HER2-enriched was ER-,PR-,HER2+ (n=2), and triple-negative was ER-,PR-,HER2- (n=7). Eight breast cancer carcinomas had incomplete genetic subtyping and were excluded from molecular subtype analysis.

Statistical analysis

All data shown as mean with error bars representing SEM. All sample sizes reported in the study are the minimum number of samples. For animal studies, sample sizes were estimated according to our previous experience. Statistical differences were analyzed using either a two-tailed *t*-test, ANOVA with Tukey's test for *a posteriori* (post-hoc) multiple comparisons, or a two-tailed unpaired *t*-test with Bonferroni correction for *a priori* comparisons between a control group and experimental treatment groups of interest. Assumptions for ANOVA and *t*-test (independent samples, approximately normal distributions) for samples $n > 5$ were sufficiently met, or used if a random sample of $n = 5$ were selected from an approximately normally distributed population. Non-normally distributed data was analyzed using a two-tailed Mann-Whitney *U*-test or a two-tailed Wilcoxon signed-rank test for matched-pairs. All tests were considered significant at $P < 0.05$, or in case of *k* comparisons, $P < 0.05/k$. Data analyses were complete using Prism 6 (GraphPad Software).

Results

Breast cancer cells overexpress integrin $\beta 3$ within the bone microenvironment

To determine the potential of targeting $\alpha v \beta 3$ at different metastatic sites, we evaluated breast cancer expression of integrin αv or $\beta 3$ at the primary site as compared to secondary metastases. Using the murine breast cancer cell line PyMT-Bo1 that models the luminal B subtype, primary MFP tumors were established by orthotopic injection, or metastases within the bone and visceral organs were established by intracardiac injection, into separate cohorts of mice. Tumors were removed 12 days post-injection and stained for integrin $\beta 3$ or integrin αv expression using immunohistochemistry. Bone metastases expressed elevated levels of $\beta 3$, as compared to MFP tumors or visceral metastases within the lung or kidney (Fig. 1A and Supplemental Fig. S1A). Unlike the selective upregulation of integrin $\beta 3$ on bone metastases, we observed expression of integrin αv across all primary and metastatic tumors

(Supplemental Fig. S1B). To determine whether the observed $\beta 3$ expression was tumor-cell specific, we used flow cytometry to quantify cell surface $\beta 3$ expression. Using PyMT-Bo1 cells or murine 4T1 triple-negative breast cancer cells, MFP tumors or bone metastases were established by orthotopic injection or intracardiac injection, respectively. Isolated tumor cells were identified based on cytokeratin 18 (CK18+) expression (Supplemental Fig. S1C). In both cell lines, tumor cells from bone metastases expressed significantly elevated $\beta 3$ levels, as compared to MFP tumor cells (Fig. 1B,C).

To assess the translational implications of this observation, we examined $\beta 3$ expression on biopsies from 42 breast cancer patients, comparing patient-matched primary tumors to bone metastases. Immunohistochemistry for $\beta 3$ was semi-quantitatively scored based on the extent and intensity of tumor-associated $\beta 3$ expression. Across nearly all patients, human bone metastases expressed significantly higher levels of tumor-associated $\beta 3$, as compared to the matching primary tumor (Fig. 2A and Supplemental Fig. S1D). Furthermore, this elevated expression of bone metastatic $\beta 3$ was observed across all breast cancer patient subtypes: luminal A, luminal B, HER2-enriched, and triple-negative (Fig. 2B).

Tumoral $\beta 3$ is induced in the bone microenvironment and mediated by TGF- β signaling

We next asked whether bone metastases express elevated $\beta 3$ due to preferential seeding and colonization of a $\beta 3^{\text{hi}}$ tumor cell subpopulation in the bone. Using fluorescence-activated cell sorting (FACS), PyMT-Bo1 cells were sorted into three different subpopulations based on surface $\beta 3$ expression: $\beta 3$ -negative cells ($\beta 3^-$), $\beta 3$ -expressing cells ($\beta 3^+$), and control cells sorted without $\beta 3$ discrimination ($\beta 3\text{-all}$). These PyMT-Bo1 subpopulations were collected and injected intracardially into separate groups of mice, which all developed bone metastases (Fig. 3A). Flow cytometry revealed that regardless of initial $\beta 3$ status, each FACS subpopulation developed into bone metastases that strongly expressed tumoral $\beta 3$ (Fig. 3B). This result demonstrates that elevated expression of bone metastatic $\beta 3$ is not due to preferential seeding of $\beta 3^{\text{hi}}$ tumor cells to the bone, and suggests that tumoral $\beta 3$ is induced in the bone microenvironment.

To ascertain pathways that might be responsible for this induction, we evaluated a panel of cytokines and growth factors present in the bone microenvironment for their effect on $\beta 3$ expression. Of the tested factors, only members of the TGF- β family upregulated integrin $\beta 3$ expression, observed in both PyMT-Bo1 and 4T1 cells (Fig. 3C,D). To assess the specificity of TGF- β -mediated upregulation of integrin $\beta 3$ as compared to other related integrin subunits, we evaluated how TGF- β alters expression of integrin αv , as well as a subfamily of β -integrin subunits that can also heterodimerize with integrin αv (integrin subunits $\beta 1$, $\beta 5$, $\beta 6$ and $\beta 8$). In addition, we evaluated integrin αIIb (glycoprotein-IIb), which is largely restricted to platelets and megakaryocyte-lineage cells but can also heterodimerize with integrin $\beta 3$ (16), and integrin $\alpha 2$, which facilitates adhesion to type I collagen and is upregulated on prostate cancer lines in response to TGF- β (38).

Collectively, we evaluated gene expression of integrin subunits $\beta 1$, $\beta 3$, $\beta 5$, $\beta 6$, $\beta 8$, αv , αIIb , and $\alpha 2$ on PyMT-Bo1 and 4T1 cells, following 24 hours of *in vitro* TGF- β stimulation. Integrin $\beta 3$ was the most upregulated subunit in both PyMT-Bo1 and 4T1 cells (Supplemental Figure S2A,B). In PyMT-Bo1 cells, integrin $\alpha 2$ was the next most

upregulated subunit, though 5-fold less than the level of $\beta 3$ induction (Supplemental Figure S2A). In 4T1 cells, $\beta 5$ and $\alpha 2$ were the next most upregulated subunits, though 4-fold less than the level of $\beta 3$ induction (Supplemental Figure S2A). TGF- β -mediated changes in αv , αIIb , and the other β -integrin subunits were either unchanged, reduced, or displayed a less-than 2-fold upregulation (Supplemental Figure S2A,B). These results provide support for TGF- β as a potent inducer of integrin $\beta 3$ as compared to these other integrin subunits.

TGF- β signals through TGF- β Receptor 1 (TGF β R1), which canonical phosphorylates the transcription factors SMAD2/SMAD3. In addition, TGF β R1 can activate 'non-canonical' signaling pathways, most commonly p38 MAP kinase (p38), MAPK/ERK Kinase-1&2 (MEK1/2), and c-Jun N-terminal kinase (JNK) (39). To evaluate how TGF- β induces $\beta 3$, tumor cells were treated with TGF- β in combination with pharmacological inhibitors for p38, MEK1/2, JNK, or TGF β R1 kinase activity at the site specific for SMAD2/SMAD3 phosphorylation (see Fig. 4 for details). In both PyMT-Bo1 and 4T1, only pharmacological inhibition of SMAD2/SMAD3 phosphorylation completely ablated $\beta 3$ upregulation. This was observed by flow cytometry for surface $\beta 3$ expression (Fig. 4A,B) and qPCR analysis for $\beta 3$ mRNA levels (Supplemental Fig. S3A). Western blot analysis confirmed selective inhibition of SMAD2/SMAD3 phosphorylation (Fig. 4C) and suppression of total $\beta 3$ protein (Fig. 4D) with TGF β R1 kinase inhibition. To determine whether TGF- β signaling was responsible for tumoral $\beta 3$ induction *in vivo*, mice bearing human MDA-MB-231 triple-negative breast cancer bone metastases were treated daily with a pharmacological TGF β R1 kinase inhibitor. TGF β R1 kinase inhibition significantly suppressed $\beta 3$ expression on MDA-MB-231 breast cancer bone metastases (Fig. 4E), demonstrating the role of TGF- β signaling in $\beta 3$ induction on breast cancer cells within the bone microenvironment. TGF β R1 kinase inhibition resulted in an approximately 1.6-fold reduction in MDA-MB-231 bone metastatic tumor burden (Supplemental Fig. S3B), consistent with a previous report (30).

Integrin $\alpha v\beta 3$ -targeted micelle nanoparticles colocalize with breast cancer bone metastases

To evaluate whether bone metastatic induction of $\beta 3$ could be therapeutically exploited, we sought to examine the potential of nanotherapy targeting integrin $\alpha v\beta 3$. We used single-lipid phospholipid/polysorbate-80 micelle nanoparticles (MPs, ~12.5 nm), coated with a well-characterized quinolone nonpeptide targeting ligand with enhanced specificity for activated $\alpha v\beta 3$ (Supplemental Fig. S4A). The specificity of this targeting ligand for integrin $\alpha v\beta 3$ has been demonstrated through a variety of assays both *in vitro* and *in vivo* (32-36) (see Materials and Methods for details). To test the effectiveness of integrin $\alpha v\beta 3$ as a target for enhancing drug delivery to bone metastases, rhodamine-labeled $\alpha v\beta 3$ -targeted MPs ($\alpha v\beta 3$ -MPs) or non-targeted MPs were administered intravenously into mice bearing PyMT-Bo1 bone metastases. Immunofluorescent analysis of bone metastases revealed strong colocalization of $\alpha v\beta 3$ -MPs with bone metastases, while non-targeted MPs displayed only minor colocalization (Fig. 5A). Furthermore, accumulation of either $\alpha v\beta 3$ -MPs or MPs within tumor-free bone marrow was negligible (Supplemental Fig. S4B). Together, these results demonstrate the targeting potential and specificity of $\alpha v\beta 3$ -MPs for bone metastases.

Next, we sought to evaluate the therapeutic efficacy of $\alpha v\beta 3$ -MP-mediated drug delivery. Nanotherapeutics often suffer from a premature loss of drug payloads during circulation and diminished intracellular drug bioavailability due to endosomal entrapment (40). To overcome these problems, a lipase-labile phospholipid-prodrug concept was employed, in which drug cargo is coupled to the Sn2 acyl-chain of phosphatidylcholine. This phospholipid-prodrug can be stably incorporated into the MP membrane during self-assembly and provides drug retention during circulation (35). Upon $\alpha v\beta 3$ -MP binding to activated $\alpha v\beta 3$ on target cells, a hemifusion complex forms between MPs and the plasma membrane, enabling endocytosis-independent “contact-facilitated drug delivery” (see Fig. 5B for details) (36,41).

The chemotherapeutic agent selected for nanoparticle-delivery was docetaxel (DTX), a potent microtubule inhibitor employed as a first-line agent against breast cancer (42). We modified DTX as an Sn2 lipase-labile phospholipid-prodrug (DTX-PD) to enable $\alpha v\beta 3$ -MP delivery (Fig. 5B) (32). *In vitro*, PyMT-Bo1 cells were markedly sensitive to both DTX and DTX-PD, with a bioequivalent IC₅₀ of 5.5 nM (Fig. 5C). Unfortunately, chemotherapeutics such as DTX rarely eradicate bone metastases in human patients (3,4) and can induce off-target toxicity such as hair loss, neuropathy, pancytopenia, and liver toxicity (42). To test the efficacy of DTX against PyMT-Bo1 cells *in vivo*, mice were intracardiac injected with PyMT-Bo1 cells. BLI analysis confirmed equivalent establishment of bone metastases on day 3 post-intracardiac injection, and mice bearing PyMT-Bo1 metastases received intravenous DTX treatments beginning on day 4 post-intracardiac injection (see Fig. 5D). Animals experienced dose-dependent DTX-induced hematological toxicity (Supplemental Fig. S5A), yet metastatic tumor burden in the liver, kidney, or bone was not attenuated by DTX treatment, and lung metastatic tumor burden was only significantly reduced at the highest DTX dose of 20 mg/kg/week (Fig. 5E). Thus, while DTX was potently suppressive against PyMT-Bo1 *in vitro*, DTX displayed limited efficacy against PyMT-Bo1 metastases *in vivo*.

$\alpha v\beta 3$ -MP-mediated drug delivery of docetaxel attenuates bone metastases

To evaluate the therapeutic potential of $\alpha v\beta 3$ -targeted delivery of DTX-PD against PyMT-Bo1 bone metastases, mice were treated with DTX, or an equimolar amount of DTX-PD encapsulated by $\alpha v\beta 3$ -MP ($\alpha v\beta 3$ -MP/DTX-PD). In parallel, two control nanoparticle treatments were evaluated to assess the *in vivo* specificity of $\alpha v\beta 3$ -MP targeting, and the specificity of docetaxel-mediated tumor-suppressive effects: non-targeted MP/DTX-PD and cargo-free $\alpha v\beta 3$ -MP without DTX-PD cargo, respectively.

As before, BLI analysis on day 3 post-intracardiac injection confirmed PyMT-Bo1 bone metastatic establishment and treatment began on day 4, with a cumulative dose of 5.55 mg/kg DTX or equimolar dose of MP-encapsulated DTX-PD (see Fig. 5D). On day 12, *ex vivo* BLI analysis of bone metastases revealed that $\alpha v\beta 3$ -MP/DTX-PD significantly attenuated bone metastatic tumor burden, while no significant attenuation was observed with DTX treatment (Fig. 6A,B). Consistent with this result, histological analysis of bone tumor burden (Fig. 6C) and x-ray analysis of tumor-associated bone loss (Fig. 6D) revealed a significant reduction with $\alpha v\beta 3$ -MP/DTX-PD treatment as compared to saline, and no

significant attenuation with DTX. BLI analysis of visceral metastases within the liver, lungs, kidneys, and brain revealed that neither $\alpha v\beta 3$ -MP/DTX-PD nor DTX resulted in significant attenuation (Supplemental Fig. S5B), supporting our previous observations concerning bone-specific $\beta 3$ expression and resistance of PyMT-Bo1 metastases to DTX.

Hepatotoxicity was tested by serum liver function tests for aspartate transaminase (AST) and alanine transaminase (ALT). DTX treatment resulted in elevated levels of AST and ALT outside of the normal ranges, while $\alpha v\beta 3$ -MP/DTX-PD treatment displayed no evidence of hepatotoxicity (Fig. 6E). Both renal function, assessed by blood urea nitrogen (BUN), and whole blood counts were within the normal range among mice treated with saline, DTX, or $\alpha v\beta 3$ -MP/DTX-PD (Fig. 6E and Supplemental Fig. S5C).

Neither non-targeted MP/DTX-PD nor cargo-free $\alpha v\beta 3$ -MP treatment significantly altered bone metastatic tumor burden or bone destruction, demonstrating the necessity of $\alpha v\beta 3$ -MP targeting and the specificity of docetaxel in mediating the tumor-suppressive effects of this nanotherapy (Supplemental Fig. S6A-D). Control $\alpha v\beta 3$ -MP treated mice displayed elevated levels of AST, but ALT, renal, and hematological toxicities were within the normal range for $\alpha v\beta 3$ -MP and non-targeted MP/DTX-PD treatments (Supplemental Fig. S6E,F).

To evaluate the potential mechanism of $\alpha v\beta 3$ -MP/DTX-PD anti-bone metastatic activity, we quantified osteoclast number at the tumor-bone interface, which was unchanged between saline, DTX, and $\alpha v\beta 3$ -MP/DTX-PD treatments (Fig. 6F), demonstrating that $\alpha v\beta 3$ -MP/DTX-PD attenuates tumor-induced bone loss independent of inhibition of osteoclast formation or osteoclast killing. To assess whether tumor cells responded to the effects of the chemotherapy, we measured tumor proliferation by immunohistochemistry for proliferating cell nuclear antigen (PCNA). Bone metastatic tumor cells treated with $\alpha v\beta 3$ -MP/DTX-PD displayed a significantly lower proliferation index than saline or DTX (Fig. 6G). Collectively, this work provides support for safer, more effective drug delivery against breast cancer bone metastases through exploitation of $\alpha v\beta 3$ expression.

Discussion

Breast cancer bone metastases often irreversibly damage the skeleton, severely impacting quality of life and overall survival (2). Treating bone metastases has proven difficult, in part due to the bone microenvironment's status as a chemo-protective niche (7), and coupled with inefficient delivery of drug to tumor cells in bone (43). While drug or nanoparticle conjugation to hydroxyapatite-avid molecules like bisphosphonates have provided positive results against mouse models of bone metastases (13,14), they lack direct specificity for tumor cells (8,15). In this study, we provide new evidence for integrin $\beta 3$ as a molecular target on breast cancer bone metastases in mice and humans, and demonstrate the potential for improving therapeutic efficacy against this metastatic site via $\alpha v\beta 3$ -targeted approaches.

We first investigated differences in the physiological expression of integrin $\beta 3$ on breast cancer tumors growing in different organs, in search of a tumor target on cells within the bone microenvironment. We demonstrated that orthotopic injection of murine breast cancer cell lines into the MFP establishes primary tumors with weak $\beta 3$ expression. Intracardiac

injection establishes metastases within the lung and kidney with similarly weak $\beta 3$ expression, but establishes bone metastases with significantly stronger $\beta 3$ expression, observed by both immunohistochemistry and flow cytometry of tumoral surface expression. In contrast, integrin αv was strongly expressed on tumors at all evaluated sites. We employed the widely-published intracardiac injection model to establish experimental bone and visceral metastases in these experiments. While this model does not recapitulate all steps of the metastatic cascade, circulating tumor cells still need to extravasate from the vessels to establish within the bone and other organs.

We also evaluated $\beta 3$ expression on 42 human bone metastatic tissue samples, as compared to matching primary breast cancer biopsies from the same patient. Across nearly all patients, tumor-associated $\beta 3$ expression was significantly higher on bone metastases. Furthermore, we show for the first time that $\beta 3$ is highly expressed on breast cancer bone metastases of all subtypes, including those with the worst overall survival that have proven difficult to target (44), supporting the translational potential of targeting $\beta 3$ in bone metastatic breast cancer patients.

Based on previous studies demonstrating that ectopic overexpression of $\beta 3$ enhances tumor cell establishment in bone (26,28), we considered the possibility that breast cancer bone metastases display elevated $\beta 3$ due to preferential bone colonization of a tumor cell subpopulation with high basal $\beta 3$ expression. We established bone metastases from FACS-sorted tumor cell subpopulations, which were initially positive or negative for basal $\beta 3$ expression. Here, we demonstrated that initial $\beta 3$ expression is dispensable for establishing breast cancer bone metastases with elevated $\beta 3$ expression. This finding does not contradict the role of tumoral $\alpha v\beta 3$ in enhancing bone colonization (26,28), as there are numerous ligands for $\alpha v\beta 3$ within the bone microenvironment (17,18); rather, it indicates that tumoral $\beta 3$ can be induced during the establishment of bone metastases, suggesting that $\beta 3$ expression might be regulated by the bone microenvironment itself.

The bone is a natural reservoir for TGF- β , which is stored in the matrix as an inactive latent complex that must be liberated for bioactivation (45). Bioactive TGF- β plays a critical role in both the homeostatic and pathologic bone microenvironment, regulating osteolytic destruction and pathologic muscle weakness (30,46). TGF- β has been shown to induce $\beta 3$ expression on normal and transformed mammary epithelial cells (47-49), but the physiological regulation of tumoral $\beta 3$ *in vivo* has not been explored. Here, we demonstrated that TGF- β strongly induces tumoral $\beta 3$, and analysis of other integrin subunits of interest revealed that TGF- β induces integrin $\beta 3$ more strongly than any other. Furthermore, we determined that TGF- β induces $\beta 3$ through TGF β RI phosphorylation of SMAD2/SMAD3, evaluated at the transcriptional, total protein, and cell surface expression level. And for the first time, we demonstrate that TGF- β signaling is required for integrin $\beta 3$ induction by breast cancer cells within the bone.

We were surprised by the lack of tumoral $\beta 3$ upregulation in the MFP tumor or visceral metastases, where TGF- β can be present. This observation suggests that other microenvironments either lack a sufficient amount of bioactive TGF- β necessary for tumoral $\beta 3$ induction, or contain inhibitors of TGF- β or SMAD2/SMAD3 signaling that prevent

TGF- β -mediated induction of tumoral β 3. Studies are in progress to define the molecular mechanism underlying the low expression of tumoral β 3 outside of the bone.

Selective elevation of β 3 on bone metastases prompted us to explore α v β 3-targeted nanotherapy as a means to overcome the barriers limiting effective treatment. We selected phospholipid/polysorbate-80 micelle nanoparticles (MPs) for their small size (~12.5 nm) and unique mechanism of drug delivery (see Fig. 5B for details), which overcomes two problems that often hinder effective nanotherapy: poor intracellular drug bioavailability and premature loss of drug during circulation (40). Micelle nanoparticles deliver phospholipid-prodrug cargo directly to the target cell's plasma membrane, where bioactive free-drug is enzymatically liberated directly into the cytoplasm by phospholipase activity (36,41). Furthermore, phospholipid-prodrug is stably incorporated into the MP-single lipid layer, thereby minimizing passive drug loss during circulation (35). Administering rhodamine-labeled MPs or α v β 3-MPs into mice bearing breast cancer bone metastases resulted in stronger α v β 3-MP colocalization with bone metastases, compared to a 6.5-fold reduction in colocalization with non-targeted MPs. To examine the importance of MP's small size in bone metastatic colocalization, we also evaluated the colocalization potential of significantly larger α v β 3-targeted perfluorocarbon nanoparticles (~250nm) (35). We observed that fluorescently-labeled α v β 3-targeted perfluorocarbon nanoparticles were much less effective at localizing to the center of bone metastases (data not shown). These observations prompted us to proceed with α v β 3-MP-mediated drug delivery, and we selected the chemotherapeutic docetaxel (DTX) as cargo for lipase-labile phospholipid-prodrug modification (DTX-PD).

While PyMT-Bo1 breast cancer cells are equally sensitive to both DTX and DTX-PD *in vitro*, PyMT-Bo1 metastases were strikingly resistant *in vivo*, with bone metastatic tumor burden essentially unaffected by DTX treatment even at the highest, most toxic dose tested (20 mg/kg/week). These observations highlight the difficulty of achieving an inhibitory dose of chemotherapy at metastatic sites *in vivo*. To test the efficacy of MP-encapsulated DTX-PD, mice bearing PyMT-Bo1 metastases were treated with a suboptimal DTX dose (5.55mg/kg/week), 3.6-fold lower than the previously tested 20 mg/kg/week DTX dose which did not significantly attenuate bone metastases. At this suboptimal dose, we observed a significant attenuation of bone metastatic tumor burden and tumor-associated bone loss with α v β 3-MP/DTX-PD treatment, as compared to no significant attenuation by equimolar DTX treatment. Furthermore, neither cargo-free α v β 3-MP treatment nor non-targeted MP/DTX-PD treatment significantly altered bone metastatic tumor burden or osteolytic bone destruction. The observation that micelle coating with the α v β 3-targeting ligand was necessary for bone metastatic colocalization, coupled with fact that α v β 3-MP/DTX-PD failed to attenuate metastases outside of β 3-expressing bone metastases, provides additional support for the *in vivo* specificity of the α v β 3-targeting ligand for integrin α v β 3, in line with previous reports (32-36).

To examine the potential mechanism of α v β 3-MP-mediated activity, we quantified osteoclast number at the tumor/bone interface, which is reflective of osteoclast formation and serves as a useful indicator of bone resorption. Previous studies have found that osteoclast formation is markedly sensitive to inhibition by DTX, even at nanomolar concentrations (50). Osteoclast number at the tumor/bone interface was similar between

$\alpha v\beta 3$ -MP/DTX-PD and saline treatment groups, demonstrating that $\alpha v\beta 3$ -MP/DTX-PD treatment attenuates bone metastases and tumor-associated bone loss independent of inhibiting osteoclast formation or direct osteoclast killing. It is possible that there remains an effect of $\alpha v\beta 3$ -MP/DTX-PD treatment on osteoclast function that was not revealed by histomorphometric analyses.

We evaluated tumor cell proliferation through expression quantification of proliferating cell nuclear antigen (PCNA), a DNA polymerase processivity factor required for DNA synthesis during replication. DTX inhibits tumor proliferation through effects on microtubule stabilization and disruption of mitotic spindle assembly (42). We found that $\alpha v\beta 3$ -MP/DTX-PD treatment significantly decreased PCNA expression on bone-residing tumor cells, as compared to saline and DTX treatment. Taken together with the osteoclast histomorphometry result, these observations suggest that $\alpha v\beta 3$ -MP/DTX-PD attenuated bone metastases due to enhanced therapeutic efficacy against bone-residing tumor cells.

We observed that DTX administration resulted in increased hepatotoxicity, while hematological values and liver function tests remained within normal limits following $\alpha v\beta 3$ -MP/DTX-PD treatment. This work thus provides support for safer, more effective drug delivery against bone metastases through exploitation of $\alpha v\beta 3$ expression on breast cancer cells within bone. Going forward, $\alpha v\beta 3$ -targeted drug cargo could be modified to fit specific treatment needs.

We recognize the limitation of $\alpha v\beta 3$ -targeted nanotherapy against breast cancer metastases outside of the bone. Nevertheless, bone metastases occur in approximately 70% of metastatic breast cancer patients and represent the only metastatic site in approximately 30% of patients, suggesting that a substantial number of patients could benefit from this approach (1,44). Collectively, we provide support for integrin $\alpha v\beta 3$ -targeted drug delivery as a bone-specific therapeutic strategy to address the unmet clinical need for effective treatments against breast cancer bone metastases.

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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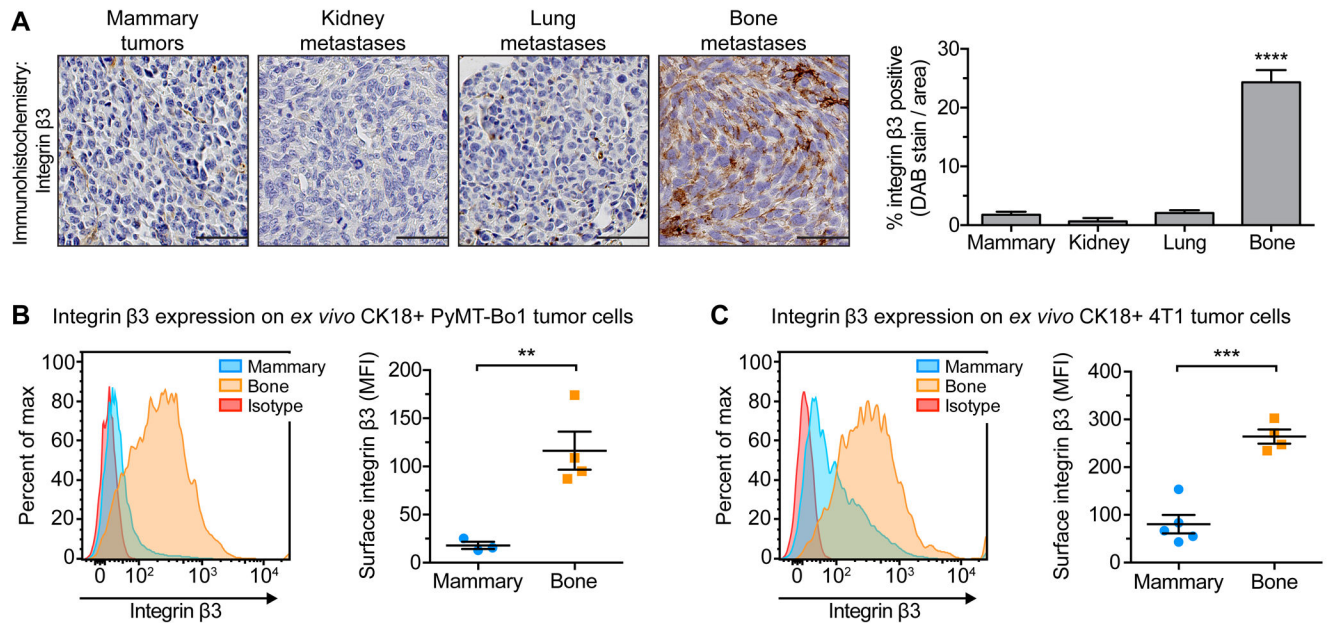


Figure 1.

Integrin $\beta 3$ is preferential induced on breast cancer cells within the bone microenvironment. (A) Immunohistochemistry for $\beta 3$ on PyMT-Bo1 mammary tumors or metastases, established by orthotopic or intracardiac injection into separate cohorts of mice, respectively. Tumors were removed 12 days post-injection. Representative images (left), quantification of DAB-stained tumors (right), $n=4$ per group. Scale=50 μm . One-way ANOVA with Tukey's post-hoc test, **** $P < 0.0001$. (B,C) Mammary tumors or bone metastases were established as previously described. Isolated tumor cells were identified based on cytokeratin 18 expression (CK18+) and evaluated by flow cytometry for surface $\beta 3$ expression. Representative samples (left). (B) PyMT-Bo1 cells, 13 days post-injection, $n=3$ mammary, $n=4$ bone. (C) 4T1 cells, 15 days post-injection, $n=5$ mammary, $n=4$ bone. Two-tailed unpaired t-test, *** $P < 0.001$, ** $P < 0.01$. Data presented as mean \pm SEM.

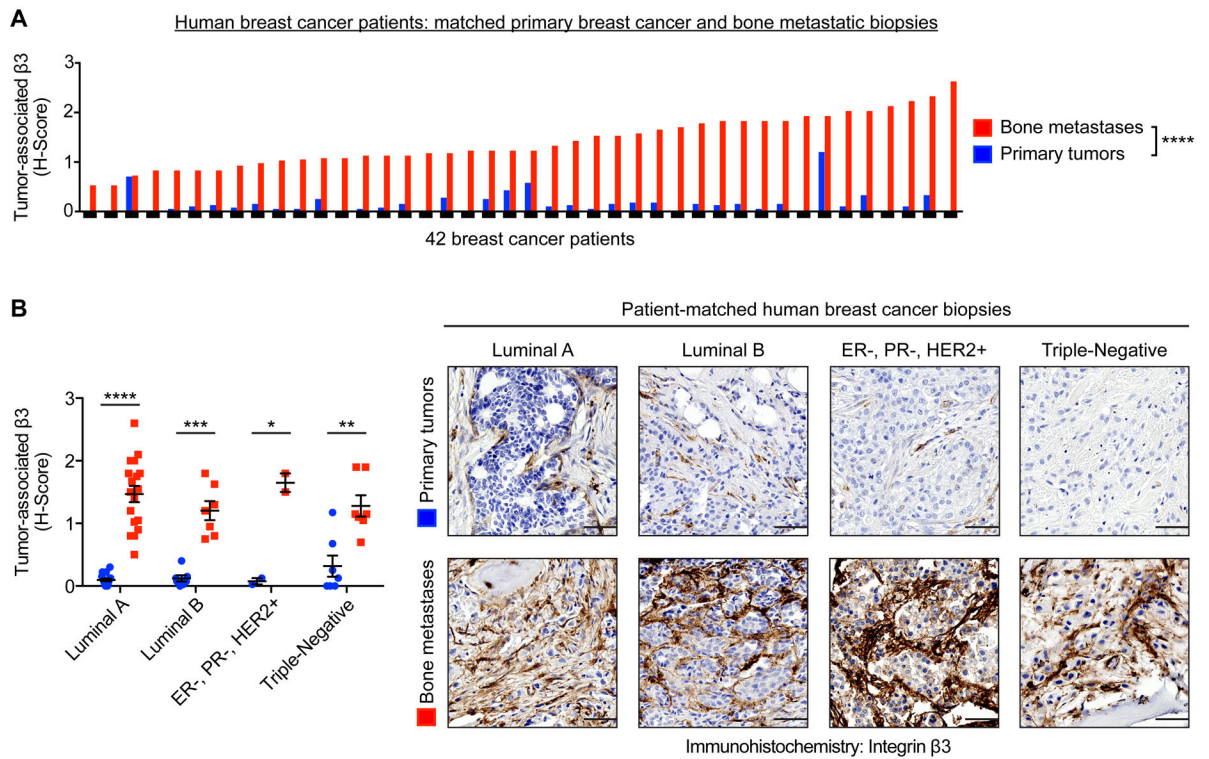


Figure 2. Immunohistochemistry for $\beta 3$ on patient-matched primary breast cancer and bone metastatic biopsies. **(A)** Semi-quantitatively analysis of the extent and intensity of tumor-associated $\beta 3$ expression, using the histoscore (H-score) system, n=42 matched-pairs, two-tailed Wilcoxon signed-rank test, **** $P < 0.0001$. **(B)** Subdivision of Fig. 2A by molecular subtype (see Materials and Methods for details). Representative images of patient-matched primary tumors and bone metastases (right). Scale=50 μm . Two-tailed paired t-test, **** $P < 0.0001$, *** $P < 0.001$, ** $P < 0.01$, * $P < 0.05$. Data presented as mean \pm SEM.

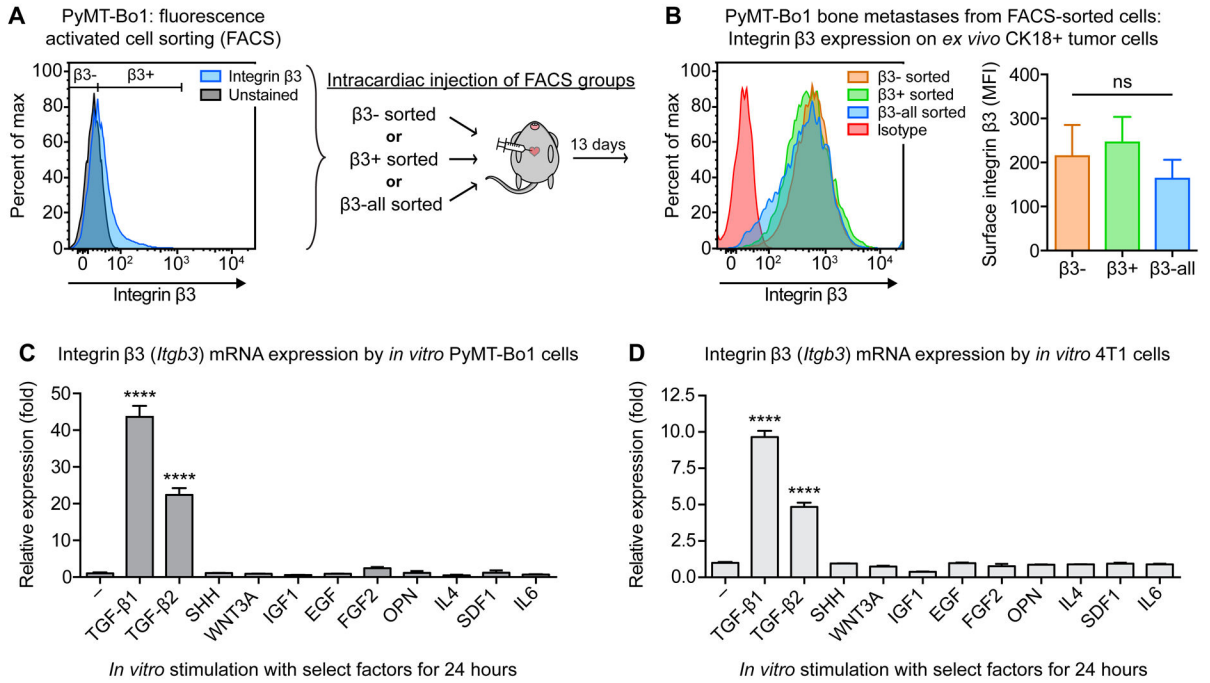


Figure 3.

Bone microenvironment and TGF- β stimulation induce tumoral $\beta 3$. **(A)** *In vitro* PyMT-Bo1 cells were FACS sorted into three groups based on basal $\beta 3$ expression: $\beta 3^-$, $\beta 3^+$, and control $\beta 3$ -all. Immediately after collection, cells were intracardiac injected into separate groups of mice. **(B)** 13 days post-injection, isolated bone metastatic PyMT-Bo1 cells were identified by CK18+ and evaluated by flow cytometry for surface $\beta 3$ expression.

Representative samples (left), n=4 $\beta 3^-$, n=4 $\beta 3$ -all, n=5 $\beta 3^+$ (right). One-way ANOVA with Tukey's post-hoc test, ns=(not significant). **(C,D)** qPCR analysis of $\beta 3$ (*Itgb3*) mRNA expression by PyMT-Bo1 or 4T1 cells cultured *in vitro*, following 24 hours stimulation with the listed factors (see Materials and Methods for details). One of two biological replicates, each in technical duplicate. One-way ANOVA with Tukey's post-hoc test, **** $P < 0.0001$. Data presented as mean \pm SEM.

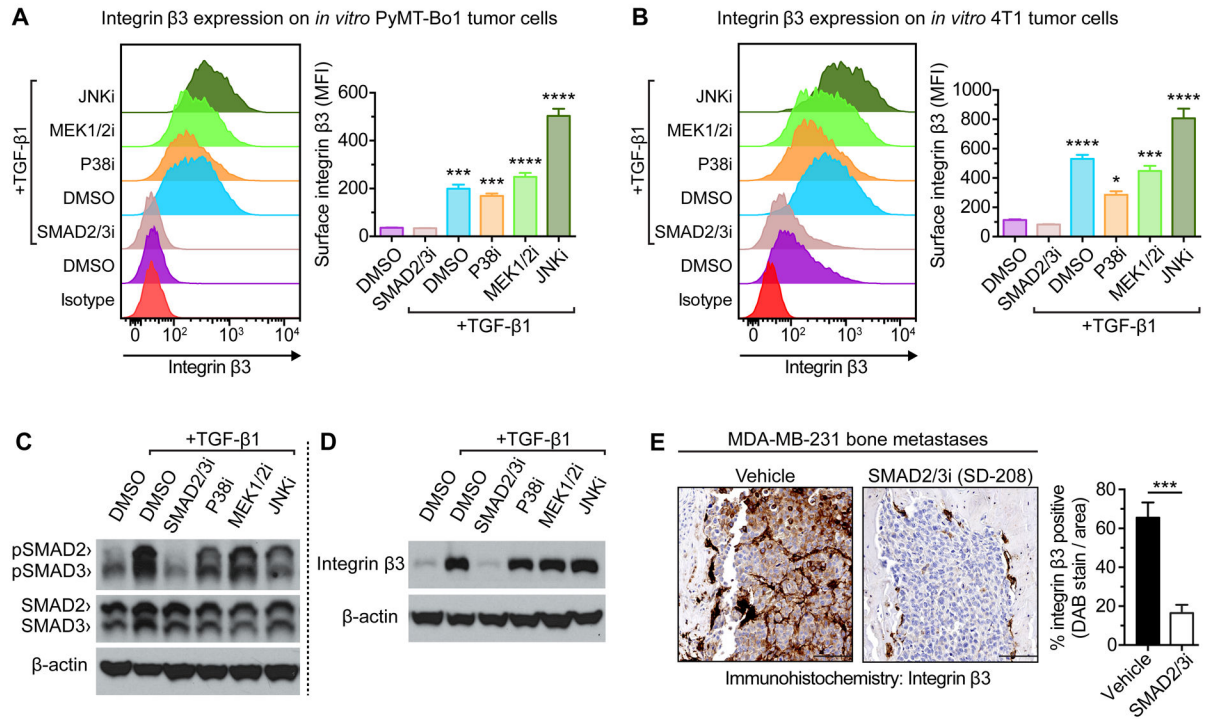


Figure 4.

TGF- β induces tumoral $\beta 3$ through TGF β RI-mediated phosphorylation of SMAD2/SMAD3. (**A,B**) *In vitro* tumor cells treated with either 2 ng/mL TGF- $\beta 1$ or DMSO control, in the presence of a pharmacological inhibitor: SMAD2/3i (20 μ M SB431542), MEK1/2i (20 μ M U0126), p38i (20 μ M SB203580), or JNKi (50 μ M SP600125). After 48 hours, flow cytometry for surface $\beta 3$ expression was evaluated on (**A**) PyMT-Bo1 cells, or (**B**) 4T1 cells. Representative experiment (left), n=3 biological replicates (right). One-way ANOVA with Tukey's post-hoc test, with denoted significance in relation to DMSO control, **** $P < 0.0001$, *** $P < 0.001$, * $P < 0.05$. (**C,D**) Western blot analysis of *in vitro* PyMT-Bo1 cells treated as previously described, for (**C**) 3 hours, or (**D**) 24 hours. (**E**) Mice intracardiac injected with MDA-MB-231 cells were treated daily with a TGF β RI kinase inhibitor of SMAD2/3 phosphorylation (SD-208, 60 mg/kg/d) or vehicle control (1% methylcellulose) for 28 days. Immunohistochemistry for $\beta 3$ with representative images (left) and quantification of DAB-stained bone metastases, n=4 (right). Scale=100 μ m. Two-tailed unpaired t-test, *** $P < 0.001$. Data presented as mean \pm SEM.

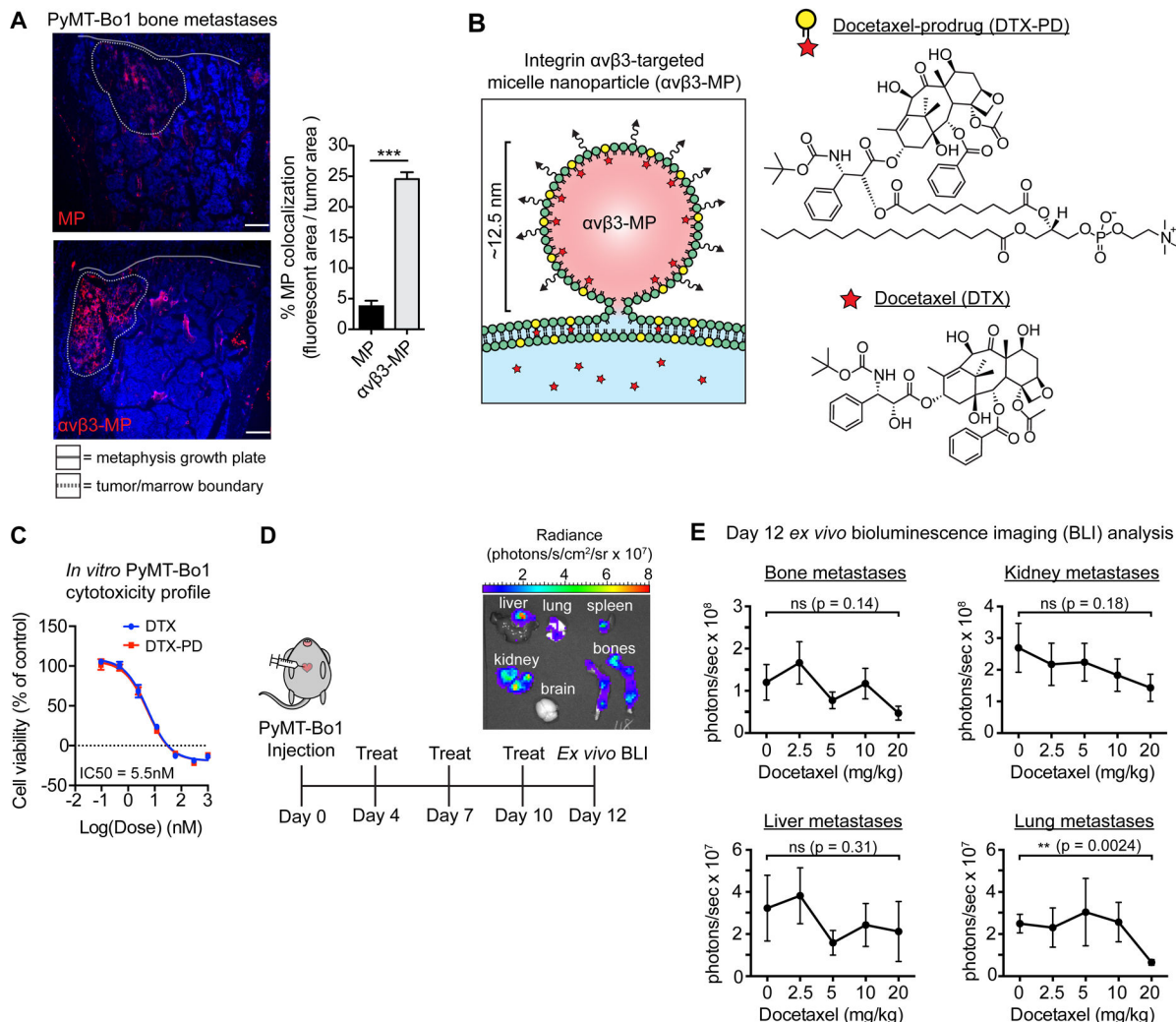


Figure 5. Micelle nanoparticles targeting integrin $\alpha v \beta 3$ colocalize with breast cancer bone metastases and are designed to carry the chemotherapeutic docetaxel. **(A)** Mice bearing PyMT-Bo1 bone metastases were intravenously injected with rhodamine-labeled (red) non-targeted MPs or $\alpha v \beta 3$ -MPs. After 3 hours, bones were removed and fresh-frozen sections were immunofluorescently imaged. DAPI nuclear counterstain (blue). Representative images (left), quantification of fluorescent colocalization with the bone metastases, $n=3$ per group (right). Scale=200 μm . Two-tailed unpaired t-test, *** $P<0.001$. **(B)** Schematic of $\alpha v \beta 3$ -MP-mediated “contact-facilitated drug delivery.” Upon hemifusion, phospholipid-conjugated docetaxel-prodrug (DTX-PD) transfers to the target cell’s plasma membrane, where bioactive DTX is enzymatically liberated by phospholipases and released directly into the cytoplasm. **(C)** *In vitro* PyMT-Bo1 cell viability via MTT assay after 72 hours of DTX or DTX-PD treatment. $n=2$ biological replicates, each in technical triplicate. **(D)** Treatment schematic of mice intracardiac injected with PyMT-Bo1 cells. Representative *ex vivo* BLI of tumor-bearing organs on day 12. **(E)** Following the schematic in Fig. 5D, mice were treated

with increasing concentrations of docetaxel, with the cumulative dose as indicated. Day 12 *ex vivo* PyMT-Bo1 metastatic tumor burden by BLI analysis, n=6. Bone, Kidney, Lung: two-tailed unpaired t-test. Liver: two-tailed Mann–Whitney *U*-test. All with Bonferroni correction for *a priori* multiple comparisons between control 0 mg/kg and each DTX treatment group, ** $P < (0.01/4)$, * $P < (0.05/4)$, ns=(not significant). Data presented as mean \pm SEM.

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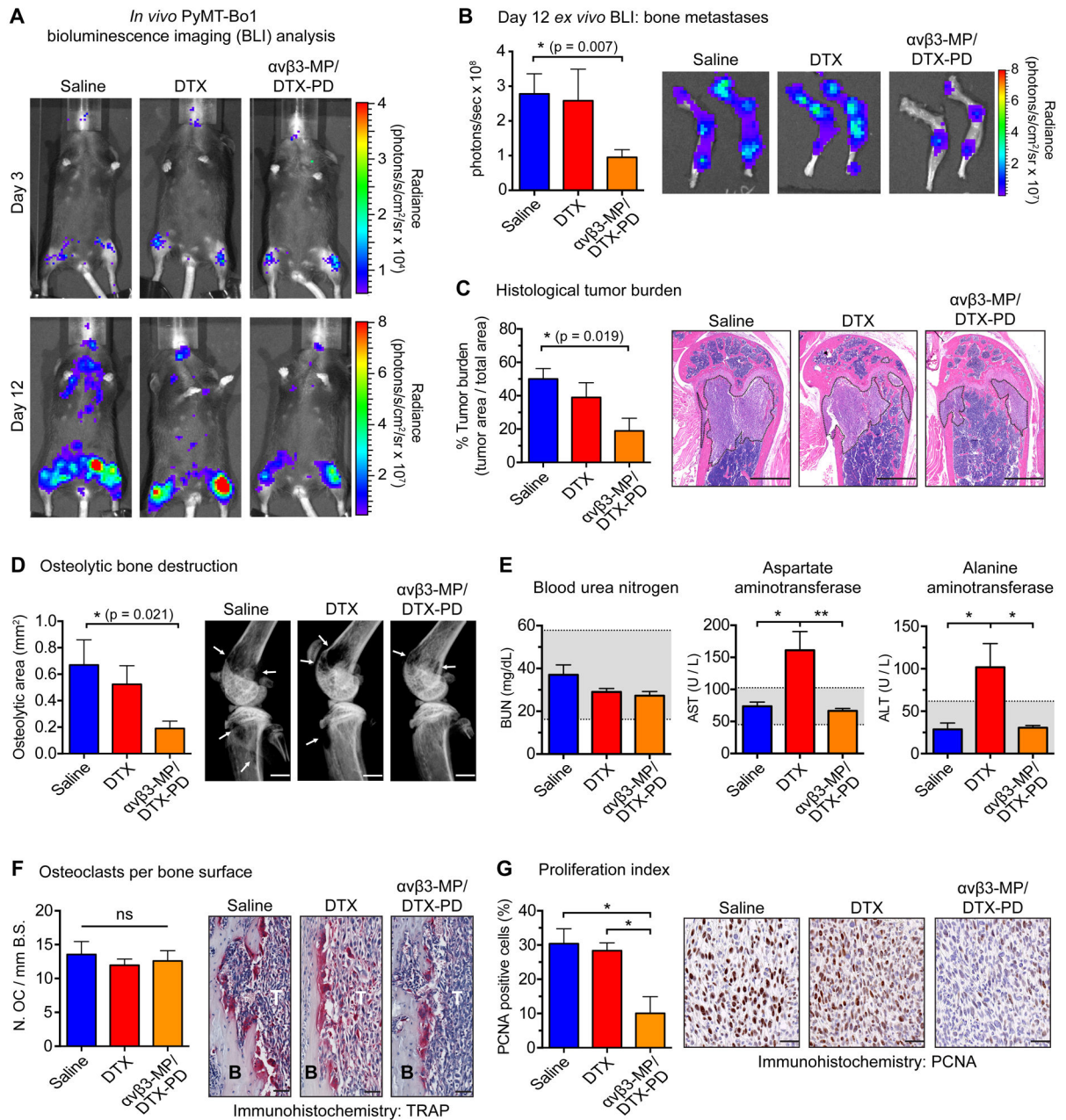


Figure 6. Integrin $\alpha v \beta 3$ -targeted nanotherapy attenuates breast cancer bone metastases. Following the schematic described in Fig. 5D, mice were treated with either a cumulative dose of 5.55 mg/kg docetaxel (DTX), an equimolar dose of docetaxel-prodrug encapsulated by $\alpha v \beta 3$ -MP ($\alpha v \beta 3$ -MP/DTX-PD), or saline. Analyses completed on samples collected on day 12 post-injection. (A) Representative *in vivo* BLI of mice bearing PyMT-Bo1 bone metastases, matching day 3 and day 12 post-injected mice from each group (B) *Ex vivo* PyMT-Bo1 bone metastatic tumor burden by BLI analysis, n=9. (C) Histological analysis of tumor burden within the tibiofemoral joint, n=4. (D) X-ray analysis of osteolytic bone destruction, n=9.

(B-D) Scale=1 mm, two-tailed unpaired t-test with Bonferroni correction for *a priori* multiple comparisons between saline and each experimental treatment, * $P < (0.05/2)$. **(E)** Serum chemistry analysis of BUN, AST, and ALT, n=5. Gray range illustrates the normal reference range (mean \pm 2*SD) for female C57BL/6 mice bearing PyMT-Bo1 metastases. **(F)** TRAP staining for quantification of osteoclast number per millimeter of bone surface (N.OC/mmB.S.) at the tumor (T), bone (B) interface, n=4. **(G)** Quantification of PCNA-positive cells within the bone metastatic region, n=3. **(F-G)** Scale=50 μ m, one-way ANOVA with Tukey's post-hoc test, ** $P < 0.01$, * $P < 0.05$, ns=(not significant). All images are representative and data presented as mean \pm SEM.