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Pre-Operative Cerebral Hemodynamics from Birth to Surgery in Neonates with Critical Congenital Heart Disease

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Abstract

Objective—Hypoxic-ischemic white mater brain injury commonly occurs in neonates with critical congenital heart disease (CHD). Recent work has shown that longer time-to-surgery is associated with increased risk for this injury. Here we investigate changes in perinatal cerebral hemodynamics during the transition from fetal to neonatal circulation to ascertain mechanisms that may underlie this risk.

Disclosures

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Methods—Neonates with either transposition of the great arteries (TGA) or hypoplastic left heart syndrome (HLHS) were recruited for pre-operative non-invasive optical monitoring of cerebral oxygen saturation (ScO₂), cerebral oxygen extraction fraction (OEF), and cerebral blood flow (CBF) using diffuse optical spectroscopy and diffuse correlation spectroscopy, two non-invasive optical techniques. Measurements were acquired daily from day of consent until the morning of surgery. Temporal trends in these measured parameters during the preoperative period were assessed with a mixed-effects model.

Results—Forty-eight neonates with TGA or HLHS were studied. ScO₂ was significantly and negatively correlated with time, and OEF was significantly and positively correlated with time. CBF did not significantly change with time during the pre-operative period.

Conclusions—In neonates with TGA or HLHS, increasing cerebral oxygen extraction combined with an abnormal cerebral blood flow response during the time between birth and heart surgery leads to a progressive decrease in cerebral tissue oxygenation. The results support and help explain the physiological basis for recent studies that show longer time-to-surgery increases the risk of acquiring white matter injury.

Graphical abstract



Introduction

Approximately 30,000 children are born each year in the United States with congenital heart disease (CHD). Nearly one third of these children are born with critical CHD, defined as lesions that require cardiac surgery in the neonatal period.¹ In the last 3 decades, survival of neonates with CHD has improved dramatically, with the majority of these patients now reaching school age.² The focus of research has shifted from survival beyond the neonatal period to addressing the neurodevelopment disabilities seen among long-term survivors. Nearly half of the school-age survivors exhibit neurobehavioral symptoms, such as inattention, hyperactivity, and impaired executive function.^{3–5}

Increasing evidence suggests that underlying these neurobehavioral symptoms is hypoxicischemic white matter injury (WMI) seen on brain magnetic resonance imaging (MRI) termed periventricular leukomalacia (PVL).^{6–9} We have previously reported that longer time

between birth and surgery was associated with an increased risk for WMI/PVL in infants with transposition of the great arteries (TGA) and hypoplastic left heart syndrome (HLHS). ^{10, 11} Due to this common risk of increased time-to-surgery, the objective of this study was to investigate pre-operative cerebral physiology and hemodynamics in neonates with HLHS and TGA to elucidate the pathology underlying the increased risk for brain injury with longer waiting times for surgery. Diffuse optical and diffuse correlation spectroscopies (DOS and DCS, respectively) were utilized for non-invasive bedside quantification of pre-operative cerebral hemodynamics^{12, 13}, and the time course of these parameters during the pre-operative period explored.

Materials and Methods

Patient Population

All term (37-42 weeks gestation) newborns with pre- or post-natally diagnosed critical CHD admitted to the cardiac intensive care unit (CICU) at The Children's Hospital of Philadelphia were screened for study inclusion and approached for participation as early as possible. Exclusion criteria included: birth weight less than 2 kg, a history of neonatal depression (e.g., 5 minute APGAR<5, cord blood pH<7.0, sepsis, or birth asphyxia), perinatal seizures, evidence of end-organ injury, pre-operative cardiac arrest, and significant pre-operative intracerebral hemorrhage such as grade 3 or 4 intraventricular hemorrhage. Infants with identified or suspected genetic syndromes were not excluded.

Study Protocol

All procedures were approved by the Institutional Review Board at the Children's Hospital of Philadelphia. Patient demographic data were recorded. Daily DOS/DCS measurements of cerebral tissue oxygen saturation (ScO₂), oxygen extraction fraction (OEF), and cerebral blood flow (CBF) were made as soon as consent was obtained, with the last measurement made on the morning of surgery prior to induction of anesthesia. Vitals data was captured continuously (CNS Technology, LLC, Ambler, PA), and daily measurements of peripheral capillary oxygen saturation (SpO₂) from pulse-oximetry are reported from the time that the daily DOS/DCS measurements were performed. Preoperative blood gases were acquired per clinical protocol, and arterial hemoglobin concentration (Hgb) on day of birth and day of surgery are reported.

DOS/DCS Measurements

Diffuse optical spectroscopy (DOS) and diffuse correlation spectroscopy (DCS) utilize nearinfrared light to noninvasively probe the static and dynamic properties of cortical brain tissue. Our custom-made optical instrument combines these two techniques on a mobile cart that can be used in the MRI suite, the operating room, and peri-operatively at the bedside. 14–16

DOS (also known as frequency-domain near-infrared spectroscopy or fd-NIRS) is a widely accepted method to quantify tissue oxygenation. Multi-separation frequency domain DOS, employed in this study, is capable of accurate quantification of cerebral tissue oxygen saturation (ScO₂), i.e., in contrast to, commercial oximeters that employ continuous-wave

NIRS to monitor trends in cerebral oxygen saturation.^{17–19} DOS uses photon diffusion theory to relate the measured amplitude attenuation and phase shift of modulated and multiply scattered light detected on the tissue surface to the wavelength-dependent tissue absorption (μ_a) and scattering (μ_a') properties. The wavelength- and time-dependent absorption coefficient, $\mu_a(\lambda, t)$, depends linearly on oxy-([HbO₂]) and deoxy-hemoglobin ([Hb]) concentration; thus measurements at multiple wavelengths yields these two parameters. From [HbO₂] and [Hb], we derive total hemoglobin concentration (THC=[HbO₂]+[Hb]) and cerebral tissue oxygen saturation (ScO₂=[HbO₂]/THC). Cerebral oxygen extraction fraction (OEF) can be calculated from ScO₂ and peripheral capillary oxygen saturation (SpO₂) measured clinically from a pulse-oximeter using the formula

 $OEF = \frac{1}{\gamma} \frac{SpO_2 - ScO_2}{SpO_2}$, where γ is the fraction of blood in the venous compartment, assumed

to be 0.75.^{14, 20} Cerebral blood volume (CBV, mL/100g of tissue) can be calculated from THC. The DOS device employed in the present study (Imagent, ISS Inc., Champaign, IL) is amplitude modulated at 110 MHz and employs source lasers at 2 wavelengths, λ =688 and 830 nm.

DCS uses near-infrared light to non-invasively monitor CBF. DCS measures the temporal fluctuations of the light intensity emerging in remission at the tissue surface; these fluctuations are caused primarily by moving red blood cells.^{12, 21–25} Correlation diffusion theory is then employed to convert these temporal fluctuations into a blood flow index (BFI, measured in units of cm²/s).¹² Although this index does not have traditional physiological units of cerebral blood flow (CBF), recent studies have shown that BFI correlates strongly with other gold standard measures of CBF.^{15, 16, 26–30} Specifically, Jain et al. validated BFI against CBF measured in the superior sagittal sinus with phase contrast MRI in a similar population of infants with critical CHD.¹⁶ Further, BFI can be combined with OEF, calculated using the equation above to give an index of cerebral metabolic rate of oxygen consumption (CMRO_{2,i}) using the formula *CMRO*_{2,i} = *OEF* × *BFI* × *CaO*₂ where CaO₂ is the arterial oxygen concentration which can be approximated as *CaO*₂ ≈ 1.39 × *SpO*₂ × *Hgb*. 14, 15

DOS and DCS measurements were conducted once daily from the day of consent until the morning of surgery. The time of the measurements was recorded with respect to the subject's time of birth. Measurements were made noninvasively over both the right and left frontal cortex. At each location, four repetitions of the basic measurement were acquired in order to account for local inhomogeneities under the optical probe. These eight repetitions were then averaged to derive a global measure of ScO_2 and BFI.

Brain MRI

In a subset of patients (n=33), a brain MRI was obtained immediately prior to surgery as part of a different study protocol.^{11, 31} All images were acquired using a 1.5T Avanto MRI system (Siemens Medical Systems, Malvern, Pa) using a 12-channel head coil. The studies included T₁-weighted magnetization-prepared rapid acquisition gradient echo and T₂weighted sampling perfection with application-optimized contrasts using different flip angle evolution sequences acquired in the axial plane. Two independent observers, who were

unaware of the clinical data, evaluated the total brain maturation score (TMS) using axial T_1 - and T_2 -weighted images.^{32, 33}

Statistical Analysis

For analysis purposes, patients were grouped according to cardiac diagnosis. Continuous variables were summarized by standard descriptive statistics (mean, standard deviation (SD), or median, interquartile range (IQR) as appropriate), and frequencies and percentages were used for categorical variables.

The pre-operative temporal trends in cerebral hemodynamics were examined using a linear mixed-effects model implemented within the SAS mixed procedure, a method commonly used for analyzing correlated data such as repeated measures or clustered data. The model was used to predict the mean outcome variable (*i.e.*, ScO₂, OEF, BFI, CMRO_{2,i}, and SpO₂) as a function of time and cardiac diagnosis. In this study, since a single measurement was taken on the same patient at multiple time points, these these measures (*i.e.*, ScO₂, OEF, BFI, CMRO_{2.i}, and SpO₂) are correlated with each other; we refer to this as "within-subject correlation". Specifically, subject-specific random effects were included in the model to account for within-subject correlations resulting from the repeated measures. Random intercept and slope were assumed in the linear mixed-effects model to capture potential difference in the baselines and trajectories among individuals. For the covariance structure, we compared the compound symmetry (CS) with the autoregressive (1) (AR(1)), and we used the Akaike information criterion (AIC) to determine the optimal covariance matrices. CS assumes that correlations between all pairs of measures within the same subject are the same, while AR(1) assumes that correlations between two measures decrease exponentially with distance (*i.e.*, decrease with the time between the two measures). Normality of the outcome variables was examined graphically and statistically using Shapiro-Wilk test. In the mixed-effects model, we considered both linear and non-linear temporal trends by including a term quadratic in time into the model. All analyses were performed using SAS 9.4 statistical software (SAS Institute Inc, Cary, NC). Statistical significance was declared for P values < 0.05.

Results

From March 2013 to March 2016, a total of N=70 neonates with complex CHD were recruited. Cardiac diagnoses included HLHS (n=24), TGA (n=24), tetralogy of Fallot (n=6), hypoplastic arch (n=3), interrupted aortic arch (n=3), aortic atresia (n=3), double inlet left ventricle (n=2), truncus arteriosis (n=2), coarctation of the aorta (n=2), and double outlet right ventricle (n=1). Due to challenges in grouping patients with shared physiology, and small numbers in certain groups, our analysis was limited to only patients with TGA and HLHS.

Patient demographics for the subset of patients with TGA or HLHS (n=48) are summarized in Table 1. All patients were full-term with an average gestational age of 38.9 ± 0.7 weeks and an average time-to-surgery of 4.3 ± 2.5 days. In this cohort, patients with a diagnosis of TGA had on average an older gestational age than those with a diagnosis of HLHS. No

differences in birth weight, time-to-surgery, head circumference or brain maturation were observed between diagnoses.

Initial measurements of ScO₂, OEF, BFI, and CMRO_{2,i} are reported in Table 1. The first measured ScO₂ was lower on average (p=0.04) in patients with TGA (46.8±8.9%) compared to patients with HLHS (52.0±7.2%). The average initial ScO₂ amongst all subjects was 49.4±8.4%. Daily measurements of ScO₂, OEF, BFI, and CMRO_{2,i} for all subjects are shown in Figure 1. Preoperative measurements of Hgb and daily measurements of SpO₂ are shown in Figure 2.

We performed a linear mixed-effects model to assess the effects of time and cardiac diagnosis on the daily measurements of ScO₂, OEF, BFI and CMRO_{2,i} (Table 2, Figure 1) and on daily measurements of SpO₂ (Table 3, Figure 2). Since preoperative ScO₂ was different between the two cohorts, cardiac diagnosis was included in the mixed-effects model as a covariate. Only the results from a linear model are reported because higher order of effects of time were not found to be significant. Time from birth was a significant predictor of pre-operative ScO₂ (p=0.02), and OEF (p=0.01). Cardiac diagnosis (HLHS or TGA) significantly predicts pre-operative ScO₂ (p<0.01), BFI (p=0.05), and SpO₂ (p=0.01). The interaction between cardiac diagnosis and time was not a significant predictor of any of the outcome variables. We also performed a linear mixed-effects model on the subset (n=33) of subjects who received brain MRIs on the morning of surgery to assess the effect of brain maturation on preoperative CMRO_{2,i} (Table 4); the latter was computed using a simple steady-state model described in the Methods section. Total brain maturation score did not affect the temporal trends of CMRO_{2,i} (p=0.03).

Discussion

This investigation is the first report on longitudinal monitoring of pre-operative cerebral hemodynamics in neonates with critical CHD. Previous studies have looked at cross-sectional trends in pre-operative saturations in these two patient populations independently. $^{10, 11}$ Our group previously used the same non-invasive optical techniques (DOS/DCS) to measure ScO₂ immediately prior to surgery in infants with HLHS.¹¹ In our cross-sectional analysis, preoperative ScO₂ was negatively correlated with a longer time between birth and surgery, suggesting that ScO₂ decreases between birth and surgery. This initial observation is further supported by the present study as daily measurements of preoperative ScO₂ were found to negatively correlate with time. In both the previous¹¹ and current study, the differences in timing of surgery between subjects were a result of "modifiable" logistics including availability of the requested surgeon and the day of the week on which the patient was born. No patients went to surgery early (*e.g.*, for pulmonary over-circulation) or had surgery delayed for medical reasons (*e.g.*, for infection, bleeding, seizures).

Although pre-operative cerebral hemodynamics have been previously studied using DOS/DCS in neonates with TGA, the relationship to time-to-surgery has not been previously investigated. In 2009, Petit et al. reported that preoperative brain injury in neonates with transposition of the great arteries was associated with systemic hypoxemia

and longer time-to-surgery, again suggesting that increased risk of WMI/PVL with longer time-to-surgery could be due to decreasing ScO_2 during the preoperative period.¹⁰ With the present study we were able to confirm this finding and were able to demonstrate longitudinal decrease in ScO_2 similar to the decreases in ScO_2 measured in neonates with HLHS. Since the increase in pre-operative oxygen extraction exists independent of cardiac diagnosis, our findings suggest a commonality in the mechanism behind the previously reported increased risk for WMI/PVL with longer time-to-surgery in both populations.

The decreases in ScO₂ measured in this patient population are larger in magnitude than what would be expected for a healthy neonate. Franceschini et al. similarly used diffuse optical spectroscopy to study trends in ScO₂ in healthy infants over the first year of life.³⁴ They reported an average decrease of 10 percentage points in ScO₂ from 0 to 6 weeks, without corresponding changes in cerebral blood volume or CMRO₂; this change was attributed to the decrease in hematocrit during the transition from fetal to adult hemoglobin. This relatively minimal change in ScO₂ is not sufficient to explain the large decrease in ScO₂ of -2.2% per day observed in this CHD population. Additionally, Franceschini et al. report an average ScO₂ of 67% in healthy neonates measured during the first week of life, whereas the average initial ScO₂ measured in this cohort of infants with CHD is 49.4 ± 8.4%. Therefore, it appears that infants with complex CHD are born with a lower than normal cerebral tissue oxygen saturation and also experience a greater than normal drop in saturation during the first week of life.

Cerebral oxygen extraction is related to oxygen delivery and metabolism through the equation $CMRO_{2,i} = OEF \times BFI \times CaO_2$, valid in steady state, where CaO₂ is the arterial oxygen concentration which can be approximated as $CaO_2 \approx 1.39 \times SpO_2 \times Hgb.^{14, 15}$ Therefore, an increase in OEF could be caused by an increase in CMRO2,i, a decrease in BFI, a decrease in SpO₂, a decrease in Hgb, or a combination of these factors. In this study, it is reasonable to speculate that the observed increase in OEF after birth is due to a decrease in oxygen carrying capacity caused by decreased hemoglobin after repeated blood draws. However, we did not observe a statistically significant difference between Hgb measured on day of birth and Hgb measured on day-of-surgery (Figure 2). A decrease in arterial oxygen saturation would also explain an increase in oxygen extraction, but we did not observe a decrease in SpO₂ during the preoperative period. Furthermore, the expected physiological response to a decrease in oxygen carrying capacity caused by a decrease in hemoglobin, would be to increase CBF to keep oxygen supply constant; CBF did not exhibit this increase in our mixed effects model results from the whole study population. This absence of CBF compensation suggests a failure of compensatory mechanisms, for example a failure of cerebrovascular resistance. Further, the mismatch between increased oxygen extraction and stagnant oxygen delivery explains the association of longer time-to-surgery with increased risk for WMI/PVL before surgery in TGA and after surgery in HLHS.

Another possible cause for increased oxygen extraction during the preoperative period is an increased oxygen demand during the newborn period. However, $CMRO_{2,i}$ was not found to be increasing within error in this study. Previously, $CMRO_2$ has been shown to increase during the first few weeks of life in premature infants with similar brain maturation as full term infants with complex CHD.^{33, 35}, In the present study baseline CMRO_{2,i} was found to

be inversely related to brain maturation, thus supporting previous research that suggests brain immaturity is correlated with cerebral oxygen metabolism.³⁵ An increase in oxygen demand would be expected to cause a corresponding increase in oxygen delivery, but again an increase in CBF was not observed indicating a failure of compensatory mechanisms.

Understanding the fetal circulation is salient to understanding the failure of CBF compensation to meet increasing pre-operative oxygen extraction. Prenatal studies using Doppler ultrasound have shown fetuses with HLHS have lower than normal cerebral vascular resistance (CVR).^{36, 37} Lower fetal CVR is likely due to decreased oxygen delivery to the brain caused by the altered anatomy that results from ductal dependent CBF.^{36, 38} Doppler ultrasound in fetuses with TGA also demonstrates a decrease in fetal CVR, reflecting a deficit in oxygen delivery that is due to the lower oxygen saturations caused by the transposed great vessels.^{38, 39} Sustained decrease in CVR during fetal life could exhaust the compensatory mechanisms that are needed to increase CBF in response to increasing OEF.

The significance of longer time-to-surgery has been previously demonstrated.^{10, 11, 40} Further, we have shown that in patients with HLHS there exists a strong correlation between lower cerebral oxygen saturations and longer time-to-surgery and that these factors increased the risk for both the prevalence and severity of WMI/PVL. The current results provide insight into the underlying cause of this increased risk. These findings demonstrate the critical role of the preoperative period in the development of risk for WMI/PVL. If further corroborated, these observations could lead to a shift in the emphasis of neuroprotective strategies from the operative period to the preoperative period. However, as both of the aforementioned studies were conducted at a single center, it is imperative to investigate the preoperative period and risk for WMI/PVL with age at time of Norwood procedure at different centers with different perioperative and operative clinical care strategies. A larger, multicenter study between the Children's Hospital of Philadelphia and Texas Children's Hospital is currently being pursued to further investigate the changing cerebral hemodynamics during the preoperative period and the effect on risk for white matter injury.

Study Limitations

A significant limitation of the present study was that measurements of preoperative cerebral hemodynamics were taken only once per day starting with the day of study inclusion when consent was obtained. Thus, the timing of the first measurement differed between subjects. Furthermore, measurements were performed at times of convenience rather than a standardized to time of day. Because of this relatively low frequency of data acquisition, analysis with a mixed effects model was limited to low order models, and although we found that BFI and CMRO_{2,i} did not significantly change with time, the uncertainties associated with these measurements were relatively large. Thus, it is possible that CBF and oxygen metabolism were changing during the preoperative period, but the sensitivity of our measurements could have been too low to discern these changes. We note that application of simple steady-state models to our whole data set, relating OEF, CBF and oxygen metabolism (based on the mixed effects model results) are consistent within the measurement error bars. Higher frequency of data acquisition is needed to fit higher order models to these

preoperative variables and to decrease uncertainty, and these improvements will be necessary to begin to elicit an "optimal" timing of surgery with respect to cerebral hemodynamics. Additionally, the current study protocol did not permit for blood gas measurements at the same time as optical measurements, limiting analysis of the effect that changes in hemoglobin may have to the measured cerebral hemodynamics.

Another significant limitation in the present study is that it was conducted at a single site. Since preoperative care, specifically time from birth until surgery, varies between different institutions, the results presented here may be less applicable to other sites. Further investigation into different preoperative management strategies, operative strategies, and their effect on development of brain injury and trends in cerebral hemodynamics is necessary to further understand the relationship between clinical care and neurodevelopmental outcomes. The multicenter study described above aims to accomplish this goal.

Conclusion

We investigated the pre-operative trends in cerebral hemodynamics in neonates with TGA or HLHS awaiting surgery. We observed that cerebral tissue oxygenation decreases during the pre-operative period in all patients, regardless of cardiac diagnosis. This decrease in oxygenation was associated with an increase in oxygen extraction, but not with a corresponding increase in cerebral blood flow. The observed increase in oxygen demand without compensating oxygen delivery could lead to the previously reported increase in risk for white matter brain injury with longer time-to-surgery.

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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Abbreviations and Acronyms

BFI	blood flow index
CBF	cerebral blood flow
CBV	cerebral blood volume
CHD	congenital heart disease
CICU	cardiac intensive care unit

CMRO ₂	cerebral metabolic rate of oxygenation
DCS	diffuse correlation spectroscopy
DOS	diffuse optical spectroscopy
Hb	deoxyhemoglobin, measured DOS
HbO ₂	oxyhemoglobin, measured with DOS
Hct	hematocrit, measured from blood gas
Hgb	hemoglobin, measured from blood gas
HLHS	hypoplastic left heart syndrome
OEF	cerebral oxygen extraction fraction
SaO ₂	arterial oxygen saturation
SpO ₂	peripheral capillary oxygen saturation
ScO ₂	cerebral tissue oxygen saturation
TGA	transposition of the great arteries

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Figure 1.

Time profiles of ScO_2 (a), OEF (b), BFI (c) and $CMRO_{2,i}$ (d). Each thin line represents measurements for a single subject with either hypoplastic left heart syndrome (red) or transposition of the great arteries (blue). Thick lines represent linear trends derived from a mixed effects model reported in Table 2.



Figure 2.

Left: Boxplot demonstrating preoperative hemoglobin on day of birth and on day of surgery. Right: Time profiles of SpO_2 . Each thin line represents measurements for a single subject with either a hypoplastic left heart syndrome (red) or transposition of the great arteries (blue). Thick lines represent linear trends derived from a mixed effects model reported in Table 3 and shaded area represents the 95% confidence interval of the model.



Video 1.

Demonstration of optical measurements of cerebral blood flow and oxygen saturation.

Patient demographics and initial optical measurements.

	All (n=48)	HLHS (n=24)	TGA (n=24)	P value
Demographics				
Female, n (%)	17 (35.4)	9 (37.5)	8 (33.3)	0.76
Time-to-surgery, day	4.3 ± 2.5	4.8 ± 3.0	3.9 ± 1.7	0.42
Gest. Age, wk	38.9 ± 0.7	39.2 ± 0.7	38.7 ± 0.6	0.03
Birth weight, kg	3.4 ± 0.5	3.5 ± 0.4	3.3 ± 0.5	0.31
Head circumference, cm	34.3 ± 1.6	34.5 ± 1.2	34.1 ± 1.9	0.18
Total Brain Maturation Score [*]	10.2 ± 1.1	10.0 ± 1.2	10.5 ± 1.0	0.23
Optical measurements				
Number of measurements	4.0 ± 2.4	4.6 ± 3.1	3.3 ± 1.3	0.12
Initial ScO ₂ (%)	49.4 ± 8.4	52.0 ± 7.2	46.8 ± 8.9	0.04
Initial OEF	0.59 ± 0.13	0.57 ± 0.11	0.62 ± 0.15	0.20
Initial BFI (10 ⁻⁸ cm ² /s)	1.7 ± 0.7	1.5 ± 0.6	1.9 ± 0.7	0.07
Initial CMRO _{2,i} $(10^{-7} \text{ ml/dl} \times \text{cm}^2/\text{s})$	1.9 ± 0.9	1.7 ± 0.9	2.1 ± 0.9	0.10

ScO2, cerebral tissue oxygen saturation; *OEF*, oxygen extraction fraction; *BFI*, blood flow index; *CMRO2, j*, cerebral metabolic rate of oxygenation; *TGA*, Transposition of the Great Arteries; *HLHS:* Hypoplastic Left Heart Syndrome.

*Total Brain Maturation Score measured only for a subset of patients (HLHS: n=20; TGA: n=13)

Coefficients and standard error of the linear mixed-effects model for the optically derived outcome variables ScO₂, OEF, BFI, and CMRO_{2,i}.

Outcome Variable	Estimate (SE) of Coefficient	P value
ScO ₂ , %		
Intercept	50.7 (2.2)	< 0.0001
Time, hr	-0.09 (0.04)	0.02
Cardiac Dx	8.2 (2.8)	< 0.01
Time×Cardiac Dx	-0.05 (0.05)	0.24
OEF		
Intercept	0.56 (0.03)	< 0.0001
Time, hr	0.0014 (0.0005)	0.01
Cardiac Dx	-0.07 (0.04)	0.09
Time×Cardiac Dx	0.0005 (0.0007)	0.45
BFI, 10 ⁻⁸ cm ² /s		
Intercept	2.0 (0.1)	< 0.0001
Time, hr	-0.003 (0.003)	0.16
Cardiac Dx	-0.35 (0.18)	0.05
Time×Cardiac Dx	0.001 (0.003)	0.69
$CMRO_{2,i},10^{-7}\ ml/dl\times cm^{2}/s$		
Intercept	2.0 (0.2)	< 0.0001
Time, hr	0.002 (0.004)	0.68
Cardiac Dx	-0.28 (0.27)	0.30
Time×Cardiac Dx	0.0006 (0.006)	0.91

For each outcome variable, the table reports the y-intercept for the linear model as well as the coefficients for the 3 variables: time after birth, cardiac diagnosis (HLHS and TGA), and an interaction term between diagnosis and time. For cardiac diagnosis, TGA was used as the reference group. The linear model for each outcome variable is $y = \beta_0 + \beta_1 \times Time + \beta_2 \times Cardiac Diagnosis + \beta_3 \times Time \times Cardiac Diagnosis$.

Coefficients and standard error of the linear mixed-effects model for the clinically derived outcome variable SpO₂.

Outcome Variable	Estimate (SE) of Coefficient	P value
SpO ₂ , %		
Intercept	88.7 (1.2)	< 0.0001
Time, hr	-0.03 (0.02)	0.19
Cardiac Dx	4.1 (1.6)	0.01
Time×Cardiac Dx	0.003 (0.029)	0.91

Table reports the y-intercept for the linear model as well as the coefficients for the 3 variables: time after birth, cardiac diagnosis (HLHS and TGA), and an interaction term between diagnosis and time. For cardiac diagnosis, TGA was used as the reference group. The linear model for each outcome variable is $y = \beta_0 + \beta_1 \times Time + \beta_2 \times Cardiac Diagnosis + \beta_3 \times Time \times Cardiac Diagnosis$.

Coefficients and standard error from the linear mixed-effect model using time after birth, cardiac diagnosis (HLHS and TGA), total brain maturation score (TMS), and an interaction term between TMS and time as predictors for optically derived $CMRO_{2,I}$ on a subset of patients who received a pre-operative brain MRI (n=33). For cardiac diagnosis, TGA was used as the reference group.

Outcome Variable	Estimate (SE) of Coefficient	P value
$\text{CMRO}_{2,i}$, $10^{-7} \text{ ml/dl} \times \text{cm}^2/\text{s}$		
Intercept	5.1 (1.2)	< 0.0001
Time, hr	-0.01 (0.03)	0.61
Cardiac Dx	-0.75 (0.23)	< 0.01
TMS	-0.25 (0.11)	0.03
Time×TMS	0.001 (0.003)	0.62

The linear model for each outcome variable is $y = \beta_0 + \beta_1 \times Time + \beta_2 \times Cardiac Diagnosis + \beta_3 \times TMS + \beta_4 \times Time \times TMS$