



Published in final edited form as:

*Mol Pharm.* 2018 May 07; 15(5): 1814–1825. doi:10.1021/acs.molpharmaceut.7b01169.

## A DNA thioaptamer with homing specificity to lymphoma bone marrow involvement

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### Abstract

Drug accumulation in the malignant tissue is a prerequisite for effective cancer treatment. However, most drug molecules and their formulated particles are blocked *en route* to the destiny tissue due to the existence of multiple biological and physical barriers including the tumor microvessel endothelium. Since the endothelial cells on the surface of the microvessel wall can be modulated by inflammatory cytokines and chemokines secreted by the tumor or stromal cells, an effective drug delivery approach is to enhance interaction between the drug particles and the unique spectrum of surface proteins on the tumor endothelium. In this study, we performed *in vivo* screening for thioaptamers that bind to the bone marrow endothelium with specificity in a murine model of lymphoma with bone marrow involvement (BMI). The R1 thioaptamer was isolated based on its high homing potency to bones with BMI, and 40–60% less efficiency in accumulation to healthy bones. In cell culture, R1 binds to human umbilical vein endothelial cells (HUVEC) with a high affinity ( $K_d \approx 3$  nM), and the binding affinity can be further enhanced when cells were

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Conflict of interest disclosure statement: The authors declare no competing financial interests.

treated with a mixture of lymphoma cell and bone marrow cell conditioned media. Cellular uptake of R1 is through clathrin-mediated endocytosis. Conjugating R1 on to the surface of liposomal doxorubicin nanoparticles resulted in 2–3 fold increase in drug accumulation in lymphoma BMI. Taking together, we have successfully identified a thioaptamer that preferentially binds to the endothelium of lymphoma BMI. It can serve as an affinity moiety for targeted delivery of drug particles to the disease organ.

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## INTRODUCTION

Lymphoma is a common malignancy in the lymphatic system, and bone marrow plays an important role in lymphoma development and progression. Clinical studies have revealed that bone marrow involvement (BMI) is common in patients with advanced stages of lymphoma [1–3]. BMI is a key indicator for negative prognosis, and is associated with significantly shorter survival in patients with intermediate- to high-grade non-Hodgkin's lymphoma [2]. Numerous strategies have been tried to block proliferation and survival of lymphoma cells in the bone marrow, lymph nodes, and other lymphatic organs, such as chemotherapy, radiation therapy, and bone marrow transplantation [4,5]. One common practice in clinic is to overwhelm the body with a large quantity of drugs with the hope to send a sufficient amount of drug molecules to the bone; however, such an approach leads to severe systemic toxicity caused by drug accumulation in non-disease organs [6]. Another strategy is to package drug molecules into nanometer-size particles, such as liposomes and micelles [7–9]. It has been demonstrated that the microvessels inside the tumor tissue are leaky, which allows accumulation and retention of the drug particles [10,11]. However, there are many biological barriers for the drug molecules to overcome *en route* to the destiny organ/tissue/cell [12], nanoformulation only enable them to pass a number of them. Most drug nanoparticles will be blocked at the rest checkpoint steps. A recent analysis revealed that, on average, less than 1% of the total injected drug particles could reach the tumor tissues successfully [13], highlighting the challenge in development of effective cancer nanotherapeutic agents [14].

The unique structure of the bone marrow poses an additional barrier to target the lymphoma cells. Inside the bone marrow, the sinusoidal vessels are surrounded by a tight layer of perivascular reticular cells [15]. Although affinity moieties have been identified to target specific elements in bone marrow environment including osteoclasts [16], osteoblasts [7] and bone hydroxyapatite [17], the drug particles will need to pass the vascular barrier before reaching the malignant cells that reside in the endosteal and vascular niches [15]. Thus, effective approach for drug delivery to the lymphoma BMI is to target the unique features in the bone marrow vasculature.

Aptamers are single strand DNA or RNA sequences with unique 3-dimensional structures that are capable of recognizing and binding to their targets with high affinity. With a technique called systematic evolution of ligands by exponential enrichment (SELEX) [18,19], aptamers can be easily selected from a pooled oligonucleotide library towards defined targets. By screening aptamers based on protein or cells *in vitro*, a series of aptamers have been identified on lymphoma targeting and therapies [20–26]. However, the

composition and spatial arrangement of abnormal microenvironment in bone marrow induced by lymphoma may provide an extra shield to hide the designated targets, and make them unreachable. Furthermore, aptamers cross-binding to blood components, which may cause the failure of the aptamer candidates, will be quickly eliminated during blood circulation.

Alternatively, *in vivo* SELEX in live animal, which a library was injected into a murine model of disease, and then organs or cells of interest were harvested for aptamer selection, was applied to select organ specific aptamers [26–28]. Although the actual protein or cell targets probably stays unknown, selected aptamers are more likely able to bind to the indicated organ and accumulate thereupon. Furthermore, the selected aptamer may serve as delivery guidance of drugs or diagnosis probes due to its natural homing ability.

In this study, live animal based SELEX technique was applied to isolate thioaptamers against Burkitt's lymphoma. To identify thioaptamers with enhanced affinity to bone marrow involvement of Burkitt's lymphoma, a DNA thioaptamer library, in which thiol modification ensures the oligo stability *in vivo* [29], was injected to mice with Raji lymphoma BMI *in vivo*, and the bone marrow was collected for thioaptamer screening. After 10 rounds of selection, several thioaptamer candidates were selected for validation of bone homing ability. Accumulation in healthy bones was also tested and compared. One of the candidates was found highly interacted with the endothelial cells in bone marrow, and the uptake depended on the presence of lymphoma, which suggested a drug recruitment in diseased tissues. After conjugation with liposome, the thioaptamer successfully promoted the accumulation of doxorubicin in femur, tibia and spine with lymphoma involvement.

## MATERIALS and METHODS

### Cell culture

Human Burkitt's lymphoma cell lines Raji and Daudi, human T-anaplastic large cell lymphoma cell line KARPAS 299 (K299), human mantle cell lymphoma cell line Mino, acute monocytic leukemia THP-1 and non-small cell lung cancer cell line H358 were cultured in RPMI 1640 (Corning, USA) supplemented with 10% fetal bovine serum (FBS, GIBCO, USA) and 100 U/mL penicillin-streptomycin. Raji cells were transduced with a Plenti6/V5-DEST-luciferase lentivirus and selected in 3  $\mu$ g/mL blasticidin (InvivoGen, USA) to establish luciferase-expressing clones (Raji/Luc). Human MDA-MB-231 breast cancer cells were maintained in Dulbecco's modified eagle medium (DMEM, Corning, USA) with 10% FBS and 100 U/mL penicillin-streptomycin. Human umbilical vein endothelial cells (HUVEC) were obtained from PromoCell (Germany) and maintained in Medium 200 with low serum growth supplement (GIBCO, USA). All cell cultures were maintained at 37°C with 5% CO<sub>2</sub>.

### Murine models of human Burkitt's lymphoma bone marrow involvement

All animal experiments were performed in accordance with a protocol approved by the Institutional Animal Care and Use Committee (IACUC) of Houston Methodist Research Institute in Houston, Texas. To generate murine models of Burkitt's lymphoma, each of the

6–10 week old female SCID/beige mice (Charles River Laboratories) was inoculated with  $1 \times 10^6$  Raji/Luc cells by tail vein injection. Tumor growth was monitored with a Xenogen IVIS-200 imaging system. All mice developed bone marrow involvement two weeks later, and lymph node enlargement was detected in half number of them. Mice with intensive luciferase signals from the femur, tibia and spine 3 weeks after inoculation were applied for *in vivo* SELEX. Mice with similar tumor growth status were grouped randomly for *ex vivo* and *in vivo* biodistribution studies.

### Preparation of duplex thioaptamer library

A library of random single strand DNA (ssDNA) oligonucleotides without backbone modifications was obtained from The Midland Certified Reagent Company (Midland, TX). This library consisted of a 30 base pair random region flanked by a 21 base 5'-primer (5'-CGCTCGATAGATCGAGCTTCG-3') and a 23 base 3'-primer (5'-GTCGATCACGCTCTAGAGCACTG-3'). To synthesize a duplex thioaptamer library, the ssDNA random library was annealed with a reverse primer and incubated with Taq DNA polymerase and a mixture of dATP, dTTP, dCTP, and dGTP (800  $\mu$ M each) for 5 hours at 37 °C to synthesize the reverse strand. The library (500 nM) was then amplified by PCR using forward primer (400 nM), 5'-biotinylated reverse primer (400 nM), MgCl<sub>2</sub> (2.5 mM), Taq DNA polymerase (5 units) and a mixture of  $\alpha$ S-dATP, dTTP, dCTP, and dGTP (300  $\mu$ M each). PCR was run for 20 cycles (94 °C for 1 min, 59 °C for 1 min, and 72 °C for 1 min). This resulted in a library containing monothiophosphate substitutions on the 5' side of every dA residue except for those in the forward and reverse PCR primers. PCR amplification was repeated using the selected ssDNA oligonucleotides following each selection cycle. PCR products were filtered through a Millipore YM-30 filter to remove excess reagents and isolate dsDNA product. The dsDNA product was combined with streptavidin coated magnetic beads in a buffer containing 10 mM Tris-HCl, 2M NaCl, and 1 mM EDTA (pH 7.5) and was incubated for 15 min. Biotin on the reverse strand of the dsDNA binds to the streptavidin beads. The beads were washed 3 times with buffer to remove any unbound DNA. Melting solution (0.1 M NaOH) was then added to separate the two DNA strands. Biotinylated reverse strands remained bound to the beads while the nonbiotinylated forward strands were collected in the supernatant. The forward strands were filtered through Millipore YM-10 filter and collected for selection rounds.

### *In vivo* SELEX for lymphoma-homing thioaptamers

To initiate *in vivo* SELEX, a library of 10  $\mu$ g thioaptamers was injected via tail vein into SCID/beige mice with Raji lymphoma. Mice were sacrificed 4 hours later, and femur and tibia were flushed with PBS to collect bone marrow and lymphoma cells. Cell-bound thioaptamers were isolated and applied to generate a mini-library for the next round *in vivo* SELEX screening. After 10 rounds of *in vivo* SELEX enrichment, cell-bound thioaptamers were PCR amplified using normal dNTPs with extended primers that contained one of the three short additional sequences (bar codes) on one of the primers, and the resulting sequence mixture was sent to SeqWright Genomic Services for next generation sequencing. The fastq file was analyzed using the Aptaligner software and a library design file [30]. Bottom-up clustering of the top 250 aptamers was automatically performed with the

Aptaligner software. Structure predictions for the aptamers were determined with Mfold [31].

### Synthesis and purification of individual thioaptamers

Individual thioaptamers-of-interest were synthesized on an Expedite 8909 Oligo Synthesizer using standard phosphoramidite chemistry and manufacturer-recommended monomer coupling times, as previously described [29]. Deprotection of dye-labeled thioaptamers was conducted for 24 hours at room temperature with ammonium hydroxide to preserve the dye. All thioaptamers were purified by reverse phase chromatography on a semi-prep scale Hamilton PRP-1 column running on an AKTA-10 purifier system (GE) at a flow rate of 2 ml/min. They were loaded in 100% Buffer A (100 mM triethylamine acetate, pH 8.4, TEAA), stepped up to 8 to 12% Buffer B (acetonitrile), and eluted with increasing Buffer B gradient at the rate of 1% per 3–4 minutes up to ~25–30%. The fractions corresponding to well-resolved thioaptamer peaks were analyzed with 15% polyacrylamide gel electrophoresis to determine their purity and integrity prior to pooling and concentration by freezing drying or centrifugation in Amicon 3kD WMCO filters. The final concentrations of thioaptamer solutions and dye labeling efficiencies were determined spectrophotometrically by measuring OD at 260nm (DNA) and 650 nm (Cy5), and using calculated extinction coefficients (OligoCalc at Northwestern University) for the thioaptamers and values for the dyes suggested by the Glen Research website [32].

### Binding specificity of thioaptamer to bone marrow cells

Bone marrow cells were prepared to determine binding specificity of selected thioaptamers to different cell types. Briefly, femur and tibia were collected from mice with Raji lymphoma and sheared into small pieces. The tissue samples were digested with 250 unit/mL collagenase type III (Worthington Biochem, USA) at 37°C for 2 hours to prepare single cell suspension. Cells were incubated with 25 nM Cy5-thioaptamer at 37 C for 20 minutes, and then stained with cell specific antibodies from Tonbo Biosciences (USA) or Biolegend (USA) on ice for 30 minutes (T cell: CD45<sup>+</sup>/CD3<sup>+</sup>, B cell: CD45<sup>+</sup>/B220<sup>+</sup>, Raji cell: HLA-ABC<sup>+</sup>, endothelial cell: CD45<sup>-</sup>/CD31<sup>+</sup>, macrophage: CD11b<sup>+</sup>/F4/80<sup>+</sup>/Ly6G<sup>-</sup>, granulocyte: CD11b<sup>+</sup>/Ly6G<sup>+</sup>). All antibodies were 1:100 diluted in PBS containing 2% FBS. Thioaptamer binding potency was measured using a BD LSR Fortessa analyzer and analyzed with the Flowjo 7.6.1 software (Tree Star, USA).

### Uptake of thioaptamer by vascular endothelial cells

To analyze thioaptamer-binding affinity to endothelial cells, 1×10<sup>4</sup> HUVECs were seeded in a 48-well plate and cultured overnight. On the next day, thioaptamers were added into cell culture and cells were kept incubated for another 20 minutes before they were detached from plate with 20 mM EDTA and analyzed with flow cytometry. To identify route of cell entry by the thioaptamer, HUVEC cells were co-incubated with the following inhibitors before co-culture with thioaptamer: cytochalasin D (phagocytosis inhibitor, 100 μM, MP Biomedicals), amiloride (macropinocytosis inhibitor, 500 μM, Sigma-Aldrich), chlorpromazine (inhibitor of clathrin mediated endocytosis, 10 μM, 20 μM, 30 μM and 60 μM, MP Biomedicals), genistein (inhibitor of caveolae mediated endocytosis, 100 μM, Sigma- Aldrich) and dynasore (inhibitor of dynamin-dependent endocytosis, 100 μM, 300 μM and 500 μM,

ApexBio Technology). After a 30-minute treatment with the inhibitors, cells were mixed with 12.5 nM of the R1 thioaptamer (R1) and incubated for 20 minutes before they were harvested for flow cytometry analysis. All samples for flow cytometry analysis were prepared in triplicate.

The above procedure was also applied to HUVECs that were activated with conditioned media (CM) for 6 hours. Due to the high binding affinity after stimulation, HUVECs were incubated with a reduced concentration (1 nM) of the R1 thioaptamer. For the competition assay, a 50-fold excess of non-labeled R1 was mixed with Cy5-R1 before incubation with HUVECs. To visualize intracellular trafficking of thioaptamer, cells were seeded in an 8-well chamber slide cell culture system, and then incubated with the thioaptamer (100 nM for naive HUVECs, or 5 nM for activated HUVECs). They were then fixed with 10% phosphate buffered formalin and permeabilized with 0.1% triton X-100. Anti-EEA1 (early endosome marker), anti-Rab7 (late endosome marker) and anti-LAMP1 (lysosome marker) antibodies (Abcam, UK) were 1:300 diluted and incubated with HUVECs overnight at 4°C, followed by incubation with an AlexaFluor-488 conjugated secondary antibody (1:400 dilution, Life Technologies). Images were captured with a Nikon Eclipse 80i fluorescent microscope.

### Impact of cell conditioned medium on thioaptamer uptake by vascular endothelial cells

Conditioned media from bone marrow cells isolated from tumor-free SCID/beige mice (4 million cells per mL) and tumor cells (0.5 million cells per mL) were applied to supplement HUVEC growth before cells were used to test thioaptamer binding. Briefly, HUVECs were grown in fresh RPMI-1640 medium either without CM supplement or supplemented with tumor CM (CM<sub>T</sub>), bone marrow CM (CM<sub>BM</sub>) or a mixture of CM<sub>T</sub> and CM<sub>BM</sub> at a 1:1 (v/v) ratio for 6 hours or otherwise indicated. Cells were washed with PBS and then incubated for 20 minutes with 12.5 nM R1 aptamer in a binding buffer containing 1 mg/mL bovine serum albumin (BSA), 4.5 mg/mL glucose, 0.1 mg/mL yeast t-RNA, and 5 mM MgCl<sub>2</sub> in PBS. R1 uptake by HUVECs was assessed with a BD Accuri C6 flow cytometer. All samples were run in triplicate.

### Preparation and characterization of thioaptamer-conjugated liposomal doxorubicin (Dox)

*Thioaptamer conjugation:* R1 or a control thioaptamer was chemically conjugated to the distal end of 1,2-distearoyl-sn-glycero-3-phosphoethanolamine-N-[maleimide(polyethylene glycol)-2000 (DSPE-PEG-Mal, Avanti Polar Lipids, USA) via reaction of thiol with maleimide group (R1-lipid or Ctrl Apt-lipid, respective). Briefly, thioaptamers with a 5' thiol group (Integrated DNA Technologies, USA) were treated with tris(2-carboxyethyl)phosphine hydrochloride (TCEP, Thermo Fisher Scientific, USA) to convert any disulfide aptamer dimers back into thiol monomers, and then mixed with DSPE-PEG-Mal micelle in PBS (pH7.0, 50 mM) at room temperature overnight with gentle shaking.

*Liposomal Dox preparation:* Dox-loaded long circulating liposomes were prepared by following a previously described ammonium sulfate gradient method [33]. Briefly, 1,2-dipalmitoyl-sn-glycero-3-phosphocholine (DPPC), cholesterol, 1,2-distearoyl-sn-glycero-3-phosphoethanolamine-N-[methoxy(polyethylene glycol)-2000 (DSPE-PEG2000) (Corden Pharma International GmbH, Germany) and the above thioaptamer-micelle (in aqueous solution) were mixed at the molar ratio of 63:32:4.5:0.5. The mixture was lyophilized to

remove solvent. Lipid powder was then hydrated with 150 mM ammonium sulfate and sonicated until clear. Unencapsulated ammonium sulfate was removed by dialysis against 1 L 20 mM HEPES buffered saline (pH 7.4) for 4 hours in a dialysis tubing with 10,000 Da molecular weight cut off (Thermo Fisher Scientific, USA). Next, Dox was added into empty liposomes at a drug-to-lipid ratio of 1:10 (w/w) and incubated at 60 °C for 1 hour with gentle shaking. Unencapsulated Dox was removed by dialysis as described above.

*Liposomal Dox characterization:* To calculate drug-loading efficiency, a 2-fold (Vol.) 1% triton X-100 in methanol was added to the liposomes, and Dox content was measured based on absorbance at 480 nm. Dynamic light scattering (DLS) measurement with a Zetasizer Nano ZS (Malvern, UK) was applied to monitor size distribution of the liposomes.

### **Biodistribution of thioaptamers and bone marrow-targeted liposomal doxorubicin**

To determine biodistribution and bone marrow-homing efficiency of selected thioaptamers, each mouse with Raji lymphoma was treated *i.v.* with 0.5 nmol Cy5-labeled thioaptamer (n = 3–4 mice/group). Mice were euthanized 4 hours post injection, and major organs including the bone were collected. Thioaptamer content in each organ was quantified based on fluorescent intensity from Cy5 with an IVIS-200 imaging system. Thioaptamer distribution in the femur and tibia was further evaluated based on immunohistochemical staining. Briefly, tissue samples were fixed in 10% formalin overnight, decalcified with phosphate buffered 500 mM ethylenediaminetetraacetic acid (EDTA, pH 7.4) and processed for tissue staining with an anti-mouse E-selectin antibody (Abcam, USA). Unlike endothelial cells in other organs, one of the important features of bone marrow endothelial cells is the constitutive expression of E-selectin [34,35].

To determine biodistribution of bone marrow-targeted liposomal doxorubicin, SCID/beige mice with Raji (n = 4 mice/group) were treated *i.v.* with 6 mg/kg dox-equivalent thioaptamer-conjugated liposomal Dox. Mice were sacrificed 28 hours post drug treatment, and Dox was extracted from blood and major organs. Dox content was analyzed by high performance liquid chromatography (HPLC) with a Zorbax 300SB-C18 reverse phase column (Agilent, USA) and a fluorescence detector (Hitachi LaChrom Elite, Japan), and daunorubicin was used as an internal standard [36].

### **Statistical analysis**

Statistical analysis was performed with the GraphPad Prism 5 program (GraphPad Software, Inc, California, USA). Comparison between two values was evaluated with a two-tailed, unpaired Student's t-test. Pairs of values in multiple groups were analyzed by one-way ANOVA with Tukey's correction method. When comparing multiple values to a single value, such as negative control or R1, one-way ANOVA was used with Dunnett's correction for multiplicity adjustment. P <0.05 (\*) and P <0.01 (\*\*) indicated statistically significant and very significant, respectively. Data are expressed as means ± SD. Sample size was pre-determined based on preliminary results and the number of qualified mice.

## RESULTS

### ***In vivo* SELEX identifies lymphoma bone marrow involvement-enriched thioaptamers**

Lymphoma mice with BMI were systematically characterized before they were applied for *in vivo* SELEX. Intensive Raji/Luc tumor growth could be detected in the lymph nodes, spine, femur and tibia based on bioluminescence (Fig. 1A), and confirmed by histological analysis (Fig. 1B). Thioaptamers were enriched in the lymphoma-bearing organs after 10 rounds of *in vivo* SELEX (Fig. 1C), and four oligos (R1, R2, R3 and R4) with the highest level of bone marrow accumulation based on deep sequencing were listed (Fig. 1D). The thioaptamers were resistant to plasma deoxyribonuclease (DNase) digestion in an *in vitro* setting, and intact fragments could still be detected by gel electrophoresis after more than 7 hours of incubation in peripheral blood (Supplementary Fig. 1). Inside the body, high plasma R1 concentration was maintained within the first hour (Supplementary Fig. 2).

Biodistribution analysis was performed to confirm enrichment of the selected thioaptamers in lymphoma with BMI. Overall, all 4 thioaptamers accumulated more in the relevant organs (spine, femur, tibia) comparing to the negative control (Fig. 2A). In addition, high thioaptamer concentration was detected in kidney, indicating a rapid renal clearance due to their relatively small size (24 kD molecule weight) and high solubility (Fig. 2A-B). Quantitative analysis revealed high enrichment in the spine (2.6 folds and 2.3 folds, respectively) and femur and tibia (3.4 folds and 2.6 folds, respectively) by R1 and R4 over the control thioaptamer (Fig. 2C). R1 also displayed a preference to the disease over the healthy organs (Fig. 2A), and its level was elevated by 2.3 folds in the spine and 1.8 folds in the femur and tibia in lymphoma mice over lymphoma-free mice (Fig. 2D). Although R2 and R3 also accumulated in lymphoma with BMI, the degree of enrichment was not as significant as R1 and R4, a result confirmed by histological analysis (Fig. 2E).

### **Thioaptamers bind to bone marrow endothelium with high affinity and specificity**

There exist multiple cell types inside the bone marrow in a lymphoma-bearing mouse including adipocytes, endothelial cells, fibroblasts, leukocytes, osteoblasts and osteoclasts. In order to identify cells that preferentially interacted with the thioaptamers, we treated lymphoma mice with Cy5-labeled thioaptamers, and analyzed cell populations from spine, femur and tibia. While Raji cells and the hematopoietic cells did not show a significant binding to the thioaptamers, a large number of endothelial cells were associated with the thioaptamers, especially with R1 (Fig. 3A), indicating that the bone marrow endothelium might be the target for the thioaptamers.

We measured thioaptamer-binding affinity to HUVEC, an endothelial cell lines that has been widely used in endothelium-related studies [37]. R1 had the highest binding affinity to HUVECs with an equilibrium dissociation constant (Kd) of 3 nM, while R2 had a moderate binding affinity (Kd =13.8 nM), and other two aptamers showed weaker binding to the cells with bind affinities above 50 nM (Fig. 3B). Consistent with the binding assay results, fluorescent imaging revealed that R1 had the strongest interaction with HUVECs among all 4 thioaptamers (Fig. 3C, 3D). In addition, R1 binding did not trigger HUVEC cell death (Supplementary Fig. 3). Thus, R1 was chosen for all further studies.



### **R1 enters endothelial cells through clathrin-mediated endocytosis**

Cy5-labeled R1 (Cy5-R1) was incubated with HUVECs, and cell uptake of the thioaptamer was monitored. The red fluorescent Cy5-R1 could be co-localized with the EEA1-positive early endosomes (in green) 30 minutes after incubation (Fig. 4A), indicating that the thioaptamer entered endothelial cells through the vesicular transport system. Between the 1h and 3 h time points, we observed increasing separation of the red Cy5-R1 from the green early endosomes, and most red fluorescent Cy5-R1 dots did not co-localize with the Rab7-positive late endosomes or LAMP1-positive lysosomes (Fig. 4A), suggesting that the thioaptamers had gradually left vesicles and entered the cytosol. To identify routes of R1 internalization, we pre-treated HUVECs with inhibitors of different cell entry pathways followed by aptamer co-incubation. R1 uptake by HUVECs was significantly blocked by the clathrin-mediated endocytosis inhibitors dynasore and chlorpromazine, but not affected by inhibitors of phagocytosis (cytochalasin D), macropinocytosis (amiloride) or caveolar-mediated endocytosis (genistein) (Fig. 4B).

### **Tumor and stromal cell-secreted factors promote R1 binding by endothelial cells.**

We have previously shown that, inside the tumor-growing bone marrow, tumor cell-secreted inflammatory cytokines promote expression of endothelial cell surface proteins, such as E-selectin, which serve as docking sites for targeted delivery of drug particles to the bone [38]. In order to determine whether R1 binding to and uptake by endothelial cells could also be modulated in a lymphoma BMI microenvironment, we incubated HUVECs with bone marrow cell conditioned medium (BM CM), Raji cell conditioned medium (Raji CM), or a mix of BM CM and Raji CM, and measured R1-HUVEC binding affinity. BM CM or Raji CM alone only had a low to moderate effect on R1 binding. Surprisingly, R1 binding was dramatically enhanced by HUVECs pretreated with a mixture of BM CM and Raji CM (Fig. 5A). In addition, the ratio between the two CM had an impact on R1 binding, with an equal ratio providing the highest capacity (Fig. 5B).

To determine whether enhanced aptamer binding capacity was Raji cell-specific, we collected conditioned media from a group of malignant cells including lymphoma, leukemia and solid tumor cells, and mixed them individually with BM CM to treat HUVECs. We observed dramatically enhanced HUVEC binding of the R1 aptamer in media from 3 of the 4 lymphoma cell lines (Raji, K299, and Mino); in comparison, media from the 2 epithelial tumor cell lines (MDA-MB-231 and H358) or one leukemia cell line (THP-1) did not have a comparable effect (Fig. 5C). Thus, enhanced R1 binding by endothelial cells is promoted by lymphoma cell-derived factors only. In addition, binding of the Cy5-labeled R1 aptamers (Cy5-R1) to HUVECs could be blocked by an excessive amount of unlabeled R1 aptamers (Fig. 5D).

### **R1 serves as an affinity-targeting moiety for lymphoma BMI-specific drug delivery.**

Lymphomas are traditionally treated with cytotoxic chemotherapy drugs such as the R-CHOP containing rituximab, cyclophosphamide, doxorubicin (Dox), vincristine and prednisone [39]. However, heart accumulation of Dox induces severe cardiac toxicity, which limits the overall life time dosage a patient can receive for the drug. The unique binding specificity from R1 to the tumor endothelium indicates that the thioaptamer may serve as an

affinity moiety for targeted delivery of therapeutic agents to lymphoma BMI, which not only changes the overall biodistribution pattern of the therapeutic agent but also reduces dosage needed for cell killing activity.

A lymphoma BMI-targeted liposomal Dox (R1-lipo Dox) and a control liposomal Dox formulation (Ctrl-lipo Dox) were prepared by incorporating the R1 or 0tamer-conjugated lipid in the formulation. The average size of liposomes from both formulations was similar (R1 Apt-Dox liposome: 116.7 nm; Ctrl Apt-Dox liposome: 115.2 nm), and both had a narrow polydispersity index (PDI) (Table 1). With an active remote loading technique [40], over 90% of Dox was encapsulated in the liposomes. Comparing to Ctrl-lipo Dox, R1-lipo Dox bound to activated HUVECs with a much higher affinity (Fig. 6A). Drug formulation did not compromise nuclear accumulation of the active drug ingredient. In cell culture, the red Dox molecules co-localized with the green fluorescent R1 aptamer within the first 30 minutes (pointed with a yellow arrow). Nuclear accumulation of Dox could be visualized at the 1 hour time point, and red fluorescence from Dox in the nuclei was even stronger 3 hours after incubation (Fig. 6B).

Pharmacokinetics and biodistribution of the R1 -lipo Dox and Ctrl-lipo Dox were compared in SCID/beige mice with Raji lymphoma. Comparing to Ctrl-lipo Dox, the R1 -lipo Dox showed a faster distribution phase and a similar elimination phase (Table 1, Fig. 6C). Biodistribution in the major organs was similar between the two formulations; however, the bones with lymphoma involvement received a significantly higher level of drug in mice treated with R1-lipo Dox over those with Ctrl-lipo Dox. There was a 2 to 3 fold enhancement in spine, femur and tibia in mice treated with R1 -lipo Dox (Fig. 6D).

## DISCUSSION

Aptamers are short oligonucleotides with low immunogenicity and toxicity, and can be manipulated in large scale with simplicity. In addition, the high diversity of sequences and related structures provide a very large pool to screen for ligands that bind targets with high affinity and specificity. Thus, aptamers are emerging diagnostic and therapeutic agents for clinic applications [26,41,42]. Pegaptanib (Macugen™ from Pfizer) is the first aptamer-based drug approved by the Food and Drug Administrations in the United States. It is a single stranded aptamer that binds to the vascular endothelial growth factor with specificity, and is used to treat age-related macular degeneration [43]. The thioaptamers used in the current study contain monothiophosphate substitutions on the 5' side of every dA residue in the sequence, which provides more resistance to the plasma and tissue DNases comparing to the conventional aptamers [44] [45].

Lymphoma is a group of heterogeneous diseases consisting of more than 60 different subtypes, and the interaction and regulation of the components in the tumor microenvironment are diverse and complicated [46,47]. Depending on their unique characteristics, lymphoma cells may either hide behind normal tissues or efface normal tissues due to abnormally fast growth and autonomous survival [48], which is the case in the murine model of Raji Burkitt's lymphoma. Infiltrating leukocytes, endothelial cells, fibroblasts, adipocytes and extracellular matrix are all actively participating in the cross-

regulation process with lymphoma cells. On one hand, it raises the requirement of therapeutic strategy that not only kills the cancer cells, but also conquers the dysfunction of stromal cells. On the other hand, it provides a unique environment that differs from healthy tissues for targeted drug delivery. In this study, we have identified a thioaptamer that preferentially binds the vascular endothelium in bone marrow with lymphoma over the healthy medullary cavity. We have also demonstrated the feasibility of applying R1 as an affinity moiety to achieve lymphoma BMI-targeted delivery of doxorubicin, a chemotherapy drug that is commonly applied in lymphoma treatment but may cause severe toxic side effects [49]. Targeted delivery of the drug may provide the benefit of enhanced therapeutic efficacy with significantly reduced toxicity, as we have recently shown in solid epithelial tumors [36].

Our study has indicated that R1 binding to the inflammatory endothelium is subjected to regulation by soluble factors secreted by both endothelial and lymphoma cells. Although the identity of such factors is not known, it is highly likely that a group of cytokines and chemokines are involved in the process. To support this notion, we have revealed that E-selectin is overexpressed by the vascular endothelial cells in a tumor microenvironment [38]. A group of tumor and stromal cell-secreted cytokines can promote E-selectin expression, such as TNF- $\alpha$  and interleukin-1  $\beta$  [50]. Since neither conditioned medium from the bone marrow cells and lymphoma cells could provide the strongest R1 binding to HUVEC (Fig. 5), expression of the cell surface docking protein must be regulated by a combination of factors from both media.

In conclusion, we have successfully isolated a novel thioaptamer that can be applied for drug enrichment to lymphoma BMI. R1 preferentially binds to endothelial cells, and R1-endothelium interaction is enhanced when the vascular endothelial cells are stimulated by a combination of factors secreted from the lymphoma and stromal cells. In a proof-of-principal study, we have applied R1 as an affinity moiety to develop a lymphoma BMI-targeted drug formulation, and successfully demonstrated drug enrichment in the malignant tissues. This thioaptamer should provide a powerful tool in the development of effective treatments for lymphoma BMI.

## Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

## Acknowledgments

Financial support: This work was supported by National Cancer Institute grants 1R01CA193880-01A1 (HS), U54CA151668 (MF and DG), U54CA210181 (MF), and Department of Defense grant W81XWH-12-1-0414 (MF). MF is an Ernest Cockrell Jr. distinguished endowed chair.

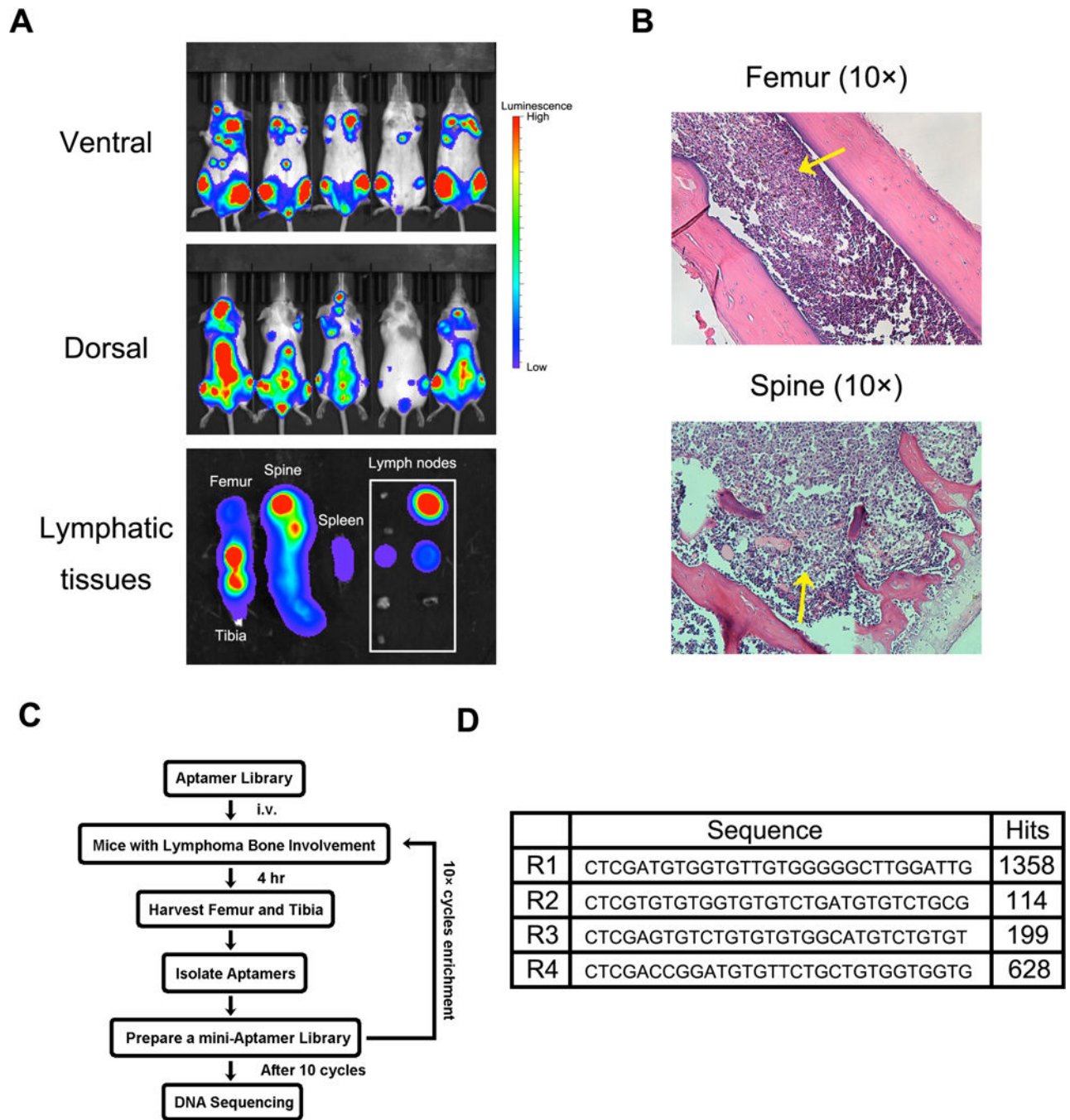
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**Figure 1:** Murine model of human Burkitt’s lymphoma with bone marrow involvement for in vivo SELEX of aptamer. (A). Growth of Raji cells with luciferase gene in SCID/Beige mice was monitored by an Xenogen IVIS-200 system. Pictures were taken on both ventral and dorsal sides. The ex vivo images showed lymphoma in lymphatic tissues (femur, tibia, spine, spleen and lymph nodes). Lymphoma cells widely invaded into bones and lymph nodes, but less were observed in spleen. (B). Histological analysis of Raji lymphoma in medullary cavities

of spine and femur. Raji cells invaded into bone marrow and effaced normal tissues. Yellow arrows indicate the tumor nodules. (C). Schematic diagram of in vivo SELEX process.

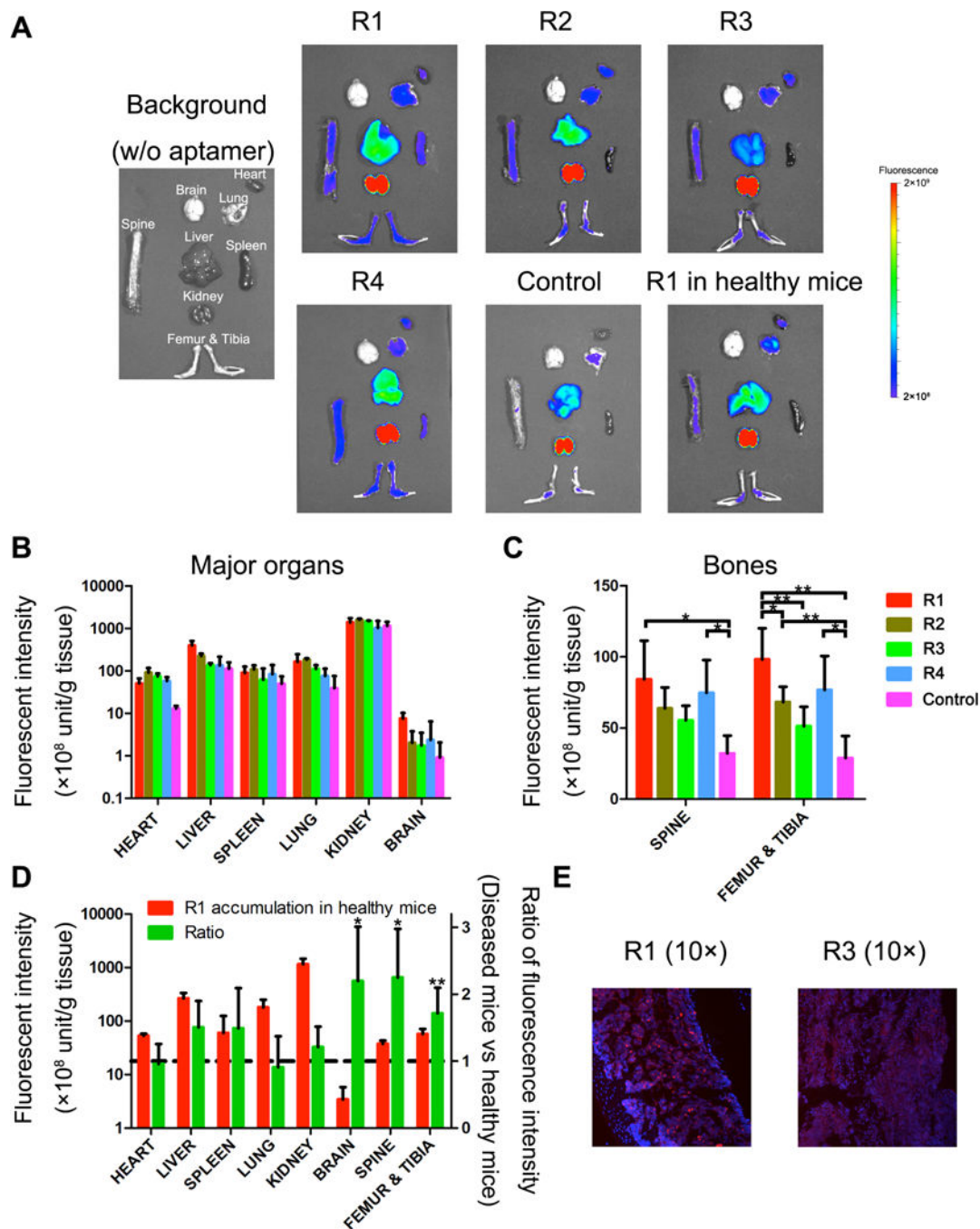
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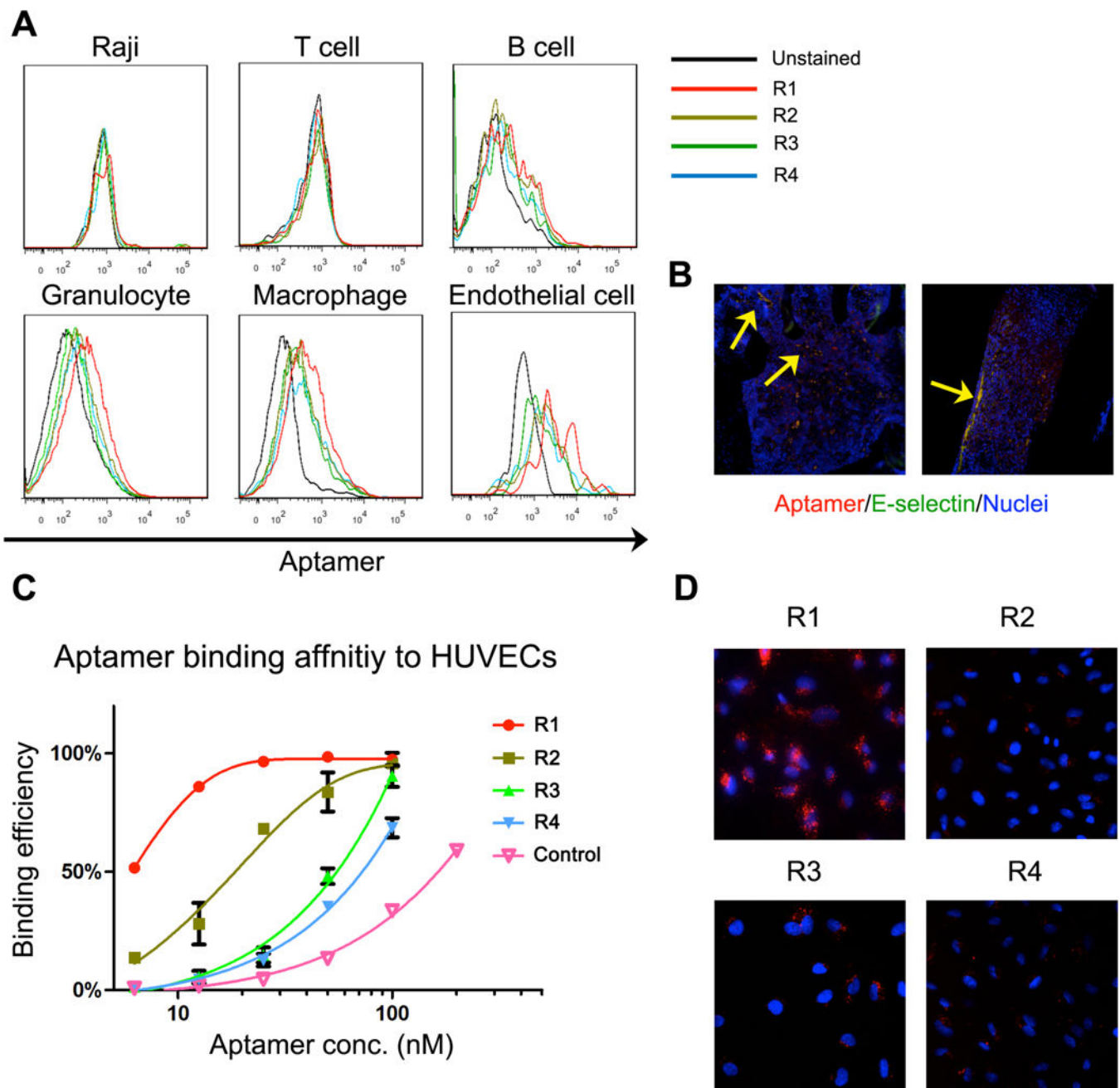
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**Figure 2.** Accumulation of Cy5-aptamers in major organs. Aptamers selected from in vivo SELEX and control aptamers were intravenously injected into mice with Raji lymphoma BMI (0.5 nmol per mouse, n=3–4). Mice were sacrificed 4 hours post injection, and tissues of interest were collected for fluorescence analysis of aptamer content. R1 was also dosed to healthy mice, and mice without aptamer administration were measured for adjustment of figure setting and subtraction of autofluorescence background. (A). Representative figures of fluorescence imaging. Fluorescence intensity of soft organs (B) and bones (C) ex vivo were

quantified and plotted. Data were normalized by weight of the organs. (D). Fluorescent signals on healthy mice and diseased mice were compared. Left Y-axis: Fluorescence intensity, right Y-axis: ratio of aptamer in diseased mice versus healthy mice. (E). Histological analysis of Cy5-R1 and Cy5-R3 aptamers in the bone marrow of femur samples. Red: Cy5 labeled aptamer, Blue: DAPI stained nuclei.



**Figure 3.** Identification of targeted cells of selected aptamers. (A). Representative figures of flow cytometry analysis. Bone marrow cells were stained with Cy5-aptamers, and different cell populations were isolated by flow cytometry for aptamer analysis. R1 aptamer was found bound to endothelial cells with higher affinity. (B) Distribution of R1 aptamer in bone marrow. Blood vessels were costained with E-selectin antibody. Yellow arrows indicated the binding of R1 on bone marrow endothelium (yellow spots). (C). Binding affinity of aptamers to HUVECs was evaluated by flow cytometry. R1 was able to bind to HUVECs with high

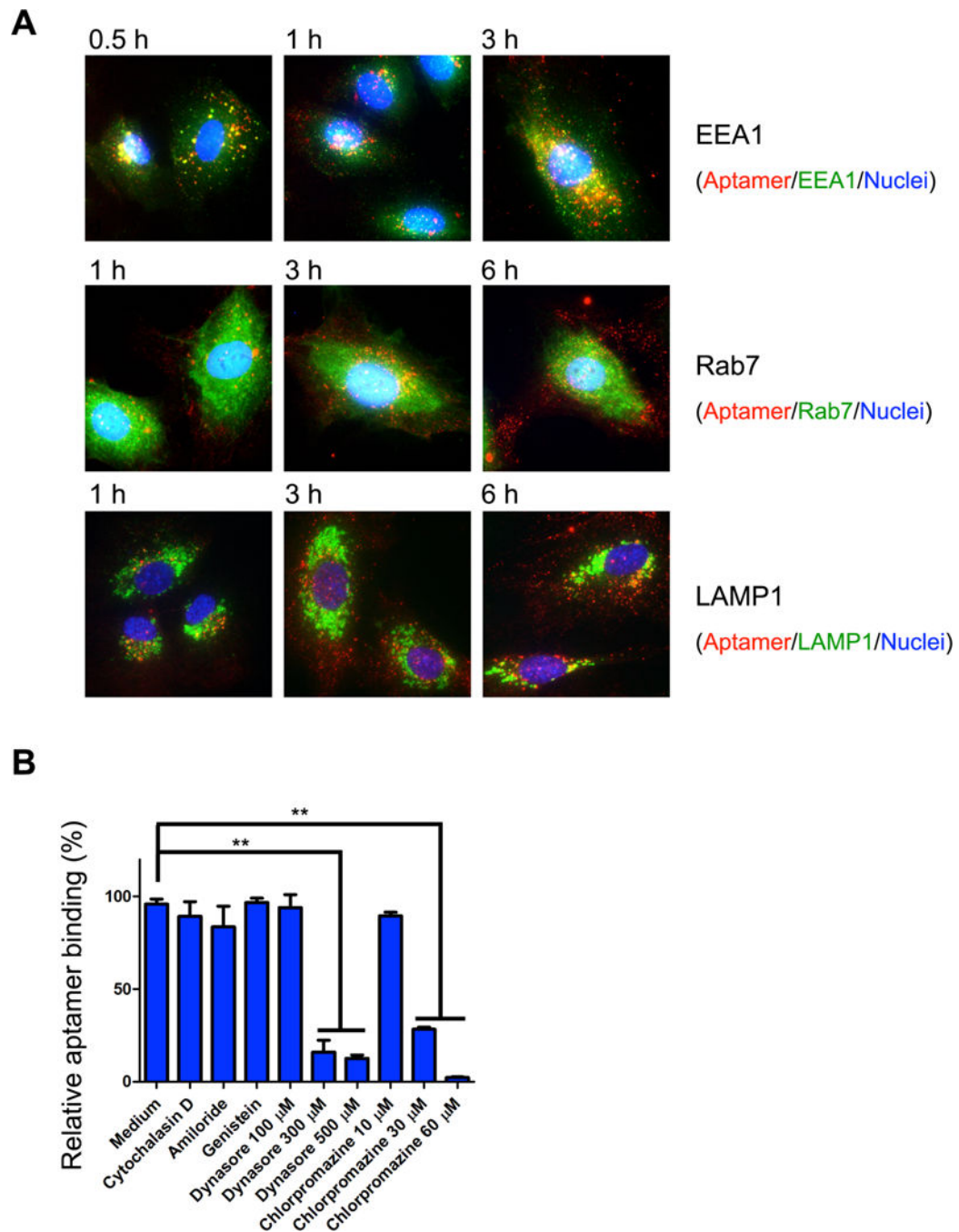
affinity. (D). Fluorescence microscope images of HUVECs with Cy5-aptamers. Red: Cy5 labeled aptamer, Blue: DAPI stained nuclei.

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**Figure 4.** Internalization of R1 aptamer in HUVECs. (A) HUVECs were incubated with Cy5-R1 aptamer, and then fixed and co-stained with EEA1 (early endosome marker), Rab7 (late endosome marker) or LAMP1 (lysosome marker) antibodies, in the top, middle, and bottom rows, respectively. Red: Cy5-R1 aptamer, Green: organelle markers (EEA1, Rab7 or LAMP1), Blue: DAPI stained nuclei. (B) Identification of internalization pathway. HUVECs were pre-treated with endocytosis inhibitors, and then incubated with Cy5-R1 aptamer. Dose

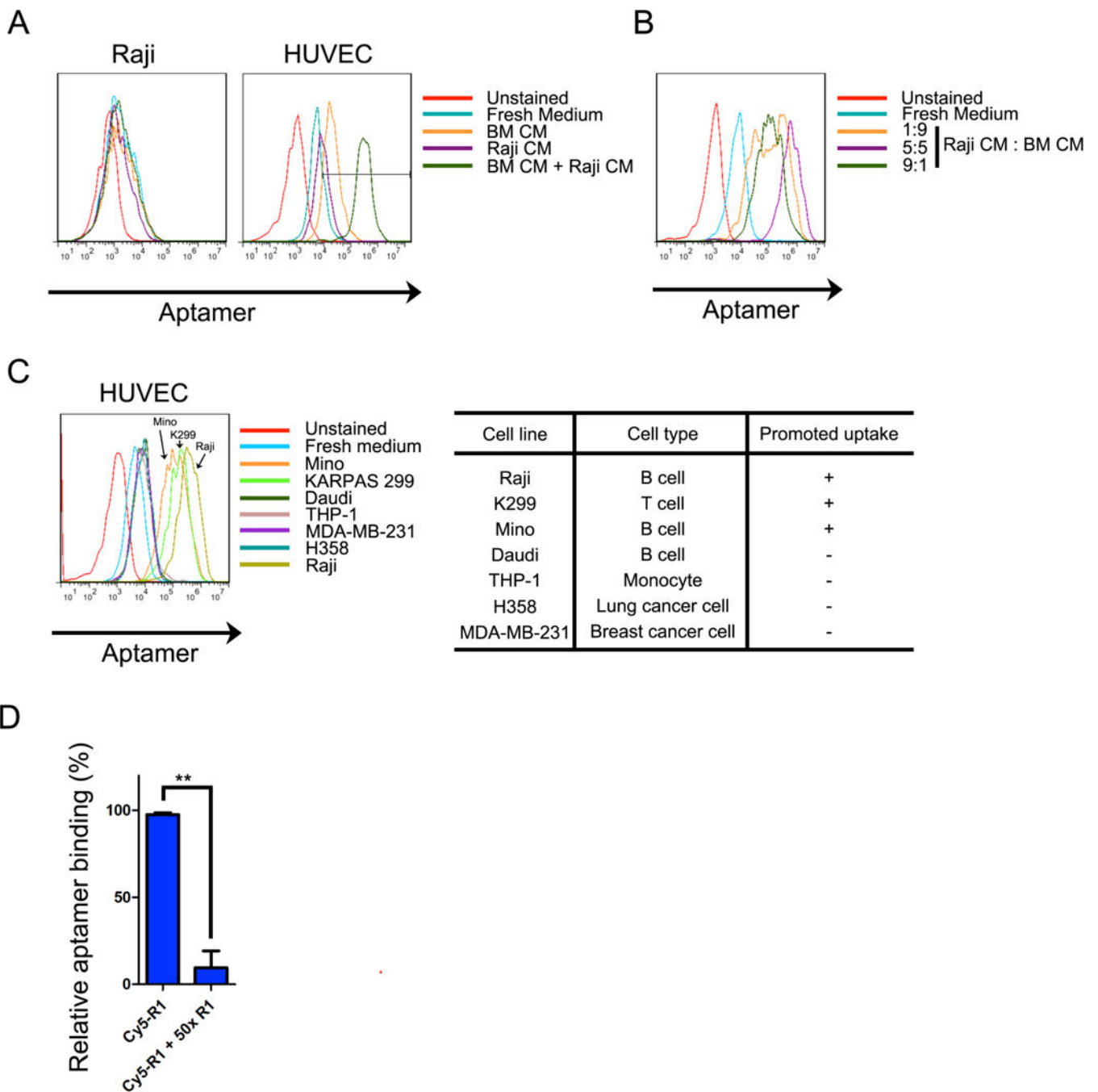
dependent attenuation of R1 uptake was found after chlorpromazine or dynasore pre-treatments, which indicated R1 uptake is mediated by the clathrin dependent pathway.

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**Figure 5.** Accelerated uptake of R1 aptamer on HUVECs treated with mixed Raji/BM CMs. (A). Raji or HUVECs were treated with Raji CM, BM CM or their mixture thereof prior to R1 incubation. R1 uptake was assessed with flow cytometry, and representative figures are shown. R1 uptake of HUVECs was enhanced with co-incubation of mixed Raji/BM CMs. Such phenomenon cannot be found in Raji cells. (B). Impact of CM mixture ratio. (C). Enhanced R1 uptake on HUVECs activated with BM CM and CMs from selected cells. Most of lymphoma CMs, but not myeloid leukemia or solid tumor cell lines, can accelerate

R1 uptake. (D) Internalization of R1 on CM activated HUVECs. HUVECs were stimulated by mixed Raji CM and BM CM, followed by R1 incubation for different periods. Cells were then co-stained with anti-EEA1 antibody to visualize early endosomes. (E) Identification of internalization pathways. Activated HUVECs were treated with different endocytosis inhibitors, and incubated with 1 nM Cy5-R1 afterwards. (F) Competitive inhibition of cellular uptake by flow cytometry. Binding of Cy5-R1 was measured with or without co-incubation of 50-fold non-labeled R1.

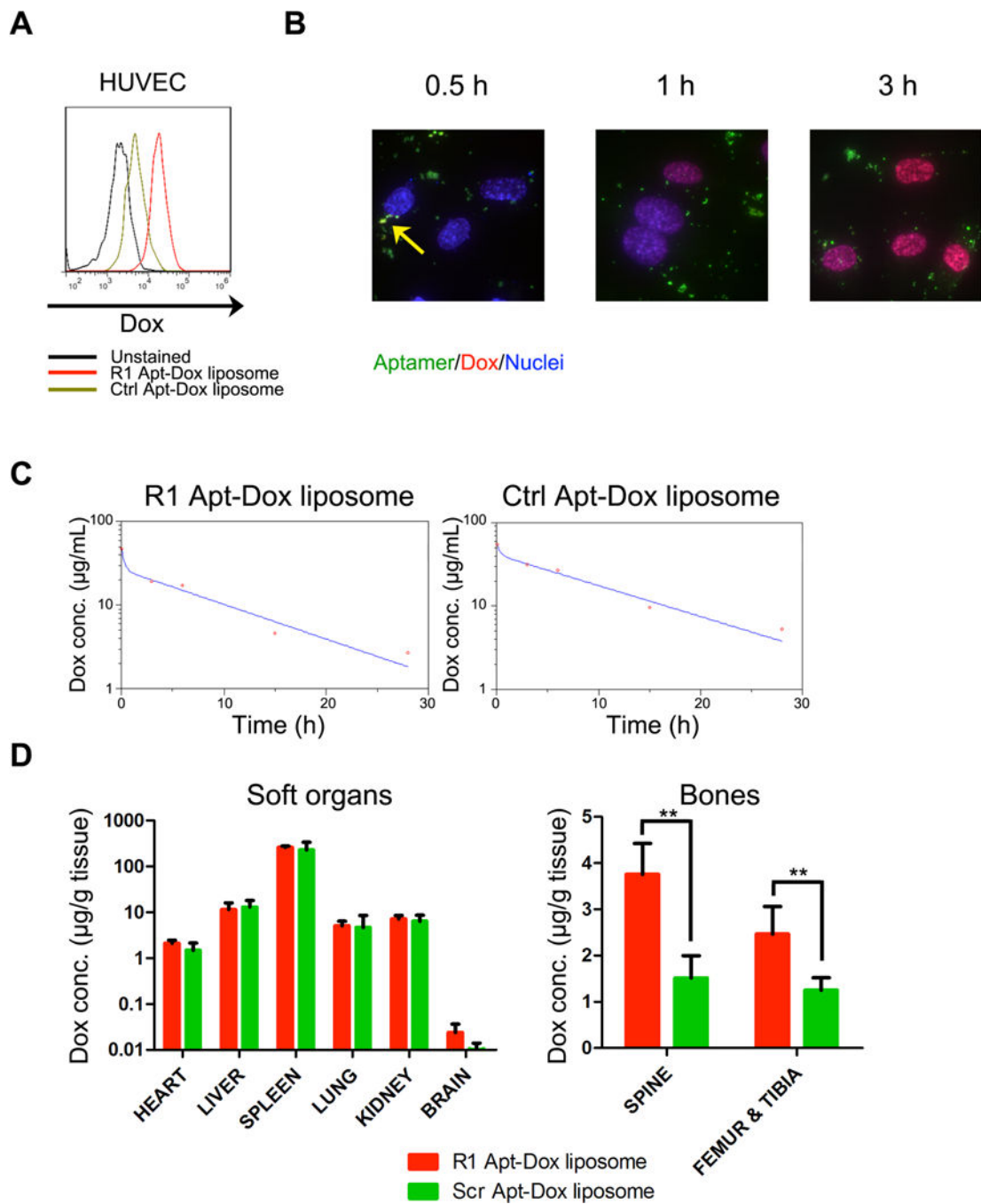
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**Figure 6.** Pharmacokinetics and biodistribution studies of R1 aptamer conjugated liposomal doxorubicin. Mice with lymphoma BMI were dosed with 6 mg/kg Ctrl Apt-Dox liposome or R1 Apt-Dox liposome (n=4). (A). Conjugation of R1 on liposomal Dox promotes uptake by HUVECs in vitro. (B) Intracellular trafficking and drug release of R1 Apt-Dox liposome. Time dependent Dox concentration in peripheral blood (C) and biodistribution of Dox content in soft organs and bones at 28 h post treatment (D) were analyzed.

**Table 1.**

Characterization of aptamer conjugated Dox liposome

	Size (nm)	PDI	LE	T <sub>1/2α</sub> (h)	T <sub>1/2β</sub> (h)	T <sub>1/2Kel</sub> (h)	AUC (μg h/mL)
R1	116.7 ± 1.1	0.250 ± 0.010	92.10%	0.181	7.25	3.99	284.6
Ctrl	115.2 ± 2.1	0.251 ± 0.029	96.70%	0.224	8.11	6.05	487.7