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## Genetically Encoded RNA-based Sensors for Intracellular Imaging of Silver Ions

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### Abstract

Silver has been widely used for disinfection. The cellular accumulation of silver ions  $(Ag^+)$  is critical in these antibacterial effects. The direct cellular measurement of  $Ag^+$  is useful for the study of disinfection mechanisms. Herein, we reported a novel genetically encoded RNA-based sensor to image  $Ag^+$  in live bacterial cells. The sensor is designed by introducing a cytosine- $Ag^+$ -cytosine metallo base pair into a fluorogenic RNA aptamer, Broccoli. The binding of  $Ag^+$  induces the folding of Broccoli and activates a fluorescence signal. This sensor can be genetically encoded to measure the cellular flux and antibacterial effect of  $Ag^+$ .

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A genetically encoded RNA-based sensor to measure the flux and antibacterial effect of silver ions in living cells.

## **Graphical Abstract**

Conflicts of interest There are no conflicts to declare



Silver has been applied for disinfection since the 1st century BC and is still widely used nowadays.<sup>1</sup> Compared with antibiotics that can always cause resistant pathogenic strains, silver is promising for the prevention and broad-spectrum treatment of infections.<sup>2</sup> Silver nanoparticles (AgNPs) are a popular type of nanomaterial in consumer products, with various applications in medical devices, surgical coating, textiles, dietary supplement, and water disinfection.<sup>3</sup> However, concerns have been raised over the toxicity of AgNPs on human health and environment.<sup>4,5</sup> It is critical to prepare AgNPs within proper therapeutic windows to improve both antibacterial efficiency and specificity.

The antibacterial effect of AgNPs is known to be largely correlated with the cellular accumulation of Ag<sup>+</sup>.<sup>1,6</sup> Silver ions can interact with the thiol groups in proteins and interfere with DNA replication to stop bacterial proliferation.<sup>7</sup> Several strategies have been developed for the *in vitro* measurement of Ag<sup>+</sup> using atomic spectroscopy,<sup>8</sup> inductively coupled plasma mass spectrometry,<sup>9</sup> potentiometry,<sup>10,11</sup> and fluorescence spectroscopy.<sup>12-14</sup> However, these *in vitro* assays cannot be used to measure the cellular concentrations of Ag<sup>+</sup>. Inside cells, Ag<sup>+</sup> can bind with proteins and nucleic acids, form precipitation or colloidal dispersion with halides and sulfides, and be actively pushed out by the efflux pumps.<sup>15</sup> Thus, intracellular level of Ag<sup>+</sup> could be quite different from that in the extracellular solution.

Herein, we report a genetically encoded RNA-based sensor to selectively image Ag<sup>+</sup> in live bacterial cells. Our sensor is developed based on a fluorogenic RNA aptamer, named Broccoli. Broccoli can specifically bind and activate a small molecule dye, (Z)-4-(3,5-difluoro-4-hydroxybbenzylidene)-1,2-dimethyl-1*H*-imidazol-5(4*H*)-one (DFHBI-1T).<sup>16</sup> Together with Spinach,<sup>17</sup> these fluorogenic aptamers have been widely used for RNA imaging in living systems.<sup>18</sup> Recently, we and others have engineered Spinach/Broccoli into selective sensors for imaging metabolites<sup>19-22</sup> and proteins.<sup>23</sup> These RNA-based sensors normally comprise three parts: Spinach/Broccoli, a target-binding aptamer, and a transducer

(Fig. S1a, ESI<sup> $\dagger$ </sup>). The target-binding aptamer is linked via transducer into a structurally critical H<sub>1</sub> helix of Broccoli (Fig. S1b, ESI<sup> $\dagger$ </sup>). The binding of target induces aptamer folding, which further recovers Broccoli to activate the fluorescence of DFHBI-1T.

Here, without introducing the target-binding aptamer or the transducer region, we describe a new fluorogenic RNA sensor platform to detect metal ions. Our sensor is designed based on a specific cytosine- $Ag^+$ -cytosine (C- $Ag^+$ -C) metallo base pair. C- $Ag^+$ -C is structurally similar with the canonical Watson-Crick base pair and adopt a standard A-form RNA conformation.<sup>24</sup> We propose that selective  $Ag^+$  sensor can be developed by introducing C-C mismatches into the structurally critical H<sub>1</sub> helix of Broccoli (Fig. 1a). The DFHBI-1T-binding pocket of Broccoli is formed by a coaxial helical stack of two A-form helices separated by a G-quadruplex.<sup>25,26</sup> The formation of an upper H<sub>1</sub> helix is required to stabilize the DFHBI-1T-binding pocket. In the absence of  $Ag^+$ , C-C mismatches prevent Broccoli from folding and fluorescence. While in the presence of  $Ag^+$ , the formation of C- $Ag^+$ -C enables the refolding of H<sub>1</sub> helix and the overall structure of Broccoli, which leads to DFHBI-1T fluorescence for the measurement of  $Ag^+$  concentrations.

To test this idea, we first used a NUPACK software to predict the RNA folding after replacing 1-3 base pairs in the  $H_1$  helix of Broccoli with C-C mismatches. Interestingly, by replacing only one A-U base pair with C-C, the overall secondary structure of Broccoli was dramatically disrupted (Fig. S2, ESI<sup>†</sup>). Guided by these simulation results, we designed four Ag<sup>+</sup> sensors, S1 to S4, which are different from each other in the number and position of C-C mismatches in the  $H_1$  helix (Fig. 1b).

We next tested the *in vitro* performance of these sensors. The fluorescence spectrum of S1-S4 was collected with a mixture of 20  $\mu$ M DFHBI-1T and 1  $\mu$ M RNA after *in vitro* transcription (Fig. 1b). An optimal Ag<sup>+</sup> sensor was obtained using S1 RNA, with a 4.9-fold fluorescence increase upon adding 100  $\mu$ M AgNO<sub>3</sub>. There is only a single C-C mismatch in S1, which is adjacent to the DFHBI-1T-binding pocket of Broccoli. A 3.7-fold increase in fluorescence was observed with S3 under this condition. However, considering the overall low fluorescence intensity of S3, we chose to use S1 for further studies.

To examine if S1 can be used to detect  $Ag^+$  within its antibacterial concentration range (1-20  $\mu$ M),<sup>1</sup> a dose-response curve was measured after adding various amounts of  $Ag^+$  (Fig. 1c). Indeed, S1 can be potentially useful by detecting  $Ag^+$  levels within the antibacterial therapeutic window, with 10% fluorescence shown after adding 610 nM  $Ag^+$  and 90% signal with 6.2  $\mu$ M  $Ag^+$ . Half-maximal fluorescence was reached in the presence of 2.0  $\mu$ M  $Ag^+$ . This detection range is not influenced by the concentration of DFHBI-1T, while the increase of S1 concentration from 1  $\mu$ M to 10  $\mu$ M shifts the half-maximal fluorescence to 4.6  $\mu$ M Ag <sup>+</sup> (Fig. S3, ESI†). As a control, the Broccoli fluorescence will not be influenced by adding  $Ag^+$  (Fig. S4, ESI†). The moderate detection range of S1 can be potentially used to measure  $Ag^+$  levels at which antibacterial effects exhibit.

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We next asked if S1 can selectively recognize only Ag<sup>+</sup>. Here, the Ag<sup>+</sup> selectivity stems from the unique C-Ag<sup>+</sup>-C metallo base pair. Other cations will not bind in between two cytosines and/or maintain a standard A-form RNA conformation. Indeed, our results indicates that none of Al<sup>3+</sup>, Ca<sup>2+</sup>, Co<sup>2+</sup>, Cu<sup>2+</sup>, Fe<sup>2+</sup>, Fe<sup>3+</sup>, Mn<sup>2+</sup>, Na<sup>+</sup>, Ni<sup>2+</sup> or Zn<sup>2+</sup> could enhance the fluorescence signal of S1 (Fig. 1d). In addition, most of these ions, except Cu<sup>2+</sup> and Ni<sup>2+</sup>, when added together with Ag<sup>+</sup>, will not influence the fluorescence detection of Ag <sup>+</sup> (Fig. S5, ESI<sup>†</sup>). While at the low nanomolar physiological level,<sup>27</sup> Cu<sup>2+</sup> and Ni<sup>2+</sup> will not influence the S1 performance. It is worth to mention that Mg<sup>2+</sup> and K<sup>+</sup> are essential for Broccoli folding and fluorescence activation. Both ions are used at a constant physiological concentration in these tests. Overall, S1 can detect Ag<sup>+</sup> with good selectivity.

We next cloned S1 into a pET28c vector and transformed it into a BL21 (DE3)\* *E. coli* for live cell imaging of Ag<sup>+</sup>. Cellular fluorescence was first measured at 2 h after the addition of various concentrations of AgNO<sub>3</sub> (1-100  $\mu$ M). Indeed, Ag<sup>+</sup>-dependent cellular fluorescence was clearly observed (Fig. 2a and Fig. S6, ESI<sup>†</sup>). After analyzing the fluorescence intensity of 450 individual *E. coli* cells, our data indicated that on average a 2.2-fold, 3.8-fold, and 7.1-fold fluorescence increase was observed after adding 10, 20, and 100  $\mu$ M AgNO<sub>3</sub>, respectively (Fig. 2b). Interestingly, there is a substantial difference between the *in vitro* (0.61-6.2  $\mu$ M) and intracellular (6.8-127  $\mu$ M) dynamic range of S1 (Fig. 2c), in addition to the effect of cellular environment on S1 properties, it also indicates that the cellular free Ag<sup>+</sup> level may be indeed much lower than that in the extracellular solution.

Our next goal is to study the correlations between the cellular  $Ag^+$  levels and their antibacterial efficiencies. Antibacterial efficiency can be measured based on the viability of bacterial cells after various silver treatment, as indicated by the propidium iodide (PI) staining. PI has been widely used for staining the dying/dead cells, which exhibit significantly increased membrane permeability.<sup>28</sup> By imaging cellular  $Ag^+$  levels (S1 channel) and cell viability (PI channel) simultaneously, our results indicated that the vast majority of the dying/dead cells indeed also contained relatively high levels of  $Ag^+$  (Fig. 2a). The percentage of PI-stained cells increased from 2.3% in the absence of  $Ag^+$  to 6.0%, 14.4%, and 17.4% after 2 h incubation with 1, 10, and 100  $\mu$ M AgNO<sub>3</sub>, respectively. This result is consistent with previously identified antibacterial  $Ag^+$  concentrations of 1-20  $\mu$ M.<sup>1</sup> The overall low percentage of PI-stained cells may be due to the relatively short incubation time. There is indeed a direct correlation between  $Ag^+$  concentrations and their antibacterial efficiency (Fig. 4b).

We also wondered if it is possible to monitor the dynamic variations of cellular  $Ag^+$  levels using S1. After adding 100 µM AgNO<sub>3</sub>, the cellular fluorescence was imaged every 10 min over 1 h. About 2/3 of cells started to light up within 30 min, and most majority of cells displayed stable bright fluorescence after 1 h (Fig. 3a and Fig. S7, ESI<sup>+</sup>). 14.6% of cells exhibited high cellular  $Ag^+$  levels with fast response, i.e., emitted more than 80% S1 fluorescence within 30 min. 44.6% and 40.8% of cells displayed moderate and slow response, respectively. There are some cell-to-cell variations in the accumulation rate of Ag <sup>+</sup>.

We further tracked the fluorescence signal of 50 individual cells with high PI signals (Fig. 3b). Interestingly, the maximum S1 fluorescence of these cells was observed after 20-30 min, with continually fluorescence decrease after 30 min. To study if this reduced signal was due to the cellular degradation of RNAs, we measured the time-dependent cellular fluorescence of Broccoli. The Broccoli fluorescence remained constant during the 2 h imaging time (Fig. S9, ESI<sup>†</sup>). Thus, the decreased S1 fluorescence after 30 min may be explained by the reduced free Ag<sup>+</sup> levels, due to their binding with cellular proteins/nucleic acids or removal through membrane efflux pumps. While indeed, S1 can be used to monitor the cellular dynamics of Ag<sup>+</sup>.

In the above-mentioned kinetic measurement, we have also simultaneously monitored the changes in cell viability via PI staining (Fig. 3a and Fig. S7, ESI<sup>†</sup>). PI signal continuously increased over the 2 h detection period. The large majority of PI-stained cells (95%) at 2 h also exhibited high S1 fluorescence before 30 min. The same experiment was also tested with 10  $\mu$ M AgNO<sub>3</sub>. Indeed, a lower S1 fluorescence but similar correlation with the PI signal was observed (Fig. S10, ESI<sup>†</sup>).

We have further examined the kinetics of both S1 and PI channels at the single-cell level (Fig. 3b, 3c and Fig. S11, ESI<sup>†</sup>). Within the 50 cells we analysed, 30 cells exhibited PI signal at least 10 min later than that of S1. The rest 20 cells exhibited both green and red fluorescence almost at the same time. Considering the fast PI staining kinetics once cell membrane is permeable, together with the relatively slower kinetics of S1 response (Fig. S12, ESI<sup>†</sup>), these results suggested a ~10-20 min delay time for Ag<sup>+</sup> to disrupt the *E. coli* membrane permeability. This knowledge can be potentially useful in studying the mechanism of Ag<sup>+</sup>-induced antibacterial effects.

As a first step in understanding the antibacterial mechanisms of silver nanoparticles, we next applied S1 to study the cellular  $Ag^+$  accumulation after its release from AgNPs. It is known that the particle size and concentration play critical roles in the antibacterial efficiency of AgNPs.<sup>29</sup> First, to study the effect of particle size on the cellular  $Ag^+$  levels, polyvinylpyrrolidone-coated AgNPs (PVP-AgNPs) with diameters of 5, 25, and 110 nm were incubated at 200 µg/mL concentration with S1-expressing BL21 (DE3)\* cells. This concentration is chosen based on the reported 30-180 µg/mL minimum bactericidal concentration of AgNPs for *E. coli* stains.<sup>29</sup> As expected from the large surface-area-to-volume ratio of small nanoparticles, 5 nm AgNPs induced the highest S1 sensor fluorescence, followed by 25 nm AgNPs (Fig. 4a and Fig. S13, ESI†). Using the above-mentioned AgNO<sub>3</sub> solution as a reference, a cellular Ag<sup>+</sup> level equivalent to >1 mM, 35.5 µM, and 5.1 µM AgNO<sub>3</sub> was observed after adding these 5, 25, and 110 nm PVP-AgNPs, respectively (Fig. S14, ESI†).

Lastly, we asked if the amount of cellular  $Ag^+$  accumulation is directly correlated with the antibacterial effect of AgNPs. As shown with the PI staining, all three sizes of PVP-AgNPs exhibited larger percentage of PI-stained cells (~2.0-fold) than corresponding AgNO<sub>3</sub> of the same S1 fluorescence (Fig. 4b). This result indicated that the cellular release of Ag<sup>+</sup> may count for ~50% of the antibacterial effect of PVP-AgNPs. Other mechanisms should also make large contributions. We have further studied the effect of AgNP concentrations on the

Ag<sup>+</sup> release and cell viability. 25-200  $\mu$ g/mL of 5 nm and 25 nm PVP-AgNPs were incubated with S1-expressing *E. coli* cells for 2 h. For both sizes of AgNPs, an increasing level of S1 and PI fluorescence was observed as a function of AgNP concentrations (Fig. 4c and Fig. S15, S16, ESI<sup>+</sup>). Indeed, there is a direct correlation between cellular Ag<sup>+</sup> accumulation and the antibacterial effect of AgNPs (Fig. S17 and S18, ESI<sup>+</sup>).

 $Ag^+$  has been widely used for disinfection. However, due to the lack of tools for the direct intracellular measurement of  $Ag^+$ , the detailed correlation between the  $Ag^+$  accumulation and its antibacterial effect is still unclear. In this study, we reported the first  $Ag^+$  sensor that can be genetically encoded to image  $Ag^+$  levels at the single-cell level. Single cell studies are critical in understanding cell-to-cell variations in the dynamics of  $Ag^+$  accumulation and the corresponding antibacterial effects. Small molecule- and DNA-based sensors could be powerful *in vitro* tools for  $Ag^+$  detection. However, their intracellular applications are still hindered by challenges in cell delivery, degradation, and interference with biological functions. In contrast, RNA-based sensors, which can be genetically encoded and transcribed within living systems, hold great potential for the intracellular applications.

Our results indicated that there is a direct correlation between cellular Ag<sup>+</sup> level and the antibacterial efficiency of AgNPs. While in addition to the Ag<sup>+</sup> release, some other mechanisms can also result in the AgNPs-induced disinfection. We can now directly monitor the accumulations and antibacterial effects of Ag<sup>+</sup> in each individual cell. These knowledge are important in improving the specificity and efficiency of silver-based antibacterial consumer products, as well as in studying the mechanism of antibacterial resistance. This new fluorescent RNA sensor is developed based on a specific C-Ag<sup>+</sup>-C metallo base pair. Similar design principle may be applied for the cellular imaging of several other metal ions. 30

#### Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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#### Fig. 1.

Design and *in vitro* characterization of RNA-based Ag<sup>+</sup> sensors. (a) Schematic illustration of modified Broccoli. The green region indicates sequences from the original Broccoli and C-C mismatch is highlighted in blue. (b) Sequence design of the Ag<sup>+</sup>-binding H<sub>1</sub> helix in S1-S4 (left) and the corresponding fluorescence response at 2 h after adding various amounts of AgNO<sub>3</sub> (right). All spectra were measured in a solution containing 1  $\mu$ M RNA and 20  $\mu$ M DFHBI-1T. (c) Dose response curve of the S1 sensor. (d) Selectivity of S1 against different ions. All the ions were tested at 10  $\mu$ M in a solution containing 1  $\mu$ M S1, 20  $\mu$ M DFHBI-1T, 100 mM K<sup>+</sup> and 1 mM Mg<sup>2+</sup> at pH 7.5. Control was measured in this solution without adding other cations. Shown are the mean and S.E.M. values from three independent replicates.



#### Fig. 2.

Imaging of  $Ag^+$  in live *E. coli* cells. (a) Confocal fluorescence imaging of S1 sensorexpressing BL21 (DE3)\* cells after 2 h incubation with 0-100 µM AgNO<sub>3</sub>. The S1 sensor channel (green), propidium iodide channel (red) and merged images are shown. Scale bar: 20 µm. (b) Cellular distribution of  $Ag^+$  as indicated from S1 fluorescence intensities. Each individual cell was binned according to the brightness. The percentage of cells in each bin was plotted and fitted with Gaussian distribution curves. A total of 450 cells were measured in each case from three experimental replicates. (c) Cellular dose response curve of the S1 sensor based on the mean and S.E.M. fluorescence intensities from the Gaussian fitting.



#### Fig. 3.

Monitoring Ag<sup>+</sup> accumulation and cell viability changes. (a) Confocal microscopy images of live BL21 (DE3)\* cells at different time points after adding 100  $\mu$ M AgNO<sub>3</sub>. Scale bar: 5  $\mu$ m. (b) Tracking of the S1 fluorescence from 50 individual cells that exhibited high PI signal at 2 h. The fluorescence of each cell was plotted in a gray line. The averaged signal of these 50 cells was plotted in green. (c) Tracking of the PI fluorescence from the same 50 cells. The PI signal of each individual cell was plotted in a gray line. The averaged signal of 50 cells was plotted in red.



#### Fig. 4.

Cellular Ag<sup>+</sup> accumulation from silver nanoparticles. (a) Confocal microscopy imaging of S1 sensor-expressing cells at 2 h after adding 200  $\mu$ g/mL of 5, 25, and 110 nm PVP-AgNPs. (b) The correlation between S1 fluorescence and percentage of PI-stained cells after adding AgNO<sub>3</sub> (grey line) or 200  $\mu$ g/mL AgNPs of various sizes (blue line). Shown are the mean and S.E.M. fluorescence. (c) S1 sensor fluorescence imaged at 2 h after adding different concentrations of 25 nm PVP-AgNPs. Scale bar: 20  $\mu$ m.