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# Pharmacological profiling of sigma 1 receptor ligands by novel receptor homomer assays

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# Abstract

The sigma 1 receptor ( $\sigma_1 R$ ) is a structurally unique transmembrane protein that functions as a molecular chaperone in the endoplasmic reticulum (ER), and has been implicated in cancer, neuropathic pain, and psychostimulant abuse. Despite physiological and pharmacological significance, mechanistic underpinnings of structure-function relationships of  $\sigma_1 R$  are poorly understood, and molecular interactions of selective ligands with  $\sigma_1 R$  have not been elucidated. The recent crystallographic determination of  $\sigma_1 R$  as a homo-trimer provides the foundation for mechanistic elucidation at the molecular level. Here we report novel bioluminescence resonance energy transfer (BRET) assays that enable analyses of ligand-induced multimerization of  $\sigma_1 R$  and its interaction with BiP. Haloperidol, PD144418, and 4-PPBP enhanced  $\sigma_1 R$  homomer BRET signals in a dose dependent manner, suggesting their significant effects in stabilizing  $\sigma_1 R$ multimerization, whereas (+)-pentazocine and several other ligands do not. In non-denaturing gels, (+)-pentazocine significantly decreased whereas haloperidol increased the fraction of  $\sigma_1 R$ multimers, consistent with the results from the homomer BRET assay. Further, BRET assays examining heterometric  $\sigma_1$ R-BiP interaction revealed that (+)-pentazocine and haloperidol induced opposite trends of signals. From molecular modeling and simulations of  $\sigma_1 R$  in complex with the tested ligands, we identified initial clues that may lead to the differed responses of  $\sigma_1 R$  upon binding of structurally diverse ligands. By combining multiple in vitro pharmacological and in

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Author contribution: HY and LS designed the study. AB performed the binding assays; HY carried out the BRET assays; MX and ADF performed molecular docking and dynamics simulations; WCH and SNS designed and performed non-denaturing gel assays; DAG performed the  $pK_a$  titrations; MX, ADF, AMA, and LS analyzed the modeling results, HY, AB, MX, WCH, AHN and LS interpreted the experimental results; HY and LS wrote the initial draft, with all authors participating in revising the manuscripts.

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*silico* molecular biophysical methods, we propose a novel integrative approach to analyze  $\sigma_1 R$ ligand binding and its impact on interaction of  $\sigma_1 R$  with client proteins.

# Keywords

sigma 1 receptor; BRET; assay development; (+)-pentazocine; haloperidol; BiP

# 1. Introduction

The sigma 1 receptor ( $\sigma$ 1R) is an intriguing transmembrane protein that does not share sequence homology to any known eukaryotic protein family, except for a fungal sterol isomerase (Hanner et al., 1996). It has been characterized as a molecular chaperone in the endoplasmic reticulum (ER) (Hayashi and Su, 2007), and may be a promising therapeutic target for several neuropsychiatric disorders (Kourrich et al., 2012; Maurice and Su, 2009). In addition,  $\sigma_1 R$  has been shown to be involved in pain (Romero et al., 2016; Sanchez-Fernandez et al., 2017), psychostimulant abuse (Katz et al., 2017; Sabino et al., 2017), and neurodegenerative diseases (Maurice and Goguadze, 2017; Nguyen et al., 2017) among others (Albayrak and Hashimoto, 2017; Soriani and Rapetti-Mauss, 2017; Wang et al., 2017). Depending on the physiological readout,  $\sigma_1 R$  ligands have been described as "agonists" or "antagonists", as for G-protein coupled receptors (GPCRs). For instance,  $\sigma_1 R$ "antagonists" demonstrate efficacy in counteracting neuropathic pain (Romero et al., 2016) and drug seeking behavior in stimulant abuse (Katz et al., 2017), whereas  $\sigma_1 R$  "agonists" display favorable effects in depression (Fishback et al., 2010). However, it is worth noting that the efficacy distinction between "agonist" and "antagonist" has not reached consensus in a therapeutic context. For instance, in the development of antipsychotics both an "antagonist" (Ferris et al., 1986; Gilmore et al., 2004) and an "agonist" (Albayrak and Hashimoto, 2017) have been found to be beneficial. Furthermore, the underlying molecular mechanistic differences between agonists and antagonists have not been well characterized across different pathological contexts (Katz et al., 2016; Merlos et al., 2017), and it must be noted that some of the observations and interpretations are not monolithic (Katz et al., 2017). For example, the  $\sigma_1 R$  ligand BMY 14802 was characterized as both an antagonist and an agonist (Schoenwald et al., 1995; Taylor et al., 1993). This discrepancy can be attributed to readouts and interpretations at different downstream effector levels. Indeed only a few studies have evaluated the efficacy of  $\sigma_1 R$  ligands specifically at the level of  $\sigma_1 R - \sigma_1 R$ interaction (Gomez-Soler et al., 2014; Gromek et al., 2014; Mishra et al., 2015).

 $\sigma_1 R$  has a multitude of client proteins and the interactions with them may influence the nature of ligand action and signaling outcome (Su et al., 2016). Thus, client protein coupling and subsequent effector activation or inactivation have been reported as the major biological function of  $\sigma_1 R$  (Su et al., 2016). Among the different client proteins, in particular, binding immunoglobulin protein (BiP), also known as heat shock 70 kDa protein 5, has been well-characterized (Ha et al., 2014; Miki et al., 2015; Ono et al., 2013; Penas et al., 2011) and shown to regulate ER-originated events such as calcium release and receptor trafficking (Hayashi and Su, 2007).

To understand the molecular mechanism of ligands on  $\sigma_1 R$ , simplified signalingindependent methods are expected to better categorize the ligands, which may require going beyond the canonical agonist/antagonist definitions. In light of recent studies on  $\sigma_1 R$ homomerization in response to a variety of ligands (Gromek et al., 2014; Mishra et al., 2015), ligand-induced changes on receptor multimerization state may provide at least qualitative criterion for functional categorization. Recent crystal structures of ligand-bound  $\sigma_1 R$ , which are solved in homo-trimers, have revealed its transmembrane topology as well as the ligand binding site (Schmidt et al., 2016). Even though discrepancies with previous reports with regard to the structural topology (Ortega-Roldan et al., 2015; Ossa et al., 2017) remain, the high-resolution structural information revealed by the crystal structures sets the path to fundamental understanding of biophysical and pharmacological properties of  $\sigma_1 R$  at the molecular level. Specifically, the identification of the homomerization interface provides a framework to design the constructs that are feasible to study the ligand-induced changes of multimerization state with pharmacological assays.

The bioluminescence resonance energy transfer (BRET) assay is a reliable protein-protein proximity assay. The methodology is capable of uncovering both distance changes between two proteins (Pfleger et al., 2006), and large conformational rearrangements within a protein such as ligand-induced conformational changes of GPCRs (Lohse et al., 2012). Importantly, BRET is suited for real-time kinetic tracking of the movements of labeled proteins. Here we develop novel BRET assays to characterize the ligand-induced changes in the homomerization of  $\sigma_1 R$  and its interaction with BiP. The findings in  $\sigma_1 R$  homomer BRET assay were validated by a biochemical assay, and were further shown to correlate with the results from computational modeling. Herein, we report the pharmacological characterizations of 8 known  $\sigma_1 R$  ligands in a signaling-independent manner.

# 2. Materials and methods

# 2.1. σ<sub>1</sub>R radioligand binding in guinea pig cortex

Male Hartley guinea pig cortices were dissected from freshly harvested brains (shipped cold in phosphate-buffered saline (PBS) buffer from BioReclamation IVT) and frozen at -80 °C for future use. On test day, thawed guinea pig cortices were suspended and homogenized in 20 volumes (w/v) (10 mM Tris.HCl, 0.32M Sucrose, pH 7.4 at 25 °C) with a glass-teflon apparatus and centrifuged (~1,200 rpm) for 10 min at 4 °C. The supernatant was collected in a clean tube and the pellet re-suspended in 10 ml of cold buffer and centrifuged again  $(\sim 1,200 \text{ rpm})$  for 10 min at 4 °C. The supernatants were pooled together and centrifuged (20,000 rpm) for 15 min at 4 °C. The final pellet was suspended in ice-cold binding buffer at 50 mg/ml concentration (original wet weight). A Bradford protein assay (Bio-Rad, Hercules, CA) was used to determine the protein concentration present in the tissue preparation (1.25 mg/ml). All test compounds were freshly dissolved in 30% DMSO and 70% H<sub>2</sub>O to a stock concentration of 1 mM or 100  $\mu$ M. To assist the solubilization of free-base compounds, 10  $\mu$ l of glacial acetic acid was added along with the DMSO (in place of  $10 \,\mu$ l final H<sub>2</sub>O volume). Each test compound was then diluted into 10 half-log serial dilutions using 30% DMSO as the vehicle. Radioligand competition experiments were conducted in 96-well plates containing 300 µl fresh binding buffer, 50 µl of diluted test compound, 100 µl of tissue

preparation (125  $\mu$ g/well total protein amount), and 50  $\mu$ l of radioligand diluted in binding buffer ([<sup>3</sup>H]-(+)-pentazocine: 3 nM final concentration, ARC, Saint Louis, MO). Nonspecific binding was determined using 10 µM PRE-084 and total binding was determined with 30% DMSO vehicle (3% DMSO final concentration). All compound dilutions were tested in triplicate and the competition reactions started with the addition of the tissue preparation and incubated for 120 min at room temperature. The reaction was terminated by filtration through Perkin Elmer Uni-Filter-96 GF/B, presoaked for 120 min in 0.05% polyethylenimine, using a Brandel 96-Well Plates Harvester Manifold (Brandel Instruments, Gaithersburg, MD). The filters were washed 3 times with 3 ml ( $3 \times 1$  ml/well) of ice cold binding buffer. 65 µL Perkin Elmer MicroScint 20 Scintillation Cocktail was added to each well and filters were counted using a Perkin Elmer MicroBeta Microplate Counter (calculated efficiency: 31%). IC50 values for each compound were determined from inhibition curves and  $K_i$  values were calculated using the Cheng-Prusoff equation;  $K_d$  values for  $[{}^{3}H]$ -(+)-pentazocine ( $\sigma_{1}R$ : 5.18 nM) and  $B_{max}$  (1091 fmol/mg) were determined via separate homologous competitive binding experiments.  $K_i$  values were determined from at least 3 independent experiments and are reported as mean  $\pm$  SEM.

# 2.2. σ<sub>1</sub>R radioligand binding in HEK293 cell membranes

HEK293T cells were grown as described below in section 2.4. Upon reaching 80-90% confluence, non-transfected HEK293T cells were harvested using pre-mixed Earle's Balanced Salt Solution (EBSS) with 5 mM EDTA (Life Technologies) and centrifuged at 3,000 rpm for 10 min at 21 °C. The supernatant was removed and the pellet was resuspended in 10 mL hypotonic lysis buffer (5 mM MgCl<sub>2</sub>, 5 mM Tris, pH 7.4 at 4 °C) and centrifuged at 20,000 rpm for 30 min at 4 °C. The pellet was then resuspended in fresh EBSS binding buffer made from 8.7 g/L Earle's Balanced Salts without phenol red (US Biological, Salem, MA) and 2.2 g/L sodium bicarbonate, pH to 7.4. A Bradford protein assay (Bio-Rad, Hercules, CA) was used to determine the protein concentration. On test day, the experiments were conducted in 96-well plates containing 300 µL fresh binding buffer, 50 µL of diluted test compound, 100 µL of membranes (100 µg/well total protein), and 50 µL of radioligand diluted in binding buffer ([<sup>3</sup>H]-(+)-pentazocine: 3 nM final concentration, [<sup>3</sup>H]-haloperidol: 2 nM final concentration, Saint Louis, MO). Nonspecific binding was determined using 10 µM (+)-pentazocine or 10 µM haloperidol, respectively (final concentrations), and total binding was determined with 30% DMSO vehicle (3% DMSO final concentration). All compound dilutions were tested in triplicate and the reactions incubated for 120 min at room temperature. The reactions were terminated by filtration through Perkin Elmer Uni-Filter-96 GF/B, presoaked for 120 min in 0.5% polyethylenimine, and the filters counted as described above (calculated efficiency 31% and 29% for [<sup>3</sup>H]-(+)-pentazocine and [<sup>3</sup>H]-haloperidol, respectively).  $K_d$  ( $\sigma_1$ R: 7.76 nM) and B<sub>max</sub> (2080 fmol/mg) for [<sup>3</sup>H]-(+)-pentazocine, as well as  $K_d$  ( $\sigma_1 R$ : 9.25 nM) and  $B_{max}$  (5784 fmol/mg) for [<sup>3</sup>H]-haloperidol, were determined via separate homologous competitive binding experiments. Ki values were determined from at least 3 independent experiments and are reported as mean  $\pm$  SEM.

# 2.3. [<sup>3</sup>H]-(+)-Pentazocine association kinetics and competition kinetics by other $\sigma_1 R$ ligands

Membranes from non-transfected HEK293T were collected as described above. HEK293T cells, either intact or transfected with  $\sigma_1$ R-Venus and  $\sigma_1$ R-NanoLuciferase, were harvested using pre-mixed Earle's Balanced Salt Solution (EBSS) with 5 mM EDTA (Life Technologies) and centrifuged at 1,200 rpm for 5 min at 21 °C to prevent cell lysis. The supernatant was removed and the pellet was then resuspended in fresh EBSS binding buffer made from 8.7 g/L Earle's Balanced Salts without phenol red (US Biological, Salem, MA) and 2.2 g/L sodium bicarbonate, pH to 7.4. A Bradford protein assay (Bio-Rad, Hercules, CA) was used to determine the protein concentration. The experiments were conducted in 96-well plates containing 300 µl fresh binding buffer, 50 µl of 30% DMSO vehicle (3% DMSO final concentration for total binding) or  $10 \,\mu$ M (+)-pentazocine (final concentration for non-specific binding), 100 µl of membranes or whole cell preparation (100 µg/well total protein), and 50  $\mu$ l of radioligand diluted in binding buffer ([<sup>3</sup>H]-(+)-pentazocine: 3 nM final concentration). The reactions were incubated at room temperature and terminated by filtration through Perkin Elmer Uni-Filter-96 GF/B (presoaked in 0.5% polyethylenimine) at different time points. Non-specific binding was subtracted from the total binding at each time point and the obtained specific binding values were normalized to the maximum specific binding achieved at 120 min. T<sub>1/2</sub> values represent the time necessary to obtain 50% of the radioligand bound. Bmax values (membranes: 871 fmol/mg; whole non-transfected cells: 1041 fmol/mg and BRET-transfected cells: 4289 fmol/mg) were calculated as well from the association kinetic experiments. All the values were determined from at least 3 independent experiments performed in triplicate and are reported as mean  $\pm$  SEM. For time dependent specific competition of  $\sigma_1 R$  ligands in different cell preparations versus [<sup>3</sup>H]-(+)pentazocine, HEK293 membranes, whole non-transfected cells and whole BRET-transfected cells were collected as described above. Each test compound was tested for its ability to displace the total amount of radioligand bound at different time points. The concentration used for each compound was determined as the minimum concentration necessary to fully compete with the radioligand at the equilibrium (120 min). The experiments were conducted in 96-well plates containing 300 µl fresh binding buffer (8.7 g/L Earle's Balanced Salts without phenol red and 2.2 g/L sodium bicarbonate, pH to 7.4.), 50 µl of 30% DMSO vehicle (3% DMSO final concentration for total binding) or the drug dilution at the desired concentration, 100 µl of membranes or whole cell preparation (100 µg/well total protein), and 50 µl of radioligand diluted in binding buffer ([<sup>3</sup>H]-(+)-pentazocine: 3 nM final concentration). The reactions were incubated at room temperature and terminated by filtration through Perkin Elmer Uni-Filter-96 GF/B (presoaked in 0.5% polyethylenimine) at different time points. For each time point the amount of specific binding was normalized to 100% (total specific binding in presence of the vehicle) and 0% (residual radioligand bound in presence of 500 nM (+)-pentazocine). The data represent the average of two independent experiments with triplicate determinations for each drug concentration at the different time points. The multiple statistical comparison was obtained by two-way ANOVA followed by post-hoc Tukey analysis.

# 2.4. DNA constructs, transfection, and cell culture

Human  $\sigma_1 R$  is fused in pcDNA3.1 plasmid to the NanoLuciferase fragments, full length NanoLuciferase (NL), or mVenus (VN; monomeric YFP variant) N-terminally or Cterminally by introduction of restriction enzyme site to generate the following constructs. The N-terminal fragment (NL1) or C-terminal fragment (NL2) of NanoLuciferase is subcloned as follows: KpnI-NL1-BamHI- $\sigma_1 R$ , KpnI-NL2-BamHI- $\sigma_1 R$ ,  $\sigma_1 R$ -BamHI-NL1-XhoI,  $\sigma_1 R$ -BamHI-NL2-XhoI. Full length NanoLuciferase or mVenus is subcloned as follows: KpnI-NL-BspEI- $\sigma_1 R$ , NheI-VN-HindIII- $\sigma_1 R$ ,  $\sigma_1 R$ -XhoI-VN-XbaI,  $\sigma_1 R$ -XhoI-NL-XbaI. N-terminal fusion of FLAG-2×His<sub>8</sub> to  $\sigma_1 R$  is made as previously described (Hong et al., 2017). Human BiP is fused in pcDNA3.1 plasmid to venus as follows: NheI-VN-HindIII-BiP, BiP-XhoI-VN-XbaI. All the constructs were confirmed by sequence analysis.

For luciferase complementation, a constant amount of total plasmid (2  $\mu$ g) was transfected in human embryonic kidney cells 293T (HEK 293T) using polyethylenimine (PEI; Sigma-Aldrich, St. Louis, MO) in a 1 to 2 ratio in 6-well plates. For acceptor saturating BRET, using PEI, a constant amount of total plasmid cDNA (5  $\mu$ g) in varied donor:acceptor ratios was transfected in HEK 293T in 6-well plates. For drug induced BRET, a constant amount of total plasmid cDNA (15  $\mu$ g) in 1:24 (= donor:acceptor ratio) was transfected using PEI. Cells were maintained in culture with Dulbecco's modified Eagle's medium supplemented with 10% fetal bovine serum and kept in an incubator at 37 °C and 5% CO<sub>2</sub>. Experiments were performed approximately 48 h post-transfection.

# 2.5. Luciferase complementation and bioluminescence resonance energy transfer (BRET)

Luciferase complementation is conducted as follows. Cells were harvested, washed, and resuspended in PBS. Approximately 200,000 cells/well were distributed in 96-well plates. Luminescence was measured at 485 nm using a Mithras LB940 reader (Berthold Technologies, Bad Wildbad, Germany).

Acceptor saturating BRET is performed as described previously (Sohy et al., 2009). Briefly, after cell resuspension and distribution in 96-well plates as described in luciferase complementation, expression of venus fusion proteins was estimated by measuring fluorescence at 535 nm following excitation at 485 nm. Expression of NL fusion proteins was estimated by measuring the luminescence of the cells after incubation with 5  $\mu$ M coelenterazine h. In parallel, BRET was measured as a ratio between measurements at 535 nm (fluorescence) and at 485 nm (luminescence) using a Mithras LB940 reader (Berthold Technologies, Bad Wildbad, Germany). Results are plotted as fluorescence over luminescence vs. basal-subtracted BRET ratio.

Drug induced BRET is conducted as reported previously (Urizar et al., 2011). Cells were prepared in 96-well plates as in acceptor saturating BRET. 5  $\mu$ M coelenterazine h (substrate for BRET) was added to each well. Three minutes after addition of coelenterazine h, ligands [(+)-pentazocine (Sigma), PRE-084 (Tocris), NE100 (Tocris), JHW007 (Newman lab), cocaine (NIDA), PD144418 (Tocris), haloperidol (Tocris), 4PPBP (Tocris)] in series of dilution were added to each well. BRET was measured as in acceptor saturating BRET. Results are calculated for the BRET change (BRET ratio for the corresponding drug minus

BRET ratio in the absence of the drug).  $E_{max}$  values are expressed as the basal subtracted BRET change in the dose-response graphs.

### 2.6. Non-denaturing gel assay

As previously described (Hong et al., 2017), HEK293 cells were stably transfected with Nterminal FLAG-2×His<sub>8</sub> tagged  $\sigma_1 R$  (FH- $\sigma_1 R$ ). Confluent cells in 24-well plates were first incubated with haloperidol or vehicle at 37 °C for 0.5 h in culture medium, followed by addition of (+)-pentazocine (if indicated) and incubation at 37 °C for 1 h. Cells were then washed with cold PBS with 1 mM MgCl<sub>2</sub> and 0.1 mM CaCl<sub>2</sub> (PBSCM), harvested and lysed with lysis buffer (0.1% glyco-diosgenin, NaCl 150 mM, EDTA 1 mM, Tris 50 mM, pH 7.5, and protease inhibitors) for 2 h at 4 °C. Supernatants after centrifugation (20,000 *g*, 10 min) were mixed with 2× sample buffer (8% perfluorooctanoic acid (PFO), 40% glycerol, bromophenol blue 0.005%, Tris 100 mM, pH 7.5) to a final concentration of 4% PFO, and heated at 37 °C for 10 min. Samples were run in 5-15% polyacrylamide Tris-glycine gels (running buffer: 0.1% PFO, 25 mM Tris, 192 mM glycine, pH 8.3). Proteins were transferred to PVDF membranes and immunoblotted with rat monoclonal anti-Flag L5 antibody (Biolegend, San Diego, CA).

### 2.7. Data analysis

All experiments were repeated at least three times. Regression and other statistical analyses were performed using GraphPad Prism version 7.0 (GraphPad Software, San Diego, CA).

### 2.8. Molecular docking and simulations

The crystal structure of  $\sigma_1 R$  in complex with PD144418 ( $\sigma_1 R$ /PD144418, PDB ID 5HK1 (Schmidt et al., 2016)) was used as the starting point for our modeling studies. Except for PD144418, all other compounds described in this study were docked into the binding site revealed by the crystal structure using the induced-fit docking (IFD) protocol (Sherman et al., 2006) implemented in the Schrodinger suite (release 2016-4). Since all of these compounds, except for PRE-084, possess a nitrogen that should be protonated at pH 7, they are expected to form a salt bridge with Glu172 in the binding site. The  $pK_a$  of the nitrogen on PRE-084 was calculated to be  $5.82 \pm 1.47$  at pH 7 (which is consistent with the experimentally measured value of 6.2, see text), using the Epik protocol in the Schrodinger suite (release 2016-4). However, PRE-084 was still prepared as the protonated form since the protonation is likely to happen in the micro-environment of the binding site (see Supplementary Method and Supplementary Results). Therefore, the formation of the salt bridge was used as a filter for the docking poses. We considered all stereoisomers for each ligand, including those for the phenylcyclohexane ring of PRE-084, and those resulting from two possible ways in protonating the aforementioned nitrogen for haloperidol, 4-PPBP, cocaine, (+)-pentazocine, and JHW007. Several poses for each ligand or stereoisomer with significantly different orientations in the binding site were further evaluated by binding pose metadynamics simulations (Clark et al., 2016) in which the ligand RMSD deviation from the starting pose was set to be the collective variable. Poses that are clearly unfavored in the metadynamics simulations, i.e., with higher RMSD fluctuations and lower hydrogen bond persistency, were discarded, while others were selected for the molecular dynamics (MD)

simulations. In the end, one to three poses were selected for each compound for the following MD simulations (Table S1).

MD simulations of the  $\sigma_1 R$ /ligand complexes were performed in an explicit water and 1palmitoyl-2-oleoylphosphatidylcholine (POPC) lipid bilayer environment using Desmond MD System (version 4.9; D. E. Shaw Research, New York, NY) with the OPLS3 force field for protein, ligand, and lipids (Harder et al., 2016) and with the SPC water model. The missing residues at the N-terminus of  $\sigma_1 R$  in the crystal structure of  $\sigma_1 R/PD144418$  were constructed using MODELLER (John and Sali, 2003). Each of the  $\sigma_1 R$ /ligand complexes were then placed into the POPC lipid bilayer using the orientation of  $\sigma_1 R/PD144418$ retrieved from the Orientation of Proteins in Membranes database (Lomize et al., 2006). The system charges were neutralized, and 150 mM NaCl was added. Simulations were performed with a cutoff distance of 12 Å for the nonbonded interactions; and the particle mesh Ewald method was used to evaluate long-range electrostatic effects. In the isothermalisobaric (NPT) ensemble, constant temperature (310 K) and 1 atm constant pressure were maintained with Langevin dynamics on an anisotropic flexible periodic cell, with a constantratio constraint applied on the lipid bilayer in the X-Y plane. Each system was first minimized and then equilibrated with restraints on the ligand heavy atoms and protein backbone atoms, followed by production runs with all atoms unrestrained, as described previously (Michino et al., 2017; Michino et al., 2015). For each complex, we collected multiple trajectories (Table S1).

# 2.9. Ligand pose analysis

The stability of each ligand in the MD simulations were evaluated by calculating i) the RMSD of the ligands using the ligand pose in the last frame of each trajectory as the reference, and ii) the distance of the hydrogen on the charged N to the carboxyl group of Glu172. For the following analysis, we chose the most stable pose of each ligand that had the ligand RMSD below 1.5 Å for at least 300 ns with the persistent formation of the salt bridge – whereas most of the compounds had only one pose that was clearly better than the others, the two isomers of (+)-pentazocine were similarly stable in the MD simulations and both were included in the subsequent studies.

To classify the  $\sigma_1 R$  ligands based on their binding modes, we calculated the interaction frequencies of these ligands with the binding site residues. For the reasons described in the Discussion (section 4), we did not include cocaine in this analysis. Two poses of (+)pentazocine were combined so the following analysis was not biased. A protein residue was considered to form an interaction with the ligand if any heavy atom-heavy atom distance between them was within 4 Å. To obtain the mean interaction frequency, we randomly sampled 100 frames from each of the MD trajectories of the stable poses of each complex, which was repeated for 30 times and the mean contact frequency values were plotted as the heat map. Then, a hierarchical clustering was performed to classify the  $\sigma_1 R$  ligands based on the identities of contacting residues and their interaction frequencies with the ligands. To prevent the big difference caused by some individual residues, e.g., those with high contact frequency, we used Canberra distance to calculate the pairwise distances between two ligands (  $d(\mathbf{p}, \mathbf{q}) = \sum_{i=1}^{n} \frac{|p_i - q_i|}{|p_i| + |q_i|}$ , in which  $p_i$ ,  $q_i$  represent the contact frequency between the ligand p or q and the residue  $\dot{i}$ , while n represents the total number of interaction residues being considered; if  $p_i = q_i = 0$ , then  $d_i = 0$ ). Then, Ward's method was applied to merge the clusters.

# 3. Results

# 3.1. The endogenous $\sigma_1 R$ in HEK 293T cells has similar binding affinities for $\sigma_1 R$ ligands asthose in guinea pig cortex

Several cellular models have been used for the functional characterization of  $\sigma_1 R$ . While differentiated cells may have advantages in addressing signaling effects of  $\sigma_1 R$ , transfectable heterologous cells are amenable for addressing biophysical and pharmacological aspects of  $\sigma_1 R$  due to their ability to robustly express membrane proteins. In order to pursue  $\sigma_1 R$  pharmacology in the latter strategy, we first investigated expression levels of endogenous  $\sigma_1 R$  in HEK 293T cells so that later the levels of heterologous expression could be derived (see section 3.3). Thus, we measured  $\sigma_1 R$  expression levels ( $B_{max}$ ) and  $\sigma_1 R$  ligand binding affinities ( $K_d$ ) with [<sup>3</sup>H]-(+)-pentazocine (a previously reported  $\sigma_1 R$  "agonist" (Maurice and Su, 2009; Rousseaux and Greene, 2015)) in the membrane preparation of HEK 293T cells, and found they were comparable to those determined in guinea pig cortex (Table 1,  $K_d$  values were determined by homologous competitive binding as described in the Methods section), which has been routinely used in pharmacological studies of  $\sigma_1 R$  ligands (Su, 1982; Tam and Cook, 1984). Note the  $K_d$  value of (+)-pentazocine for guinea pig cortex was similar to that reported previously (Bowen et al., 1993).

Next, based on wide usage reported in the literature, eight structurally diverse  $\sigma_1 R$  ligands (Figure 1) were selected for the HEK 293T cell-based pharmacological characterizations. As expected, in the competition assays with [<sup>3</sup>H]-(+)-pentazocine, the  $K_i$  values for these eight compounds showed a consistent match between the HEK 293T cells and guinea pig cortex (Table 2, representative binding curves are shown in Supplementary Figure 1), indicating the binding affinities characterized by the cell-based assay can capture those in the tissue, the latter of which is in a more physiological context. We further assessed  $\sigma_1 R$  affinities using another  $\sigma_1 R$  radioligand, [<sup>3</sup>H]-haloperidol (a previously reported  $\sigma_1 R$  "antagonist" (Rousseaux and Greene, 2015)) (Table 1). The  $K_i$  values were generally higher (lower affinity) across all the tested compounds using [<sup>3</sup>H]-haloperidol compared to [<sup>3</sup>H]-(+)-pentazocine (Table 2). Nonetheless, the relative differences of the  $K_i$  values among the tested compounds were similar between [<sup>3</sup>H]-(+)-pentazocine and [<sup>3</sup>H]-haloperidol.

# 3.2. Topology analysis by proximity assays indicate N- and C-termini of $\sigma_1 R$ are on differentsides of membranes

A few different topological orientations of N- and C-termini relative to the membrane have been proposed for  $\sigma_1 R$ , based on the hydrophobicity analysis and truncation mutation studies (Brune et al., 2013; Kourrich et al., 2012). Such topological insight of  $\sigma_1 R$  is key to understanding its homomeric interaction as well as its interactions with client proteins. Thus, guided by the recent homotrimeric crystal structures, we studied the relative topology

between N- and C-termini by both bimolecular complementation and BRET approaches (Figure 2).

By fusing recently reported NanoLuciferase split fragments (i.e. NL1 and NL2) (Yano et al.) to proteins, the level of complementation between NL1 and NL2 is assessed by luminescence (Figure 2A), from which we can deduce the protein-protein proximity. As a positive control, we used dopamine D<sub>2</sub> receptor (D<sub>2</sub>R) C-terminal fusions of NL1 and NL2 (D<sub>2</sub>R-NL1:D<sub>2</sub>R-NL2), a pair of constructs that are known to readily complement (Figure 2A). As a negative control, we used D<sub>2</sub>R-NL1 and a non-membrane associated cytosolic protein FRB fused to NL2 (D<sub>2</sub>R-NL1:FRB-NL2), because they approach to each other only randomly (Figure 2A). For  $\sigma_1$ R, NL1 and NL2 are fused not only to the same ends, i.e., either both to the N-terminus, NL1- $\sigma_1$ R:NL2- $\sigma_1$ R (NL1- $\sigma_1$ :NL2- $\sigma_1$ ), or both to the C-terminus,  $\sigma_1$ R-NL1: $\sigma_1$ -NL2 ( $\sigma_1$ -NL1: $\sigma_1$ -NL2), but also to the opposite ends, i.e., NL1- $\sigma_1$ : $\sigma_1$ -NL2 or NL2- $\sigma_1$ : $\sigma_1$ -NL1 (Figure 2A). Consistent with the topology revealed by the crystal structures that N- and C-termini are on two sides of the membrane, only the same-end fusion  $\sigma_1$ R pairs and the D<sub>2</sub>R-NL1:FRB-NL2 pair showed a significantly higher luminescence level above the D<sub>2</sub>R-NL1:FRB-NL2 pair (Figure 2C).

We then used an acceptor saturating BRET method, a commonly-used ratiometric assay that has the advantage of withstanding off-target ligand interaction with a luciferase. As previously reported (Marullo and Bouvier, 2007), a saturating profile and higher net BRET values are the signature of specific interactions between the donor and acceptor (i.e., NL and VN), whereas linear or low net BRET values indicate a random collision between the donor and acceptor and thus not likely to form a complex between the two fused-proteins. Consistent with the findings from the above bimolecular NanoLuciferase complementation, only the same-end fusion construct pairs, the N-terminal pair NL- $\sigma_1$ R:VN- $\sigma_1$ R (NL- $\sigma_1$ :VN- $\sigma_1$ ) and the C-terminal pair  $\sigma_1$ -NL: $\sigma_1$ -VN, satisfied the high and saturable BRET signals, whereas the opposite-end fusion construct pairs (NL- $\sigma_1$ : $\sigma_1$ -VN and  $\sigma_1$ -NL:VN- $\sigma_1$ ) exhibited a low linear BRET profile (Figure 2B,D).

# 3.3. PRE-084 shows unique kinetics in entering the ligand binding site of $\sigma_1 R$

Photoaffinity labeling experiments (Fontanilla et al., 2008) and the recently solved  $\sigma_1 R$  crystal structures (Schmidt et al., 2016) demonstrate that  $\sigma_1 R$  ligand binding site is on the same side of the membrane as its C-terminus. However, the locale of the binding site with regard to the membrane topology is much less certain. The C-terminus (and therefore the binding site) has been variously asserted to be located within the ER lumen (Hayashi and Su, 2007), in the cytoplasm (Aydar et al., 2002), or outside the cell (Balasuriya et al., 2013). More recently, based on the crystal structures, Schmidt et al. have asserted that the  $\sigma_1 R$  ligand binding site is in the cytoplasm (Schmidt et al., 2016). In this configuration, the binding site consistently remains within the cell, regardless of  $\sigma_1 R$  being at the ER or translocated to the cell membrane. Such a locale would require ligands to permeate through the plasma membrane first in order to access the binding site, which may result in different binding kinetics in intact whole cells compared to membrane preparations. To explore this possibility, we examined ligand binding kinetics in both preparations.

First, in both the intact whole cell and membrane preparations, we studied the displacement of  $[{}^{3}H]$ -(+)-pentazocine by the  $\sigma_{1}R$  ligands listed in Table 1, for which the concentration was determined based on their  $K_i$  values (Supplementary Figure 2A,B). Normalized to total binding in the absence of cold ligand and complete displacement by 500 nM cold (+)pentazocine as 100% and 0%, respectively, haloperidol, JHW007, and NE100 showed immediate displacement even at 15 min of incubation for both membrane preparation and whole cells (note the negative values indicate that the tested cold ligand may reach the binding sites faster than (+)-pentazocine). However, PRE-084 showed significantly slower kinetics than the others in the whole cell assay, whereby it only displaced 60.6% [<sup>3</sup>H]-(+)pentazocine at 15 min and its displacement remained below 76.1% at 120 min. In contrast, at these timepoints it displaced 92.4–96.1%  $[^{3}H]$ -(+)-pentazocine in the membrane preparation. The experimentally determined  $pK_a$  (6.2 for PRE-084 and 9.2-9.3 for (+)-pentazocine) suggests that PRE-084 is not charged in the solutions (pH 7.4), whereas (+)-pentazocine is. Although this difference indicates that PRE-084 is more plasma-membrane permeable at a physiological pH, other properties may play a role in entering the ligand binding site, thus yielding the slower access of PRE-084 to the site.

Next, HEK 293T cells transfected with the C-terminal BRET construct pair  $\sigma_1$ -NL: $\sigma_1$ -VN were characterized by binding kinetics analysis (Supplementary Figure 2C). We found all the tested ligands, including PRE-084, displaced [<sup>3</sup>H]-(+)-pentazocine in these cells as fast as in the membrane preparation of the non-transfected cells, indicating that the transiently transfected plasma membrane is permeable to  $\sigma_1$ R ligands, possibly due to compromised membrane integrity (Grandinetti et al., 2012).

From the binding kinetics, we calculated  $B_{max}$  and  $K_d$  for intact whole cells (1041 ± 540 fmol/mg and 1.7 ± 0.1 nM, respectively), BRET-transfected whole cells (4289 ± 2745 fmol/mg and 2.0 ± 0.3 nM), and membrane preparation (871 ± 403 fmol/mg and 3.3 ± 1.4 nM). As expected, BRET-transfected whole cells showed ~5-fold higher  $B_{max}$  than intact cells, confirming that transient transfection adds binding sites and the transfected fusion  $\sigma_1 R$  constructs retain the functional integrity of the protein. Binding kinetic analysis of (+)-pentazocine association time (T<sub>1/2</sub>, the time to bind 50% of the available binding sites) among intact whole cells, BRET-transfected whole cells, and membrane preparation yielded near identical values (21.4 ± 3.86, 21.3 ± 4.54, and 21.1 ± 4.44 min, respectively) and suggested fast permeability of (+)-pentazocine (Supplementary Figure 2D).

Taken together, while other tested ligands exhibited cell permeability comparable to  $[{}^{3}H]$ -(+)-pentazocine in intact cells, PRE-084 showed slower kinetics. The lack of slower kinetics of PRE-084 in the membrane preparation and the BRET-transfected cells suggests that the process of permeation through the intact membrane may play a role in its kinetics. However, whereas the involvement of the plasma membrane permeation is consistent with the ligand binding site of  $\sigma_1 R$  being on the cytoplasmic side, p $K_a$  values suggest that PRE-084 is more permeable than (+)-pentazocine. Thus, the locale of the binding site with regard to membrane topology requires further investigation.

# 3.4. $\sigma_1 R$ homomer BRET defines two categories of $\sigma_1 R$ ligands

Next, we used the C-terminal  $\sigma_1$ -NL: $\sigma_1$ -VN BRET construct pair to evaluate whether the ligand-induced BRET signal changes have any applicability in differentiating the  $\sigma_1 R$ ligands in a dose dependent manner. In all four time points tested, there were clear doseresponse effects by haloperidol, 4-PPBP, and PD144418, but weaker or almost no effects by (+)-pentazocine, PRE-084, NE-100, JHW007, and cocaine (Figure 3A-D). The results at later time points (10, 30, and 60 min) showed more prominent increases in the induced BRET signals for haloperidol, 4PPBP, and PD144418, but very little by the others (Figure 3A-D). The differences in potencies among haloperidol, 4PPBP, and PD144418 correlated with their different binding affinities (Table 2), although the potencies are consistently lower than the  $K_i$  values. We categorized haloperidol, 4PPBP, and PD144418 to be active, whereas the other compounds were inactive in this assay. Even though there could be a spectrum of  $E_{max}$  values depending on the  $\sigma_1 R$  ligands, we set the threshold by two-way ANOVA Dunnett test at the level of PD144418 E<sub>max</sub> (~0.02) resulting in the classification of ligands into two groups: haloperidol, 4PPBP, and PD144418 that showed positive dose-dependent induction of BRET signaling, and (+)-pentazocine, PRE-084, NE100, JHW007, and cocaine that produced no detectable effects on BRET signaling.

To demonstrate that the lack of BRET signals in the single-ligand mode was not due to the inability of (+)-pentazocine, PRE-084, NE-100, JHW007, or cocaine to bind to  $\sigma_1$ R, we used a competition mode of the assay by adding 1 µM haloperidol (Figure 3E-H) or 1 µM PD144418 (Figure 3I-L) prior to addition of the tested ligands (see Methods). We found all five compounds showed dose-dependent effects in the competition mode – the negative values in Figure 3E-L indicate direct competition, as the BRET signals induced by the pre-added haloperidol or PD144418 were subtracted to 0 in the analysis. The inhibition potencies for these drugs were correlated with their relative differences in binding affinities as well, though the overall potency values were more right-shifted (less potent) than the  $K_i$  values. Further, when the lower efficacy ( $E_{max}$  shown in the single-ligand mode) ligand PD144418 was displaced by haloperidol or 4PPBP, both of which have higher  $E_{max}$  values, positive BRET signals were induced as compared to the negative signal observed for the non-efficacious ligands (Figure 3I-L).

Of note, when we carried out the same assays using the N-terminal NL- $\sigma_1$ :VN- $\sigma_1$  construct pair (Supplementary Figure 3), the data could not be deciphered by conventional regression analysis. Thus, even though the BRET ratios for the N-terminal pair were higher than the Ctermini pair, it was more feasible to study the structure-activity relationships (SAR) of these  $\sigma_1 R$  ligands in the  $\sigma_1 R$  homomerization with the C-terminal fusion constructs.

# 3.5. Haloperidol promotes the formation of higher order $\sigma_1 R$ homomers in a non-denaturinggel assay

Because haloperidol increased  $\sigma_1 R$  homomeric interaction in our BRET assays, we further explored ligand effects on  $\sigma_1 R$  multimerization using a biochemical method described recently (Hong et al., 2017). In non-denaturing gels, we observed low molecular weight (MW) bands likely corresponding to monomer and dimer of  $\sigma_1 R$ , and high MW bands indicative of  $\sigma_1 R$  multimers. Concentrations of 0.1 or 1  $\mu$ M haloperidol dramatically

increased the multimer band intensities and decreased the low MW band intensities, in a dose dependent manner. Consistent with enhanced BRET signals by haloperidol in Figure 2, this result showed that haloperidol promoted or stabilized  $\sigma_1 R$  multimerization. On the other hand, 10  $\mu$ M (+)-pentazocine decreased the density of multimer bands while increasing those of low MW bands (Figure 4). In addition, we evaluated the capability of (+)-pentazocine to inhibit the multimer-promoting effect by haloperidol, using two ratios of haloperidol and (+)-pentazocine, 0.1:10  $\mu$ M (1:100) and 1:10  $\mu$ M (1:10). Results showed that (+)-pentazocine inhibited haloperidol's effect in a dose dependent manner (Figure 4).

These results suggest that the well-characterized  $\sigma_1 R$  agonist (+)-pentazocine and antagonist haloperidol had distinct effects on the multimerization state of  $\sigma_1 R$ . Whereas haloperidol promotes the formation of higher order homomers, (+)-pentazocine shifts the equilibrium in the opposite direction.

## 3.6. Computational study reveals a structural basis for ligand categorization

The crystal structures of  $\sigma_1 R/PD144418$  and  $\sigma_1 R/4$ -IBP (PDB ID 5HK1 and 5HK2) (Schmidt et al., 2016) reveal an occluded and elongated binding cavity in a cupin-like  $\beta$ -barrel, with the highly conserved Glu172 located near the center of the cavity, forming a salt bridge with the ligands.

Because the crystal structures have revealed an unexpected topology for the number of transmembrane segments and the locations of the N- and C-termini, we first evaluated the stability of these structures in the lipid bilayer environment. Thus, we immersed the trimers of  $\sigma_1 R/PD144418$  complex and the apo state of  $\sigma_1 R$  (starting from the structure with PDB ID 5HK1) in the explicit lipid-bilayer (see section 2.8) and carried out prolonged MD simulations (Table S1). We found the integrities of the  $\sigma_1 R$  structure and the trimer interface were well retained in both conditions. Thus, whereas the functional dynamics of the homomer states of  $\sigma_1 R$  remains to be fully characterized, these studies support the crystal structures as providing a reliable framework to investigate the SAR of structurally diverse  $\sigma_1 R$  ligands.

We then systematically characterized the binding modes of all the  $\sigma_1 R$  ligands in Figure 1. We carried out molecular docking of these compounds in all their possible stereoisomeric forms and selected several potential binding poses to be further evaluated by both metadynamics and prolonged conventional MD simulations (see section 2.7). From the simulation results, we identified the most stable modes for each ligand (see section 2.8, and Supplementary Figure 5). Whereas we could narrow down the most stable pose for the other ligands to one, we found two isoforms of (+)-pentazocine that are protonated differently on the charged N atom were similarly stable, and thus we have included the results of both forms in our following interacting-residue analysis.

Based on the MD simulation results, we carried out a hierarchical clustering analysis of  $\sigma_1 R$  ligands according to their interacting patterns with the binding site residues (see section 2.9). When the number of clusters is reduced to two, we found that haloperidol, PD144418 and 4-PPBP form one cluster, while the rest compounds are in the other cluster, the results of which are correlated well with those from the homomer BRET assay. Interestingly, a

fluorophenyl ring of JHW007 protruded into a small pocket that was not occupied by any of haloperidol, PD144418 and 4-PPBP (Figure 5C) and formed a polar interaction with Thr189 (Figure 5D). Similarly, PRE-084 and one of the (+)-pentazocine isomers could also occupy this pocket, with the latter stably forming a hydrogen bond (H-bond) with Thr189 (Figure 5D). This pocket is encircled by Val84, Asn85, Ala86, Leu186, Asp188, Thr189, Thr198, and Thr202, and a water molecule is found in this pocket in the crystal structure of  $\sigma_1 R$ /PD144418. Among these residues, Asn85 and Asp188 face the central tunnel formed by the trimer, while Thr198 forms a H-bond with Asp195, which interacts with His116 and Arg119 of another monomer. Thus, this small pocket appears to be associated with multimerization, and the different interactions with this pocket between the two groups of ligands are potentially correlated with their divergent propensities in promoting or stabilizing the formation of  $\sigma_1 R$  multimer.

# 3.7. Haloperidol and (+)-pentazocine have opposite impacts on σ<sub>1</sub>R-BiP coupling

To demonstrate the applicability of the BRET approach in investigating the functional coupling between  $\sigma_1 R$  and its client proteins, we focused on characterizing the interaction between  $\sigma_1 R$  and BiP. First, the acceptor-saturating BRET between  $\sigma_1 R$  and BiP showed robust increases in BRET signals in two out of four tested BRET construct pairs, i.e., NL- $\sigma_1$ :VN-BiP and  $\sigma_1$ -NL:VN-BiP, with the saturability indicating specific interactions between the two proteins (Supplementary Figure 4A,B). BiP-VN C-terminal fusion does not seem to be a good sensor for BRET since the C-terminal domain plays a role in substrate binding for BiP (Yang et al., 2015). To be consistent with the  $\sigma_1 R$  homomer BRET, we used the  $\sigma_1$ -NL:VN-BiP pair to evaluate the impact of  $\sigma$ 1R ligand binding on this coupling. Interestingly, (+)-pentazocine showed the bimodal dose response effect at 2.5 and 10 min time points, whereas haloperidol showed a negative induced BRET signal at 60 min (Figure 6). In the competition mode of the assay, the presence of 1  $\mu$ M (+)-pentazocine diminished the negative BRET signal induced by haloperidol. These results suggest two temporally distinct events: one immediately after the ligand addition and one at a later time point. A similar trend was observed in the N-terminal fusion pair (NL- $\sigma_1$ R:VN-BiP; see Supplementary Results and Supplementary Figure 4C).

# 4. Discussion

In our binding experiments, the B<sub>max</sub> determined by [<sup>3</sup>H]-haloperidol showed a statistically nonsignificant trend to be higher than that determined by [<sup>3</sup>H]-(+)-pentazocine (Table 1), suggesting the presence of off-target binding site(s) for haloperidol, such as the  $\sigma_2$  receptor ( $\sigma_2$ R) and aminergic GPCRs. However, the curve fitting could not detect or differentiate more than one binding site. Nevertheless, our results are consistent with  $\sigma_2$ R contributing to the B<sub>max</sub> in [<sup>3</sup>H]-haloperidol but not in [<sup>3</sup>H]-(+)-pentazocine binding – in a recent study, the  $\sigma_2$ R was found to have a  $K_d$  of 54.1 nM for haloperidol, which is similar to that of  $\sigma_1$ R and cannot be resolved in slope analysis; in comparison,  $\sigma_2$ R has a  $K_d$  of 2.47 µM for (+)pentazocine, which is a much higher value than the  $K_d$  at  $\sigma_1$ R (Alon et al., 2017).

Employing a novel  $\sigma_1 R$  homomer BRET assay that detects ligand-induced changes between  $\sigma_1 R$  monomers, we are able to identify ligands that produced a positive dose-dependent

increase of  $\sigma_1 R \cdot \sigma_1 R$  homomer BRET signals, such as haloperidol, 4-PPBP, and PD144418. Although (+)-pentazocine and other ligands did not produce clear response in this assay, it is possible that a higher sensitivity is necessary to discern subtle BRET signals in transiently transfected cells with abundantly expressed BRET sensor proteins. However, they attenuated the increase in BRET signals elicited by haloperidol, PD144418 or 4-PPBP. The fact that the displacement of PD144418 by haloperidol or 4-PPBP resulted in a higher  $E_{max}$  value is consistent with graded effects among the haloperidol-like ligands (Figure 3K,L).

Because  $\sigma_1 R$  homomer BRET assays did not directly measure functional outcomes after  $\sigma_1$ R ligand binding, we do not use "agonist" and "antagonist" in the interpretation of our results. While traditionally  $\sigma_1 R$  agonists and antagonists are defined by various functional assays such as anti-nociception, the molecular mechanisms that delineate  $\sigma_1 R$  agonists and antagonists remain to be elucidated. Indeed, in label-free dynamic mass redistribution assays, we did not see significant changes by all tested  $\sigma_1 R$  ligands, indicating that their  $\sigma_1$ R-dependent signaling events are very different from GPCR-dependent ones (Schroder et al., 2010) and perhaps not as robust near the plasma membrane (Supplementary Results and Supplementary Figure 6). Although some ligands exhibited unexpected results in the BRET assays, we did observe similar phenotypes in "agonists" ((+)-pentazocine and PRE-084) and "antagonists" (haloperidol and PD144418), consistent with their characterization in the literature (Maurice and Su, 2009). Nonetheless, the unexpected phenotypes of NE-100, and 4-PPBP are intriguing. It is plausible that such discrepancies could be attributed to subtle responses by these ligands that are not detected by our BRET assays, or masked by their offtarget effects, or likely due to extrinsic factors such as client proteins. In addition, the inactivity of cocaine in our  $\sigma_1 R$  homomer BRET assay is worth noting. Although the low potency of cocaine in the single-ligand homomer BRET assays renders it difficult to interpret its phenotype, based on the results at 30 and 60 min time points (Figure 3C,D), it is tempting to speculate that cocaine is more like haloperidol in this aspect. Interestingly, JHW007 has been found to counter-act the stimulant and reinforcing effects of cocaine (Hiranita et al., 2017), and is different from haloperidol in our BRET assays. Indeed, JHW007 is a dual acting ligand that binds to both  $\sigma_1 R$  and the dopamine transporter (DAT) with high affinities (Agoston et al., 1997; Hiranita et al., 2017; Katz et al., 2004). JHW007 stabilizes DAT in a more inward-facing conformation from that stabilized by cocaine (Abramyan et al., 2017; Beuming et al., 2008; Bisgaard et al., 2011; Loland et al., 2008). Thus, if cocaine and JHW007 belong to different categories of  $\sigma_1 R$  ligands, we can envision that JHW007 antagonizes the actions of cocaine at both DAT and  $\sigma_1 R$ , two important targets that have been found to interact dynamically at or near the plasma membrane (Hong et al., 2017; Sambo et al., 2017). Interestingly, to the extent of our simulations in this study, we could identify a stable pose of cocaine that does not protrude into the small pocket occupied only by JHW007, (+)-pentazocine, and PRE-084.

Homomer BRET does not provide information directly on how many monomers constitute the  $\sigma_1 R$  complex as the BRET ratio is not quantitative for a donor:acceptor stoichiometric ratio. However, it is worth noting that the  $E_{max}$  are saturable (e.g., haloperidol, PD144418, and 4PPBP) indicating that the equilibrated donor:acceptor ratio is capped at a certain level within the BRET-participating populations. Although we may not know the stoichiometric

ratio, it is interesting to observe graded saturation levels of  $E_{max}$  among different  $\sigma_1 R$  ligands, which may indicate different higher order homomers.

To evaluate the ligand effects on the homomerization state of  $\sigma_1 R$  directly, we employed a biochemical assay described recently (Hong et al., 2017). By comparing the results from these non-denaturing gels and BRET assays, we conclude that the increase of the BRET signal is associated with the formation of higher-order homomers, based on the following two common trends: first, the observation that haloperidol promotes the multimerization and (+)-pentazocine competes against that effect in gel assays is in line with the differences observed between these two ligands in the homomer BRET assay; second, the multimer band is made of different populations and distinctly heavier than a trimer, indicating the possibility of several high-order multimers, which may be reflected by different strengths of BRET signals elicited by the haloperidol-like ligands; third, the density changes for the multimer are inversely correlated with those of low-MW populations (monomer and dimer), consistent with the observed displacement of haloperidol by (+)-pentazocine in the competition BRET assay.

 $\sigma_1 R$  has been shown to regulate chaperone activities of BiP in the ER via  $\sigma_1 R$ -BiP interaction (Hayashi and Su, 2007; Ortega-Roldan et al., 2013). The opposite effects of (+)pentazocine and haloperidol demonstrated by our  $\sigma_1$ R-BiP BRET assay, along with their effects in the homomer BRET assay, argue that the  $\sigma_1$ R-BiP interaction is modulated differently by these  $\sigma_1 R$  ligands. Indeed, they also induced distinct effects on  $\sigma_1 R$ homomerization in biochemical assays using non-denaturing gels. Interestingly, the opposite pharmacological profiles between the homomer BRET and  $\sigma_1$ R-BiP BRET can be interpreted as that the promotion of homomerization by haloperidol diminishes  $\sigma_1$ R-BiP interaction, whereas unchanged or diminished homomerization by (+)-pentazocine may facilitate  $\sigma_1 R$  interacting with BiP. We propose that the physiological significance of  $\sigma_1 R$ homomerization is tightly linked to the interaction with its client protein BiP. Such a scenario closely resembles the hypothesis proposed on the interaction between  $\sigma_1 R$  and DAT in a recent study (Hong et al., 2017). Determining whether similar changes occur during the interaction of  $\sigma_1 R$  with other client proteins will require further investigations. Although there may be different interpretations of ligand effects on the  $\sigma_1$ R-BiP interaction, both current and previous studies (Hayashi and Su, 2007) suggest that  $\sigma_1 R$  ligands dynamically regulate  $\sigma_1$ R-BiP interactions. In BRET assays, we were able to examine time-course and dose-response of  $\sigma_1 R$  ligand in live cells, which was not achieved by previous coimmunoprecipitation methods. Thus, the bimodal dose response and time dependent change of the (+)-pentazocine effect (Figure 6) may indicate that the ligand-induced cellular trafficking of  $\sigma_1 R$  affects its interaction with ER-resident BiP. Indeed, a (+)-pentazocineinduced decrease in  $\sigma_1$ R-BiP interaction at later time points in our study here coincides with a previous report of 30 min (+)-pentazocine incubation time point (Su et al., 2016).

Note, however, since BRET appears to happen across the membrane in our HEK 293T cell model, our BRET results on  $\sigma_1$ R-BiP interaction are consistent with, but do not definitively prove the orientation of  $\sigma_1$ R relative to the ER lumen and cytoplasm depicted in the cartoons in Figure 6 and Supplementary Figure 4, i.e., with the N terminus facing the ER lumen (or

the extracellular side). Interestingly, recent work by the Yang group (Mavylutov et al., 2017) suggests that the C terminus of  $\sigma_1 R$  may face the ER lumen.

In our MD simulations, we found that the trimer models of the  $\sigma_1$ R/PD144418 complex and its *apo* form embedded in lipid bilayers are highly stable in terms of the integrity of the ligand binding site and the trimer interface. This finding supports that the crystal structure from which these models were derived is in a valid conformation, thereby the N- and Ctermini of the protein are on two different sides of the membrane. The results of our topological analysis of  $\sigma_1$ R by the BRET assay resonate with this conclusion as well. Based on these consistent conclusions from different approaches, we carried out a  $\sigma_1$ R structurebased SAR study to investigate the structural basis for the different BRET profiles of the two groups of  $\sigma_1$ R ligands. In particular, we found JHW007, (+)-pentazocine, and PRE-084 protrude into a small pocket near the trimer interface that was not occupied by haloperidol, 4PPBP, and PD144418. Thus, our computational results described herein reveal the initial clues of the SAR profile for the tested ligands.

Whereas our work establishes a novel molecular biophysical approach to classify  $\sigma_1 R$  ligands, it is important to point out that the resulting classifications of the ligands are not necessarily in contradiction to previous characterizations of these ligands, many of which are based on functional readouts downstream of the initial  $\sigma_1 R$ -ligand interactions. Such readouts are assumed to have integrated their impact from the interactions between  $\sigma_1 R$  and its client proteins, and the off-target effects of ligands. Thus, our BRET approach sheds light on the ligand-induced conformational changes of  $\sigma_1 R$ , in combination and correlation with the  $\sigma_1 R$  structure-based SAR studies, it would provide a framework at the atomistic level to investigate the structure-function relationship of  $\sigma_1 R$ .

# 5. Conclusions

We established a novel  $\sigma_1 R$  homomer BRET assay to profile the pharmacological properties of  $\sigma_1 R$  ligands based on induced changes in  $\sigma_1 R$  homomerization, and identified multimerpromoting and non-promoting ligands, the conclusion of which is substantiated by a biochemical assay at the protein-protein interaction level. The results of a complementary BRET assay on the  $\sigma_1 R$ -BiP interaction reflected the reciprocal pharmacological behavior seen in  $\sigma_1 R$  homomerization. In characterizing the binding modes of the experimentally tested compounds at  $\sigma_1 R$  with extensive MD simulations, we revealed initial clues for the structural basis that may be responsible for stabilization of the homomer.

# Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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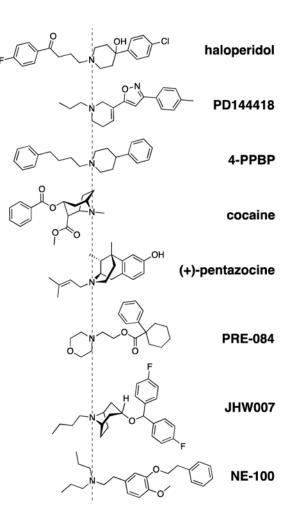
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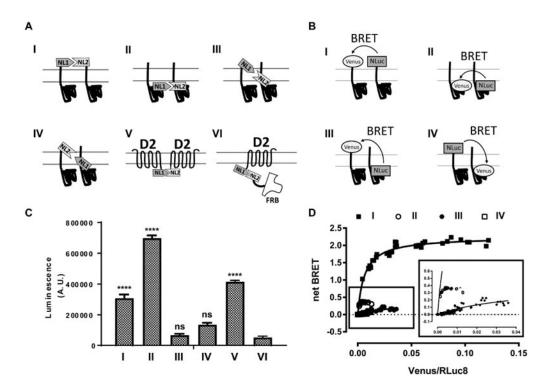
# Highlights

- Both our experimental and computational results support the topology revealed by the crystal structures of  $\sigma_1 R$ .
- Novel BRET assays are capable of examining  $\sigma_1 R$  homomeric and  $\sigma_1 R$ -BiP heteromeric interactions upon ligand binding.
- Our findings shed light on the ligand-induced conformational changes of  $\sigma_1 R$ .



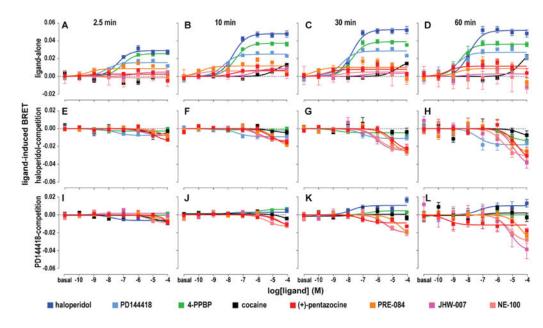
# Figure 1.

Chemical structures of the eight compounds aligned by their overall binding orientations. The compounds are oriented based on the resulting poses in the ligand binding pocket of  $\sigma_1 R$  from our molecular modeling and simulation results, and are aligned by the charged N atom.



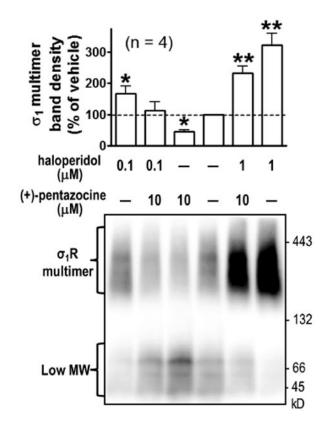
# Figure 2.

N- and C-termini of  $\sigma_1 R$  are not close to each other in the proximity assays. (A) Schematic representation for NanoLuciferase complementation assay. (B) Schematic representation for BRET assay. (C) NanoLuciferase complementation is performed between  $\sigma_1 R$  and  $\sigma_1 R$  with four different configurations (I-IV; NL1- $\sigma_1$ :NL2- $\sigma_1$ ,  $\sigma_1$ -NL1. $\sigma_1$ -NL2, NL1- $\sigma_1$ : $\sigma_1$ -NL2,  $\sigma_1$ -NL1:NL2- $\sigma_1$ ), between D2R-NL1 and D2R-NL2 (V), or between D2R-NL1 and FRB-NL2 (VI). One way ANOVA followed by posthoc Dunnett's test against D2R-NL1:FRB-NL2 (VI) shows significance (p < 0.0001) for NL1- $\sigma_1$ :NL2- $\sigma_1$  (I),  $\sigma_1$ -NL1: $\sigma_1$ -NL2 (II), and D2R-NL1:D2R-NL2 (V). Data represents mean  $\pm$  S.E.M. (n = 3 or more). (D) Acceptor-saturating BRET between  $\sigma_1 R$  and  $\sigma_1 R$  using N- and C-terminal fusion constructs to address the relative transmembrane topology: NL- $\sigma_1$  and  $\nabla_1$ - $\nabla_1$  (I, solid square),  $\sigma_1$ -NL and  $\sigma_1$ -VN (II, open circle),  $\sigma_1$ -NL and VN- $\sigma_1$  (III, solid circle), and NL- $\sigma_1$  and  $\sigma_1$ -VN (IV). The results of both assays are consistent with the crystal structure showing N- and C-termini on opposite sides of membrane.



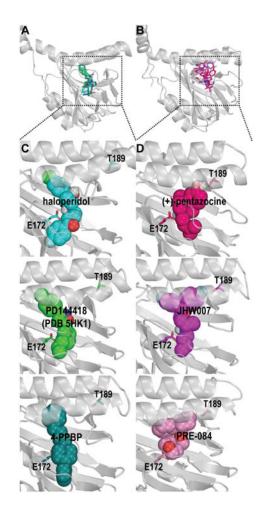
### Figure 3.

Drug induced  $\sigma_1 R$  homomer BRET changes. Drug induced BRET between C-terminally fused  $\sigma_1$ -NL and  $\sigma_1$ -VN is detected at 2.5, 10, 30, or 60 min for ligand alone (**A-D**), ligand in the presence of 1  $\mu$ M haloperidol (**E-H**), or 1  $\mu$ M PD144418 (**I-L**).  $\sigma_1 R$  ligands are represented in different colors – (+)-pentazocine (red), PRE-084 (orange), NE100 (pink), JHW007 (magenta), cocaine (black), haloperidol (blue), PD144418 (cyan), and 4PPBP (green). Data represents mean ± S.E.M. (n = 5 or more).



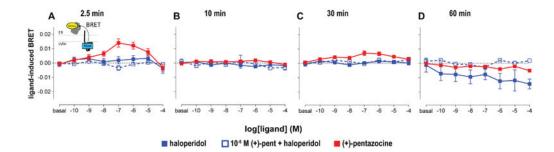
# Figure 4.

Non-denaturing gel analysis of drug-induced  $\sigma_1 R \cdot \sigma_1 R$  interaction. Cells expressing FH- $\sigma_1 R$  (MW: 32 kDa) were incubated with haloperidol in culture medium at 37 °C for 0.5 h, followed by incubation of (+)-pentazocine for 1 h. Cells were lysed with GDN lysis buffer and subjected to PFO-PAGE. Flag antibodies detected high-MW multimeric and low-MW (likely monomer and dimer) bands, based on their apparent MW. Quantified results of multimeric band signals (mean ± SEM, n = 4 experiments), with a representative blot. \* P < 0.05, \*\* P < 0.01, one way ANOVA and post-hoc Dunnett's test, compared with vehicle. Faint signals (~ 50 kDa) are likely due to partial degradation of dimeric  $\sigma_1 R$ .



### Figure 5.

Molecular modeling and simulations of  $\sigma_1 R$  in complex with its ligands reveal distinct interaction patterns. The stable poses of ligands with multimer-promoting effect (haloperidol, PD144418, and 4-PPBP) and those without ((+)-pentazocine, PRE-084, JHW007, and NE-100) are shown in panels **A** and **B**, respectively. The zoom-in views of the representative ligands from each group are shown in panels **C** and **D**. Note JHW007, (+)-pentazocine, and PRE-084 protrude into a pocket that is not occupied by the multimer-promoting ligands.



# Figure 6.

Drug induced  $\sigma_1$ R-BiP BRET changes. Dose response change in BRET is detected between C-terminally fused  $\sigma_1$ -NL and VN-BiP at 2.5 (**A**), 10 (**B**), 30 (**C**), 60 (**D**) min for (+)-pentazocine (red), haloperidol (blue solid), haloperidol in the presence of 1  $\mu$ M (+)-pentazocine (blue open). Data represents mean  $\pm$  S.E.M. (n = 5 or more).

# Table 1 Radioligand binding properties for [<sup>3</sup>H]-haloperidol and [<sup>3</sup>H]-(+)-pentazocine

 $K_d$  and  $B_{max}$  are determined using [<sup>3</sup>H]-haloperidol and [<sup>3</sup>H]-(+)-pentazocine in HEK 293T cell (second column) and guinea pig cortex (third column) membrane preparations.

Compound	HEK 293T membran	e	Guinea pig cortex	
[ <sup>3</sup> H]-haloperidol	$K_d \pm \text{SEM} (\text{nM})$	n		
	$7.87\pm3.47$	5	NA	
	$B_{max} \pm SEM \text{ (fmol/mg)}$	n	NA	
	$5847 \pm 2221$	5		
[ <sup>3</sup> H]-(+)-pentazocine	$K_d \pm \text{SEM} (\text{nM})$	n	$K_d \pm \text{SEM} (\text{nM})$	n
	$7.76\pm0.52$	3	$5.18\pm0.75$	3
	$B_{max} \pm SEM (fmol/mg)$	n	$B_{max}\pm SEM~(fmol/mg)$	n
	$2080\pm163$	3	$1091\pm79$	3

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# Radioligand competition binding with [<sup>3</sup>H]-haloperidol or [<sup>3</sup>H]-(+)-pentazocine

Competition results using [<sup>3</sup>H]-haloperidol (second column) or [<sup>3</sup>H]-(+)-pentazocine (third and fourth columns) are shown. For [<sup>3</sup>H]-(+)-pentazocine binding, results for membrane preparation of guinea pig cortex (third column) in addition to HEK 293T (fourth column) are shown.

Compound	Compound Competition vs. 2 nM [ <sup>3</sup> H]-haloperidol Competition vs. 3 nM [ <sup>3</sup> H]-(+)-pentazocine	<i>M</i> [ <sup>3</sup> H]-haloperidol	Competition vs. 3 nN	М	[ <sup>3</sup> H]-(+)-pentazoci	ne
	HE	HEK 293T membrane	Guinea pig cortex		HEK 293T membrane	ane
	$K_{i} \pm SEM (nM)$	u	$K_{\rm i} \pm { m SEM} \ ({ m nM})$	a a	$K_{i} \pm SEM (nM)$	=
haloperidol $8.24 \pm 4.11$	$8.24\pm4.11$	3	$0.835 \pm 0.315$	3	$0.965\pm0.016$	3
(+)-pentazocine	$174 \pm 48.4$	3	$5.11 \pm 0.514$	3	$7.63\pm0.318$	3
cocaine	cocaine $32100 \pm 9110$	3	$3710 \pm 1170$	3	$4660 \pm 1920$	3
PD144418	$PD144418  2.67 \pm 0.578$	4	$0.842 \pm 0.307$	3	$0.894\pm0.110$	3
JHW007	JHW007 $1.85 \pm 0.0579$	3	$1.48 \pm 0.289$	4	$0.554\pm0.172$	3
PRE-084	$208\pm43.2$	3	$11.0 \pm 0.640$	3	$21.0\pm5.93$	3
NE-100	NE-100 $16.3 \pm 4.43$	4	$1.14 \pm 0.283$	4	4 1.75 $\pm$ 0.382	9
4-PPBP	4-PPBP $2.28 \pm 0.558$	3	$0.857 \pm 0.153$	3	$1.16\pm0.219$	3