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A β -induced vulnerability propagates via the brain's default mode network

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The link between brain amyloid- β (A β), metabolism, and dementia symptoms remains a pressing question in Alzheimer's disease. Here, using positron emission tomography ([¹⁸F] florbetapir tracer for A β and [¹⁸F]FDG tracer for glucose metabolism) with a novel analytical framework, we found that A β aggregation within the brain's default mode network leads to regional hypometabolism in distant but functionally connected brain regions. Moreover, we found that an interaction between this hypometabolism with overlapping A β aggregation is associated with subsequent cognitive decline. These results were also observed in transgenic A β rats that do not form neurofibrillary tangles, which support these findings as an independent mechanism of cognitive deterioration. These results suggest a model in which distant A β induces regional metabolic vulnerability, whereas the interaction between local A β with a vulnerable environment drives the clinical progression of dementia.

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The relationship between regional cerebral amyloid- β (A β) aggregation and hypometabolism has been a topic of significant debate in Alzheimer's disease (AD). Whereas some studies suggest an association^{1–3}, others refute that these pathological processes are directly related^{4,5}. The lack of association between these pathologies has been supported by studies, showing the absence of hypometabolism in some brain regions with high A β load, as well as the presence of hypometabolism in other areas with low A β concentrations^{1,6,7}. Notably, the lack of association between regional A β and hypometabolism contrasts with the idea of a direct deleterious effect of A β on disease progression, as initially proposed in the A β hypothesis⁸.

One possible explanation that links A β with disease progression and integrates the aforementioned conflicting observations is the idea that regional hypometabolism is caused by the toxic effects of A β aggregation from distant rather than topographically overlapping brain regions. Indeed, early observations using [¹⁸F]fluorodeoxyglucose ([¹⁸F]FDG) positron emission tomography (PET) support this notion, by showing that brain damage may lead to hypometabolism in remote, but metabolically connected cortical areas^{9–11}. These results highlight the possibility of a direct deleterious effect of A β on distant hypometabolism, which might be being overlooked by the current biomarker studies.

Regardless of the presence of a regional correlation between A β and hypometabolism, it is well established that the topographic coexistence of these pathologies in some brain regions such as the posterior cingulate cortex constitutes a signature of forthcoming dementia symptoms^{12–15}. Also, studies have shown that either A β or hypometabolism may be the first abnormality in these regions^{16,17}, and that cognitive changes may be potentiated by an interaction between these processes¹⁸. Together, these results indicate that although regional A β may not be the cause of its overlapping hypometabolism, progression to dementia may be the result of local interactions between these pathologies.

Here, we tested the hypothesis that distant and local A β effects play a distinct role in the progression of AD. We find that distant A β determines the region's metabolic vulnerability, whereas the synergy between this regional vulnerability with co-localized concentrations of A β determines dementia. These results were obtained in cognitively normal (CN) and mild cognitive impairment (MCI) individuals as well as transgenic rats that display A β single pathology in the absence of other brain human proteinopathies, such as neurofibrillary tangles. We therefore conclude that the deleterious effect of A β on the progression of AD occurs in a two-step process, in which distant A β determines regional vulnerability and local A β drives cognitive decline.

Results

A β is unrelated to local hypometabolism. Demographics and key characteristics of the human population are summarized in Table 1. Voxel-wise analysis of covariance showed that compared with CN A β -negative individuals, CN A β positive and MCI A β positive had reduced gray matter density in the medial temporal cortex (Supplementary Fig. 1a, d). CN A β positive and MCI A β positive had reduced metabolism in the precuneus, posterior cingulate, inferior parietal, and temporal cortices (Supplementary Fig. 1b, e), and had widespread A β deposition (Supplementary Fig. 1c, f).

Voxel-wise models showed that A β was not locally associated with hypometabolism in CN A β -positive and MCI A β -positive individuals. On the other hand, these models showed that global A β was associated with hypometabolism in the posterior cingulate, precuneus, lateral temporal, and inferior parietal cortices in CN A β positive (Fig. 1a, d; Supplementary Fig. 2a; and Supplementary Fig. 3a) and MCI A β positive (Fig. 1b, e; Supplementary Fig. 2b; and Supplementary Fig. 3b). In addition, a bootstrap-scheme supported that regional A β did not affect the stability of the global A β effects on hypometabolism in the models mentioned above (Supplementary Fig. 4).

We further replicated the results found in humans using a cohort of 20 rats (10 homozygous McGill-R-Thy1-APP rats overexpressing human A β precursor protein and 10 wild-type Wistar rats). They were 11-month-old, and the wild-type rats provided the means for determining that 11-month McGill-R-Thy1-APP transgenic rats presented mild cognitive symptoms, with a significant baseline genotype effect on the Morris Water Maze (MWM) ($P = 0.03$). In the transgenic A β rats, voxel-wise regressions supported that local A β and hypometabolism were unrelated to one another. On the other hand, the model revealed that global A β load was strongly associated with hypometabolism in the retrosplenial (which corresponds to the posterior cingulate in humans¹⁹), medial and lateral temporal, and inferior parietal cortices (Fig. 1c, f).

A β leads to hypometabolism in functionally connected regions.

In CN A β -negative (Fig. 2a), CN A β -positive (Fig. 2b), and MCI A β -positive (Fig. 2c) individuals, metabolic connectivity analysis showed that the regions comprising the brain's DMN in the precuneus, posterior cingulate, lateral temporal, inferior parietal, and medial prefrontal cortices were highly correlated with each other.

Partial correlation matrices using anatomical segregated regions-of-interest revealed that A β was negatively associated

Table 1 Demographics and key characteristics of the population

	CN A β negative	CN A β positive	MCI A β positive	P-values
Number of subjects	99	53	170	–
Age, y, mean (SD)	74.5 (6.7)	75.3 (6.9)	73.2 (6.7)	0.090
Male, no. (%)	56 (57) ^b	15 (28)	88 (52) ^b	0.002
Education, y, mean (SD)	16.5 (2.8)	16 (2.3)	15.9 (2.7)	0.234
APOE ϵ 4, no. (%)	20 (20)	20 (38) ^a	106 (62) ^{a,b}	<0.001
[¹⁸ F]Florbetapir, mean SUVR (SD)	1.07 (0.05)	1.30 (0.09) ^a	1.35 (0.11) ^{a,b}	<0.001
MMSE, score, mean (SD)	29.1 (1.2)	28.9 (1.1)	27.7 (1.9) ^{a,b}	<0.001
MMSE, slope of change, y, mean (SD)	–0.08 (0.52)	–0.12 (0.57)	–0.95 (1.65) ^{a,b}	<0.001
Follow-up, y, mean (SD)	3.41 (0.97)	3.49 (1.0)	3.26 (1.07)	0.256
Visits, no. (SD)	3.75 (0.69)	3.75 (0.81)	4.06 (1.08) ^a	0.010

P-values indicate the values assessed with analyses of variance for each variable, except for gender and APOE ϵ 4 status where a contingency chi-square was performed. Post-hoc analysis provided significant differences between groups from:

^aCN A β negative

^bCN A β positive

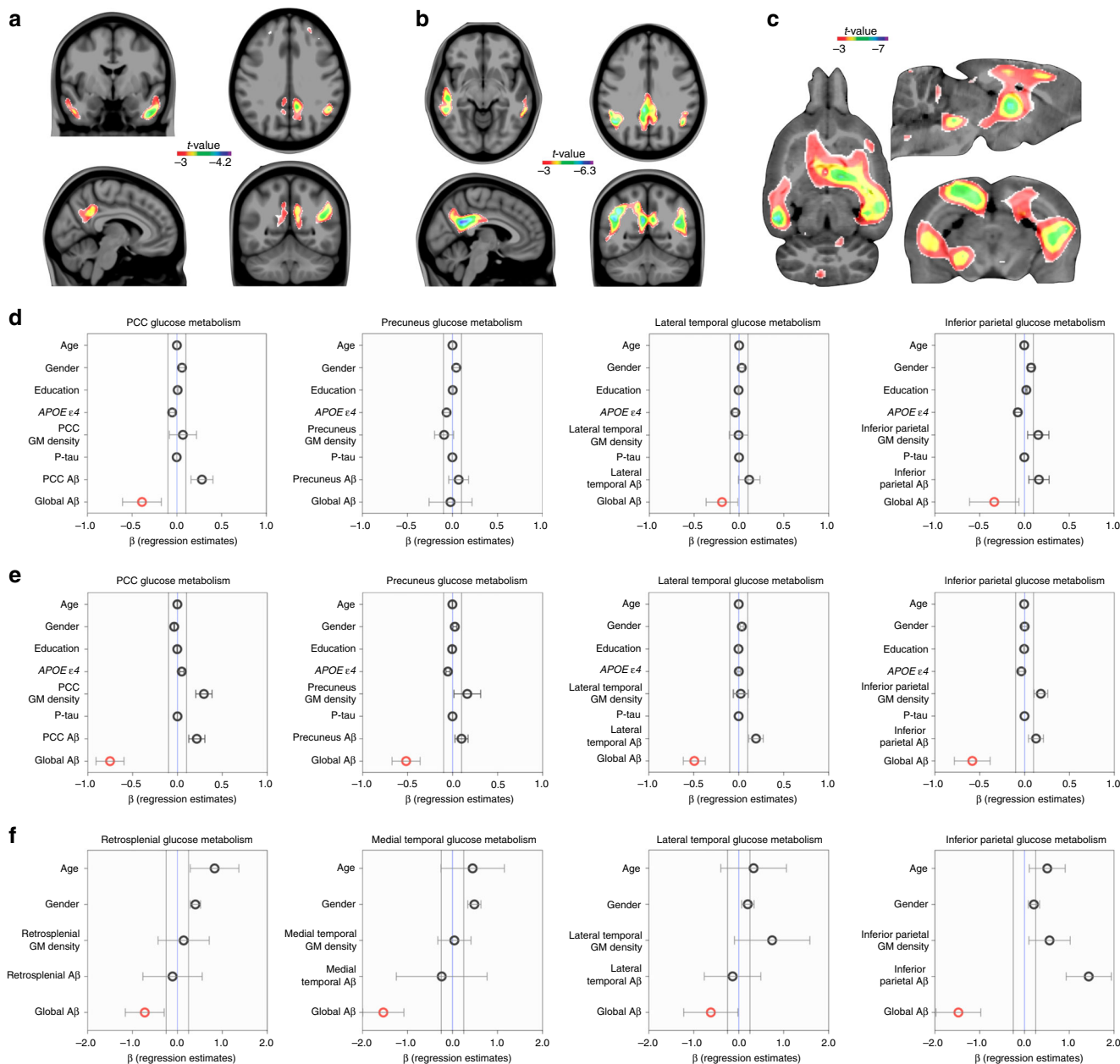


Fig. 1 Global rather than local amyloid-β (Aβ) is associated with DMN hypometabolism. Voxel-wise models, taking voxel and global Aβ values into consideration, showed that global Aβ is associated with hypometabolism in **(a)** CN Aβ positive ($n = 53$) and in **(b)** MCI Aβ-positive ($n = 170$) individuals in the posterior cingulate, precuneus, lateral temporal, and inferior parietal cortices, and in **(c)** transgenic Aβ rats ($n = 10$) in the retrosplenial (which corresponds to the posterior cingulate in humans), medial and lateral temporal, and inferior parietal cortices. The effects of regional Aβ values on its overlapping hypometabolism were negligible in the voxel-wise models. Regression models performed in **(d)** CN Aβ-positive and in **(e)** MCI Aβ-positive individuals within anatomically segregated regions further supported that the effects of local Aβ on hypometabolism (i.e., in the same region) were negligible. Similarly, inside segregated clusters, local Aβ effects on hypometabolism were negligible in **(f)** transgenic Aβ rats. In panels **d-f**, the dots and bars represent β estimates and standard error, respectively, of the independent variables used in the models. Parametric images were FWER corrected at $P < 0.05$ and adjusted for age, gender, education, APOE $\epsilon 4$ status, p-tau, and gray matter (GM) density in humans, and age, gender, and gray matter density in rats

with metabolism in distant, but metabolically connected brain regions in CN Aβ-positive (Fig. 2d) and MCI Aβ-positive (Fig. 2e-l; Supplementary Movie 1) individuals. Notably, the elements of the Aβ-glucose and glucose-glucose matrices were highly negatively correlated with one another in these individuals ($r = -0.5$, $P < 0.0001$), which reinforced the link between metabolic connectivity and Aβ effect. Furthermore, the lack of correlation between the Aβ-glucose matrix elements and the Euclidean distance between regions ($r = 0.1$, $P = 0.3294$)

supported that regions' proximity did not drive these correlations.

Voxel-wise network analysis showed that Aβ load in the precuneus, posterior cingulate, lateral temporal, inferior parietal, and medial prefrontal cortices were associated with distant, but within-DMN hypometabolism in CN Aβ-positive (Fig. 3) and MCI Aβ-positive (Fig. 4b-f) individuals. On the other hand, Aβ outside of the DMN either did not associate with hypometabolism or was associated with hypometabolism predominantly in

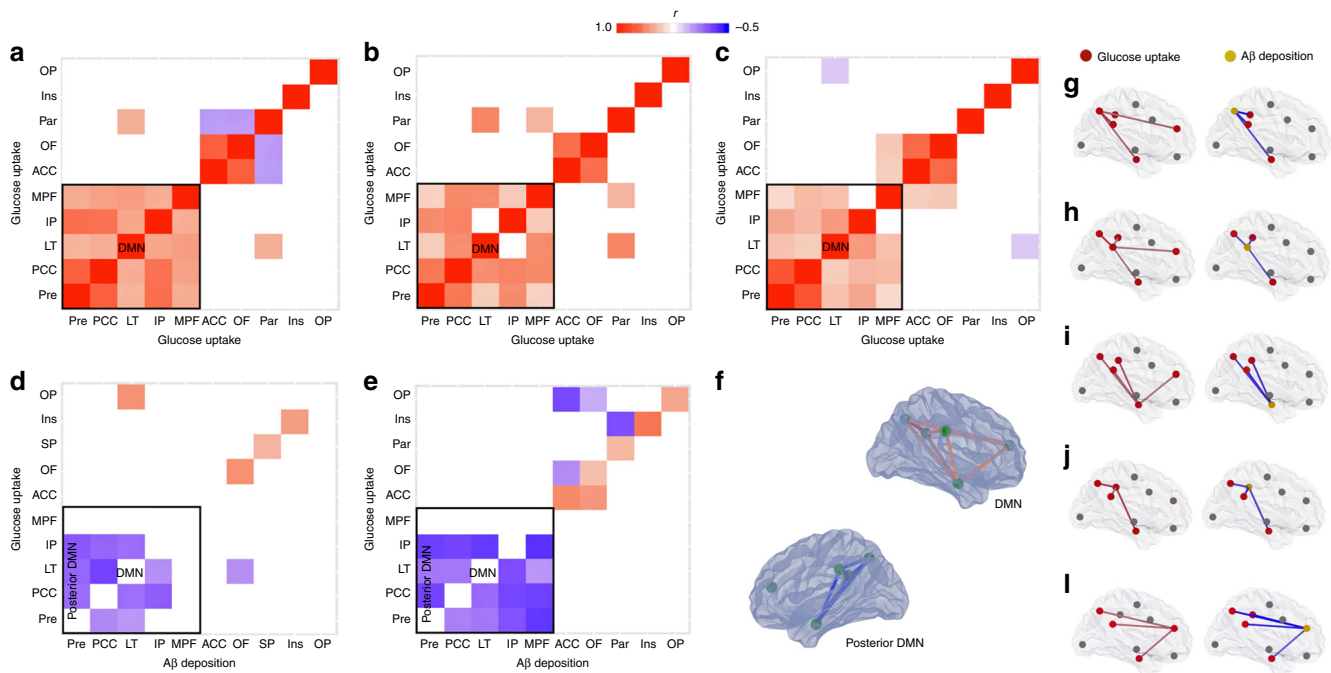


Fig. 2 Amyloid- β ($A\beta$) is associated with hypometabolism in distant, but functionally connected brain regions. Metabolic connectivity analysis between eight regions-of-interest used to compose the global $A\beta$ value in the precuneus (Pre), posterior (PCC) and anterior (ACC) cingulate, inferior parietal (IP), paracentral (Par), medial prefrontal (MPF), lateral temporal (LT), and orbitofrontal (OF), as well as two additional regions in the insular (Ins) and occipital pole (OP) cortices demonstrated that regions comprising the DMN were highly correlated with each other in (a) CN $A\beta$ negative ($n = 99$), (b) CN $A\beta$ positive ($n = 53$), and (c) MCI $A\beta$ positive ($n = 170$) individuals. Partial correlation analysis showed that $A\beta$ within the DMN was associated with distant but within-network hypometabolism in (d) CN $A\beta$ -positive and (e) MCI $A\beta$ -positive individuals. Note that $A\beta$ and its overlapping metabolism showed positive or non-correlation in these individuals. Correlation maps displayed in 3D brain surfaces show the representations of (f) the DMN and posterior DMN and correlations of glucose-glucose (left side) and $A\beta$ -glucose (right side) in the (g) Pre, (h) PCC, (i) LT, (j) IP, and (l) MPF cortices in MCIs $A\beta$ positive (see Supplementary Movie 1). The matrices are presented with Pearson partial correlation coefficients (r) controlled for age, gender, education, $APOE \epsilon 4$ status, p -tau, gray matter density, and Bonferroni-corrected at $P < 0.05$

regions comprising other brain networks, such as the limbic and ventral attention networks (Fig. 4g, h).

In the transgenic $A\beta$ rats, a voxel-wise regression analysis confirmed that $A\beta$ was associated with distant, rather than co-localized, hypometabolism (Fig. 5). As expected, there were no associations between $A\beta$ uptake and metabolism in the wild-type control rats.

Synergy of $A\beta$ and local hypometabolism on cognitive decline.

A voxel-wise interaction model showed that high local levels of $A\beta$ and low local levels of glucose uptake in the precuneus, posterior cingulate, inferior parietal, and lateral temporal cortices synergistically determined subsequent cognitive decline up to 5.6 years in MCI $A\beta$ -positive individuals (Fig. 6a, c; Supplementary Fig. 5; Supplementary Movie 2). In addition, a bootstrap analysis supported that the effect of the local interaction between $A\beta$ and metabolism on cognitive decline was not influenced by a global $A\beta$ effect (Supplementary Fig. 6). Moreover, analysis of variance reinforced that the models with the interaction term best described the relationship between overlapping biomarkers and cognitive decline as compared with reduced models assessing: (1) only $A\beta$, (2) only metabolism, and (3) $A\beta$ plus metabolism, with a $P < 0.0001$ in all three cases. In CN $A\beta$ -positive individuals, the aforementioned interaction was not significantly associated with cognitive decline.

In the transgenic $A\beta$ rats, a voxel-wise interaction model supported the synergy between $A\beta$ and overlapping hypometabolism in the retrosplenial, inferior parietal, and mediolateral temporal cortices as a determinant of cognitive decline over

8 months (Fig. 6b, d). This interaction was absent in the wild-type control rats.

Distant and local $A\beta$ effects on hypometabolism. Structured equation modeling (SEM) showed that the construct in which $A\beta$ occurring in distant regions drives hypometabolism, whereas the interaction between this hypometabolism and the co-localized $A\beta$ determines cognitive decline well describe AD progression (Fig. 7).

Discussion

In summary, our results suggest that $A\beta$ is related to vulnerability in distant brain regions functionally connected by the DMN, whereas the synergy between this vulnerability with local $A\beta$ levels is associated with the clinical progression to dementia (Fig. 8). Remarkably, similar results in transgenic $A\beta$ rats, which do not form neurofibrillary tangles²⁰, supported this model as an independent mechanism of cognitive deterioration.

Our results suggest that the regional hypometabolism observed in AD may derive from distant $A\beta$ effects within brain regions connected by the DMN. This observation is supported by early studies showing that lesions in remote brain regions are associated with DMN hypometabolism^{9–11}. For instance, studies in non-human primates show that localized surgical lesions lead to hypometabolism in metabolically connected brain areas, and that the severity of the inflicted lesion correlates with the degree of remote hypometabolism¹¹. These studies suggest that this occurs due to a synaptic disconnection between the damaged and the remote brain region¹¹. Based on these observations, one may

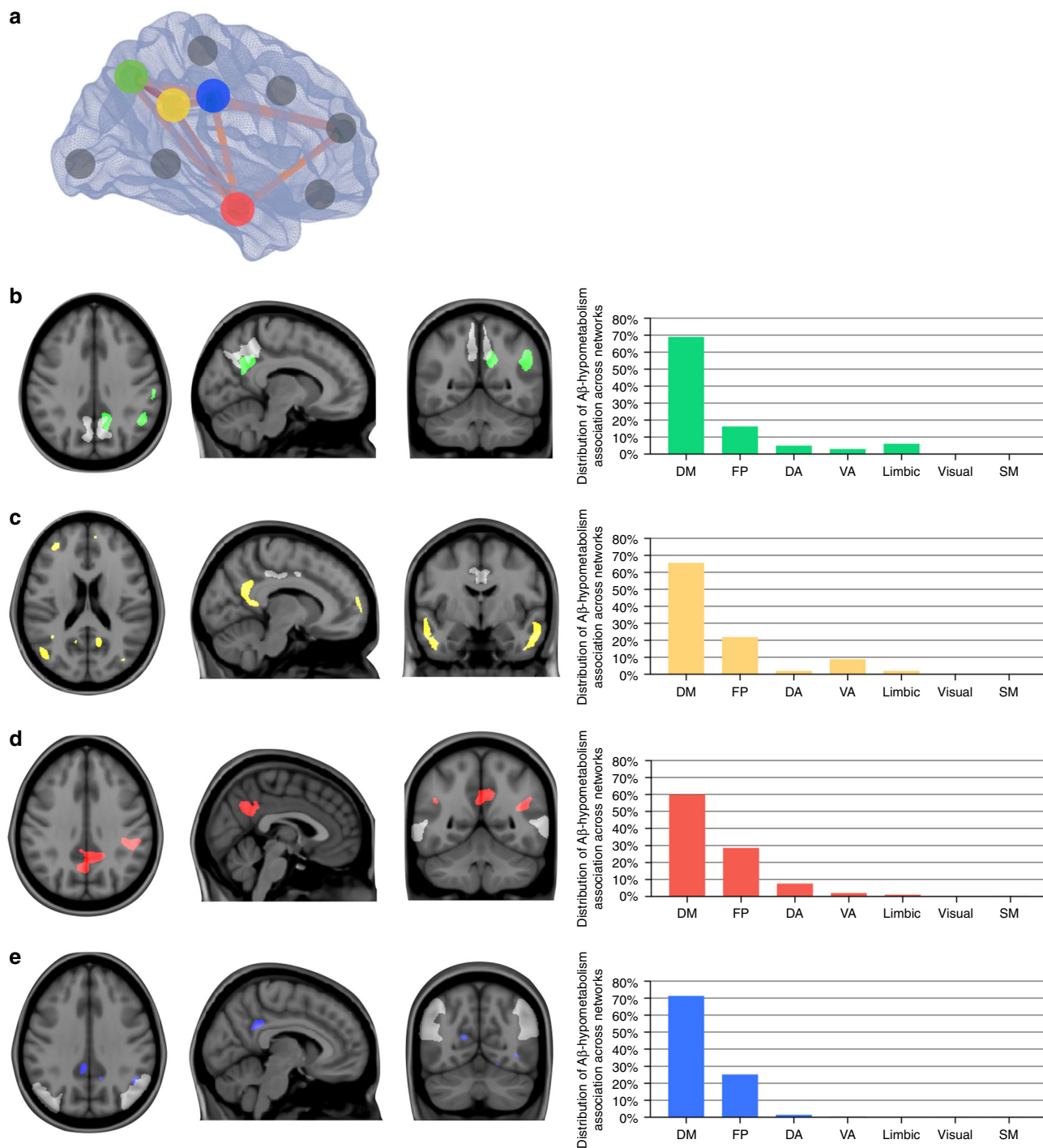
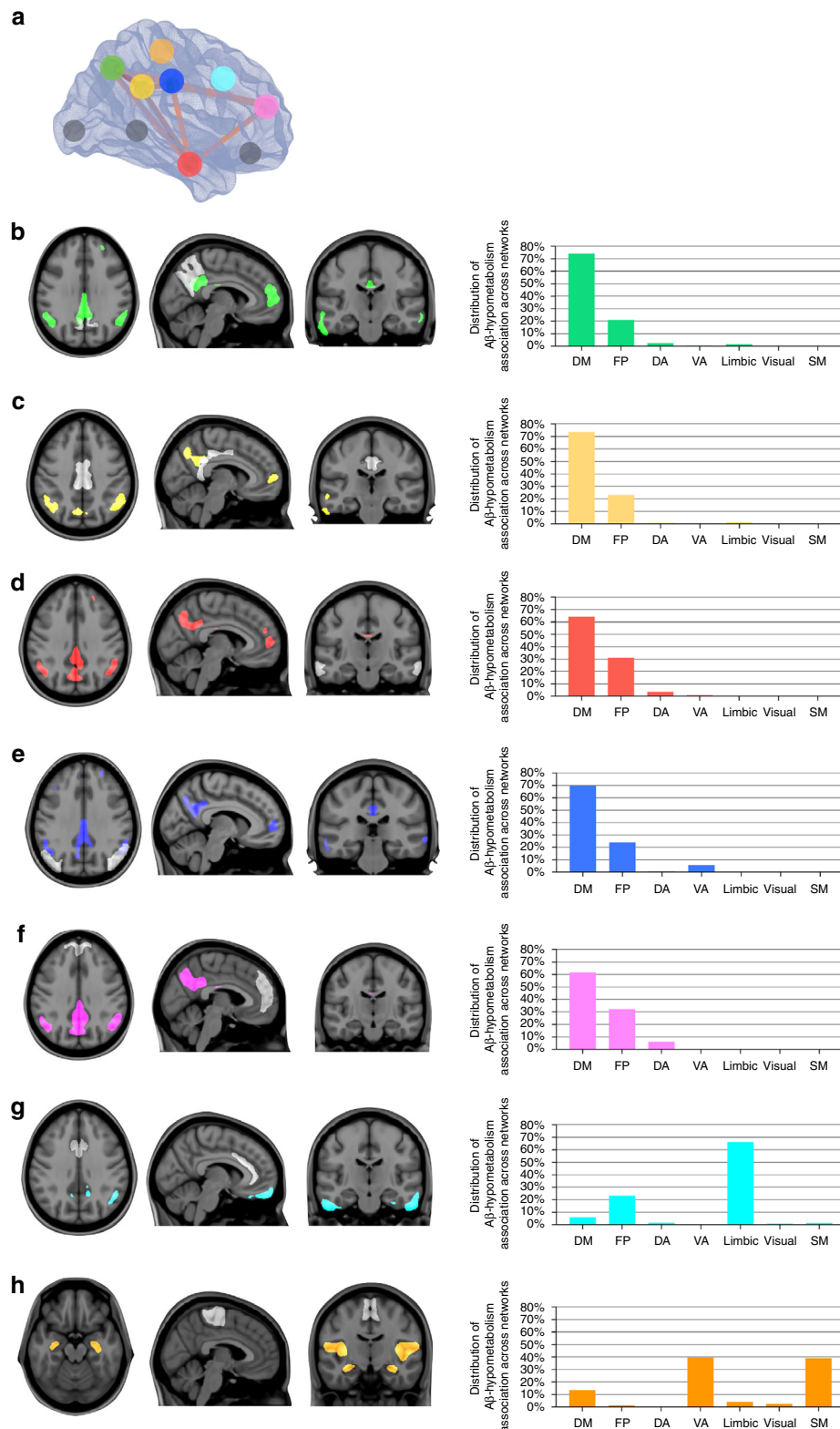


Fig. 3 Amyloid- β ($A\beta$) in DMN is predominantly associated with distant within-network hypometabolism in CN $A\beta$ positive. **a** In the 3D brain, the dots represent the regions-of-interest in which $A\beta$ values were obtained. The regions in which $A\beta$ values were obtained are also shown in white, superimposed on the structural MRI templates in panels **b–e**. Statistical parametric maps, overlaid on a structural MRI template, show the brain regions where voxel-wise glucose metabolism was negatively associated with $A\beta$ load in the **(b)** precuneus (green), **(c)** posterior cingulate (yellow), **(d)** lateral temporal (red), and **(e)** inferior parietal (blue) cortices in CN $A\beta$ positive ($n = 53$). The bar graphs show the distribution of the voxels in the aforementioned statistical parametric maps across seven functional brain networks (DM default mode, FP frontoparietal, DA dorsal attention, VA ventral attention, limbic visual, SM somatomotor). Thus, the sum of the seven bars in each graph is 100%. $A\beta$ in the medial prefrontal, anterior cingulate, orbitofrontal, paracentral, insular, and occipital pole cortices (gray dots) did not significantly associate with hypometabolism. Parametric images were FWER corrected at $P < 0.05$ and adjusted for age, gender, education, APOE $\epsilon 4$ status, p-tau, and gray matter density

argue that the regional patterns of hypometabolism in AD derive from a decreased synaptic input from distant, but DMN connected brain areas affected by $A\beta$. Also, we have shown that global $A\beta$ load, rather than local, is associated with regional DMN

hypometabolism, which is in line with previous studies⁴. Expanding upon these studies, our findings indicate that this might be explained by the fact that $A\beta$ from several distant brain regions contributes to regional hypometabolism. Therefore, it



seems reasonable that a global A β composite contemplating all distant brain regions shows a better association with regional hypometabolism than merely local A β levels. Altogether, our results corroborate the deleterious effects of A β on the DMN as previously suggested by the network neurodegeneration hypothesis of AD^{15,21,22}, by showing that A β leads to hypometabolism in distant brain regions interconnected by the DMN, rather than locally, as inferred from the traditional view²².

On the other hand, our results support the synergy between A β and topographically overlapping DMN vulnerability as a driving force behind dementia symptoms. It is well known that individuals might respond differently to A β based on their capacity to compensate through the reconfiguration of pre-existent or recruitment of alternative synapses using the DMN^{22,23}. Moreover, DMN hypometabolism has been repeatedly suggested to represent underlying network

Fig. 4 Amyloid- β ($A\beta$) in DMN is predominantly associated with distant within-network hypometabolism in MCI $A\beta$ positive. **a** In the 3D brain, the dots represent the regions-of-interest in which $A\beta$ values were obtained. The regions in which $A\beta$ values were obtained are also shown in white, superimposed on the structural MRI templates in panels **b-h**. Statistical parametric maps, overlaid on a structural MRI template, show the brains regions where voxel-wise glucose metabolism was negatively associated with $A\beta$ load in the **(b)** precuneus (green), **(c)** posterior cingulate (yellow), **(d)** lateral temporal (red), **(e)** inferior parietal (blue), **(f)** medial prefrontal (pink), **(g)** anterior cingulate (light blue), and **(h)** paracentral (orange) cortices in MCI $A\beta$ positive ($n = 170$). The bar graphs show the distribution of the significant voxels in the aforementioned statistical parametric maps across seven functional brain networks (DM default mode, FP frontoparietal, DA dorsal attention, VA ventral attention, limbic visual, SM somatomotor). Thus, the sum of the seven bars in each graph is 100%. $A\beta$ in the orbitofrontal, insular, and occipital pole cortices (gray dots) did not significantly associate with hypometabolism. Parametric images were FWER corrected at $P < 0.05$ and adjusted for age, gender, education, APOE $\epsilon 4$ status, p-tau, and gray matter density

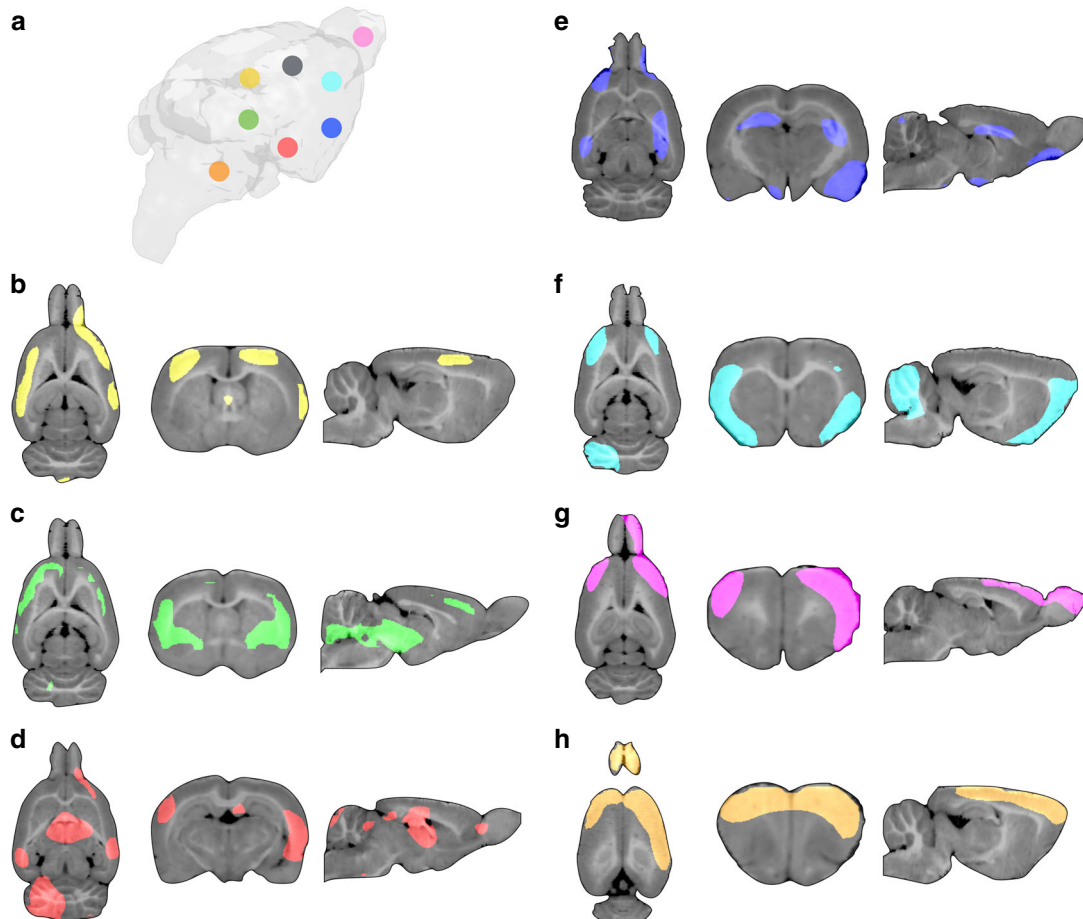


Fig. 5 Amyloid- β ($A\beta$) is associated with distant within-network hypometabolism in transgenic $A\beta$ rats. **a** 3D brain representation of the regions-of-interest in which the $A\beta$ values were obtained. Statistical parametric maps, overlaid on a structural MRI template, show the brains regions where voxel-wise glucose metabolism was negatively associated with $A\beta$ load in the **(b)** retrosplenial (yellow), **(c)** medial temporal (green), **(d)** lateral temporal (red), **(e)** inferior parietal (blue), **(f)** frontoparietal (light blue), **(g)** olfactory bulb (pink), and **(h)** cerebellar (orange) cortices in transgenic $A\beta$ rats ($n = 10$). $A\beta$ in the somatosensory cortex (gray dot) did not significantly associate with hypometabolism. Parametric images were FWER corrected at $P < 0.05$ and adjusted for age, gender, and gray matter density

dysfunction^{4,14,24}, and metabolic connectivity has been shown to represent synaptic pathways in the human brain²⁵⁻²⁷. Thus, the hypometabolism in our results may indicate the dysfunction of the DMN in recruiting alternative synapses in the face of toxic effects of $A\beta$. As such, our model could be understood to mean that the toxic effects of $A\beta$ and the underlying local levels of DMN dysfunction in handling these toxic effects synergistically determine the severity of the subsequent cognitive deterioration. Together, these findings support that regional vulnerability to $A\beta$ plays an important role in the progression to AD and that this occurs through the decrease of the capacity of the DMN to compensate for the deleterious effects of $A\beta$ ²⁸⁻³⁰.

Although our results suggested that regional metabolic vulnerability depends on distant $A\beta$, other factors may potentiate this vulnerability in AD. Determinants of such vulnerability might include inflammatory agents and pathology related stressors that might lead to biochemical dysregulations, resulting in decreased synaptic exchanges and therefore hypometabolism^{29,31-33}. Other factors may include cerebral vascular diseases, systemic metabolic disorders, and allele variants implicated in brain plasticity and resilience³⁴⁻³⁶. Also, previous studies have proposed that APOE $\epsilon 4$ may lead to hypometabolism independently of $A\beta$ ^{37,38}. Recently, it has been shown that astrocytes play an important role in [¹⁸F]FDG signal³⁹. Since astrocytes have been associated with numerous mechanisms involving neuronal plasticity and transmission⁴⁰,

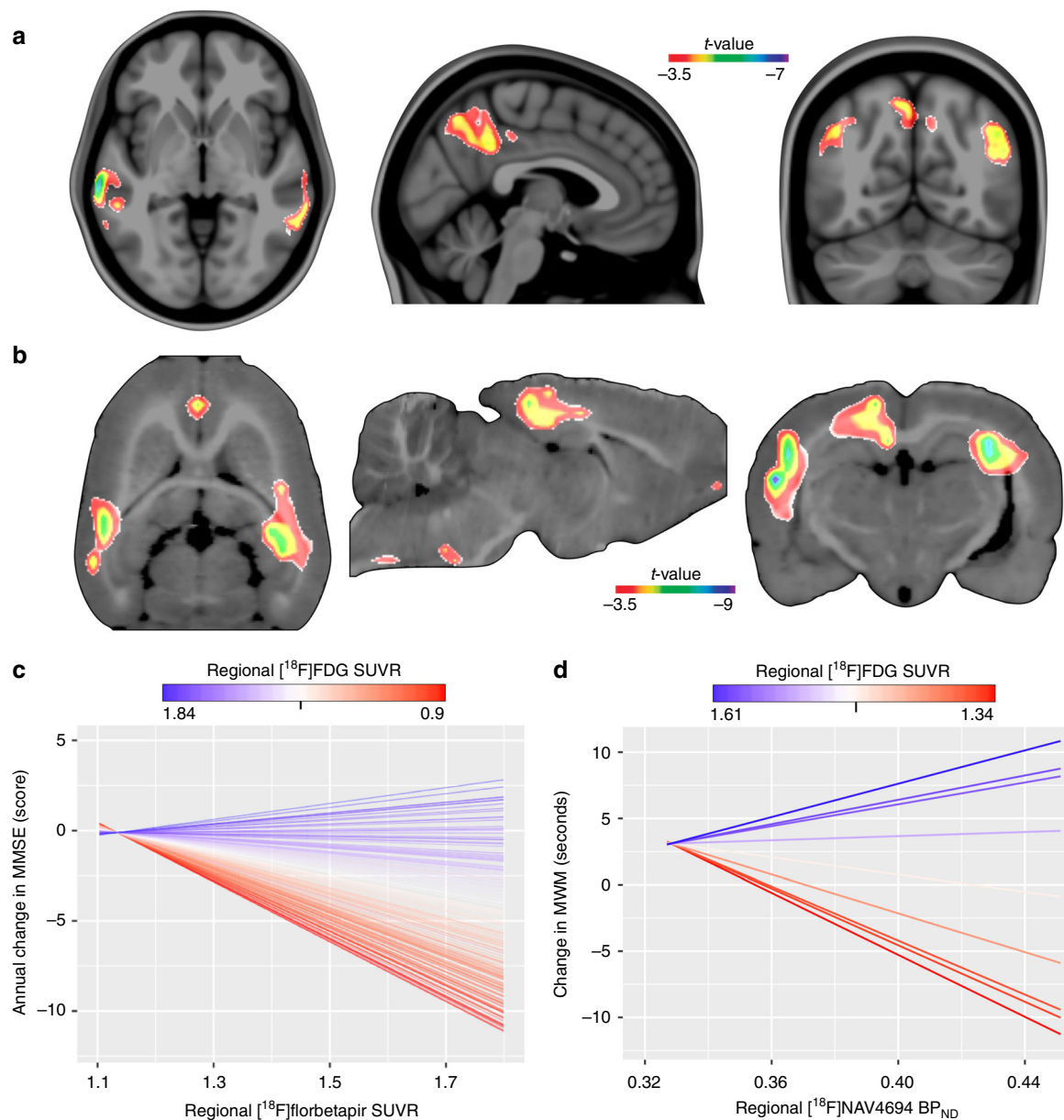


Fig. 6 The synergy of amyloid- β ($A\beta$) with overlapping hypometabolism drives cognitive decline. **a** The parametric map shows significant interactive effects at a voxel level between $A\beta$ and glucose uptake on MMSE worsening over up to 5.6 years in the precuneus, posterior cingulate, inferior parietal, and lateral temporal cortices in MCIs $A\beta$ positive ($n = 170$). The aforementioned interaction was not significantly associated with cognitive decline in CN $A\beta$ positive. **b** In transgenic $A\beta$ rats, significant voxel-wise interactive effects between $A\beta$ and glucose uptake on MWM worsening over 8 months were found in the retrosplenial cortex, which corresponds to the posterior cingulate in humans, inferior parietal, and mediobasal and lateral temporal cortices. The plots show the graphical representation of the interaction in **(c)** MCIs $A\beta$ positive (see Supplementary Movie 2) and in **(d)** transgenic $A\beta$ rats, where each parallel line represents a single subject. For longitudinal changes in MMSE and MWM, lower values indicate greater impairment. Parametric images were FWER corrected at $P < 0.05$ and adjusted for global $A\beta$, age, gender, education, $APOE \epsilon 4$ status, p-tau, gray matter density, and follow-up duration in humans, and adjusted for global $A\beta$, age, gender, and gray matter density in rats

astrocytic dysfunction may be involved in the DMN vulnerability reported here.

As previously reported by our group and others, interactions between $A\beta$ and tau proteins determine AD progression^{34,41,42}. Since glucose metabolism is proposed to be closely linked to tau pathology³⁶, the regional effects of hypometabolism in this study could be merely inferred as a proxy of neurofibrillary tangles. Therefore, we used the McGill-R-Thy1-APP rats overexpressing human $A\beta$ pathology to clarify our results. Remarkably, the similar results in our transgenic $A\beta$ rats, which do not form tangles²⁰, supported the associations between $A\beta$ and DMN

vulnerability as a tau-independent mechanism of cognitive deterioration. It is worth to mention that, although independent, this model is likely to be highly potentiated by neurofibrillary tangles, which is supported by the more markedly cognitive deterioration found in humans as compared with the transgenic $A\beta$ rats. Indeed, it is probable that the $A\beta$ -induced metabolic vulnerability reported here will create a favorable environment, also for neurofibrillary tangles to determine cognitive decline. Importantly, the DMN is an evolutionarily conserved feature involved in the integration of cognitive abilities in humans and rodents^{19,43}.

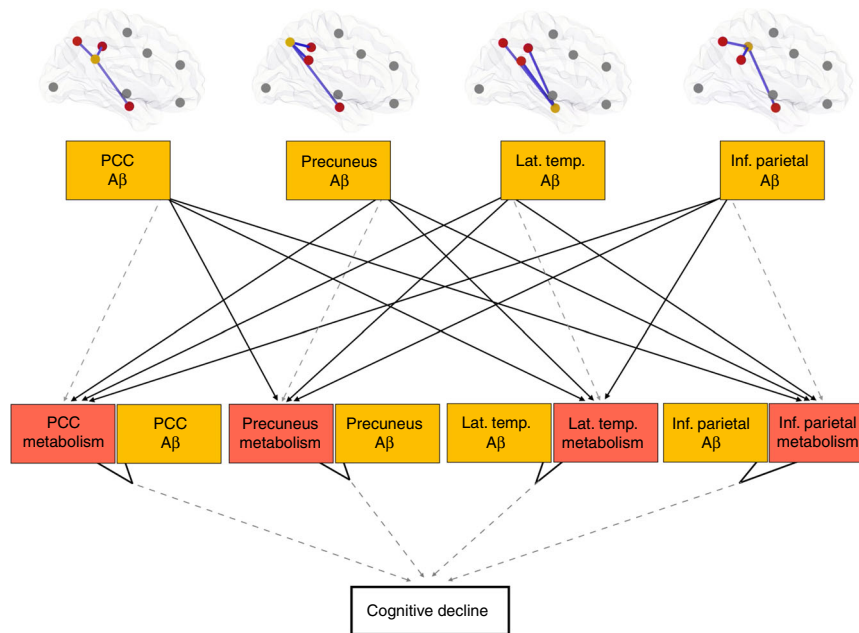


Fig. 7 Structured equation modeling showed that the distant and local amyloid- β ($A\beta$) effects on hypometabolism well describe AD progression. This model represents the hypothesis that distant and local $A\beta$ effects (yellow) on posterior DMN hypometabolism (red) are associated with cognitive decline. The model used CN $A\beta$ -positive and MCI $A\beta$ -positive individuals, and the associations were adjusted for age, gender, education, APOE $\epsilon 4$ status, p-tau, and gray matter density. Negative associations are shown in solid lines, whereas dashed lines show positive associations. Notably, $A\beta$ showed positive association with its overlapping metabolism but negative associations with distant metabolism. The hypothesized model fitted the data well ($n = 223$, $\chi^2 = 81$, degrees of freedom = 21, $P < 0.01$, standardized root mean square residual (SRMR) = 0.092, and Comparative Fit Index (CFI) = 0.966)

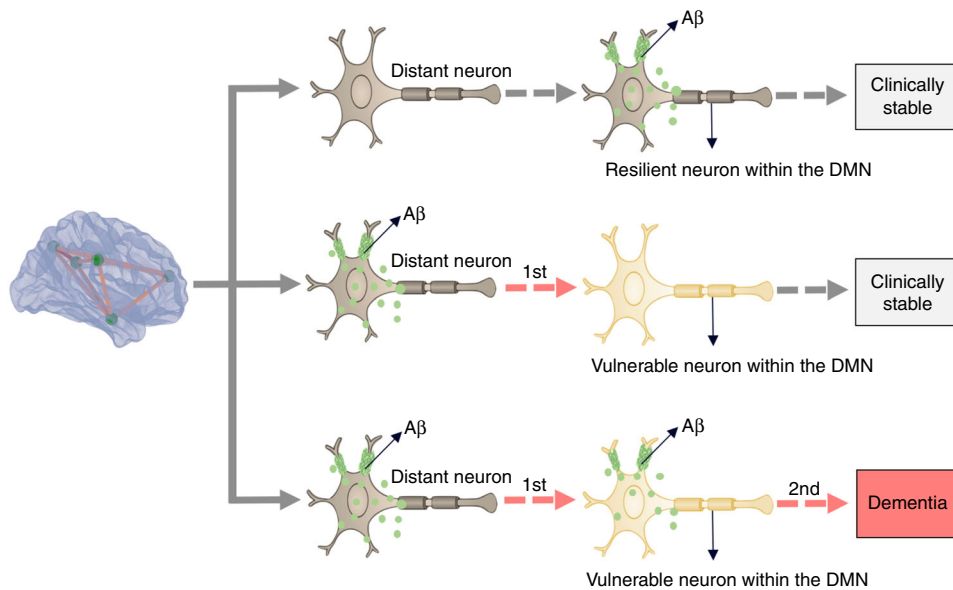


Fig. 8 Schematic representation of the distant and local amyloid- β ($A\beta$) effects on metabolism. $A\beta$ from distant brain regions leads to regional metabolic vulnerability, whereas the synergy between this vulnerability with local $A\beta$ effects drives the clinical progression of dementia. Importantly, either $A\beta$ or metabolic vulnerability as a single abnormality is insufficient to determine dementia

Methodological strengths of this study include the use of continuous biomarkers analyzed with a robust voxel-wise approach and the use of an animal model in a controlled experimental setting, which permitted assessing the effects of $A\beta$ on metabolism independent of possible confounding factors, such as neurofibrillary tangles. This study has methodological limitations. Our studied population represents a self-selected group of elderly individuals motivated to participate in an AD study. Therefore, these individuals may not

represent a general elderly population. Importantly, the model proposed in this study should be confirmed by future studies using different populations and long-term sequential biomarkers and clinical observations performed at multiple time points. In a heterogeneous population such as MCIs, some individuals have early $A\beta$ deposition and may present a positive association between $A\beta$ and metabolism⁴⁴, while others in later disease stages may present a negative association. Thus, these opposing phenomena in the same population

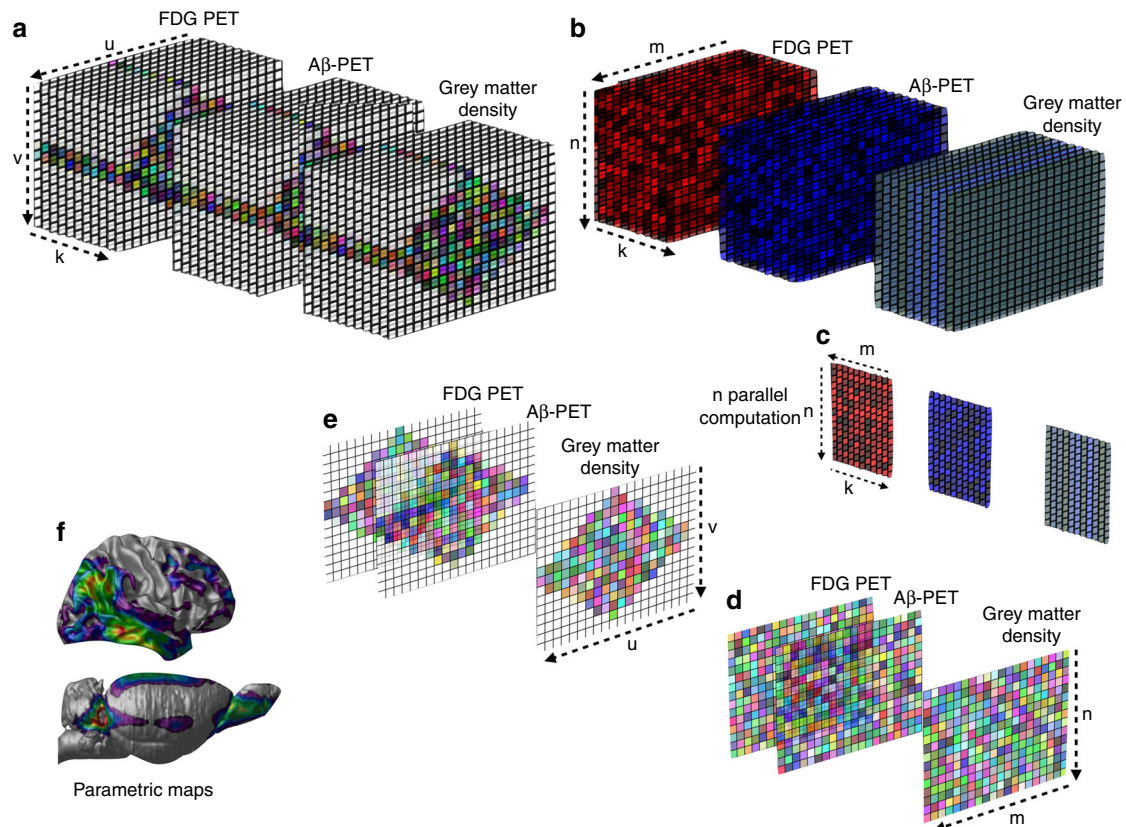


Fig. 9 Multimodal analytical operations performed at every brain voxel. The illustration shows the analytical model developed to perform statistical operations on multiple scalar variables and with multiple imaging modalities at every brain voxel in humans and rats. Briefly, **(a)** the brain image data were retrieved from a 3D image space and converted to a 2D matrix in the image space for each subject. **(b)** Then, the image data were transformed into the processing space using artificial parcellation. **(c)** In the computational phase, the statistical modeling was performed in every brain voxel accounting for voxel and global PET uptake values, as well as voxel gray matter density and covariates. **(d)** Subsequently, statistical matrices were generated from the results and **(e)** transformed back to the 3D image space. **(f)** Finally, 3D parametric maps displaying the results of the regression models were generated. k = subjects, u = image slice, v = slice elements, m = artificial parcellation, n = elements in each parcellation

may obscure the regional association between these biomarkers. Although we restricted our analyses to A β -positive individuals and adjusted the models for p-tau levels, we cannot exclude that other pathological processes than A β —such as tau aggregates, neuroinflammation, cholinergic depletion, cerebrovascular disease, α -synuclein, and TDP-43—have influenced the interpretation of these results⁴⁵. Also, the lack of tau PET images is an important limitation of these results. McGill-R-Thy1-APP rats develop A β plaque and oligomeric species⁴⁶. Since regional A β load is highly associated with regional oligomeric A β ³², the deleterious effects of A β on metabolism reported here might reflect oligomers rather than fibrillar conformations. Also, there are large pathophysiological differences between human AD and transgenic models overexpressing A β . However, it is important to mention that the less aggressive progression of A β in rats, compared with mice, makes this model more similar to the insidious disease progression of elderly with sporadic AD. For instance, McGill-R-Thy1-APP mice and rats express exactly the same mutations, but rats present plaques at 6–9 months while mice do as early as at 4 months²⁰. Importantly, the much larger brain size of rats (approximately five times bigger than mice) makes the identification of specific brain structures using techniques with low spatial resolution, such as PET, possible to be performed in this study⁴⁷.

To conclude, our results suggest that within the brain's DMN, regional vulnerability is associated with distant A β , while the

interaction between this vulnerability with local A β is associated with dementia.

Methods

Human subjects. The data used in the preparation of this article were obtained from the Alzheimer's Disease Neuroimaging Initiative (ADNI) database, phases GO, and 2 (adni.loni.usc.edu). ADNI was launched in 2003 as a public-private partnership, led by Principal Investigator Michael W. Weiner, MD. The primary goal of ADNI has been to test whether serial magnetic resonance imaging (MRI), PET, other biological markers, and clinical and neuropsychological assessments can be combined to measure the progression of MCI and early AD. ADNI study was conducted according to Good Clinical Practice guidelines, US 21CFR Part 50—Protection of Human Subjects, and Part 56—Institutional Review Boards, and pursuant to state and federal HIPAA regulations and was approved by the Institutional Review Board of each participating site (adni.loni.usc.edu). Written informed consent for the study was obtained from all participants and/or authorized representatives. We studied participants who had [¹⁸F] FDG PET, [¹⁸F]florbetapir PET, MRI, and cerebrospinal fluid (CSF) p-tau at baseline, as well as cognitive assessments at baseline and follow-up. Cognition was assessed with Mini-Mental State Examination (MMSE), Rey Auditory Verbal Learning Test 30-min delayed recall, Trail Making Test Part A and B, and Boston Naming Test. For this study, we selected CN individuals and MCI A β -positive individuals. CN individuals had an MMSE score of 24 or higher, and a clinical dementia rating (CDR) of 0. MCIs had MMSE scores equal to or greater than 24, a CDR of 0.5, subjective and objective memory impairments, essentially normal activities of daily living, and were not demented (National Institute of Neurological and Communicative Disorders and Stroke–Alzheimer's Disease and Related Disorders Association criteria for probable AD⁴⁸). Individuals did not present other neuropsychiatric disorders (further information about ADNI cognitive tests and inclusion/exclusion criteria may be found at www.adni-info.org).

Animal use. We imaged and cognitively assessed 20 rats, 10 homozygous McGill-R-Thy1-APP rats overexpressing human A β precursor protein²⁰ with the Swedish

double mutation (K670N, M671L⁴⁹) and the Indiana mutation (V717F⁵⁰), along with 10 wild-type Wistar rats. Half of the rats in each group were males. The rats performed MRI, [¹⁸F]FDG PET, and [¹⁸F]NAV4694 PET at baseline (11-month-old (SD 0.14)), as well as the MWM test at baseline and at 8 months follow-up. The MWM was performed with four trials per day, over 4 consecutive days. The rats were placed on the platform if they failed to find it within 90 s, and we assumed a maximum trial length of 90 s⁵¹. The time to find the platform was measured with overhead camera tracking using ANY-maze software (Stoelting Co.). One probe trial (no platform) and one visible platform trial were also conducted at the end of the 4th day. All rats were kept in ventilated cages in groups of two in environmentally controlled conditions: 12 h light/dark cycle at 21 °C with access to food and water ad libitum. All procedures involving rats were performed in accordance with the ethical regulations for animal testing and research from the Canadian Council on Animal Care and the National Institutes of Health and received ethical approval from the Animal Care Ethics Committee of the McGill University.

Human imaging methods. MRI and PET acquisitions followed ADNI protocols (<http://adni.loni.usc.edu/methods>). T1-weighted MRIs were corrected for field distortions, non-uniformity corrected, brain masked, segmented, and non-linearly transformed to the MNI reference space using the CIVET pipeline⁵². Subsequently, gray matter density was computed using voxel-wise morphometry. PET scans used [¹⁸F]florbetapir tracer for imaging A β and [¹⁸F]FDG tracer for imaging glucose metabolism. Briefly, PET images were non-linearly registered to the MNI space using the individual's PET/T1-weighted native MRI registration and the individual's non-linear MRI transformation to MNI space. PET images were spatially smoothed to achieve a final 8-mm full-width at half-maximum resolution and corrected for partial volume effects using region-based voxel-wise (RBV) method⁵³. [¹⁸F]Florbetapir and [¹⁸F]FDG SUVR images were obtained using the cerebellum gray matter and the pons as reference regions, respectively. A global [¹⁸F]florbetapir SUVR value was obtained using the precuneus, posterior and anterior cingulate, inferior parietal, paracentral, medial prefrontal, lateral temporal, and orbitofrontal cortices. Individuals were A β positive if [¹⁸F]florbetapir SUVR > 1.15⁵⁴. Further information and the schematic representation of the human imaging methods pipeline may be found elsewhere³⁴ and in the Supplementary Fig. 7.

Rat imaging methods. MRIs were acquired using a Bruker 7T BioSpec 70/30 USR animal dedicated. First, the rats were anesthetized with 5% isoflurane/medical air, which was then maintained at 1–2% after placing the animals in the scanner, with the breathing at 20–30 breaths per min. We used a 37 °C constant airflow to maintain the rats warm. The structural images were generated using the 7T Bruker standard 3D-True Fast Imaging with Steady State Precession (FISP) pulse sequence⁵⁵. Gray matter density was computed using voxel-wise morphometry. PET images were acquired using a CTI Concorde R4 microPET for rodents (Siemens). PET scans used [¹⁸F]NAV4694 tracer for imaging A β and [¹⁸F]FDG tracer for imaging glucose metabolism. In preparation for the scans, rats received anesthesia using 5% isoflurane, which was then maintained at 2% throughout the procedure. The animals underwent a 9-min transmission scan using a rotating⁵⁷ Co point source before each PET image acquisition. For [¹⁸F]NAV4694, a 60-min dynamic emission scan began concomitantly with the bolus injection of the radiotracer via the tail vein. For [¹⁸F]FDG, after fasting for 12 h, the animals received the radiotracer injection during the awake state via the tail vein. Then, a 20-min dynamic emission scan at 50 min post injection was performed. PET images were reconstructed using a maximum a posteriori algorithm and corrected for scattering, dead time, and decay. [¹⁸F]NAV4694 non-displaceable binding potential (BP_{ND}) parametric images were generated using the Simplified Reference Tissue Method with the cerebellar gray matter as a reference⁵⁶. [¹⁸F]FDG SUVR images were generated using the pons as the reference region. PET images were co-registered to the animal's MRI and non-linearly transformed to a standardized rat brain space created based on the wild-type rats MRIs. PET images were spatially smoothed using a Gaussian kernel with a full-width at half-maximum of 2.4 mm. Further information and the schematic representation of the rat imaging methods pipeline may be found elsewhere⁴⁷ and in Supplementary Fig. 8.

Human CSF analysis. CSF p-tau at threonine 181 was measured using a multiplex xMAP Luminex platform (Luminex Corp, Austin, TX) with INNO-BIA AlzBio3 immunoassay kit-based reagents (Innogenetics, Ghent, Belgium)^{57,58}. Details about CSF acquisition and quantification can be found at www.adni-info.org.

Statistical analysis. Regressions were performed using R Statistical Software Package version 3.1.2 (<http://www.r-project.org/>) to test for significant associations between biomarkers and also demographic differences between groups for continuous variables, whereas chi-square was used for categorical variables. The voxel-wise analyses were performed using MATLAB software version 9.2 (<http://www.mathworks.com>) with a computational framework developed to perform complex voxel-wise statistical operations, such as interaction models, using multiple imaging modalities in humans and rats (Fig. 9)⁵⁹.

In humans, we evaluated the brain abnormalities associated with the clinical diagnosis using a voxel-wise analysis of variance, in which the signal intensity of

the imaging modality was used as the dependent variable, while the diagnosis was used as the independent variable.

Subsequently, voxel-wise regression models, taking into consideration voxel and global A β concentrations, tested the association between A β deposition and glucose metabolism in humans and rats. In humans, we also considered age, gender, education, APOE $\epsilon 4$ status, p-tau, and gray matter density in the models, whereas in rats, age, gender, and gray matter density were considered.

Then, connectivity analysis was performed using eight regions-of-interest used to assess the global PET A β value in the precuneus, posterior and anterior cingulate, inferior parietal, paracentral, medial prefrontal, lateral temporal, and orbitofrontal cortices as well as two additional regions in the insular and occipital cortices, using coordinates in the MNI ICBM atlas⁶⁰. The edge values were assumed to be the correlation coefficients between regions, which were used as the matrix elements. Interregional correlation coefficients were computed using Pearson partial correlation analysis controlling for age, gender, education, APOE $\epsilon 4$ status, p-tau, and gray matter density. Metabolic connectivity was assessed with a symmetric matrix showing the strength of the correlation of glucose uptake between regions. An asymmetric matrix assessed the associations of A β deposition and hypometabolism between regions-of-interest. The matrices were corrected for multiple comparisons using Bonferroni at $P < 0.05$. FDG-FDG and FDG-A β matrix elements were further correlated using Pearson's correlation. We also tested the correlation between the matrix elements and the Euclidean distance between nodes (mm) to ensure that the results were not driven by regions' proximity.

In humans, we further performed a voxel-wise connectivity analysis using A β values within the 10 regions-of-interest mentioned above as independent predictors and glucose metabolism at every voxel as the outcome accounting for age, gender, education, APOE $\epsilon 4$ status, p-tau, and gray matter density. In addition, a brain network atlas provided the means to assess the overlap between the results and functional networks (default mode, frontoparietal, dorsal and ventral attention, limbic, visual, and somatomotor networks⁶¹). In rats, a voxel-wise connectivity analysis was performed using A β values in eight regions-of-interest, based on previous literature, in retrosplenial, medial temporal, lateral temporal, inferior parietal, frontoparietal, olfactory bulb, cerebellar, and somatosensory cortices as independent predictors and glucose metabolism at every voxel as the outcome accounting for age, gender, and gray matter density^{19,43}.

The association between image biomarkers and cognitive changes was tested in humans with a voxel-wise model using the slope of change in cognitive performance as the dependent variable and the main and interactive effects of [¹⁸F]florbetapir SUVR and [¹⁸F]FDG SUVR at every voxel as independent predictors. The slope of change in cognitive performance was defined using all available MMSE evaluations for each subject with a mean of 4 (SD: 0.96) evaluations spanning up to 5.6 years (mean of 3.4 years (SD: 1.02)). The analysis was adjusted for global A β , age, gender, education, APOE $\epsilon 4$ status, p-tau, gray matter density, and follow-up duration. The voxel-wise interaction model was built as follows:

$$\begin{aligned} \Delta\text{MMSE} = & \beta_0 + \beta_1(\text{Florbetapir SUVR}) \\ & + \beta_2(\text{FDG SUVR}) \\ & + \beta_3(\text{Florbetapir SUVR} * \text{FDG SUVR}) \\ & + \text{covariates} + \text{error} \end{aligned} \quad (1)$$

In rats, we built the same voxel-wise model performed in humans using the slope of change in the MWM as the dependent variable and the main and interactive effects of [¹⁸F]NAV4694 BP_{ND} and [¹⁸F]FDG SUVR as independent predictors. A slope of change in cognitive performance was defined for each rat using the MWM changes in average (four trials) latency to find the platform over 8 months. The model was adjusted for global A β , age, gender, and gray matter density. The voxel-wise interaction model was built as follows:

$$\begin{aligned} \Delta\text{MWM} = & \beta_0 + \beta_1(\text{NAV4694 BP}_{\text{ND}}) \\ & + \beta_2(\text{FDG SUVR}) \\ & + \beta_3(\text{NAV4694 BP}_{\text{ND}} * \text{FDG SUVR}) \\ & + \text{covariates} + \text{error} \end{aligned} \quad (2)$$

Statistical parametric maps were corrected for multiple comparisons, and the statistical significance was defined using a family-wise error rate (FWER) threshold of $P < 0.05$.

The presence of collinearity between regional and global A β PET values could inflate the variance of estimates, potentially leading to incorrect the statistical results of significance when both effects are used in the same model. To assess whether such case occurred in our analysis, we investigated the stability of estimates by measuring the variance based on a resampling scheme repeated 10,000 times. In addition, the adequacy of the models with the interaction term was further assessed with an analysis of variance comparing the interaction model with each reduced model: (1) A β , (2) metabolism, and (3) A β plus metabolism.

The relationship between A β , metabolism, and the longitudinal cognitive decline was further assessed with SEM using the R package Lavaan⁶². SEM was built to test the specific hypotheses demonstrated in the figure's meta-model⁶³. SEM was classified as satisfactory whether: comparative fit index (CFI) > 0.95 and standardized root mean-square residual (SRMR) < 0.1⁶⁴.

Data availability

All human data used in this study were downloaded online at the Alzheimer's Disease Neuroimaging Initiative database (adni.loni.usc.edu). The locally processed human brain images (MRI and PET) and the animal data are not publicly available for download, but might be retrieved from the correspondent author on a request.

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References

- Edison, P. et al. Amyloid, hypometabolism, and cognition in Alzheimer disease: an [¹¹C]PIB and [¹⁸F]FDG PET study. *Neurology* **68**, 501–508 (2007).
- Engler, H. et al. Two-year follow-up of amyloid deposition in patients with Alzheimer's disease. *Brain: a J. Neurol.* **129**, 2856–2866 (2006).
- Lowe, V. J. et al. Association of hypometabolism and amyloid levels in aging, normal subjects. *Neurology* **82**, 1959–1967 (2014).
- Altmann, A. et al. Regional brain hypometabolism is unrelated to regional amyloid plaque burden. *Brain: a J. Neurol.* **138**, 3734–3746 (2015).
- Furst, A. J. et al. Cognition, glucose metabolism and amyloid burden in Alzheimer's disease. *Neurobiol. aging* **33**, 215–225 (2012).
- Li, Y. et al. Regional analysis of FDG and PIB-PET images in normal aging, mild cognitive impairment, and Alzheimer's disease. *Eur. J. Nucl. Med. Mol. imaging* **35**, 2169–2181 (2008).
- Forster, S. et al. Regional expansion of hypometabolism in Alzheimer's disease follows amyloid deposition with temporal delay. *Biol. Psychiatry* **71**, 792–797 (2012).
- Hardy, J. & Selkoe, D. J. The amyloid hypothesis of Alzheimer's disease: progress and problems on the road to therapeutics. *Science* **297**, 353–356 (2002).
- Nagasawa, H., Kogure, K., Fujiwara, T., Itoh, M. & Ido, T. Metabolic disturbances in exo-focal brain areas after cortical stroke studied by positron emission tomography. *J. Neurol. Sci.* **123**, 147–153 (1994).
- Akiyama, H., Harrop, R., McGeer, P., Peppard, R. & McGeer, E. Crossed cerebellar and uncrossed basal ganglia and thalamic diaschisis in Alzheimer's disease. *Neurology* **39**, 541–541 (1989).
- Meguro, K. et al. Neocortical and hippocampal glucose hypometabolism following neurotoxic lesions of the entorhinal and perirhinal cortices in the non-human primate as shown by PET. *Brain: a J. Neurol.* **122**, 1519–1531 (1999).
- Buckner, R. L. et al. Molecular, structural, and functional characterization of Alzheimer's disease: evidence for a relationship between default activity, amyloid, and memory. *J. Neurosci.: Off. J. Soc. Neurosci.* **25**, 7709–7717 (2005).
- Mosconi, L. Glucose metabolism in normal aging and Alzheimer's disease: Methodological and physiological considerations for PET studies. *Clin. Transl. Imaging* **1**, 217–233 (2013).
- Landau, S. M. et al. Amyloid deposition, hypometabolism, and longitudinal cognitive decline. *Ann. Neurol.* **72**, 578–586 (2012).
- Sperling, R. A. et al. Amyloid deposition is associated with impaired default network function in older persons without dementia. *Neuron* **63**, 178–188 (2009).
- Jack, C. R. Jr. et al. Amyloid-first and neurodegeneration-first profiles characterize incident amyloid PET positivity. *Neurology* **81**, 1732–1740 (2013).
- Palmqvist, S. et al. Earliest accumulation of beta-amyloid occurs within the default-mode network and concurrently affects brain connectivity. *Nat. Commun.* **8**, 1214 (2017).
- Mormino, E. C. et al. Synergistic effect of beta-amyloid and neurodegeneration on cognitive decline in clinically normal individuals. *JAMA Neurol.* **71**, 1379–1385 (2014).
- Lu, H. et al. Rat brains also have a default mode network. *Proc. Natl. Acad. Sci. USA* **109**, 3979–3984 (2012).
- Do Carmo, S. & Cuello, A. C. Modeling Alzheimer's disease in transgenic rats. *Mol. Neurodegener.* **8**, 37 (2013).
- Seeley, W. W., Crawford, R. K., Zhou, J., Miller, B. L. & Greicius, M. D. Neurodegenerative diseases target large-scale human brain networks. *Neuron* **62**, 42–52 (2009).
- Buckner, R. L., Andrews-Hanna, J. R. & Schacter, D. L. The brain's default network. *Ann. New Y. Acad. Sci.* **1124**, 1–38 (2008).
- Elman, J. A. et al. Neural compensation in older people with brain amyloid- β deposition. *Nat. Neurosci.* **17**, 1316–1318 (2014).
- Passow, S. et al. Default-mode network functional connectivity is closely related to metabolic activity. *Hum. brain Mapp.* **36**, 2027–2038 (2015).
- Riedl, V. et al. Metabolic connectivity mapping reveals effective connectivity in the resting human brain. *Proc. Natl. Acad. Sci. USA* **113**, 428–433 (2016).
- Lee, D. S. et al. Metabolic connectivity by interregional correlation analysis using statistical parametric mapping (SPM) and FDG brain PET; methodological development and patterns of metabolic connectivity in adults. *Eur. J. Nucl. Med. Mol. Imaging* **35**, 1681–1691 (2008).
- Stern, Y. et al. Brain networks associated with cognitive reserve in healthy young and old adults. *Cereb. Cortex* **15**, 394–402 (2005).
- Walsh, D. M. & Selkoe, D. J. A critical appraisal of the pathogenic protein spread hypothesis of neurodegeneration. *Nat. Rev. Neurosci.* **17**, 251–260 (2016).
- Mattson, M. P. & Magnus, T. Ageing and neuronal vulnerability. *Nat. Rev. Neurosci.* **7**, 278–294 (2006).
- Jackson, W. S. Selective vulnerability to neurodegenerative disease: the curious case of Prion Protein. *Dis. Models Mech.* **7**, 21–29 (2014).
- Savas, J. N. et al. The sorting receptor SorCS1 regulates trafficking of neuroligin and AMPA receptors. *Neuron* **87**, 764–780 (2015).
- Lesne, S. E. et al. Brain amyloid- β oligomers in ageing and Alzheimer's disease. *Brain: a J. Neurol.* **136**, 1383–1398 (2013).
- Kreisler, W. C. et al. In vivo radioligand binding to translocator protein correlates with severity of Alzheimer's disease. *Brain: a J. Neurol.* **136**, 2228–2238 (2013).
- Pascoal, T. A., et al. Amyloid- β and hyperphosphorylated tau synergy drives metabolic decline in preclinical Alzheimer's disease. *Mol. Psychiatry* **22**, 306–311 (2016).
- Mesulam, M. M. Neuroplasticity failure in Alzheimer's disease: bridging the gap between plaques and tangles. *Neuron* **24**, 521–529 (1999).
- Ossenkoppele, R. et al. Tau, amyloid, and hypometabolism in a patient with posterior cortical atrophy. *Ann. Neurol.* **77**, 338–342 (2015).
- Jagust, W. J., Landau, S. M., Alzheimer's Disease Neuroimaging, I. & Apolipoprotein, E. not fibrillar beta-amyloid, reduces cerebral glucose metabolism in normal aging. *J. Neurosci.: Off. J. Soc. Neurosci.* **32**, 18227–18233 (2012).
- de Leon, M. J. et al. Positron emission tomography studies of normal aging: a replication of PET III and 18-FDG using PET VI and 11-CDG. *Neurobiol. Aging* **8**, 319–323 (1987).
- Zimmer, E. R., et al. [¹⁸F]FDG PET signal is driven by astroglial glutamate transport. *Nature Neurosci.* **20**, 393–395 (2017).
- Volterra, A. & Meldolesi, J. Astrocytes, from brain glue to communication elements: the revolution continues. *Nat. Rev. Neurosci.* **6**, 626–640 (2005).
- Pascoal, T. A., et al. Synergistic interaction between amyloid and tau predicts the progression to dementia. *Alzheimer's Dement.* **13**, 644–653 (2016).
- Fortea, J. et al. Cerebrospinal fluid beta-amyloid and phospho-tau biomarker interactions affecting brain structure in preclinical Alzheimer disease. *Ann. Neurol.* **76**, 223–230 (2014).
- Swanson, L. Brain maps: structure of the rat brain (2nd edn). *Nature* **363**, 347–350 (1992).
- Ashraf, A., Fan, Z., Brooks, D. J. & Edison, P. Cortical hypermetabolism in MCI subjects: a compensatory mechanism? *Eur. J. Nucl. Med. Mol. Imaging* **42**, 447–458 (2015).
- Jicha, G. A. et al. Neuropathologic outcome of mild cognitive impairment following progression to clinical dementia. *Arch. Neurol.* **63**, 674–681 (2006).
- Leon, W. C. et al. A novel transgenic rat model with a full Alzheimer's-like amyloid pathology displays pre-plaque intracellular amyloid- β -associated cognitive impairment. *J. Alzheimer's Dis.: JAD* **20**, 113–126 (2010).
- Zimmer, E. R., Parent, M. J., Cuello, A. C., Gauthier, S. & Rosa-Neto, P. MicroPET imaging and transgenic models: a blueprint for Alzheimer's disease clinical research. *Trends Neurosci.* **37**, 629–641 (2014).
- McKhann, G. et al. Clinical diagnosis of Alzheimer's disease: report of the NINCDS-ADRDA Work Group under the auspices of Department of Health and Human Services Task Force on Alzheimer's Disease. *Neurology* **34**, 939–944 (1984).
- Mullan, M. et al. A pathogenic mutation for probable Alzheimer's disease in the APP gene at the N-terminus of beta-amyloid. *Nat. Genet.* **1**, 345–347 (1992).
- Murrell, J., Farlow, M., Ghetti, B. & Benson, M. D. A mutation in the amyloid precursor protein associated with hereditary Alzheimer's disease. *Science* **254**, 97–99 (1991).
- Morris, R. Developments of a water-maze procedure for studying spatial learning in the rat. *J. Neurosci. Methods* **11**, 47–60 (1984).
- Zijdenbos, A. P., Forghani, R. & Evans, A. C. Automatic "pipeline" analysis of 3-D MRI data for clinical trials: application to multiple sclerosis. *IEEE Trans. Med. Imaging* **21**, 1280–1291 (2002).
- Thomas, B. A. et al. The importance of appropriate partial volume correction for PET quantification in Alzheimer's disease. *Eur. J. Nucl. Med. Mol. Imaging* **38**, 1104–1119 (2011).
- Pascoal, T. A. et al. Amyloid and tau signatures of brain metabolic decline in preclinical Alzheimer's disease. *Eur. J. Nucl. Med. Mol. Imaging* **45**, 1021–1030 (2018).

55. Oppelt, A. et al. FISP—a new fast MRI sequence. *Electromedica* **54**, 15–18 (1986).
56. Gunn, R. N., Lammertsma, A. A., Hume, S. P. & Cunningham, V. J. Parametric imaging of ligand-receptor binding in PET using a simplified reference region model. *NeuroImage* **6**, 279–287 (1997).
57. Shaw, L. M. et al. Cerebrospinal fluid biomarker signature in Alzheimer's disease neuroimaging initiative subjects. *Ann. Neurol.* **65**, 403–413 (2009).
58. Toledo, J. B., Xie, S. X., Trojanowski, J. Q. & Shaw, L. M. Longitudinal change in CSF Tau and Aβ biomarkers for up to 48 months in ADNI. *Acta Neuropathol.* **126**, 659–670 (2013).
59. Mathotaarachchi, S. et al. VoxelStats: A MATLAB package for multi-modal voxel-wise brain image analysis. *Front Neuroinform* **10**, 20 (2016).
60. Mazziotta, J. et al. A probabilistic atlas and reference system for the human brain: International Consortium for Brain Mapping (ICBM). *Philos Trans. R. Soc. Lond. B Biol. Sci.* **356**, 1293–1322 (2001).
61. Yeo, B. T. et al. The organization of the human cerebral cortex estimated by intrinsic functional connectivity. *J. Neurophysiol.* **106**, 1125–1165 (2011).
62. MacCallum, R. C. & Austin, J. T. Applications of structural equation modeling in psychological research. *Annu Rev. Psychol.* **51**, 201–226 (2000).
63. Schermelleh-Engel, K., Moosbrugger, H. & Müller, H. Evaluating the fit of structural equation models: tests of significance and descriptive goodness-of-fit measures. *Methods of psychological research online* **8**, 23–74 (2003).
64. Kievit, R. A. et al. Distinct aspects of frontal lobe structure mediate age-related differences in fluid intelligence and multitasking. *Nat. Commun.* **5**, 5658 (2014).

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Author contributions

T.A.P., S.G. and P.R.-N. performed the conception of the study and interpreted the data. T.A.P., S.Ma., A.L.B., S.Mo., M.S.K., M.C. and J.T. performed the processing, analysis, and quality control of the image data. M.S.K., M.S. and M.J.P. performed the acquisition of the animal data. A.C.C. developed the transgenic rat model. B.M. assisted in the metabolic network analysis. A.Y.P., J.A.D.A. and H.H. assisted in the statistical analysis. T.A.P., J.P.S., A.C.C., S.G. and P.R.-N. prepared figures, table, and drafted the paper. All authors revised and approved the final paper draft.

Additional information

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