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## Electrochemical-Mediated Gelation Of Catechol-Bearing Hydrogels Based On Multimodal Crosslinking

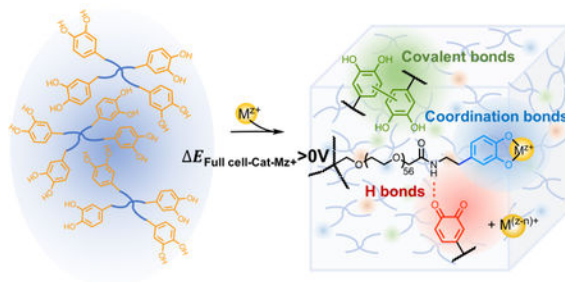
Chenchen Mou<sup>a</sup>, Faisal Ali<sup>b</sup>, Avishi Malaviya<sup>a,b</sup>, Christopher J. Bettinger<sup>a,c</sup>

<sup>a</sup>Department of Biomedical Engineering, Carnegie Mellon University, Pittsburgh, PA 15213, USA. cbetting@andrew.cmu.edu <sup>b</sup>Department of Chemical Engineering, Carnegie Mellon University, Pittsburgh, PA 15213, USA <sup>c</sup>Department of Materials Science and Engineering, Carnegie Mellon University, Pittsburgh, PA 15213, USA

### Abstract

Catechol-bearing polymers form hydrogel networks through cooperative oxidative crosslinking and coordination chemistry. Here we describe the kinetics of cation-dependent electrochemical-mediated gelation of precursor solutions composed of catechol functionalized four-arm poly(ethylene glycol) combined with select metal cations. The gelation kinetics, mechanical properties, crosslink composition, and self-healing capacity is a strong function of the valency and redox potential of metal ions in the precursor solution. Catechol-bearing hydrogels exhibit highly compliant mechanical properties with storage moduli ranging from  $G' = 0.1\text{--}5$  kPa depending on the choice of redox active metal ions in the precursor solution. The gelation kinetics is informed by the net cell potential of redox active components in the precursor solution. Finally, redox potential of the metal ion precursor can differentially alter the effective density of crosslinks in networks and confer properties to hydrogels such as self-healing capacity. Taken together, this parametric study generates new insight to inform the design of catechol-bearing hydrogel networks formed by electrochemical-mediated multimodal crosslinking.

### Graphical Abstract



Applying full cell potential estimation in redox pairs of  $[\text{PEG-Cat}]_4 + \text{M}^{z+}$  to elucidate contributions of metal ion precursors on hydrogel properties.

## 1. Introduction

Catechol-bearing hydrogels are highly tunable polymer networks that have applications ranging from medical materials to soft robotics.<sup>1-6</sup> The versatility of catechol-bearing hydrogels is attributed to the following properties of catechols: redox activity, multimodal bonding, metal ion chelation, and thus coordination bond formation between catechols and metal ions.<sup>7-10</sup> Furthermore, the properties of coordination bonds can be tuned by controlling metal ion composition. Redox active metal ions such as  $\text{Fe}^{3+}$  promote crosslink formation and gelation of catechol-functionalized precursors through multiple mechanisms such as oxidative covalent coupling of  $\alpha$ -quinones/semiquinones or coordination bond formation through metal-catechol complexes.<sup>7, 11, 12</sup> The redox activity and valency of metal cations can alter the balance between oxidative covalent coupling of catechols relative to other types of bonds such as coordination bonds.<sup>11, 13-15</sup> While increasing the concentration of oxidizing agent can promote crosslinking in hydrogel networks,<sup>16-18</sup> the composition and stoichiometry of metal ions can also influence network properties through multiple mechanisms.<sup>10, 19-21</sup> For example, controlling the stoichiometric ratios of metal ions to catechols along with pH can alter the mechanical properties of the resulting hydrogel by promoting coordination bonds with properties that approximate covalent bonds.<sup>8</sup> Complexing catechols with metal ions such as  $\text{Fe}^{3+}$  can create mono-, bis-, or tris-catechol- $\text{Fe}^{3+}$  depending on the pH.<sup>7, 19</sup> Furthermore, the storage moduli of gels prepared from catechol-bearing polyallylamine crosslinked with multivalent cations such as  $\text{Fe}^{3+}$ ,  $\text{Al}^{3+}$ ,  $\text{Ga}^{3+}$ , or  $\text{In}^{3+}$  is highly pH-dependent. The maximum storage moduli of hydrogels is observed when the pH value approximates the pKa of primary amines.<sup>12</sup> Networks composed of catechol-bearing polyallylamine are highly branched and topologically complex since the combination of primary amines and catechols can create covalent bonds through Michael addition and Schiff base formation.<sup>12, 22</sup> Catechol-functionalized four-arm poly(ethylene glycol) ([PEG-Cat]<sub>4</sub>) is potentially a more convenient model precursor polymer to isolate the contributions of metal ion composition on crosslink formation and gelation of hydrogel networks. Catechol-bearing PEG-based networks have been previously used to measure the characteristic relaxation times in hydrogels crosslinked with various metal ions.<sup>10</sup> 4-arm [PEG-Cat]<sub>4</sub> precursors have a tractable molecular weight between crosslinks, which facilitates calculations of swelling and simplifies comparative assessment.<sup>23</sup>

The multimodal bonding in these networks provides simultaneous tunability and complexity as the precise distribution of these crosslinks is difficult to decipher. Understanding the role of metal ion composition on intermolecular bonding, crosslinking, and eventual gelation is important because the distribution of crosslinking chemistry can further influence the physical properties of the hydrogel network including gelation kinetics, mechanical properties, and self-healing capacity. We hypothesize that in low pH environments ( $\text{pH} < \text{pK}_{\text{a},-\text{NH}_2}$ ;  $\text{pH} < \text{pK}_{\text{a},\text{Cat}}$ ), the full cell potential of metal ion and catechol ( $\text{M}^{z+}:\text{Cat}$ ) redox pairs in polymer precursors can predict network gelation, independent of the cation valency  $z^+$ . Here, we describe a parametric study to test this hypothesis and elucidate the relative contributions of the valency and redox potential of metal ions on networks prepared from precursor solutions of [PEG-Cat]<sub>4</sub> and  $\text{M}^{z+}$ .

## 2. Materials and methods

[PEG-Cat]<sub>4</sub> was synthesized as previously described albeit with minor modifications.<sup>11, 16, 24</sup> Briefly, under an N<sub>2</sub> (g) blanket, four-arm poly(ethylene glycol) succinimidyl carboxymethyl ester ( $M_w \sim 10,000$  g/mol; Jenkem Technology Ltd, Plano, TX) was combined with dopamine hydrochloride (2:3 mol ratio, neutralized with *N*-methylmorpholine) in anhydrous *N,N*-dimethylformamide (DMF) for 18 h. The product was dialyzed against H<sub>2</sub>O with pH~3.5 (titrated with 1M HCl) for 24 h and then against ddH<sub>2</sub>O for 2 h. The final product of [PEG-Cat]<sub>4</sub> was lyophilized and stored at -15 °C until further use. Purified [PEG-Cat]<sub>4</sub> and dehydrated hydrogel samples were characterized using <sup>1</sup>H NMR (300 MHz, DMSO-d<sub>6</sub>,  $\delta$ , ppm; Bruker Avance 300 MHz), Fourier transform infrared spectroscopy (FTIR; 16 scans at 4 cm<sup>-1</sup> resolution; Spectrum 100 ATR-FTIR, PerkinElmer), and UV-vis spectroscopy (model UV-2600, Shimadzu, Tokyo, Japan). UV-vis tests were performed with a sealed cuvette for 3 h with diluted precursor solutions (1:64 with ddH<sub>2</sub>O) for hydrogel preparation. Prior to measurements, ddH<sub>2</sub>O was purged with N<sub>2</sub> gas for at least 30 min to displace dissolved O<sub>2</sub>.

[PEG-Cat]<sub>4</sub>+M<sup>z+</sup> hydrogels were prepared by combining solutions of [PEG-Cat]<sub>4</sub> with the appropriate metal ion (M<sup>z+</sup>) precursor (see Table 1 and Table S1, concentrations of [PEG-Cat]<sub>4</sub> were maintained at 8 mM in mixtures). Gelation kinetics, mechanical properties, and self-healing capacity were characterized using rheometry (Discovery HR-2, TA instrument, New Castle, DE USA). Gelation time  $\tau_{gel}$  was defined as  $\tau_{gel} = G'_t/G'_\infty = 0.9$ . Storage  $G'$  and loss  $G''$  moduli were measured at frequencies of  $\omega = 0.1 - 100$  rad/s with maximum strain amplitudes of  $\gamma_0 = 5\%$ . The self-healing capacity of hydrogel networks was studied with cyclic sweep with strain increased from  $\gamma = 1$  to 1000% at  $\omega = 5$  rad/s over 100 s, following by another 100 s period for healing.

The swelling behaviour of hydrogels was characterized in ddH<sub>2</sub>O ( $n = 3$ ). The swelling ratio  $Q$  of hydrogel was calculated by the mass ratio of samples in swollen and dehydrated state ( $Q = w_s/w_0$ ). Dimensional swelling was defined as  $q = Q^{1/3}$ . The average molecular weight between crosslinks  $\overline{M}_c$  (g/mol) was calculated using the following equation:<sup>23, 25</sup>

$$\frac{1}{\overline{M}_c} = \frac{2}{M_n} - \frac{\ln(1 - \nu_s) + \nu_s + \chi_1 \nu_s^2}{\rho_p V_1 \nu_r [(\nu_s/\nu_r)^{1/3} - (\nu_s/2\nu_r)]} \quad (1)$$

where  $\nu_s$  is the volume fraction of polymer in the swollen hydrogel,  $\nu_r$  is the volume fraction of polymer in the initial pre-swollen state.  $V_1$  is molar volume of the solvent (18 mL/mol for H<sub>2</sub>O),  $\rho_p$  is the mass density of the polymer ( $\rho_{PEG} = 1.123$  g/cm<sup>3</sup>, and  $\chi_1$  is the polymer-solvent interaction parameter ( $\chi_{PEG-H_2O} = 0.462$ ).<sup>23, 26</sup> The relationship between mechanical properties and effective crosslink density  $\rho_{x,eff}$  (mol/m<sup>3</sup>) was determined using a modified rubber elasticity model:<sup>27, 28</sup>

$$G' = Q_r^{-\frac{1}{3}} RT \rho_{x,eff} \quad (2)$$

where  $Q_r$  is the swelling ratio in reference to the amount of water in sample at initial pre-swollen state,  $R$  is the gas constant and  $T$  is the temperature in kelvin.

### 3. Results and Discussion

The redox-mediated gelation of catechol-bearing PEG is largely controlled by the net cell potential of redox active components in the precursor solution. The central redox reaction that precedes gel formation is the reduction of metal ions and oxidation of catechols into 1,2-benzoquinone.<sup>11, 14</sup> 1,2-benzoquinones subsequently couple oxidatively to create covalent crosslinks.<sup>8, 14</sup> The forward reaction proceeds spontaneously if the reduction potential of metal ion is more positive than that of 1,2-benzoquinone such that the full cell potential  $E_{\text{full-Cat-M}z^+} > 0$ . The full cell potentials and changes in Gibbs free energy of each reaction for catechols with select metal ions  $M^{z+}$  are summarized in Table 1 while the gelation time and mechanical properties are summarized in Fig. 1. Hydrogel networks form when [PEG-Cat]<sub>4</sub> precursors are combined with the following metal cations: Fe<sup>3+</sup>, V<sup>5+</sup>, Au<sup>3+</sup>, or Ag<sup>+</sup>. Notably, monovalent Ag<sup>+</sup> ( $z = 1$ ;  $E_{\text{full-Cat-Ag}^+} = +49.0$  mV) can induce gelation, albeit with slow kinetics (Fig. 1b, Fig. S4c). [PEG-Cat]<sub>4</sub>+Ag<sup>+</sup> hydrogels possess an equilibrium storage modulus of  $G' = 603 \pm 15$  Pa. In comparison, Fe<sup>3+</sup> ( $z = 3$ ;  $E_{\text{full-Cat-Fe}^{3+}} = +21.0$  mV) combined with [PEG-Cat]<sub>4</sub> form hydrogel networks within 30 min. UV-vis spectra have prominent absorption peaks at  $\lambda = 390$  nm and  $\lambda = 280$  nm (Fig. 2), which are attributed to *o*-quinones and catechols/phenolic intermediates, respectively. The concentrations of these species can be estimated from previously reported extinction coefficients (Fig. 2b).<sup>29-31</sup> Values for  $A_{390\text{nm}}$  and  $A_{280\text{nm}}$  decrease and increase, respectively, as the reaction proceeds. The temporal evolution of these species suggests that the initial bolus of *o*-quinones relaxes to phenolic intermediates that have similar absorbance peaks as catechols.<sup>23, 32</sup> [PEG-Cat]<sub>4</sub>+Fe<sup>3+</sup> hydrogels prepared from [Fe<sup>3+</sup>]:[Cat] = 2 are mechanically robust with storage moduli of  $G' = 4730 \pm 210$  Pa (Figs. 1 and 3b). Similarly, [PEG-Cat]<sub>4</sub> precursors combined with V<sup>5+</sup> (VO<sub>3</sub><sup>-</sup>;  $z = 5$ ;  $E_{\text{full-Cat-V}^{5+}} = +250$  mV) promote efficient network formation and gelation. Upon initial mixing of the precursors, UV-vis spectra have an absorption shoulder at  $\lambda = 270$  nm that emerges immediately and persists for 3 h observation (Fig. S4b). [PEG-Cat]<sub>4</sub>+V<sup>5+</sup> hydrogels exhibit a storage modulus of  $G' = 1530 \pm 46$  Pa. Finally, [PEG-Cat]<sub>4</sub> precursors combined with Au<sup>3+</sup> (AuCl<sub>4</sub><sup>-</sup>;  $z = 3$ ;  $E_{\text{full-Cat-Au}^{3+}} = +180$  mV) yield hydrogel networks within ~2 h. Similar trends in the UV-vis spectra of [PEG-Cat]<sub>4</sub>+Fe<sup>3+</sup> and [PEG-Cat]<sub>4</sub>+Au<sup>3+</sup> mixtures were observed. Namely, the concentration of *o*-quinone decreases while the adsorption shoulder around  $\lambda = 258$  nm increases during the first 3 h (Fig. 2c). [PEG-Cat]<sub>4</sub>+Au<sup>3+</sup> hydrogels exhibit an equilibrium storage modulus of  $G' = 57 \pm 8$  Pa, an order of magnitude (or more) smaller than hydrogels prepared using metal ion precursors composed of Fe<sup>3+</sup> or V<sup>5+</sup>.

[PEG-Cat]<sub>4</sub> precursors combined with metal ions  $M^{z+}$  where  $z \geq 2$ , but  $E_{\text{full-Cat-M}z^+} < 0$  V remained as polymer solutions. For instance, precursor solutions of [PEG-Cat]<sub>4</sub>+V<sup>4+</sup> in the

form of  $\text{VO}^{2+}$  remained soluble while UV-vis spectra during 3 h observation exhibit only minor changes in redox behavior, thereby confirming slow reaction kinetics. The UV-vis spectra of precursor solutions of  $[\text{PEG-Cat}]_4+\text{Cu}^{2+}$  and  $[\text{PEG-Cat}]_4+\text{Al}^{3+}$  also support the conclusion that  $E_{\text{full-Cat}} > 0 \text{ V}$  is necessary and sufficient for network formation (Fig. S4e, S4f, S4h). Importantly, pH values for each precursor solution studied herein are  $< 5$  and thus significantly lower than the  $\text{pK}_{\text{a,Cat}} = 9.5$ .<sup>34, 35</sup> Previous reports suggest that  $[\text{PEG-Cat}]_4/\text{dopamine-grafted polyallylamine}$  combined with  $\text{Al}^{3+}$  can form gels under slightly basic conditions ( $\text{pH} \sim \text{pK}_{\text{a,Cat}}$ ).<sup>10, 12</sup> In addition to possible coordination bonds, gelation of dopamine-grafted polyallylamine could be attributed to catechol-primary amine reactions such as Michael addition and Schiff base formation.<sup>12, 22</sup> Taken together, this work suggests that redox reactions between  $[\text{Cat}]$  and  $\text{M}^{z+}$  such that  $E_{\text{full-Cat-M}^{z+}} > 0 \text{ V}$  is necessary and sufficient for network formation.

Where applicable, we posit that redox-mediated covalent coupling of pendant catechols is the primary crosslinking mechanism of  $[\text{PEG-Cat}]_4$  precursors. It follows that  $[\text{PEG-Cat}]_4+\text{M}^{z+}$  precursors with more positive values for  $E_{\text{full-Cat-M}^{z+}}$  should assume larger equilibrium concentrations of *o*-quinones and therefore an increased rate of gelation. The trend in values of  $E_{\text{full-Cat-M}^{z+}}$  for  $[\text{PEG-Cat}]_4+\text{M}^{z+}$  precursors as a function of metal ion composition is  $\text{V}^{5+} > \text{Au}^{3+} > \text{Ag}^+ > \text{Fe}^{3+}$ . However, neither the observed reaction rate (gelation kinetics) nor the final value of  $G'$  were directly proportional to calculated values for  $E_{\text{full-Cat-M}^{z+}}$ . Rather, the observed trends in storage modulus  $G'_{\text{M}^{z+}}$  of  $[\text{PEG-Cat}]_4+\text{M}^{z+}$  hydrogels as a function of metal cation assessed by rheometry is as follows:  $G'_{\text{Fe}^{3+}} > G'_{\text{V}^{5+}} > G'_{\text{Ag}^+} > G'_{\text{Au}^{3+}}$ . While all  $[\text{PEG-Cat}]_4+\text{M}^{z+}$  hydrogels fail at strain amplitudes of  $\gamma_0 > 1000\%$ ,  $[\text{PEG-Cat}]_4+\text{Fe}^{3+}$  hydrogels possess a relatively high torsional toughness compared to other  $[\text{PEG-Cat}]_4+\text{M}^{z+}$  hydrogels (Fig. 3). Furthermore, the storage modulus of  $[\text{PEG-Cat}]_4+\text{Fe}^{3+}$  hydrogels is largely constant across frequencies of  $\omega = 0.1$ – $100 \text{ rad/s}$  suggesting the domination of covalent bonds.<sup>36, 37</sup> Other hydrogel network properties such as effective crosslink density  $\rho_{\text{x,eff}}$  and swelling behaviour  $Q$  were independent of the expected trends based on values for  $E_{\text{full-Cat-M}^{z+}}$ . Specifically, the estimated crosslink density of  $[\text{PEG-Cat}]_4+\text{Fe}^{3+}$  hydrogels is  $\rho_{\text{x,eff}} = 4.38 \text{ mol/m}^3$  which is the highest among all  $[\text{PEG-Cat}]_4+\text{M}^{z+}$  hydrogels. These data coupled with UV-vis spectra support the following observation: the effective crosslinks in  $[\text{PEG-Cat}]_4+\text{Fe}^{3+}$  and  $[\text{PEG-Cat}]_4+\text{Au}^{3+}$  hydrogels prepared using formulations described here are primarily attributed to covalent bonds formed through redox reactions. The UV-vis spectra of  $[\text{PEG-Cat}]_4+\text{Au}^{3+}$  networks exhibit a new absorption peak at  $\lambda = 533 \text{ nm}$ , which is attributed to the formation of  $\text{Au}^0$  nanoparticles (Figs. 2c and S5).<sup>38–40</sup> Additionally, the absorbance peaks at  $\lambda = 264 \text{ nm}$  are optical signatures assigned to covalently coupled catechols (Fig. S6).<sup>41, 42</sup>  $[\text{PEG-Cat}]_4+\text{Ag}^+$  precursor solutions exhibit slow reaction kinetics compared to other  $[\text{PEG-Cat}]_4+\text{M}^{z+}$  formulations that contain transition metal ions. Furthermore,  $[\text{PEG-Cat}]_4+\text{Ag}^+$  precursor solutions exhibit a successive change in color from orange, brown to black, then gradually to yellow-green grey throughout the  $\sim 18 \text{ h}$  gelation period. These observations suggest that slow, but spontaneous redox reactions generate silver nanoparticles.<sup>13, 39</sup> Taken together, these observations suggest that  $\text{Au}^{3+}$  and  $\text{Ag}^+$  promote redox-mediated coupling and oligomerization of pendant catechols.

Given the trends in the physical properties of [PEG-Cat]<sub>4</sub>+M<sup>Z+</sup> hydrogels vs.  $E_{\text{full-Cat}}$ , other types of bonds likely contribute to crosslinking and network formation. Multivalent cations can create additional types of chemical bonding in network that confers unique mechanical properties.<sup>22</sup> For example, coordination bonds confer additional mechanical robustness or self-healing capacity.<sup>7, 8, 22</sup> Fe<sup>3+</sup> rapidly oxidizes catechols based on both the Gibbs free energy of the full redox reaction and UV-vis data. In addition to covalent coupling of catechols, absorption peaks at  $\lambda = 750$  nm suggest the formation of mono-catechol-Fe<sup>3+</sup> complexes (Fig. 2a), reconfigurable bonds that can confer self-healing properties to crosslinked networks.<sup>7, 15, 43, 44</sup> The values of  $A_{750\text{nm}}$  and  $A_{280\text{nm}}$  decrease and increase in UV-vis spectra, respectively, suggesting the shift of equilibrium from mono-Cat-Fe<sup>3+</sup> complexes to phenolic intermediates.<sup>16, 23</sup> Thus, in this stepwise manner, coordination bonds cooperatively enhance the mechanical properties of covalently bound networks. Previous reports of [PEG-Cat]<sub>4</sub>+Fe<sup>3+</sup> hydrogels prepared in basic buffers describe optical signatures that are consistent with bis- and tris-cat-Fe<sup>3+</sup> complexes (absorption peak  $\lambda = 575$  nm and 492 nm respectively).<sup>7, 12, 45</sup> The present findings are consistent with previous reports that mono-Cat-Fe<sup>3+</sup> complexes form in acidic conditions. Reconfigurable bonds are significant contributors to crosslinks observed in [PEG-Cat]<sub>4</sub>+V<sup>5+</sup> hydrogels as inferred through rheological properties. We posit that crosslinking in [PEG-Cat]<sub>4</sub>+Fe<sup>3+</sup> hydrogels have substantial concentrations of covalent bonds formed through oxidative coupling since networks exhibit incomplete healing after rupture, as measured by the recovered storage modulus  $G'$  (Fig. 4a). In contrast, [PEG-Cat]<sub>4</sub>+V<sup>5+</sup> hydrogels can recover the initial value of  $G'$  restored after stress-free recovery periods of 100 s for each successive cycle (Fig. 4b). This mechanical behaviour is attributed to the reversible self-healing ability of H-bonds and coordination bonds.<sup>8, 46, 47</sup> The frequency sweep of rheology test shows frequency-dependent storage modulus first at low angular frequencies and then exhibits largely constant with increasing frequency (Fig. 3b), indicating the presence of reversible bonds in the hydrogel network.<sup>10, 36, 48</sup> Furthermore, [PEG-Cat]<sub>4</sub>+V<sup>5+</sup> precursor solutions produce a yellow tint immediately upon combination, suggesting that networks likely form in a redox-independent manner.<sup>49</sup> Compared to other species of metal ions, the FTIR spectra of [PEG-Cat]<sub>4</sub>+V<sup>5+</sup> hydrogels exhibit relatively symmetric peaks between peaks at 962 cm<sup>-1</sup> (C-H vibration) and 929 cm<sup>-1</sup> (V-O stretching) (Fig. 5).<sup>50</sup> In addition, spectra recorded from [PEG-Cat]<sub>4</sub>+V<sup>5+</sup> networks exhibit a new peak at 1491 cm<sup>-1</sup>, which is assigned to benzenoid ring stretching.<sup>51-54</sup> Notably, the V<sup>5+</sup> (VO<sub>3</sub><sup>-</sup>) induced hydrogel dissolves within 30 min of incubation in water. Taken together, these data suggest that hydrogels prepared from precursor compositions with [VO<sub>3</sub><sup>-</sup>]:[Cat] = 2 are mostly composed of non-covalent coupling between vanadium complexes and catechol groups.<sup>21, 55</sup>

In addition to bonding type, coordination chemistry between metal cations and the pendant catechols can also help to explain the mechanical behavior of [PEG-Cat]<sub>4</sub>+M<sup>Z+</sup> hydrogels.<sup>12, 22</sup> Based on the Pearson acid-base concept, early and late transition metals are characterized as “hard” and “soft” acids, respectively.<sup>56, 57</sup> Accordingly, the order from hard to soft ions of metals in this work is as follows: V, Fe, Ag, and Au. The binding strength of M<sup>Z+</sup> to catechol ligands is proportional to the hardness of the ion.<sup>56, 57</sup> These trends can partially explain the mechanical robustness in [PEG-Cat]<sub>4</sub>+M<sup>Z+</sup> hydrogels prepared from V<sup>5+</sup>, Au<sup>3+</sup>, and Ag<sup>+</sup>. [PEG-Cat]<sub>4</sub>+V<sup>5+</sup> hydrogels prepared from hard acids exhibit a higher

value for  $G'$  and more rapid gelation kinetics compared to [PEG-Cat]<sub>4</sub>+M<sup>Z+</sup> hydrogels prepared from ions that are soft acids such as Ag<sup>+</sup> and Au<sup>3+</sup>. The chemical hardness  $\eta$  of Fe<sup>3+</sup> is  $\eta_{\text{Fe}^{3+}} = 13.1 \text{ eV}$ .<sup>57</sup> When placed in context with the UV-vis spectra, Fe<sup>3+</sup> functions as a “hard” acid that promotes coordination bond formation. Then the transition from coordination bonds to covalent bonds thereby increasing the  $G'$  of [PEG-Cat]<sub>4</sub>+Fe<sup>3+</sup> hydrogel networks in a stepwise manner. In comparison, weak Lewis acids such as monovalent Ag<sup>+</sup> ( $\eta_{\text{Ag}^+} = 6.9 \text{ eV}$ <sup>57</sup>) promote network formation in [PEG-Cat]<sub>4</sub>+Ag<sup>+</sup> hydrogel solely through covalent bonds formation.

## 4. Conclusions

Catechol-functionalized four-arm PEG ([PEG-Cat]<sub>4</sub>) serves as a convenient model to elucidate the role of metal ion composition on gelation including vanadium (V<sup>4+</sup>; V<sup>5+</sup>), iron (Fe<sup>3+</sup>), gold (Au<sup>3+</sup>), aluminium (Al<sup>3+</sup>), copper (Cu<sup>2+</sup>) and Silver (Ag<sup>+</sup>). The full cell potential between pendant catechols and metal ions can predict the redox-mediated gelation behavior of [PEG-Cat]<sub>4</sub>+M<sup>Z+</sup> acidic precursor solutions with pH values smaller than pK<sub>a,-NH2</sub> and pK<sub>a,-Cat</sub>. Multivalent redox active metal ion precursors such as Fe<sup>3+</sup> produce crosslinks through both covalent bonds and metal-organic coordination bonds while strongly oxidative precursors such as Au<sup>3+</sup> and Ag<sup>+</sup> create hydrogel networks primarily through covalent bond formation. Therefore, catechol oxidation is necessary and sufficient for gelation of catechol-bearing hydrogel precursors. While coordination bonds are not necessary for hydrogel formation, they can contribute to the increase of crosslinking density and confer properties such as self-healing owing to their reconfigurable nature. This parametric study can provide forward guidance to designing catechol-bearing networks that are formed from metal ion precursors.

Catechol-bearing hydrogels can match the mechanical properties of excitable tissues. As such, this class of materials is a promising substrate material for flexible electronics and biointegrated electronics that can potentially bridge the biotic-abiotic interface for applications ranging from neuromodulation to implantable sensors.

## Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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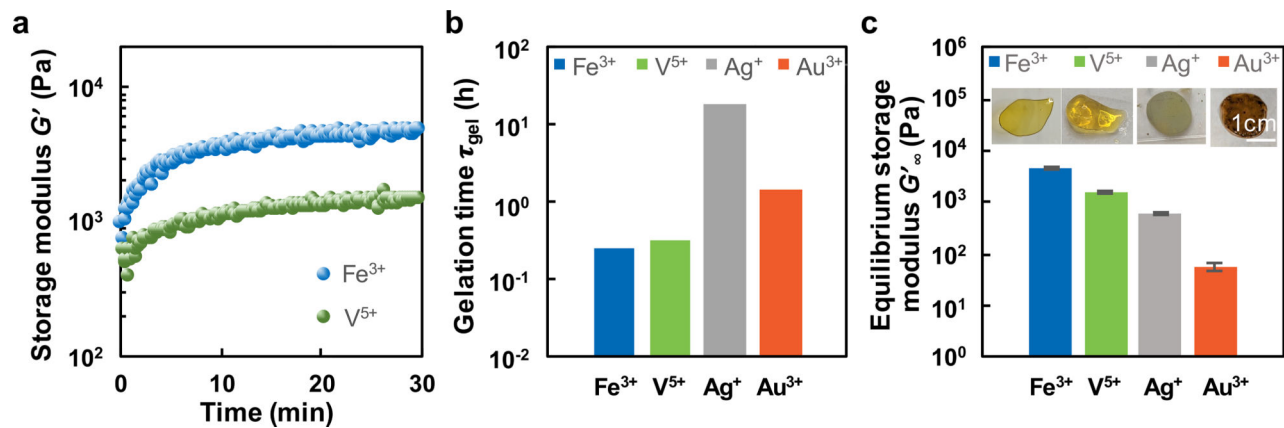
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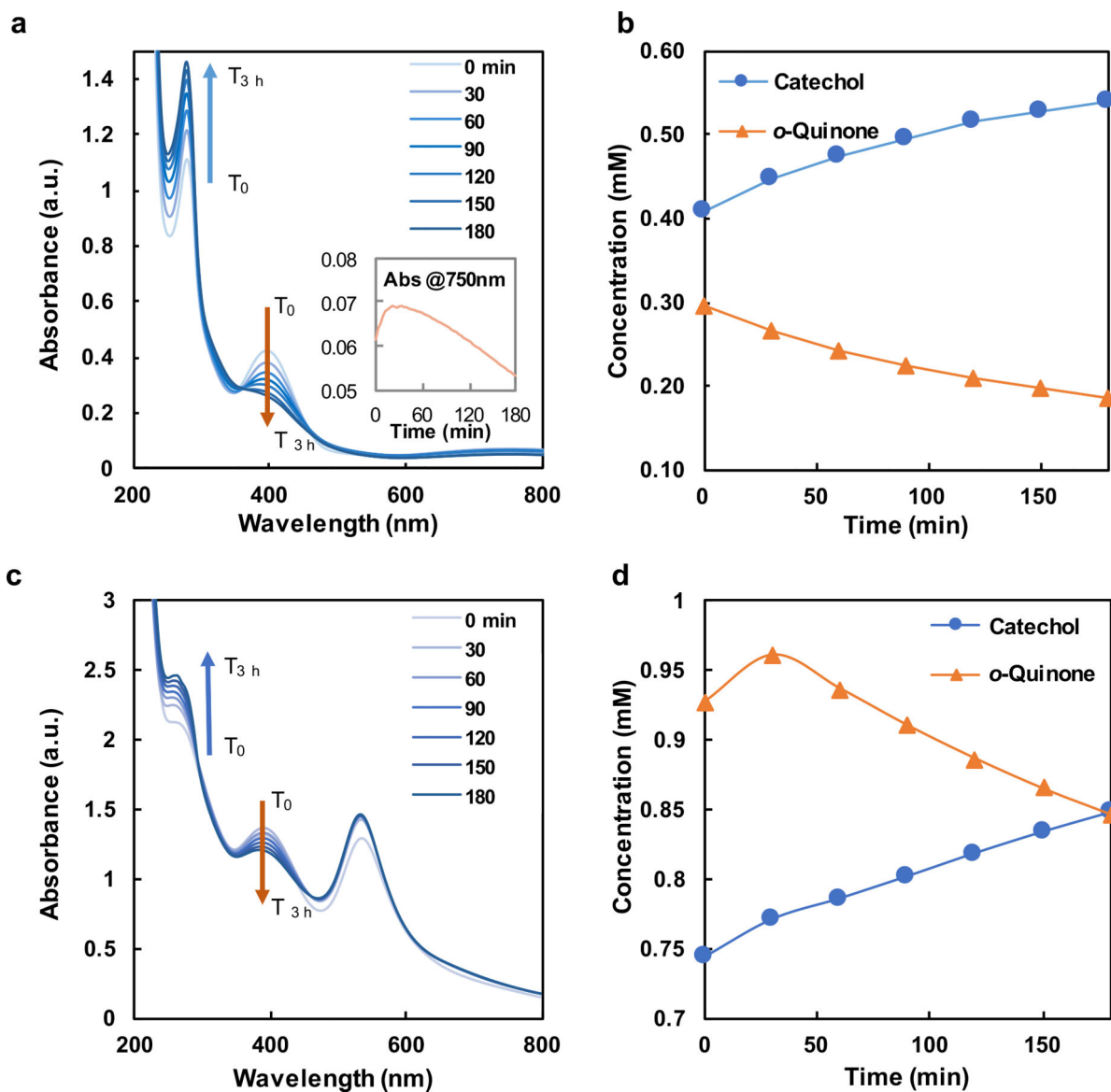


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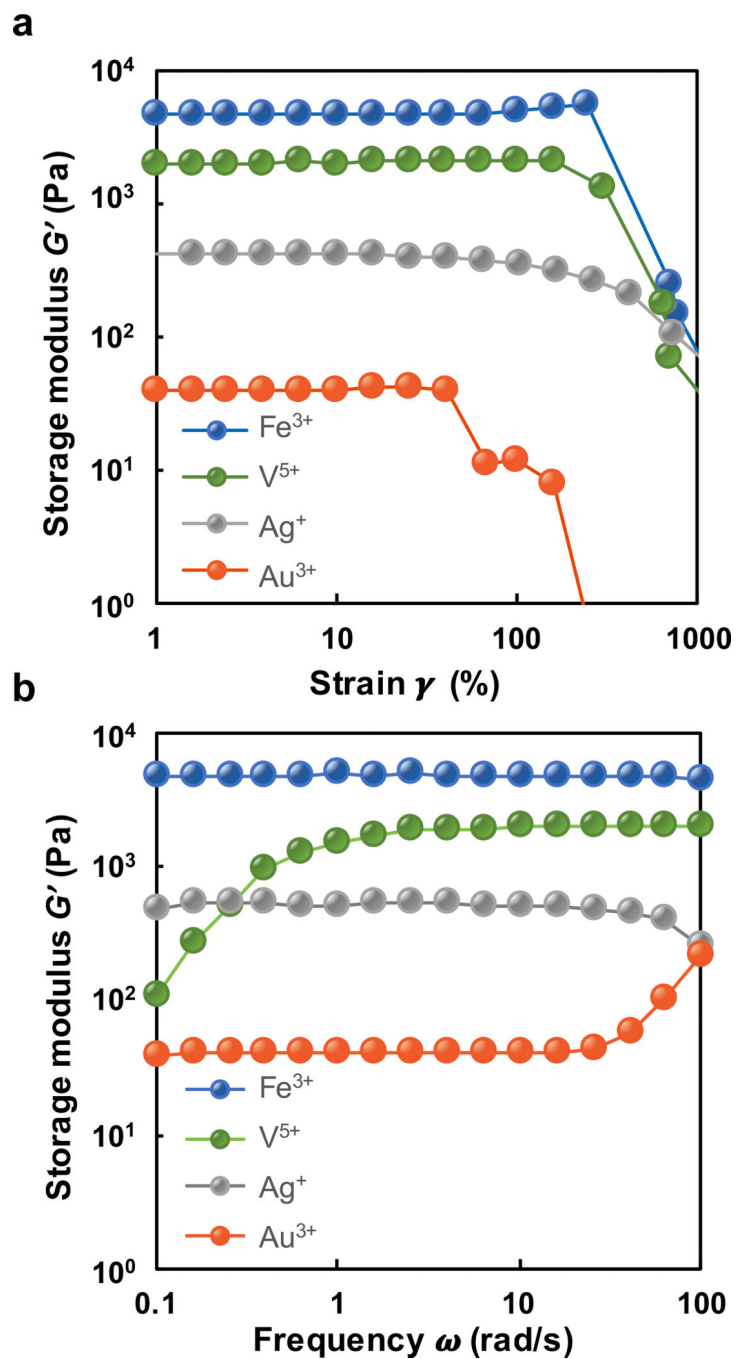
**Figure 1.**

(a) Gelation kinetics of [PEG-Cat]<sub>4</sub>+M<sup>Z+</sup> for select metal ion compositions. (b) Gelation time for [PEG-Cat]<sub>4</sub>+M<sup>Z+</sup> networks as a function of metal ion composition. (c) Equilibrium storage modulus and physical appearance of [PEG-Cat]<sub>4</sub>+M<sup>Z+</sup> hydrogels.

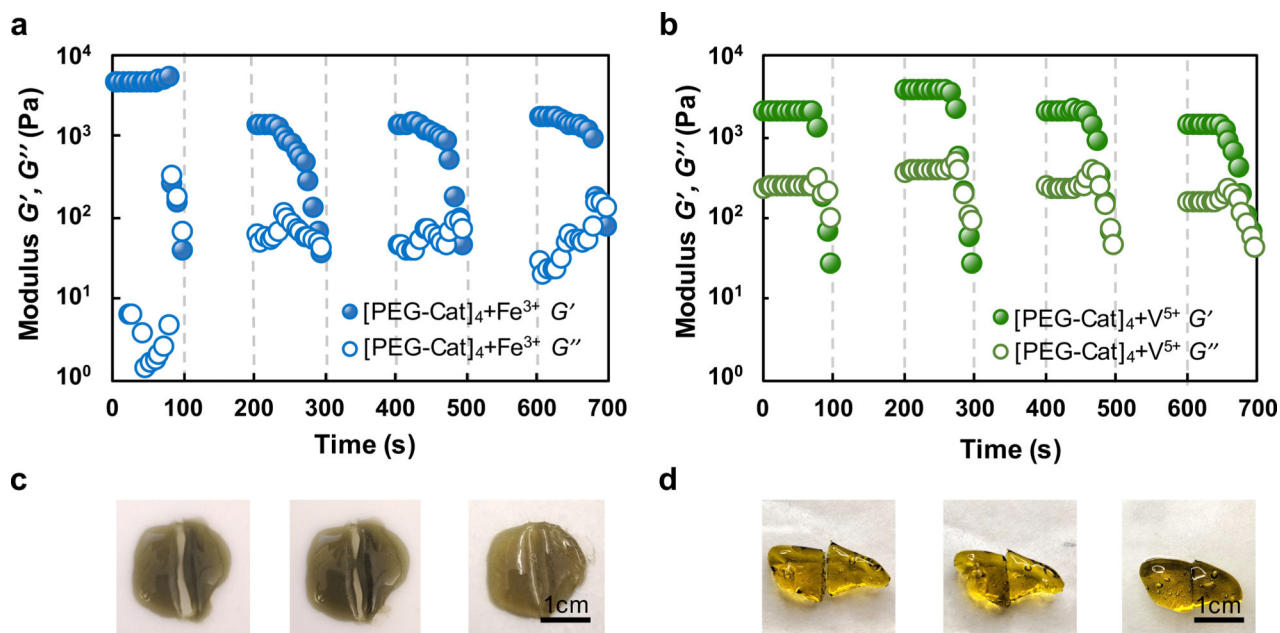


**Figure 2.**

(a) UV-vis spectra along with (b) temporal evolution of  $[\text{H}_2\text{Q}]$  and  $[\text{Q}]$  in dilute polymer solutions of  $[\text{PEG-Cat}]_4 + \text{Fe}^{3+}$  as calculated from  $A_{280\text{nm}}$  and  $A_{390\text{nm}}$ , respectively. (c) Raw UV-vis spectra and (d) temporal evolution of  $[\text{H}_2\text{Q}]$  and  $[\text{Q}]$  in dilute polymer solutions of  $[\text{PEG-Cat}]_4 + \text{Au}^{3+}$  precursors.

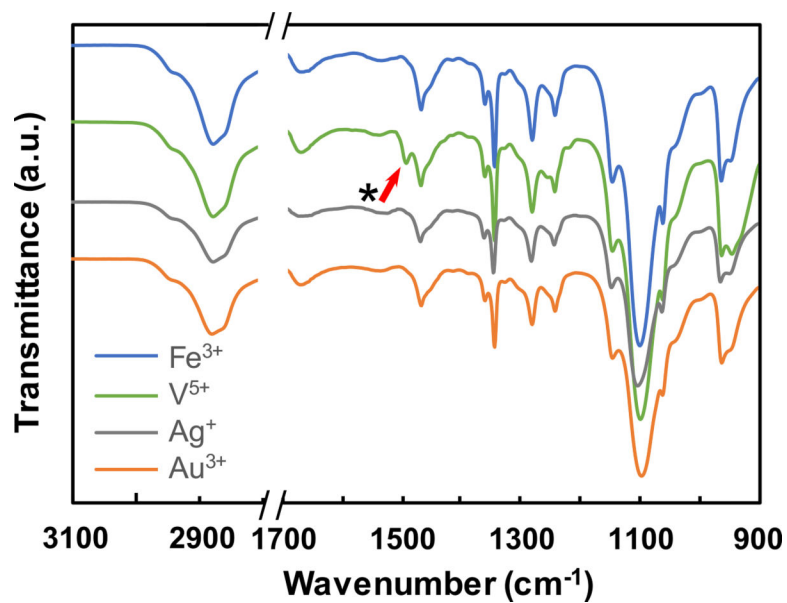


**Figure 3.** Storage modulus of  $[\text{PEG-Cat}]_4+\text{M}^{z+}$  hydrogels with (a) amplitude sweep from  $\gamma = 1$ –1000% strain and (b) frequency sweep from  $\omega = 1$ –100 rad/s.



**Figure 4.**

Plots of storage  $G'$  and loss  $G''$  modulus for  $[\text{PEG-Cat}]_4+\text{M}^{Z+}$  hydrogels with the following program: successive amplitude sweeps of  $\gamma = 1-1000\%$  with a 100 s ramp; recovery time of 100 s. This program was repeated a total of four times for each sample including (a)  $[\text{PEG-Cat}]_4+\text{Fe}^{3+}$  and (b)  $[\text{PEG-Cat}]_4+\text{V}^{5+}$  hydrogels. Representative samples of (c)  $[\text{PEG-Cat}]_4+\text{Fe}^{3+}$  hydrogels (d)  $[\text{PEG-Cat}]_4+\text{V}^{5+}$  hydrogels that undergo self-healing after physical damage.



**Figure 5.** FTIR spectra of [PEG-Cat]<sub>4</sub>+M<sup>Z+</sup> hydrogels prepared using metal ion precursors of different compositions. The peak indicated by the arrow is observed only in [PEG-Cat]<sub>4</sub>+V<sup>5+</sup> hydrogels and is attributed to benzenoid ring stretching.

**Table 1.**

Standard Gibbs free energy calculations and experimentally observed gelation times.

M <sup>z+</sup>	Standard Reduction Potential (mV) (vs. SHE) <sup>a</sup>	Net Reaction <sup>b</sup>	Full Cell Potential E <sub>0</sub> (mV)	Standard Gibbs Free Energy G <sub>0</sub> (kJ/mol)	Gelation Time (min)
Fe <sup>3+</sup>	771	2Fe <sup>3+</sup> + QH <sub>2</sub> → 2Fe <sup>2+</sup> + Q + 2H <sup>+</sup>	21.0	-4.05	15.0
V <sup>5+</sup>	1000	2VO <sub>3</sub> <sup>-</sup> + 8H <sup>+</sup> + QH <sub>2</sub> → 2VO <sup>2+</sup> + Q + 4H <sub>2</sub> O	250	-48.3	20.7
Ag <sup>+</sup>	799	2Ag <sup>+</sup> + QH <sub>2</sub> → 2Ag + Q + 2H <sup>+</sup>	49.0	-9.46	1080
Au <sup>3+</sup>	930	2[AuCl <sub>4</sub> <sup>-</sup> ] + 3QH <sub>2</sub> → 2Au + 3Q + 6HCl + 2Cl <sup>-</sup>	180	-104	90.0
Cu <sup>2+</sup>	159 <sup>c</sup>	2 Cu <sup>2+</sup> + QH <sub>2</sub> → 2Cu <sup>+</sup> + Q + 2H <sup>+</sup>	-591	114	∞
Cu <sup>2+</sup>	337 <sup>d</sup>	Cu <sup>2+</sup> + QH <sub>2</sub> → Cu + Q + 2H <sup>+</sup>	-413	79.7	∞
Al <sup>3+</sup>	-1680	2Al <sup>3+</sup> + 3QH <sub>2</sub> → 2Al + 3Q + 6H <sup>+</sup>	-2430	1407	∞
V <sup>4+</sup>	340	2VO <sup>2+</sup> + 2H <sup>+</sup> + QH <sub>2</sub> → 2V <sup>3+</sup> + 2H <sub>2</sub> O + Q	-410	79.1	∞

<sup>a</sup>Standard hydrogen electrode.<sup>b</sup>Note: QH<sub>2</sub> - fully reduced catechol; Q - fully oxidized *o*-quinone. E<sub>red, quinone</sub> = 750 mV<sup>33</sup><sup>c</sup>Reduction of Cu<sup>2+</sup> to Cu<sup>+</sup><sup>d</sup>Reduction of Cu<sup>2+</sup> to Cu<sup>0</sup>

**Table 2.**Relevant network properties of [PEG-Cat]<sub>4</sub>+M<sup>Z+</sup> hydrogels.

M <sup>Z+</sup>	<i>Q</i>	<i>q</i>	M <sub>c</sub> (g/mol)	$\rho_x$ (mol/m <sup>3</sup> )
Fe <sup>3+</sup>	15.9 ± 0.3	2.51 ± 0.02	2650 ± 63	4.38 ± 0.19
V <sup>5+</sup>	— <sup>a</sup>	— <sup>a</sup>	— <sup>a</sup>	1.41 ± 0.04
Ag <sup>+</sup>	47.5 ± 7.2	3.61 ± 0.20	4210 ± 290	0.56 ± 0.01
Au <sup>3+</sup>	41.8 ± 2.5	3.47 ± 0.07	4400 ± 60	0.05 ± 0.01

<sup>a</sup>Hydrogel dissolved within 30 min incubation in H<sub>2</sub>O.