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## Autologous Adipose-Derived Mesenchymal Stem Cells Improve Healing Of Coiled Experimental Saccular Aneurysms: An Angiographic And Histopathological Study.

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### Abstract

**Purpose:** Long-term occlusion of coiled aneurysms frequently fails, likely due to poor intrasaccular healing and inadequate endothelialization along the aneurysm neck. The purpose of this study was to determine if seeding coils with autologous stem cells could improve the healing response of experimental aneurysms.

**Material and Methods:** With institutional animal care and use committee approval, aneurysms were created in rabbits and embolized with control platinum coils (Axium, Medtronic) (n=6) or coils seeded *ex vivo* with autologous adipose-tissue mesenchymal stem cells (MSC) (n=7). Stability of aneurysmal occlusion after embolization was evaluated at one month with DSA. Histological samples were analyzed with gross imaging and graded based on neck and dome healing on hematoxylin-eosin staining. Fibrosis was evaluated using a ratio of the total area presenting collagen. Endothelialization of the neck was quantitatively analyzed using CD31 immunohistochemistry. Chi-squared and student's t-test were used to compare groups.

**Results:** Healing score (11.5 versus 8.0, p=.019), fibrosis ratio (10.3 versus 0.13, p= 0.006.), endothelialization (902,262  $\mu\text{m}^2$  versus 14,106  $\mu\text{m}^2$ , p= 0.04113) were significantly greater in the MSC group compared with controls. The MSC group showed marked cellular proliferation and

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#### AUTHOR CONTRIBUTIONS

Guarantors of integrity of entire study, R.K., D.D.; study concepts/study design or data acquisition or data analysis/ interpretation, all authors; manuscript drafting or manuscript revision for important intellectual content, all authors; manuscript final version approval, all authors; literature research, A.R., W.B., D.F.K.; experimental studies, A.R., Y.H.D., D.D., D.S., R.K., D.F.K.; statistical analysis, T.G.; and manuscript editing, A.R., W.B, R.K., D.D., D.F.K.

#### DISCLOSURES OF CONFLICTS OF INTEREST

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thrombus organization, with continuous membrane bridging the neck. Angiographic stable or progressive occlusion rate was significantly lower in the MSCs group (0.00, 95% CI: 0.00-0.41) compared to controls (0.67, 95% CI: 0.22-0.96) ( $p=.02$ ).

**Conclusions:** MSCs significantly improved histological healing of coiled aneurysms, but angiographic outcomes were not improved. This indicates the need for larger experiments to evaluate the safety and long-term outcomes of stem-cell therapy for intracranial aneurysms.

## INTRODUCTION

Endovascular therapy of intracranial aneurysms is the gold standard and has supplanted the surgical approach in many types of aneurysms(1). However, numerous clinical studies indicate that up to 30% of aneurysms recur within one year after coiling(2, 3), leading not only to frequent re-treatment and its associated perioperative risks but also to risk of hemorrhage if untreated(4–6). Thus, complete and durable aneurysm occlusion following coiling remains an important unmet clinical need. The recanalization phenomenon attributable to coil compaction is particularly observed in wide-necked or large aneurysms(7–13). The frequent recurrence is most likely due to the inert nature of the platinum(14, 15), which fails to induce homing and proliferation of either circulating or resident cells that might reconstruct the deficient segment of the vessel wall. Lack of cells, rare endothelialization at the entrance zone of the aneurysm and deficient deposition of extracellular matrix proteins within aneurysm cavities represent the main biological reasons for recurrence of aneurysms after endovascular therapy(9, 13, 16–18). Thus, the aneurysm cavity remains unable to withstand the ongoing mechanical stress from continued arterial pulsation, leading to aneurysm recurrence and possible rupture.

Many different strategies have been proposed to improve aneurysm occlusion rates, including modification of coils with addition of polymers, growth factors, beta emitters, and cells(14, 19–28). To date, clinical trials have been disappointing regarding the efficacy of these second-generation, modified coil technologies(2, 29–40). Other studies have used cell therapy with mature and differentiated cells to promote aneurysm healing(41–52). However, terminally differentiated, implanted cells do not differentiate into other cell types normally present with in the blood vessel wall. Ideally, the cells lining the implanted coils would differentiate into arterial endothelial cells and those residing deep to the endothelial lining would become medial smooth muscle cells(13, 53, 54). From a biological perspective, mesenchymal stem cells (MSCs) represent an ideal cell type to populate saccular aneurysms(26, 41, 53, 55–58).

To study the effect of autologous MSCs on aneurysm healing, We conducted a case-control study comparing the healing effects of MSCs on coils compared to bare platinum coils in treatment of elastase-induced aneurysm model in rabbits. The purpose of this study was to determine if seeding platinum coils with autologous MSCs could improve the healing response of experimental aneurysms.

## MATERIAL AND METHODS

The animal care and use committee at our institution approved the animal procedures.

### **Aneurysm creation**

Elastase-induced saccular aneurysms were induced in 13 rabbits as previously described(59). Briefly, under general anesthesia, the right common carotid artery (RCCA) was exposed and ligated distally. A 5 F vascular sheath was advanced retrogradely into the RCCA, and a 3 F Fogarty balloon inflated with iodinated contrast medium was advanced through the sheath to the level of the origin of the RCCA under fluoroscopic guidance. Porcine elastase was incubated within the lumen of the RCCA above the inflated balloon for 20 min, after which the catheter, balloon and sheath were removed. The RCCA was then ligated below the arteriotomy. No morbidity or mortality was observed with aneurysm creation.

### **Autologous MSCs isolation and culture**

Adipose tissue was harvested during the aneurysm creation procedure from the neck of the rabbit. Autologous MSCs were isolated from adipose tissue extracted from the fat of the rabbit neck. Briefly, adipose tissue was digested with collagenase, then passed through a 70µm cell strainer (BD Biosciences, San Diego, California, USA) and incubated in red blood cell lysis buffer (Sigma-Aldrich). Harvested cells were cultured in a medium consisting of Dulbecco's Modified Eagle Medium with 10% fetal bovine serum and 2 mM l-glutamine. Adherent MSCs were cultured until  $5 \times 10^6$  cells had been obtained from each rabbit with about four cell passages for each rabbit. MSC membranes were labeled with fluorescent Dil (Sigma/Aldrich Chemical Co).

### **Coil preparation**

Axium detachable coils (Medtronic, Irvine, California, USA) were placed in 15mL Falcon tubes. An MSC suspension ( $1 \times 10^6$  cells/mL) was poured into the Falcon tubes containing the coils. The tubes were agitated at 300 rpm for 1 hour in an orbital shaker, and then the coils were cultured in the same culture medium as previously described and stored in the cell incubator for 24 hours at 37°C. Cell-seeded coils were then thoroughly washed with phosphate-buffered saline to exclude non-adherent cells, and resheathed in the delivery sheath. Axium coils incubated with culture medium without MSCs served as controls. Figure 1 illustrates MSCs growing on the coil 24 hours after seeding viewed by scanning electronic microscopy (figure 1A) and by fluorescence microscopy after nuclear staining (Syto16; Thermo Fisher Scientific, Waltham, Massachusetts, USA) (figure 1B).

To confirm that the resheathing and delivery of the coil through the microcatheter had not stripped a large proportion of cells off the coils, we pushed a cell-seeded coil through an Excel (Target Therapeutics) delivery microcatheter ex vivo and then flushed the catheter with saline. We measured the number of non-adherent cells afterwards, which was less than 5% of the initial number of cells seeded on the coil. The non-adherent cells were cultured in the culture medium to confirm that the cells were alive after the resheathing and delivery steps.

### **Coiling of the experimental aneurysms**

Aneurysms were treated at least 3 weeks after aneurysm creation(60). Under general anesthesia, a 5 F catheter was advanced from the right common femoral artery into the

brachiocephalic artery. Using coaxial technique, an Excel (Target Therapeutics) microcatheter was advanced into the aneurysm. Aneurysms were embolized with Axium coils without MSCs (control group, n=6) or Axium coils carrying autologous MSCs (test group, n=7). Following the embolization, a final control DSA was performed. A blinded reader with 20 years of experience estimated aneurysm occlusion and packing density with the Angiocalc tool (<http://www.angiocalc.com>).

### Follow-up

Control DSA was performed 4 weeks after coiling via the left auricularis rostralis artery under general anesthesia. All angiograms at death were compared with immediate post-treatment angiograms and assessed for any increase or decrease in contrast filling of the aneurysms. Aneurysms were assigned to one of three result groups: stable occlusion (no modification between immediate post-treatment and 4-week angiograms), progressive occlusion (decrease in aneurysm opacification between immediate post-treatment and 4-week angiograms), or coil compaction (increase in aneurysm opacification between immediate post-treatment and 4-week angiograms). Angiography results are expressed as the proportion of aneurysms demonstrating stable or progressive occlusion comparing immediate post-coiling and follow-up results. For this evaluation, the reader was blinded to the treatment group.

### Tissue harvest and processing

After follow-up DSA, animals were killed by lethal injection of pentobarbital. Median sternotomy and pericardiectomy were performed. The animals were then perfusion-fixed with 10% buffered formalin for 10 min followed by flushing with heparinized saline for 5 min. The coiled aneurysm was then harvested and immersed in Tris-buffered saline (TBS). Under a dissection microscope (Leica MZ 125), the parent artery was cut longitudinally to expose the neck orifice for gross inspection to evaluate tissue growth at the neck; the sample was then photographed using the MicroPublisher 5.0 RTV camera attached to the dissection microscope. After photography, the sample was fixed in 10% formalin for 2 hours for further whole tissue mount staining.

### Whole-mount en face immunostaining

Details of the procedure are described in a previous study (61). Briefly, after the macrophotographs were taken, the aneurysms were fixed in 10% neutral buffered formalin and then washed with TBS; they were then incubated with 5% normal donkey serum in 0.3% Tween in TBS. The samples were then incubated with primary antibodies against CD31 (1:30; Dako, Carpinteria, California, USA) or smooth muscle actin (1:200; Dako) at 4°C. Specific binding was visualized using a secondary antibody Cy3 or fluorescein isothiocyanate-conjugated IgG (1:200; Jackson Immuno Research, West Grove, Pennsylvania, USA). Sytox green (1:1000; Life Technologies, Grand Island, New York, New York, USA) served as a nuclear counterstain to identify inflammatory cells.

## Histologic analysis

Tissues were embedded in paraffin and then sectioned at 1000 microns. Metallic coils were gently removed under a dissecting microscope. Paraffin sections were then re-embedded in paraffin blocks and sectioned at 4  $\mu\text{m}$  intervals. Mounted sections were stained with either Hematoxylin and Eosin (H&E) for conventional histopathological evaluation or Masson Trichrome stain for collagen deposition. Sections were viewed by 2 blinded and independent experienced reviewers paying particular attention to the thickness of the cellular layer across the neck of aneurysms and the cellularity within the aneurysm dome. An ordinal grading system was used to evaluate histological healing (62). Briefly, neck healing score was calculated based on tissue coverage, coil microcompaction at the neck was based on the shape of the coil mass across the neck, and the healing characteristics in the dome was categorized based on the density of cellular infiltration and area of organized tissue. These scores, neck average, microcompaction and healing, were added together to obtain a total score representative of the aneurysm's healing. The degree of inflammation was defined and scored as 0) no inflammatory cell infiltration; 1) mild, scant, scattered inflammatory cells infiltration; 2) moderate, patchy inflammatory cells infiltration; and 3) marked, attenuated, diffuse inflammatory cells infiltration(47).

**Neck endothelialization at the level of the aneurysm neck analysis**—For endothelialization analysis, we used whole-mount en face immunostaining with primary antibodies against CD31. We quantitatively analyzed the endothelialization of the neck area with measurement of the CD31 positive field viewed from neck orifice.

**Collagen deposition analysis**—We quantitatively analyzed collagen deposition or fibrosis identified with Masson Trichrome staining using an image analysis technique based on Photoshop software (Adobe Systems, San Jose, CA)(47). A fibrosis ratio, the total area of fibrosis within the aneurysmal cavity and neck divided by the total area of the aneurysmal cavity and neck, was calculated for each aneurysm.

## Immunohistochemistry (IHC)

Sections were immunostained for RAM-11(63)(1:50, macrophage-specific monoclonal antibody for rabbit, Dako, Carpinteria, California, USA). RAM-11 is a macrophage-specific monoclonal antibody(64) used to detect inflammation in the aneurysm dome.

## Statistical Analyses

Wilcoxon rank-sum tests were performed to compare geometries and packing density between groups. Differences between groups for histological finding were assessed with between-group Wilcoxon rank-sum test. Results are expressed as median and interquartiles (25<sup>th</sup> & 75<sup>th</sup>). For DSA outcomes, groups were compared using Fisher's exact test and reported with exact Klopfer-Pearson 95% confidence intervals. Statistical significance was set at  $p < .05$ .

## RESULTS

### Seeding of autologous MSCs on Axium coils

Diffuse, confluent cells growth on the coil's surface, and between coil loop was obtained after 24 hours seeding, which was confirmed by scanning electronic microscopy and fluorescence microscopy (Figure 1).

### Angiographic findings

There were no significant differences in aneurysm neck size ( $p = .69$ ), aneurysm width ( $p = .37$ ), and aneurysm height ( $p = .64$ ) between groups. Packing density was significantly different between groups, with median (IQR) of 22.5% (18.8-24.8) for the control group and 30.0% (25.0-34.0) for the MSCs group ( $p = .01$ ).

All the aneurysms in the MSCs group presented coils compaction at follow-up with neck recurrences, whereas there were 2 cases of coil compaction, 3 stable total occlusions and one progressive total occlusion in the control group. Stable or progressive occlusion rate was significantly lower in the MSCs group (0.00, 95%CI: 0.00-0.41) as compared to controls (0.67, 95%CI: 0.22-0.96) ( $p = .02$ ).

### Qualitative histology

Gross microscopy showed the coil loops at the neck orifice were bare without membranous tissue covering (Figure 2b) in the control group; endothelialization on the coil surface was not noticed with CD-31 immunostaining (Figure 2c). In the test group, the coil loops which crossed over the neck orifice were covered with transparent and translucent membranous tissue (Figure 3b); this membranous tissue was lined with a layer of CD31 positive cells (Figure 3c), indicating endothelialization on the coil surface.

Microscopy showed six of six aneurysms in control group demonstrated large neck remnant with poorly organized thrombus crossing over neck interface (Figure 2d); loose connective tissue associated with scattered macrophages and thin ECM filling in the aneurysm dome; collagen deposit was few to be detected (Figure 2d-f); whereas endothelium-lined, thin and thick neointima completely covered neck interface in the test group (Figure 3d). Denser connective tissue associated with diffuse macrophage infiltration, thick ECM and collagen deposit within the aneurysmal cavity was also observed in the test group (Figures 3d-f).

### Histologic scoring

The MSCs group did have a significantly higher inflammation score than the control group (3.0, 3.0-3.0 vs 2.0, 2.0-2.0,  $p < .01$ ) indicating a larger amount of multinuclear giant cells and macrophages. In total, there was a significantly greater total histologic healing score in MSCs (11.5, 11.0-12.0) versus control (8.0, 6.25-9.0) groups ( $p = .019$ ).

### Quantitative analysis of aneurysm fibrosis

The quantitative analysis of aneurysm fibrosis based on the evaluation of collagen within the aneurysm cavity, demonstrated that the MSCs group (10.3, IQR: 7.98-28.3) had a



significantly higher fibrosis ratio compared to the control group (0.13, IQR: 0.055-0.272),  $p=0.006$ .

### Quantitative analysis of coils endothelialization at the level of the aneurysm neck

We noted a significant higher amount of endothelialization of the aneurysm necks in the MSCs group (902,262  $\mu\text{m}^2$ , IQR: 608,991-179,9849) than in the control group (31,810  $\mu\text{m}^2$ , IQR: 14,106 - 397,315),  $p= 0.041$ .

## DISCUSSION

This study demonstrated that autologous MSCs attached to platinum coils improved endothelial cell growth across the neck of the aneurysm and increased fibrosis within the aneurysm sac. Thus, *ex vivo* loading of standard coils can achieve improved biological healing of aneurysm cavities.

Notably, however, angiographic outcomes were not improved over controls with MSCs. It remains possible that the induced fibrosis from the implanted cells actually caused retraction of coils, rather than stabilization, at the aneurysm neck. Prior to clinical translation, therefore, substantial additional preclinical evaluation of *ex vivo* autologous MSCs implantation is warranted.

Previous studies have used cell therapy with mature and differentiated cells to promote aneurysm healing(41–52). However, none of these studies demonstrated the improvements in healing responses in both aneurysm neck and aneurysm sac seen in our study. Some authors showed that fibroblasts could improve intra-saccular fibrosis without positive effect on the endothelium and neo-intima formation(47, 48, 50, 51). Furthermore, fibroblasts have an important procoagulant activity due to intense expression of tissue factor (53). As opposed to fibroblasts, mesenchymal stem cells (MSCs), either from adipose tissue of bone-marrow, poorly express TF and are devoid of procoagulant activity, limiting thrombus formation(53). Others have used smooth muscle cells delivered into the aneurysm. Raymond et al.(45), as well as Marbacher et al.(42), observed thicker neointima but without significant impact on fibrosis and endothelium reconstruction through implantation of smooth muscle cells. Use of endothelial progenitor cells in preclinical aneurysm models led to development of confluent monolayers of endothelial cells with underlying neointima but without effect on intra-saccular healing(42, 49).

Those previous studies confirm that terminally differentiated implanted cells do not differentiate into other cell types normally present within the blood vessel wall. Ideally, the cells lining the implanted coils would differentiate into arterial endothelial cells and those residing deep to the endothelial lining would become medial smooth muscle cells(13, 53, 54). From a biological perspective, MSCs represent an ideal cell type to populate saccular aneurysms because of their potential to differentiate into various cell types based on their specific environment(26, 41, 53, 55–57). While our current methodology did not allow specific histopathologic identification of implanted versus recruited cells, previous studies have demonstrated that transplanted MSCs can differentiate into specific phenotypes of damaged cells *in vivo* under the influence of local host factors(65–67). Under conditions of

laminar flow, shear stress induces MSCs to differentiate into endothelial cells, so the implanted MSCs lining the neck of the aneurysm preferentially differentiate into cells lining the arterial wall(68, 69). This was also observed in the present study using autologous stem cells with continuous endothelium at the aneurysms necks and thick neo-intima. Furthermore, the embolized aneurysm cavity is rich in platelets stimulating MSCs to differentiate toward smooth muscle cell phenotypes(70); this was observed in our study with smooth muscle cells largely present in the aneurysms sacs with production of collagen responsible for fibrosis and wound healing.

Recently published studies demonstrate the benefits of MSCs in promoting intracranial aneurysm healing(53, 58, 71). Rouchaud et al. used autologous MSCs from bone marrow directly injected into the aneurysm by endovascular route through a catheter with no scaffold. They observed good results regarding the reduction of the aneurysms size and histological healing but there was a low yield of cells effectively attached into the aneurysm sac because of the absence of scaffold to hold them inside the aneurysm(53). This diminished the beneficial effect of the MSCs therapy and also increased the risk of cells trafficking and subsequent ischemic stroke. Recently, Adibi et al. published a series of 3 rabbits treated with combined endovascular coiling and intra-aneurysmal allogeneic MSCs from bone marrow injected into the aneurysm just after the framing coil and observed a significant improvement in histological scores(58). The authors used allogeneic MSCs with no deleterious impact in rabbits but this technique is likely to induce an immune response against transplanted cells in other animals or in humans(72). Another limitation of this study is the fact that the authors relied on framing coil to promote intra-aneurysmal stasis, thus containing the implanted cells in the aneurysm sac and avoiding cell migration and to evaluate the risk of ischemic lesions.

### Limitations

Our study is limited by its small sample size. Another limitation is that the rabbits were killed at only one time point, making it impossible to evaluate if the effects were permanent; also it is possible that the beneficial effects on histological healing observed with MSCs could appear earlier than 1 month. Furthermore, only a dose of  $5 \times 10^6$  cells was evaluated, which might not be the appropriate dose. Also, MSCs were not labeled for in vivo tracking, therefore we cannot determine if the implanted cells were viable at the time of death or whether the cells were responsible for the tissue changes noted. Furthermore, the packing density was significantly different between the groups, being higher in the MSC group, which may have biased some of the histological results.

To the best of our knowledge, this study is the largest to use autologous stem cells for the treatment of intracranial aneurysms in an experimental study. Furthermore, despite the small sample size, the effect was statistically significant in favor of MSCs for histological healing, encouraging larger experiments to evaluate safety and long-term outcomes. Further studies are required to evaluate outcomes at different time points to determine the effect of MSCs over time and evaluate the stability or progression of neck remnants. Also, an autologous approach with MSCs does not seem to be appropriate for acute treatment of ruptured aneurysms, since time is needed to produce sufficient cells for each patient.



We used a cell dose of  $5 \times 10^6$  cells used in the previous studies by Adibi et al.(58) and Rouchaud et al.(53), but further studies with different amount of cells would be needed to determine the appropriate dose-response efficiency.

## CONCLUSION

Autologous MSCs attached to platinum coils significantly improve histological healing compared with standard coils, with more endothelial cells across the neck of the aneurysm and collagen matrix within the aneurysm sac. However, these findings did not correlate with the angiographic findings.

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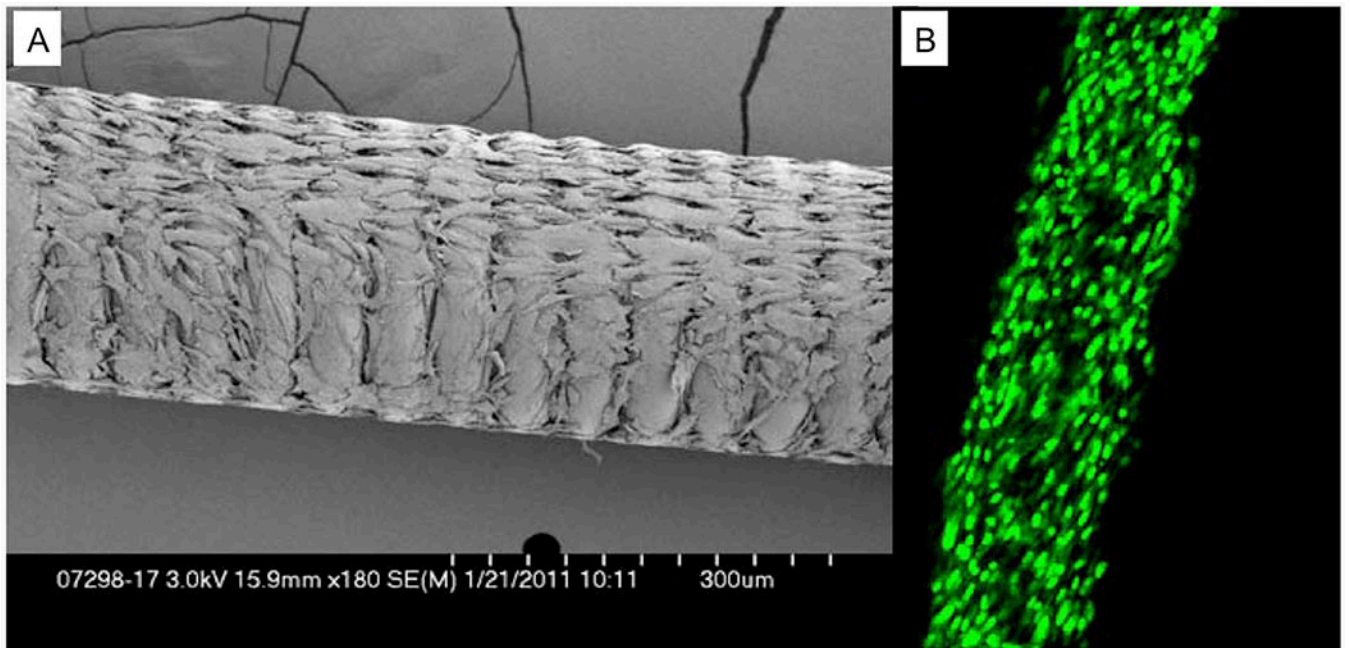
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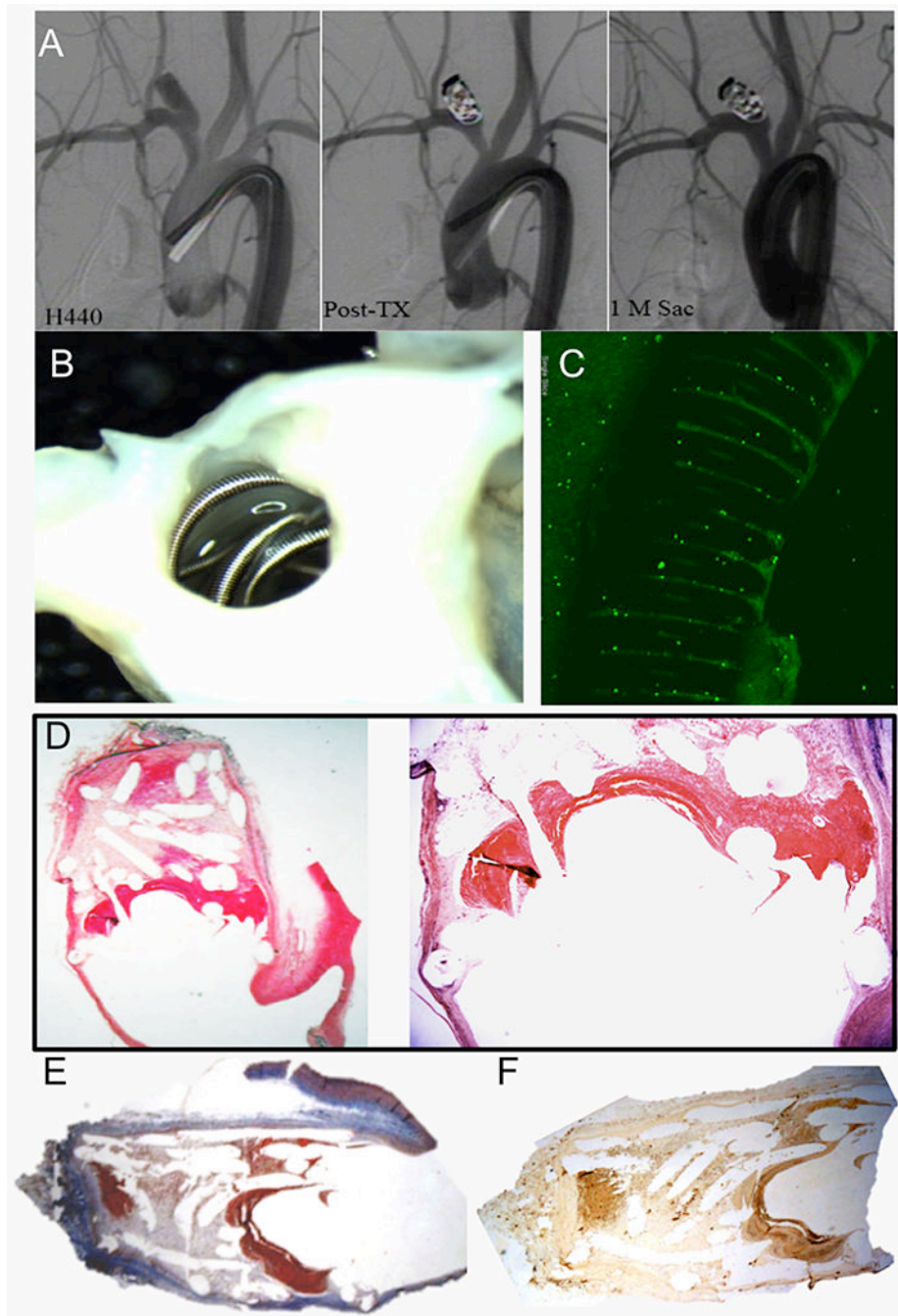
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**Figure 1. Platinum coils seeded with adipose-derived autologous mesenchymal stem cells (MSCs).**

A) Scanning electron microscopic image showing coil seeded with MSCs. B) Confocal microscopic image of MSCs seeded on the coil surface, stained with nuclear stain Syto16 (green).



**Figure 2. A set of representative images of a single aneurysm packed with Axium coils without MSC (control group).**

(A) Angiograms show stability of the aneurysm occlusion between the immediate post-treatment and 1-month follow-up angiograms with Raymond I occlusion of the aneurysm. (B) Macrophotography taken from the neck orifice demonstrates the coil loops crossing over the neck orifice are bare (original magnification, 3.2 $\times$ ). (C) Whole tissue mount staining (antibody for CD31) shows there are no CD31+ cells detected on the coil surface at the neck orifice (water lens, original magnification 20 $\times$ ). (D) Microphotograph shows poor organized thrombus at the neck interface; loose connective tissue with thin extra-cellular matrix within

the dome (H&E), original magnification 12.5× and 40×) (E) Masson Trichrome staining shows the aneurysm barely has collagen deposit within the cavity (Masson Trichrome, original magnification 12.5×) (F) Immunohistochemistry ( IHC) for RAM-11 shows a few, scattered macrophages within the dome tissue (IHC, antibody for RAM11, original magnification 25×).

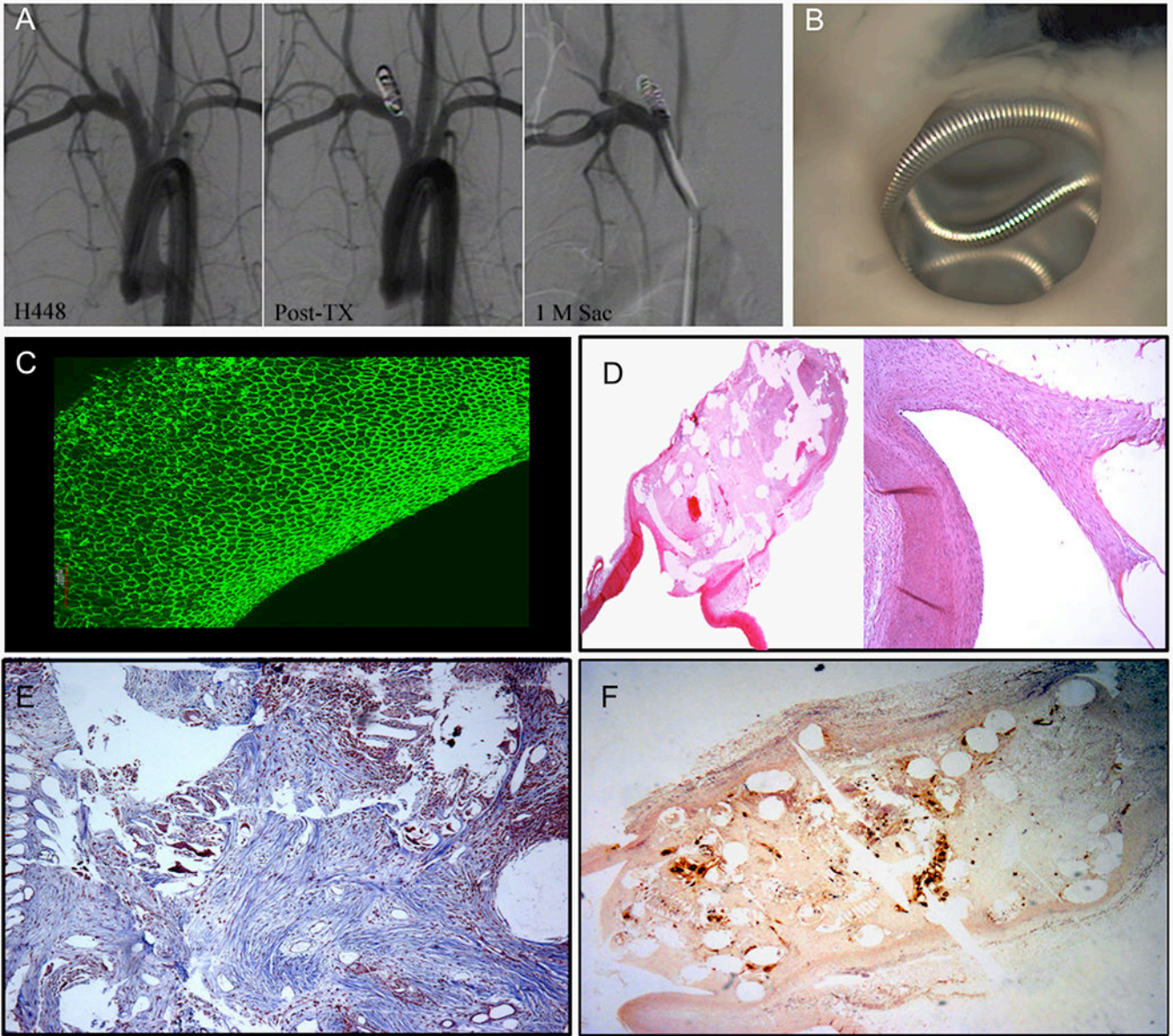
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**Figure 3. A set of representative images of a single aneurysm packed with Axiom coils with seeded autologous MSCs (MSCs group).**  
 (A) Angiograms show stability of the aneurysm occlusion between the immediate post-treatment and 1-month follow-up angiograms with Raymond I occlusion of the aneurysm.  
 (B) Macrophotograph taken from the neck orifice shows the coil loops at the neck orifice are almost covered with white, translucent and transparent membranous tissue (original magnification 6.3×). (C) Whole tissue mount staining (antibody for CD31) shows single layer, confluent, CD31 positive cells on the coil loop at neck orifice (water lens, original magnification 20×). (D) Microphotograph shows the dome is completely filled with dense connective tissue; endothelium lined thin and thick neointima completely transverses the entire neck interface. Local, dense inflammation is also shown at the top of the dome (H&E, original magnification 12.5×). (E) Masson Trichrome shows a dense packing of collagen deposition in an organized fashion in the aneurysm sac (Masson Trichrome, original

magnification 100×). (F) RAM-11 immuno-staining shows local or and diffuse, dense macrophages within the dome surrounding the coil struts (IHC, original magnification 25×).

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