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# Dietary Advanced Glycation End Products Have Sex- and Age-Dependent Effects on Vertebral Bone Microstructure and Mechanical Function in Mice

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# Abstract

Back pain is a leading cause of global disability that can arise from vertebral fracture and osteoporosis. Although poor general health and obesity are among the strongest risk factors for back pain, there is remarkably little known about how diet influences spinal diseases. Advanced glycation end-products (AGEs) are implicated in increased fracture risk, yet no studies investigated how dietary AGEs affect spinal health. We tested the hypothesis that high dietary AGE ingestion will diminish vertebral structure and function in a sex- and age-dependent manner. Female and male mice were fed low-AGE (L-AGE) or high-AGE (H-AGE) isocaloric diets for 6 and 18 months and multiple measurements of bone structure and function were taken. AGE levels in serum and cortical vertebrae were increased only for 6-month-old H-AGE female mice while blood glucose and body weight remained normal for all animals. When fed an H-AGE diet, 6month-old female mice had inferior vertebral trabecular structure with decreased bone mineral density (BMD) and bone volume fraction. Biomechanical testing and analytical modeling further showed functional deterioration in 6-month-old H-AGE females with reduced shear and compression moduli, and maximum load to failure. At 18 months, H-AGE mice of both sexes had significant but small decreases in cortical BMD and thickness, yet functional biomechanical behaviors were not distinguishable from other aging changes. We conclude that an H-AGE diet, without diabetic or overweight conditions, diminished vertebral microstructure, mechanical behaviors, and fracture resistance in young female mice in a manner suggesting accelerated bone aging.

# Keywords

Spine; Vertebral Fracture; Advanced Glycation End Products; Nutrition; Animal Model; Aging; Bone Qct/µCt; Biomechanics; Fracture Risk Assessment

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# Introduction

Back pain is the most common physical condition for doctor visits and the leading cause of global disability,<sup>(1)</sup> affecting approximately 20% of the population at any time<sup>(2)</sup> and resulting in substantial loss of productivity and increasing medical treatment costs.<sup>(3)</sup> Back pain is associated with multiple interacting spinal pathologies including vertebral fracture and endplate defects as well as intervertebral disc herniation and degeneration. Poor general health and obesity are among the strongest risk factors for back pain,<sup>(2,4,5)</sup> motivating investigations of how diet influences spinal diseases.

A causal link between diabetes and spinal pathology was identified in animal studies where accumulation of advanced glycation end-products (AGEs) in spinal tissues was suggested as a mechanism for the observed vertebral bone loss and disc degeneration.<sup>(6,7)</sup> AGEs are formed by spontaneous reactions between aldehyde groups of reducing sugars and free functional groups of proteins as well as lipids and nucleic acids (the Maillard reaction).<sup>(8)</sup> AGEs can be produced endogenously as a result of hyperglycemia (eg, with diabetes) or exogenously in food processed, for example, under dry heat.<sup>(9)</sup> Bone tissue accumulation of AGEs has also been correlated with osteoporo-sis<sup>(10)</sup> and increased vertebral fracture risk. <sup>(11)</sup> Nonenzymatic glycation can reduce the strength of cortical and trabecular bone<sup>(12,13)</sup> and can also reduce intervertebral disc water content.<sup>(14)</sup> AGEs are elevated in serum and bone tissue of diabetic patients, and diabetics are known to have increased risk of fracture and spinal stenosis.<sup>(8,15–20)</sup> Diabetic complications such as heart attacks or fractures occur more often in women than in men, $^{(21,22)}$  motivating studies on both sexes. There is also a known sex-dependent fracture risk in diabetics,<sup>(18,19)</sup> further motivating studies on vertebral pathology in both sexes. Taken together, AGEs are strongly implicated as contributing to painful spinal pathologies and diminished vertebral and disc quality, and these effects may have sex differences. However, there are very few studies investigating a direct role of AGEs in spinal pathology.<sup>(11,19,23,24)</sup>

AGEs are prevalent in standard western diets and 10% of ingested AGEs can be found in the blood circulation.<sup>(25)</sup> Diets high in fructose increase AGEs in collagen-rich tissues and cause crosslinking of collagen fibers. These crosslinks can result in increased collagen stiffness, reduced elasticity,<sup>(26)</sup> and crosslinked collagen matrix in bones, which in turn can contribute to decreased bone toughness.<sup>(12)</sup> AGEs can also act via inhibiting parathyroid hormone secretion<sup>(27)</sup> that, in relation to diminished bone formation and turnover, inhibits osteoblast function<sup>(27)</sup> and thus might contribute to the effect of AGEs on inferior bone mechanical behaviors in long bones.<sup>(28,29)</sup> However, spinal tissues often have distinct effects from long bones, and many outstanding questions remain. Dietary AGEs are likely to impact spinal tissues because reduced ingestion of the AGE precursor methylglyoxal in mice was protective of aging-related decreases in vertebral bone quality.<sup>(23)</sup> However, it remains unclear if a high-AGE diet can induce pathological spinal changes and result in functional biomechanical alterations. It also remains unclear if these changes accumulate differently in male or female mice, and if these changes are affected by or accelerate aging. This study tested the overall hypothesis that high dietary AGE ingestion, independent from diabetes, will result in accumulation of AGEs in spinal tissues and induce vertebral changes in young

female mice which amplify vertebral changes and increased fracture risk known to occur with aging.

# Materials and Methods

# Mouse model

This study was carried out in accordance to recommendations stated in the Guide for the Care and Use of Laboratory Animals of the National Institutes of Health (US Department of Health, Education, and Welfare, NIH 78-23, 1996) and all animal protocols were approved by the Mount Sinai Institutional Animal Care and Use Committee (protocol # 2013-1428-PD).

To investigate the sex- and age-dependent effects of dietary AGEs on vertebral bone, 80 male and female C57BL/6J mice were used (Table 1). After weaning, mice were assigned to two pair-fed groups receiving either a low-AGE chow (L-AGE; containing 7.6 µg/mg AGE; Test Diet Low AGE 5053; WF Fisher & Son Co, Somerville, NJ, USA), or high-AGE chow (H-AGE; 40.9 µg/mg, 10 female and 10 male per age group; NIH-31 open formula chow autoclaved for 30min at 120°C). The L-AGE group served as age-and sex-matched control to determine effects of dietary AGEs. Apart from AGE content, diets were identical in caloric and nutritional content.<sup>(30)</sup> Mice were fed ad libitum with ample amounts of water and provided unrestricted cage access. Enrichment tools (safety houses) were added to increase welfare.<sup>(31)</sup> At 6 months or 18 months of age, mice were anesthetized by Ketamine-Xylazine-Acepromazine injection (Forane, Baxter, IL, USA), and then euthanized via cardiac puncture at the termination of the experiment. General observations at termination included body weight, fasting blood glucose, and serum AGE content. Thoracic, lumbar, and coccygeal spines were collected for vertebral structure, mechanical testing, and AGE analyses (Table 2).

# Serum AGEs and fasting blood glucose determination

Blood was collected for analysis of fasting glucose (Aimstrip Plus Glucose Meter; Germaine Laboratories, San Antonio, TX, USA) and serum AGEs (competitive ELISA; developed in our laboratory using an anti-AGE antibody; Abcam, Cambridge, MA, USA; ab23722), for this study 1 unit (U) corresponds to 3 µg AGE-BSA).

## Vertebrae harvest

Following blood collection, thoracic (T<sub>12</sub>), lumbar (L<sub>5</sub>), and coccygeal (CC<sub>4</sub>–CC<sub>6</sub>) spinal segments were dissected and surrounding soft tissue was removed. Thoracic vertebrae were immediately stored at  $-80^{\circ}$ C until mechanical testing. Coccygeal vertebrae were separated into individual cortical and trabecular bone compartments. Collected tissue was submerged in 1% saline and immediately stored at  $-80^{\circ}$ C until further usage for the assessment of total fluorescent AGE content. Lumbar vertebrae were washed in 1× phosphate-buffered saline and scanned by micro–computed tomography ( $\mu$ CT).

# µCT scanning, reconstructions, and volume of interest selections

Lumbar spines were kept hydrated while  $\mu$ CT scanned in air. Lumbar L<sub>5</sub> vertebrae were scanned with a nominal resolution of 4.9  $\mu$ m/pixel with an aluminum filter, 1767 ms of Xray exposure time, and 80 kV × 80  $\mu$ A power (SkyScan 1172; Bruker Corp., Kontich, Belgium). Five consecutive projections were taken and averaged every 0.3 degrees to increase signal to noise ratio. Hydroxyapatite phantoms (0.25 and 0.75 mg/cm<sup>3</sup>) were equally scanned for mineral density calibration. After scanning,  $\mu$ CT projections were reconstructed into cross-sectional images using a modified back-projection algorithm (N-Recon, V1.01; Bruker). Reconstructed  $\mu$ CT images were digitally aligned (Dataviewer V1.01; Bruker) to a common global coordinate system to allow for accurate and consistent measurements of anisotropy. Regions of interest for trabecular bone and cortical bone were hand-drawn (Ctan, V1.01.0; Bruker) and used for cortical and trabecular compartment separation. Analyses of bone densitometry (bone quantity), microarchitecture (bone quality), and anisotropy (bone quality) were performed (Ctan, V1.01.0; Bruker).

3D measures of trabecular bone were assessed using sphere-fitting methods and total pixel counting methods to compute trabecular thickness, separation, number, and bone surface to volume ratio. A mineral density standard curve was generated from the hydroxyapatite phantoms and used along with a global thresholding technique to compute tissue bone mineral density (BMD). Finally, trabecular bone anisotropy was analyzed in 3D using the mean-intercept-length method (MIL), which generated a  $3 \times 3$  tensor of eigenvalues describing the three principal axes along which bone mass is distributed. MIL eigenvalues were transformed into the fabric tensor, which is most commonly used in describing anisotropy, using previously described methods <sup>(32)</sup> to evaluate directional dependent mechanical properties of the bone structure.

Individual 2D cross-sections of cortical bone were analyzed for tissue mineral density, BMD, bone surface area, cross sectional thickness, and porosity. Each measure was then averaged providing a mean value.

# AGE content of cortical and cancellous vertebral bone

Tail vertebrae were dissected and organic tissue and vertebral end plates were removed using standard dissection tools. Bone marrow was removed by flushing the vertebrae with  $1\times$  phosphate-buffered saline. A precision drill (Dremel-4300; Dremel, Racine, WI, USA) was used to separate trabecular and cortical bone by boring a cylinder into the center of the vertebrae using a 26G needle. Trabecular bone tissue was collected by pushing a 30G needle through the 26G needle. Cortical and trabecular bone samples were washed in  $1 \times$  Tris-Buffered-Saline+Tween-20 and sonicated for 5 min (Sonic Dismembrator; Fisher Scientific, Waltham, MA, USA) to remove any remaining organic tissues. AGE content was determined using published protocols.<sup>(12,13)</sup> Briefly, cortical or trabecular bone tissues were flushed with cold Nanopure water until free of blood, defatted, lyophilized, and hydrolyzed according to dry mass in 6 N HCl (10 µL/mg bone) for 16 hours at 110°C. The bulk fluorescence of the hydrolysates was measured using a micro-plate reader (370 nm excitation and 440 nm emission) and normalized to a quinine sulfate standard. The amount of collagen in the sample was estimated based on the amount of hydroxyproline. AGE

# Whole-vertebra mechanical testing to failure

Thoracic vertebrae were stored at-80°C until testing. A precision drill (Dremel-4300) was used to remove the vertebral processes. Superior and inferior vertebral endplates were removed ( $\sim 0.25$  mm total) using a scalpel to create flat and parallel loading surfaces, similar to methods as described.<sup>(33)</sup> Removing endplates provided a more accurate mechanical response with uniform reaction forces across the vertebrae that were interpreted as average properties across vertebral bone, including both cortical and trabecular components but not endplate behaviors. Sample length and diameter (including trabecular and cortical compartments) were measured in multiple locations for each vertebrae. Cross-sectional area was calculated using the average diameter of each vertebrae assuming a circular crosssectional area. Thoracic vertebrae were loaded into parallel-platens of an axial testing machine (Bose ElectroForce 3220; TA Instruments, New Castle, DE, USA), and held in place on the lower platen using a thin layer of cyanoacrylate. Samples were loaded to failure in compression with a displacement-controlled test (at a rate of 0.05 mm/s).<sup>(34)</sup> Forcedisplacement and stress-strain curves were created, from which we determined the maximum values at failure for each specimen of the load, displacement, stress, and strain data. The area under the force-displacement curve to failure and toughness were calculated by integrating the force-deformation and stress-strain curves until the point of failure, respectively.

## Analytical model for trabecular mechanics

The compressive and shear moduli of trabecular bone was calculated using a previously validated analytical model of the trabecular network that accounts for trabecular TMD, fabric anisotropy and bone volume fraction, which were previously measured by  $\mu$ CT scanning and the mean intercept length method.<sup>(32,35)</sup> Trabecular bone fabric anisotropy exhibited orthotropic symmetry, providing three planes of symmetry. The nonzero diagonal elements of the fourth rank elasticity tensor were then calculated using the relationships described by Cowin<sup>(32)</sup> and Turner and colleagues<sup>(36)</sup> with the coefficients calculated by Kabel and colleagues<sup>(35)</sup> and Wagner and colleagues.<sup>(37)</sup> The following equations were used:

$$c_{1111} = E_t [0.0291 + 0.133 \| -0.511\lambda_1 + 0.821\lambda_1^2] + E_t [0.865 - 5.5 \| +5.14\lambda_1 - 0.0754\lambda_1^2] BVF^{1.6}$$

(1)

$$C_{1133} = E_t [-0.00652 + 0.276 \| -0.263 (\lambda_1 + \lambda_3) + 0.263 (\lambda_1^2 + \lambda_3^2) + 0.274\lambda_1\lambda_3] + E_t [0.624 + 11.6 \| -13.4 (\lambda_1 + \lambda_3) + 11.6 (\lambda_1^2 + \lambda_3^2) + 18.8\lambda_1\lambda_2] BVF^{1.6}$$
(2)

$$\log_{10} E_t = -8.58 + 4.05 * \log_{10} \left( 400 / \left( 1 + \left( 0.504 / \text{TMD} \right) \right) \right)$$
(3)

where  $E_t$  is the elastic modulus;  $\lambda_1$ ,  $\lambda_2$ , and  $\lambda_3$  are the three normalized eigenvalues of the fabric tensor; // is the trace of the fabric tensor (// = sum( $\lambda_i \lambda_j$ ), i j, and i, j = 1,2,3); Ciiii is the elastic modulus (C<sub>1111</sub> = compressive elastic modulus in the principal trabecular orientation); and Ciijj is the shear modulus (C<sub>1122</sub> = shear elastic modulus perpendicular to the principal trabecular direction).

# Statistical analyses

For statistical analyses, two-way ANOVAs were used to assess the effects of diet and sex, and the effects of diet and age on the vertebral bone (Tables 3–5). When significant effects were detected, a two-tailed unpaired Student's *t* test with Bonferroni correction to compensate for the number of comparisons was used to identify significant differences between H-AGE and L-AGE diet effects as a function of sex and time. Error bars are displayed as ±SD on all graphs. For all analyses, p < 0.05 was considered significant.

# Results

# H-AGE diet caused elevated serum AGE levels in female mice independent of diabetes or overweight

Serum AGE levels of 6-month-old female H-AGE mice increased by ~78% compared to L-AGE female mice (p = 0.03; Fig. 1*A*). The H-AGE group exhibited significantly elevated blood glucose for 18-month-old females and 6-month-old males, yet the fasting blood glucose levels of all mice were all below prediabetic levels (<100mg/dL; Fig. 1*B*). Body weights of female and male mice were also in normal ranges for mice of this strain at both time points (Fig. 1*C*).<sup>(38)</sup>

# Dietary AGE ingestion had a sex- and age-dependent effects on vertebral AGE accumulation

**Trabecular bone**—Measurements of AGE autofluorescence revealed increased accumulation of fluorescent AGEs in trabecular bone of 18-month-old female and male H-AGE mice compared to 18-month-old L-AGE (female: p = 0.032; male: p = 0.005) or 6-month-old H-AGE mice (female: p < 0.001; male p < 0.001; Fig. 2*A*). Age-dependent effects of L-AGE diet were only observed in female mice (female: p = 0.014; male p > 0.99). No differences were observed in 6-month-old mice (p > 0.99).

**Cortical bone**—AGE accumulation was increased in 6-month-old female H-AGE mice (p = 0.04, Fig. 2*B*), while no differences were observed in male mice (p > 0.99). Compared to

6-month-old mice, in 18-month-old female and male mice H-AGE diet increased AGE accumulation (female: p = 0.009; male: p = 0.035), while L-AGE diets had no effect on aging (p > 0.99). In 18-month-old mice no differences were observed between diets (p > 0.99).

# Dietary AGE ingestion had a sex-dependent effect on vertebral bone microstructure

**Trabecular bone**—µCT analysis of lumbar vertebrae revealed that chronic dietary H-AGE ingestion caused diminished microstructure in 6-month-old female mice (Fig. 3A). At 6 months old, compared to 6-month-old female L-AGE mice, female H-AGE mice had significantly reduced trabecular BMD (p = 0.022, Fig. 3B) and a slight decrease in trabecular bone volume fraction; however, this change was not significant (Table 5). Dietary AGE ingestion did not affect the bone microstructure of male mice (trabecular BMD: p >0.99: trabecular bone volume fraction: p = 0.99) at 6 months old. As expected, aging was identified as an additional risk factor for diminished bone microstructure caused by H-AGE diet for both male and female mice. In female mice, aging caused significantly decreased trabecular BMD for both dietary groups (L-AGE: p = 0.002; H-AGE: p = 0.0001). Trabecular bone volume density decreased with age in both female and male mice (female: L-AGE p = 0.0008, H-AGE p = 0.0004; male: L-AGE p = 0.0088, H-AGE p = 0.0448). No differences between diets were observed at 18 months old (Fig. 3B-F, Table 6), which were likely masked by aging effects as indicated by the large structural changes between age groups. No differences between dietary groups were observed for trabecular thickness, number, spacing, bone surface to volume ratio, bone volume density, degree of anisotropy, and tissue mineral density (Fig. 3*C*–*F*, Table 6).

**Cortical bone**—Contrary to trabecular bone, dietary AGEs did not affect cortical bone quality or quantity of 6-month-old mice (Table 6, Fig. 4*A*–*C*). Interestingly, in 18-month-old mice H-AGE diets caused a decrease in bone quality with decreased cortical BMD and cortical tissue mineral density in both sexes (cortical BMD 18-month-old female = 0.002; 18-month-old male p = 0.03; cortical tissue mineral density: 18-month-old female p = 0.002; 18-month-old male p = 0.01; Table 6, Fig. 4*B*, *C*).

# Dietary AGE ingestion decreased vertebral mechanical properties of 6-month-old female mice

Load to failure testing of thoracic vertebrae demonstrated that, compared to 6-month-old female L-AGE mice, the H-AGE diet and aging caused lower maximum load to failure (6-month-old H-AGE versus L-AGE: p = 0.048; Fig. 5A) while aging resulted in lower maximum stress only in female low-AGE groups (L-AGE 6 months old versus 18 months old: p=0.003; Fig. 5B) and lower maximum strain in female H-AGE mice (H-AGE 6 months old versus 18 months old: p=0.027; Fig. 5D), which was also decreased compared to 18-month-old female L-AGE mice. Only in male mice aging resulted in a lower area under the curve (H-AGE 6 months old versus 18 months old resulted in a lower area under the curve (H-AGE 6 months old versus 18 months old versus 18 months old p= 0.019; Fig. 5E). An H-AGE diet had no further effects on aging. No differences between groups were observed for maximum displacement or toughness (Fig. 5C, F). To assess if the diminished microstructure of trabecular bone was associated with impaired mechanical properties, we performed analytical modeling for trabecular bone. Modeling the trabecular bone properties

revealed that in 6-month-old female mice the H-AGE diet significantly reduced trabecular compressive stiffness (p = 0.048) and shear modulus (p = 0.048) when compared to the L-AGE diet. Aging mainly affected properties of female mice with significantly decreased shear (L-AGE: p = 0.002; H-AGE: p = 0.001) and compressive modulus (L-AGE: p = 0.002; H-AGE: p = 0.001) and compressive modulus (L-AGE: p = 0.044; H-AGE: p = 0.004; H-AGE: p = 0.048). No significant changes were found at 18 months old with H-AGE diet for either female or male mice indicating a larger effect of age than diet on the bone structure as seen by the significant decrease in both compressive and shear stiffness in the H-AGE groups and the L-AGE groups (Fig. 6A, B).

# Discussion

This study determined that a high-AGE diet can result in inferior vertebrae bone quality and inferior mechanical behaviors. We tested the hypothesis that ingestion of dietary AGEs induces vertebral changes in young female mice causing increased vertebral fracture risk that amplifies age-related vertebral changes in mice. The H-AGE diet primarily affected 6-month-old female mice and led to AGE accumulation in serum and cortical bone. The H-AGE diet caused changes in bone mechanical structure and mechanics including reduced trabecular BMD and bone mineral fraction, reduced maximum load to failure, and reduced compressive and shear moduli in 6-month-old females, as well as higher serum AGE, total fluorescent AGE accumulation, inferior vertebral microstructure, and mechanical properties. Aging dominated dietary effects of AGEs in the 18-month-old animals, yet the H-AGE groups had significantly reduced cortical BMD, reduced maximum strain and area under the curve, as well as the lowest mean values for shear and compressive moduli. Together, our data indicate that young females may be at higher risk for developing inferior vertebral structure and function by consuming high levels of dietary AGEs.

Chronic consumption of dietary AGEs can affect a broad-spectrum of diseases<sup>(39)</sup> and AGE accumulation in tissues is implicated in osteoarthritis.<sup>(40,41)</sup> atherosclerotic calcification.<sup>(42)</sup> and vascular/renal and diabetes-related complications.<sup>(8,25,43,44)</sup> In our study mice were fed an H-AGE diet originating from autoclaved mouse chow. Similar to autoclaved chow, bread crust also contains relatively high amounts of AGEs<sup>(45)</sup> and studies on young rats that were fed a diet enriched with bread crust demonstrated increased accumulation of AGEs in serum<sup>(45)</sup> and tibia,<sup>(29)</sup> which led to decreased BMD, and decreased stiffness with lower ability to withstand force and absorb energy to failure.<sup>(29)</sup> Ionova-Martin and colleagues<sup>(46)</sup> demonstrated that a high-fat diet caused AGE accumulation in tibias of 3-week-old adolescent and 15-week-old adult mice, which correlated with a marked reduction in mechanical performance of cortical bone. Although studies on high-fat diets demonstrate significant effects of diet on long bones and serum AGEs, high-fat diet mice are also obese and can develop diabetes, preventing a direct correlation of AGEs with bone morphology. Vertebral bone can have distinct responses compared to long bones, and our study isolated dietary AGEs on vertebral tissues. We concluded that dietary AGE ingestion, in the absence of obesity and diabetes, caused AGE accumulation in serum and vertebral bone tissue and resulted in inferior vertebral bone quantity and mechanical performance.

AGE accumulation is also known to occur in bones with aging, increasing by fourfold to 10fold by age 50 years, <sup>(47)</sup> and increased levels of AGEs in bone tissues have been associated with diminished bone mechanical function<sup>(47–49)</sup> and reduced cortical and trabecular bone strength.<sup>(12,13)</sup> This aging-related increase in vertebral AGE accumulation has been considered a potential cause for vertebral fractures in elderly women and men.<sup>(50,51)</sup> In our study, trabecular and cortical AGE accumulation was also increased with aging, and effects were more prominent for the H-AGE animals than for the L-AGE animals. Together, results suggest that a high-AGE diet may result in an accelerated bone aging phenomena in both sexes. AGEs irreversibly alter proteins, and although we did not measure protein turnover in this study, the accumulation of AGEs in older animals might be due to the decline in protein turnover rate that is known to occur during aging.<sup>(15)</sup> On the other hand, we did not detect increased AGE content in trabecular bone of young animals, which could be associated with the relatively high protein turnover rate in young animals. AGEs increased in cortical bone of young female mice, and it is possible that other AGEs were present but not detectable with our measurement, which did not detect the entire spectrum of AGEs. The standard for AGE measurements in bone are based on fluorescent assays<sup>(52)</sup>; however, the bestcharacterized dietary AGEs are the nonfluorescent AGEs methylglyoxal-H1 and carboxymethyl lysine (CML),<sup>(9,53)</sup> and it is likely that accumulation of these AGEs may have contributed to the inferior bone structure and properties observed in this study.

High-AGE diets and aging both resulted in reduced trabecular bone compression and shear moduli, and these effects were most significant in young female mice. Female mice also exhibited significant reductions in bone failure properties from diet and aging. Therefore, both analytical and experimental

biomechanical data point to functional differences in female vertebrae from diet and aging. Some discrepancies between biomechanical results identified from the analytical model of trabecular bone and whole-vertebra biomechanical testing are likely due to the differences in trabecular bone and whole-vertebrae assessments. Interestingly, a recent study on correlations of diabetes with hip fractures showed that diabetes exerted a much stronger effect on hip fracture risk in younger than older individuals.<sup>(54)</sup> Although that study did not assess sex-dependent effects, results from another study indicated that AGE accumulation could be correlated to vertebral fracture risk in women but not in men.<sup>(55)</sup> Taken together, these studies strongly support our finding that AGE accumulation is most detrimental for young female mice, where bone quantity is at lower levels than for males.

Bone morphology and strength differ between female and male mice, and during aging some of these properties change more rapidly in females than males, limiting the utility of direct comparison between sexes.<sup>(56)</sup> Willinghamm and col-leagues<sup>(56)</sup> reported that female BALB/c mice had superior vertebral mechanical properties with greater strength than male mice, despite inferior trabecular bone mass. In our studies, male mice had greater moduli than female mice, although no differences in failure behaviors were noted between the sexes. It was notable that L-AGE had the strongest effects in females, with young female mice having vertebrae with largest maximum load to failure and greatest compressive and shear moduli.

AGEs form intrafibrillar and interfibrillar crosslinks in collagen networks that can affect trabecular and cortical bone mechanical properties.<sup>(12,13)</sup> AGE accumulation is also thought to directly affect cells and bone formation by impairing osteoclastic bone resorption<sup>(57)</sup> and osteoblast proliferation and differentia-tion.<sup>(52,58)</sup> The literature and our study together show that AGE ingestion can result in AGE accumulation in bone, diminished microstructure and inferior vertebral mechanical properties, decreased whole-bone postyield strength and toughness, and potentially result in the phenomenon known clinically as brittle bone.<sup>(59,60)</sup> Sex hormones may play a role on the AGE-mediated changes in vertebral structure and function observed in this study. Chatzigeorgiou and colleagues<sup>(61)</sup> found that a high-AGE diet increased serum glucose, insulin, and testosterone levels, as well as decreased estradiol and progesterone levels, suggesting there may exist a metabolic and hormonal dysregulation attributed to high-AGE dietary ingestion. Consequently, this study highlights a need for future investigations to identify sex-dependent tissue and cellular mechanisms for these observed effects and means of intervention.

In this study we assessed the direct effects of AGEs on vertebral structures and therefore chose a relatively mild dietary intervention to avoid the development of prediabetes or obesity. AGE content in our autoclaved mouse chow resembled a typical western diet in its high abundance of a variety of different AGEs. One major AGE in the H-AGE diet is the stable and relatively inert CML, which is not very reactive. It is likely that diets higher in reactive AGEs might induce more severe vertebral pathologies, as observed in our previous studies on diabetic<sup>(7)</sup> and prediabetic<sup>(23)</sup> mice, so the risks associated with these dietary AGEs may be larger than those reported here. Compared to the L-AGE diet, the autoclaved diet was harder and crisper and H-AGE mice might have consumed less chow than L-AGE mice. Because of the difference in chow consistency and because mice were grouped housed, we were not able to determine the amount of food ingested.

To our knowledge, this is the first study to demonstrate a sex-dependent effect of a high-AGE diet on vertebral structures and function in mice. Results indicated that dietary AGE ingestion, independent of diabetes and obesity, caused younger female mice to have altered vertebral bone structure with reduced moduli and failure strength, with values that were similar to aged female mice. Results therefore suggest that dietary AGE ingestion is a potential cause of accelerated spinal aging, especially in females.

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Authors' roles: SIJ designed and planned the study, performed and analyzed experiments, wrote the manuscript and was involved in all aspects of the submission. PPM designed, performed and analyzed experiments and was involved in manuscript preparation. WFK performed and analyzed experiments and was involved in manuscript preparation. XC and GES developed assays, performed experiments, reviewed and edited the manuscript. DV analyzed and interpreted data, reviewed and edited the manuscript. JCI designed and planned the study, analyzed and interpreted data, and reviewed and edited the manuscript.

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### Fig. 1.

H-AGE diet significantly increased serum AGE levels only in 6-month-old female mice indicating sex-dependent effects of dietary AGE ingestion on (*A*) serum AGE accumulation. Although the H-AGE diet resulted in some significant increases in blood glucose levels, (*B*) fasting blood glucose (16 hours) remained in euglycemic levels (50-10 mg/dL) and (*C*) body weight remained in normal ranges demonstrating that dietary AGEs induced AGE accumulation independent from diabetes and obesity. \*p < 0.5. mo = months.



# Fig. 2.

H-AGE diet led to AGE accumulation in (*A*) Tb bone in 18-month-old mice of both sexes. In addition to dietary AGE accumulation, in female mice, aging caused AGE accumulation independent from diet. (*B*) H-AGE diet caused increased AGE accumulation in Ct bone of 6-month-old female mice, while aging dominated diet effects in both sexes, indicating sexand diet-dependent effects of AGE accumulation in bone. \*p < 0.05; \*\*p < 0.001. mo = months; Tb = trabecular; Ct = cortical; COL = collagen.



# Fig. 3.

H-AGE intake induced pathological changes in trabecular vertebrae of 6-month-old female mice. (*A*) 3D  $\mu$ CT images of Tb bone of (top) 6-month-old and (bottom) 18-month-old mice. (*B*) Tb.BMD, (*C*) Tb.BV/TV and (*D*) Tb.Sp demonstrate inferior Tb microstructure in female 6-month-old H-AGE mice. (*B-F*) Aging dominated diet effects in both sexes. \**p* < 0.05, \*\**p* < 0.001. Tb = trabecular; Tb.BMD = trabecular bone mineral density; Tb.BV/TV = trabecular bone volume fraction; Tb.Sp = trabecular separation; Tb.Th = trabecular thickness; Tb.N = trabecular number; mo = months.



# Fig. 4.

H-AGE intake led to inferior microstructure of cortical vertebrae in 18-month-old mice. (A) 3D  $\mu$ CT images of Ct bone for (top) 6-month-old and (bottom) 18-month-old mice. H-AGE diet decreased (*B*) Ct.BMD in 18-month-old mice; (*C*) Ct.Th decreased with age, and aging effects dominated any potential diet effects. \*p < 0.05, \*\*p < 0.001. mo = months; Ct = cortical; Ct.BMD = cortical bone mineral density; Ct.Th = cortical thickness.





H-AGE diet led to lower ex vivo vertebral fracture resistance in mice. (*A*) Max load at failure; (*B*) max stress; (*C*) max displacement; (*D*) max strain; (*E*) AUC; and (*F*) toughness were defined by a fracture mechanics load-displacement curve. \*p < 0.05. Max = maximum; AUC = area under the curve; Displ = displacement.



# Fig. 6.

H-AGE diet led to lower Tb bone moduli in 6-month-old female mice with significantly lower (A) shear modulus and (*B*) compression modulus along the principal Tb axis that were calculated from an anisotropic model in the direction of the principal trabecular axis. Moduli were computed considering effects of mass density, porosity, and structural directionality. \**p* < 0.05, \*\**p* < 0.001. mo = months; Tb = trabecular.

# Table 1

# Study Design

Diet	п	Age (months)	Sex
Low AGE (L-AGE)	10/group	6	Male
		6	Female
		18	Male
		18	Female
High AGE (H-AGE)	10/group	6	Male
		6	Female
		18	Male
		18	Female

AGE = advanced glycation end-product.

				Table 2
Sample	Collection	for	Dependent	Variables

Sample collection	Dependent variable
Blood	Fasting glucose
	Serum AGEs
Thoracic spine	Maximum load from fracture mechanics
Lumbar spine	Microstructure, analytical mechanical properties
Coccygeal spine	Total fluorescent AGE

AGE= advanced glycation end-product.

# Values of p from Two-Way ANOVA for General Observation and AGE Accumulation

			Diet:.	Age (p)					Diet:S	ex ( <i>p</i> )		
	و ًا	months		18	months			Female			Male	
	Interact	Diet	Sex	Interact	Diet	Sex	Interact	Diet	Age	Interact	Diet	Age
Body weight	0.122	0.233	0.017	0.503	0.816	0.774	0.890	0.723	0.009	0.638	0.054	0.018
Blood glucose	0.02	0.189	0.679	0.025	0.008	0.127	0.060	0.270	0.881	0.056	0.020	0.232
AGE serum	0.195	0.001	0.040	0.126	0.396	0.501	0.016	0.237	0.044	0.634	0.011	<0.001
AGE trabecular	0.213	0.202	0.741	0.269	<0.001	0.119	0.016	0.016	<0.001	0.001	0.024	<0.001
AGE cortical	0.340	0.017	0.683	0.901	0.119	0.314	0.596	0.119	<0.001	0.927	0.002	0.231

AGE = advanced glycation end-product; Interact = interaction.

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Table 4

Values of p From Two-Way ANOVA Results for Trabecular and Cortical Bone Quantity and Quality From µCT Analysis

				Diet: /	Age (p)					Diet: S	iex (p)		
		9	months		1	8 months			Female			Male	
		Interact	Diet	Sex	Interact	Diet	Sex	Interact	Diet	Age	Interact	Diet	Age
Trabecular	Tb.Th (mm)	0.037	0.590	0.487	0.626	0.181	0.579	0.619	0.094	0.014	0.066	0.741	0.156
	Tb.N (1/mm)	0.9120	0.032	<0.001	0.675	0.362	<0.001	0.918	0.122	<0.001	0.521	0.239	<0.001
	Tb.Sp (mm)	0.589	0.070	<0.001	0.626	0.567	<0.001	0.934	0.297	<0.001	0.608	0.509	<0.001
	Tb.BS/BV (mm <sup>-1</sup> )	0.041	0.693	0.552	0.910	0.113	0.234	0.618	0.016	0.651	0.155	0.984	0.384
	Tb.DA ([])	0.891	0.460	<0.001	0.820	0.903	0.986	0.707	0.875	0.413	0.794	0.603	<0.001
	Tb.TMD (g HA/cm <sup>3</sup> )	0.0550	0.810	0.981	0.384	0.140	0.158	0.842	0.033	0.002	0.261	0.628	<0.001
	Tb.BMD (g/cm <sup>3</sup> )	0.206	0.203	<0.001	0.680	060.0	<0.001	0.910	0.015	<0.001	0.527	0.523	0.003
	Tb.BV/TV (%)	0.298	0.214	<0.001	0.893	0.213	<0.001	0.771	0.059	<0.001	0.640	0.526	<0.001
Cortical	Ct.BS/BV (mm <sup>-1</sup> )	0.011	0.944	<0.001	0.388	0.608	0.001	0.127	0.259	<0.001	0.087	0.695	<0.001
	Ct.TMD (g HA/cm <sup>3</sup> )	0.132	0.850	0.001	0.942	<0.001	0.606	0.290	0.002	0.001	0.007	0.236	0.510
	Ct.BMD (g/cm <sup>3</sup> )	0.159	0.992	0.001	0.955	<0.001	0.613	0.202	0.004	<0.001	0.010	0.281	0.842
	Ct.Th (mm)	0.023	0.823	<0.001	0.863	0.907	0.015	0.206	0.227	<0.001	0.256	0.395	0.001
	Tt.Ar (mm <sup>2</sup> )	0.174	<0.001	0.958	0.321	0.169	0.612	0.752	0.133	0.097	0.235	0.494	0.003

Bold values are signifcant.

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tissue mineral density; Tb.BMD =trabecular bone mineral density; Tb.BV/TV =trabecular bone volume density; Ct.BS/BV = cortical bone surface to volume ratio; Ct.TMD =cortical tissue mineral density; Ct.BMD= cortical bone mineral density; Ct.BMD = cortical thickness; Tt.Ar=cortical total area. Tb.Th = trabecular thickness; Tb.N = trabecular number; Tb.Sp=trabecular separation; Tb.BS/BV=trabecular bone surface to volume ratio; Tb. DA = trabecular degree of anisotropy; Tb.TMD= trabecular

Table 5

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			Diet:	Age (p)					Diet:Se	ex ( <i>p</i> )		
	9	months		1	8 months			Female			Male	
	Interact	Diet	Sex	Interact	Diet	Sex	Interact	Diet	Age	Interact	Diet	Age
Maximum load (N)	0.091	0.015	0.055	0.939	0.357	0.004	0.089	0.014	0.194	0.940	0.356	0.026
Toughness (MPa)	0.195	0.307	0.866	0.331	0.046	0.367	0.879	0.017	0.417	0.482	0.752	0.132
Maximum displacement (mm)	0.918	0.703	0.854	0.208	0.222	0.092	<0.001	<0.001	<0.001	0.697	0.99	<0.001
Maximum stress (MPa)	0.043	0.146	0.063	0.897	0.018	0.855	0.010	0.326	0.034	0.399	0.098	0.915
Maximum strain (MPa)	0.447	0.350	0.060	0.039	<0.001	0.535	0.00	0.014	0.837	0.053	0.974	0.004
AUC (N*m)	0.946	0.386	0.315	0.450	0.1057	0.013	0.697	0.223	0.046	0.795	0.288	0.001
Shear modulus (GPa)	0.277	0.323	<0.001	0.828	0.253	<0.001	0.423	0.035	<0.001	0.543	0.598	0.002
Compressive modulus (GPa)	0.261	0.449	<0.001	0.995	0.163	<0.001	0.526	0.011	<0.001	0.489	0.720	<0.001
Bold values are signifcant.												

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Table 6

Trabecular and Cortical Bone Quantity and Quality From µCT Analysis

				0 DC	sunus				-					0 Vers	us 18 mon	(b)	
			Female			Male			Female			Male		Femi	ale	Ma	e
		L-AGE	H-AGE	Ρ	L-AGE	H-AGE	P	L-AGE	H-AGE	Ρ	L-AGE	H-AGE	Ρ	L-AGE	H-AGE	L-AGE	H-AGE
ular	Tb.Th (mm)	$0.58 \pm 0.01$	$0.56 \pm 0.01$	0.607	$0.06 \pm 0.01$	$0.06 \pm 0.01$	0.513	$0.056 \pm 0.01$	$0.06 \pm 0.01$	>0.99	$0.06 \pm 0.06$	$0.06 \pm 0.01$	>0.99	0.42	0.277	0.032	>0.99
	Tb.N (1/mm)	$3.65 \pm 0.24$	$3.37 \pm 0.40$	0.337	$4.42 \pm 0.18$	$4.12 \pm 0.64$	>0.99	<b>2.34</b> ±0.73	<b>2.12</b> ±0.56	0.001	$3.30\pm\!0.55$	$3.21 \pm 0.66$	>0.99	0.001	0.001	0.001	0.015
	Tb.Sp (mm)	$0.25 \pm 0.01$	$0.27\pm0.03$	0.311	$0.19 \pm 0.01$	$0.20\pm0.04$	>0.99	$0.39\pm0.08$	$0.40\pm0.07$	>0.99	$0.23\pm0.04$	$0.24\pm0.03$	>0.99	0.001	0.001	0.001	0.051
	Tb.BS/BV $(mm^{-1})$	57.11 ±2.85	$60.10 \pm 2.97$	0.135	58.92 ±3.27	56.87 ±5.36	>0.99	$57.16 \pm 3.88$	$59.15 \pm 3.06$	0.737	55.67 ±4.36	57.66 ±5.52	>0.99	>0.99	>0.99	0.179	>0.99
	Tb.DA ([])	$2.10 \pm 0.17$	$2.05 \pm 0.13$	>0.99	$2.34 \pm 0.15$	$2.30 \pm 0.15$	>0.99	$2.02 \pm 0.12$	$2.03 \pm 0.26$	>0.99	$2.04\pm\!0.19$	$2.02\pm0.20$	>0.99	>0.99	>0.99	0.001	0.006
	Tb.TMD (g HA/cm <sup>3</sup> )	$0.90\pm0.03$	$0.87\pm0.02$	0.542	$0.88\pm0.03$	$0.89 \pm 0.01$	0.984	$0.92\pm0.03$	$0.90\pm0.04$	0.525	$0.93\pm0.03$	$0.92\pm0.04$	>0.99	0.091	0.184	0.004	0.004
	Tb.BW/TV (%)	$21.11\pm1.56$	$18.84 \pm 2.40$	0.096	$24.80\pm2.25$	$24.60\pm4.98$	>0.99	$14.16 \pm 4.54$	$12.49 \pm 3.57$	>0.99	$20.28 \pm 4.25$	$18.93 \pm 4.30$	>0.99	0.001	0.001	0.001	0.045
	Tb.BMD (gm/cm <sup>3</sup> )	$0.25 \pm 0.02$	$0.23\pm0.02$	0.022	$0.28 \pm 0.03$	$0.28 \pm 0.05$	>0.99	$0.19\pm\!0.05$	$0.16\pm\!0.03$	>0.99	$0.25\pm0.04$	$0.24\pm0.04$	>0.99	0.002	0.001	>0.99	060.0
I	Ct.BS/BV (mm <sup>-1</sup> )	$35.41 \pm 1.85$	37.41	0.21	$40.34 \pm 2.21$	$38.45 \pm 2.61$	0.384	$40.84 \pm 2.59$	$40.54\pm2.64$	>0.99	$43.75 \pm 3.51$	$44.94\pm3.09$	>0.99	0.377	0.001	0.026	0.001
	Ct.TMD (g HA/cm <sup>3</sup> )	$1.06 \pm 0.41$	$1.04\pm0.03$	0.95	$1.01 \pm 0.05$	$1.02\pm0.02$	>0.99	$1.04 \pm 0.02$	$1.00\pm0.02$	0.002	$1.04\pm0.02$	$0.10\pm\!0.02$	0.011	0.561	0.004	0.284	0.277
	Ct.BMD (gm/cm <sup>3</sup> )	$1.05\pm0.04$	$1.04\pm0.02$	>0.99	$1.00\pm0.05$	$1.02\pm0.02$	>0.99	$1.03 \pm 0.02$	$1.00\pm0.22$	0.002	$1.02\pm0.03$	$0.99\pm0.04$	0.024	>0.99	0.001	>0.99	>0.99
	Ct.Th (mm)	$0.07\pm0.00$	$0.07 \pm 0.01$	>0.99	$0.06\pm0.00$	$0.06\pm0.00$	>0.99	$0.06\pm0.00$	$0.06\pm0.01$	>0.99	$0.07\pm0.01$	$0.06\pm0.00$	>0.99	0.001	0.07	>0.99	0.02
	TLAr (mm <sup>2</sup> )	$0.35\pm\!0.03$	$0.34\pm0.04$	>0.99	$0.29 \pm 0.02$	$0.31 \pm 0.03$	>0.99	$0.34\pm0.03$	$0.32\pm0.04$	>0.99	$0.32\pm\!0.02$	$0.32\pm0.02$	>0.99	>0.99	>0.99	0.009	>0.99

Values are mean  $\pm$  SD. Bold values are significant.

L-AGE = low level of advanced glycation end-products; H-AGE = high level of advanced glycation end-products; Tb.Th = trabecular thickness; Tb.N = trabecular number; Tb.Sp = trabecular separation; Tb.BS/BV = trabecular bone surface to volume ratio; Tb.DA = trabecular bone surface of anisotropy; Tb.TMD = trabecular tissue mineral density; Ct.BMD = trabecular bone wineral density; Tb.BV/TV = trabecular bone volume density; Ct.BS/BV = cortical bone surface to volume ratio; Ct.TMD = cortical tissue mineral density; Ct.BMD = cortical bone surface to volume ratio; Ct.TMD = cortical tissue mineral density; Ct.BMD = cortical bone with the trabecular bone with the trabecular bone volume density; Ct.BS/BV = cortical bone surface to volume ratio; Ct.TMD = cortical tissue mineral density; Ct.BMD = cortical bone with the trabecular bone with the tr mineral density; Ct.Th = cortical thickness; Tt.Ar = cortical total area.