

Abnormal Low-Frequency Oscillations Reflect Trait-Like Pain Ratings in Chronic Pain Patients Revealed through a Machine Learning Approach

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Measures of moment-to-moment fluctuations in brain activity of an individual at rest have been shown to be a sensitive and reliable metric for studying pathological brain mechanisms across various chronic pain patient populations. However, the relationship between pathological brain activity and clinical symptoms are not well defined. Therefore, we used regional BOLD signal variability/amplitude of low-frequency oscillations (LFOs) to identify functional brain abnormalities in the dynamic pain connectome in chronic pain patients that are related to chronic pain characteristics (i.e., pain intensity). Moreover, we examined whether there were sex-specific attributes of these functional brain abnormalities and whether functional brain abnormalities in patients is related to pain intensity characteristics on different time scales. We acquired resting-state functional MRI and quantified frequency-specific regional LFOs in chronic pain patients with ankylosing spondylitis. We found that patients exhibit frequency-specific aberrations in LFOs. Specifically, lower-frequency (slow-5) abnormalities were restricted to the ascending pain pathway (thalamus and S1), whereas higher-frequency abnormalities also included the default mode (i.e., posterior cingulate cortex; slow-3, slow-4) and salience (i.e., mid-cingulate cortex) networks (slow-4). Using a machine learning approach, we found that these abnormalities, in particular within higher frequencies (slow-3), can be used to make generalizable inferences about patients' average pain ratings (trait-like pain) but not current (i.e., state-like) pain levels. Furthermore, we identified sex differences in LFOs in patients that were not present in healthy controls. These novel findings reveal mechanistic brain abnormalities underlying the longer-lasting symptoms (trait pain intensity) in chronic pain.

Key words: bold variability; chronic pain; fMRI; low-frequency oscillations

Significance Statement

Measures of moment-to-moment fluctuations in brain activity of an individual at rest have been shown to be a reliable metric for studying functional brain associated with chronic pain. The current results demonstrate that dysfunction in these intrinsic fluctuations/oscillations in the ascending pain pathway, default mode network, and salience network during resting state display sex differences and can be used to make inferences about trait-like pain intensity ratings in chronic pain patients. These results provide robust and generalizable implications for investigating brain mechanisms associated with longer-lasting/trait-like chronic pain symptoms.

Introduction

The temporal dimension of chronic pain is often overlooked, yet patients commonly report that their symptoms can fluctuate

from moment to moment, and even on the order of hours and days. The mechanisms that contribute to chronic, fluctuating levels of pain and how they differ across individuals provide a

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window into underlying etiologies and potential treatment approaches. However, most brain imaging studies of chronic pain do not distinguish pain at the time of the study (state pain) from average pain experienced over time (trait pain). State and trait pain can reflect different aspects of chronic pain conditions.

One chronic pain condition that affects primarily younger adults devoid of comorbidities commonly seen in other chronic pain disorders is ankylosing spondylitis (AS). AS is a form of arthritis resulting from inflammation of the sacroiliac joint, resulting in debilitating lower back pain (Bidad et al., 2017). These patients have aching, tender and sore pain that can be shooting or stabbing (Wu et al., 2013), of intensity ebbs and flows throughout the day (Sieper et al., 2002).

One approach to investigate temporal mechanisms underlying chronic pain is to quantify low-frequency oscillations (LFOs) of brain activity during resting-state functional MRI (fMRI). This can be measured by BOLD signal variability, the SD of the BOLD signal time course (Garrett et al., 2010; Rogachov et al., 2016). We recently demonstrated that regional BOLD signal variability is a sensitive indicator of individual differences of pain sensitivity and coping in healthy individuals (Rogachov et al., 2016). Moreover, others have reported abnormalities in LFOs in chronic pain patients with back pain (Baliki et al., 2011), osteoarthritis (Baliki et al., 2014), migraine (Hodkinson et al., 2016), and neuropathic pain (Alshelhi et al., 2016), but they reported conflicting findings. Baliki et al. (2011) reported that LFO abnormalities dynamically track fluctuations in patients' ongoing (state-like) pain during fMRI in low back pain patients; however, later work has also shown LFO abnormalities in low back pain and osteoarthritis to be related to more longer-lasting/trait-like pain characteristics (i.e., disease duration; Baliki et al., 2014). Likewise, recent work from our group has shown unique brain connectivity patterns associated with chronic pain characteristics of different time scales that represent trait-like and state-like pains (Cheng et al., 2018). In addition, an important consideration to LFO studies is frequency-specific and sex-related effects. Chronic pain-related disruption on LFOs and subsequent correlations to ongoing levels of pain (pain state; Baliki et al., 2011) and longer-lasting features (disease duration; Baliki et al., 2014) were found exclusively within higher frequencies (0.12–0.20 Hz; slow-3). Similarly, Hong et al. (2013) reported differences in frequency-specific alterations in resting-state brain oscillations between men and women patients with chronic visceral pain.

Therefore, the primary aims of this study were to (1) identify abnormalities in slow-3, -4, and -5 BOLD signal variability/LFOs associated with chronic pain in patients with AS and (2) determine whether frequency-specific abnormalities are related to pain intensity ratings. We also considered whether these abnormalities related to patients' pain intensity levels on different time scales [current pain (state-like characteristic) vs average pain intensity over 7 d (trait-like characteristics)] and whether these abnormalities are impacted by sex. Toward these goals, we collected resting-state fMRI from chronic pain patients with AS ($n = 71$) and from 62 age- and sex-matched healthy controls. We also asked patients to rate their average pain over the previous week (trait-like pain) as well as the intensity of their pain immediately before the scan (current pain levels that reflects state-like pain). Importantly, we used a machine learning algorithm to determine whether functional brain differences between patients and controls can be used to make generalizable inferences related to patients' pain intensity ratings. We hypothesized that AS patients would show increased LFOs compared with healthy controls (HCs) and that higher-frequency (slow-3) LFOs would be related

to their trait-like pain represented by average pain intensity over the previous week.

Materials and Methods

Subjects. The study consisted of 71 right-handed chronic pain patients diagnosed with AS (51 men, 20 women; average age \pm SD, 34.9 ± 11.1 ; 18–61 years old) and 62 right-handed HCs (43 men, 19 women; average age \pm SD, 34.0 ± 11 ; 18–55 years old) who underwent a neuroimaging session and psychophysical testing. The AS cohort reported an average (\pm SD) years living with pain of 15.5 (9.8), which ranged from 2 to 38 years. Although AS pain is classically associated with pathology localized to the sacroiliac joint (lower back), many patients reported bilateral pain radiating into their lower extremities, as well as other joints (e.g., knees and wrists). Forty-two of the patients were being treated with anti-TNF- α (biologics) medication (i.e., Embrel, Humira, Remicade, and Simponi), and 27 were treated with nonsteroidal anti-inflammatory drugs (i.e., Voltaren, Naprosyn, and Celebrex). All participants provided informed written consent to procedures approved by the University Health Network research ethics board. Patients with chronic pain were recruited from the Spondylitis clinic at Toronto Western Hospital. The inclusion criteria for the chronic pain patients was a diagnosis of AS according to the modified New York criteria (van der Linden et al., 1984). Exclusion criteria for patients and HC participants were as follows: (1) a previous diagnosis of a psychiatric, neurological, or metabolic disorder; (2) major surgery in the past 2 years; (3) serious infection (associated with hospitalization or intravenous antibiotics) within 4 weeks of testing; and (4) any standard contraindications to MRI scanning (i.e., pregnancy, metal in the body, claustrophobia).

Neuroimaging acquisition. Brain imaging data were acquired with a 3T MRI scanner fitted with an eight-channel phase-array head coil (GE Medical Systems). For each study participant, we collected a high-resolution T1-weighted anatomical scan (3D IR-FSPGR sequence; 180 axial slices; TR, 7.8 ms; TE, 3 ms; flip angle, 15°; 256×256 matrix; $1 \times 1 \times 1$ mm voxels) and a 9 min, 14 s T2*-weighted resting-state fMRI scan (echo-planar imaging sequence; 36 slices; TR, 2000 ms; TE, 30 ms; 64×64 matrix; $3.125 \times 3.125 \times 4$ mm voxels). During the resting-state fMRI scan, the subjects were instructed to “close your eyes, do not try to think about anything in particular; do not fall asleep.” Two subjects (both AS patients) were excluded from further analyses because of signal dropout within the orbitofrontal cortex, leaving a total of 69 subjects.

Questionnaires and pain ratings. All study subjects completed psychological/personality questionnaires, including the Beck Depression Inventory (BDI; Beck et al., 1961) and the State/Trait Anxiety Inventory (Spielberger et al., 1983), and patients filled out additional pain-specific assessments such as their average pain intensity over the past week and their current level of pain before imaging (0, no pain; 10, worse pain imaginable). Average pain intensity ratings were collected from 65 of 69 AS patients included in the study. Nine patients [all of whom were treated with anti-TNF- α (biologics) medication] reported an average weekly pain of 0 of 10. As the goal of this study was to investigate the relationship between LFOs and pain intensity, these nine patients were removed, leaving a total of 56 AS patients in the main analysis. All 56 patients provided ratings of average pain; however, only 50 of 56 patients also provided a current pain intensity rating.

Preprocessing of fMRI data. Data were preprocessed using the fMRI Expert Analysis Tool (FEAT) in FSL version 5.0 (Jenkinson et al., 2012). First, we deleted the first four volumes of the resting-state scan, and then we removed nonbrain voxels using the Brain Extraction Tool (BET) within FEAT and performed motion correction (MCFLIRT). T1-weighted anatomical images were skull stripped using optiBET (Lutkenhoff et al., 2014). The functional images were registered to the skull-stripped, T1-weighted anatomical images using FLIRT [rigid-body transformation with 6 df], which was followed by a nonlinear registration to MNI152-2 mm space using FNIRT. Next, aCompCor (Napadow et al., 2010; Chai et al., 2012) was used to remove scanner-related and physiological noise from the fMRI using FSL, Matlab (MathWorks), and fMRISTAT (Worsley et al., 2002). Using FSL's FAST, we first segmented the T1-weighted anatomical images into partial volume gray matter (GM), white matter (WM), and CSF maps. The WM and CSF partial volume maps, which were derived

from the subject's anatomical space, were linearly registered to their fMRI space. To prevent the possibility of removing any GM signal, the WM and CSF maps were thresholded to the top 198 and 20 cm³ probability of WM and CSF voxels, respectively, leaving the voxels with the highest probability of correctly being mapped as WM and CSF. This approach allowed us to exclude voxels that may have contained more than one tissue type (Chai et al., 2012). These thresholded maps were then multiplied by the resting-state fMRI data, and the top five WM and CSF components derived from a whole-brain principal component analysis were regressed out. The six motion parameters derived from MCFLIRT were also regressed out of the data, which was followed by spatial smoothing (6 mm full-width at half-maximum kernel). AFNI's 3dBandpass function was used to temporally filter the fMRI data into respective slow-wave frequency bands (slow-5, 0.01–0.027 Hz; slow-4, 0.027–0.073 Hz; slow-3, 0.073–0.198 Hz; Buzsaki and Draguhn, 2004; Di Martino et al., 2008; Zuo et al., 2010).

Definition of resting-state network/pathways of interest. Using the Harvard Oxford Cortical and Subcortical Atlases (Frazier et al., 2005; Desikan et al., 2006; Makris et al., 2006; Goldstein et al., 2007) and as per described previously (Rogachov et al., 2016), a mask of core regions of the ascending nociceptive system was created in the standard MNI152-2 mm space. This mask included the bilateral thalamus, bilateral primary and secondary somatosensory cortices (S1, S2), bilateral insula, and anterior and mid-cingulate cortices. We also included masks of the default mode network [DMN; medial prefrontal cortex, posterior cingulate/precuneus (PCC/PCu), lateral temporal cortex, and lateral parietal cortex] and the salience network [SN; mid-cingulate cortex (MCC), dorsolateral prefrontal cortex (dlPFC), and temporoparietal junction; Hemington et al., 2016] because they are important in shaping an individual's pain experience and are key networks of the dynamic pain connectome (Kucyi and Davis, 2015).

Calculation of regional BOLD signal variability. BOLD signal variability/LFOs was calculated on a voxel-wise basis using tools from FSL (Jenkinson et al., 2012). Specifically, using *fslmaths*, the SD of each voxel's time course was calculated for each subject. Next, since the global mean BOLD signal variability did not reveal significant group differences between AS patients and HCs ($p = 0.34$), each subject's BOLD signal variability map was standardized (z -scored) on an individual basis (Martino et al., 2016). This was done to mitigate potential extraneous sources of variance in the BOLD signal between subjects (i.e., differences in magnetic gain between scans). The standardization process involved subtracting from each voxel the subject's mean BOLD signal variability across their gray matter and dividing this by the SD of the BOLD signal variability across the gray matter. Thus, a BOLD signal variability z -score value of 0 represents oscillations that are equal to the individual's average across the entire whole brain (gray matter). Positive values represent BOLD signal variability that is greater than the whole-brain (gray matter) average, and negative values represent those that are lower than the whole-brain (gray matter) average. The computed SD is related to the amplitude of the resting-state fluctuations in the time domain and reflects the strength or intensity of the low-frequency fluctuation (Zuo et al., 2010).

Group voxel-wise analysis. For each frequency band of interest, comparisons between the HC and AS groups' subject-level amplitude maps were performed using a two-sample unpaired t test using *Randomise*, FSL's tool for nonparametric permutation inferencing (Winkler et al., 2014). We combined our masks/networks of interest (ascending nociceptive system, DMN, and SN) and ran voxel-wise permutation tests (positive and negative contrasts with 5000 permutations) with threshold-free cluster enhancement (TFCE). The presented group-level results are thresholded at $p < 0.05$ [family-wise error (FWE) corrected for multiple comparisons]. Although there were no group differences in age ($p = 0.194$) and residual head motion ($p = 0.533$), previous studies have demonstrated that both factors can impact amplitude recordings (Garrett et al., 2010). Thus, to limit any possible confounding effects of age or head motion, both age and mean relative head displacement for each subject were included as variables of no interest in the design matrix.

Cross-validation regression: BOLD signal variability/LFOs and pain ratings. Using PRoNTo (Pattern Recognition for Neuroimaging Toolbox; Schrouff et al., 2013), we applied a machine learning approach to

examine multivariate brain patterns that are related to patients' pain (Rogachov et al., 2015). To do this, voxel-wise BOLD signal variability was regressed against patients' pain ratings using cross-validation (10-fold) kernel ridge regression. Of note, only the voxels that were statistically significant from the group-level BOLD signal variability analysis, between AS patients and HCs, were included in this analysis. Two separate models were created: one for patients' state pain intensity (current pain collected right before the MRI scan; $n = 50$) and one for their trait-like pain intensity (average pain over the week; $n = 56$). Follow-up permutation testing (5000 iterations) was conducted to determine the statistical significance of the correlation between actual and model-estimated pain ratings, as well as the mean squared error (MSE), the magnitude of error in the model.

Sex-related analyses. To examine whether the spatial distribution of the frequency-specific abnormalities we found in the main analysis were driven/explained by sex, we performed, within each frequency band of interest, a two-sample unpaired t test on the subject-level amplitude maps for men [AS men ($n = 19$) vs HC men ($n = 19$)] and women [AS women ($n = 19$) vs HC women ($n = 19$)] separately. The frequency-specific group contrasts were masked and run through a voxel-wise permutation test (positive and negative contrasts with 5000 permutations) using TFCE. All reported results are thresholded at $p < 0.05$ (FWE corrected).

Moreover, we examined sex differences within each condition (AS men vs AS women; HC men vs HC women) separately. The same networks (ascending nociceptive system, DMN, and SN) were amalgamated, masked, and run through a voxel-wise permutation test (positive and negative contrast with 5000 permutations) using TFCE. All reported results are thresholded at $p < 0.05$ (FWE corrected).

Results

BOLD signal variability is increased in AS chronic pain patients

We found that compared with the HC group, AS patients had abnormally greater LFOs within regions of the dynamic pain connectome. Specifically, AS patients had increased LFOs within left ventrolateral thalamus and S1 of the ascending pain pathway in the slow-5 frequency band (Fig. 1). Within the slow-4 frequency band, AS patients exhibited increased LFOs in S1 of the ascending pain pathway and in the PCC and MCC of the DMN and SN, respectively (Fig. 1). Finally, patients had increased LFOs in S1 and PCC/PCu compared with HCs in the slow-4 frequency band (Fig. 1). Within brain regions that showed statistically significant group differences, HCs had negative z -score values in slow-5 and positive z -score values in slow-3 and slow-4. On the other hand, AS patients had positive z -score values in all frequency bands examined (Fig. 1, Table 1).

BOLD signal variability impairments reflect trait-like pain ratings

Of the 65 AS patients who provided an average pain intensity rating, 56 reported experiencing some pain in the week before testing (average week pain, 1–10 of 10), while 9 of the patients (all of whom were undergoing treatment with biologic agents) reported being completely pain free. Only patients with pain were included in our analysis. The mean (\pm SD) trait pain intensity rating over the last week of the AS patients was 4.03 ± 2.18 . Using cross-validated multivariate regression, we found that a model based on LFOs could generalize to make inferences about unseen patients' average pain intensity ratings [trait pain; $n = 56$; $r = 0.43$, $p = 0.005$; MSE, 4.94 ($p = 0.0088$); Fig. 2]. The brain regions with the greatest predictive weights/magnitude to make inferences on unseen patients' for average pain ratings were the PCC/PCu and right S1 (Fig. 2C).

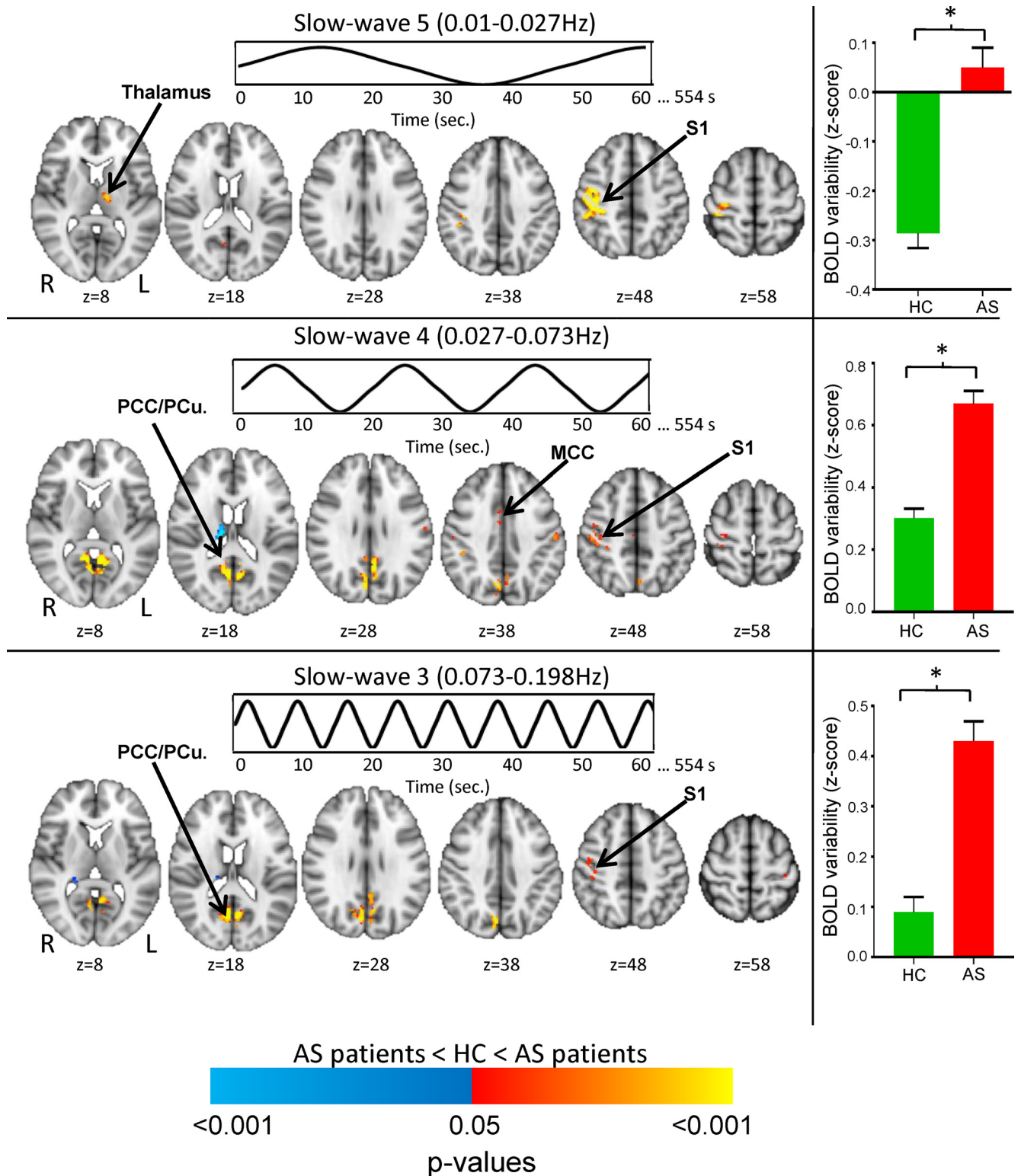


Figure 1. Frequency-specific changes in BOLD signal variability/LFOs. The contrast maps represent the differences in BOLD signal variability/LFOs between AS patients ($n = 56$) and HCs ($n = 62$) within three frequency bands: slow-5 (0.01–0.027 Hz), slow-4 (0.027–0.073 Hz), and slow-3 (0.073–0.198 Hz). Since there was no significant group differences in global BOLD variability ($p = 0.34$), subject-level standardization (z-scored) was performed. The corresponding raw z-scored BOLD signal variability values averaged across the whole significant cluster are represented in the bar graphs. All statistical images display significant clusters ($p < 0.05$, FWE corrected). Warm colors represent brain areas in which AS patients had greater BOLD signal variability/LFOs than HCs, and cool colors represent brain areas in which AS patients had lower BOLD signal variability/LFOs than HCs. All axial slices are represented in radiological orientation. S1, Primary somatosensory cortex, MCC, Mid-cingulate cortex, and PCC/PCu - Posterior cingulate cortex/precuneus; L, left; R, right. * $p < 0.05$, FWE-corrected.

Sex-related differences in BOLD signal variability

To investigate whether the abnormalities reported in our main result were driven by sex, a follow-up analysis was performed in men [AS ($n = 19$) vs HC ($n = 19$)] and in women [AS ($n = 19$) vs

HC ($n = 19$)], separately. Within the slowest frequency band (slow-5), the majority of the results (e.g., thalamus and right S1) are driven by women. Likewise, our main findings in slow-3 with the PCC/PCu are also primarily explained by women. On the

Table 1. Peak MNI coordinates from brain regions that had significantly increased and decreased BOLD signal variability in AS patients ($n = 56$) compared with HCs ($n = 62$)

Frequency band	Contrast	Number of voxels	MNI coordinates (mm)			Brain region	
			x	y	z		
Slow-5 (0.01–0.027 Hz)	AS > HC	441	42	–28	42	Right primary somatosensory cortex	
		67	–10	–14	8	Left thalamus	
		4	6	–60	16	Posterior cingulate cortex	
Slow-4 (0.027–0.073 Hz)	AS > HC	1056	8	–52	10	Precuneus	
		291	46	–36	42	Right supramarginal gyrus	
		57	–56	–16	36	Left primary somatosensory cortex	
		31	6	–2	40	Mid-cingulate cortex	
		10	62	–6	24	Right primary somatosensory cortex	
		AS < HC	99	16	–26	16	Right thalamus
			13	–14	–28	16	Left thalamus
Slow-3 (0.073–0.198 Hz)	AS > HC	598	6	–70	34	Precuneus	
		81	40	–22	50	Right primary somatosensory cortex	
		19	42	–28	46	Right primary somatosensory cortex	
		23	18	–24	14	Right thalamus	

All statistical images were thresholded at $p < 0.05$ (FWE corrected for multiple comparison) using TFCE.

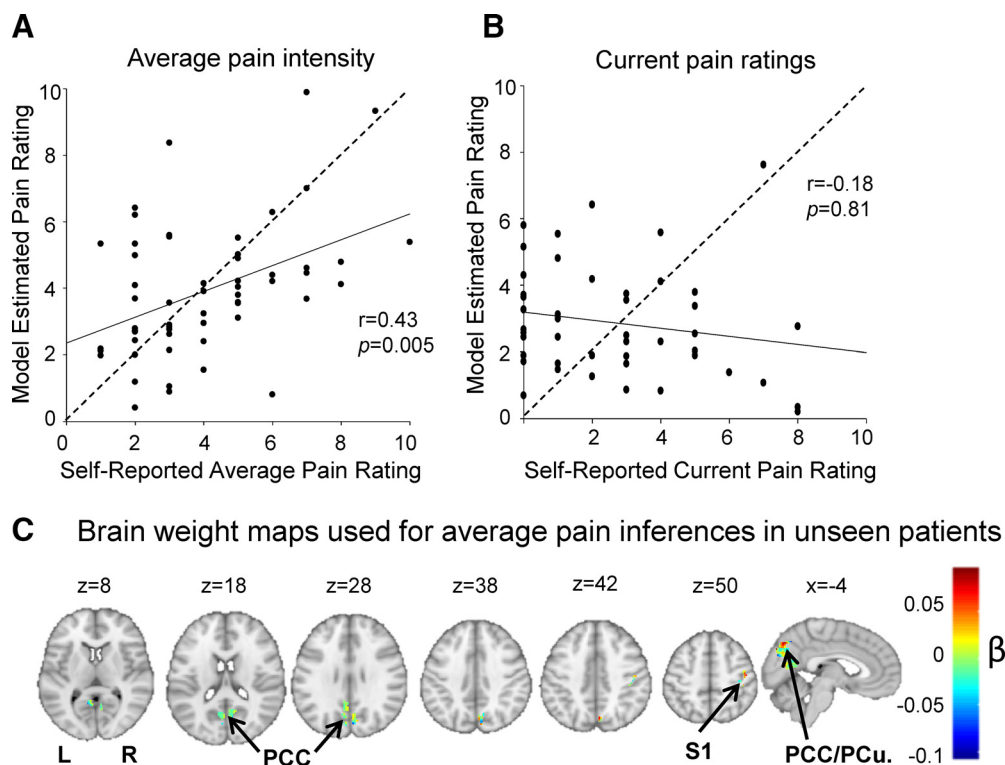


Figure 2. Group differences in BOLD signal variability/LFOs within slow-3 are generalizable for average pain intensity ratings. **A**, Positive, significant correlation between self-reported average pain intensity ratings and model-estimated average pain intensity ratings using BOLD signal variability/LFOs in areas (i.e., PCC and S1) that showed group differences in slow-3 between AS patients and HCs ($r = 0.43, p = 0.005, n = 56$). **B**, No relationship between self-reported state pain ratings and model-estimated state pain ratings in areas that had group differences in slow-3 between AS patients and HCs ($r = -0.18, p = 0.81, n = 50$). **C**, The distribution of brain regions and their associated weights that were used in the machine learning model to make inferences about average pain intensity ratings. PCC, Posterior cingulate cortex; S1, Primary somatosensory cortex; L, Left; R, right.

other hand, slow-4 results show to have been driven by both sexes fairly equally, with men accounting for a marginally larger proportion in the PCC/PCu. This suggests that the majority of our findings with our main analysis, particularly with slow-3 and slow-5, are explained by women subjects (Table 2, Fig. 3).

Furthermore, we explored sex differences within the subjects used in this study. Among the AS patients (19 men, 19 women), although both positive, men exhibited lower slow-5 BOLD signal variability/LFOs in the PCC compared with women (average \pm SEM: men, 0.35 ± 0.08 ; women, 0.90 ± 0.07 ; $p < 0.05$). However, in the higher-frequency bands, men had higher, positive BOLD signal variability/LFOs than the women, who had negative BOLD

signal variability/LFOs in dlPFC (slow-4; men, 0.42 ± 0.19 ; women, -0.67 ± 0.11) and right primary S1 (slow-3; men, 0.09 ± 0.11 ; women, -0.71 ± 0.07 ; $p < 0.05$; Fig. 4, Table 3). None of these effects were seen in HCs. Finally, there were no sex differences in trait pain ($z = -0.157, p = 0.8858$).

State versus trait pain characteristics

The temporal dimension of chronic pain is often overlooked, yet patients commonly report that their symptoms can fluctuate from moment to moment and even on the order of hours and days. Brain imaging studies of chronic pain typically examine brain function related to the amount of pain that a patient re-

Table 2. Peak MNI coordinates from brain regions that show sex-related effects from the main analysis

Frequency band	Contrast	Number of voxels	MNI coordinates (mm)			Brain region
			x	y	z	
Slow-5 (0.01–0.027 Hz)	Men < women (AS patients)	36	–2	–44	26	Posterior cingulate cortex
Slow-4 (0.027–0.073 Hz)	Men > women (AS patients)	8	–32	50	28	Left dorsolateral prefrontal cortex
Slow-3 (0.073–0.198 Hz)	Men > women (AS patients)	9	48	–28	62	Right primary somatosensory cortex

The AS patients and HCs both consisted of 19 men and 19 women. All statistical images were thresholded at $p < 0.05$ (FWE corrected for multiple comparison) using cluster-free threshold enhancement.

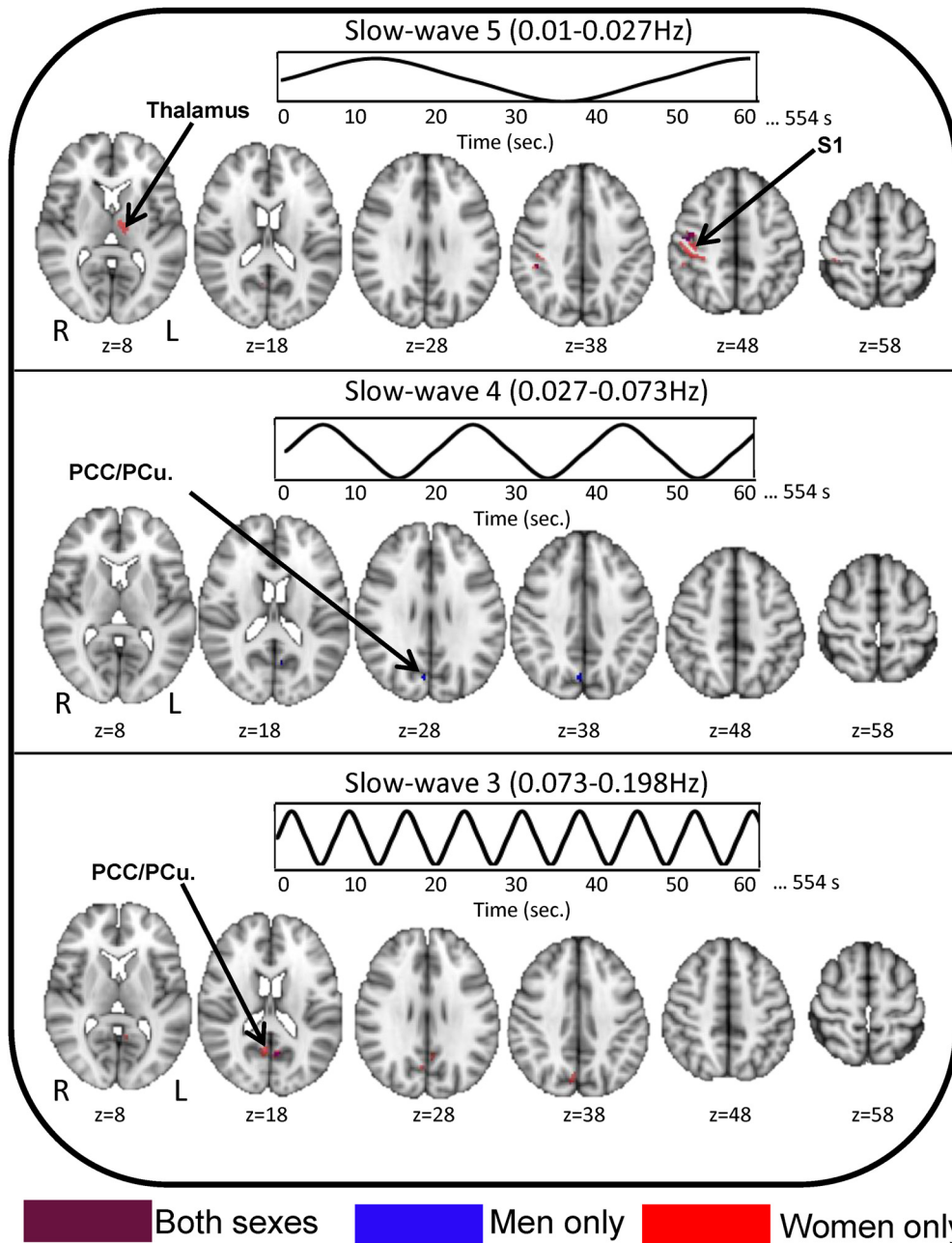


Figure 3. Frequency-specific differences in BOLD signal variability/LFOs between AS patients and HCs is primarily driven by female subjects. The contrast map indicates the extent to which the differences in BOLD signal variability/LFOs between all AS patients versus all HCs is explained by male subjects (male AS patients vs male HCs; blue clusters), by female subjects (AS patients vs female HCs; red clusters), or by both sexes (purple clusters). All statistical images display significant clusters ($p < 0.05$, FWE corrected). All axial slices are represented in radiological orientation. S1, primary somatosensory cortex; PCC/PCu, Posterior cingulate cortex/precuneus.

ports. However, most studies do not distinguish pain at the time of the study (i.e., state pain) from average pain experienced over time (i.e., trait pain). Both state and trait pain reflect important but different aspects of chronic pain conditions. One of the sec-

ondary aims of this study was to raise the issue that functional brain abnormalities commonly reported in chronic pain patients may not explain both state- and trait-like pain characteristics. Our results show that, even though state- and trait-like pain char-

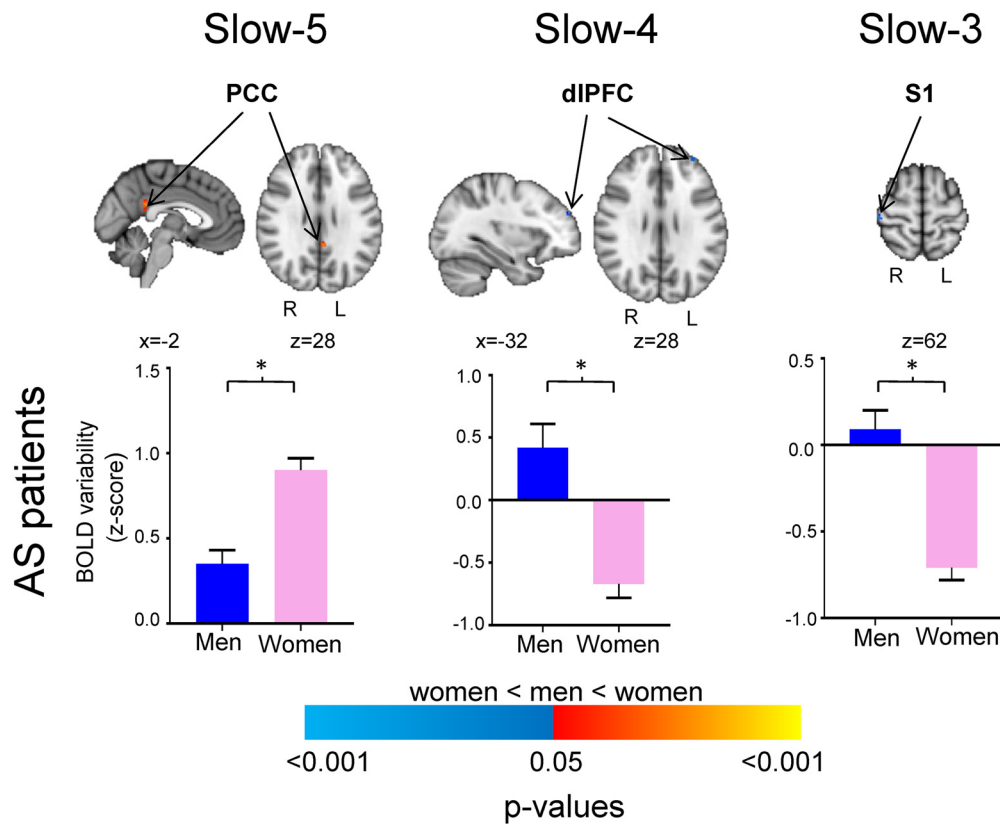


Figure 4. Frequency-specific sex differences in BOLD signal variability/LFOs in healthy controls and AS patients. The histograms (blue, men; pink, women) represent the standardized BOLD signal variability values (z-scores) extracted from the significant clusters derived from the contrast maps between men and women. The significant clusters are depicted in the brain maps shown to the right of each graph. All significant clusters are thresholded at $p < 0.05$ (FWE corrected). Warm colors represent brain areas in which women had greater BOLD signal variability/LFOs compared with men, and cool colors represent brain areas in which women had lower BOLD signal variability/LFOs compared with men. S1, Primary somatosensory cortex; dlPFC, Dorsolateral prefrontal cortex; PCC, Posterior cingulate cortex; * $p < 0.05$, FWE-corrected.

Table 3. Peak MNI coordinates from brain regions that showed sex-differences in BOLD signal variability/LFOs

Frequency Band	Contrast	Number of voxels	MNI coordinates (mm)			Brain region
			x	y	z	
Slow-5 (0.01–0.027 Hz)	AS men > HC men	49	46	-16	50	Right primary somatosensory cortex
		14	42	-36	40	Right supramarginal gyrus
	AS women > HC women	10	38	-20	54	Right primary somatosensory cortex
		289	46	-38	40	Right primary somatosensory cortex
Slow-4 (0.027–0.073 Hz)	AS men > HC men	23	-6	-10	6	Left thalamus
	AS women > HC women	57	6	-72	34	Precuneus
Slow-3 (0.073–0.198 Hz)	AS men > HC men	21	-6	-62	18	Posterior cingulate cortex
	AS women > HC women	154	8	-60	18	Posterior cingulate cortex
		90	-6	-60	16	Posterior cingulate cortex

The AS patients consisted of 19 men and 19 women. All statistical images were thresholded at $p < 0.05$ (FWE corrected for multiple comparison) using cluster-free threshold enhancement.

acteristics are highly correlated ($\rho = 0.732, p < 0.001$), functional brain impairments, as revealed through LFO, cannot explain patients' current (state-like) pain intensity ratings (Fig. 2B).

Additional analysis: impact of head motion, psychiatric metrics, and treatment effects

One important consideration of this study is the potential of physiological rhythms and head motion artifacts being aliased into the BOLD signal, particularly at higher frequencies (Cordes et al., 2001). We performed additional analyses to examine whether any of our findings were impacted by technical factors (i.e., head motion) or by psychiatric and treatment effects.

There was no significant differences in mean relative frame-wise displacement between AS patients and HCs (HCs, $0.09 \pm$

0.06 mm; AS patients, 0.07 ± 0.04 mm; independent-samples Mann–Whitney U test, $z = -0.128, p = 0.898$). Also, including mean relative head motion as a covariate of no interest into the multivariate regression model had a marginal effect on the ability of slow-3 LFOs to make generalizable inferences about patients' trait pain ($r = 0.43, p = 0.0082$; MSE, 4.94; $p = 0.0126$).

As expected, there were statistically significant differences between the patients and HCs in psychiatric metrics, specifically depression (BDI: $z = -3.98, p < 0.05$), state anxiety ($z = -4.25, p < 0.05$), and trait anxiety ($z = -3.73, p < 0.05$), although none of the patients had clinical levels indicative of a psychiatric disorders. However, we did not find any significant relationship between BOLD signal variability/LFO group contrast results in any of the frequency bands and these psychiatric measures (slow-5:

BDI, $n = 56$, Spearman's $\rho = 0.02$, $p = 0.886$; state anxiety, $n = 56$, $\rho = -0.216$, $p = 0.11$; trait anxiety, $n = 56$, $\rho = -0.048$, $p = 0.726$; slow-4: BDI, $n = 56$, $\rho = -0.069$, $p = 0.613$; state anxiety, $n = 56$, $\rho = 0.005$, $p = 0.973$; trait anxiety, $n = 56$, $\rho = -0.048$, $p = 0.726$; slow-3: BDI, $n = 56$, $\rho = -0.043$, $p = 0.753$; state anxiety, $n = 56$, $\rho = 0.043$, $p = 0.755$; trait anxiety, $n = 56$, $\rho = -0.024$, $p = 0.858$). Therefore, it is unlikely that the relationship between BOLD signal variability and patients' average pain are driven by anxiety or depression.

Finally, since our cohort contained patients both treated ($n = 31$) and nontreated ($n = 25$) with biologics, we performed a follow-up analysis to ensure that our results were not driven by treatment. Within the clusters that showed significant group differences between AS patients and HCs, treated and nontreated patients did not show significant differences in BOLD signal variability/LFOs within any of the tested frequency bands [mean \pm SEM BOLD signal variability (z -scores); slow-5: treated, -0.122 ± 0.06 ; nontreated, -0.04 ± 0.07 ; $z = -0.700$, $p = 0.721$; slow 4: treated, 0.65 ± 0.06 ; nontreated, 0.69 ± 0.06 ; $z = -0.783$, $p = 0.883$; slow 3: treated, 0.41 ± 0.06 ; nontreated, 0.46 ± 0.07 ; $z = -0.882$, $p = 0.383$].

Discussion

This is the first study to use a multivariate, machine learning approach to examine LFOs in the dynamic pain connectome of patients with chronic pain. Our main finding is that chronic pain patients with AS exhibit higher-frequency-specific aberrations in BOLD signal variability/LFOs compared with HCs. Within slower frequencies (slow-5), patients had abnormal LFOs in the ascending pain pathway, whereas at higher frequencies (slow-4 and slow-3) these abnormalities were also found in the DMN and SN. Furthermore, our machine learning algorithm revealed that the pattern of slow-3 LFO abnormalities can be used to make generalizable inferences about average pain intensity ratings in previously unseen patients.

Our finding that patients with chronic pain have higher brain signal variability in the dynamic pain connectome (i.e., within the ascending pain pathway, DMN, and SN) are in line with previous studies of LFOs (Baliki et al., 2011, 2014; Alshelhi et al., 2016; Hodkinson et al., 2016). These findings could arise through several mechanisms. First, increased resting-state LFOs within the ascending pain pathway could result from the heightened level of sensory traffic that manifests as part of the ongoing, fluctuating chronic pain intensity. This is supported by other studies in neuropathic pain patients that found increased LFOs within the thalamus and S1 within a similar frequency range (0.04 Hz; slow-5–slow-4 border; Alshelhi et al., 2016), suggesting that this effect is generalizable to many chronic pain conditions. Pain-related rumination and negatively valenced internal thought are other factors that could contribute to increased BOLD signal variability/LFOs. For example, activity in the DMN has previously been attributed to episodes of internally directed and self-referential thought (Fox and Raichle, 2007). Disruption of the DMN has been shown across multiple chronic pain populations (Baliki et al., 2008; Napadow et al., 2010), as well as abnormal increases in LFOs in the DMN of chronic low back pain patients (Baliki et al., 2008). Our patients also exhibited heightened LFOs in the MCC, an area associated with pain affect (Vogt, 2005). The MCC receives projections from the amygdala (Phan et al., 2002), a region implicated in fear (Whalen et al., 1998) and nociception (Bernard et al., 1992). Given the convergence of fear- and pain-related input into the MCC, its elevated engagement in chronic pain is

thought to relate to avoidance behavior often reported in these patients (Vogt, 2005). Together, a heightened level of resting-state activity in the DMN and MCC could reflect the affective-motivational aspect of AS chronic pain.

The neurobiological mechanisms underlying LFOs in the brain are unknown but could involve neuronal and non-neuronal activity (Y. F. Wang et al., 2014; Alshelhi et al., 2016). Preclinical studies have shown that low-frequency brain oscillations, within the 0.1–0.5 Hz frequency range, are generated primarily through perpetual excitation within the cerebral cortex (Sanchez-Vives and McCormick, 2000) and maintained by rhythmic depolarization–hyperpolarization sequence via regulated excitatory and inhibitory postsynaptic potentials (Steriade et al., 1993). The continuous yet fluctuating influx of unpleasant, sensory input experienced by chronic pain patients may be related to the elevated LFOs responsible for the sensory discriminatory and affective-motivation aspects of pain. Moreover, others have speculated that non-neuronal cells (astrocytes) may contribute to LFO regulation and maintenance (Bernard et al., 1992; Alshelhi et al., 2016).

Our study also examined the relationship between LFOs and average (trait) pain intensity but would also like to put forth the importance of studying pain characteristics on different time scales. Few studies have examined brain mechanisms underlying shorter-lasting (state) and longer-lasting (trait) chronic pain, and those that have explored this topic have reported conflicting results. For example, Baliki et al. (2011) showed that when spontaneous pain ratings are collected simultaneously with brain imaging data from chronic low back pain patients, the fluctuating patterns of the pain ratings followed a similar time course as the hemodynamic response from which the LFOs are derived, an effect that was only present in the upper slow-3 range (0.12–0.2 Hz). However, more recently the same group also showed that increased LFO amplitudes (upper half of slow-3, 0.12–0.2 Hz) in the DMN were correlated with the duration of pain in low back pain and osteoarthritis patients, proposing a relationship between LFOs and trait-like features (Baliki et al., 2014). In line with these studies, we found a relationship between higher-frequency LFOs (slow-3) and average pain intensity. However, unlike the aforementioned studies, we used a robust, multivariate machine learning technique that highlights the generalizability between slow-3 LFO abnormalities and average pain intensity ratings. Similar to Baliki et al. (2014), our brain weight maps also suggested that slow-3 LFO abnormalities within DMN (PCC) holds the greatest prediction power for trait pain rating in unseen patients (Fig. 2C).

The mechanisms underlying state- and trait-like chronic pain features may not necessarily be mutually exclusive but, nevertheless, pose a crucial consideration when investigating neural correlates of chronic pain characteristics. The current findings complement our recent work showing a unique pattern of brain connectivity that can be used to differentiate state and trait pain (Cheng et al., 2018). Trait pain ratings reflect intensity levels that act as an anchor around which state pain levels fluctuate throughout the course of the day. Our findings suggest that aberrations in brain mechanisms that are present in chronic pain patients are reflective of the persistent, longer-lasting intensity of pain and not shorter, state-like representations. The brain plasticity that is responsible for the manifestation of impaired brain mechanisms that develop as a result of chronic pain symptoms presumably occurs over the course of multiple days/weeks and, therefore, is unable to track a single state-like rating that is bound to fluctuate throughout the course of the day. Thus, it is important to con-

sider not only pain intensity levels during testing but also across ratings over longer time scales, which may actually be more informative when investigating brain mechanisms. Of note, there are a number of different approaches to assess trait-like pain characteristics. In this study, patients provided one rating to represent their average pain rating in the week before testing on test date. An alternative approach could have been to have patients use a pain diary to document their pain levels multiple times per day in the week before our testing. Both approaches have advantages and disadvantages, but our straightforward approach was made primarily for practical and compliance issues and is one commonly used by clinicians to obtain a general sense of a patient's pain.

Many patients with chronic pain can have comorbidity with various psychiatric disorders. Although we screened patients and excluded those with a confirmed psychiatric diagnosis, some of our patients had increased levels of anxiety (state and trait) and depression scores compared with the HCs. Therefore, we also investigated whether our main study findings can be explained by these psychiatric effects. Overall, all three traits demonstrated a low correlation with BOLD signal variability group differences in each of the frequency bands, thus limiting the possibility that these effects are driven by any psychiatric involvement and emphasizing their specificity to pain severity.

A secondary aim of this study was to examine sex-related effects. First, we found that the majority of the results obtained from our main analysis, particularly with slow-3 and slow-5, are primarily driven by women subjects. Compared with male patients, women patients show greater functional impairments in pain-associated brain regions, including the ascending pain pathway, compared with their respective controls. Since no sex-differences in average pain ratings exist, this finding suggests that women may have greater engagement of the antinociceptive system to offset these differences. Although the current study did not specifically probe the antinociceptive system, our previous work has shown that, compared with men, women have stronger functional connectivity between the subgenual cingulate cortex and the periaqueductal gray, proposing a greater engagement of the descending modulation system in women (G. Wang et al., 2014). Second, unlike in HCs, our findings suggest frequency-specific sex differences in BOLD oscillations in AS patients, which are consistent with previous studies showing decreased amplitude of LFOs at higher frequencies in the sensorimotor cortex in women compared with men with chronic pain (Hong et al., 2013; Fig. 4). Whereas the neurophysiological significance behind these discrepancies is unclear, it may suggest sex-specific sensory discrimination/perception in chronic pain patients.

In conclusion, we report that patients with chronic pain exhibit frequency-specific abnormalities in LFOs within the dynamic pain connectome as revealed through BOLD signal variability/LFOs, an effect that was not impacted by technical (i.e., head motion) or psychiatric (i.e., depression, anxiety) factors. These abnormalities were localized to the ascending pain pathway at slow oscillation frequencies (slow-5) but also engaged the DMN and SN at higher frequencies (slow-4 and slow-3). Aberrations in BOLD signal variability/LFOs in slow-3 could be used to make generalizable inference about patients' average pain intensity ratings. Thus, our findings indicate that measurable impairments in brain activity in chronic pain patients reflect persistent, longer-lasting levels of trait pain, as opposed to shorter-scale state-like pain.

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