

Desynchronization of Fronto-Temporal Networks During Working Memory Processing in Autism

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Abstract: *Background:* Mounting evidence suggests that autism is a network disorder, characterized by atypical brain connectivity, especially in the context of high level cognitive processes such as working memory (WM). Accordingly, atypical WM processes have been related to the social and cognitive deficits observed in children with autism spectrum disorder (ASD). *Methods:* We used magnetoencephalography (MEG) to investigate connectivity differences during a high memory load (2-back) WM task between 17 children with ASD and 20 age-, sex-, and IQ-matched controls. *Results:* We identified reduced inter-regional alpha-band (9–15 Hz) phase synchronization in children with ASD during the WM task. Reduced WM-related brain synchronization encompassed fronto-temporal networks ($ps < 0.04$ corrected) previously associated with challenging high-level conditions (i.e. the left insula and the anterior cingulate cortex (ACC)) and memory encoding and/or recognition (i.e. the right middle temporal gyrus and the right fusiform gyrus). Additionally, we found that reduced connectivity processes related to the right fusiform were correlated with the severity of symptoms in children with ASD, suggesting that such atypicalities could be directly related to the behavioural deficits observed. *Discussion:* This study provides new evidence of atypical long-range synchronization in children with ASD in fronto-temporal areas that crucially contribute to challenging WM tasks, but also emotion regulation and social cognition processes. Thus, these results support the network disorder hypothesis of ASD and argue for a specific pathophysiological contribution of brain processes related to working memory and executive functions on the symptomatology of autism. *Hum Brain Mapp* 37:153–164, 2016. © 2015 Wiley Periodicals, Inc.

Key words: alpha oscillations; phase-locking values; executive functions; MEG; children

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INTRODUCTION

Autism is a neurodevelopmental disorder characterized by social deficits but also restricted and repetitive behavior [American Psychiatric Association, 2013]. Mounting evidence suggests that several behavioral symptoms of autism spectrum disorder (ASD) are the consequence of a “network disorder” [Frith, 2004; Geschwind and Levitt, 2007] that may itself result from an atypical differentiation of complex networks underlying high level cognitive tasks such as language, mental flexibility, or working memory [Anagnostou and Taylor, 2011; Barendse et al., 2013; Belmonte et al., 2004; Geschwind and Levitt, 2007; Minshew and Williams, 2007; Misic et al., 2014; O’Hearn et al., 2008; Vissers et al., 2012; Ye et al., 2014].

Functional magnetic resonance imaging (fMRI) studies have shown reduced long-distance connectivity (i.e. cortical underconnectivity) in ASD compared with control groups across several brain regions including the frontoparietal [Just et al. 2007; Kana et al., 2006], fronto-fusiform [Koshino et al. 2008], or fronto-striatal [Silk et al., 2006] networks. While some results show local over-connectivity in the frontal and temporal areas, long-range disconnection between frontal and posterior areas are predominant findings in ASD [see Just et al., 2012; Maximo et al., 2014 for a recent review].

To our knowledge only two studies have investigated both structural and functional connectivity simultaneously in ASD. Ray et al. [2014] showed that patients with ASD exhibited higher connectivity in structural and functional networks within but not between the “rich-club” (i.e. hub) networks, while Verly et al. [2014] found that a reduction of both functional and structural connectivity processes was predictive of language difficulties in autism. These results suggest a direct relation between structural and functional abnormalities in ASD. Accordingly, it has been hypothesized that the structural abnormalities, but also the associated compensatory brain processes (unusual activation of alternative brain regions) observed in ASD, may lead to inefficient functional connectivity processes among brain regions to achieve task performance [Just et al., 2007; Maximo et al., 2014]. In particular, high level cognitive functions such as language, mental flexibility, or working memory that are impaired in ASD rely on optimal inter-regional connectivity (i.e. the transfer of information) of complex networks that synchronize fronto-posterior speci-

alized areas through the white matter tracts [Just et al., 2012; O’Hearn et al., 2008]. Accordingly, structural MRI studies have shown some atypicalities in ASD such as abnormal white matter volume or white matter microstructure [Herbert et al., 2004; Shukla et al., 2011] as well as altered long-range white matter connections that might be related to socio-cognitive symptoms of ASD [see Ameis and Catani, 2015 for a recent review]. In addition, an abnormal neurodevelopmental trajectory of white matter maturation processes and of several cortical, subcortical, and cerebellar brain volumes have been identified in children with ASD [Sussman et al., 2015; Weinstein et al., 2011; Wolff et al., 2012].

In the present study, we investigated the brain connectivity mechanisms that underlie working memory (WM) processes in ASD as it represents an essential feature of social cognition and executive processes that could explain many behavioural symptoms of ASD [Barendse et al., 2013].

The development of WM functions that allows one to transiently store and manipulate “online” information [Baddeley, 2012], relies mainly on the functional specialization and integration (communication) of three brain regions; (1) the prefrontal cortex that allows the manipulation and maintenance of information in WM [Curtis and D’Esposito, 2003; D’Esposito et al., 1999], (2) the inferior parietal lobe which acts as an information buffer [Koshino et al., 2005] and (3) the temporal lobe which allows the encoding storage and retrieval of information in WM [Bergmann et al., 2012].

Impaired WM processes, have been frequently reported in autism, with WM deficits reported most often in the visuo-spatial domain in ASD [Landa and Goldberg, 2005; Steele et al., 2007; Williams et al., 2014] and when the task imposes a heavier load on WM [de Vries and Geurts, 2014; Landa and Goldberg, 2005; McGonigle-Chalmers et al., 2008; Williams et al., 2006]. However, behavioral results are inconsistent as a number of studies also found normal WM performance in this population [Geurts et al., 2004; Happe et al., 2006; Ozonoff and Strayer, 2001; Sinzig et al., 2008].

One possible explanation for these discrepant results may be related to the atypical strategies that some children with ASD use to perform complex tasks [Rump et al., 2009; Salter et al., 2008]. We recently identified using magnetoencephalography (MEG), important qualitative differences in the timing and localisation of brain activations underlying WM processes in children with ASD. WM-related brain processes were associated with the activation of the left insula from 225 to 275 ms and of the left intraparietal sulcus (IPS) from 325 to 375 ms in typically developing children. However, although no between-group difference was observed at the behavioral level, the ASD group recruited the left angular gyrus and the left precuneus in this time window, suggesting that WM processes rely on different brain networks in ASD [Urbain et al., 2015].

Abbreviations

ACC	anterior cingulate cortex
ASD	autism spectrum disorder
fMRI	functional magnetic resonance imaging
IFG	inferior frontal gyrus
IPS	intraparietal sulcus
MEG	magnetoencephalography
PLV	phase locking value
WM	working memory

TABLE I. Demographic information

		Autism (<i>n</i> = 17)	Control (<i>n</i> = 20)		
Age (years)	Mean ± SD	11.17 ± 1.69	11.26 ± 1.64	<i>t</i> (35) = 0.17	<i>P</i> = 0.85
IQ	Mean ± SD	109.94 ± 13.92	115.95 ± 10.97	<i>t</i> (35) = 1.46	<i>P</i> = 0.15
Sex	Male:female	13:7	13:4	$\chi^2(1)=0.57$	<i>P</i> = 0.44
Handedness	Right:left	17:3	16:1	$\chi^2(1)=0.79$	<i>P</i> = 0.37

IQ, intellectual quotient; SD, standard deviation; *t*, value from Student's *t*-distribution; χ^2 , value from chi-squared distribution.

Functional connectivity studies showed that, although the specific areas involved may differ according to the task specificities, WM involves the long-range communication of fronto-posterior brain areas [Koshino et al., 2005; Koshino et al., 2008]. In their first study, Koshino et al. [2005] found that during an *n*-back WM task with letters, brain activity within bilateral frontal regions was correlated with the left parietal regions in control adults but with the right parietal regions in ASD participants. In their second study, Koshino et al. [2008] found, using an *n*-back task that relied on face stimuli, reduced connectivity between the left frontal regions (IFG and MFG) and the temporal (fusiform) areas in the adult ASD group.

Although of interest, these results were obtained using fMRI which has a good spatial but a poor temporal resolution (> 1 s). This might have precluded a precise understanding of the timing of WM processes in the ASD population as an increasing number of studies in healthy adults suggest a crucial role of slow oscillations (i.e. < 15Hz; e.g. alpha, theta) during WM tasks [Brookes et al., 2011; Jensen et al., 2002; Jensen and Tesche, 2002; Palva et al., 2010a]. As MEG measures neuronal activity directly with millisecond (ms) time resolution and good spatial resolution, it has the ability to analyze interregional phase-locking information [Engel et al., 2013]. In particular, the synchronization of theta (4–8 Hz) and/or alpha (9–15 Hz) frequency ranges help the communication between fronto-posterior areas that serve the sub-functions of WM processes [Klimesch et al., 2008; Sauseng et al., 2010]. For instance, connectivity analyses performed in adults showed that better memory performance (i.e., picture recognition) is associated with a short-lasting event-related increase in alpha and theta phase synchronization from 50 to 250 ms post-stimulus onset [Klimesch et al., 2004]. Further evidence suggests that theta and alpha phase synchronization could reflect different processes of WM. Whereas anterior-posterior alpha coherence seems to be involved in the manipulation of stored information [Palva et al., 2010b; Palva and Palva, 2011; Sauseng et al., 2005a], theta coherence may serve instead the central executive aspects of the WM task [Sauseng et al., 2006]. Moreover, looking at WM processes in a paediatric population using MEG, Doesburg et al. [2011], showed altered long-range alpha-band synchronization in children born very preterm.

Together, the above studies show that MEG enables the precise understanding of brain oscillatory correlates of

WM constraints [Brookes et al., 2011; Doesburg et al., 2010; Doesburg et al., 2011; Jensen et al., 2002; Jensen and Tesche, 2002; Palva et al., 2010a] and may help us to better understand how these frequency-specific mnemonic processes might be altered in atypical maturation conditions such as autism. To date, no studies have investigated the oscillatory and related brain connectivity mechanisms for WM in children with ASD.

The present study addresses this gap by investigating, with MEG, the inter-regional brain synchronization elicited in a WM task in children with ASD compared to age-, sex-, IQ-matched typically developing children. We hypothesize that although children with ASD may reach the same level of performance as typically developing children at the behavioral level, long-range connectivity processes involving slow oscillatory mechanisms such as theta or alpha may differ between groups. Specifically, we predict that atypical WM processes may be associated with reduced brain synchronization of fronto-posterior areas.

MATERIAL AND METHODS

Participants

Seventeen children with high functioning ASD and 20 age-, sex-, handedness, and IQ-matched typically developing (TD) controls participated to this study. See Table I for demographic characteristics. These children were selected from a larger sample of 38 children with high functioning ASD and 26 TD control children [age range (year-month): 7y 1mo–13y 11mo].

Children with autism were not included in the study if they had an associated metabolic or genetic disorder, the presence of other neurological disorders, medical illnesses, any current significant Axis I psychiatric comorbidities, uncorrected vision, developmental delay, or learning disability as the primary diagnosis. TD children were not included if they reported a developmental delay, learning disability, any psychiatric, neurological, academic problem, or visual impairment. We arrived at our final sample of 37 children (20 TD and 17 ASD) after sex- and age-matching and excluding children with inadequate task performance (e.g., performance below chance level) or excessive movement in the MEG or MRI scanners.

Clinical diagnoses of ASD were confirmed in all cases with a combination of the Autism Diagnostic Observation

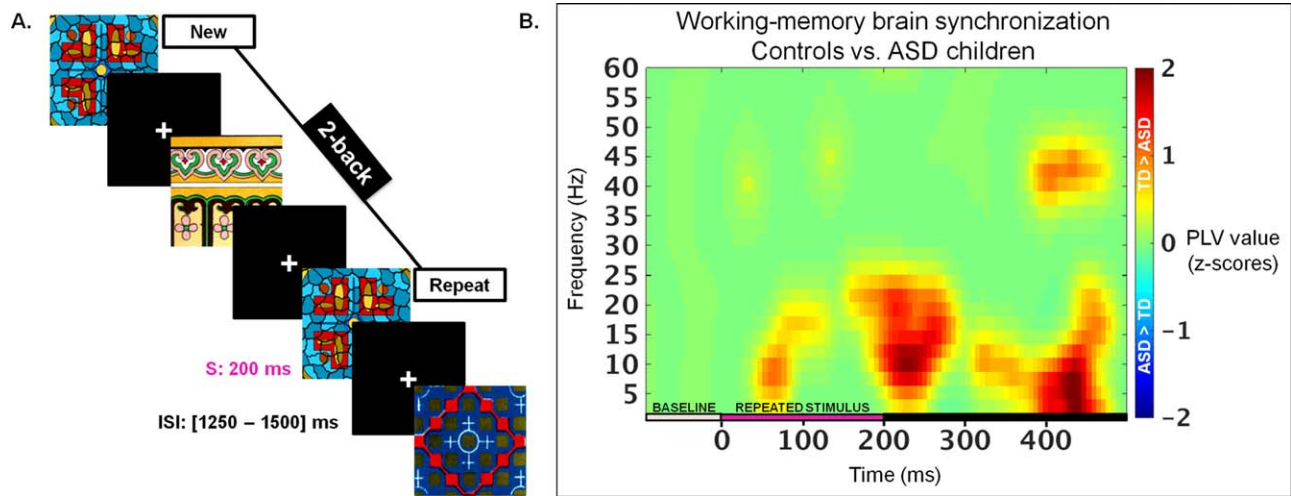


Figure 1.

A: The N-back task. Schematic of the 2-back condition where the child is required to recognize that an image (Repeat) is the same as two images before (New; first occurrence of a picture). Each image (stimulus, S) appeared for 200 ms and was followed by a fixation cross displayed with an ISI varying between 1250 and 1500 ms to reduce anticipation of the next trial. **B:** Differences in

WM-related brain synchronization processes between groups. Differences of averaged PLV values (inter-regional brain synchrony; z-scores; $P < 0.05$) between children with ASD and TD children across time and frequencies from which were selected the time windows and frequency bands of interest that were submitted to the nonparametric Network Based Statistic (NBS) toolbox.

Schedule-General (ADOS-G; Lord et al., 2000) and expert clinical judgment. Nine children with ASD were on one psychotropic medication (Dexamethylphenidate, concerta, biphentin, fluoxetine, Prozac). Their MEG data were examined in comparison to children with ASD who were not taking medication, and the data did not differ between these subgroups (see results section).

Children with ASD were recruited through parent support groups, community support centres and hospital advertisements and TD children were recruited through brochures and flyers posted at the hospital and the surrounding community. MEG and MRI scanning, as well as cognitive and clinical testing, were performed at the Hospital for Sick Children in Toronto. All children gave informed assent and the parents provided informed written consent. Experimental procedures were approved by the Hospital's Research Ethics Board.

Experimental MEG Task and Procedure

Inter-regional synchronization (connectivity) of neuronal oscillations associated with WM was investigated using a classical n-back task (2-back) that children performed in the MEG scanner. In the 2-back task, where high level load is imposed on WM, children were instructed to press a key when they recognised the repetition of a complex multi-coloured abstract image (target) presented two trials earlier (Fig. 1A).

The 2-back task had a maximum of 330 trials including 221 'NEW' and 109 'REPEAT' stimuli. Practice series were

given prior to entering the MEG to ensure that children understood the task. Stimuli used in the practice trials were not included in the experimental blocks. The 2-back task was projected on a screen located 80 cm from the children's eyes; with a visual angle of approximately 4° of their visual field. Each complex picture (NEW and REPEAT) was shown for 200 ms followed by a fixation cross with an inter-stimulus interval (ISI) varying between 1250 and 1500 ms – this jitter prevented anticipation of the next trial.

All children completed the Wechsler Abbreviated Scale of Intelligence (WASI) as well as the Forward and Backwards Digit Recall, Listening Recall, Mazes Memory and Block Recall subscales of the Working Memory Test Battery for Children (WMTB-C) to supplement behavioral data collected during the MEG task.

MEG and MRI Data Acquisition

MEG data were recorded inside a magnetically-shielded room on a CTF Omega 151 channel system (MISL Inc., Coquitlam, Canada) at 600 Hz. Throughout the run, head position was continuously recorded by three fiducial coils placed on the nasion, and left and right pre-auricular points. After the MEG session, anatomical 3T MRI images were acquired (Magnetom 3T Tim Trio, Siemens AG, Erlangen, Germany), T1-weighted magnetic resonance images using high resolution 3D MPRAGE sequences on a 12 channel head coil. MEG data were coregistered to the

MRI structural images using the reference fiducial coil placements.

MEG and MRI Data Processing

Preprocessing, seed definition, and virtual electrode analyses

MEG analyses were performed only on trials associated with correctly recognized REPEAT stimuli. A third-order spatial gradient environmental noise-cancellation was applied to the MEG data that were band-pass filtered off-line at 1-60 Hz. Data were then epoched from 200 ms prior to 1200 ms after stimulus (REPEAT picture) onset. Epochs contaminated by motion (>5 mm) were excluded from the analyses.

MEG data were coregistered with each participant's MRI image. Multisphere head models were constructed based on initial fiducial positions using each individual MRI scan [Lalancette et al., 2011]. MRIs were then normalized into standard MNI space using ANTS (<http://picsl.upenn.edu/software/ants>) with 5-mm voxel-grid of source power [Chau et al., 2004; Singh et al., 2003] viewable in AFNI software (<http://afni.nimh.nih.gov/afni/>). The coordinates of 90 seed locations representing the cortical and subcortical areas from the Automated Anatomical Labeling (AAL) atlas [Tzourio-Mazoyer et al., 2002] were then unwrapped from standard MNI space into each individual headspace.

An event-related minimum variance vector beamformer was used to estimate the broadband time series for each source location and trial for each subject representing the activity of each of the 90 AAL sources. This beamformer technique allows the precise localization of cortical sources and deep brain structures as previously demonstrated by our group using the same n-back task in a sample of healthy adults [Hung et al., 2013; Quraan et al., 2011]. Individual weight vectors were applied to each sensor measurement and summated to give an estimated source activity to each cortical or subcortical AAL seed location [Quraan and Cheyne, 2010].

Beamforming is a spatial filtering approach to MEG inverse source modeling. It relies on a minimization of total brain power, while being optimally sensitive to activity in a given brain location (i.e. each of the 90 seed locations), resulting in the suppression of background noise [Brookes et al., 2011]. Accordingly, beamformers are effective at suppressing ocular artefacts generated by eye movements, and non-ocular artefacts, such as cardiac and muscle activity [Muthukumaraswamy, 2013].

Assessing functional connectivity: Inter-regional phase-locking analysis

We first extracted the instantaneous phase of each sample from a short-time Fourier transform (sliding 200 ms time windows). Then, we performed a functional connec-

tivity analysis between all pairwise combinations of the seeds. This was done by computing the degree of inter-regional phase synchronization for every time (from -200 ms to 600 ms) and frequency (1-60 Hz) point across trials using the phase locking value (PLV). Ranging between 0 and 1, PLV indexes reflect phase synchrony between two sources, which is understood to be a neurophysiological mechanism mediating communication among brain regions referred to as functional connectivity [Fries, 2005].

To study task-dependent connectivity dynamics at the group level, PLVs were averaged across source pairs for each time point and frequency then subsequently averaged across individuals of each group. This produced time series representing source-by-source (90 × 90) adjacency matrices of the global network connectivity dynamics for each group (TD and ASD) at every time (from -200 ms to 600 ms) and frequency (1-60 Hz).

Statistical analysis

Averaged PLV values (mean inter-regional brain synchrony; z-scores) were compared between groups (TD vs. ASD) across time and frequency using a permutation test (3000 permutations; $P < 0.05$) to identify the time windows and frequency bands of interest subsequently submitted to the nonparametric Network Based Statistic (NBS) toolbox (see Supporting Information Fig. S1 for a schematic representation of the statistical analyses).

As illustrated on Figure 1B, we found stronger mean connectivity values (PLV, z-scores $C > ASD$; $P < 0.05$) in TD compared to ASD children from 0 to 150 ms and from 150 to 300 ms in the alpha band (9-15 Hz) and from 350-500 both in the theta (4-8 Hz) and the low gamma (40-50 Hz) bands. Theta (4-8 Hz), alpha, beta (16-30 Hz) and gamma (31-60 Hz) frequency ranges were selected as prior research has indicated they are critical for organizing communication among distributed brain areas in the context of working memory tasks [Brookes et al., 2011; Doesburg et al., 2011; Jensen et al., 2002; Jensen and Tesche, 2002; Palva et al., 2010a].

Adjacency matrices (90 by 90 ROIs) associated with the three time windows and frequency bands of interest [i.e. from 0 to 150 ms and from 150 to 300 ms in the alpha band (9-15 Hz) and from 350 to 500 both in the theta (4-8 Hz) and the gamma (30-60 Hz) bands, see above] were then submitted to a statistical between-group comparison of inter-regional connectivity differences using the non-parametric Network Based Statistic [NBS; Zalesky et al., 2012; Zalesky et al., 2010].

NBS initially performs multiple univariate tests on all analyzed edges [in this case each element in the adjacency matrix; see Maris and Oostenveld, 2007; Nichols and Holmes, 2002 for similar approaches). Using the NBS method, statistical significance is assigned at the level of the connectivity component as a whole, rather than at the level of the individual connections. As different stringencies for initial univariate threshold can yield

differential sensitivities under various scenarios of differential connectivity (for example, small focal changes compared with weak diffuse changes) this threshold must be adapted to the data distribution under investigation [see Zalesky et al., 2012; Zalesky et al., 2010]. Accordingly and as recommended in previous studies [e.g. Bangel et al., 2014; Ye et al., 2014] the initial univariate test thresholds were set to $t \geq 3$ for comparison of ASD participants with TD. This threshold corresponds to a P -value of $P = 0.005$ (2-tailed) according to our sample size ($df = 35$; $t = 3$).

To assess the statistical reliability of differences in network connectivity, connectivity components are first identified, defined as groups on nodes which are contiguously connected by supra-threshold edges/connections. The adjacency matrices are then shuffled between the to-be compared groups and the largest connectivity component in the surrogated data is identified. This process is repeated 10,000 times to produce a null distribution. The sizes of connectivity components identified in the ‘real’ data are then compared with those from the surrogate data to assess the statistical reliability of connectivity differences. Since each component in the surrogate distribution is the largest difference in connectivity that could occur by chance considering each edge/connection in the entire 90×90 adjacency matrix, NBS effectively controls for false positives because of multiple comparisons. This statistical correction is effective for any initial univariate threshold since it is applied equally to obtain component extent for both the real and the surrogate data [Zalesky et al., 2012; Zalesky et al., 2010]. Time series of node strength and eigenvector centrality were calculated from the adjacency matrices using the Brain Connectivity Toolbox [Rubinov and Sporns, 2010] to index the network involvement of particular regions.

Results obtained using NBS and graph theoretical analysis for individual regions were plotted using the Brain Net Viewer toolbox [Xia et al., 2013]. Nodes and edges belonging to statistically significant components were plotted, and the size of each node represents connectivity strength for edges in the significant connectivity component.

Complementary correlation analyses were performed to investigate *a priori* associations between functional connectivity patterns and behavioural parameters. To do so, we computed Pearson correlations ($P < 0.05$ uncorrected) between the main significant connectivity hub difference (the right fusiform) and 3 measures of interest (1) task performance (2-back accuracy), (2) a standardized visuo-spatial WM measure (Block recall subtest of the Working Memory Test Battery for Children), and (3) the severity of the disorder (ADOS) which have shown negative relations between the various functional connectivity measures in different brain networks, such as fronto-motor or fronto-parietal networks [Just et al., 2007; Koshino et al., 2008] but also with hypoactivation of the fusiform area [Schultz, 2005].

Finally, non-parametric analyses (Mann–Whitney U-test for independent samples) examined whether the medica-

TABLE II. Mean behavioral performance to the 2-back task

		Autism (17)	Control (20)	
Mean \pm SD	Acc (%)	59.34 \pm 15	68.17 \pm 16.66	$P = 0.10$
	RTs (sec)	0.66 \pm 0.10	0.61 \pm 0.09	$P = 0.13$
	V (%)	0.39 \pm 0.10	0.39 \pm 0.06	$P = 0.87$

Percentage of correct recognition associated with the repeated (target) picture, Accuracy [Acc], mean reaction times [RT], and RT coefficient of variation [CV] (calculated for each subject as the standard deviation of the mean RT divided by mean RT). SD, standard deviation.

tion taken by some ASD children (9 with vs. 8 without medication) affected the connectivity results. To do so, the node strength values of the primary underconnected hubs (i.e. the left anterior insula (from 0–150 ms) and the right fusiform gyrus (from 150–300 ms); see the results section) were statistically compared between the two subgroups of ASD participants.

RESULTS

Working Memory Behavioral Performance

T-test for independent samples analyses demonstrated only a trend for children with ASD to perform the task less accurately and more slowly than TD children ($ps < 0.14$; see Table II), while variation coefficients (i.e. relative standard deviation) were similar between groups ($P = 0.87$).

No effect of Group ($P > 0.34$) and no interactions were found between the group factors and the standardized subscales scores of the Working Memory Test Battery for Children (subscales of the WMTB-C X Group; $P > 0.41$). However, we found a main effect of subscales of the WMTB-C ($F(4,140) = 8.74$, $P < 0.00001$) suggesting that regardless of the group of children, WM performance differed between subtests, with better performance for Digit Recall and Listening recall than for Backward Digit Recall, Block Recall and Mazes Memory ($ps < 0.012$) which otherwise did not differ from each other ($ps > 0.19$) as demonstrated by LSD Fisher post-hoc analyses.

Brain Synchronization Differences During Working Memory Processing Between Children With ASD and TD Children

Statistical between-groups comparisons revealed atypical alpha-band brain synchronization processes in children with ASD ($ps < 0.04$). Atypical functional connectivity maps in axial and sagittal orientations are shown in Figure 2A,B, with the size of the node scaled to the magnitude of the significant connectivity difference between the groups; significant edges are also marked as interconnecting lines between AAL seed regions.

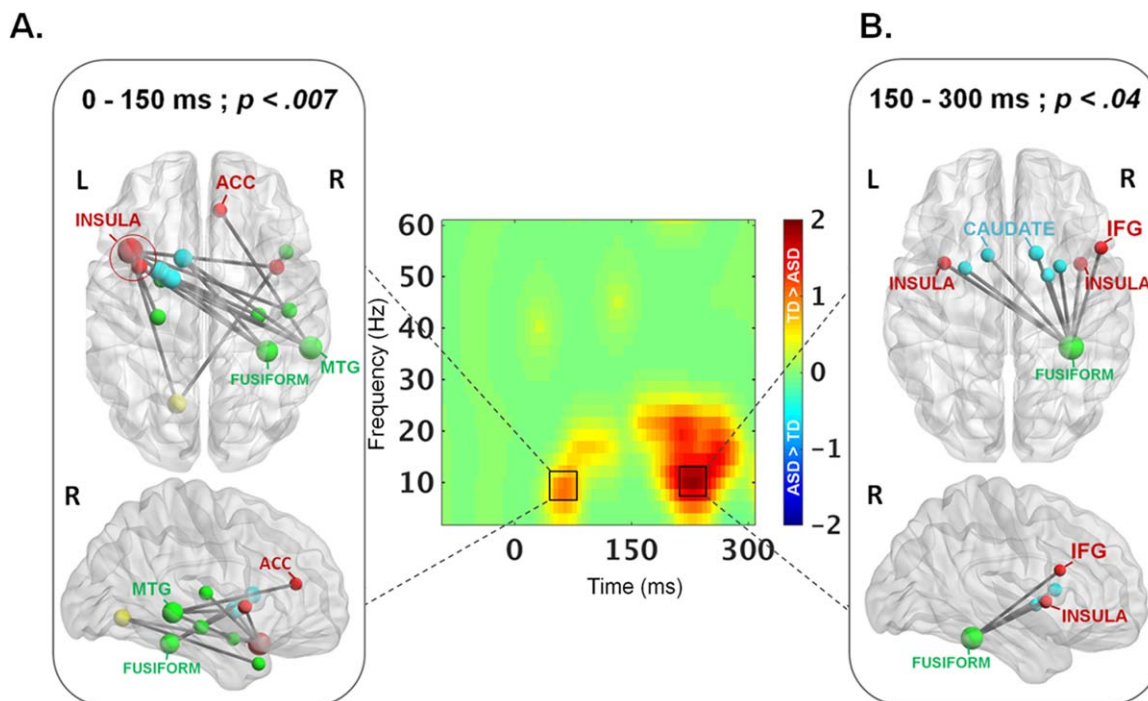


Figure 2.

Reduced WM-related fronto-temporal alpha synchronization in ASD compared to TD children. Statistical between-groups (TD>ASD) differences in the alpha band brain synchronization from (A) 0–150 ms and (B) from 150–300 ms in two fronto-

striato-temporal networks. Nodes are scaled to the magnitude of the significant connectivity difference between the groups (TD>ASD); significant edges are also marked as interconnecting lines between AAL seed regions.

Abnormal oscillatory mechanisms found in ASD encompassed two fronto-striato-temporal networks from 0 to 150 ms and from 150 to 300 ms. Whereas the right fusiform, basal ganglia, and the bilateral insulae were consistently underconnected in children with ASD compared with controls within the first 300 ms, other connections differed more specifically during the first or the second 150 ms time window. In particular, the anterior cingulate cortex (ACC) but also the hippocampi and the left lingual gyrus were underconnected in ASD from 0 to 150 ms ($P < 0.007$) whereas the right inferior frontal gyrus was specifically underconnected from 150 to 300 ms in ASD compared to controls ($P < 0.04$).

Of note, the desynchronization pattern over the fronto-temporal areas observed in ASD compared to TD children occurred in the absence of power differences between the groups (see Supporting Information Figs. S2 and S3), strengthening the finding of a lack of alpha synchronization in children with ASD during WM processes.

Graph theory analyses revealed that the left anterior insula (from 0 to 150 ms) and the right fusiform gyrus (from 150 to 300 ms) were the primary underconnected hubs in ASD compared to TD children according to eigenvector centrality values. Similarly, high-strength node differences were noted in the left anterior insula and the

right middle temporal gyrus from 0 to 150 ms and in the right fusiform gyrus from 0 to 300 ms after stimulus onset.

Complementary analyses investigated if medication taken by some ASD participants (9 with vs. 8 without medication) affected the connectivity results. Non-parametric Mann-Whitney U-test for independent samples did not reveal any differences of node strength values in either primary underconnected hub (i.e. the left anterior insula (from 0 to 150 ms; $P = 1$) or the right fusiform gyrus (from 150 to 300 ms; $P = 0.63$)) between the two subgroups of ASD participants.

Correlations Between Functional Connectivity Measures and Behavioral Measures

Brain-behavior analyses revealed a significant positive correlation between the connectivity index (i.e. node strength) of the right fusiform and behavioral performance (i.e. 2-back accuracy) in TD but not in children with ASD (average $r = +0.49$; $P = 0.02$ in TD children vs. $r = +0.09$; $P = 0.73$ in ASD children, see Fig. 3A). A similar correlation was observed between the right fusiform node strength and performance on the block recall subtest of the Working Memory Test Battery for Children (WMTB-C) in TD but not in children with ASD (average $r = +0.44$;

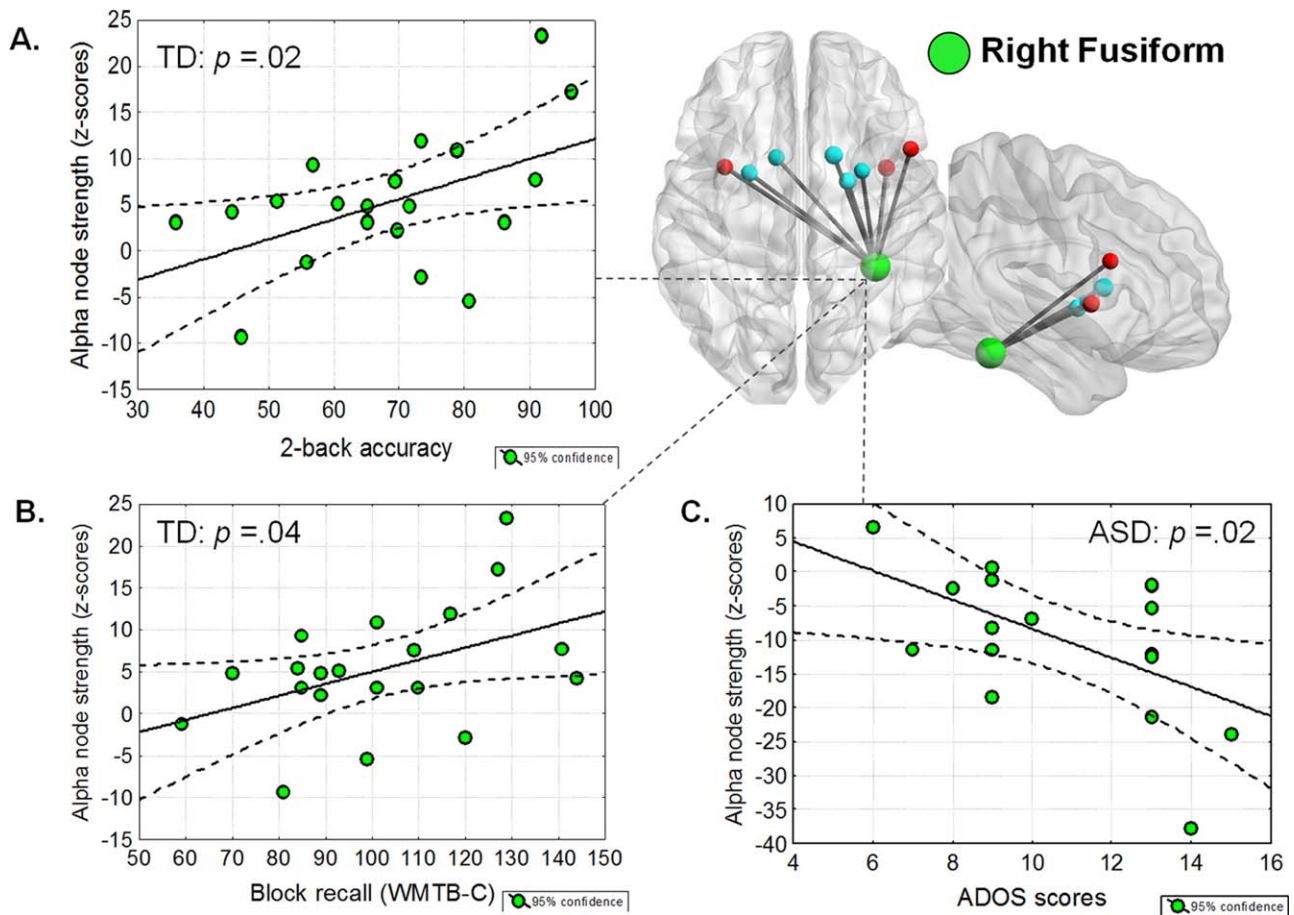


Figure 3.

Correlation analyses. Significant correlation coefficients (all $P < 0.05$) between connectivity processes (alpha node strength; z-scores) related to the right fusiform and WM performance (accuracy) in **(A)** the 2-back task (average $r = +0.49$; $P = 0.02$ in TD children vs. $r = +0.09$; $P = 0.73$ in ASD children and in **(B)** the block recall subtest of the Working Memory Test Bat-

tery for Children (WMTB-C) (average $r = +0.44$; $P = 0.04$ in TD children vs. $r = -0.23$; $P = 0.38$ in ASD children. **C:** Significant correlation coefficient ($P < 0.05$) between connectivity processes (alpha node strength; z-scores) related to the right fusiform and symptoms severity in ASD.

$P = 0.04$ in TD children vs. $r = -0.23$; $P = 0.38$ in ASD children, see Fig. 3B). Finally, we observed a significant negative correlation between the right fusiform node strength during this 2-back task and the severity of autistic symptoms assessed through the ADOS scores (average $r = -0.54$; $P = 0.02$ in ASD children, see Fig. 3C). This last result indicates that the more severe the symptoms in children with ASD, the less right fusiform received connections during this working memory task.

DISCUSSION

Our study found abnormal alpha-band brain synchronization in children with ASD compared to age-, sex- and IQ-matched controls during a 2-back task. Although mod-

ulations of alpha amplitudes have been related to the inhibition of task irrelevant brain areas in the context of WM tasks, mounting evidence suggests that the synchronization of alpha rhythms, which reflect the time-locked firing of inter-regional neuronal processes [Varela et al., 2001], serve core WM processes [Freunberger et al., 2009; Klimesch et al., 2007; Sauseng et al., 2005a]. Hence, an atypical synchronization of alpha rhythms could reflect an inexact timing or dynamic of neural interconnectivity and, thus, result in less efficient WM-related brain mechanisms. In line with this hypothesis, Freunberger et al. [2009] found that, in the context of a WM task, increased alpha phase-locking synchronization processes were associated with the recognition of pictures that participants had to remember whereas pictures that had to be ignored (not-to-remember) were associated with an increase of alpha

amplitude [Freunberger et al., 2009]. Thus, several studies have demonstrated a specific role of alpha synchronization in the top-down control and binding of memory processes [Bauml et al., 2008; Freunberger et al., 2009; Sauseng et al., 2005b; von Stein et al., 2000].

In the present study, atypical alpha synchronization occurred in ASD within the first 300 ms after the repetition of the 2-back trials (that were correctly recognized) in fronto-temporal networks, in particular, between the left anterior insula and the right fusiform, that crucially contribute to WM processes. Long-range fronto-temporal alterations of brain structure and white matter tracts have been consistently reported in the ASD literature [see Ameis and Catani, 2015 for a review]. A recent meta-analysis including voxel-wise structural MRI studies shows a prevalence of alteration within the hippocampi, the fusiform gyri, the cingulate, and the insula in children and adolescents with ASD [Duerden et al., 2012]. In addition, an abnormal structure (i.e. enlargement, reduction or displacement) of the fusiform gyri has been identified in different studies in ASD [Koshino et al., 2008; van Kooten et al., 2008; Waiter et al., 2004], suggesting a possible overlap between structural and functional disruption of connectivity processes related to the fusiform, as well as some structural underpinnings to the atypical WM-related connectivity processes identified in this study.

Graph theory analysis provided evidence of reduced connectivity processes in children with ASD among regions that are especially involved in challenging situations, such as the insula, the ACC and the inferior frontal gyrus (IFG).

These brain areas are involved in the executive control processes required in the context of a WM task [Bunge et al., 2002; Casey et al., 2002; Dove et al., 2000; Scherf et al., 2006] and challenging situations [Barch et al., 1997; Deng et al., 2015; Gehring and Knight, 2000] that involve decision making, response inhibition, error detection, conflict monitoring, problem solving, and performance monitoring [Casey et al., 2000; Huettel et al., 2005; Kim et al., 2014; Thielscher and Pessoa, 2007]. Moreover, the anterior insula is hypothesized to represent a network hub that is critical for switching among brain systems during task performance [Eckert et al., 2009; Sridharan et al., 2008] but also to provide a link between attention-related problem solving and salience systems during the evaluation and the coordination of task performance [Eckert et al., 2009]. In parallel, hypoactivation in these brain regions has been related to the social and emotional difficulties of ASD [Di Martino et al., 2009; Leung et al., 2014], suggesting that the atypical connectivity processes found in these areas in our study might significantly affect the ability of ASD to process more complex WM situations such as real life interactions and, therefore, may contribute to some social deficits observed in autism.

This hypothesis is strengthened by the observation of a positive correlation between atypical connectivity (node strength) pattern in the right fusiform and the severity of

symptoms in ASD. The right fusiform is known to facilitate the encoding and the recognition of visual objects [Haxby et al., 2000] and has been related to an object-based encoding strategy in children [Scherf et al., 2006]. Moreover, increase of activity in the right fusiform is associated with both the manipulation and/or the maintenance of information in a WM task for faces but also is modulated by WM load [Druzgal and D'Esposito, 2001], suggesting its impact on core WM processes.

The central role of the right fusiform in WM processes in our study was further reinforced by the presence of a positive correlation between connectivity in this region and improved behavioural performance in the 2-back task but also in the block recall subtest of the Working Memory Test Battery for Children (WMTB-C) in TD children whereas a similar correlation was not present in children with ASD.

The fact that children with ASD achieved similar behavioural performance as TD controls in our study suggest that ASD performance may rely on a compensatory reorganization of function [Schafer et al., 2009]. However, we did not identify any obvious compensatory mechanisms as, across all frequency bands there was no evidence of any networks that were more synchronized in ASD compared to TD children. Thus, our results suggest that, although atypical WM-related brain processes enable children with ASD to maintain a normal performance in the 2-back task, the desynchronized networks found in our study may not support more challenging WM task conditions such as social interactions in this population.

In summary, this study is the first to demonstrate a desynchronization of alpha rhythms in fronto-temporal networks in children with ASD during a working memory task. Poor brain connectivity encompassed fronto-temporal areas previously associated with the processing of WM and challenging situations but also with social cognition and the regulation of emotion. Furthermore, atypical connectivity processes related to the right fusiform were associated with the severity of symptoms in ASD. Therefore, our results suggest that the atypical connectivity processes observed in the fronto-temporal areas in children with ASD and, in particular, between the left anterior insula and the right fusiform, may contribute to the social cognitive deficits of autism. Finally, this study further strengthened the relevance of investigating neuronal synchronization processes in clinical populations to understand how these oscillatory codes are disrupted in pathophysiological conditions associated with neurodevelopmental disorders.

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