



NT3-chitosan enables de novo regeneration and functional recovery in monkeys after spinal cord injury

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Spinal cord injury (SCI) often leads to permanent loss of motor, sensory, and autonomic functions. We have previously shown that neurotrophin3 (NT3)-loaded chitosan biodegradable material allowed for prolonged slow release of NT3 for 14 weeks under physiological conditions. Here we report that NT3-loaded chitosan, when inserted into a 1-cm gap of hemisectioned and excised adult rhesus monkey thoracic spinal cord, elicited robust axonal regeneration. Labeling of cortical motor neurons indicated motor axons in the corticospinal tract not only entered the injury site within the biomaterial but also grew across the 1-cm-long lesion area and into the distal spinal cord. Through a combination of magnetic resonance diffusion tensor imaging, functional MRI, electrophysiology, and kinematics-based quantitative walking behavioral analyses, we demonstrated that NT3-chitosan enabled robust neural regeneration accompanied by motor and sensory functional recovery. Given that monkeys and humans share similar genetics and physiology, our method is likely translatable to human SCI repair.

nonhuman primate | spinal cord injury repair | chitosan | NT3 | CST regeneration

Neurons in the central nervous system (CNS) do not regenerate, not only because their innate regeneration potential is attenuated compared with neurons in the peripheral nervous system but also due to the hostile CNS injury environment composed of inhibitory myelin debris (1–3), extracellular matrix molecules including chondroitin sulfate proteoglycans (CSPGs) (4, 5), as well as inflammatory cytokines (6, 7), which further dampen the regeneration process. As a result, spinal cord injury (SCI) often leads to permanent motor, sensory, and autonomic functional loss. Previous attempts were made through local applications of neurotrophic factors (8–11), transplantation of exogenous neural stem cells (12, 13), Schwann cells (14, 15), peripheral nerve grafts (16, 17), chondroitinase ABC (18, 19), knocking out the CSPG receptor (20), and usage of biomaterials (10, 21–24) to provide an optimal microenvironment for neural repair in rodent SCI models. Measurable improvement in axonal regeneration and functional recoveries had been observed. However, studies using rodent models may not be translatable to humans because of quite dramatic differences in the genome (similarity between the rodent and human genomes is only around 80%), immune system development and function, and certainly the structure and function of the CNS (25, 26). Therefore, in the drug development field, it has been well-acknowledged that an overwhelmingly large number of drugs

that cured mouse diseases ended up failing in clinical trials (25). SCI research using nonhuman primate (NHP) models, on the other hand, has been rather limited (27–31). Some of the interventions tested in monkeys were relevant to clinical settings, such as application of localized cooling (hypothermia) to reduce edema and inflammation to curb secondary lesions (32). In recent years, the use of trophic factors (33), antibodies (34–36), and transplantation of neural stem cells (37, 38) to promote regeneration has attracted a lot of attention in NHP SCI research; however, whether these methods could in the future be applicable to human SCI repair is yet to be investigated. In addition, although peripheral nerve (39, 40) or other biocompatible scaffolds (40) had been examined and proposed for clinical applications, positive clinical trial results remain to be seen.

Significance

Spinal cord injury (SCI) is a severe medical condition often leading to permanent loss of sensory, motor, and autonomic functions, currently with no cure. This study provides evidence that in monkeys with severe SCI, a bioactive and biodegradable material, NT3-chitosan, elicited robust de novo neural regeneration including, for example, long-distance axonal growth of cortical motor neurons in the cortical spinal tract, as well as sensory and motor functional recovery. In this study, we utilized a battery of minimally invasive outcome measures including fMRI, magnetic resonance diffusion tensor imaging, and kinematics walking analyses, which are all clinical trial-compatible. Essentially, success in this approach in nonhuman primate SCI models provides a solid foundation for its potential therapeutic application.

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We used chitosan to serve as a matrix scaffold to load neurotrophin3 (NT3) so that this critical neurotrophic factor could be gradually and continuously released into the milieu after implantation, in a relatively long term manner. Our NT3-chitosan allowed for controlled release of NT3 at 37 °C when cocultured with neural stem cells (NSCs) for at least 14 wk (10). In rodent SCI models, the NT3-chitosan scaffold effectively prevented infiltration of inflammatory cells and attracted endogenous NSCs to proliferate, migrate, and differentiate into neurons, forming nascent relay neuronal networks to transmit ascending and descending neural signals to proper targets (41, 42). In addition, NT3-chitosan also promoted robust axonal regeneration (22, 41, 42). In this study, which is one step closer to human clinical trials, we developed a rhesus monkey spinal cord hemisection and extraction SCI model leaving a 1-cm gap, which was either left alone (lesion control) or inserted with NT3-chitosan material (NT3-chitosan). Since, from rodent studies, we found that either the chitosan scaffold alone or chitosan scaffold plus chitosan matrix without NT3 only elicited an antiinflammatory effect in preventing immune cell infiltration into the control chitosan material without attracting NSC infiltration and did not enable neural regeneration, we omitted such control groups in this monkey study for ethical concerns regarding excessive use of NHPs. Using biotinylated dextran amine (BDA) injection to label cortical motor neurons, we tracked the corticospinal tract (CST) and discovered that regenerated axons entered the lesion area into the bioscaffold, grew across the 1-cm-long lesion area, and extended into the distal spinal cord. In addition, a combination of minimally invasive functional magnetic resonance imaging (fMRI), diffusion tensor imaging (DTI), electrophysiology, and kinematics walking behavioral analyses indicated neural regeneration as well as substantial motor and sensory functional recovery in the NT3-chitosan group. Quantitative outcome measures clearly demonstrated significant differences between the lesion control and NT3-chitosan groups. The bioactive material is antiinflammatory and growth-promoting with no risk of tumor formation (compared with exogenous NSC-based therapies). Success in this approach in NHP-SCI models provides a solid foundation for its potential therapeutic application.

Results

Morphological Analyses Demonstrating NT3-Chitosan Elicited Robust Axonal Regeneration. In our previous studies using rodents, complete spinal cord transection and segment removal were used (42). However, due to animal care concerns, complete spinal cord transection in monkeys was avoided due to high instances of mortality (40, 26). Thirty-two animals were subjected to spinal cord hemisection at thoracic level T8 (the eighth vertebral bone) followed by removal of a 1-cm segment of the right half of the spinal cord (Fig. 1A). A 1-cm-long NT3-chitosan matrix in a tubular scaffold was inserted individually into the lesion gap of 20 animals, and the remaining 12 animals were used as lesion controls. Suturing of the dura was performed to protect the lesion site. Another six animals without SCI were used as non-injury controls. All information on each of the animals used in the study regarding the occurrence of bedsores, time of death post surgery, cause of death, and types of analyses performed is listed in *SI Appendix, Tables S1–S3*. We are fully aware that such an extreme injury condition almost never happens in human SCI in the clinic; however, to demonstrate the superb de novo neural regeneration, namely generation of connecting neural tissue from an empty space, we chose this extreme model. We will discuss the clinical implications of our study later in the article.

Interestingly, bedsores, a clinically relevant outcome following SCI, also frequently happen in monkeys after SCI (43). NT3-chitosan significantly reduced the incidence of bedsores, with a 58.3% occurrence rate in the lesion control group and reduced to 10.5% in the NT3-chitosan group, which could be indicative of

better SCI recovery. At gross anatomical levels, over 1 y after the surgery, a neural cable-like “bridging” structure connecting the rostral and caudal ends of the severed right side of the spinal cord appeared in the NT3-chitosan matrix, whereas only scar tissues were found in the lesion control group (Fig. 1A and B). In *SI Appendix, Fig. S1*, gross anatomy of regenerated monkey spinal cord from five additional animals is shown, and lesion size of each of the 32 SCI animals going through the injury operation is listed, indicative of consistent lesion operations and similar sizes of lesion areas. In fact, the surgical team performed the hemisection before knowing the subsequent lesion control (LC) or NT3-chitosan (NT3) group assignment, which added more objectivity to the design of the study. This de novo regenerated tissue shared stark similarity in gross anatomical appearance with NT3-chitosan-elicited de novo regeneration of rat neural tissues after complete SCI (Fig. 1B, *Right*) (42). Moreover, immunohistological and electron microscopic analyses demonstrated that the cable-like regenerated neural tissues contained many myelinated and neurofilament (NF)-positive nerve fibers (Fig. 1C and D and *SI Appendix, Table S4*). Moreover, many cell bodies aligned well along the anterior–posterior axis, which could be NF-positive neuronal cells (Fig. 1C). H&E staining and NF staining on regenerated tissues at 11, 15, and 24 mo post operation (*SI Appendix, Figs. S2 and S3*) demonstrated that when axons or cell bodies encountered chitosan particles, they detour around and extend or migrate only in spaces between particles, making axon tracks difficult to see (*SI Appendix, Figs. S2 and S3*). However, after chitosan particles disappeared (degraded), relatively more longitudinally oriented fibers could be observed. The two-end funnel-like structures made tracking of axons difficult, especially at the two funnel ends. As the axons likely curve in and out of the section plane, it would appear that they suddenly were disrupted (*SI Appendix, Figs. S2 and S3*). In the LC group, although some levels of neural tissue invasion from the uninjured part of the spinal cord were apparent, major portions of the lesion area were filled with scarring cells that were NF-negative, and no myelinated axons were detected (Fig. 1C and D). In some cases, watery cysts may form in the LC group, which after perfusion left a big empty space on the lesion side (Fig. 2C). In this monkey study, we found that GFAP-positive reactive astrocytes (*SI Appendix, Fig. S4*) and CD45-positive leukocytes and microglia (*SI Appendix, Fig. S5*) were substantially reduced with NT3-chitosan treatment, indicative of reduced inflammation and glial scar formation. As expected from our previous rat studies, revascularization occurred in regenerated neural tissues (*SI Appendix, Fig. S5*).

Robust Axonal Regeneration Elicited by NT3-Chitosan as Demonstrated by CST Tracking. To evaluate whether NT3-chitosan enabled long-distance axonal regeneration, we performed CST tracking using BDA. BDA was injected unilaterally into the motor cortex via a stereotactic method to achieve labeling of the CST over the years after the initial injury/transplantation operation. As shown in *SI Appendix, Fig. S6*, while no BDA signals could be detected about 15 mm distal to the caudal lesion edge in LC monkeys, plenty of BDA signals were detected in the expected column in the NT3 group (*SI Appendix, Fig. S6A, Right*). In addition, longitudinal sectioning of additional animals clearly demonstrated that regenerated CSTs grew through the GFAP-positive reactive astrocytic zone/barrier at the interface of the severed spinal cord and NT3-chitosan scaffold, entering the lesion/repared area and then exiting the scaffold, and grew into the distal spinal cord (Fig. 2). These results demonstrate clear long-distance axonal regeneration.

Electrophysiological Results Indicating Partial Restoration After NT3-Chitosan Treatment. To examine whether NT3-chitosan also triggered sensory, particularly proprioception, recovery, we used Keypoint-II electromyography (Medtronic) to measure the somatosensory evoked potential (SEP) from both left and right anterior tibial muscles (Fig. 3). Proper signals were detected in the corresponding somatosensory cortex when either the left or the right tibial muscles

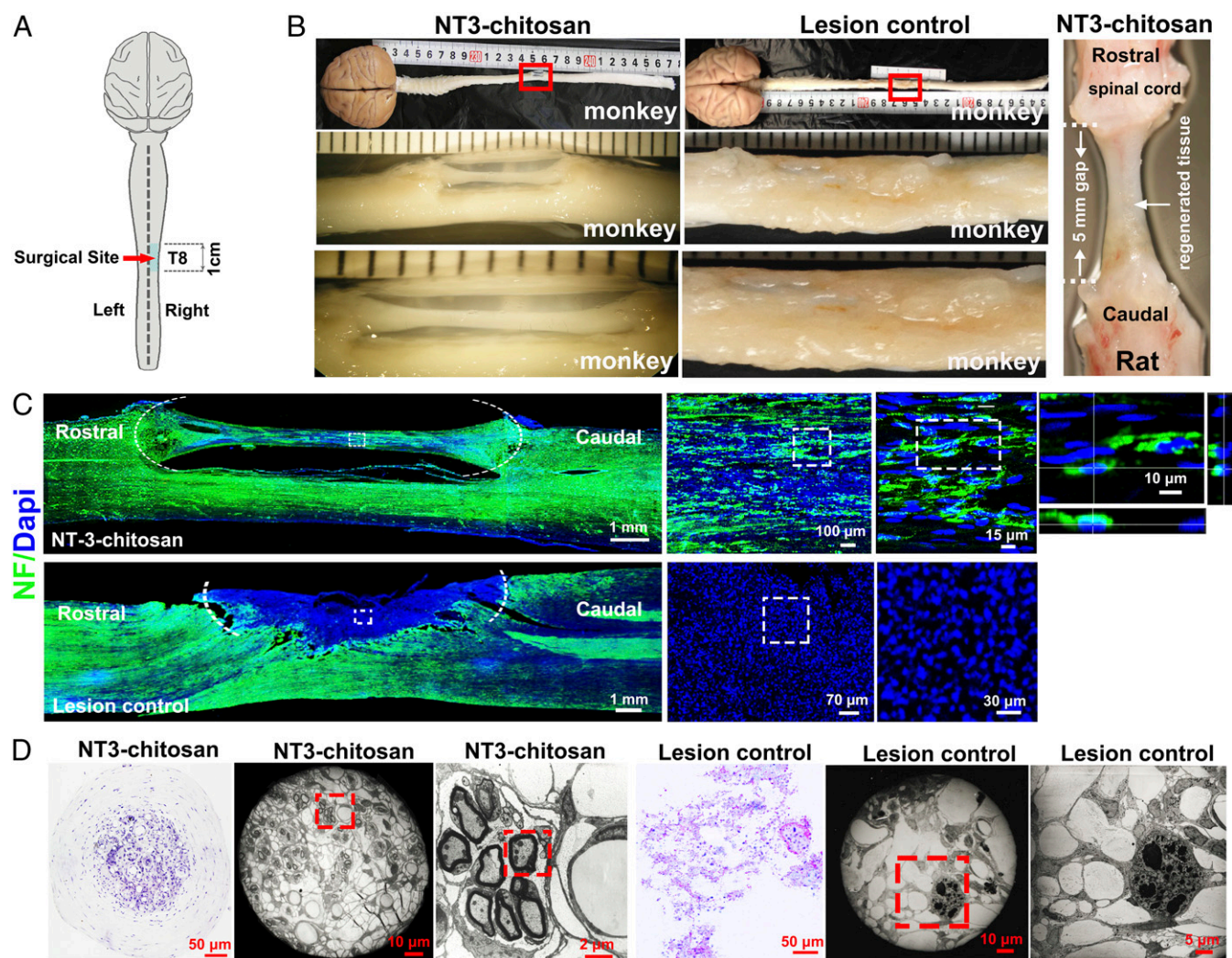


Fig. 1. Histological analyses demonstrating NT3-chitosan elicited de novo neural tissue reconstruction after a severe case of SCI. (A) A schema illustrating spinal cord hemisection and extraction leaving a 1-cm gap in monkey right spinal cord at thoracic level T8 (eighth vertebra), which was either left alone (lesion control) or inserted with NT3-chitosan matrix-containing tubular biomaterial (NT3-chitosan). (B) Gross anatomical analysis demonstrated regeneration of neural cable-like tissues in the NT3 group at the lesion/regeneration site, while only scar tissues filled the injury site in the LC group. (B, Right) NT3-chitosan-induced regeneration of neural cable-like structure in rat 9 mo after complete transection and extraction of rat thoracic spinal cord is shown. Results demonstrate the similarity between monkey and rat de novo regenerated neural tissues. (C) Immunofluorescent neurofilament staining (green) detected in regenerated neural tissues with NT3-chitosan treatment, while the LC group showed a lack of NF immunoreactivity in a major part of the lesion area. Quantitative measures of the bridge tissue diameter and the NF staining fiber density for the NT3 group are shown in *SI Appendix, Table S4*. (D) Over 24 mo after the operation, 1-mm-long spinal cord tissue was selected around the middle point of the regenerated tissue in the tube, and then semithin slices were made by staining with toluidine blue. The light micrographs show a large amount of regenerated blood vessels and myelinated and unmyelinated axons surrounded by epineurium- or perineurium-like structures in the regenerated cable tissue.

were stimulated in uninjured animals. In the LC group, no signals could be detected in the left or right somatosensory cortex when the right hind limb was stimulated. Interestingly, when the left hind limb was stimulated, SEP signals detected in the right cortex were reduced in the LC group compared with uninjured controls (Fig. 3). This was probably due to influence from injury to the right spinal cord, including inflammation, edema, demyelination, and so forth. As expected, in the NT3 group, clear SEP signals were detected in the left somatosensory cortex with stimulation of the right tibial muscle (Fig. 3). SEP signals in the right cortex when stimulating the left muscle were also greater than those in the LC group, indicative of better neural protection. To confirm that such SEP signals were not mediated by any kind of compensation from the intact left spinal cord, right after the initial SEP measurement we performed transection to the left spinal cord also at vertebral T8 followed by a 1-cm segment removal. Three months later, we

found that retranssection completely eliminated left hind limb-evoked SEP signals in the right cortex but did not ablate SEP signals detected in the left somatosensory cortex, which were evoked by stimulation of the right hind limb (Fig. 3). In contrast, when we recut the regenerated neural tissue on the right spinal cord, regained SEP signals in the left cortex completely disappeared after stimulation of the right hind limb. This observation suggested that the cortical–spinal connection through the injured right spinal cord was reestablished in the NT3-chitosan group.

In addition to SEP, we also measured motor evoked potential (MEP) (Fig. 4). Similar to sensory recovery, NT3-chitosan also triggered motor recovery as measured by MEP. It is worth mentioning that cortical motor axons have two branches. The main branch decussates the midline and continues down the spinal cord on the contralateral side. The minor branch does not decussate, and remains on the ipsilateral side. We examined responses from both the

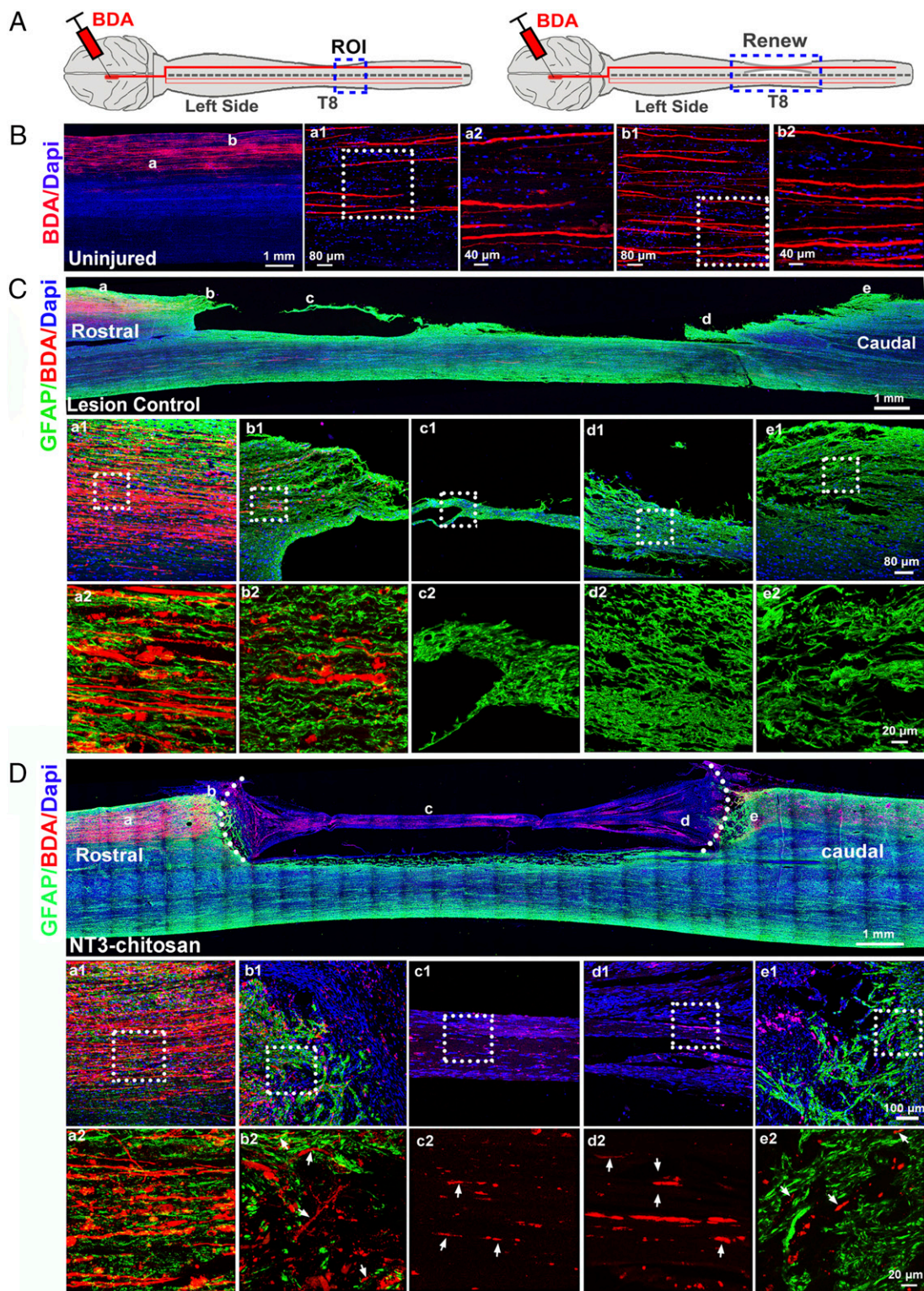


Fig. 2. CST tracking with unilateral BDA injections. (A) A diagram of BDA injections in uninjured and NT3-chitosan monkeys. (B–D) Longitudinal sections of monkey spinal cord 11 wk after BDA injections in normal (uninjured, animal 30) (B), lesion control (animal 5) (C), and NT3-chitosan (animal 18) (D) monkeys more than a year after the initial operation. DAPI (blue), BDA (red), and GFAP (green) fluorescent images are shown. ROI, region of interest; small white arrows marked regenerated BDA-positive fibers.

contralateral and ipsilateral sides when stimulating either left or right motor cortices. NT3-chitosan-triggered partial restoration of MEP signals was again not mediated by any sprouting or compensation from the intact left spinal cord but from de novo regenerated neural

tissue in the right spinal cord, because 3 mo after second surgeries, the main (contralateral) MEP signals detected from the right hind limb persisted after transection of the left (intact) spinal cord and were abolished after retransection of the regenerated neural tissue

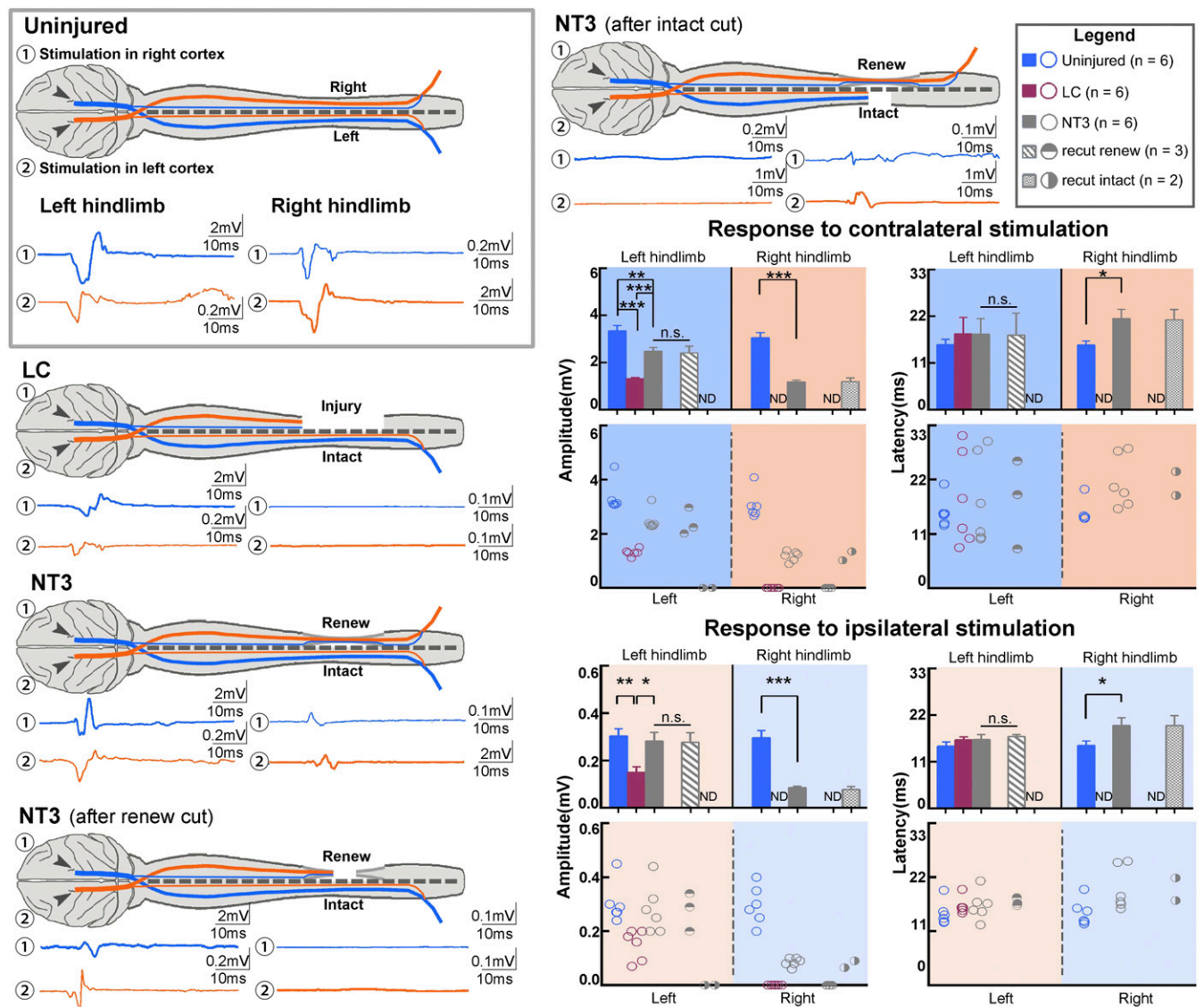


Fig. 4. MEPs demonstrating partial restorations with NT3-chitosan treatment. Stimulation of the right motor cortex evoked MEPs in left anterior tibial muscles (blue), and stimulation of the left motor cortex evoked MEPs in the right hind limb muscles (orange). The relationship between the LC and NT3 groups on MEPs is similar to that on SEPs shown in Fig. 3. Both contralateral (major; thick waveform lines) and ipsilateral (minor; thin waveform lines) responses were analyzed. Quantification and statistical analyses of amplitude and latency period for the aforementioned experiments are shown. Resection results of each animal are also displayed. Technical measurements were repeated twice. Shown are mean \pm SEM. * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$ by ANOVA or two-tailed independent sample t test. See *SI Appendix, Tables S10 and S11* for exact n and P values.

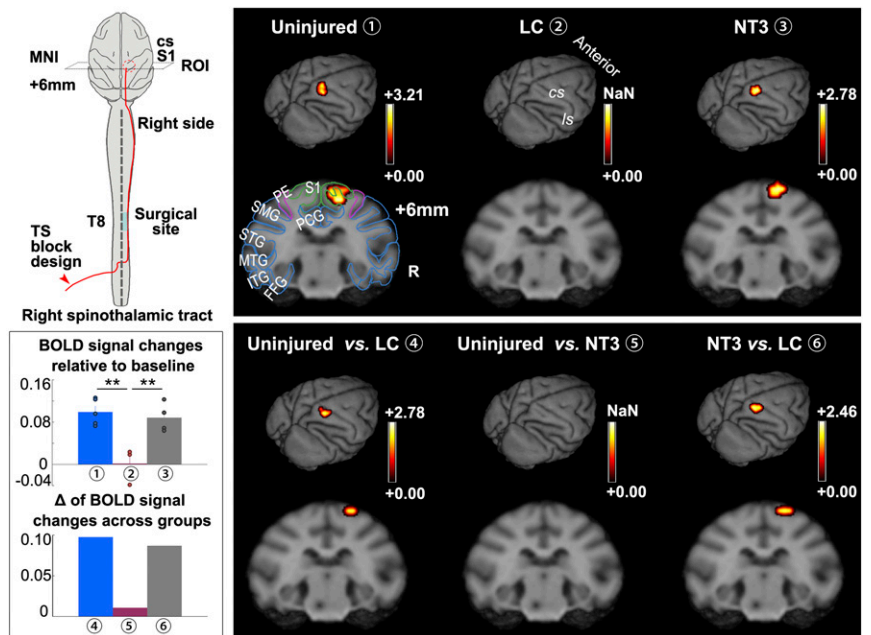
demonstrate that the left spinal cords of all three groups of animals were intact and functional (*SI Appendix, Fig. S7*).

Kinematics-Based Analyses Indicating Recovery of Walking Behavior After NT3-Chitosan Treatment. To evaluate potential improvement of animal walking behavior by NT3-chitosan treatment, we used kinematics-based analyses. Monkeys are naturally quadrupedal and, to measure hind limb motor function, we developed bipedal kinematics analyses for monkeys. Monkeys were trained to walk on two legs on a treadmill (Fig. 6A). The bipedal gait cycle is composed of a swing phase and a stance phase, which alternate. The bipedal movement of monkeys could initially be elicited by the treadmill; through adaptation, animals could accomplish rhythmic stepping with alternating left and right feet. Kinematics analysis is very sensitive in describing even small abnormalities in animal walking behavior (Fig. 6B). We detected the end point trajectory, and found that in the LC group, animals dragged their right legs most of the

time (*SI Appendix, Fig. S8*), presenting abnormal stick plots (Fig. 6C and *Movie S1*). In the NT3 group, the animal's right leg demonstrated a successive gait cycle (stepping almost without dragging) (Fig. 6D and *SI Appendix, Fig. S8*). We analyzed 127 parameters from kinematics analyses using pairwise correlation and clustering (*SI Appendix, Fig. S9 and Table S5*). Moreover, we selected the 12 clinically most relevant parameters and showed good walking recovery with NT3-chitosan treatment (Fig. 6E). Fig. 6F demonstrates one complete gait cycle. It was obvious that LC animals' right hind limbs (green) dragged and could not complete a stepping cycle, whereas NT3-chitosan animals demonstrated stepping (Fig. 6F). These results strongly indicated that good motor functional recovery was achieved in the NT3 group.

Diffusion Tensor Imaging Analyses Indicating Neural Tissue Regeneration Progress Noninvasively. Magnetic resonance imaging, particularly diffusion tensor imaging (DTI), can be used noninvasively to

Fig. 5. fMRI analyses indicating recovery of sensory function with NT3-chitosan treatment. Diagram illustrating fMRI experimental design with heat/temperature stimuli applied to the left hind limb. The lateral spinothalamic tract is transmitting the corresponding sensory signal to the somatosensory cortex as illustrated. Averaged fMRI signals within each group were superimposed onto a 3D monkey brain and coronal structural images, respectively ($P < 0.05$, GRF-corrected). Uninjured and NT3 groups displayed significant activation in the S1 area representing the left hind limb receptor field upon thermal stimulation, but LC animals showed no signal. Quantitative BOLD signal changes of the three groups are shown in a bar graph ($n = 3$ to 5 animals). Intergroup comparisons demonstrate obvious differential activation between the uninjured and LC groups and between the NT3 and LC groups, with no difference between uninjured and NT3 groups (quantitative data are also demonstrated in a bar graph). The schema of brain structures is superimposed onto coronal images. Color scales indicate t values. MNI coordinates are shown. Technical measurements were repeated twice. Error bars represent the mean \pm SEM. $**P < 0.01$ by ANOVA. See [SI Appendix, Tables S10 and S11](#) for exact n and P values. cs, central sulcus; FFG, fusiform gyrus; ITG, inferior temporal gyrus; Is, lateral sulcus; MNI, Montreal Neurological Coordinates; MTG, middle temporal gyrus; PCG, posterior cingulate cortex; PE, sensory association cortex; R, right; S1, primary somatosensory cortex; SMG, supramarginal gyrus; STG, superior temporal gyrus; T, thoracic vertebra; TS, temperature stimulation; NaN, not a number.



longitudinally track spinal cord neural regeneration progress, which could be an ideal outcome measure for human SCI clinical studies. We used DTI to track spinal cord damage and regeneration in the LC and NT3 groups (Fig. 7A). Different colors were used to track the direction of fiber orientations ([SI Appendix, Fig. S10](#)). In uninjured spinal cords, blue fiber signals filled the whole spinal cord structure in an orderly manner (Fig. 7B). After hemitransection and removal of the right thoracic spinal cord segment, the ascending and descending blue fiber tracks were disconnected, leaving a gap on the right side of the spinal cord. The gap persisted 1 y post surgery in lesion controls (Fig. 7C). NT3-chitosan treatment led to regeneration based on DTI images 1 y post surgery (Fig. 7D). Fractional anisotropy (FA) values and percentage of rostral-caudal voxels of the 2-mm segment at the center of the surgical site demonstrated significant tissue regeneration with NT3-chitosan treatment, while the LC group showed no signs of regeneration (Fig. 7E). Longitudinal studies demonstrated that at 2 mo post surgery, in the NT3 group, regenerating blue-colored fiber tracks started to extend into the injury/regeneration regions whereas, for the LC group, no obvious regenerating fiber images were detected (Fig. 7F). By 6 mo, ascending and descending fiber tracks merged, and the gap was filled with NT3-chitosan treatment, while the gap (fiber interruption) still persisted in lesion controls. Quantitative analyses of FA values and percentage of rostral-caudal voxels demonstrated significant improvement elicited by NT3-chitosan compared with lesion controls by 6 mo post operation (Fig. 7G).

Discussion

We have previously shown that in a rat complete spinal cord transection and extraction model, NT3-chitosan triggered robust de novo neural tissue regeneration and functional recovery (42). Bridging neural structures grown in NT3-chitosan matrix in rats are very similar to those grown in monkeys. In rodents, enhanced neurogenesis from endogenous stem cells and formation of nascent relay neural networks participate in sensory and motor functional recovery, in addition to robust axonal regeneration (42). In monkeys, we also observed what appeared to be neuronal cell bodies in addition to axon bundles in the regenerated tissue. CST labeling

experiments demonstrated robust long-distance axonal regeneration, where CSTs grow into the lesion area and also exit the distal boundary and extend into the distal spinal cord. How these newly generated axons manage to reconnect to the correct alpha motor neurons and conduct voluntary movement remain to be determined. Since, in monkeys, we used a spinal cord hemisection, rather than complete transection as in rats, potential contributions/compensations from the left intact cord for the sensory and motor functional recovery become a formal possibility. Resections of intact left cord or regenerated neural cable demonstrated via MEP and SEP that sensory and motor functional recoveries appeared to be dependent on de novo regenerated neural tissues.

To assess whether differences in size of the lesions long-term after the initial surgical procedure may influence motor functional outcomes, we attempted to have a rough assessment of the size of the lesions more than 1 y post operation. We picked middle spinal cord longitudinal sections (serial sections 27, 28, and 29 from 10- μ m longitudinal section series) and demarcated the lesion area and spared area, the summation of which gives the total corresponding spinal cord area. We measured each area and calculated the relative lesion area (i.e., lesion area over total corresponding area) ([SI Appendix, Fig. S11 and Table S6](#)). Subsequently, we performed correlation analyses between the resultant lesion size and 12 clinically relevant kinematics walking parameters ([SI Appendix, Tables S7–S9](#)) in the LC and NT3 groups separately and in combination. Our conclusion is that there is no positive correlation, suggesting that the smaller the initial or final lesion size the better the walking behavior. It is obvious that the NT3 group has a relatively regular lesion area, while in the LC group the final lesion area is more variable in shape and size. This is likely due to the antiinflammatory function of NT3-chitosan, which inhibited secondary lesions.

In this monkey SCI model, the mode of regeneration is very similar to that of rats (42, 44). We have previously shown in rats that NT3-chitosan is neural-protective, neurogenic, provascularizing, and highly antiinflammatory. The antiinflammatory effect of NT3-chitosan also contributed to better regeneration in rodent models (44). In this study, damage to the right spinal cord appeared to influence the function of the left spinal cord, as revealed by reduced SEP and MEP signals. Such influence on the left spinal cord was

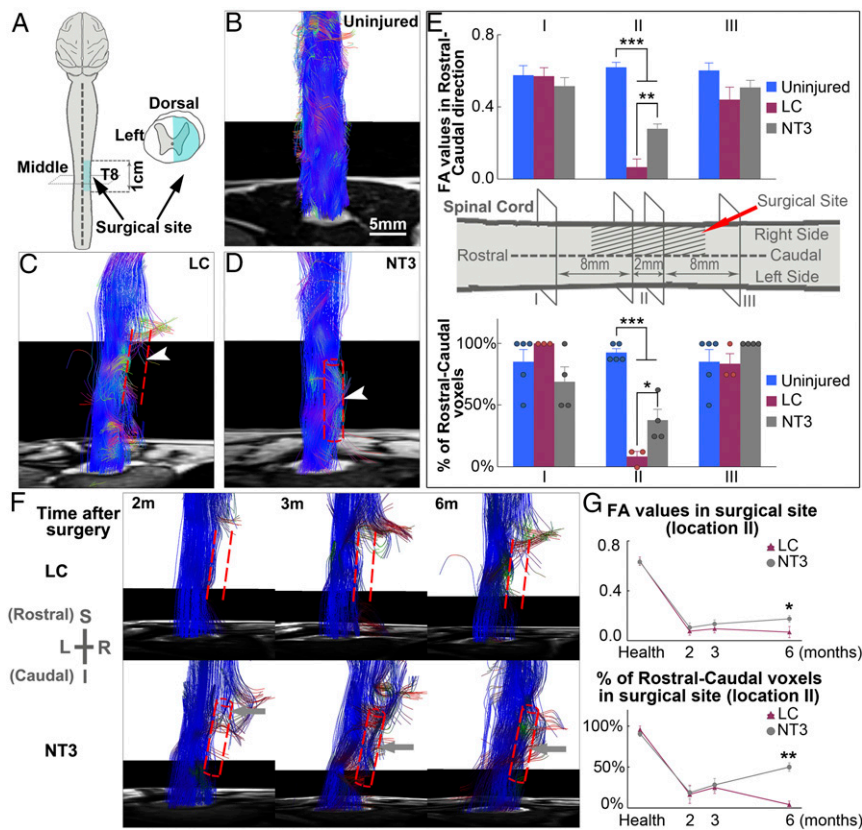


Fig. 7. MRI results indicating NT3-chitosan enabled neural tissue regeneration after SCI. (A) Diagram illustrating the spinal cord hemisection and extraction model. (B–D) Typical fiber tract reconstruction for the uninjured (B), LC (C), and NT3 (D) groups is displayed. In the LC group, fiber tracts were interrupted, deformed, and distorted at the border rostral and caudal to the lesion, with no fiber tracts present within the lesion (C). In contrast, in the NT3 group, numerous regenerated fiber tracts extend across the surgical site, reconnecting the rostral and caudal ends of the injured cord (D). Arrowheads indicate the surgical sites. Red dashed lines indicate the damaged zone, and tubular structures in the NT3 group represent positions of chitosan tubes. (E) Graph of averaged FA values and percentages of rostral–caudal voxel numbers of the three groups in three locations (I to III). Results of two levels in the middle site were gathered as location II. The NT3 group showed significantly higher FA values and percentages of voxels compared with the LC group ($n = 3$ to 5 animals). (F) Diffusion tensor fiber tracking tractography showed longitudinal changes of lesion (Top) and treated (Bottom) spinal cord with time after operation. LC animals showed a lack of neural fibers in the damaged zone, while NT3 animals displayed regenerated fiber bundle growth progressively with time and eventually connecting the two ends of the severed cord at 6 mo. I, inferior; L, left; R, right; S, superior. (G) Time courses of changes in FA values and percentages of rostral–caudal voxels at the center of the surgical site (location II) from LC and NT3 groups up to 6 mo post operation ($n = 3$ or 4 animals). Technical measurements were repeated twice. Shown are mean \pm SEM. * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$ by ANOVA or two-tailed independent sample t test or two-tailed Mann–Whitney U test. See *SI Appendix, Tables S10 and S11* for exact n and P values.

only elicit fresh lesion responses but also to create a physical space for transplanting the NT3-chitosan tube. With this, long-distance axonal regeneration could be induced within an optimal neurotrophic and antiinflammatory microenvironment. Of course, studies using NT3-chitosan to repair chronic lesion models using NHPs are currently ongoing. To achieve functional recovery, long-distance axonal regeneration must be coupled with new synapse formation and neural circuitry remodeling. Detailed circuitry mapping will be required in the near future to reveal the logic of neuronal wiring (connectivity) during regeneration. Moreover, as rehabilitation is likely among the most effective clinical means of eliciting neural plasticity and engaging circuitry wiring and pruning, it should be indispensable for good functional recovery after SCI.

Taken together, this study using NHPs represents an important milestone, paving the way to clinical studies using NT3-chitosan for SCI treatment.

Materials and Methods

NT3-Chitosan Tube Fabrication. The chitosan tube was fabricated by the method previously published (41, 42, 47). For detailed methods, see *SI Appendix, Materials and Methods*.

Animal Models. Thirty-eight female rhesus monkeys (*Macaca mulatta*, 4 to 6 y old), each weighing 5 ± 1 kg, were used for these experiments. All surgical and experimental procedures in monkeys were approved by and performed in accordance with the standards of the Experimental Animal Center of Capital Medical University and the Beijing Experimental Animal Association. Details are provided in *SI Appendix, Materials and Methods*.

Immunohistochemistry/Fluorescence Staining. Morphological analysis was performed as detailed in *SI Appendix, Materials and Methods*.

Light and Electron Microscopies. These observations were performed as detailed in *SI Appendix, Materials and Methods*.

BDA Tracing. This observation was performed as detailed in *SI Appendix, Materials and Methods*.

SEP and MEP Examination. Electrophysiological study was carried out for each group ($n = 6$ animals). For detailed information, see *SI Appendix, Materials and Methods*.

Anesthesia for MRI Examinations. Animals of each group ($n = 3$ to 5 animals) were anesthetized for MRI scanning. For detailed information, see *SI Appendix, Materials and Methods*.

fMRI Stimulation. Innocuous heat stimulation was used for the fMRI somatosensory test. For detailed information, see *SI Appendix, Materials and Methods*.

MRI Data Acquisition. All MRI research was accomplished with the Siemens 3T MRI instrument. Detailed scanning parameters are provided in *SI Appendix, Materials and Methods*.

fMRI Data Processing. All fMRI data were processed with Statistical Parametric Mapping (SPM) version 8 (www.fil.ion.ucl.ac.uk/spm/). For detailed processes, see *SI Appendix, Materials and Methods*.

DTI Data Processing. DTI scans were processed and analyzed by means of dedicated MedINRIA software (www-sop.inria.fr/asclepios/software/MedINRIA). For detailed processes, see *SI Appendix, Materials and Methods*.

Kinematics Analyses of Bipedal Locomotion. The bipedal locomotion of the animals was characterized by gait test. More details are provided in *SI Appendix, Materials and Methods*.

Statistical Analyses. Standard statistical tests were used to analyze the data. Please see *SI Appendix, Materials and Methods* for further information.

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