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Lymph Node Staging in Prostate Cancer

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Abstract

Nodal staging is important in prostate cancer treatment. While surgical lymph node dissection is the classic method of determining whether lymph nodes harbor malignancy, this is a very invasive technique. Current noninvasive approaches to identifying malignant lymph nodes are limited. Conventional imaging methods rely on size and morphology of lymph nodes and have notoriously low sensitivity for detecting malignant nodes. New imaging techniques such as targeted positron emission tomography (PET) imaging and magnetic resonance lymphography (MRL) with iron

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oxide particles are promising for nodal staging of prostate cancer. In this review, the strengths and limitations of imaging techniques for lymph node staging of prostate cancer are discussed.

Keywords

Prostate cancer; Lymph node staging; Imaging

Introduction

Prostate cancer is a common human malignancy and the second leading cause of cancer death in American men [1]. When prostate cancer is confined to the gland, it has an excellent chance for cure. However, the presence of lymph node metastases portends a less favorable prognosis. Accurate lymph node (LN) staging is critical for treatment planning and therapy monitoring [2]. Lymph node involvement in prostate cancer is commonly treated initially with androgen deprivation therapy and radiation therapy to the pelvis. In patients with high-risk prostate cancer (serum prostate-specific antigen (PSA) >20 ng/dL, Gleason score 8, or extra-prostatic spread), there is an increased risk of biochemical recurrence after definitive treatment due to local recurrence, nodal recurrence, or metastatic disease. [3]. Lymph node metastases can portend a poor prognosis, however, the 5-year survival rate depends on the total number of metastatic LNs ranging from a 5-year survival of 75–80 % in patients with a single metastatic LN to only 20–30 % in patients with more than five metastatic LNs [4]. Currently, surgical pelvic LN dissection with histo-pathological examination is the standard of care and the most commonly used method of LN staging. However, pelvic LN dissection can be a technically challenging and is associated with higher rates of complications such as lymphocele, deep venous thrombosis, pelvic hematoma, fever, and urinary retention that may result in longer hospital stays [5]. Moreover, once a lymph node dissection has been performed, it is difficult to reoperate on the same patient due to postoperative scarring. Nodes outside the normal resection template may also be missed and, hence, undersampled, at surgery. Thus, there is a need for accurate noninvasive imaging methods to accurately detect nodal disease. In this article, we will discuss traditional and novel noninvasive imaging techniques used for LN staging in prostate cancer.

Conventional Computed Tomography (CT) and Magnetic Resonance Imaging (MRI)

The conventional approach to LN staging in prostate cancer patients includes the use of contrast-enhanced CT and MRI. For both modalities, the definition of suspicious LNs is based mostly on size thresholds for enlarged LNs. The most commonly used threshold is 10 mm in short axis diameter [6]. However, recommended thresholds vary from 8 to 15 mm [7–10]. Lower thresholds have higher sensitivity but lower specificity, whereas higher thresholds have lower sensitivity and higher specificity, thus defining a receiver operator characteristic (ROC) curve. Attempts to standardize these thresholds have been made, such as with the Response Evaluation Criteria in Solid Tumors (RECIST) 1.1 criteria [11]. The RECIST criteria include guidelines for specific dimensions of LNs on CT. The updated

version 1.1 states that LNs are normal if the short axis is <10 mm and is a target lesion if the short axis is >15 mm [12]. Using size criteria alone often leads to incorrect staging, however, due to the fact that smaller lymph nodes can commonly harbor microscopic foci malignancy [8, 13]. Thus, in high-risk prostate cancer patients, conventional CT and MRI may underestimate LN stage [14, 15]. A large review by Hovels et al. determined the pooled diagnostic accuracy of CT and MRI in determining LN status in patients with prostate cancer using RECIST criteria. The pooled sensitivity and specificity for CT were 0.42 (95 % CI 0.26–0.56) and 0.82 (95 % CI 0.80–0.83), respectively, compared to 0.39 (95 % CI 0.22–0.56) and 0.82 (95 % CI 0.79–0.83) for MRI [15]. Most of the studies that were examined used only a limited, not extended, pelvic lymph node dissection to confirm imaging findings. Hovels et al. concluded that CT and MRI have limited ability to correctly identify malignant LNs, and, thus, should not be used for LN staging in prostate cancer patients. Their finding corroborates what many other studies in the literature have reported previously, that CT and MRI have poor sensitivity for LN detection [7, 16–18]. An imaging method incorporating both anatomical and functional information for accurate imaging of pelvic lymph nodes is needed for successful prostate cancer nodal staging.

There is some disagreement in the literature regarding the comparative performance of CT versus conventional MRI in LN staging in prostate cancer (Table 1). One large historical study indicated that CT and MRI are roughly equal in detecting malignant LNs as they use the same criteria [19]. This finding has been confirmed by a more recent study by Lecouvet et al. using whole body MRI including diffusion-weighted (DW-MRI) sequences [11]. The use of DW-MRI has been examined as an approach for staging independent of lymph node dissection techniques in prostate cancer patients. Budiharto and colleagues prospectively evaluated DW-MRI for LN staging and concluded that it was still inferior to extended lymph node dissection in determining lymph node status in prostate cancer patients [14]. Countering the supposition that CT and MRI are equivalently poor at LN staging, a recent study has shown MRI to be superior in the identification of the greatest number of suspicious LNs [6]. Saokar and colleagues postulated that MRI is a better method for LN identification compared to CT due to its improved soft tissue resolution and ability to distinguish LNs from vascular structures in the pelvis. They reported that differentiating nodes from vasculature was difficult on CT owing to inadequate opacification of small blood vessels in the pelvic region [6]. The results of this study correlated well with findings reported previously by Yang et al. that showed that MRI identified a greater number of pelvic LNs compared to CT in cervical cancer patients [20]. A major limitation of this study is the lack of tissue validation to determine malignancy status. This is of particular relevance since in their study MRI identified significantly more LNs with diameters of 1 to 5 mm. While these would be classified as benign by common size thresholds and the RECIST 1.1 criteria, Saokar and colleagues complemented size criteria with imaging features like border appearance, mottled heterogeneous appearance, and signal intensity characteristics which are more subjective and qualitative, therefore, less likely to be reproducible across different observers [6]. These features have previously been reported to be helpful in evaluating LN metastases from rectal cancer on MRI [21, 22]. Recently, Thoeny et al. prospectively assessed the diagnostic performance of DW-MRI in the detection of pelvic lymph node metastases in patients with prostate and/or bladder cancer staged as N0 (no evidence of

lymph node involvement) with other preoperative cross-sectional imaging. A total of 4846 lymph nodes were resected in 120 patients and 88 lymph node metastases were found in 33 of 120 patients (27.5 %). Short-axis diameter of these metastases was less than or equal to 3 mm in 68, between 3–5 mm in 13, between 5–8 mm in five, and between 8–10 mm in two nodes. On a per-patient level, the three readers in the study correctly detected metastases in 26 (79 %; 95 % CI 64 %, 91 %), 21 (64 %; 95 % CI 45 %, 79 %), and 25 (76 %; 95 % CI 60 %, 90 %) of the 33 patients with metastases, with respective specificities of 85 % (95 % CI 78 %, 92 %), 79 % (95 % CI 70 %, 88 %), and 84 % (95 % CI 76 %, 92 %). Nodal metastases were detected with histopathologic examination in 44 of 240 pelvic sides (18 %); the three readers correctly detected these on DW-MR images in 26 (59 %; 95 % CI 45 %, 73 %), 19 (43 %; 95 % CI 27 %, 57 %), and 28 (64 %; 95 % CI 47 %, 78 %) of the 44 cases. They concluded that DW-MRI enabled detection of small lymph node metastases in normal-sized nodes in a substantial percentage of patients with prostate and bladder cancer diagnosed as N0 with conventional cross-sectional imaging techniques [23]. This combined approach of DW MRI with anatomic imaging has potential to obtain more accurate results for nodal staging than conventional CT and MRI especially in the presence of normal lymph nodes; however, these initial results need to be validated.

Magnetic Resonance Lymphography with Ultrasmall Superparamagnetic Iron Oxide (USPIO)

MR imaging can be improved by the use of contrast agents containing USPIO nanoparticles, which are taken up by subcapsular macrophages within LNs. The iron oxide within the USPIO turns normal lymph nodes dark on T2- and T2*-weighted MRI. This allows for the detection of early histological changes caused by microscopically infiltrating tumor cells, even before the LNs enlarge in size [24•]. The lymphographic properties of USPIOs have been known for over 15 years. In 1999 Harisinghani et al. (1999) investigated USPIO lymphography in 19 patients with primary abdominal and pelvic malignancies [25].

Several USPIOs have been suggested for human use. Initially, ferumoxtran-10, or Combidex, was the agent of choice. Ferumoxtran-10 was a biodegradable, dextran coated USPIO that exhibited, prolonged circulatory time and was avidly taken up by macrophages at relatively low iron doses of 2–4 mg/kg. Once injected, ferumoxtran-10 extravasates through capillary walls and is transported via the lymphatic system to the lymph node where it is phagocytized by macrophages [26]. In the presence of normal LN macrophages, ferumoxtran-10 is taken up within 24 h resulting in reduced signal intensity and darkened lymph nodes. The iron oxide (Fe^{2+} and Fe^{3+}) core of ferumoxtran-10 strongly shortens the T1, T2, and T2* of tissue turning normal nodes very dark. Over time, the particles disassociate and are metabolized with iron either entering the body's iron stores or being slowly eliminated via feces [27]. Lymph nodes that fail to take up ferumoxtran-10 remain either high or heterogeneous in signal intensity, suggesting possible metastasis. Metastases as small as 3–10 mm have been identified using ferumoxtran-10 imaging. Overall ferumoxtran-10 MR lymphography (MRL) demonstrates a high sensitivity (~90 %) and specificity (~95 %) for lymph node metastases in several malignancies including prostate

cancer [26]. Unfortunately, ferumoxtran-10 was not pursued as a product by its manufacturer and is currently not widely available outside of The Netherlands.

Before it was discontinued, ferumoxtran-10 was used in a variety of studies with varying results. Traintafyllou et al. (2013) used extended pelvic lymph node dissection (ePLND) as a reference standard to detect lymph node metastases in prostate and bladder cancer patients with nodes smaller than 5 mm by using ferumoxtran-10-enhanced MRI at 3T and found positive and negative predictive values of 58.3 and 84.4 % per patient respectively, suggesting that USPIO and MRI may aid in disease management but cannot be considered definitive [28]. This study is notable because of the small size of the nodes detected. This observation was confirmed by Birkhauser and colleagues, who showed that among 54 lymph nodes that were histologically confirmed for metastases, 47 (87 %) were smaller than 8 mm in their short axis, and of these, 38 (87 %) were successfully detected on combined ferumoxtran-10-enhanced MRL and diffusion-weighted MRI. The smallest subset of lymph nodes were smaller than 3 mm, and MRL detected 14 of 16 (88 %) in this category [29].

Field strength may play a role in the success of USPIO MRL. Heesakkers et al. performed MRL in 48 prostate cancer patients at 3T and showed significantly improved image quality for the higher field strength with improved nodal detection [30]. Harisinghani and colleagues conducted a study with ferumoxtran-10 in 80 patients with stage T1–3 prostate cancer. This study included 334 lymph nodes that were resected or biopsied. Of the 63 nodes with metastases detected by USPIO, 45 (71.4 %) did not fulfill the classic size or morphology criteria for malignancy. On a node-by-node basis, ferumoxtran-10 MRL had a significantly higher sensitivity than conventional MRI (90.5 vs. 35.4 %, $P<0.001$) [24•]. Several authors have compared ferumoxtran-10 MRL with other imaging methods. For instance, Fortuin et al. compared ferumoxtran-10-enhanced MRL to ^{11}C -choline PET/CT in prostate cancer patients, showing that MRL detected significantly more positive lymph nodes than PET/CT (151 metastases positive LNs in 23/29 patients vs. 34 metastases positive LNs in 13/29 patients for MRL vs. PET/CT, respectively) ($p<0.001$) [31].

MRL with ferumoxtran-10 has several limitations, including the need to perform imaging pre-contrast and 24–36 h post-contrast due to the slow accumulation of the contrast agent within lymph nodes. Furthermore, the USPIO agent ferumoxtran-10 must be administered slowly through a filtered needle over 15–30 min to minimize infusion reactions including hypersensitivity and back pain. Approximately one fourth of patients participating in phase 3 clinical trials using ferumoxtran-10 reported headache, back pain, vasodilation, or urticaria as adverse events [32]. As mentioned, the agent is currently only available at one center in Europe on a research basis. Thus, there has been interest in other candidate USPIO agents with wider availability and better side effect profiles [32, 33].

Ferumoxytol was originally developed as an iron replacement therapy in chronic renal failure patients by the same company that developed ferumoxtran-10 [34–36]. Unlike ferumoxtran-10, ferumoxytol is an FDA-approved semi-synthetic carbohydrate-coated magnetic iron oxide preparation that is administered as a bolus versus slow infusion with ferumoxtran-10 [35]. There is still limited clinical experience with ferumoxytol-enhanced MRI for metastatic lymph node mapping. One aspect of ferumoxytol that differs from

ferumoxtran-10 is that it appears to have less affinity for macrophages, thus requiring higher doses. Harisinghani et al. reported using ferumoxytol in 10 prostate cancer patients at a dose of 4 mg Fe/kg body weight (typical dose of ferumoxtran-10 is 2.6 mg Fe/kg). Among 26 nodes in 10 patients, ferumoxytol demonstrated a significant drop in the signal-to-noise ratio (SNR) in benign nodes, but little change in SNR within malignant nodes. Like ferumoxtran-10, ferumoxytol showed maximal reduction in node signal at 24 h after injection [37]. Turkbey and colleagues (2014) conducted a phase I dosing study of ferumoxytol to determine the optimal iron dose of this agent for MR lymphography [38]. Homogenous loss of signal in normal lymph nodes on MRI was consistently achieved at 7.5 mg Fe/kg [38]. This is considerably higher (~3 fold) iron dose compared with ferumoxtran-10. It should be noted that the recommended dose of ferumoxytol for iron replacement is 510 mg Fe (one vial) at day 1 with an additional 510 mg Fe vial 3–8 days later. This corresponds to ~7.3 mg Fe/kg for a 70 kg man. Thus, although the 7.5 mg Fe/kg dose is higher than the recommended iron replacement dose for the first injection of ferumoxytol, the total dose is about the same as the recommended dose. The two phase injection strategy for ferumoxytol was implemented because ferumoxytol exhibits dose-dependent, capacity-limited elimination from plasma with a half-life of approximately 15 h in humans and the clearance decreases with increasing doses of ferumoxytol [39]. The inconvenience of this regimen prompted a recent safety and efficacy study of 60 patients with iron deficiency anemia; 58 patients received a single-infusion dose of two vials of ferumoxytol totaling 1020 mg (14.6 mg Fe/kg in a 70 kg person) over 15 min. Among the 58 patients, 2 failed to complete the dose due to an infusion reaction including cough, flushing, swollen lips, and pruritis, without hypotension, tachypnea, tachycardia, wheezing, stridor, or periorbital edema. Both patients recovered rapidly after treatment. Overall, 26 out of 60 (43.3 %) patients reported adverse events (AEs) of which 13 were mild and transient during infusion. Among the AEs, most common ones were self-limited arthralgias, myalgias, and/or headache within 24–48 h [40]. The safety data and the recent results from double dose studies implies that the clearance issue may be less of a problem for higher dose of ferumoxytol provided it is administered slowly. Further research is needed to continue to characterize the clinical applications of iron oxide nanoparticles as they relate to oncologic outcomes and clinical decision-making.

Positron Emission Tomography (PET) CT

The use of PET in combination with computed tomography (PET/CT) is established in the diagnosis, staging, restaging, and monitoring of tumor responses in many tumor types using FDG. However, the use of FDG in prostate cancer has been somewhat disappointing. Thus, a variety of different tracers have been developed for staging, assessment of biochemical recurrence (BCR) in patients with treated prostate cancer and monitoring of metastatic castration-resistant prostate cancer (CRPC). The use of PET/CT in the assessment of local and regional pelvic lymph node (LN) metastases is commonly limited by high urinary bladder tracer activity of tracers excreted via the kidneys. In addition, due to limited resolution of PET/CT scanners (4–5 mm), sensitivity for small (<5 mm) LN metastases is low [41]. Currently employed radiotracers include the following: ^{18}F -FDG, ^{18}F - and ^{11}C -

choline compounds, prostate-specific membrane antigen (PSMA)-targeted tracers (^{18}F -DCFBC), ^{18}F -FDHT, ^{18}F -FACBC, and ^{11}C -acetate.

^{18}F -Fluorodeoxyglucose (^{18}F -FDG)

The benefits of ^{18}F -FDG PET/CT in prostate cancer are limited, although it is successfully used to stage many other cancer types. The ability of ^{18}F -FDG PET to detect cancer is based on the altered glucose metabolism in tumor cells and aerobic glycolysis in malignant tissue relative to normal tissue (Warburg effect). The limited use of ^{18}F -FDG PET/CT in prostate cancer has been attributed to the presumed low glucose metabolism rate and lower expression of glucose transporter 1 (GLUT-1) in prostate cancer. However, British researchers found GLUT-1 gene expression to be significantly higher in prostate cancer than in benign prostatic hyperplasia and that GLUT-1 gene expression correlated with Gleason score [42, 43]. This may explain the observation of increased ^{18}F -FDG uptake in CRPC.

^{18}F -FDG PET can potentially be useful in detecting sites of biochemical recurrence (BCR). In a retrospective review of 91 patients with BCR after radical prostatectomy, PSA levels were higher in patients with FDG PET-positive findings than in patients with negative findings and a PSA of 2.4 ng/mL and PSA velocity of 1.3 ng/mL/y provided the best tradeoff between sensitivity (80 %; 71 %) and specificity (73 %; 77 %) of FDG PET in a receiver operating curve analysis. Overall, ^{18}F -FDG PET detected local or systemic disease in 31 % of patients with BCR [44]. It is important to note that ^{18}F -FDG is not specific for cancer, and false positive findings may occur in benign prostatic hyperplasia (BPH) and inflammatory processes such as prostatitis or lymphadenitis [45].

^{11}C -Choline/ ^{18}F -Choline

Radiolabeled choline accumulates in prostate tumors and choline and their extension to the lymph nodes [46]. Tumors exhibit upregulation of choline kinase, leading to increased trapping of choline in the form of phosphatidylcholine in the cell membrane. Choline can be labeled with ^{18}F or ^{11}C . Compared to FDG PET, ^{11}C -choline has the advantage of minimal urinary excretion (it is excreted in the pancreas) and, therefore, minimal urinary bladder accumulation, allowing for improved detection of pelvic adenopathy. The disadvantage of ^{11}C -cho-line is its short half-life of 20 min requiring an onsite cyclotron and radiochemistry facility for production. ^{18}F -choline has a longer half-life of 110 min and is therefore more easily provided by commercial sources (similar to ^{18}F -FDG), but it has substantially more urinary excretion than ^{11}C -choline limiting its use in the prostatic fossa.

PET/CT using ^{11}C or ^{18}F -labeled choline has been reported to have higher sensitivity and specificity than ^{18}F -FDG PET and has been investigated for staging and restaging of prostate cancer. In a study by Tilki et al. evaluating 1149 lymph nodes in 56 patients, ^{18}F -choline had a sensitivity and specificity of 40 and 96 %, respectively [47]. The sensitivity and specificity of ^{18}F -choline for detecting lymph node metastases in the primary staging of prostate carcinoma has been reported to be 19 to 80 % and 82 to 98 %, respectively [48]. This indicates a wide range of sensitivity likely due to the size of the lesions, but a consistently low false positive rate.

The detection rate of malignant lymph nodes with choline PET improves with increasing size of lymph nodes. Choline PET is not sensitive for nodes smaller than 5 mm due to the limited spatial resolution of the PET/CT scanner and relatively low uptake of the agent in prostate cancer. In the restaging of patients with BCR, choline PET has been more successful in patients with higher PSA (>4 ng/mL), higher Gleason score, and CRPC [49]. However, it is hoped that PET agents could detect disease at an early state.

Prostate-Specific Membrane Antigen (PSMA) Targeting PET Tracers

PSMA is a transmembrane protein that is a highly specific marker for prostate cancer. Increased expression of PSMA is found in all prostate cancers, particularly in high grade, hormone-refractory, and metastatic disease [50]. As such, PSMA is an ideal target for detecting prostate cancer and several molecular imaging approaches targeting PSMA are currently being investigated. The initial focus of PSMA targeting was on radiolabeled monoclonal antibodies directed against the intracellular domain of PSMA. Indium (^{111}In) capromab pendetide was approved by the Food and Drug Administration since 1996 as a gamma camera and/or SPECT agent (ProstaScint, Cytogen). Although PSMA is ubiquitous in the prostate, PSMA expression is normally low in normal prostate glandular epithelium as it is only found in the luminal cells of the gland but in cancer cells PSMA is found on the basal layer far more available for targeting with a PET agent. PSMA expression correlates with tumor grade and is significantly upregulated in androgen-independent prostate cancer. However, the target of capromab pendetide is intracellular, and thus, cell membranes must be disrupted to allow binding, which is an important limitation of this method. Anatomic localization of capromab pendetide uptake has been challenging because of its nonspecific binding and high blood pool activity. Moreover, SPECT imaging has inferior spatial resolution compared to PET (6–7 mm). Antibody imaging with capromab pendetide can detect lymph node metastases, recurrence after prostatectomy, and occult metastatic involvement; however, recurrences usually have to be quite large. Although techniques such as fusion with anatomic images and combined SPECT-CT improve the specificity of capromab pendetide antibody imaging, its overall accuracy is still low [51, 52]. Schettino et al. evaluated indium-111 Prosta-Scint SPECT scans in 58 patients with 161 positive sites of disease. False positives in 74 sites subsequently were due to bowel, vessel, or marrow activity. Twenty-five patients previously thought to have nodal disease appeared to have only local disease after fusion [52].

Several radiolabeled small molecules targeting the external domain of PSMA have been developed. The 2-PMPA analog (2S,4S)-2- ^{18}F -fluoro-4 (phosphonomethyl) pentanedioic acid (BAY1075553) is one such tracer. Early studies have shown that this tracer is safe and well tolerated in human subjects and shows potential in detecting prostate cancer in patients with localized and advanced disease [53]. More recently, the *N*-[*N*-[(*S*)-1,3-dicarboxypropyl] carbamoyl]-4- ^{18}F fluorobenzyl-L-cysteine (^{18}F -DCFBC) was developed at Johns Hopkins University and allows for targeting the external domain of PSMA [54]. Early clinical studies have shown promising results and others are currently underway [NCT02190279] to determine the efficacy of ^{18}F -DCFBC in accurately identifying metastatic disease [55].

PSMA-binding agents have also been labeled with ^{68}Ga , which can be radiolabeled on site using a chelate. Afshar et al. performed a retrospective analysis in 319 patients who underwent ^{68}Ga -PSMA-ligand PET/CT for detection of recurrent PCa. Histological verification was performed in 42 patients after the ^{68}Ga -PSMA-ligand PET/CT. In 82.8 % of the patients, at least one lesion indicative of recurrent PCa was detected. Among lesions investigated by histology, 30 were false-negative in 4 different patients, and all other lesions ($n=416$) were true-positive or true-negative. A lesion-based analysis of sensitivity, specificity, NPV, and PPV were 76.6, 100, 91.4, and 100 %, respectively. A patient-based analysis revealed a sensitivity of 88.1 % [56].

^{18}F -fluoro-5 α -dihydrotestosterone (FDHT)

Androgen deprivation therapy (ADT) is an adjunct treatment for prostate cancer. The androgen receptor (AR) plays a major role in the pathogenesis of prostate cancer and it binds dihydrotestosterone (DHT) causing the translocation of the AR from the cytoplasm to the nucleus whereupon AR acts as a transcription factor. The agent ^{18}F -fluoro-5 α -dihydrotestosterone (^{18}F -FDHT) created first at Washington University (St. Louis, MO) but most widely used at Memorial Sloan Kettering, is a labeled radiotracer analog of DHT [57]. The uptake of this radiotracer can be measured quantitatively and uptake correlates with the degree of AR expression [58]. This agent has not been extensively studied in nodal staging; however, a 2005 study by Dehdashti et al. included nodal detection on a per-patient basis [57]. CT identified nodal abnormalities in 14 of 19 cases (73.6 %) compared to only 8 of 19 cases (42.1 %) using ^{18}F -FDHT PET. The validation techniques were limited in this study, since there was no reference standard other than conventional imaging for defining the extent of disease [57]. Thus, the status of ^{18}F -FDHT PET as a lymph node imaging agent is still unclear.

Anti-1-amino-3- ^{18}F -fluorocyclobutane-1-carboxylic acid (^{18}F -FACBC)

^{18}F -FACBC is a radiolabeled analog of leucine and has been shown to accumulate at sites of prostate cancer and local recurrence [59]. Early studies have shown encouraging results in the ability of ^{18}F -FACBC to accurately stage cancer, with a reported increase of 20–40 % in lesion detection versus the more commonly used ^{18}F -choline PET/CT technique [60]. Kairemo et al. reported the ability of ^{18}F -FACBC PET to assist in restaging prostate cancer, particularly in patients with short PSA doubling times. In 26 patients, ^{18}F -FACBC PET identified 58 lesions, 19 of which (32.7 %) were in the lymph nodes. The mean serum PSA level in patients with positive ^{18}F -FACBC PET findings was $9.5 \pm 16.9 \mu\text{g/L}$ (0.54–69 $\mu\text{g/L}$) and in patients with negative ^{18}F -FACBC PET findings was $1.96 \pm 1.87 \mu\text{g/L}$ (0.11–5.9 $\mu\text{g/L}$), but the difference was not statistically significant. However, the PSA doubling time (PDT) in patients with positive findings was significantly shorter than the PDT in patients with negative findings: 3.25 ± 2.09 months (0.3–6 months) versus 31.2 ± 22.02 months (8–84 months), $P < 0.0001$ [61]. More research is warranted to determine the extent to which ^{18}F -FACBC PET can be utilized in the setting of staging nodal spread or in the treatment of recurrent prostate cancer.

¹¹C-Acetate

Acetate is a molecule that is converted to acetyl coenzyme A (acetyl-CoA) via fatty acid synthase (FAS) for use in lipid metabolism. Thus, acetate may be used by prostate cancer as a means of providing energy using fatty acid metabolism [62, 63]. Various studies have shown the utility of ¹¹C-acetate in the detection of primary prostate cancer, including nodal disease and bone metastases. Its short half-life of 20 min, however, is its main limitation. Early studies by Oyama et al. (2002) and Fricke et al. (2003) showed a 60 % increase in per-patient nodal detection with ¹¹C-acetate when compared to FDG PET [64, 65]. Oyama et al. found no correlation between lesion uptake and serum PSA, whereas Fricke et al. reported a strong positive correlation between lesional tracer uptake and serum PSA [64, 65]. A more recent comprehensive study on ¹¹C-acetate PET by Hasseebuddin et al. (2013) examined 107 patients in whom ¹¹C-acetate PET/CT was performed prior to radical prostatectomy for the purpose of staging and predicting treatment failure [66]. The sensitivity, specificity, positive predictive value, and negative predictive value were reported to be 68.0, 78.1, 48.6, and 88.9 %, respectively. The ¹¹C-acetate PET/CT was positive in 36 of 107 patients, while histopathology confirmed nodal metastases in 25 patients (23.4 %) [66]. While further multi-institutional studies are needed, this technique may provide more accurate information than conventional imaging for the initial treatment planning and surgical management of patients with moderate to aggressive prostate cancer.

Conclusion

Lymph node involvement is a crucial prognostic factor in prostate cancer. Currently, available routine imaging techniques such as CT and MRI are limited due to their dependence on size criteria resulting in their low sensitivity. There are novel imaging approaches for improving nodal staging of prostate cancer such as lymphotropic iron oxide particles and PET imaging with targeted radiotracers. Although results reported from several groups are promising in these approaches, further research is required to optimize these novel imaging techniques and implement them into standard clinical practice.

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Table 1

Comparison of the different techniques used in LN staging

Technique	Mechanism	Current Status
Conventional CT	Anatomical, using RECIST	Low sensitivity
Conventional MRI	Anatomical, using RECIST	Low sensitivity
MRI-USPIO	Iron affinity of <i>normal</i> /subcapsular macrophages	Ferumoxytol and ferumoxtran-10; currently undergoing clinical trials
PET/CT-FDG	Inc. glucose metabolism inc. GLUT-1 receptor	+ve cases PSA mean=9.5; -ve cases PSA mean=2.1
PET/CT-choline	Upregulation of choline kinase	Strong specificity; strong for PSA >4 ng/mL
PET/CT-PSMA	Antibody binding to intracellular domain of PSMA	Strong sensitivity and specificity, undergoing clinical trials
PET/CT-FDHT	Based on androgen receptor expression	Limited published data
PET/CT-FACBC	not fully defined possibly dependent on amino acid transporters (ASCT2 & LAT1)	+ve cases PSA mean=9.5; -ve cases PSA mean=1.96
PET/CT-acetate	Fatty acid metabolism requiring acetate	High false positive rate