

Ultrasound-mediated microbubble destruction: a new method in cancer immunotherapy

Jiawei Tu
Hui Zhang
Jinsui Yu
Chun Liufu
Zhiyi Chen

Department of Ultrasound Medicine,
Laboratory of Ultrasound Molecular
Imaging, The Third Affiliated Hospital
of Guangzhou Medical University,
Guangzhou, 510150, People's Republic
of China

Abstract: Immunotherapy provides a new treatment option for cancer. However, it may be therapeutically insufficient if only using the self-immune system alone to attack the tumor without any aiding methods. To overcome this drawback and improve the efficiency of therapy, new treatment methods are emerging. In recent years, ultrasound-mediated microbubble destruction (UMMD) has shown great potential in cancer immunotherapy. Using the combination of ultrasound and targeted microbubbles, molecules such as antigens or genes encoding antigens can be efficiently and specifically delivered into the tumor tissue. This review focuses on the recent progress in the application of UMMD in cancer immunotherapy.

Keywords: ultrasound, microbubble, cancer, immunotherapy

Introduction

The incidence of and mortality due to cancer remain high. Substantial progress has been made using conventional treatments, including surgery, chemotherapy and radiotherapy; however, relapse, metastasis and drug resistance remain the major roadblocks on the path to conquering cancer.¹ Therefore, effective strategies to eradicate tumors are urgently needed.²

Immunotherapy has been increasingly drawing clinicians' and scientists' attention owing to its effectiveness in cancer treatment.³ Compared with other strategies for cancer therapy, immunotherapy has the unique advantage of high specificity for the tumor cell while leaving normal cells unharmed. Therefore, the adverse reactions caused by drug therapy can be avoided. Moreover, curative effects of cancer immunotherapy are its rapid onset and long duration, which are different from other strategies.

During immunotherapy, the patient's immune system is activated and enhanced through administration of immune-stimulating substances with long-lasting therapeutic effects. In addition, the anamnestic effects of the host immune system, which account for recurrence prevention, can be induced by immunotherapy.⁴ Immunotherapy, which characteristically has mild adverse effects and sustainable efficacy, holds great promise for cancer treatment.⁵ Cancer vaccines, antibodies, cytokines and adoptive cell therapy (ACT) are widely used in cancer immunotherapy. Immune-activating molecules can be packaged into a recombinant protein or provided in the form of genes during drug administration.⁶ However, the physicochemical properties of these molecules, including their surface charge, hydrophilicity and size, may affect their specificity, eventually weakening their therapeutic effects.⁷

In recent years, with the development of materialogy, which has brought great benefits to the preparation of ultrasound (US) contrast agents, ultrasound-mediated microbubble destruction (UMMD) has become a versatile technology with great

Correspondence: Zhiyi Chen
Laboratory of Ultrasound Molecular
Imaging, The Third Affiliated Hospital of
Guangzhou Medical University, No. 63
Duobao Road, Liwan District, Guangzhou
510150, People's Republic of China
Tel +86 020 8129 1115
Email winchen@vip.126.com

potential in cancer immunotherapy. UMMD is a target-specific, non-invasive, effective and novel gene/drug delivery system, in which the microbubbles serve as a gene/drug vehicle or gene/drug delivery enhancer. UMMD leads to acoustic cavitations and induces the generation of physical forces, such as implosions, shock waves, microstreaming and liquid jets, and these forces can induce the disruption of the cytomembrane and enhance the permeability of the cytomembrane. Therefore, drugs, genes, antibodies and cytokines can be directly delivered into the cytoplasm of immune cells, thus enhancing the immune response.⁸ Differently from other technologies, UMMD has been shown to increase the delivery of immune-stimulating substances to tumors without causing any severe damage.

Cancer immunotherapy

For cancer patients, immunotherapy is a type of cancer therapy in which the antitumor immune response is activated so that it can act to directly attack tumor cells but leave normal cells unharmed.⁹ Cancer immunotherapy can be mediated in different ways: via cancer vaccines; through the application of monoclonal antibodies; via delivery of cytokines, such as interferon (IFN) and interleukins (ILs); and by adoptive cell transfer, including natural killer (NK) cells and T-regulatory cells (T cells).^{10,11}

In general, cancer immunotherapy can be divided into two types: active cancer immunotherapy and passive cancer immunotherapy. Active immunotherapy means that the immune response is generated by an antigen, such as a cancer vaccine, while passive immunotherapy refers to specific immune substances, such as antibodies or sensitized lymphocytes, that are reinjected into the host body to obtain specific immunity without any antigen.¹² Both therapeutic strategies can be enhanced by UMMD.

Effects of UMMD

UMMD is a promising technique for non-invasive, targeted drug and gene delivery, and its applications for immunomodulatory substance delivery to tumor tissues have attracted increasing interest.¹³ The movement and destruction of US-mediated microbubbles can trigger enhanced permeability of cytomembranes, open tight junctions (eg, the blood–brain barrier [BBB], blood–tumor barrier and interendothelial junctions) and promote cell endocytosis, thereby providing a transient and invertible channel for the delivery of drugs, genes or gene vehicles and other macromolecules across the endothelial gap and across biological membranes.^{14–16}

Under US irradiation, microbubbles explode and oscillation and destruction are induced.¹⁷ Thus, ruptured

microbubbles can serve as a tool to induce local energy release using the acoustic radiation force (ARF), microstreaming, shock waves, microjets and strains. These forces have a direct influence on the cell membrane and vascular wall, enhancing the delivery efficiency of a drug/gene into the cytoplasm.¹⁸ The common mechanisms of UMMD technology include a cavitation effect, a heat effect, ARF and acoustic droplet vaporization (ADV) (Figure 1).¹⁹

Cavitation effect

The cavitation effect is based on the interaction between microbubbles and US. Under a US field at low power, microbubbles oscillate symmetrically and linearly, implying an opposite tendency of the expansion and compression of a microbubble. The situation is different for higher US intensities. In a high-intensity US field, microbubbles behave nonlinearly and expand significantly to a state larger than twice the initial size followed by rupture, causing a high acoustic pressure in a local area, which may be as high as several thousand atmospheres.²⁰ These two phenomena are also known as stable cavitation (or non-inertial cavitation) and inertial cavitation. Stable cavitation refers to the oscillation phenomenon in which a microbubble dilates at its syntonous size, creating a liquid flow called microstreams around the microbubbles. When these oscillating microbubbles reach cells, shear stress is generated, enhancing the permeability of the cell membrane.^{21,22}

It is commonly recognized that inertial cavitation is a crucial mechanism of cavitation that always occurs under a high acoustic field. Inertial cavitation is characterized by sudden expansions and subsequently rapid collapses of gas microbubbles caused by microbeams.²³ Microbeams can produce a shear force on the surface of microtubules, causing microbubbles to deform or even rupture.²⁴ The energy induced by microbubble destruction can cause various biological effects, such as temporary holes in the cell membrane, which promote entry of drugs and genes into cells, subsequently enhancing the antitumor immune response of the host body (Figure 2).

The cavitation of microbubbles can trigger many cell bioeffects, especially the enhancement of cell endocytosis.²⁵ According to a recent study, Ca^{2+} can immediately excite endocytosis for cytomembrane resealing.^{26,27} Fan et al found that the intracellular Ca^{2+} concentration was simultaneously increased with the function of cavitation and onset of sonoporation, and gradually recovered to the normal level within approximately 100 seconds.²⁸ In this way, during the time window when the Ca^{2+} level was increased, endocytosis was also enhanced by the cavitation and sonoporation. Moreover,

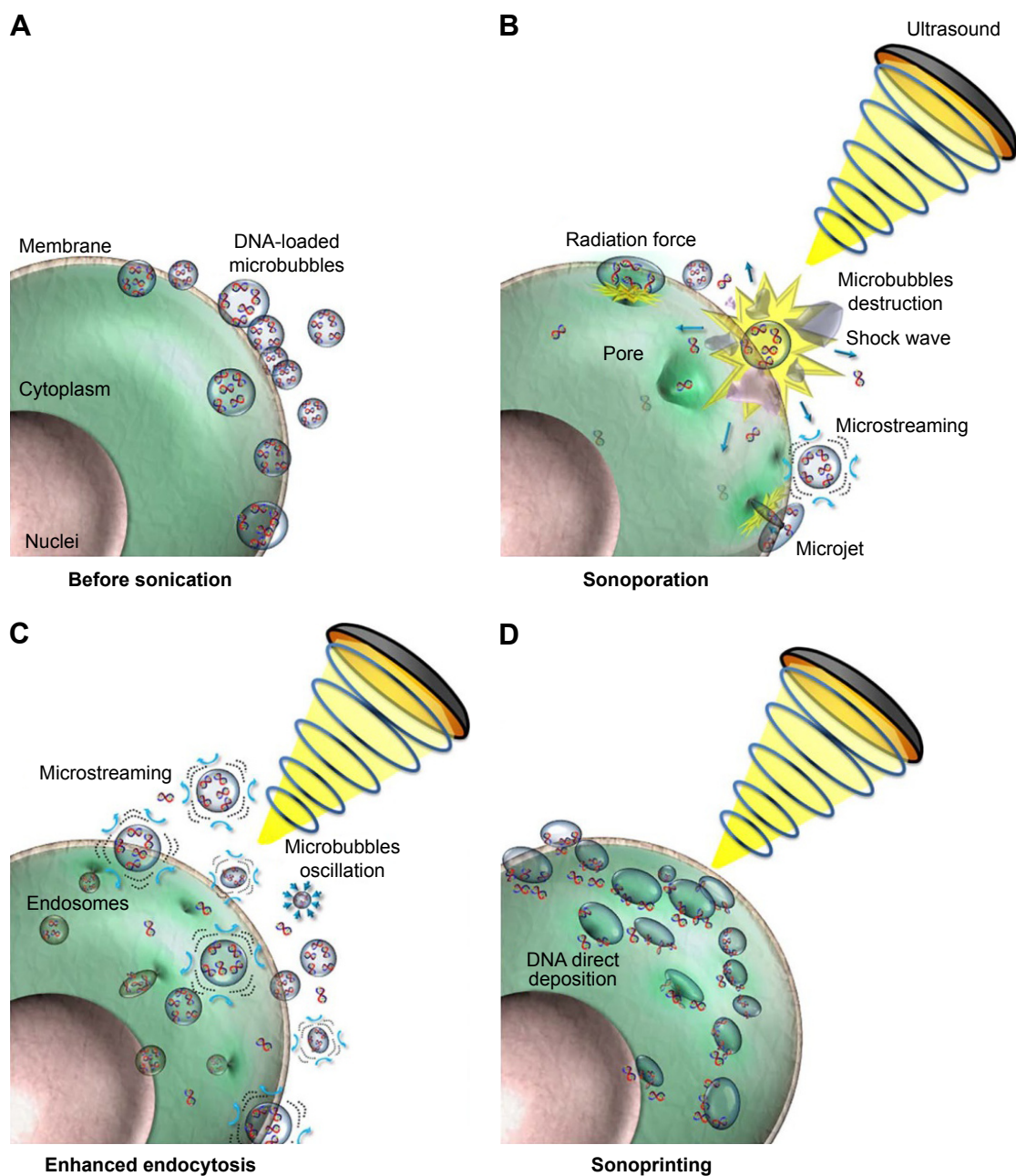


Figure 1 UMMD enhances the microbubble payload delivery into the cell.

Notes: (A) Observation of the cell and microbubble before US sonication. (B) In the field of US, the microbubbles oscillate and rupture, resulting in a series of physical effects including shock waves, microstreaming and microjets. (C) These physical effects increase the permeability of the cytomembrane so that endocytosis is enhanced. (D) The acoustic radiation force pushes the microbubble payload to the exosurface of the cell. Reprinted from Journal of Controlled Release, Volume 261, Fan CH, Lin CY, Liu HL, Yeh CK, Ultrasound targeted CNS gene delivery for Parkinson's disease treatment, pages 246–262, © 2017 with permission from Elsevier.¹⁹

Abbreviations: UMMD, ultrasound-mediated microbubble destruction; US, ultrasound.

several substances (eg, ceramide) were secreted by lysosomes (delivered to the damaged membrane), which can induce endocytosis and rapid formation of endosomes.²⁹

Acoustic radiation force

Oscillating microbubbles located inside the vascular structure in an acoustic field can translate toward the vascular wall through the ARF.³⁰ The microbubbles translate in the direction of wave diffusion in the case of a traveling acoustic wave.

It is not easy to translate freely with the restriction of fluid shear and the floating action in the vasculature. With the help of the pressure gradient induced by ARF, microtubules can move away from the sound source. Hence, microbubbles can be delivered to targeted areas and adhere to the targeted cells.³¹ According to Rychak et al, ARF can promote a shift and aggregation of microbubbles toward the vascular wall, increasing the adhesion rate of targeted microbubbles 60–80-fold.³²

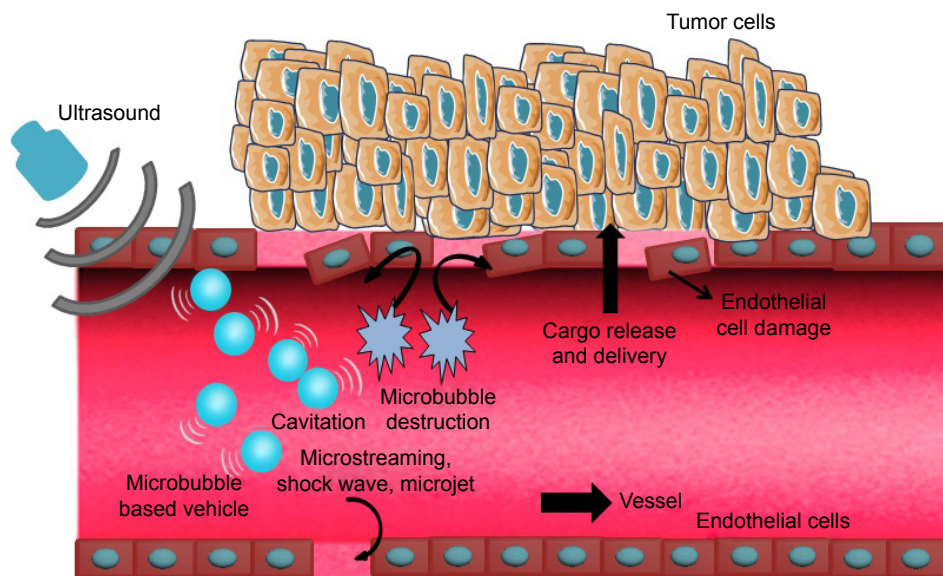


Figure 2 Schematic of enhanced delivery of UMMD.

Notes: The microbubble-based vehicles (ie, gene/drug-loaded microbubbles) oscillate and even rupture under the US irradiation. Therefore, a series of physical forces is generated (including microstreaming, shock waves and microjets), which cause damage to endothelial cells. The released cargo can be delivered into tumor tissue more effectively.

Abbreviations: UMMD, ultrasound-mediated microbubble destruction; US, ultrasound.

UMMD and ARF have a synergistic effect, which can cause tissue damage and reduces the side effects of intravenous administration while improving microbubble targeting to tissues. ARF impacts the fluidity of lipid bimolecular membranes, resulting in a shear force, broadening the space of endothelial cells, increasing the permeability of capillaries and promoting gene or drug delivery.³³

Acoustic droplet vaporization

In general, the continuous microvascular structure and dense normal endothelial gap make it difficult for macromolecules to penetrate the blood vessel wall. By contrast, the leaky blood vessels surrounding tumor tissues show heterogeneous hyperpermeability, which leads to penetration and retention of macromolecule material in the tumor bed, which is known as the enhanced permeation and retention (EPR) effect. During cancer therapy, high delivery of macromolecular drugs and genes based on the EPR effect is strongly dependent on the permeability of the tumor microvasculature.^{34–36}

Owing to the inherent leakiness of the underdeveloped tumor vasculature, the enhanced permeability enables nanoparticles loaded with drugs or genes to escape the circulation and assemble at tumor tissues.³⁷ Therefore, nanodroplets that rely on the EPR effect to target tumors prolong the half-life of drugs and enhance their efficacy, with reduced side effects. EPR-based nanodroplets are widely used in medicine. For example, albumin-bound paclitaxel nanodroplets

were approved by the US Food and Drug Administration to treat breast cancer in 2005.³⁸ Furthermore, paclitaxel-loaded nanodroplets were recently used in a clinical trial to treat non-small-cell lung cancer.³⁹ The liquefied gas nanodroplets are much smaller than microbubbles and can load much more gas. In an acoustic field of sufficient intensity, these nanodroplets are transformed into gas bubbles that are triggered by acoustic waves without obviously causing heating effects on surrounding normal tissues.⁴⁰ Such a phase-change phenomenon is called ADV, which was first described in the 1990s and has subsequently been widely used in imaging for preclinical trials.⁴¹ Recently, the application of ADV in drug delivery has received extensive attention.⁴² Since the diameter of these liquid droplets is sufficiently small to traverse the lungs, they can easily pass through the narrow space of tumor tissues.⁴³ Furthermore, transudatory nanodroplets vaporized into gas bubbles can be activated by acoustics, leading to cavitation in the membranes of tumor tissues to enhance drug delivery.⁴⁴ Thus, efficient delivery of the nanodroplets loaded with mRNA encoding a tumor antigen can induce a significant immunostimulatory effect that is meaningful for antitumor immunotherapy.

Immunotherapy assisted by UMMD

Low-frequency US combined with microbubbles simultaneously promotes dendritic cells (DCs) to differentiate and mature in the cancer microenvironment.⁴⁵ In addition, this

phenomenon promotes T lymphocytes to trigger antitumor immunity mediated by T lymphocytes, which enhance the efficacy of angiogenesis targeting.⁴⁶ UMMD has been widely applied as a tool to enhance the delivery of immunomodulatory materials, such as cancer vaccines, antibodies, adoptive cells and cytokines, resulting in enhancement of the immunotherapy effect. Relevant reports of UMMD-triggered immune effects are listed in Table 1.

Cancer vaccination

Cancer vaccination is attracting increasing attention as a promising therapy strategy for the prevention and treatment of tumor growth, as well as metastasis. Immunotherapy by cancer vaccination has gradually become the mainstream strategy in recent years. Cancer vaccines can be divided into the following types: tumor antigen vaccine (polypeptide vaccine and DNA vaccine), whole-cell vaccine (tumor cell vaccine and dendritic cell [DC]-based vaccine), bacterial vector vaccine, and so on.⁴⁷ Among these, DC-based

vaccine and DNA vaccine are mostly commonly used in cancer immunotherapy. However, effective treatment by cancer vaccination needs a high delivery efficiency of cancer antigen into host antigen-presenting cells (APCs) to activate the immune response. Consequently, cancer vaccination is a targeted therapy with quite low adverse effects.

DC-based vaccination

DCs have unique capabilities involving innate and adaptive immune responses, making them an ideal APC to boost antitumor attack.^{47,48} In numerous clinical trials, DC-based vaccines have been shown to be safe and effective in cancer immunotherapy.⁴⁹ During DC-based vaccine therapy, loading DCs with tumor antigens and subsequently activating DCs are crucial. It has been demonstrated that transfection is significantly enhanced using microtubules, and US can activate powerful immune responses *in vivo*, which can be applied as a potential method for further clinical trials (Figure 3).⁵⁰ Oda et al used microbubbles combined with US

Table 1 Summary of experiments and immune responses after treatment with UMMD

Experiment type	Animal type/ cell type	Tumor type	US-sensitive vehicle	Immunostimulation materials	US parameter	Immune effect	Reference
In vivo	C57BL/6 mice	Melanoma	Microbubbles	Antigen and mRNA	1 MHz, 2 W/cm ² , 20% duty, 30 seconds insonation time	Tumor outgrowth ↓	Dewitte et al ⁵⁰
In vivo	C57BL/6 mice	Melanoma	Liposome microbubbles	Antigens	2 MHz, 2.0 W/cm ² , 10% duty, 3×10 seconds insonation time	Melanoma lung metastases ↓	Oda et al ⁵¹
In vivo	C57BL/6 mice	Ovarian carcinoma	PEG-modified bubble lipoplexes	pDNA	Not mentioned	Antitumor effects ↑	Un et al ⁵⁷
In vivo	C57BL/6 mice	Melanoma	Mannose-modified bubble lipoplexes	pDNA	1.045 MHz, 1.0 W/cm ² , 50% duty, 1 minute insonation time	Transcriptional factors ↑	Yoshida et al ⁵⁹
In vitro	DLD1 and AGS cells	Colorectal cancer	Phase-change nanodroplets	Antibody	100 cycles at 4 MHz, 1.5 MPa peak negative pressure	Tumor cell apoptosis ↑	Ishijima et al ⁶⁴
In vivo	Nude rats	Brain metastasis	Microbubbles	Antibody	0.40–0.70 W/cm ² , 10 ms burst sonications, 0.46–0.62 MPa peak negative pressure	Tumor outgrowth ↓	Kobus et al ⁷¹
In vivo	Athymic nude rats	Breast cancers with HER2	Definity microbubble	NK-92	551.5 kHz focused transducer, 0.33 MPa average peak rarefaction pressure	NK-92 brain delivery ↑	Alkins et al ⁸²
In vitro	Tregs from HCC patients	Hepatocellular carcinoma	SonoVue microbubble	T cells	10% microbubbles, 1.4 mechanical index, 150 or 180 seconds insonation time	Treg proliferation ↑	Shi et al ⁸⁸
In vivo	C57BL/6 X C3H/He mice	Ovarian carcinoma	Bubble liposomes	pDNA	1 MHz, 0.7 W/cm ² , 60 seconds insonation time	Tumor outgrowth ↓	Suzuki et al ⁹⁴

Notes: ↑, up regulated; ↓, down-regulated.

Abbreviations: HCC, hepatocellular carcinoma; NK, natural killer; PEG, poly(ethylene glycol); Treg, regulatory T cell; UMMD, ultrasound-mediated microbubble destruction; US, ultrasound.

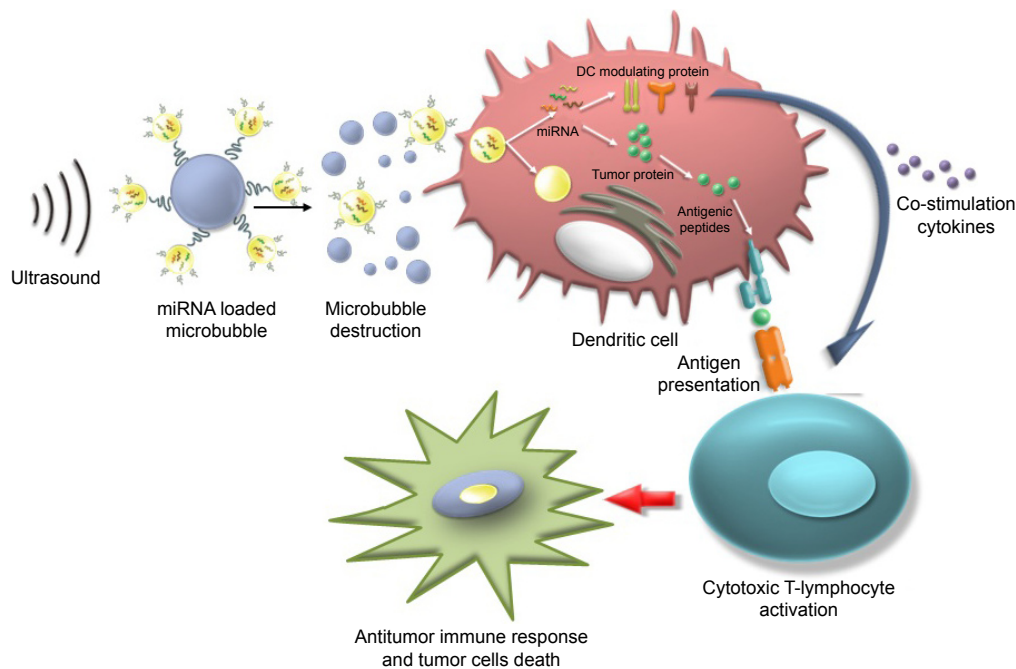


Figure 3 Schematic of the use of US with mRNA-loaded microbubbles.

Notes: The mRNA-loaded microbubbles implode upon exposure to US and sonoporate the DCs. As a result, both antigen- and DC-modulating proteins are produced by the DC, which can lead to antigen presentation and T-cell activation. Reprinted from the Journal of Controlled Release, Volume 194(12), Dewitte H, Van Lint S, Heirman C, et al, The potential of antigen and TriMix sonoporation using mRNA-loaded microbubbles for ultrasound-triggered cancer immunotherapy, pages 28–36, Copyright © 2014, with permission from Elsevier.⁵⁰

Abbreviations: DC, dendritic cell; US, ultrasound.

irradiation to deliver antigens that were extracted from tumor cells into DCs and then investigated the therapeutic effect of the treated DCs on a mouse model of lung metastasis. The results demonstrated that prophylactic immunization with this strategy showed significant suppression (a four-fold decrease) of melanoma lung metastases.⁵¹

DNA vaccination

Several studies have reported that DNA vaccination can activate the immune response, including humoral immunity and cellular immunity, using cancer antigens encoded by exogenous tumor-associated genes.^{48,52} An exogenous gene encoding cancer antigens is called a DNA vaccine.^{53,54} To achieve the full therapeutic effects of DNA vaccination, it is necessary to divert the antigen-coding gene selectively and effectively into APCs (macrophages and DCs), which play a critical role in the initiation, programming and regulation of antitumor immune responses.⁵⁵

Many researchers have demonstrated that the effects of cancer vaccination can be improved by UMMD-triggered gene transfection technologies.⁵⁶ Un et al developed a mannose-modified gene carrier called Man-PEG₂₀₀₀ [mannose-poly(ethylene glycol) 2000] bubble lipoplexes to deliver a DNA vaccine into APCs, resulting in high antitumor effects (Figure 4).⁵⁷ With the help of these transfection methods, it is

possible to deliver a large amount of gene-loaded antigen as well as antigen peptides into APCs.⁵⁸ Yoshida et al synthesized a US-responsive gene carrier (doxorubicin-encapsulated poly(ethylene glycol)-modified liposome microbubble) to deliver the DNA vaccine. The results suggested that the combination of US and the DNA vaccination-loaded liposome microbubble can increase the delivery of DNA vaccine, inducing an effective therapeutic outcome for cancer immunotherapy.⁵⁹

Antibody-based immunotherapy

Because immunoregulation of antitumor treatments is often used clinically today, therapeutic antibodies that can distinguish tumor cells have been developed in recent years. Antibodies can provide effective treatment by targeting specific molecular targets, thus inhibiting tumor cell growth.⁶⁰

Bevacizumab is a drug that targets vascular endothelial growth factor (VEGF) and tumor neovascularization, subsequently inhibiting the biological function of VEGF.⁶¹ Liu et al reported enhanced delivery of the antiangiogenic antibody bevacizumab into the central nervous system using the combination of focus US, microbubble and magnetic resonance imaging (MRI) monitoring.⁶² Rituximab is another antibody that can specifically bind to CD20⁺ lymphoma cells and induce cell apoptosis.⁶³ In 2017, Ishijima et al developed a phase-change nanodroplet conjugated with an antitumor

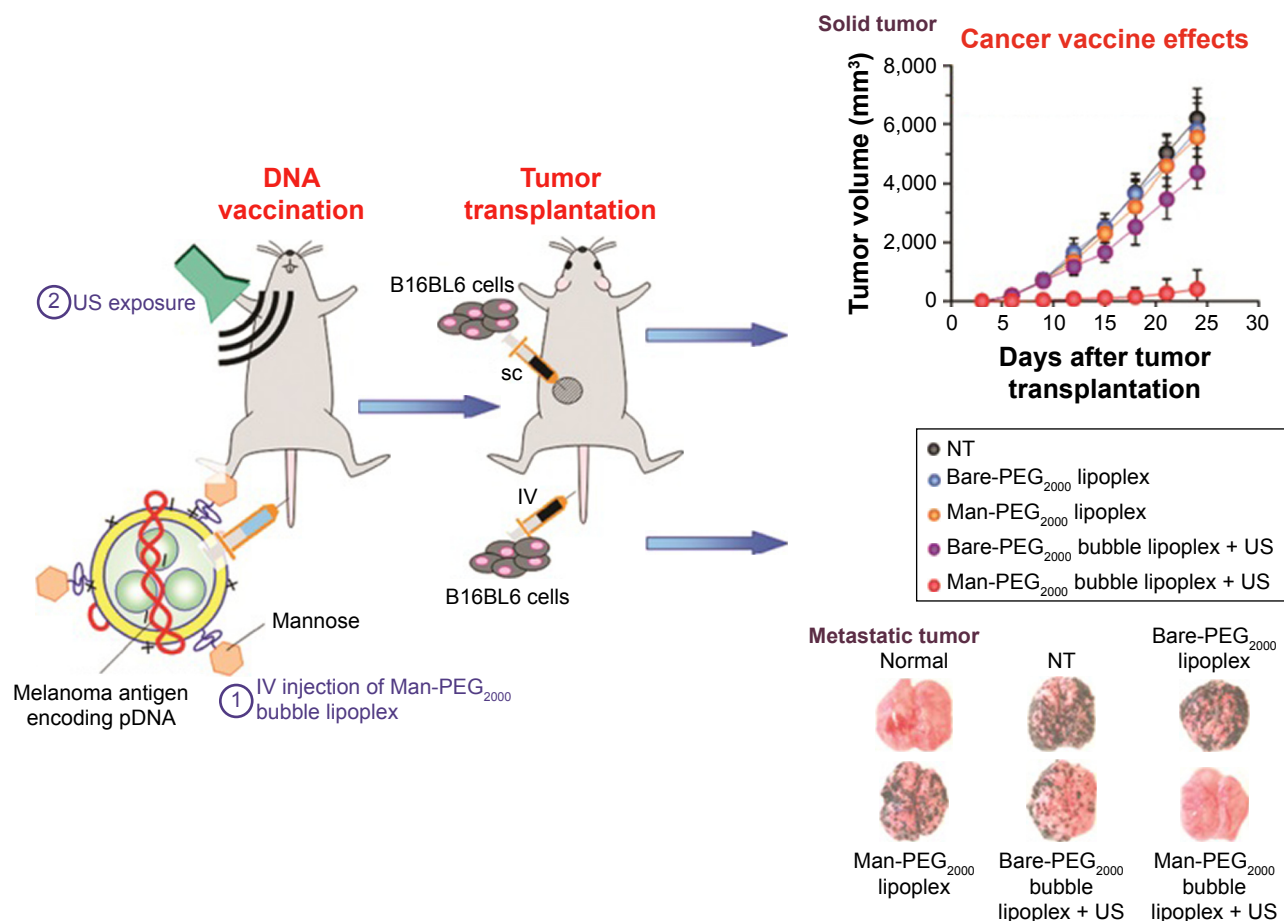


Figure 4 Schematic representation of the treatment method of US exposure combined with pDNA-loaded microbubbles.

Notes: During this treatment, the pDNA-loaded bubbles are ruptured by the US irradiation and release the loading melanoma antigen-encoding pDNA in vivo. In this way, the treated mouse obtains antimelanoma immunity. Reproduced with permission from Un K, Kawakami S, Suzuki R, Maruyama K, Yamashita F, Hashida M. Suppression of melanoma growth and metastasis by DNA vaccination using an ultrasound-responsive and mannose-modified gene carrier. *Mol Pharm*. 2011;8(2):543–554. Copyright © 2011, American Chemical Society.⁵⁷

Abbreviations: Man, mannose; PEG₂₀₀₀, poly(ethylene glycol) 2000; NT, not treatment; SC, subcutaneous; US, ultrasound.

antibody (9E5), and in vitro experiments showed that the antibody was delivered to 97.8% of high-epiregulin-expressing cancer cells and that 57% of those cancer cells were killed with US irradiation (Figure 5).⁶⁴

However, antibody-based immunotherapy is less efficient in solid tumors because it is difficult to enrich antibodies within the tumor and the bioavailability in the tumor is very poor.⁶⁵ Thus, systemic and repeated delivery of a high antibody dose is essential to reach the therapeutic concentration, which increases the side effects and costs.⁶⁶ Monoclonal antibodies targeting the HER2 protein, such as trastuzumab, have the potential to prolong the survival of patients with HER2⁺.⁶⁷ Trastuzumab is a humanized monoclonal antibody that is widely used in clinical treatment. However, several recent studies have reported that the use of a large amount of trastuzumab resulted in an increasing incidence of brain metastases.⁶⁸

Antibodies and other drugs are often unsatisfactory for the treatment of brain metastases because the BBB and

blood–tumor barrier prevent most drugs entering the brain.⁶⁹ To effectively treat brain metastases and reduce side effects, drugs or genes must be delivered efficiently to the brain.⁷⁰ In the study by Kobus et al, HER2-targeting antibodies combined with US and Optison (GE Healthcare, Milwaukee, WI, USA)TM were utilized to inhibit the growth rate of a tumor model derived from HER2-positive breast cancer metastasis to the brain. The results demonstrated that the antitumor effects of antibodies can be significantly enhanced by the synergism of US and Optison.⁷¹

Adoptive cell therapy

As a highly individualized cancer therapy, ACT involves the regulation of the tumor-bearing host's immune cells with direct antitumor activity.^{72,73} ACT has been shown to be more effective than other cancer immunotherapies, although it relies on abundant antitumor immune cells with high activity, including regulatory T cells (Tregs) and NK cells.⁷⁴

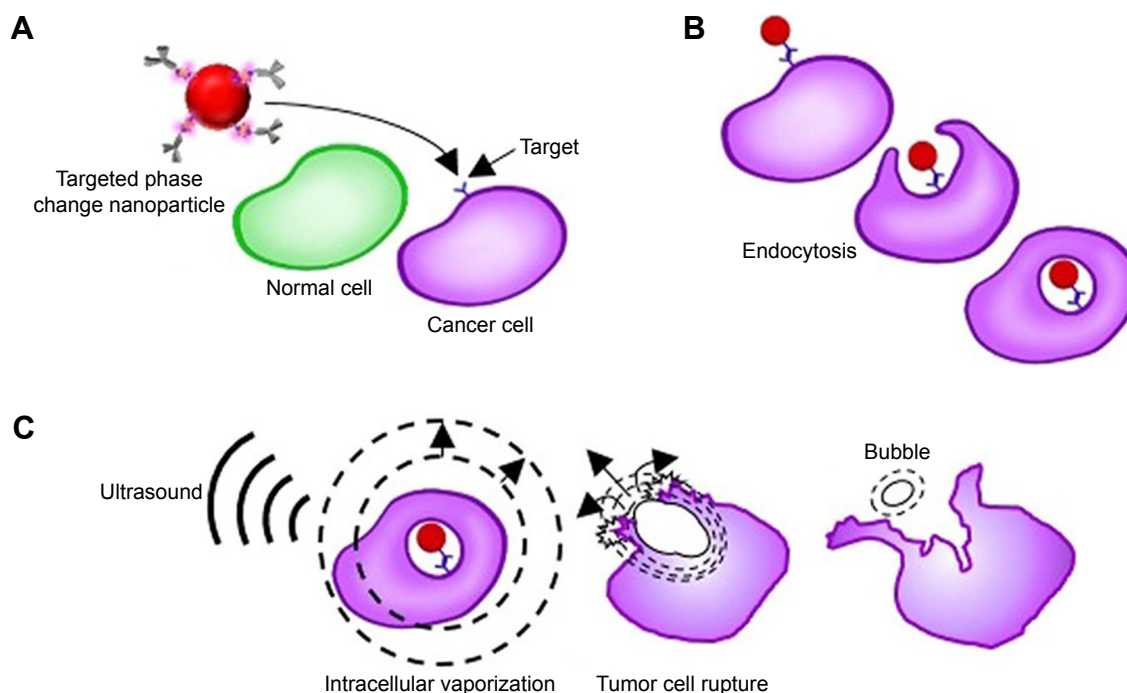


Figure 5 Schematic explaining the synergistic treatment of ultrasound with targeted liquid fluorocarbon droplets.

Notes: (A) The targeted liquid fluorocarbon droplets selectively adsorb to the cancer cell by the identification of the target. (B) Then the liquid fluorocarbon droplets enter the cancer cells via antibody-mediated endocytosis. (C) Then, vaporization by ultrasound exposure occurs in the tumor cell, resulting in a bigger bubble which induces the death of the tumor cell. Reproduced from Ishijima A, Minamihata K, Yamaguchi S, et al. Selective intracellular vaporisation of antibody-conjugated phase-change nano-droplets in vitro. *Sci Rep.* 2017;7:44077. Copyright © 2017, Springer Nature.⁶⁴

Most importantly, adoptive cell transfer provides a beneficial microenvironment to support antitumor immunity. Until now, the most widely used immune cells in ACT have been NK cells. Transferred adoptive cells can proliferate in the new host and retain their antitumor ability. First, reinjection of a large amount of adoptive cells leads to unpredictable side effects, such as pyrexia and anaphylaxis.⁷⁵ Second, the number of adoptive cells delivered to the targeted areas is always too low to play an effective role in killing tumor cells. Furthermore, the normal functions of adoptive cells may be influenced by the ex vivo expansion strategy as well as the immunosuppressive effect of the self-tumor microenvironment.⁷⁶

NK-cell-based immunotherapy

NK cells are a type of cytotoxic T-lymphocyte that play an important antitumor role in the innate immune system. In addition, NK cells can regulate immune function as well as kill tumor cells.⁷⁷ Furthermore, NK cells can induce tumor cell apoptosis in an antigen-dependent method when the antibody is adherent to the receptors. NK-92 is a human NK cell line, which has been demonstrated to have connection with tumor-associated antigens in tumor tissues. However, in clinical trials, the effectiveness of NK cells in treating cerebral tumors is restricted by their poor ability to traverse the BBB.⁷⁸ The BBB limits the passage of most substances,

including cells, nucleic acids and antibodies, from the blood circulation into the brain tissue, thus suppressing their treatment effect.

Fortunately, recent studies have shown the potential to transiently open the BBB, enabling enhanced permeation of drugs or genes. O'Reilly et al investigated the time taken for the BBB to close and the opening volume on the time scale of closure after focused US exposure; no significant differences were detected on MRI between large- and small-volume sonications, suggesting that safe BBB opening can be achieved by US combined with microbubbles.⁷⁹ Lin et al demonstrated that the BBB can be successfully opened by US-triggered microbubble destruction and thus the delivery of exogenous substances can be significantly improved, although the specific mechanisms are still unclear.⁸⁰ So far, the following statements can be made: the ARF pushes microbubbles toward the vascular wall and promotes an impact on vascular cells that induces a loose intercellular gap; and microbubbles inside the vasculature can produce microstreams and shock waves, thus compromising the stability of the vascular wall. After the safe BBB disruption with focused ultrasound (FUS) and microbubbles (Figure 6), NK-92 cells are largely delivered into brain tumor tissues and exert their anticancer effects, causing a higher suppression of tumor growth and longer survival time in a mouse brain tumor model compared to the non-treatment prototype.⁸¹

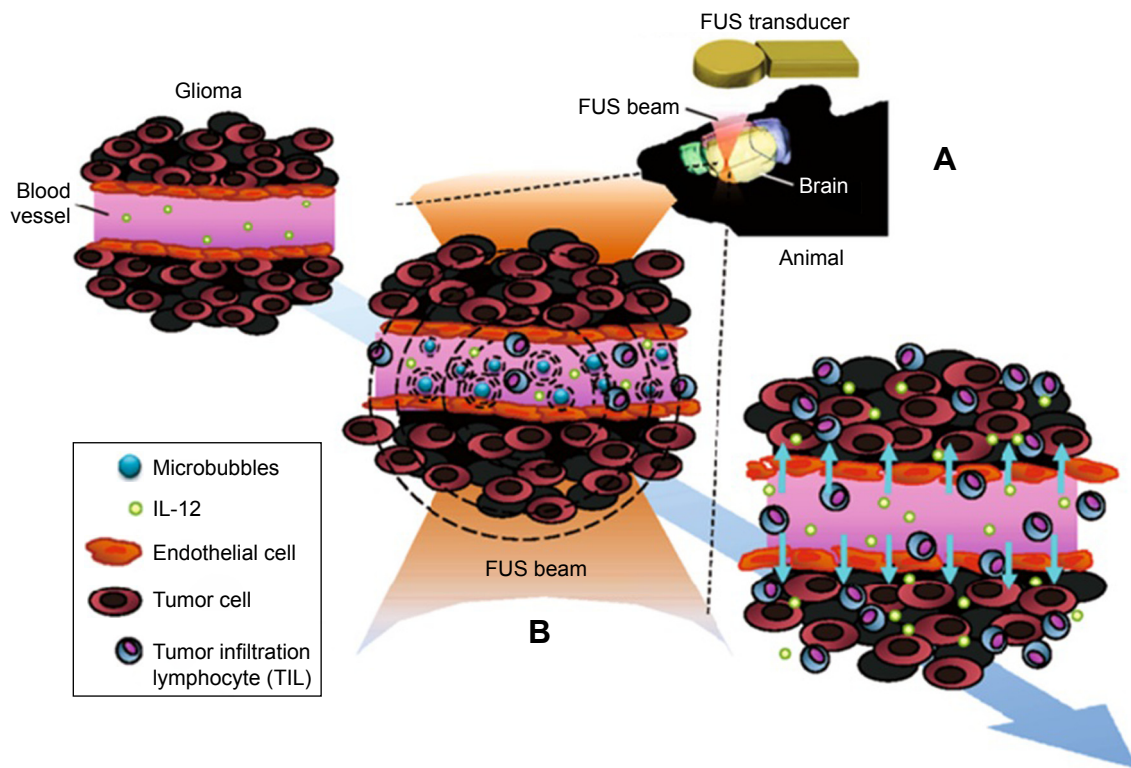


Figure 6 Schematic of FUS-induced BBB opening to enhance IL-12 delivery in brain glioma treatment.

Notes: (A) The FUS transducer produces an FUS beam to the brain. (B) The microbubbles in the capillaries of brain tissue oscillate and explode under the FUS, and thus induce BBB opening. Therapeutic molecules such as IL-12 can then be delivered into the brain tumor effectively to trigger local immunological effects to improve the antitumor effect. Reproduced from Alkins R, Burgess A, Kerbel R, Wels WS, Hynynen K, Francia G. Early treatment of HER2-amplified brain tumors with targeted NK-92 cells and focused ultrasound improves survival. *Neuro Oncol.* 2016;18(7):974–981.⁸¹

Abbreviations: BBB, blood–brain barrier; FUS, focused ultrasound; IL-12, interleukin-12.

Alkins et al labeled HER2 high-expressing breast tumor cells with superparamagnetic iron oxide (SPIO) and implanted them into nude rats. Following transcranial FUS irradiation and intravenous injection of SPIO-labeled NK cells, MRI showed a remarkable spark drop, indicating successful homing clustering of NK cells.⁸²

T-cell-based immunotherapy

Tregs are known to produce ILs and transforming growth factors, but they have an inhibitory effect on tumor-associated APCs because tumor-associated APCs, such as DCs, lose their co-stimulatory ligands, causing an inability to support T-cell activation.⁸³ In addition, CD4⁺CD25⁺ Tregs are reported to have an important effect on antitumor immune responses.⁸⁴ Tregs may induce immune tolerance to self-antigens and suppress the self-immune response against cancer by suppressing reactive immune cells. In addition, the poor clinical efficacy of antitumor immunotherapy may result from the excessive presence of Tregs.^{85,86} Therefore, the strategy of using targeted Tregs will be an effective treatment to enhance antitumor immunotherapy.⁸⁷ Shi et al studied the treatment effects on the viability of CD4⁺CD25⁺ Tregs induced by the combination of US and SonoVue® (Bracco Co. Geneva, Switzerland)

microbubbles, and explored the optimal US parameters for Treg transfection. Their results suggest that US and microbubbles have a synergistic effect on the enhancement of Treg proliferation, and the optimal Treg transfer rate was acquired by irradiation with US for 150/180 seconds under a US mechanical index of 1.4 in the presence of 10% microbubbles.^{88–90}

Cytokine immunotherapy

The aim of cytokine immunotherapy is to deliver cytokines to a local area at a high concentration to induce a forceful antitumor immune response. In the recent literature on cytokine immunotherapy triggered by US and microbubbles, several trials have delivered cytokines, including IL-2, IL-10 and IL-13, as well as tumor growth factors, to stimulate an immune response.^{72,91}

IL-based immunotherapy

ILs have been reported to have an antitumor effect because they can serve as immunostimulatory molecules that can trigger an antitumor immune response. Among the cytokines mentioned in the previous paragraph, IL-12 plays the most important role in immunity and tumor angiogenesis; thus, it has garnered the most attention. IL-12 is a heterodimeric

protein consisting of p35 and p40 subunits produced by DCs and macrophages, and has multiple immunoregulatory and antitumor effects.⁹²

In turn, activated T cells increase the level of IFN- γ , which triggers positive feedback on APCs to secrete IL-12.⁹³ Suzuki et al assessed the utility of the combination of IL-12-loaded microbubbles and US in cancer therapy and found that this system can induce a T-cell-dependent immune response that can dramatically suppress tumor growth.⁹⁴ In addition, Chen et al applied FUS to induce BBB opening and subsequent safe IL-12 delivery, and found that this method activated local immune responses to enhance antitumor effects.⁹⁵

IFN-based immunotherapy

IFN has several biological effects, such as immunoregulation and anti-proliferative activities, on some cancer cells. Moreover, IFN induces cell apoptosis, resulting in tumor inhibition. Sakakima et al examined tumor suppression after IFN gene transfection with the combination of US and a mixture of IFN and microbubbles. The results revealed that the tumor size was significantly reduced after IFN gene transfection, indicating that IFN-based antitumor immunotherapy with sonoporation may be a new treatment option for tumors.^{96,97}

Conclusions and future prospects

UMMD is now considered to be a promising non-viral gene/drug delivery system. This technology combines the advantages of microbubbles/nanodroplets and US in such a way that US-triggered microbubbles or nanodroplet destruction induces a series of physical effects. Thus, the permeability of physiological barriers can be instantaneously enhanced, allowing immunostimulatory materials (ie, antibodies, antigens, immune cells and vaccines) to traverse across the barriers to exert their effects.⁹⁸ Antitumor immune responses have been achieved by delivering immunostimulatory substances using the combination of US and microbubbles and nanoparticles. UMMD-mediated immunotherapy is in its infancy, but provides promising strategies for cancer treatment.

Recent research progress concerning the dynamic and complicated interactions between the immune system and cancer plays a role in guiding cancer immunotherapy, which will be available for innovative cancer therapy. Numerous studies have utilized microbubbles/nanoparticles as delivery vehicles in combination with US to transport antibodies, antigens and immunostimulatory molecules to APCs, which have shown enhanced CD4⁺ and CD8⁺ T responses against tumors. Likewise, other macromolecules, including miRNA and pDNA, can be delivered into tumor tissues in this way.

However, both microbubbles and nanoparticles have two major disadvantages for utilization as delivery carriers to tumor cells. First, they are too large to easily and effectively traverse many barriers. Second, the half-life of gas-filled microbubbles or nanobubbles is fairly short in vivo, resulting in a poor US-triggered ability. Furthermore, the low systemic cytotoxicity, high specificity and lasting efficacy, as well as the good bioavailability of gene/drug vehicles, are clinically challenging for optimizing delivery technology.⁹⁹

The improvement of this method relies on several main strategies. The first possible solution to this issue is replacing the gas in the microbubble with perfluorooctylbromide. Although some researchers have explored this idea and generated results, further study is required.¹⁰⁰ Another potential method is using targeting ligands specific to immune cells,¹⁰¹ so that effective immunotherapy can be optimized. Finally, when using UMMD-based immunotherapies, the differences between liquid and solid tumors should be considered.

Acknowledgments

This work is supported by the Research Projects of the National Natural Science Foundation of China (number 81671707), the Natural Science Foundation of Guangdong Province (number 2016A030311054), the Research Projects of Guangzhou Technology Bureau (number 201607010201) and the Research Fund for Lin He's Academician Workstation of New Medicine and Clinical Translation.

Disclosure

The authors report no conflicts of interest in this work.

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