FULL PAPER

Carotid artery ultrasound texture, cardiovascular risk factors, and subclinical arterial disease: the Multi-Ethnic Study of Atherosclerosis (MESA)

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Objective: This pilot study determined if the ultrasound texture feature "contrast" was associated with cardiovascular disease (CVD) risk factors and subclinical arterial disease.
Methods: We evaluated ultrasound images of the right common carotid artery (CCA) from a convenience sample of 151 participants and examined relationships between contrast, CVD risk factors, carotid intima-media thickness (IMT) and coronary artery calcium (CAC). Grey level difference statistics algorithms were used to evaluate the texture feature "contrast" from carotid ultrasound images. Right CCA IMT measurements were made in triplicate in the distal 1 cm segment of the far wall of the artery and CAC score was measured using the Agatston scoring method.

Results: In individual models that included age, sex and race, grey level difference statistics contrast (outcome) was associated independently with age [beta (standard error) = −0.87 (0.38) per year; p = 0.02], C-reactive protein [−2.22 (0.96) per mg dl^{-1}; p = 0.02], high-density lipoprotein cholesterol   [0.61 (0.24) per mg dl^{-1}; p = 0.01] and CCA IMT [−0.06 (0.02) microns; p = 0.001]. Other CVD risk factors and CAC were not associated independently with contrast.
Conclusion: These findings support the potential use of the ultrasound texture contrast for evaluating arterial injury and CVD risk.
Advances in knowledge: This paper contributes to the literature in that it describes how the greyscale texture feature "contrast" is related to CVD risk factors.

INTRODUCTION

Image processing is used to characterize tissues and detect subtle differences associated with preclinical disease states.[1] In ultrasound, image processing methods of texture analysis can characterize the arterial wall.[2–4] Greyscale median (GSM) is the most frequently used greyscale parameter to describe the overall echodensity of the arterial wall and lower GSM values (darker walls) are associated with greater cardiovascular disease (CVD) risk and risk factors.[5–7] GSM describes the echodensity of the arterial wall within a selected region of interest. However, it does not provide information about the distribution and spatial relationships of the greyscale values of the pixels,[2,4,8,9] which might be a better descriptor of arterial wall changes associated with early atherosclerosis.[2,3]

The grey level difference statistics (GLDS) method overcomes this limitation by studying the distributions of grey levels and the spatial relationships of ultrasound pixels to each other.[3,8,10–13] GLDS contrast also provides information regarding tissue heterogeneity.[10,11] In cardiac ultrasound, GLDS contrast (an ultrasound texture feature that describes spatial differences in greyscale brightness among image pixels)[8] has shown differences between normal and myopathic myocardium in humans and myocardial contusion in animal models.[10,11] GLDS methods also have been used in vascular ultrasound imaging to assess plaque and arterial wall characteristics and to relate them to cerebrovascular symptoms and histopathology findings.[3,9,13,14] Plaque with low GSM and texture measures of homogeneity has been associated with features of plaque instability at histopathology examination.[9] In unstable plaques, lipids

and/or inflammatory cells may replace normal fibrous tissue, resulting in fewer specular reflectors on ultrasound imaging and the appearance of a more homogeneous plaque.[9]

The purpose of this study was to determine if the ultrasound texture feature "contrast" was associated with CVD risk factors and subclinical arterial disease. We hypothesized that this novel texture measure of contrast may represent one of the earliest ultrasound changes of the arterial wall, prior to wall thickening and plaque formation.

METHODS AND MATERIALS

Participants

This is a pilot study of images from 151 participants in the Multi-Ethnic Study of Atherosclerosis (MESA) from 2000 to 2002. MESA is a large, prospective cohort study that investigated the prevalence and risk factors associated with subclinical CVD and its progression (Bild et al 2002).[15] We chose a convenience sample—the first 151 readable images—from participants initially selected to be part of a case–cohort study to determine the feasibility of evaluating multiple features of carotid arterial stiffness and greyscale features.

At the time of recruitment, male and female participants were 45 to 84 years old and free of clinically known CVD.[15–17] This specific study sample was obtained from four out of six MESA field centres (Baltimore City and Baltimore County, MD; Chicago, IL; Los Angeles County, CA; Northern Manhattan and the Bronx, NY) that used the same carotid ultrasound preset and greyscale map (as described below and in Table 1). All subjects provided written informed consent at their respective field centres. The MESA study objectives and design have been previously published.[15] This study was approved by all participating field centres and the University of Wisconsin Institutional Review Boards.

Risk factor measurements

Laboratory, medical history and demographic data were obtained during MESA (July 2000–August 2002). MESA participants answered a standardized questionnaire in which data regarding age, sex, race/ethnicity, medication history and cigarette smoking status were collected. High-sensitivity C reactive protein (CRP), interleukin-6, glucose and total and high-density lipoprotein cholesterol (HDL-C) levels were measured from blood samples acquired after a 12-h fast and measured at a centralized laboratory.[16–18] Impaired fasting glucose was defined as a fasting glucose level of 100–125 mg dl^{-1}[16]and diabetes mellitus was defined as a blood glucose level $\geq$126 mg dl^{-1} or use of an antidiabetes medication.[17,18]

Blood pressure was measured in triplicate in the right arm using a Dinamap model Pro 100 automated oscillometric sphygmomanometer (Critikon; Tampa, FL). All measurements were made with the participant seated in a quiet room for 5 minutes prior to blood pressure measurement and the average of the last two measurements were used for analysis.[15,17,18] Hypertension was defined as a systolic blood pressure greater than 140 mmHg, diastolic blood pressure greater than 90 mmHg or treatment with antihypertensive medication.[17,18] Cigarette smoking status was categorized as current, former or never.[17,18] Coronary artery calcium (CAC) score was measured using the Agatston scoring method and reported as a continuous variable.[19, 20] CT scanning and reading methods for MESA have been previously reported.[19]

Carotid ultrasound imaging intima-media thickness measurements

High-resolution B-mode images of the right and left common carotid arteries (CCAs) were obtained from 2000–2002.[15,21] A Logiq 700 ultrasound system and an M12L linear transducer (General Electric Medical Systems, Waukesha, WI) were used to acquire all ultrasound images and record on videotape. Images were digitized from the video tape using the Medical Digital Recording (MDR) device (PACSGEAR, Pleasanton, CA). Once digitized, images were converted to DICOM digital records[16,21] (Table 1 for ultrasound instrumentation settings).

For intima-media thickness (IMT), digital images were imported into the Syngo Ultrasound Workplace reading stations and then measured using the Arterial Health Package software (Siemens Medical, Malvern, PA).[21] Right CCA IMT measurements were made in triplicate in the distal 1 cm segment of the far wall of the artery. IMT was defined as the mean of the mean right far wall distal CCA thickness.[21] If plaque was present in the distal segment of the CCA, it was included in the CCA IMT measurement.[21] All IMT measurements were performed at the University of Wisconsin Atherosclerosis Imaging Research Program Laboratory (UW AIRP), MESA Carotid Ultrasound Reading Center (Madison, WI, PI: J. Stein).

Greyscale median and contrast measurement

Image viewing software (Access Point, Freeland Systems, Alpharetta, GA) was used to convert the carotid ultrasound DICOM files into BITMAP images that were used for greyscale analysis and measurement of GSM and GLDS contrast. Images were normalized to assign the blackest area of the blood a greyscale value of 0 and the whitest area of the middle two-fourths of the adventitia a greyscale value of 190 (LifeQ Medical, Cyprus).[22,23] Images were then standardized to a uniform pixel

Table 1. MESA carotid ultrasound instrumentation settings

Ultrasound system	Logiq 700 ultrasound system (General Electric Medical Systems, Waukesha, WI)
Transducer	M12L Linear transducer
Transducer frequency	13 MHz
Overall gain setting	Optimized for each patient
Time gain compensation settings	Optimized for each patient
Dynamic range)	66
Edge enhance	E3
Average settings	A2
Greyscale map	MG

Figure 1. (a) Demonstrates a normalized and standardized image of a common carotid artery with a far wall greyscale median (GSM) value of 8.1 and a grey level contrast value of 53.6, gain setting 31 (red circle). (b) Demonstrates an artery with a GSM value of 79.5 and contrast value of 121.6 (representative of the mean grey level difference statistics contrast value for this study), gain setting 37 (red circle). (c) Demonstrates an artery with a GSM value of 94.6 and a grey level difference statistics contrast value of 299.3, gain setting 32 (red circle). (d) Represents a GSM value of 120.9, a contrast of 68.7 and a gain setting of 38.
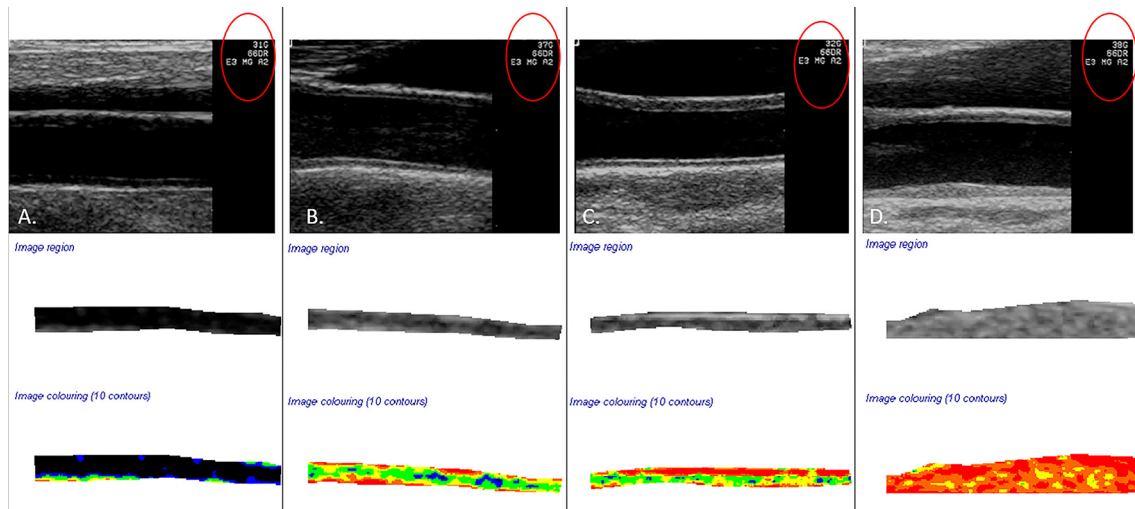
density of 20/mm.[22,23] The distal 1.0 cm of the far wall of the right CCA was traced utilizing an online ruler tool to define the length of 1.00 cm. GSM of the CCA intima-media complex was calculated by taking the median grey level value within the traced region of interest in the arterial wall using plaque texture analysis software (LifeQ Medical, Cyprus).

GLDS contrast was measured from the same region of interest as the GSM. GLDS are computed by calculating the absolute difference in greyscale values between pixels at a given distance and direction and can be used to describe pixel–greyscale relationships.[1,3,10–12,24–28] Images that have low GLDS contrast will have more pixels with the same greyscale value and images that have high GLDS contrast will have large differences in greyscale values between pixels (Figure 1). The LifeQ GLDS algorithm uses the probability density function $p_\delta(i)$ to express the likelihood that two image pixels, separated by a distance $\delta = (\Delta\chi, \Delta y)$, will have an absolute difference in greyscale value, i[27,29] (Supplementary Material 1, Supplementary material available online). For this study, we extracted the texture feature GLDS contrast using the LifeQ software [Equation (1)].[27,29]

$$CON = \sum i^2 p_\delta(i) \qquad (1)$$

where CON is contrast, i represents the difference in greyscale value between two pixels and $p_\delta(i)$ represents the individual probabilities.

Statistical analysis
Continuous variables are reported as mean (standard deviation) and categorical variables as counts and percentages. CAC Agatston values were log transformed after addition of 1 to account for zeros and skewed distributions. Pearson correlations and multivariable linear regression models (adjusted for age, sex and race/ethnicity) were used to examine relationships

between GLDS contrast (outcome variable) and CVD risk factors [age, body mass index (BMI), total cholesterol, HDL-C, low-density lipoprotein cholesterol, triglycerides, hypertension, diabetes mellitus, cigarette smoking, glomerular filtration rate, CRP, interleukin-6, D-dimer, fibrinogen, alcohol consumption, education level, physical activity level, statin use], carotidIMT, CAC and 10-year American College of Cardiology/American Heart Association (ACC/AHA) risk score for CVD.[30] Models with lipids and CRP included additional adjustment for statin use. All analyses were conducted using Stata/IC version 14.0 (College Station, Texas).

RESULTS
Participants (Table 2)
The 151 participants were of mean (standard deviation) age 68 (9) years (54% female; 31% Hispanic, 28% Black, 10% Chinese, and 31% White).

Greyscale median values
GSM was weakly correlated inversely with BMI ($r = -0.18$; $p < 0.05$) and high school education (-0.18; $p < 0.05$). GSM was also associated with race; Chinese and Hispanic participants had higher GSM values on average ($p < 0.05$). No significant correlations were noted between GSM and other CVD risk factors or with CCA IMT, CAC or CVD risk score (p values all > 0.05). In models that included age, sex and race, GSM was associated independently with BMI [beta (standard error) = -0.82 (0.38) kg m^{-2}; $p = 0.03$]. Other risk factors were not significantly associated with GSM nor were IMT, CAC or CVD risk score (p-values all >0.05)

Grey level contrast (Table 3)
GLDS contrast correlated inversely with CCA IMT ($r = -0.33$; $p < 0.05$) and CRP (-0.18; $p < 0.05$) and positively with HDL-C ($r = 0.23$; $p < 0.05$). No significant correlations were noted

Table 2. Participant characteristics

Variable	N (%) OR Mean (SD)
Age, years	68.1 (9.2)
Female, *n* (%)	82 (54.3)
Race/ethnicity	
White	47 (31.1)
Chinese	15 (9.9)
Black	42 (27.8)
Hispanic	47 (31.1)
Smoking status	
Never	77 (51.0)
Former	57 (37.7)
Current	17 (11.3)
Body mass index (kg m^{-2})	27.5 (4.8)
Total cholesterol (mg dl^{-1})	199.5 (41.8)
High-density lipoprotein cholesterol (mg dl^{-1})	53.7 (16.5)
Low-density lipoprotein cholesterol (mg dl^{-1})	121.4 (36.9)
Triglycerides (mg dl^{-1})	128.7 (82.2)
Estimated glomerular filtration rate (ml min^{-1}/1.73 m^2)	76.8 (18.5)
Intentional exercise (MET-hours/week)	24.8 (34.4)
C-reactive protein (mg l^{-1})	3.52 (3.7)
Interleukin-6 (pg ml^{-1})	1.76 (1.1)
D-dimer (µg l^{-1})	0.44 (0.55)
Fibrinogen (mg dl^{-1})	362.5 (73.8)
American College of Cardiology/American Heart Association Cardiovascular Risk Score (%)	20.4 (16.5)
CAC Score [ln (Agatston + 1)]	3.48 (2.62)
Common carotid artery intima-media thickness (microns)	866.1 (210.4)
GLDS contrast (unitless)	121.3 (42.6)
GSM (unitless)	56.8 (22.4)

CAC, coronary artery calcium; GLDS, grey level difference statistics; GSM, greyscale median; SD, standard deviation.

between GLDS contrast and other CVD risk factors, CAC or American College of Cardiology/American Heart Association risk score (*p* values all > 0.05). In individual models that included age, sex and race, GLDS contrast (outcome) was associated independently with age [beta (standard error) = −0.87 (0.38) per year; *p* = 0.02], CRP [−2.22 (0.96) per mg dl^{-1}; *p* = 0.02], HDL-C [0.61 (0.24) per mg dl^{-1}; *p* = 0.01] and CCA IMT [−0.06 (0.02) microns; *p* = 0.001]. (Table 3). Other CVD risk factors and CAC were not associated independently with GLDS contrast (*p*-values all >0.05).

DISCUSSION

In this study of individuals without known CVD, we demonstrated that low GSM was associated with greater BMI but no other CVD risk factors. However, lower greyscale texture contrast was associated with greater age, lower HDL-C, higher CRP and higher carotid IMT, observations that suggest that it may reflect a different aspect of arterial injury than GSM and may be useful for evaluating arterial injury and CVD risk.

Greyscale characteristics of the arterial wall may represent some of the earliest *in vivo* changes associated with arterial injury.[2,4] To date, the most frequently used greyscale ultrasound parameter used to study the arterial wall for assessment of CVD risk is the GSM value.[4,6,7,31] This is a simple measure that provides the overall median value of a segment of the arterial wall, but does not take into account the distribution and differences of grey levels within the wall.[8] Low GSM (*i.e.* hypoechoic/echolucent/darker) arterial walls have been associated with markers of inflammation, dyslipidemia and increased CVD risk.[5–7,32] Indeed, in our small study, lower GSM was associated with greater BMI.

Early changes in atherogenesis are associated with changes in the echo texture of the arterial wall that may occur prior to thickening detected by ultrasound.[2,4] We evaluated the GLDS texture feature, contrast, because we hypothesized that it might describe early greyscale changes associated with lipid infiltration and inflammation of the arterial wall that might not be detected by GSM. On ultrasound, fat appears hypoechoic and will have a lower GSM value than fibrous tissue or calcium.[33] Therefore, as lipids infiltrate the arterial wall, it would be expected that the wall will become more hypoechoic with less contrast due to less difference in greyscale values between pixels. Indeed, plaques with increased echolucency (lower GSM) and that were more homogeneous were associated with higher histopathological plaque classification scores, suggesting that increasing lipid content may be associated with increasing homogeneity.[9] Increasing homogeneity in a plaque represents instability based on an increased amount of lipid compared to echogenic fibrous structures.[9] If a similar process occurs in plaque-free areas of the arterial wall, it may indicate that as lipid infiltrates the wall, it becomes more hypoechoic with less contrast as lipid replaces more echogenic fibrous structures.

Inflammation associated with arteritis has also been noted to have a hypoechoic appearance on ultrasound imaging,[34] possibly due to oedema.[35,36] With treatment, the walls decrease in thickness and become more hyperechoic.[35,36] Homogeneous plaques with low GSM are associated with increased lipid content and additional features of plaque instability such as inflammation and less fibrous tissue.[9] Our findings of low contrast being associated with higher values of CRP may represent inflammation in the arterial wall, similar to the findings of increased inflammation seen with plaques, in which plaques that were more hypoechoic and homogeneous were associated with larger lipid cores and higher scores of inflammation at histopathology examination.[9]

Low ultrasound texture contrast does not necessarily represent low GSM: Arterial walls may be bright or dark but have low

Table 3. Age, sex and race-adjusted models for right common carotid artery GLDS contrast[a]

Covariate	Beta coefficient	Standard error	*p* value	95% confidence interval
Age	−0.87	0.38	**0.02**	−1.62,−0.12
Body mass index (kg m^{-2})	−0.02	0.73	0.98	−1.50, 1.47
Total cholesterol (mg dl^{-1})	0.03	0.09	0.74	−0.15, 0.20
High-density cholesterol (mg dl^{-1})	0.61	0.24	**0.01**	0.13, 1.09
Low-density cholesterol (mg dl^{-1})	−0.003	0.099	0.98	−0.19, 0.20
Triglycerides (mg dl^{-1})	−0.003	0.05	0.96	−0.10, 0.09
Estimated glomerular filtration rate (ml min^{-1}/1.73 m^2)	−0.30	0.20	0.13	−0.69, 0.09
Intentional exercise (MET-hours/week)	0.16	0.10	0.12	−0.04, 0.36
C-reactive protein (mg l^{-1})	−2.22	0.96	**0.02**	−4.11,−0.33
Interleukin-6 (pg ml^{-1})	1.29	3.26	0.69	−5.15, 7.72
D-Dimer (ug ml^{-1})	4.70	6.63	0.48	−8.40, 17.81
Fibrinogen (mg dl^{-1})	0.01	0.05	0.78	−0.08, 0.11
Smoking status				
Former	4.80	8.13	0.56	−11.27, 20.86
Current	−11.04	11.62	0.34	−34.00, 11.93
Alcohol use				
Yes	3.96	8.75	0.65	−13.34, 21.30
Diabetes mellitus				
Yes	−1.01	9.35	0.91	−19.50, 17.47
Statin use				
Yes	9.17	8.64	0.29	−7.91, 26.25
Hypertension				
Yes	−9.77	7.23	0.18	−24.05, 4.52
Common carotid artery IMT	−0.06	0.02	**0.001**	−0.09,−0.02
CAC: Ln(Agatston + 1)	−1.19	1.6	0.46	−4.34, 1.97
American College of Cardiology/American Heart Association Cardiovascular Risk Score (%)	0.06	0.29	0.84	−0.52, 0.64

CAC, coronary artery calcium; GLDS, grey level difference statistics; IMT, intima-media thickness; MET, metabolic equivalent task.
[a]All data are from models adjusted for age, sex and race with addition of the parameter in each row above. Models for total cholesterol, HDL, LDL, triglycerides and CRP are additionally adjusted for use of statins.

contrast. Risk factors associated with GSM and IMT differ when measured in the same segment.[32] We further demonstrated different patterns of CVD risk factor relationships between GSM and GLDS contrast, including a different relationship with IMT, suggesting that these ultrasound parameters measure different structural aspects of the arterial wall and that heterogeneity in specular reflectors vary with risk factors and wall thickening. As changes in the arterial wall structure occur with early injury, we hypothesize that texture contrast may change first, followed by overall echogenicity changes, such as GSM values, and then wall thickening and plaque formation.

Limitations
Imaging was performed with an ultrasound system that no longer is state of the art. At the time of acquisition, sonographers were

allowed to optimize the overall gain and time gain compensation for each subject. This may have introduced variability into our data; however, such variability would be expected to null bias our findings. Our data are from a pilot study using a convenience sample from a large, prospective longitudinal study. These measures need to be evaluated in a larger sample with standardized time gain compensation and gain settings in order to better understand their relationships with CVD risk factors and markers of subclinical atherosclerosis. A longitudinal analysis may better describe associations with risk for CVD events. Serial evaluations may better describe the time course of arterial wall changes.

CONCLUSIONS
GLDS contrast is a novel greyscale ultrasound texture feature of the carotid arterial wall that has different CVD risk factor

associations than GSM. Lower contrast is associated with increasing age, lower HDL-C, higher CRP and higher carotid IMT, supporting its potential use for evaluating arterial injury and CVD risk.

CONFLICTS OF INTEREST

FUNDING

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