

Immuno-PET of Innate Immune Markers CD11b and IL-1 β Detects Inflammation in Murine Colitis

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Inflammatory bowel disease (IBD) is a chronic relapsing and remitting inflammatory disease of the gastrointestinal tract. The diagnosis and monitoring of IBD are reliant on endoscopy, which is invasive and does not provide information on specific mediators. Symptom flare in IBD is associated with increased activation of innate immune pathways. Immuno-PET approaches have previously demonstrated the ability to detect colitis; however, a direct comparison of antibodies targeted to innate immune mediators and cells has not been done. We aimed to compare immuno-PET of antibodies to IL-1 β and CD11b against standard ¹⁸F-FDG and MRI approaches to detect colonic inflammation. **Methods:** Colonic concentrations of IL-1 β and myeloperoxidase were determined by ELISA, and colonic infiltration by CD11b-positive CD3-negative innate immune cells was determined by flow cytometry and compared between healthy and dextran sodium sulphate-treated colitic mice. PET of ⁸⁹Zr- α -IL-1 β , ⁸⁹Zr- α -CD11b, and ¹⁸F-FDG was compared by volume-of-interest analysis and with MRI by region-of-interest analysis. Imaging results were confirmed by ex vivo biodistribution analysis. **Results:** Colonic inflammation was associated with impaired colonic epithelial barrier permeability, increased colonic IL-1 β and myeloperoxidase concentrations, and increased CD11b-positive CD3-negative innate immune cell infiltration into the colon. ⁸⁹Zr- α -IL-1 β and ⁸⁹Zr- α -CD11b immuno-PET detected colonic inflammation, as did ¹⁸F-FDG, and all PET tracers were more sensitive than MRI. Although ¹⁸F-FDG volumes of interest correlated with colitis severity and a strong trend was observed with ⁸⁹Zr- α -IL-1 β , no correlation was observed for ⁸⁹Zr- α -CD11b or MRI. ⁸⁹Zr- α -IL-1 β was distributed mainly to the gastrointestinal tract, whereas ⁸⁹Zr- α -CD11b was distributed to more tissue types. **Conclusion:** Immuno-PET using antibodies directed to innate immune markers detected colonic inflammation, with ⁸⁹Zr- α -IL-1 β providing a more tissue-specific signal than ⁸⁹Zr- α -CD11b. Development of these technologies for human subjects will potentially provide a less invasive approach than endoscopy for diagnosing and monitoring IBD.

Key Words: immuno-PET; innate immune system; colitis; inflammatory bowel disease

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Inflammatory bowel disease (IBD) is a collection of chronic idiopathic inflammatory diseases of the gastrointestinal tract, including Crohn disease and ulcerative colitis (1). IBD substantially affects quality of life, and although treatable, significant gaps remain because of incomplete efficacy, lack of tolerance, and side effects, leading to variable periods of remission and relapse (2). Patients with IBD require constant surveillance because prognostic indicators of symptom flare remain poor and patients with long-standing disease have an increased risk of developing colon cancer (2,3). The diagnosis and management of IBD are currently heavily reliant on endoscopy, which is generally well tolerated but is invasive, is restricted to imaging of the superficial mucosal surface, cannot easily reach all areas of the small intestine, and does not provide immediate information on specific mediators or mechanisms. Therefore, new technologies are required for imaging IBD that are less invasive than endoscopy and can provide information on specific pathologic processes in real time.

Clinical studies support the use of PET, SPECT, and MRI for detecting inflammation in the gastrointestinal tract, satisfying the criteria for reduced invasiveness and real-time information (4,5). However, current clinical PET, SPECT, and MRI approaches in IBD are restricted to using radiolabeled autologous leukocytes and ¹⁸F-FDG in PET and SPECT and using gadolinium contrast in MRI, none of which provides information on specific mediators. This lack of detail is of increasing importance because of the increase in use of target-specific biologics, particularly antibodies, and the emergence of personalized medicine.

Monoclonal antibodies have exquisite selectivity for their target, and their applicability to immuno-PET has been appreciated for decades, particularly in the cancer field (6–8). However, the use of immuno-PET in IBD is currently limited to preclinical studies, in which T-cell infiltration into the colon of colitic animals has been demonstrated either directly by imaging the T_{HELPER} cell marker CD4 (9) or indirectly by targeting the gut-homing integrin $\alpha_4\beta_7$ (10). In contrast, immuno-PET of immune mediators is yet to be reported; however, direct labeling of the neutrophil-attracting

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chemokine CXCL8 (also known as IL-8) (11,12) and antibody-directed imaging of TNF- α (13) have shown some efficacy for SPECT in both colitic animals and human IBD.

Activation of the innate immune system is intimately linked to inflammation in IBD, most obviously illustrated by the clinical utility of detection of the neutrophil-secreted mediators calprotectin and lactoferrin in stool (3). IL-1 β is an inducible cytokine that has a key role in innate immune responses and is predominantly secreted by neutrophils, monocytes, macrophages, and dendritic cells, whereas CD11b is a pan-myeloid innate immune marker predominantly expressed on these same cell types. Here, we aimed to compare the ability of PET of ^{89}Zr -conjugated antibodies against IL-1 β and CD11b with the ability of standard (^{18}F -FDG) PET and MRI to detect inflammation in colitic mice.

MATERIALS AND METHODS

All experiments were approved by the Animal Ethics Committee of the South Australian Health and Medical Research Institute (SAHMRI) and the University of Adelaide.

Mice

Male C57BL/6jSah mice aged 10–14 wk (20–30 g) were bred and group-housed in a specific pathogen-free environment at SAHMRI. Animals had ad libitum access to food and water. Experiments were conducted with only male mice to eliminate the potential confounding effects of the estrous cycle. Mice were humanely euthanized via CO₂ inhalation and cervical dislocation to remove tissues.

DSS Colitis Model

Colitis was induced by replacing normal drinking water with 2% (w/v) dextran sodium sulphate (DSS) (molecular mass, 40–50 kDa; Alfa Aesar) for 5 d, followed by an additional 3 d of normal drinking water. Mice were assessed daily for signs of acute colitis, including a decrease in body weight and diarrhea. Healthy mice were age- and weight-matched. Colon length was measured on excised colons dissected free from surrounding tissue from the tip of the anus to the distal end of the cecum.

Ussing Chamber Studies

Distal colon segments were mounted into 0.1 cm² aperture sliders bathed in 5-mL baths with oxygenated glucose-fortified Ringers solution for Ussing chamber analysis (Physiologic Instruments) as previously described (14). Briefly, voltage-clamped tissues were equilibrated for 20 min before baseline transepithelial electrical resistance ($\Omega\cdot\text{cm}^2$) and short circuit current ($\mu\text{A}/\text{cm}^2$) were averaged over 10 min.

Myeloperoxidase Activity

Myeloperoxidase activity in the distal colon was determined as previously described (15,16). Briefly, phosphate-buffered saline-washed tissue segments were homogenized in 0.5% hexadecyl-trimethylammonium bromide (Sigma-Aldrich) and reacted with *o*-dianisidine hydrochloride (Sigma-Aldrich). Absorbance at 450 nm was averaged over 5 min at 30-s intervals. Myeloperoxidase activity is expressed as units/mg of tissue, with 1 unit of myeloperoxidase activity defined as the amount of myeloperoxidase required to degrade 1 μmol of peroxide per minute at 25°C.

IL-1 β ELISA

Proteins were extracted from the distal colon as previously described (14,15). Briefly, colon segments were homogenized for 5 min in cell extraction buffer (ThermoFisher Scientific) supplemented with protease inhibitor cocktail (Sigma-Aldrich), 1 mM phenyl-methanesulfonyl fluoride (Sigma-Aldrich), and 50 μM ethylenediaminetetraacetic acid at 1 mL/50 mg of tissue. The lysate was incubated (1 h, 4°C, with rotation), sonicated (2 min), and centrifuged (14,000 rpm, 15 min, 4°C). Supernatant

was collected and stored at -80°C until analysis. IL-1 β concentrations were determined by OptEIA IL-1 β ELISA (BD Biosciences) as previously described (14,15). The limit of sensitivity was less than 4 pg/mL. Concentrations were normalized to total protein concentration as determined by a bicinchoninic acid assay (Abcam) as previously described (15).

Flow Cytometry

Colon lamina propria mononuclear cells (LPMCs) were isolated enzymatically, essentially as previously described (14,15). Briefly, the colon was excised free of fat and blood vessels, flushed with cold phosphate-buffered saline, roughly chopped, and incubated in 4-(2-hydroxyethyl)-1-piperazineethanesulfonic acid buffered Hanks balanced salt solution supplemented with 1 mM ethylenediaminetetraacetic acid and 1 mM dithiothreitol (20 min, 37°C, gentle shaking). Tissue segments were filtered (100 μM), and the remaining tissue was minced and incubated (20 min, 37°C, gentle shaking) in complete RPMI 1640 (Gibco) supplemented with fetal calf serum, GlutaMAX (Life Technologies Corp.), penicillin/streptomycin, collagenase D (1 mg/mL), DNase I (0.5 mg/mL), and dispase (3 mg/mL) (all from Sigma-Aldrich) before being strained (40 μM) and resuspended over a 40/80 Percoll gradient and the interphase LPMC layer collected and pelleted for LPMCs. Viability was determined (trypan blue), and only preparations with at least 80% viability were investigated further. Fc-blocked LPMCs (0.5×10^6) were stained with the antimouse monoclonal antibodies CD45-BV605 (30-F11), CD3-BUV395 (145-2C11), and CD11b-APC-Cy7 (M1/70) (all from BD Biosciences). Per test, 20,000 events were analyzed using a FACS-Fortessa (BD Biosciences), and proportions of live (FVS700; BD Biosciences) singlets were determined using FlowJo (Tree Star), as described previously (14,15).

Antibody–Chelator Conjugation and Radiolabeling

^{89}Zr -oxalate was produced via proton irradiation of ^{89}Y target on a PETtrace 880 cyclotron (GE Healthcare) and purified on Aleco (Comecer) as previously described (17). Monoclonal α -CD11b (M1/70) and α -IL-1 β (B122) (BD Biosciences) were conjugated to ^{89}Zr with NCS-Bz-DFO (Macrocyclics) linkage as previously described (18,19). Competitive blocking assays determined the specificity of ^{89}Zr -conjugated antibodies, whereby 0.5×10^6 healthy mouse splenocytes were incubated with 1.25 μg of ^{89}Zr -labeled α -IL-1 β or α -CD11b for 20 min at 37°C, in the presence or absence of 50 μg of unlabeled α -IL-1 β or α -CD11b added for 20 min beforehand. Cells were pelleted and counted using a Hidex γ -counter for accumulation of ^{89}Zr . All counts were background- and decay-corrected. ^{18}F -FDG (phosphate buffer) was produced by the Molecular Imaging and Therapy Research Unit of SAHMRI on a FASTLab synthesizer (GE Healthcare).

MRI-PET

A 3 to 5 MBq quantity of ^{89}Zr - α -IL-1 β (37.5 μg) and ^{89}Zr - α -CD11b (85 μg) in 100–200 μL of saline was administered intravenously (tail vein) 24 h before imaging, and a 10 to 15 MBq quantity of ^{18}F -FDG in 100–200 μL of saline was administered intravenously 30 min before imaging. Some mice underwent MRI first. The mice were anesthetized with isoflurane (2%), and a T2-weighted rapid-acquisition-with-refocused-echoes (RARE) spin-echo sequence was acquired with a benchtop MRI system (Bruker Icon 1T; Bruker Physik GmbH) (repetition time, 84 ms; echo time, 4,314 ms; number of excitations, 1; RARE factor, 8; field of view, 80 \times 80 mm; slice thickness, 2 mm; scan time, <2 min). ITK snap (www.itksnap.org) was used for consequent segmentation of the scans (20). PET experiments were performed over 15 min using a submillimeter-resolution (0.7 mm) Albira PET-SPECT small-animal scanner (Bruker Biospin GmbH). Manually drawn volumes of interest in the area of interest were applied to analyze average and total radiotracer accumulation using the PMOD imaging suite (PMOD Technologies).

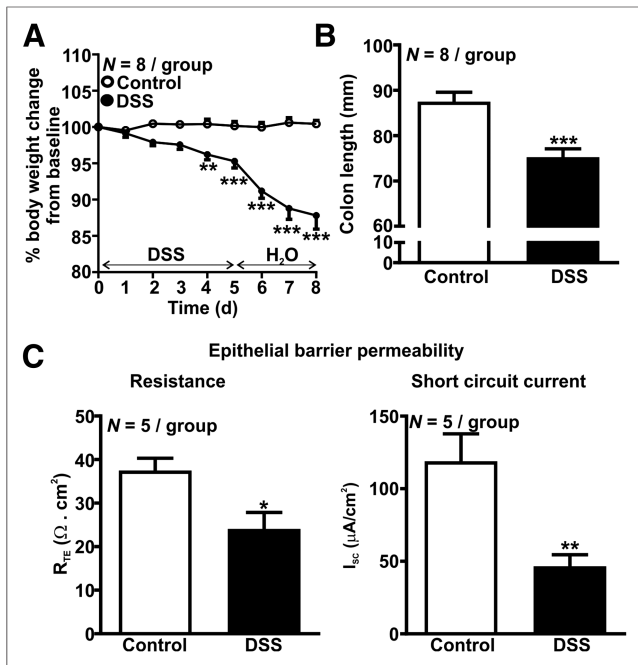


FIGURE 1. Characterization of DSS colitis. (A) Loss of body weight. (B) Shortening of colon length. (C) Impaired epithelial barrier transepithelial electric resistance (left) and short-circuit current (right). * $P < 0.05$. ** $P < 0.01$. *** $P < 0.001$. R_{TE} = transepithelial electrical resistance.

Ex Vivo Biodistribution Studies

Immediately after postimaging culling, organs of interest were dissected, weighed, and counted for ^{89}Zr accumulation as outlined above for blocking experiments.

Statistical Analysis

Data are expressed as mean \pm SEM in all cases. The significance of results was determined by unpaired t testing except for weight loss data, for which a 2-way ANOVA with Bonferroni post hoc testing was used. The strength and significance of correlations were determined by Pearson analysis. Differences with a P value of less than 0.05 were considered statistically significant.

RESULTS

DSS Colitis Association with Body Weight Loss, Colon Shortening, and Impaired Epithelial Permeability

Body weight was reduced in the DSS-treated group 4 d after treatment began ($P < 0.01$, Fig. 1A) and was further reduced by about 10% 8 d after treatment began ($P < 0.001$, Fig. 1A). By day 8, DSS-treated mice also had approximately 15% shorter colons ($P < 0.001$, Fig. 1B), an approximately 35% reduction in epithelial resistance ($P < 0.01$, Fig. 1C), and an approximately 60% reduction in short-circuit current ($P < 0.01$, Fig. 1C), indicative of colonic inflammation and damage to the epithelial barrier.

Increase in Colonic Innate Immune Infiltration in DSS Colitis

DSS-treated mice had an approximately 7.5-fold increase in colonic myeloperoxidase activity ($P < 0.001$, Fig. 2A) and an approximately 2.5-fold increase in colonic IL-1 β concentration ($P < 0.01$, Fig. 2B), indicating that innate immune mediators are increased in colitic mice. The proportion of CD11b colonic LPMCs was increased about 6-fold in DSS-treated mice ($P < 0.001$, Fig. 2C), indicative of an infiltration by innate myeloid cells, including neutrophils, monocytes, macrophages, and dendritic cells.

Immuno-PET Detection of Colonic Innate Immune Activation in Colitis

^{89}Zr was successfully conjugated to $\alpha\text{-IL-1}\beta$ and $\alpha\text{-CD11b}$ as demonstrated by outcompeting binding in the presence of excess unlabeled antibody ($^{89}\text{Zr-}\alpha\text{-IL-1}\beta$: 8,135 \pm 1,510 counts per min [cpm] hot vs. 3,026 \pm 337 cpm cold, $P < 0.05$, $n = 3$; $^{89}\text{Zr-}\alpha\text{-CD11b}$: 61,535 \pm 8,355 cpm hot vs. 34,811 \pm 4,081 cpm cold, $n = 3$, $P < 0.05$). PET imaging revealed that in DSS colitic mice, distal colonic uptake of $^{89}\text{Zr-}\alpha\text{-IL-1}\beta$ was increased about 3-fold ($P < 0.001$, Fig. 3A, Supplemental Videos 1 and 2; supplemental materials are available at <http://jnm.snmjournals.org>), $^{89}\text{Zr-}\alpha\text{-CD11b}$ was increased about 5-fold ($P < 0.05$, Fig. 3B, Supplemental Videos 3 and 4), and $^{18}\text{F-FDG}$ was increased about 3.5-fold ($P < 0.01$, Fig. 3C, Supplemental Videos 5 and 6). A robust positive correlation ($R^2 = 0.70$, $P < 0.05$) was observed between colonic uptake of $^{18}\text{F-FDG}$ and percentage body weight loss (Fig. 3C), with a strong trend toward a similar effect observed for $^{89}\text{Zr-}\alpha\text{-IL-1}\beta$ ($R^2 = 0.54$, $P = 0.09$, Fig. 3A) but not for $^{89}\text{Zr-}\alpha\text{-CD11b}$ (Fig. 3B).

Biodistribution of $^{89}\text{Zr-}\alpha\text{-IL-1}\beta$ and $^{89}\text{Zr-}\alpha\text{-CD11b}$

Ex vivo analysis indicated that uptake of $^{89}\text{Zr-}\alpha\text{-IL-1}\beta$ and $^{89}\text{Zr-}\alpha\text{-CD11b}$ was increased throughout the gastrointestinal tract in DSS-treated mice relative to control mice but also in some extragastrointestinal sites. Specifically, uptake of $^{89}\text{Zr-}\alpha\text{-IL-1}\beta$ was increased about 3-fold in the colon ($P < 0.05$), 5-fold in the cecum ($P < 0.01$), 1.5-fold in the small intestine ($P < 0.05$), and 1.75-fold in the stomach ($P < 0.05$), whereas uptake in the spleen was also increased about 1.75-fold ($P < 0.05$) (Fig. 4A). Uptake was similar between DSS-treated and control mice in all other tissues investigated. Uptake of $^{89}\text{Zr-}\alpha\text{-CD11b}$ was more discrete in the gastrointestinal tract, with increases observed only in the colon (~ 26 -fold, $P < 0.05$) and small intestine (~ 20 -fold,

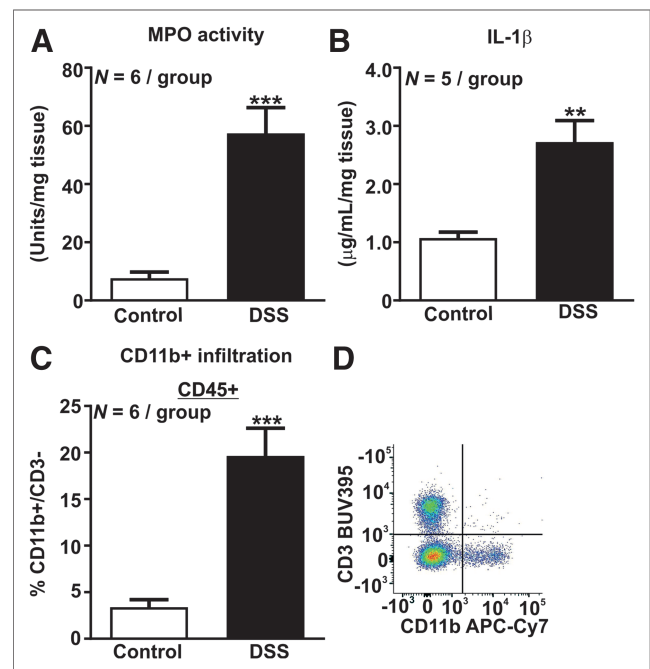


FIGURE 2. Activation of innate immune system by DSS colitis. (A) Increase in colonic myeloperoxidase activity. (B) Increase in IL-1 β concentrations. (C) Increase in CD11b-positive CD3-negative innate immune cell infiltration. (D) Gating strategy. ** $P < 0.01$. *** $P < 0.001$.

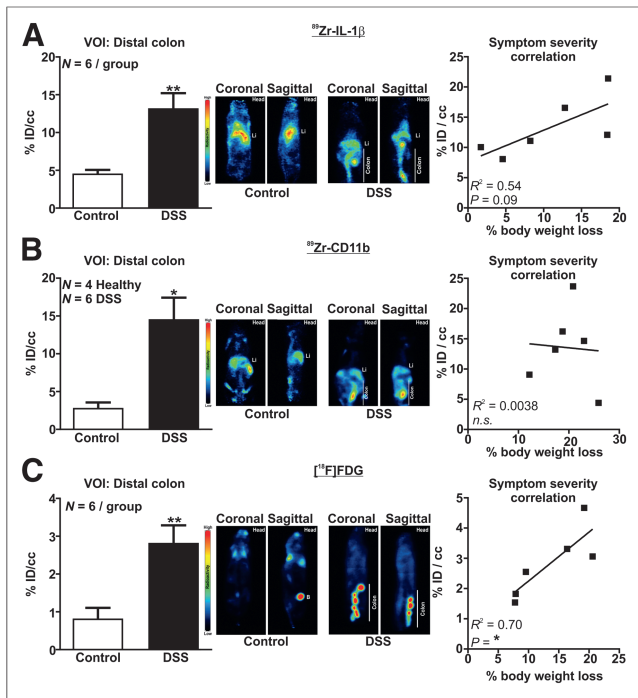


FIGURE 3. α -IL-1 β , α -CD11b, and $^{18}\text{F-FDG}$ PET detection of colonic inflammation. Shown are volume-of-interest analysis with representative PET image (coronal and sagittal) of control and DSS mice (left) and correlation of percentage body weight loss with volume of interest (right) for $^{89}\text{Zr-}\alpha$ -1 L-1 β (A), $^{89}\text{Zr-}\alpha$ -CD11b (B), and $^{18}\text{F-FDG}$ (C). Li = liver; B = bladder; ID = injected dose; n.s. = not statistically significant; VOI = volume of interest. * $P < 0.05$. ** $P < 0.01$.

$P < 0.05$) and a trend toward an increase in the cecum (~21-fold, $P = 0.083$) (Fig. 4B). However, increased uptake of $^{89}\text{Zr-}\alpha$ -CD11b was observed in more sites outside the gastrointestinal tract than $^{89}\text{Zr-}\alpha$ -IL-1 β , including approximately 6-fold in the spleen ($P < 0.05$) but also approximately 7-fold in the liver ($P < 0.05$) and 8-fold in the bone marrow ($P < 0.05$). Notably, trends toward increased uptake of $^{89}\text{Zr-}\alpha$ -CD11b were observed across most other tissues, including the cecum, tail, and stomach; however, uptake was generally more variable for $^{89}\text{Zr-}\alpha$ -CD11b than for $^{89}\text{Zr-}\alpha$ -IL-1 β , limiting the significance of these observations.

MRI Detection of Colonic Inflammation in Colitic Mice

MRI analysis of colonic inflammation revealed an approximately 2-fold increase in the T_2 signal intensity ratio in DSS colitis relative to control ($P < 0.01$, Fig. 5, Supplemental Videos 7 and 8), but this analysis did not correlate with percentage body weight loss (Fig. 5).

DISCUSSION

We demonstrate for the first time, to our knowledge, that immuno-PET directed against innate immune cells and mediators is applicable for detection of colitis. The sensitivity of ^{89}Zr -labeled α -IL-1 β and α -CD11b immuno-PET for detecting colonic inflammation was similar to that of $^{18}\text{F-FDG}$, and all PET approaches were more sensitive than MRI. Furthermore, uptake of $^{89}\text{Zr-}\alpha$ -IL-1 β was restricted to the gastrointestinal tract and spleen, whereas $^{89}\text{Zr-}\alpha$ -CD11b was distributed over a broader range of tissue types. Our comparison demonstrates the strong potential that immuno-PET of innate immune mediators has for diagnosing and monitoring IBD.

Activation of the innate immune system is a hallmark of inflammation in IBD both in humans and in animal models (3,21). DSS is directly toxic to epithelial cells, and we confirm that epithelial damage in DSS colitis is associated with increased colonic infiltration of CD11b-expressing cells and increased colonic concentrations of innate immune cell-secreted IL-1 β (22), both of which we were reliably able to detect by PET of ^{89}Zr -conjugated monoclonal antibodies. Previous immuno-PET studies have identified increased infiltration of T cells in DSS colitis, either by directly labeling of the T_{HELPER} marker CD4 or by labeling of the gut-homing integrin

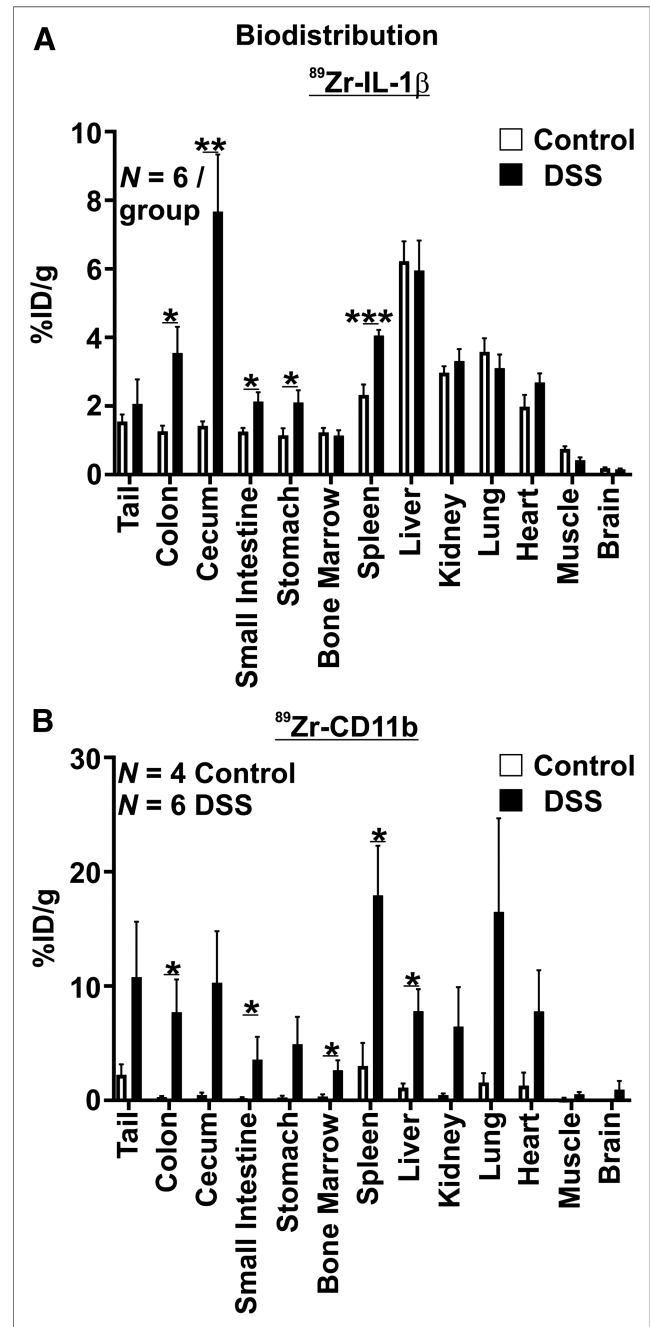


FIGURE 4. Ex vivo biodistribution of $^{89}\text{Zr-}\alpha$ -1 L-1 β (A) and $^{89}\text{Zr-}\alpha$ -CD11b (B). Decay-corrected values for uptake are displayed. * $P < 0.05$. ** $P < 0.01$. *** $P < 0.001$. ID = injected dose.

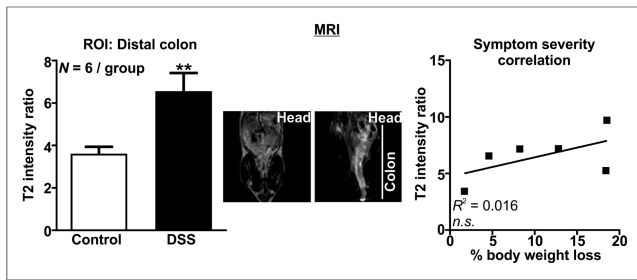


FIGURE 5. MRI detection of colonic inflammation. Region-of-interest analysis with representative MR image (coronal) of control and DSS mice (left) and correlation of percentage body weight loss with region-of-interest MRI analysis (right). ** $P < 0.01$. n.s. = not statistically significant; ROI = region of interest.

complex $\alpha_4\beta_7$, which is upregulated on T cells in IBD (9,10,23). However, we believe our study to be the first to describe the potential that radiolabeled antibodies against innate immune markers have for PET in IBD diagnosis and monitoring.

We observed a striking difference in the biodistribution of ^{89}Zr - α -IL-1 β and ^{89}Zr - α -CD11b, with ^{89}Zr - α -IL-1 β being restricted to the gastrointestinal tract and spleen whereas ^{89}Zr - α -CD11b was observed in a broad range of tissues. Furthermore, ^{89}Zr - α -IL-1 β also correlated with colitis severity whereas ^{89}Zr - α -CD11b did not. These findings are likely to relate to immunologic processes underlying innate immune activation in colitis. Innate immune cells migrate from induction sites in lymphatic tissue through the bloodstream into sites of inflammation, where they mature and secrete cytokines, including IL-1 β , before clearing from tissue by the lymphatics or dying (24). CD11b is expressed on innate cell subsets that promote inflammation, such as M1 macrophages and most neutrophil subsets, but also on innate immune cells that promote tolerance, wound healing, and immune suppression, including M2 macrophages, dendritic cells, and CXCL4-expressing neutrophil subsets (25,26). These cells express CD11b at all stages of maturity, and imaging CD11b is therefore likely to detect sites of inflammation but also migration between tissues and lymph nodes, including the bone marrow and, particularly in mice, the spleen. Furthermore, whereas CD11b expression is high on myeloid innate immune cells, it is also expressed on other immune cells, including T- and B-cell subsets, which may contribute toward the signal we observed in our imaging (27). The expression of individual markers on multiple cell types is common; for example, CD4 is expressed on macrophages in addition to T_{HELPER} cells, and complex flow cytometry using multiple markers is typically required to conclusively characterize individual immune cell subsets. For IBD, this is particularly relevant to the ever-expanding T_{HELPER} cell subsets and innate lymphoid cells, which rely on staining of cytoplasmic cytokines or nuclear transcription factors for their characterization (28). Definitively identifying these subsets for in vivo imaging is difficult in live cells because antibodies are typically too large to passively enter cells.

In contrast, IL-1 β has 2 favorable characteristics for immuno-PET. First, it is inducible rather than constitutive and therefore is secreted only by activated cells, which, in colitis, are predominantly located at sites of inflammation. Second, proteolytic processing of IL-1 β into its mature form typically occurs within the cell, and it is secreted as a mature functional protein (29). This is somewhat an anomaly for cytokines but is beneficial for immuno-PET because only mature IL-1 β is imaged. Our results support

further investigation into the use of imaging inducible and intracellularly processed immune mediators for detecting inflammation in IBD. Furthermore, immuno-PET using radiolabels with long half-lives, such as ^{89}Zr , enables longitudinal imaging, which would provide valuable information on the temporal nature of immune responses in IBD.

SPECT is a cost-effective technique for nuclear imaging but generally has reduced resolution relative to PET. Nonetheless, SPECT imaging of the neutrophil-attracting chemokine CXCL8, and CD4, has also shown potential in preclinical and human studies of IBD (11,12,30). Furthermore, whereas SPECT imaging of the TNF- α -neutralizing antibody infliximab also demonstrated some efficacy in preclinical colitis, it was hindered by high background, the cause of which was likely its chimeric mouse-human properties (13). The most readily available alternative markers for immuno-PET imaging of IBD include antibodies that are currently used for treatment, including variations targeting TNF- α , $\alpha_4\beta_7$ (vedolizumab), $\alpha_4\beta_1$ (natalizumab), and IL-12/23 (ustekinumab) (31). However, markers do not have to be limited to the immune system. Epithelial damage and increased epithelial barrier permeability are hallmarks of IBD and colitis, as we demonstrate in our model (32,33). The permeability of the epithelial monolayer to luminal contents is regulated by a large family of tight-junction proteins, many of which are reduced in degraded tissue in the inflamed intestine, impeding their use as markers. Conversely, expression of some of these proteins promotes increased permeability and is increased during IBD, such as the pore-forming claudin-2 (34,35). Other potential markers include those associated with tissue remodeling associated with the resolution of inflammation (36). Matrix metalloproteases are involved in tissue remodeling and, interestingly, are thought to play a key role in promoting fibrosis. Although an antibody against matrix metalloprotease 9 was ultimately withdrawn from clinical trials on IBD, interest in this target remains and it may have more promise as a marker of fibrosis (37).

The clinical utility of immuno-PET for IBD is currently limited by several issues. Primarily, antibodies are large molecules with molecular weights of about 150 kDa. This large size prolongs their half-life and reduces excretion, which is beneficial when used as treatments but is challenging for imaging because tissue penetration is reduced and excretion prolonged. Issues related to tissue penetration may be somewhat diminished in IBD because vascular permeability is increased in inflammation, aiding immune cell migration into inflammatory sites (38). However, increased leukocyte extravasation is unlikely to drastically reduce the time taken for systemically administered antibodies to reach inflammatory sites in IBD, and the current clinical paradigm would require dosing and imaging to occur at separate visits over several days. This requirement results in increased exposure to radiolabels, potentially increasing the risk of side effects. Promising alternatives to intact antibodies that potentially limit these concerns are in development (39). Notably, engineered small antibody fragments against anti-CD4 and β_7 have already shown promise in preclinical colitis (9,10). A different strategy uses a 2-step process for pretargeting. The initial step comprises administration of an antibody modified to incorporate a radiolabel capture site, which is allowed enough time to localize to its target. A few days later, the radiolabel is injected and binds to the antibody. This strategy has shown promise in cancer (40) but has yet to be applied to IBD and may prove difficult because the harsh protease-rich environment in inflammation may rapidly degrade targets.

CONCLUSION

We have demonstrated that radiolabeled antibodies against innate immune cells and mediators are suitable for immuno-PET of colitis. Our results provide further evidence of the clinical utility of immuno-PET for IBD diagnosis and monitoring. Development of these techniques would be of particular benefit to patients who are difficult to scope, including the pediatric population and those that have inflamed or fibrotic regions of the small intestine.

DISCLOSURE

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