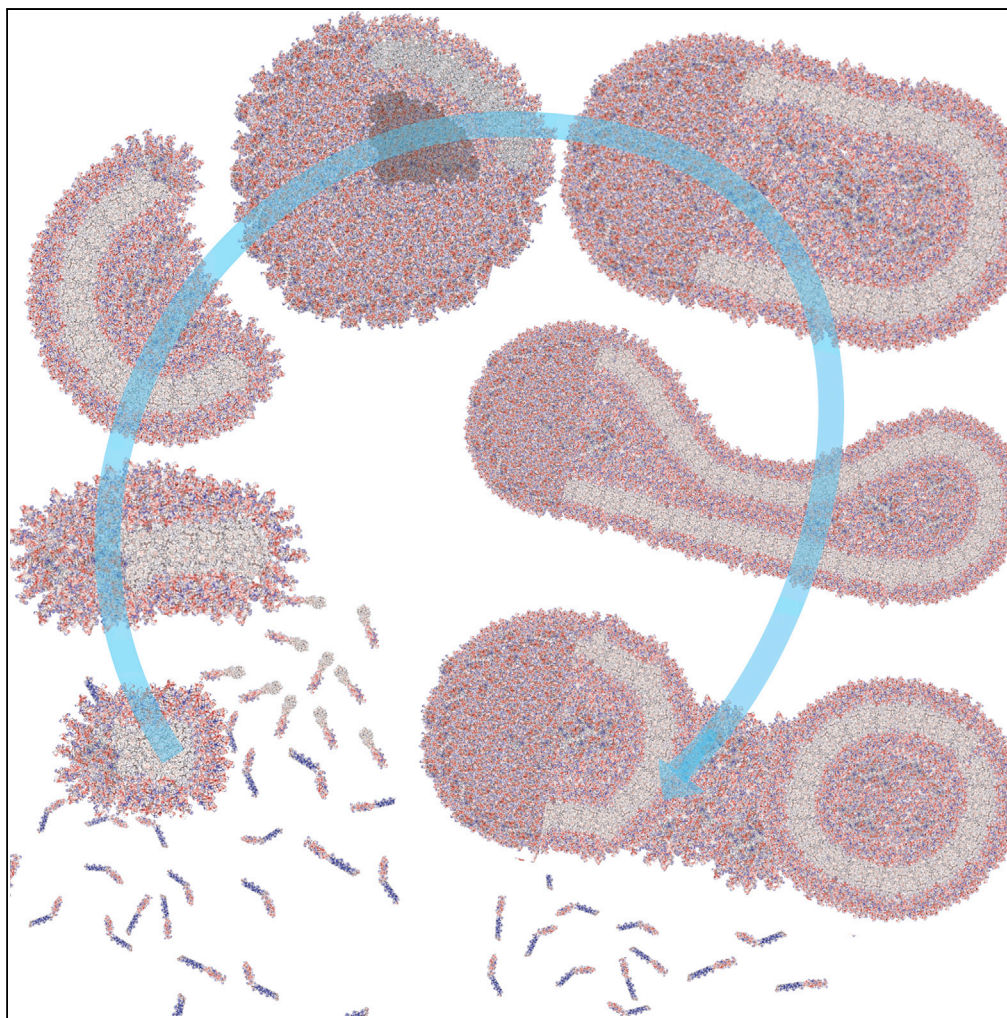


Article

Bottom-Up Evolution of Vesicles from Disks to High-Genus Polymersomes



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HIGHLIGHTS

Membrane-confined compartments are the most exquisite examples of self-assembly

We mimic compartmentalization using self-assembling polymers

We show that bottom-up assembly evolves from disk to vesicles to high-genus vesicles

We combine experiments and theory to fully elucidate vesiculation

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Article

Bottom-Up Evolution of Vesicles from Disks to High-Genus Polymersomes

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SUMMARY

Polymersomes are vesicles formed by the self-assembly of amphiphilic copolymers in water. They represent one of the most promising alternatives of natural vesicles as they add new possibilities in the amphiphiles' molecular engineering of aqueous compartments. Here we report the design of polymersomes using a bottom-up approach wherein self-assembly of amphiphilic copolymers poly(2-(methacryloyloxy) ethyl phosphorylcholine)-poly(2-(diisopropylamino) ethyl methacrylate) (PMPC-PDPA) into membranes is tuned using pH and temperature. We report evolution from disk micelles, to vesicles, to high-genus vesicles (vesicles with many holes), where each passage is controlled by pH switch or temperature. We show that the process can be rationalized, adapting membrane physics theories to disclose scaling principles that allow the estimation of minimal radius of vesiculation as well as chain entanglement and coupling. This approach allows us to generate nanoscale vesicles with genus from 0 to 70, which have been very elusive and difficult to control so far.

INTRODUCTION

Amphiphiles are molecules that contain both soluble and insoluble components with respect to a given solvent. In solution, the balance of the two counteracting interactions drives one of the most exquisite examples of self-assembly processes that give rise to supramolecularly defined nanostructures. These can be spherical or cylindrical micelles, or membranes, depending on the amphiphile packing factor, which in turn is defined by the insoluble-to-soluble molar ratio (Smart et al., 2008). For spherical micelles the geometry is defined by the molecular architecture, whereas for both cylinders and membranes, the curvature of the amphiphiles decides the formation of exposed ends or edges. These regions can be protected either by the assembly of a portion of amphiphiles into more frustrated and curved structures or by the structure closing on itself to avoid any hydrophobic exposure. For cylindrical micelles, these two scenarios corresponds to either worm-like or toroidal micelles, whereas for membranes, the two options are either disk-like micelles or closed vesicles (Smart et al., 2008). The latter are a very important structure as their geometry enables the enclosure of a given solvent volume whose composition is controlled by the same amphiphilic membrane. Assembly of natural amphiphiles such as phospholipids or their progenitors (Hanczyc et al., 2003) into vesicles provides the necessary compartmentalization to house the energy pools for feeding all biochemical processes (Szostak et al., 2001; Mann, 2013) making such a structure one of the most important element of life complexity.

It is not surprising that both natural and synthetic vesicles have been the subject of several studies. Beside the obvious biophysical drive to understand natural membranes, vesicles have been proposed as reactors and energy conversion units (Peters et al., 2012; Gaitzsch et al., 2015). Also, vesicles are one of most successful drug delivery systems as they mimic nature's way of carrying molecules, enabling the encapsulation of both soluble and insoluble drugs (Guan et al., 2015; Pattni et al., 2015; Al-Jamal and Kostarelos, 2011). Vesicles can be made using either natural or synthetic amphiphilic molecules. Among these, one of the most promising is based on the use of amphiphilic block copolymers wherein each soluble and insoluble component is macromolecular and consequently bestows the vesicles (known as polymersomes) with extra interactions arising from chain entanglement (Wang et al., 2012; Smart et al., 2008). Such a macromolecular nature allows to impart responsiveness (Li and Keller, 2009), to finely control the surface properties (Photos et al., 2003), to enhance both colloidal stability (LoPresti et al., 2009) and mechanical properties (Discher et al., 1999), as well as to augment tissue penetration (Pegoraro et al., 2013). The most common vesicle shape is spherical but tubular, prolate, discocytic, stomatocytic, toroidal, and pear-shaped vesicles have all been reported (Seifert and Lipowsky, 1995;

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Chang et al., 2014). Vesiculation is a process that strongly depends on the methods in which amphiphiles are placed in contact with water. We classify these methods as top-down and bottom-up approaches (Messenger et al., 2014). The top-down approach involves the hydration of a dry block copolymer film during which water diffusion and copolymer arrangements drive the formation of complex lyotropic liquid lamellar structures. These later break down into vesicles via unbinding of membrane-bound compartments. Such a process is complex, and its dynamics are strongly dependent on the molecular weight of the amphiphile (Battaglia and Ryan, 2006b). Moreover, the mixing of the highly viscous lamellar phase with water gives rise to finger-like instabilities, which result in the formation of tubular vesicles (Battaglia and Ryan, 2006a; Robertson et al., 2014). On the other hand, the formation of vesicles via the bottom-up approach starts with the amphiphile being fully solubilized and molecularly dispersed in solution. This can be achieved via solvent switch, tuning the amphiphile's assembly by gradually exchanging the organic solvent with water. Alternatively, the amphiphile's solubility can be controlled by pH, temperature, light, enzymatic reactions, or redox reactions (Che and van Hest, 2016; Hu et al., 2017; Liu et al., 2014; Deng et al., 2016). In all cases, the self-assembly evolves from molecularly dissolved amphiphiles to vesicles whose geometry is controlled by both thermodynamics and kinetics. This means that the final shape of the vesicle can be controlled by temperature and concentration as well as by the mixing rate. Small amphiphiles are characterized by relatively high critical assembly concentration (CAC) in water, and hence their assembly is characterized by a high exchange rate between unimers and the aggregate with consequent fast equilibration. Macromolecular amphiphiles, particularly those that assemble into membranes, have almost zero CAC, and hence once the unimer pool is depleted the assembly becomes kinetically trapped (Jain and Bates, 2003). Such a non-ergodic nature allows to access metastable phases, which are precluded for small amphiphiles. Eisenberg and colleagues noted this unique nature of polymersomes in their pioneering work (Gao et al., 1994; Zhang and Eisenberg, 1995) referring to the zoology of morphologies as crew-cut aggregates. Later on, they optimized the process controlling the final structure (Lim Soo and Eisenberg, 2004; Mai and Eisenberg, 2012) to the point that they were able to isolate complex vesicular structures. Using a similar approach, van Hest and colleagues demonstrated that the shape of polymersomes can be controlled from spherical to prolate, to disk, to stomatocytes (Meeuwissen et al., 2011; van Oers et al., 2013; Rikken et al., 2016); more recently, similar experiments were reported by Wong et al. adding extra control using aromatic groups (Wong et al., 2017). We reported a different approach using pH-sensitive poly(2-(methacryloyloxy)ethyl phosphorylcholine)-poly(2-(diisopropylamino)ethyl methacrylate) (PMPC-PDPA) (Pearson et al., 2013). Here we have shown that the PMPC-PDPA assembles into either micellar or vesicular structures depending on the kinetics of pH or temperature changes. We expanded on this study showing via a combination of different techniques that the kinetics of assembly can be controlled by either temperature or pH changes and that this allows to tune both the vesicle closing morphology and its topology.

RESULTS AND DISCUSSION

pH-Driven Self-Assembly

The chemical structures of PMPC-PDPA copolymers are shown alongside the corresponding molecular models with the DPA groups protonated (Figure 1A) and deprotonated (Figure 1B). The models were calculated minimizing the PMPC₂₅-PDPA₇₀ using Merck molecular force field molecular mechanics in Avogadro (Hanwell et al., 2012) (final structure rendered in Chimera [Pettersen et al., 2004]). PMPC and PDPA chains were minimized separately and joined together after calculation. No constraints were imposed on the PMPC and protonated PDPA chains, and we imposed an end-to-end distance $d_{AA} \propto N^{2/3}$ on the deprotonated PDPA, in agreement with the scaling reported for block copolymer micelles and membranes (Battaglia and Ryan, 2005; Jain and Bates, 2003). The displayed models show the PMPC-PDPA's charge distribution and molecular size. The PDPA chain is fully soluble when protonated, whereas it is hydrophobic when deprotonated, which drives its self-assembly (Lomas et al., 2007; Pearson et al., 2013). This process is strongly dependent on the pH switch rate, as shown in Figure S1A wherein the pH change is plotted as a function of time for different flow rates of NaOH solution titration. The pH rises exponentially with time until it reaches the PDPA pK_a , which under experimental conditions (PBS 100 mM and $T = 25^\circ\text{C}$) is 6.8. The pH stabilizes for the time necessary to complete the reaction between the protonated PDPA and the hydroxyl ions in solution to form deprotonated and hydrophobic PDPA. After all the chains are deprotonated, the pH again rises exponentially with time. The graph in Figure S1B shows that the time plateau is proportional to the flow rate and changes from a few minutes to hours. In Figures S1D–S1H we show the corresponding transmission electron microscopic (TEM) images of the samples formed at different flow rates. The final

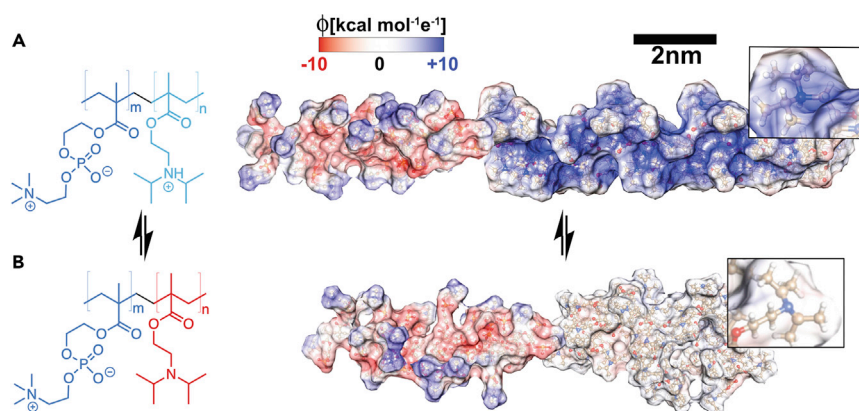


Figure 1. Chemical Structure and Molecular Model of the PMPC-PDPA Copolymers

(A and B) The copolymers are shown with the tertiary amine group protonated (A) and deprotonated (B). Note that the molecular models were calculated for PMPC₂₅-PDPA₇₂ and the structures are represented with their solvent-accessible surface (probe distance 1.4 Å) colored as a function of the molecule electrostatic potential calculated as $\phi(r) = \sum q_i/\epsilon r_i$ with $\epsilon = 4r$ being the dielectric, representing screening by the water.

morphology changes with the flow rate indicating that it is possible to modulate the formation of different architectures.

Upon more detailed inspection using cryogenic TEM imaging of the vitrified sample produced by slower rate, we observed that PMPC-PDPA assembles into a large variety of architectures, which are shown in the micrographs in Figures 2A and 2B at low and high magnification, respectively. Two populations of structures are visible, one is made of discoid micelles and the other is made of vesicles. The latter have different shapes and in some the membranes are not completely closed. We recently developed a method to separate soft particles by using density gradient fractionation (Robertson et al., 2016) and applied it to PMPC-PDPA structures made by slowest rate. At water density between 0.998 and 1.018 g cm⁻³ (as shown in the TEM image in Figure 2C), we mostly found micelles with radius varying from 10 to 20 nm. At densities between 1.018 and 1.038 g cm⁻³, the radius increases from 30 to 60 nm and the aggregates are mostly composed of spherical vesicles (Figure 2D). At higher density between 1.038 and 1.081 g cm⁻³ the sample is dominated by larger (radius from 60 to 200 nm) flattened and holed vesicles (Figure 2E). These latter structures can be described using the mathematical terminology of genus, i.e., the number of holes or handles of the vesicle (Seifert and Lipowsky, 1995), which varies from 0 for the spherical geometry to 1 for the torus to >1 for vesicles hereafter referred to as high-genus vesicles.

To further elucidate the kinetics of pH switch, we studied the self-assembly of PMPC₂₅-PDPA₇₀ copolymers using stop-flow absorbance measurements following the initial 10 s of assembly at different degrees of copolymer ionization, $\alpha = (1 + 10^{(pH-pK_a)})^{-1}$. This depends on the final solution pH and for pH = pK_a, the ionization degree $\alpha = 0.5$. For any value below this, the PDPA has not sufficient charges to remain soluble and becomes hydrophobic. As shown in Figure 2F, by normalizing the absorbance as a function of time, self-assembly occurs via two steps and can be fitted by a double exponential growth as in:

$$\frac{A}{A_{\max}} = 1 - \left(\sigma e^{-\frac{t}{\tau_1}} + (1 - \sigma) e^{-\frac{t}{\tau_2}} \right) \quad (\text{Equation 1})$$

In Figure 2G, we plotted Equation 3 parameters as a function of the ionization degree showing that the first fast relaxation time, τ_1 varies from 750 to 100 ms depending on the ionization degree, whereas the second slower relaxation time τ_2 increases slightly with the ionization degree. The relative ratio between the two processes, expressed here as σ , also changes with the ionization degree and the fast dynamics dominates with $\sigma > 0.7$ for $\alpha < 0.1$; the more the copolymer is charged, the more the two steps are balanced. This suggests that as $\alpha \rightarrow 0.5$, the unimer concentration increases.

Temperature-Driven Self-Assembly

As we previously reported (Pearson et al., 2013), the PDPA pK_a varies with temperature being about 7.5 at 5°C and going down to 5.5 at 60°C. This means that PMPC-PDPA self-assembly can be tuned by

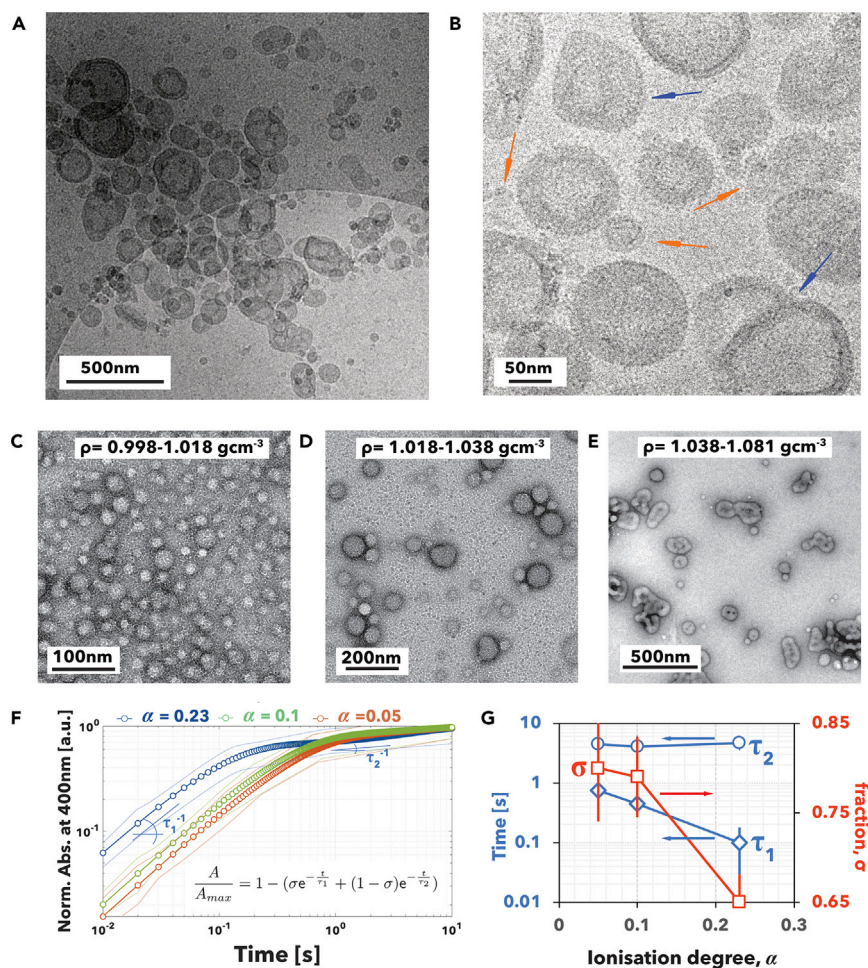


Figure 2. pH-Driven Assembly of PMPC₂₅-PDPA₇₀ Copolymers

(A–E) Low- (A) and high- (B) magnification cryogenic TEM images of PMPC₂₅-PDPA₇₀ assemblies produced at $0.5\ \mu\text{mol min}^{-1}$ of NaOH solution addition. The red arrows point to disk micelles and the blue ones to high-genus vesicles. TEM images of the sample corresponding to density $0.998\text{--}1.018\text{ gcm}^{-3}$ (C), $1.018\text{--}1.038\text{ gcm}^{-3}$ (D), and $1.038\text{--}1.081\text{ gcm}^{-3}$ (E). (F and G) Kinetics curves measured by stop-flow absorbance of PMPC₂₅-PDPA₇₀ copolymer at different ionization degrees (F) and the corresponding parameters (G) obtained using Equation 3.

temperature changes, as shown in Figure 3; we dissolved the copolymers at pH = 2, cooled the solution down to 5°C , and increased the pH to 7 triggering the formation of micelles and vesicles by heating. In Figure 3A, the dynamic light scattering (DLS) of a PMPC₂₅-PDPA₇₀ dispersion confirms that the copolymer is molecularly dispersed at pH = 7 and $T = 5^\circ\text{C}$, and as we raise the temperature it self-assembles. As shown by both DLS and TEM (Figures 3B and 3C), the final structure architecture depends on the heating rate with fast rate leading to small micellar structures, whereas slow rate leading to vesicles. Such temperature sensitivity allowed us to monitor self-assembly using proton nuclear magnetic resonance (NMR) spectroscopy following chemical shift of the copolymers' hydrogens. The resulting spectra in Figure S2A show the evolution of PMPC-PDPA proton intensity as a function of the solution temperature when dispersed at pH = 2. The NMR spectra were collected every 5 min while the temperature was increased from 5°C to 40°C at a rate of 0.2°C per minute. The spectra show no changes in the proton signal. In Figure 3D, the plot of normalized intensity of peak 1 and peaks 7–9 as a function of temperature confirms that no changes are detectable. This confirms that the PDPA is fully protonated and the copolymers are dissolved molecularly with all protons allowed to interact with the solvent (Figure 3F). However, when the solution pH is increased to 7, the NMR spectra show a decrease in several peaks. For heating rate 1°C per minute, all the PDPA peaks decrease in intensity (Figure S2B) suggesting that the protons stop interacting with water and the PDPA tertiary amines are deprotonated. The PMPC peaks, on the other hand, seem to be unaltered,

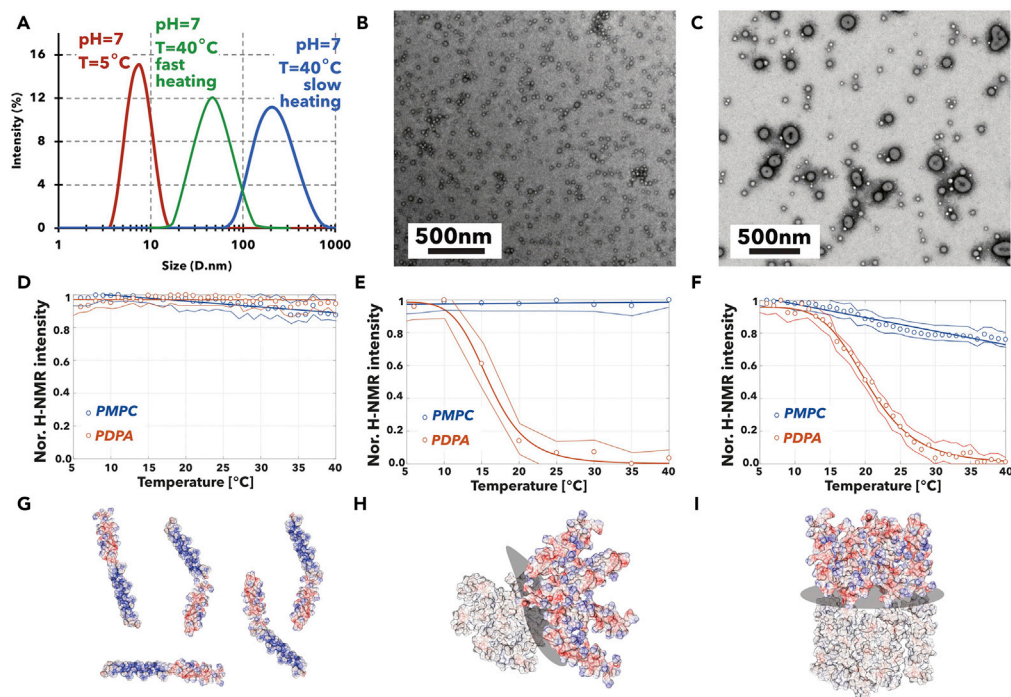


Figure 3. PMPC₂₅-PDPA₇₀ Self-Assembly Tuned by Temperature Change

(A–F) Particle size distribution measured by dynamic light scattering (DLS) of PMPC₂₅-PDPA₇₀ polymersome dispersion at pH = 7 and at T = 5 °C and 40 °C fast and slow heating (A). Corresponding TEM images of PMPC₂₅-PDPA₇₀ polymersomes formed by fast (B) and slow (C) heating. NMR titration peaks 1 and 7–9 normalized intensity as a function of the temperature and corresponding model of PMPC₂₅-PDPA₇₀ dispersion during slow heating at pH = 2 (D) and fast (E) and slow (F) heating at pH = 7. (G–I) Schematics show the corresponding arrangements of the PMPC-PDPA copolymers under the different conditions. Images were generated using the minimized structures shown in Figure 1 packed to form either planar or curved arrangements.

suggesting that the corresponding protons interact with the solvent in the same way as the unimers (Figure 3E). The normalized intensity of peaks 1 and 7–9 is plotted as a function of the temperature in Figure 3G and shows that the PDPA peaks decrease, whereas the PMPC peak 1 remains unchanged. This suggests an assembly structure with a fully deprotonated PDPA shielded into a hydrophobic core, whereas the PMPC chain remains in close contact with water and hence forms a curved structure that agrees with the micelles observed by TEM and shown in Figure 3H. Finally, for slower heating rate of 0.2 °C per minute, the NMR spectra collected as a function of the temperature (Figure S2C) show a similar decrease in most PDPA peaks as well as a decrease in most PMPC peaks. Such an effect is more visible in Figure 3J where peaks 7–9 decrease to almost zero and peak 1 decreases to about 75% of its starting value. Such a decrease suggests that most PMPC chains have a more packed configuration in agreement with the vesicular structure observed by TEM, as showed by the cartoon in Figure 3K. It is important to point out that the PDPA deprotonation process in D₂O used for the NMR experiments is slightly different, and indeed the transition temperature is a few degrees lower compared with our previous observations (Pearson et al., 2013). However, the scope of these experiments is to shed light on the molecular-level changes during the self-assembly and hence the shift in transition is irrelevant.

As shown in Figure 4A, the temperature-driven self-assembly, unlike the pH-driven one, is not reversible. Monitoring the solution turbidity by measuring the absorbance at 400 nm we noticed that whereas the copolymers assemble into dispersed phases going from 5 °C to 60 °C, with transition temperature depending on their molecular mass, the assemblies do not dissolve into unimers as the solution is cooled back to 5 °C. The low-molecular-mass PMPC₆-PDPA₁₂ shows a hysteresis of about 8 °C and the absorbance does not go down to zero at 5 °C. As the molecular mass increases, PMPC₁₂-PDPA₃₅ displays even more hysteresis, whereas PMPC₂₅-PDPA₇₀ shows no sign of disassembly upon cooling. Upon inspection by TEM (Figure 4B), we observed that PMPC₂₅-PDPA₇₀ assemble into vesicles and micelles upon heating but the morphology of

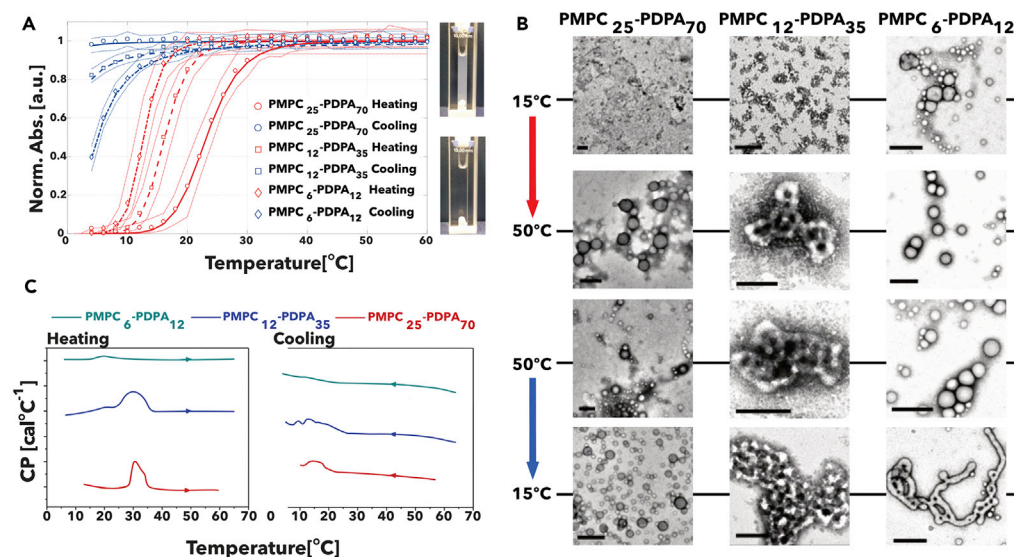


Figure 4. Temperature-Driven Self-Assembly of PMPC-PDPA Copolymer at Different Molecular Weight

(A–C) Turbidity measurement using UV/Vis absorbance at 400 nm of PMPC₂₅-PDPA₇₀, PMPC₁₂-PDPA₃₅, and PMPC₆-PDPA₁₂ solution during heating (red curves) and cooling (blue curves) starting from 5°C to 60°C; a photograph of the cuvette before and after heating is shown (A). TEM images of PMPC₂₅-PDPA₇₀, PMPC₁₂-PDPA₃₅, and PMPC₆-PDPA₁₂ structures formed during heating and after cooling. Scale bar, 200 nm (B). Micro-differential scanning calorimetry of PMPC₂₅-PDPA₇₀, PMPC₁₂-PDPA₃₅, and PMPC₆-PDPA₁₂ dispersion showing the heat exchange during heating and cooling (C).

these appear unchanged upon cooling. Both PMPC₁₂-PDPA₃₅ and PMPC₆-PDPA₁₂ also assemble into vesicles and micelles upon heating, but as their solutions are cooled down the number of vesicles increases and so does their genus number. To further understand such a hysteresis in the self-assembly behavior, we performed micro-differential scanning calorimetry for the three different PMPC-PDPA copolymers, and both the heating and cooling curves are shown in Figure 4C. All the investigated copolymers showed a thermal transition starting around 20°C to 30°C indicating that PMPC-PDPA self-assembly in water is an endothermic process. We can confidently attribute such an endothermic process to the de-protonation reaction of the PDPA with water. If we compare the pH- and temperature-driven process, in the former the acid-base reaction is mostly controlled by the presence of hydrogen and hydroxyl ions in solution, whereas in the latter the concentration of these is minimal (pH = 7) and the only changing parameter is the copolymer pK_a. The thermograms show that the endothermic peak is not mirrored by an exothermic one during the reverse cooling cycle. We instead observed a shoulder typical of glass transitions indicating that the PDPA becomes an amorphous glass below 20°C. This suggests that the PDPA membrane freezes and becomes less permeable to water hence slowing down or even stopping altogether the water diffusion with consequent arrest of the copolymer disassembly.

Disk Micelles

The two structures, disk micelles and vesicles formed both during pH- or temperature-driven assembly, are indeed quite unique and warrant further analysis. In Figure 5A we show two high-resolution cryogenic TEM images in grayscale and the fire palette of PMPC₂₅-PDPA₇₀ disk micelles. The PMPC chains were selectively stained by phosphotungstic acid before vitrification. The disk micelles are small and show highly curved edges with a few copolymers in the middle. We measured both the disk radius and membrane thickness for several PMPC-PDPA copolymers and plotted these as a function of the degree of polymerization of PDPA (Figure 5B). A given polymer chain has end-to-end distance scaling with its degree of polymerization according to the power law, $d \propto N^\nu$, where when the chains are stretched $1 \geq \nu \geq 3/5$, when unperturbed (also random coil) $\nu \sim 3/5$, and when hyper-coiled $\nu \leq 3/5$ (de Gennes, 1979; Battaglia and Ryan, 2005). Assuming that the PDPA chain extends as long as the disk radius or thickness, we can assess the hydrophobic chain configuration in both types of assembly. We and others reported that polymersome membranes are typically associated with a scaling exponent of 2/3

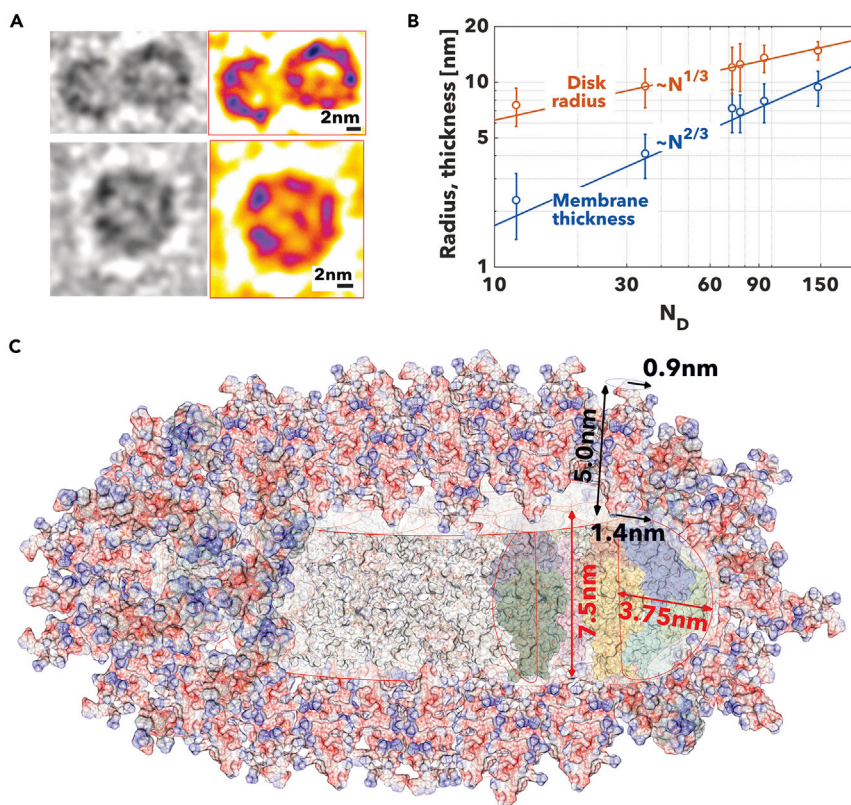


Figure 5. Disk Micelles

(A and B) High-resolution cryogenic TEM with pre-stained samples of PMPC₂₅-PDPA₇₀ disk micelles shown in gray and fire palette (A). Scaling graph between the disk radius (red) and membrane thickness (blue) and PDPA degree of polymerization (B).

(C) Schematics of the PMPC-PDPA disk shown in scale using the minimised copolymer structures shown in Figure 1.

corresponding to super-segregated copolymers (Jain and Bates, 2004; Battaglia and Ryan, 2005; Pearson et al., 2013). As shown in the graph in Figure 5B, we confirm the same trend for PMPC-PDPA membranes, whereas for the disk radius the power law scales with an exponent of 1/3. This suggests a hyper-coiled configuration indicating that the interfacial energy associated with the free edges is sufficiently strong to compress the chains. Using this scaling analysis together with NMR, the density data, and the structures observed in cryogenic TEM images in Figure 5A, we conclude that the micelles are discoid with a core made of copolymers assembling into a configuration as dense as the vesicle membrane with curved edges that shield the hydrophobic chains from water. Such a structure is shown in Figure 5C where we used the minimized PMPC-PDPA copolymers to reconstruct the final geometry. As PMPC₂₅-PDPA₇₀ forms a membrane of about 7.51 nm we can assume that to stabilize the edge, few copolymers form a semi-cylindrical region with a radius of half the membrane thickness (i.e., 3.75 nm). Such a configuration is naturally frustrated, and it can only be formed when there are not enough chains to form the vesicles as all the unimers have been depleted from the solution.

High-Genus Vesicles

For both pH- and temperature-driven assemblies, the vesicles form with different topology and different genus numbers. We hypothesize that as disk micelles close into spherical ($g = 0$) vesicles their interior becomes inaccessible to unimers. These thus insert only onto the exterior leaflet of the vesicle membrane leading to an asymmetric growth, which in turn leads to an increase in the vesicle genus. To prove this hypothesis, we exploit the self-assembly hysteresis with the temperature, which allows the co-existence of both unimers and vesicles at low temperature. We thus dissolved PMPC-PDPA at pH = 2, cooled down the solution to 5°C, and finally raised the pH to 7. We mixed such a unimer solution with PMPC-PDPA spherical vesicles, made using film hydration, which we established produces only $g = 0$ vesicles (Robertson

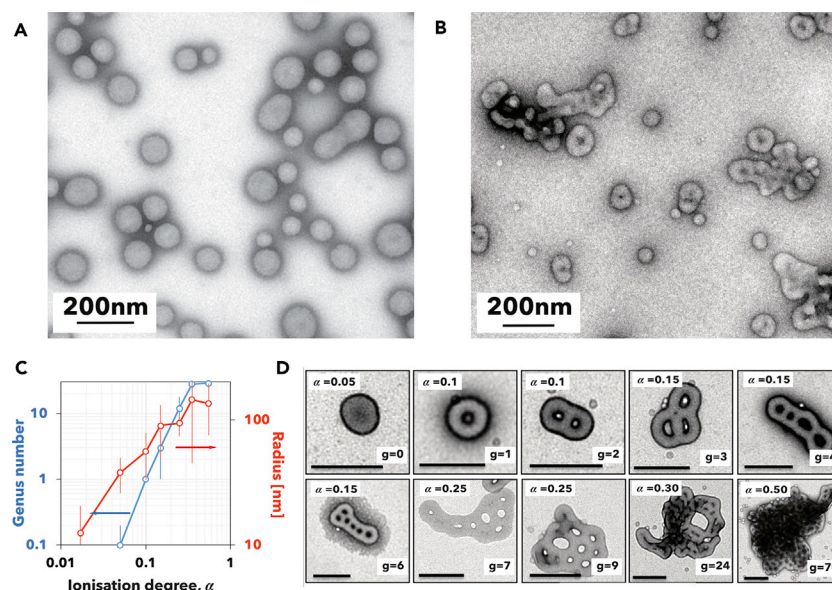


Figure 6. High-Genus Structure

(A–D) TEM images of PMPC₂₅-PDPA₇₀ polymersomes prepared by film hydration (A) and after mixing with unimers at 5°C at 1:1 ratio (B). Graph showing the genus number (blue) and average radius (red) as function of the PMPC₂₅-PDPA₇₀ ionization degree (C). TEM images of PMPC₂₅-PDPA₇₀ polymersomes with different genus numbers and formed with different ionization degrees (D).

et al., 2014) keeping the temperature at 5°C. The TEM image in Figure 6A shows the polymersomes before mixing at 5°C, confirming that they retain their structure, whereas the micrograph in Figure 6B shows the structure after 30 min of mixing the vesicle with unimer as stated above. The resulting structures are vesicles with an altered topology and higher genus number, confirming our initial hypothesis.

A similar condition of co-existence of vesicles and unimer is achieved at pH values close to the pK_a , i.e., $\alpha > 0$. We thus performed a series of experiments dissolving PMPC₂₅-PDPA₇₀ at pH = 2 and raising the pH to different values modulating its ionization degree. The graph in Figure 6C shows both the average vesicle genus number (in blue) and the radius (in red) as a function of α . It is evident that both increase with PDPA ionization degree, confirming that the longer the vesicles are allowed to grow, the higher their genus number becomes. In Figure 6D, we show the relative TEM images for the different ionization degrees further confirming the asymmetrical growth hypothesis and, moreover, demonstrating the remarkable ability to form structures with genus as high as $g = 70$ at pH = pK_a where $\alpha = 0.5$.

Proposed Mechanism and Theoretical Considerations

Based on the data discussed above, we can conclude that both pH- and temperature-driven self-assemblies occur according to the cartoon proposed in Figure 7. As we measured in Figure 2G, we can confidently assume that the kinetics of self-assembly occurs according to two regimes, and using the model proposed by Liguore et al. (Liguore and Leibler, 1990), we can estimate that this occurs with a first fast nucleation time,

$$\tau_1 = \tau_N \approx \frac{a^2}{D\phi_u^2} \quad (\text{Equation 2})$$

where a is the Kuhn statistical length of the unimer, D is the copolymer diffusion coefficient in water as unimer, and ϕ_u is the copolymer unimer volume fraction. As shown in Figure 2G, τ_N decreases with the increase of charges on the PDPA chains, which, assuming the diffusion coefficient is unvaried, confirms that with higher α the unimer concentration ϕ_u increases. The fast nucleation is followed by a much slower regime dominated by the activation barrier of the unimer to insert in the pre-formed assembly. Indeed, the unimer needs to diffuse through the PMPC brush and insert the PDPA chains into the preformed membrane. We adapt the Liguore-Leibler model (Liguore and Leibler, 1990), to estimate the construction time,

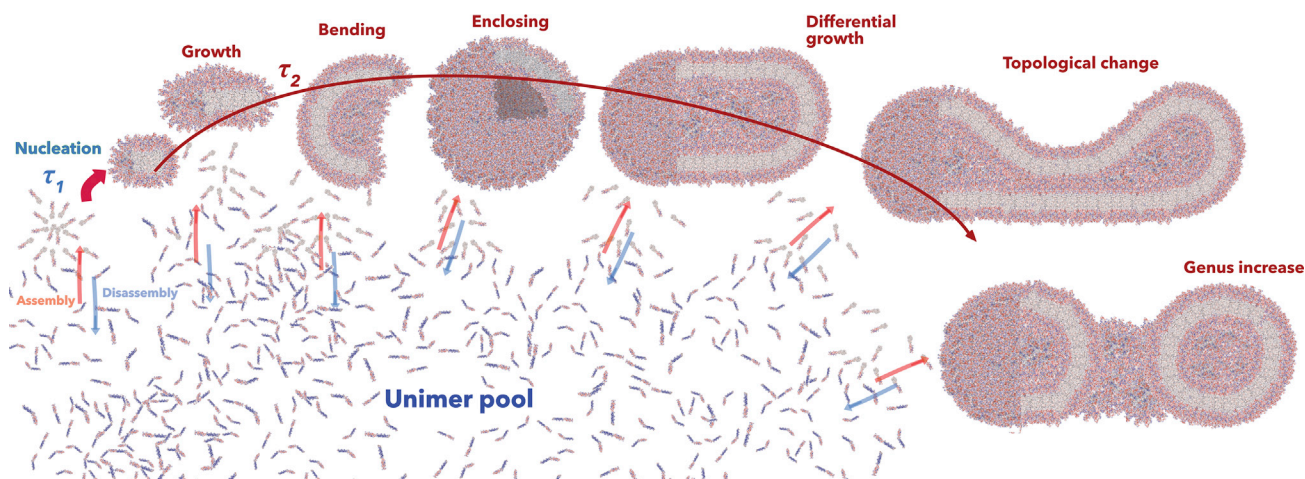


Figure 7. Proposed Mechanism of Polymersome Formation and Topological Changes.

The blue and red arrow represent assembly and disassembly processes.

$$\tau_2 = \tau_C \sim \frac{1}{a_0} (N_M + \alpha N_D) e^{\frac{\Delta G_i}{kT}} \quad (\text{Equation 3})$$

where N_M and N_D are the polymerization degree of the PMPC and PDPA blocks, ΔG_i is the free energy gain of the hydrophobic PDPA chain to insert in the membrane, k is the Boltzmann constant, and T is the temperature. From Figure 5A, we can write that the membrane thickness is $t = aN_D^{2/3}$, and we calculate for the PDPA that the Khun length $a = 0.367$ nm. Thus, we can derive the area per molecule of the copolymers in the assembly a_0 calculated as

$$a_0 = \frac{M_D N_D^{1/3}}{N_A \rho_P p a} \quad (\text{Equation 4})$$

where M_D is the DPA monomer molecular mass, N_A is the Avogadro number, ρ_P is the PDPA density, and p is the packing factor, which for membranes is $p \in [0.5, 1]$. τ_C is considerably slower than the nucleation time, and we measured it to increase linearly from 4.5 to 6 s together with α . Both times are also in strong agreement with previous studies that used rapid mixing techniques (Johnson and Prud'homme, 2003). In the graph in Figure 2G, we also calculated the relative fraction of the two different processes, σ , as a function of the ionization degree. This increases when the copolymer nucleation dominates the kinetics of the process, suggesting that at this stage the copolymers do not have enough time to perform insertion events to allow the disk micelles growing into vesicles.

This is very much confirmed by DLS in Figure 3A, TEM in Figures 2A and 3B, and NMR in Figures 3G and 3H, which show that the fast kinetics lead to a large number of disk micelles. NMR and cryogenic TEM image (Figure 5A) showed that these have highly curved interface with the PDPA core forming the corresponding membrane in the disk center but hyper-coiling at the edge as demonstrated by our scaling analysis in Figure 5B, which constructs a very accurate molecular model of its structure. As shown in Figure 7, provided the unimer pool is not depleted, these insert into the disk making them grow, and when these reach a critical radius (about 15 nm), the membrane starts bending and enclosing. The Hamiltonian associated with such a process is the sum of three components:

$$H = H_H + H_{ADE} + H_{edge} = \int [2\kappa_M(M - c_0)^2 + \kappa_G G] dA + \frac{k_m a N_D^{5/3} M_D}{8 N_A p} \int_A (\Delta N^\pm)^2 + \frac{3 N_A k T p a^2 N_D^{2/3}}{8 M_D} \int_L dL \quad (\text{Equation 5})$$

The first term H_H is the membrane bending energy of Helfrich's elastic energy with A being the total surface area, κ_M and κ_G the bending and the Gaussian moduli, and $M = 0.5(c_1 + c_2)$, $G = (c_1 c_2)$, and c_0 being the mean, Gaussian and spontaneous curvatures of a surface characterized by $c_1 = R_1^{-1}$ and $c_2 = R_2^{-1}$ curvatures. The second term H_{ADE} is the area-difference-elasticity and includes the energy contribution arising from the differential stretching and compression of the two membrane monolayers, and it depends on the

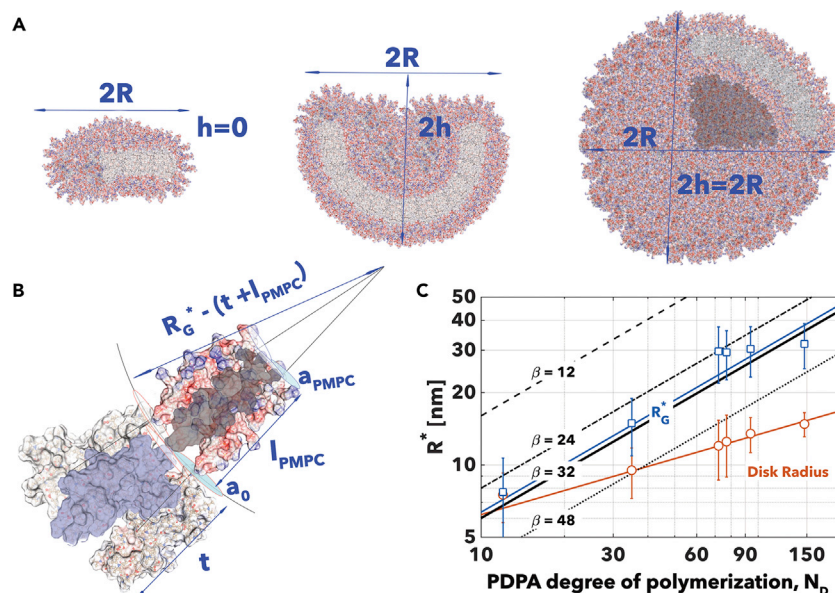


Figure 8. Transition from Disk to Closed Vesicle

(A–C) Geometry of the transition (A). Detail of three PMPC₂₅-PDPA₇₀ copolymers packed to give the highest density possible with PMPC chains (B). The elastic minimum radius of vesiculation R_E^* calculated from Equation 3 with $\beta = 12, 24, 32,$ and 48 (black lines); the geometrical minimal radius calculated using Equation 3 R_G^* (blue line) and from the experimental data (blue square); as well as the disk radius all plotted as a function of the PDPA polymerization degree N_D (C).

membrane compression modulus k_m and the difference in copolymer numbers between the outer (+) and inner (–) layers of the membrane, $\Delta N^\pm = N^+ - N^-$. Finally, the last term H_{edge} is associated with edge effect, and, as shown by the conformation of the copolymers in the disk edge (Figure 5C), we can attribute it to the entropic compression of the PDPA chain from the equilibrium end-to-end distance, i.e., the membrane thickness, t , to the radius of the disk edge, $t/2$.

Equation 3 can be used to analyze the experimental data observed above and rationalize them in thermodynamic terms. The first transition from the disks arising from the initial fast nucleation to closed vesicle is shown in Figure 8A where the disk is characterized by its radius, R , and height $h \in [0, R]$. This is the height of the spherical cap forming from the disk bending, and it allows to measure the vesiculation as $h = 0$ for the planar disk and $h = R$ for the fully closed vesicle. The very first observation is that the disk curves to limit the length of the edges with consequent membrane deformation. The spontaneous curvature, c_0 , includes molecular aspects that impose a geometrical curvature, and when only one amphiphile is considered as in our case, they can be ignored. The area-difference-elasticity H_{ADE} term can also be ignored as long as the disk inner and outer membrane layers are equally accessible by unimers and hence $\Delta N^\pm \sim 0$. For most phospholipids $\kappa_G \approx -\kappa_M$ (Huang et al., 2017), and we assume here the same for PMPC-PDPA copolymer to simplify our calculations. Finally, we define $\kappa_M = K_A a^2 N_D^{4/3} \beta^{-1}$ as a function of the K_A , the area elastic modulus, which we measured for PMPC-PDPA polymersomes using atomic force microscopy (Battaglia et al., 2011), and it is invariant with the degree of polymerization (Bermudez et al., 2002). The term β is a constant that depends on the lateral pressure distribution across the membranes (Bloom et al., 1991). When the two monolayers are coupled, the repulsion can be concentrated at the interfaces, $\beta = 4$, or distributes uniformly across the membranes, $\beta = 12$. Uncoupled membranes have larger β close to the limit because the monolayers are free to slide on each other, $\beta = 48$. We can now integrate Equation 3 for the disk geometry in Figure 8A to give:

$$H(R, h) = \frac{4\pi K_A a^2 N_D^{4/3} h^2}{\beta R^2} + \frac{3N_A k T p a^2 N_D^{2/3}}{8M_D} \sqrt{R^2 - h^2} \quad (\text{Equation 6})$$

The two extreme configurations are the flat disk, i.e., $h = 0$, where Equation 3 evolves into

$$H_{\text{Disk}} = \frac{3N_A k T p a^2 N_D^{2/3}}{8M_D} R \quad (\text{Equation 7})$$

and the closed vesicle with $h = R$ where Equation 3 evolves into

$$H_{\text{Vesicle}} = \frac{4\pi K_A a^2 N_D^{4/3}}{\beta} \quad (\text{Equation 8})$$

Only for the disk radius, R , where $H_{\text{Edge}} > H_H$, i.e., for R where $H_{\text{Disk}} > H_{\text{Vesicle}}$ vesiculation occurs spontaneously, and we thus define the elastic minimum radius of vesiculation, R_E^* , as:

$$R_E^* = \frac{8M_D K_A N_D^{2/3}}{3\beta N_A p k T} \quad (\text{Equation 9})$$

In addition to this, it is important to note that the vesiculation is also limited by the amphiphile size. For amphiphilic copolymer, the hydrophilic PMPC chains are forced together within the vesicle inner leaflet. Such Using simple geometrical considerations, as shown in Figure 8B, we can thus identify a minimum geometrical radius R_G^* as:

$$R_G^* = l_M \frac{2r - r_M}{r - r_M} + a N_D^{2/3} \quad (\text{Equation 10})$$

where $r \in [r_D, \sqrt{a_0/\pi}]$, l_M is the length of the PMPC chain, and r_M and r_D are the van der Waals radii of the two monomers, which can be measured using the model in Figure 1. This is a pure molecular limit and indeed depends on the amphiphile architecture. In Figure 8C, we plot the minimum geometrical radius R_G^* , the experimentally measured average disk radius, and different R_E^* for different β . We can conclude that $\beta > 32$ will be physically impossible for the PMPC chains to withstand. This suggests that there is some level of coupling between the two membrane leaflets and that this is in agreement with the polymersome membrane entanglement dictated by its macromolecular nature (Battaglia and Ryan, 2005; Bermudez et al., 2004). Finally, the proposed model shows again that the disks observed for fast nucleations have radius below the geometrical minimum and indeed can only be explained as disk micelles.

Most spherical vesicles have a Hamiltonian as in the Equation 3 with $H_{\text{edge}} = 0$. However, when the vesicles remain in contact with unimers and these cannot penetrate the membrane causing a larger growth of the outer layer than the inner one, we need to include the area-difference-elasticity H_{ADE} as well as break down the Helfrich elasticity in mean and Gaussian curvature as the latter is a topological invariant. According to the Gauss-Bonnet theorem, $\oint G dA = 4\pi(1 - g)$ where g is the genus number; we can thus write:

$$H_{\text{Vesicle}} = \frac{K_A a^2 N_D^{4/3}}{2\beta} (\phi M dA + 4\pi(1 - g)) + \frac{k_m a N_D^{5/3} M_D}{8N_A p \phi dA} (\Delta N^\pm)^2 \quad (\text{Equation 11})$$

Equation 3 is very difficult to minimize, and for $g > 1$ a conformational degeneracy is often found in the ground state with consequent multiple solutions (Seifert, 1991). However, so far the theory has been applied to explain observed structures in vesicles with radius much larger than the membrane thickness using optical microscopy with several structures reported including vesicles with high genus (Noguchi, 2015). High-genus vesicles so far have been reported for micrometer-sized vesicles with radius considerable larger than the membrane thickness (Haluska et al., 2002; Noguchi et al., 2015; Ichirou Akashi and Miyata, 2010) and to the best of our knowledge no example of nanoscale high-genus vesicles have been reported. Here we show that by exposing spherical vesicles to membrane-forming unimers, their topology can be considerably altered increasing the vesicle genus number. As shown in Figure 6, we can indeed control the genus by allowing longer times of contact between vesicles and unimers, in other words, by growing the outer layer and hence the term ΔN^\pm . Our data are in strong agreement with the simulations reported by Noguchi where an increase in genus number corresponds with an increase of area difference or ΔN^\pm (Noguchi, 2015). Most importantly, our data propose a very first approach to engineer the vesicle topology and indeed access structures that so far have been very elusive.

Conclusions

One of the most used top-down techniques of polymeric assembly formation is the hydration of dry polymer film with water. This mechanism often requires from days to weeks to obtain a dispersed polymersome sample. Faster approaches such as environmentally driven self-assembly, which use solvent or pH switch, are commonly exploited to accelerate the process. In this study, we have shown that the pH-responsive

amphiphilic diblock copolymers PMPC-PDPA are capable of forming a range of colloidal assemblies in water via simple temperature change. This is achieved by slowly changing the temperature of the dispersion therefore modulating the DPA pKa. This novel approach allows homogeneous control of the temperature, and consequently, assembly formation within the solution, opening new mechanisms for the formation of PMPC-PDPA assemblies with different morphologies. We also demonstrate good control over the hydrodynamic diameter and the number of genus events occurring per particle by modulating the degree of copolymer ionization. The ability to generate such a range of structures in aqueous solution from a single copolymer creates exciting new avenues for exploration and extends our understanding of the formation of complex curvatures adopted by copolymers in high-genus assemblies.

METHODS

All methods can be found in the accompanying [Transparent Methods supplemental file](#).

SUPPLEMENTAL INFORMATION

Supplemental Information includes Transparent Methods and two figures and can be found with this article online at <https://doi.org/10.1016/j.isci.2018.08.018>.

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AUTHOR CONTRIBUTIONS

C.C. and J.G. synthesized the copolymers. C.C., R.P., L.W., and L.M. performed the UV/Vis spectroscopic measurements and DLS. C.C., R.P., L.W., and L.M. performed the TEM analysis. L.R. developed and optimized the polymersome purification by density gradient. L.W. produced the titration curves at different flow rates. C.C. performed the DSC measurement. R.P. performed the stop-flow measurements. J.G. performed the NMR spectroscopy titrations. L.R.-P. analyzed the samples by cryo-TEM. G.B. produced the theoretical calculations and also designed and simulated all the molecular models. All authors wrote the manuscript.

DECLARATION OF INTERESTS

G.B. is a founder of SomaNautix Ltd. and a member of its scientific advisory board. The other authors declare no competing interests.

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REFERENCES

- Al-Jamal, W., and Kostarelos, K. (2011). Liposomes: from a clinically established drug delivery system to a nanoparticle platform for theranostic nanomedicine. *Acc. Chem. Res.* **44**, 1094–1104.
- Battaglia, G., LoPresti, C., Massignani, M., Warren, N.J., Madsen, J., Forster, S., Vasilev, C., Hobbs, J.K., Armes, S.P., Chirasatitsin, S., and Engler, A.J. (2011). Wet nanoscale imaging and testing of polymersomes. *Small* **7**, 2010–2015.
- Battaglia, G., and Ryan, A.J. (2005). Bilayers and interdigitated in block copolymer vesicles. *J. Amer. Chem. Soc.* **127**, 8757–8764.
- Battaglia, G., and Ryan, A.J. (2006a). Neuron-like tubular membranes made of diblock copolymer amphiphiles. *Angew. Chem. Int. Ed.* **45**, 2052–2056.
- Battaglia, G., and Ryan, A.J. (2006b). Pathways of polymeric vesicle formation. *J. Phys. Chem. B* **110**, 10272–10279.
- Bermudez, H., Brannan, A.K., Hammer, D.A., Bates, F.S., and Discher, D.E. (2002). Molecular weight dependence of polymersome membrane structure, elasticity, and stability. *Macromolecules* **35**, 8203–8208.
- Bermudez, H., Hammer, D., and Discher, D. (2004). Effect of bilayer thickness on membrane bending rigidity. *Langmuir* **20**, 540–543.
- Bloom, M., Evans, E., and Mouritsen, O.G. (1991). Physical properties of the fluid lipid-bilayer component of cell membranes: a perspective. *Q. Rev. Biophys.* **24**, 293–397.
- Chang, H.-Y., Sheng, Y.-J., and Tsao, H.-K. (2014). Structural and mechanical characteristics of polymersomes. *Soft Matter* **10**, 6373–6381.
- Che, H., and van Hest, J.C. (2016). Stimuli-responsive polymersomes and nanoreactors. *J. Mater. Chem. B* **4**, 4632–4647.

- de Gennes, P.-G. (1979). *Scaling Concepts in Polymer Physics* (Cornell University Press).
- Deng, Z., Qian, Y., Yu, Y., Liu, G., Hu, J., Zhang, G., and Liu, S. (2016). Engineering intracellular delivery nanocarriers and nanoreactors from oxidation-responsive polymersomes via synchronized bilayer cross-linking and permeabilizing inside live cells. *J. Am. Chem. Soc.* **138**, 10452–10466.
- Discher, B.M., Won, Y.-Y., Ege, D.S., Lee, J.C.-M., Bates, F.S., Discher, D.E., and Hammer, D.A. (1999). Polymersomes: tough vesicles made from diblock copolymers. *Science* **284**, 1143–1146.
- Gaitzsch, J., Huang, X., and Voit, B. (2015). Engineering functional polymer capsules toward smart nanoreactors. *Chem. Rev.* **116**, 1053–1093.
- Gao, Z., Varshney, S.K., Wong, S., and Eisenberg, A. (1994). Block copolymer “crew-cut” micelles in water. *Macromolecules* **27**, 7923–7927.
- Guan, L., Rizzello, L., and Battaglia, G. (2015). Polymersomes and their applications in cancer delivery and therapy. *Nanomedicine* **10**, 2757–2780.
- Haluska, C.K., Gózdź, W.T., Döbereiner, H.-G., Förster, S., and Gompper, G. (2002). Giant hexagonal superstructures in diblock-copolymer membranes. *Phys. Rev. Lett.* **89**, 238302.
- Hanczyc, M.M., Fujikawa, S.M., and Szostak, J.W. (2003). Experimental models of primitive cellular compartments: encapsulation, growth, and division. *Science* **302**, 618–622.
- Hanwell, M.D., Curtis, D.E., Lonie, D.C., Vandermeersch, T., Zurek, E., and Hutchison, G.R. (2012). Avogadro: an advanced semantic chemical editor, visualization, and analysis platform. *J. Cheminform.* **4**, 17.
- Hu, X., Zhang, Y., Xie, Z., Jing, X., Bellotti, A., and Gu, Z. (2017). Stimuli-responsive polymersomes for biomedical applications. *Biomacromolecules* **18**, 649–673.
- Huang, C., Quinn, D., Sadovskiy, Y., Suresh, S., and Hsia, K.J. (2017). Formation and size distribution of self-assembled vesicles. *Proc. Natl. Acad. Sci. USA* **114**, 2910–2915.
- ichirou Akashi, K., and Miyata, H. (2010). Lipid bilayer vesicles with numbers of membrane-linking pores. *J. Phys. Soc. Jpn.* **79**, 064801.
- Jain, S., and Bates, F.S. (2003). On the origins of morphological complexity in block copolymer surfactants. *Science* **300**, 460–464.
- Jain, S., and Bates, F.S. (2004). Consequences of nonergodicity in aqueous binary PEO-PB micellar dispersions. *Macromolecules* **37**, 1511–1523.
- Johnson, B.K., and Prud'homme, R.K. (2003). Mechanism for rapid self-assembly of block copolymer nanoparticles. *Phys. Rev. Lett.* **91**, 118302.
- Li, M.-H., and Keller, P. (2009). Stimuli-responsive polymer vesicles. *Soft Matter* **5**, 927–937.
- Ligoure, C., and Leibler, L. (1990). Thermodynamics and kinetics of grafting end-functionalized polymers to an interface. *J. Phys.* **51**, 1313–1328.
- Lim Soo, P., and Eisenberg, A. (2004). Preparation of block copolymer vesicles in solution. *J. Polym. Sci. B Polym. Phys.* **42**, 923–938.
- Liu, G., Wang, X., Hu, J., Zhang, G., and Liu, S. (2014). Self-immolative polymersomes for high-efficiency triggered release and programmed enzymatic reactions. *J. Am. Chem. Soc.* **136**, 7492–7497.
- Lomas, H., Canton, I., MacNeil, S., Du, J., Armes, S.P., Ryan, A.J., Lewis, A.L., and Battaglia, G. (2007). Biomimetic pH sensitive polymersomes for efficient dna encapsulation and delivery. *Adv. Mater.* **19**, 4238–4243.
- LoPresti, C., Lomas, H., Massignani, M., Smart, T., and Battaglia, G. (2009). Polymersomes: nature inspired nanometer sized compartments. *J. Mater. Chem.* **19**, 3576–3590.
- Mai, Y., and Eisenberg, A. (2012). Self-assembly of block copolymers. *Chem. Soc. Rev.* **41**, 5969–5985.
- Mann, S. (2013). The origins of life: old problems, new chemistries. *Angew. Chem. Int. Ed.* **52**, 155–162.
- Meeuwissen, S.A., Kim, K.T., Chen, Y., Pochan, D.J., and van Hest, J. (2011). Controlled shape transformation of polymersome stomatocytes. *Angew. Chem. Int. Ed.* **50**, 7070–7073.
- Messenger, L., Gaitzsch, J., Chierico, L., and Battaglia, G. (2014). Novel aspects of encapsulation and delivery using polymersomes. *Cur. Opin. Pharmacol.* **18**, 104–111.
- Noguchi, H. (2015). Shape transitions of high-genus fluid vesicles. *Europhys. Lett.* **112**, 58004.
- Noguchi, H., Sakashitaa, A., and Imai, M. (2015). Shape transformations of toroidal vesicles. *Soft Matter* **11**, 193–201.
- Pattni, B.S., Chupin, V.V., and Torchilin, V.P. (2015). New developments in liposomal drug delivery. *Chem. Rev.* **115**, 10938–10966.
- Pearson, R.T., Warren, N.J., Lewis, A.L., Armes, S.P., and Battaglia, G. (2013). Effect of pH and temperature on PMPC-PDPD copolymer self-assembly. *Macromolecules* **46**, 1400–1407.
- Pegoraro, C., Cecchin, D., Gracia, L.S., Warren, N., Madsen, J., Armes, S.P., Lewis, A., MacNeil, S., and Battaglia, G. (2013). Enhanced drug delivery to melanoma cells using PMPC-PDPA polymersomes. *Cancer Lett.* **334**, 328–337.
- Peters, R.J., Louzao, I., and van Hest, J.C. (2012). From polymeric nanoreactors to artificial organelles. *Chem. Sci.* **3**, 335–342.
- Pettersen, E.F., Goddard, T.D., Huang, C.C., Couch, G.S., Greenblatt, D.M., Meng, E.C., and Ferrin, T.E. (2004). UCSF chimera—a visualization system for exploratory research and analysis. *J. Comput. Chem.* **13**, 1605–1612.
- Photos, P.J., Bacakova, L., Discher, B., Bates, F.S., and Discher, D.E. (2003). Polymer vesicles in vivo: correlations with peg molecular weight. *J. Control. Release* **90**, 323–334.
- Rikken, R., Engelkamp, H., Nolte, R., Maan, J., Van Hest, J., Wilson, D., and Christianen, P. (2016). Shaping polymersomes into predictable morphologies via out-of-equilibrium self-assembly. *Nat. Commun.* **7**, 12606.
- Robertson, J.D., Rizzello, L., Avila-Olias, M., Gaitzsch, J., Contini, C., Magoń, M.S., Renshaw, S.A., and Battaglia, G. (2016). Purification of nanoparticles by size and shape. *Sci. Rep.* **6**, 27494.
- Robertson, J.D., Yealland, G., Avila-Olias, M., Chierico, L., Bandmann, O., Renshaw, S.A., and Battaglia, G. (2014). pH-sensitive tubular polymersomes: formation and applications in cellular delivery. *ACS Nano* **8**, 4650–4661.
- Seifert, U. (1991). Vesicles of toroidal topology. *Phys. Rev. Lett.* **66**, 2404.
- Seifert, U., and Lipowsky, R. (1995). Morphology of vesicles. *Handbook Biol. Phys.* **1**, 403–464.
- Smart, T., Lomas, H., Massignani, M., Flores-Merino, M.V., Perez, L.R., and Battaglia, G. (2008). Block copolymer nanostructures. *Nano Today* **3**, 38–46.
- Szostak, J.W., Bartel, D.P., and Luisi, P.L. (2001). Synthesizing life. *Nature* **409**, 387.
- van Oers, M.C., Rutjes, F.P., and van Hest, J.C. (2013). Tubular polymersomes: a cross-linker-induced shape transformation. *J. Am. Chem. Soc.* **135**, 16308–16311.
- Wang, C., Wang, Z., and Zhang, X. (2012). Amphiphilic building blocks for self-assembly: from amphiphiles to supra-amphiphiles. *Acc. Chem. Res.* **45**, 608–618.
- Wong, C.K., Mason, A.F., Stenzel, M.H., and Thordarson, P. (2017). Formation of non-spherical polymersomes driven by hydrophobic directional aromatic perylene interactions. *Nat. Commun.* **8**, 1240.
- Zhang, L., and Eisenberg, A. (1995). Multiple morphologies of “crew-cut” aggregates of polystyrene-*b*-poly (acrylic acid) block copolymers. *Science* **268**, 1728–1731.

ISCI, Volume 7

Supplemental Information

**Bottom-Up Evolution of Vesicles
from Disks to High-Genus Polymersomes**

Claudia Contini, Russell Pearson, Linge Wang, Lea Messenger, Jens Gaitzsch, Loris Rizzello, Lorena Ruiz-Perez, and Giuseppe Battaglia

1 SUPPLEMENTAL FIGURES

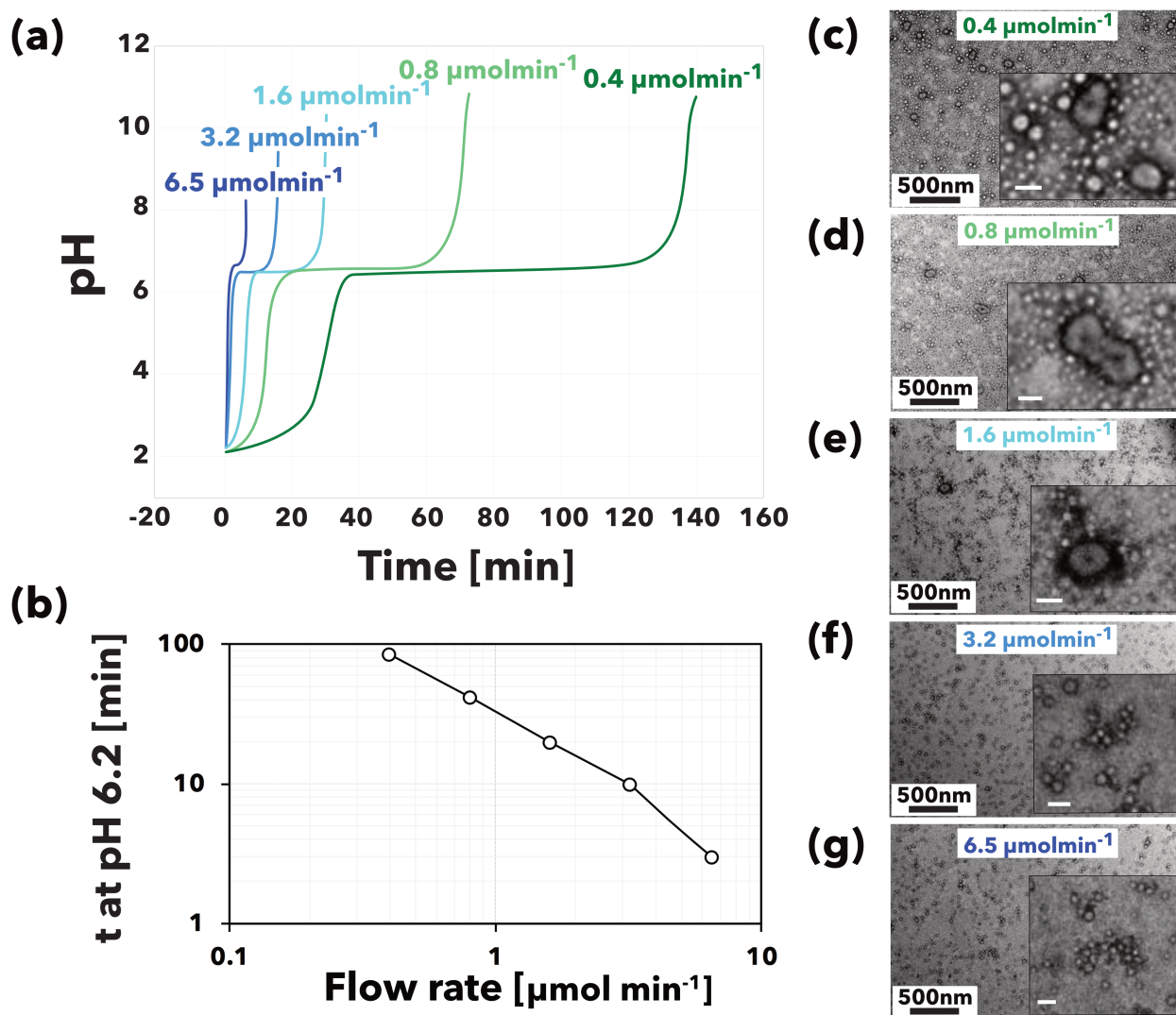


Figure 1 Related to Figure 2 pH titration. Titration curves plotted as pH versus time using different flow rates of NaOH solution addition to PMPC₂₅-PDPA₇₀ A solutions (a). The time plateau obtained from the titration curves trend lines versus the NaOH's flow rate of injection calculated graphically from the titration curves (b). TEM micrographs of the sample obtained at different flow-rates c-g. The small inset scale bar is 50nm

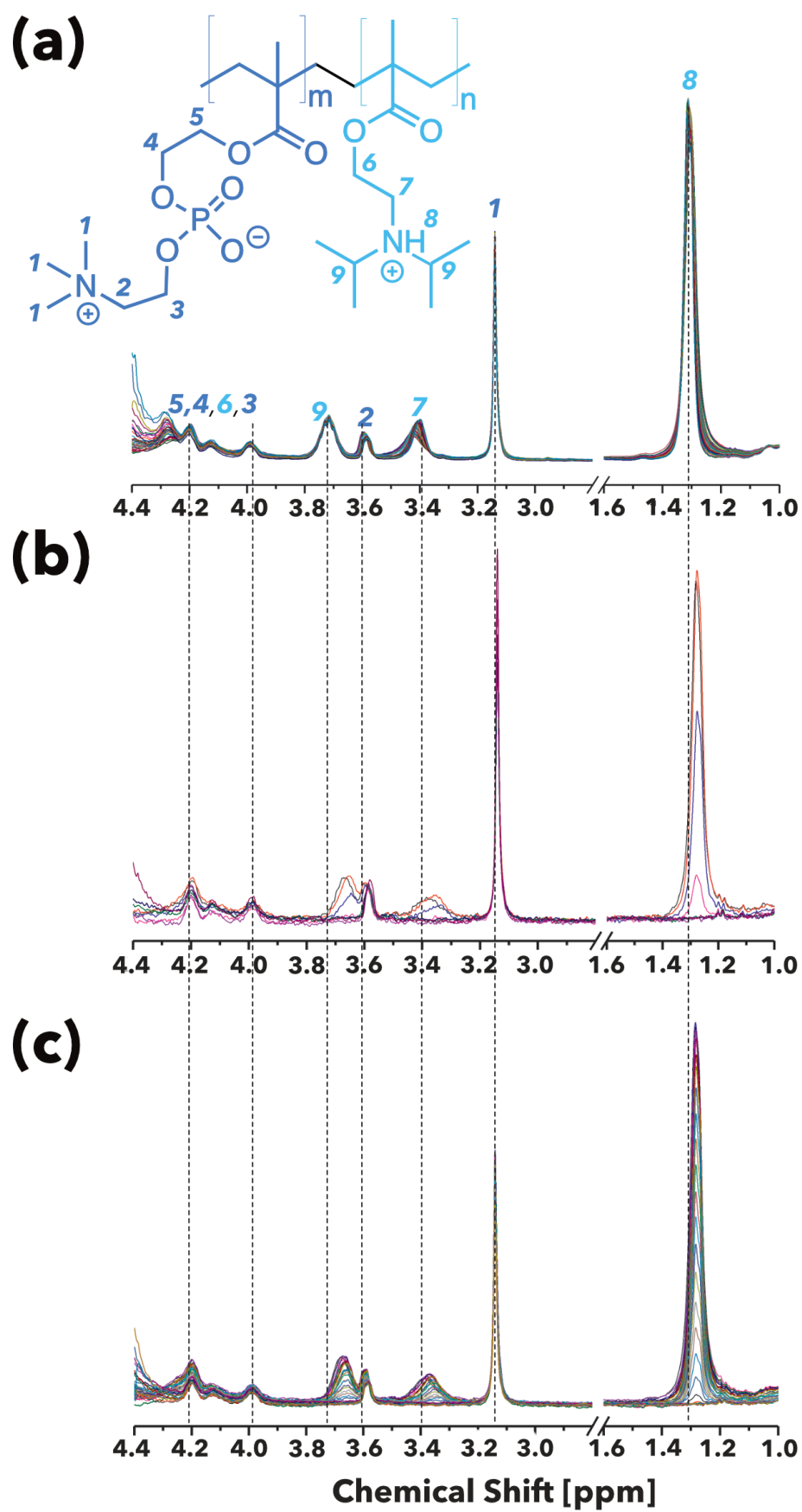


Figure 2 Related to Figure 3. NMR titration spectra as a function of temperature. PMPC₂₅-PDPA₇₀ dispersion during slow heating at pH=2 (a), fast (b) and slow (c) heating at pH=7.

1.1 TRANSPARENT METHODS

Materials. MPC monomer (99.9 % purity) was donated by Biocompatibles U.K. Ltd.. Anhydrous ethanol (99 %), anhydrous methanol (99.8 %), DPA, copper(I) bromide (99.9 %), 2,2'-bipyridine (99 %), tris (2-carboxyethyl) phosphine hydrochloride (TCEP, 98 %), dry triethylamine and phosphotungstic acid (PTA) were purchased from Sigma Aldrich UK. The silica gel 60(63-200 nm) used to remove the ATRP catalyst CuBr was purchased from E. Merck (Darmstadt, Germany). HPLC grade dichloromethane and methanol was purchased from Fisher Scientific (Loughborough, UK). All the above were used as received. Phosphate-buffered saline (PBS) was prepared from tablets obtained from Oxoid (Basingstoke, UK). Semi-permeable cellulose dialysis tubing (Spectra/Por 6 MWCO 1,000) was purchased from Fisher Scientific (Loughborough, UK).

PMPC-PDPA synthesis. The PMPC-PDPA copolymers were synthesised using the already published protocol (Lomas et al., 2007). In a typical ATRP synthesis procedure for PMPC₂₅-PDPA₇₀, a solution containing an equivalent of morpholinoethyl-bromoisobutyric acid ester (ME-Br) was mixed in a round-bottom flask with MPC (25 eq.). The mixture was then dissolved in a few milliliters of ethanol and purged with nitrogen. Subsequently, a solid mixture of 2,2'-bipyridine (2 eq.) and Cu(I)Br (1 eq.) was added under a constant nitrogen flow. The reaction mixture was stirred for 60 minutes to yield a highly viscous brown solution. Meanwhile, a solution of DPA (70 eq.) was prepared and purged with nitrogen in a separate flask before addition. Then, the reaction mixture was left overnight at room temperature. The mixture gradually turned green after dilution with ethanol, indicating the catalyst oxidation and passed through silica. The solution was then dialysed (MWCO 1,000 Da) against dichloromethane, methanol and water. The polymer was then freeze-dried under vacuum. PMPC₂₅-PDPA₇₂ was solubilised in a mixture of CDCl₃/MeOD (3:1) and analyse in ¹H NMR analysis to confirm the success of the reaction.

Preparation of PMPC-PDPA dispersions. PMPC_x-PDPA_y copolymers were solubilised at a concentration of 40 μM, at room temperature in acidified phosphate buffer saline (PBS, pH 2) solution in order to dissolve all the block copolymer chains (unimers). For the pH switch, this was raised adding drop-wise a 1 M NaOH solution. The temperature of the solution was then dropped to 5 °C and the pH was raised to 7 by adding the required 1 M NaOH solution.

UV-Vis Spectroscopy analysis. UV-vis spectroscopy experiments were carried out on a JASCO XX spectrophotometer equipped with a temperature controller. Solutions of PMPC_x-PDPA_y were prepared at low temperature with a concentration of 40 μM, and placed in the UV chamber. Absorbance was recorded from 5 to 60 °C at a constant rate of 0.3 to 3 °C/min.

Transmission Electron Microscopy (TEM) imaging. TEM imaging was performed using a JEOL 2100 TEM microscope at 200 kV, equipped with a Gatan CCD camera. The polymersomes were stained using a phosphotungstic acid (PTA) solution at 0.75 % (w/v). This PTA solution was prepared by dissolving 37.5 mg of PTA in boiling distilled water (5 mL). The pH was adjusted to 7.0 by adding a few drops of 5 M NaOH under continuous stirring. The PTA solution was then filtered through a 0.2 μm membrane. Copper grids were glow-discharged for 40 seconds in order to render their surface hydrophilic. Then 5 μL of copolymer dispersion (concentration 0.5 mg mL⁻¹) was deposited onto the grids for one minute. After that, the grids were blotted with filter paper and immersed into the PTA staining solution for 5 s for positive staining. Then the grids were blotted again and dried under vacuum for 1 min. Cryogenic TEM specimens were prepared by fast immersing a pre-sample-engrossed grid in liquid ethane using the Gatan Cryoplunge® 3 system. The grid is quickly placed in a cryogenic stage and kept at -170 °C and imaged using a GATAN cryogenic holder.

Differential Scanning Calorimetry (DSC) analysis. The analysis was carried out using a VP-DSC MicroCalorimeter with a sample cell of 0.5 mL. The sample were prepared as previously described at pH 7 and 5 °C, and analyse at a rate of 1 °C min⁻¹ from 5 to 60 °C and vice versa.

¹H NMR spectroscopy. NMR spectroscopy of PMPC-PDPA after synthesis was carried out on a Bruker AV600 spectrometer. ¹H-NMR was also used to monitor the intensity evolution of DPA and MPC protons peaks as function of temperature by using a Bruker 400 MHz instrument. In a typical experiment, block copolymer solutions in deuterated PBS using a the same protocol described above for all the PMPC-PDPA dispersions. NMR spectra were then recorded while the temperature was increased at 40 °C with a rate of 0.2 and 1 ° min⁻¹. The proton intensity of the peak 7, 8 and 9 were normalised setting the maximum value to 1. All the following intensities were set in relation to this value to give a distinct intensity correlation as a function of the temperature change. The average and standard deviation values were then calculated and used to illustrate the change in intensities.

References

- Lomas, H., I. Canton, S. MacNeil, J. Du, S. P. Armes, A. J. Ryan, A. L. Lewis, and G. Battaglia (2007). Biomimetic ph sensitive polymersomes for efficient dna encapsulation and delivery. *Adv. Mater.* 19(23), 4238–4243.