

The Obese Brain: Association of Body Mass Index and Insulin Sensitivity with Resting State Network Functional Connectivity

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Abstract: Obesity is a key risk factor for the development of insulin resistance, Type 2 diabetes and associated diseases; thus, it has become a major public health concern. In this context, a detailed understanding of brain networks regulating food intake, including hormonal modulation, is crucial. At present, little is known about potential alterations of cerebral networks regulating ingestive behavior. We used “resting state” functional magnetic resonance imaging to investigate the functional connectivity integrity of resting state networks (RSNs) related to food intake in lean and obese subjects using independent component analysis. Our results showed altered functional connectivity strength in obese compared to lean subjects in the default mode network (DMN) and temporal lobe network. In the DMN, obese subjects showed in the precuneus bilaterally increased and in the right anterior cingulate decreased functional connectivity strength. Furthermore, in the temporal lobe network, obese subjects showed decreased functional connectivity strength in the left insular cortex. The functional connectivity magnitude significantly correlated with body mass index (BMI). Two further RSNs, including brain regions associated with food and reward processing, did not show BMI, but insulin associated functional connectivity strength. Here, the left orbitofrontal cortex and right putamen functional connectivity strength was positively correlated with fasting insulin levels and negatively correlated with insulin sensitivity index. Taken together, these results complement and expand previous functional neuroimaging findings by demonstrating that obesity and insulin levels influence brain function during rest in networks supporting reward and food regulation. *Hum Brain Mapp* 33:1052–1061, 2012. © 2011 Wiley Periodicals, Inc.

Key words: independent component analysis (ICA); obesity; fMRI; insulin; food; reward



Additional Supporting Information may be found in the online version of this article.

Contract grant sponsor: “Kompetenznetz Adipositas” (Competence Network for Adiposity) German Federal Ministry of Education and Research (BMBF); Contract grant number: FKZ: 01GI0837 and 01GI0849; Contract grant sponsor: The German Center for Diabetes Research (DZD e.V.); Contract grant sponsor: Deutsche Forschungsgemeinschaft; Contract grant number: Fr 1561/3-3, Fr 1561/4-1 and Bi 195/62-1.

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Received for publication 14 September 2010; Revised 21 December 2010; Accepted 28 December 2010

DOI: 10.1002/hbm.21268

Published online 21 April 2011 in Wiley Online Library (wileyonlinelibrary.com).

INTRODUCTION

According to the World Health Organization, there are currently over 1.6 billion overweight and at least 400 million obese individuals worldwide (WHO 2010). Obesity is tightly linked to insulin resistance and is one of the major factors leading to chronic diseases like Type 2 diabetes. In this respect, obesity is associated with increased risk for numerous health conditions and heightened mortality [Flegal et al., 2002; Flegal et al. 2005].

Obesity is generated by an energy imbalance and associated with excessive food intake. Eating behavior itself is modulated by physiological, psychological, and cognitive factors. This clearly indicates that a basal brain control circuit like the hypothalamus, the major homeostatic control center, alone is not sufficient to explain eating behavior and weight control in general. Several brain imaging studies, investigating food related processing, discovered that obese individuals show altered brain activity in the gustatory and somatosensory regions, as well as reward related areas [Del Parigi et al., 2002; Del Parigi et al., 2005; Gautier et al., 2000; Gautier et al., 2001; Karhunen et al., 1997; Matsuda et al., 1999; Stice et al., 2008; Stice et al., 2009]. For instance, cortical areas associated with hunger and satiation are differentially activated in obese compared with lean individuals, which include the prefrontal cortex, hypothalamus, thalamus, several limbic/paralimbic areas, basal ganglia, temporal cortex, and the cerebellum [Del Parigi et al., 2002; Del Parigi et al., 2005; Gautier et al., 2000; Gautier et al., 2001; Karhunen et al., 1997; Matsuda et al., 1999]. Furthermore, brain regions related to motivational effects of food cues, especially the striatum, showed significantly reduced dopamine D2 receptor availability in obese individuals [Wang et al., 2001] and exhibited greater activation to high caloric food stimuli [Rothmund et al., 2007; Stoeckel et al., 2008], but less activation in response to food consumption in obese individuals [Stice et al., 2008]. Furthermore, hormonal signals, like insulin, act in the CNS as regulators of energy homeostasis through its receptors, expressed in the limbic forebrain [Marks et al., 1991; Unger et al., 1991]. Hereby it has been found in animal studies that insulin decreases the rewarding aspect of food through the “motivational circuitry,” such as by decreasing dopamine signaling [Figlewicz et al., 1994; Patterson et al., 1998]. Interestingly, in a recent magnetoencephalographic study we found that increasing insulin levels did not lead to increased neuronal activity in obese individuals in contrast to lean individuals. We called this effect cerebral insulin resistance [Tschrutter et al., 2006]. This cerebral insulin resistance is also associated with peripheral insulin resistance [Tschrutter et al., 2006; Tschrutter et al., 2007a]. Further factors that relate to insulin resistance of the brain include elevated serum free fatty acid levels [Tschrutter et al., 2009b], aging [Hennige et al., 2006; Tschrutter et al., 2009a] and genetic background [Tschrutter et al., 2007b].

However, no studies, so far, have evaluated the relationship between obesity and intrinsic brain function involved in the regulation of food and reward processing. We applied “resting state” functional magnetic resonance imaging (fMRI) to assess brain function in lean compared with obese subjects. By means of independent component analysis (ICA), we identified several temporally synchronous brain networks or “modes,” which are present in healthy subjects during rest to examine functional connectivity (FC) within these networks [Beckmann et al., 2005; Damoiseaux et al., 2006; De Luca et al., 2006]. We focused on five resting state networks (RSNs) that involve brain areas previously implicated in food and reward processing. Furthermore, these brain areas were observed to be differentially activated in obese compared with lean individuals [Del Parigi et al., 2002; Del Parigi et al., 2005; Gautier et al., 2000; Gautier et al., 2001; Karhunen et al., 1997; Matsuda et al., 1999; Stice et al., 2008; Stice et al., 2009]. The default mode network (DMN), includes regions which are active when subjects are in an awake, resting phase without any task, but whose activity diminishes during specific goal-directed behaviors [Raichle et al., 2001]. The DMN includes the precuneus, posterior cingulate, medial prefrontal, and inferior parietal cortices [Correa et al., 2007]. There has been evidence implicating changes in parietal and cingulate regions in obese individuals [Rothmund et al., 2007; Volkow et al., 2009; Wang et al., 2002]. A second network, termed temporal lobe network, includes the primary and secondary auditory cortices and the insular cortex, which is part of the primary gustatory cortex [Beckmann et al., 2005; Damoiseaux et al., 2006]. A third network, termed basal ganglia network [Robinson et al., 2009], includes subcortical structures that are also involved in food and reward processing. A fourth network, termed prefrontal lobe network, includes the dorsolateral and ventrolateral prefrontal, orbitofrontal (OFC), and frontopolar prefrontal cortex. The prefrontal cortex is involved in inhibitory processes, like termination of feeding [Del Parigi et al., 2002]. A fifth network, termed motor sensory network, includes precentral and postcentral gyri [Beckmann et al., 2005; Damoiseaux et al., 2006; De Luca et al., 2006]. A Positron Emission Tomography (PET) study found that obese relative to lean adults showed greater resting metabolic activity in the oral somatosensory cortex, a region that encodes sensation in the mouth, lips, and tongue [Wang et al., 2002]. Extending these findings, an fMRI study found that obese versus lean adolescents showed greater activation in the oral somatosensory cortex in response to the anticipated intake of chocolate milkshake [Stice et al., 2008].

We hypothesized that obese subjects would show: (i) altered RSN connectivity, especially in brain regions known to be important in food and reward regulation; and (ii) that these alterations would be associated with body mass index (BMI), fasting insulin levels and insulin sensitivity index, which are directly correlated with obesity [Stephan et al., 1972; Woods et al., 1985].

TABLE I. Subjects' characteristics in lean vs. obese group

	Lean group	Obese group	<i>P</i>
Gender (female/male)	6/5	6/6	–
Age (years)	23.5 ± 2.1	24.7 ± 2.4	0.08
BMI (kg/m ²)	20.9 ± 1.1	30.5 ± 1.8	<0.001
Fasting glucose (mmol/l)	4.94 ± 0.34	4.96 ± 0.41	0.9
Fasting insulin (pmol/l)	37 ± 15	77 ± 33	0.0014
OGTT-derived insulin sensitivity index (AU)	19.0 ± 7.1	11.5 ± 7.0	0.0067
POMS-scale: Depression (%)	0.82 ± 1.45	2.84 ± 5.31	0.236
POMS-scale: Fatigue (%)	21.53 ± 10.6	18.15 ± 14.1	0.526
POMS-scale: Anger (%)	1.40 ± 1.8	3.76 ± 7.3	0.307
POMS-scale: Vigor (%)	32.79 ± 17.29	42.33 ± 15.9	0.183

Data are presented as mean ± SD. *P* = *P*-values for comparison of unadjusted log_e-transformed data by ANOVA. POMS = Profile of Mood States.

MATERIALS AND METHODS

Subjects

Eleven lean (six women, BMI range 19.4–22.5 kg/m², and age range 22–29 years) and 12 overweight or obese subjects (six women, BMI range 28.4–34.4 kg/m², and age range 21–28 years) were recruited. Lean subjects were required to have a BMI from 18.5 to 24.0. Overweight and obese subjects were required to have a BMI >25. The overweight and obese subjects collectively will be referred to as “obese.” All subjects were healthy as ascertained by a physician; they did not suffer from psychiatric, neurological, or metabolic diseases. Any volunteer treated for chronic disease or taking any kind of medication other than oral contraceptives was excluded at screening. Impaired glucose metabolism was ruled out by standard 75 g oral glucose tolerance test (OGTT). All subjects were normal sighted or had corrected-to-normal vision. Informed written consent was obtained from all subjects and the local Ethics Committee approved the protocol. The demographic characteristics of the subjects are shown in Table I.

Study Design

After an overnight fast of at least 10 h, subjects completed two resting state functional imaging scanning visits separated on average by 4 weeks. To minimize circadian influence, subjects were scanned between 7 and 8 am. Before the experiment, subjects confirmed their fasting state. In addition, blood glucose and plasma insulin levels before each experiment were within the fasting range for all subjects. Before the experiment, subjects filled out a short German version of the “Profile of Mood States” (POMS; [McNair et al., 1981]), which is a 35 item questionnaire evaluate depression, fatigue, anger, and vigor (Table I). There was no statistical significant difference in mood states assessed by POMS between lean and obese subjects.

Data Acquisition

Whole-brain functional magnetic resonance imaging (fMRI) data was obtained by using a 3.0 T scanner (Siemens Tim Trio, Erlangen, Germany). Functional data were collected by using echo-planar imaging sequence: TR = 1.8s, TE = 30ms, FOV = 210 mm², matrix 64 × 64, flip angle 90°, voxel size 3 × 3 × 4 mm³, slice thickness 3 mm, 1 mm gap and the images were acquired in ascending order. Each brain volume comprised 28 axial slices and each functional run contained 160 image volumes, resulting in a total scan time of 4.52 min. In addition, high-resolution T1 weighted anatomical images (MPRage: 176 slices, matrix: 256 × 224, 1 × 1 × 1 mm³) of the brain were obtained. All subjects were instructed not to focus their thoughts on anything in particular and to keep their eyes closed during the resting state MR acquisition.

Data Preprocessing

Functional image preprocessing and statistical analysis were carried out by using SPM5 (Wellcome Trust Centre for Neuroimaging, London, UK). Images were realigned to the first image. Unwarping of geometrically distorted EPIs was performed using the FieldMap Toolbox available for SPM5 to account for susceptibility by movement artifacts. A mean image was created and coregistered to the T1 structural image. The anatomical image was normalized to the Montreal Neurological Institute (MNI) template, and the resulting parameter file was used to normalize the functional images (voxel size: 3 × 3 × 3 mm³). Finally, the normalized images were smoothed with a three-dimensional isotropic Gaussian kernel (FWHM: 10 mm). fMRI Data were high-pass [cut off period 128 s] and low-pass filtered (autoregression model AR(1)).

Independent Component Analysis (ICA)

Group spatial ICA [Calhoun et al., 2001] was used to decompose the smoothed, normalized fMRI images into

35 components using the GIFT software (<http://icatb.sourceforge.net/>) as follows. Dimension estimation, to determine the number of components, was performed using the minimum description length criteria, modified to account for spatial correlation [Li et al., 2007]. Data from all subjects were then concatenated and this aggregate data set reduced to 35 temporal dimensions using Principal Component Analysis, followed by an independent component estimation using infomax algorithm [Bell and Sejnowski, 1995].

Component Selection

For each subject, spatial maps were reconstructed and converted to z values. A two step process was used to select the components that most closely matched the default mode, temporal lobe, basal ganglia, prefrontal lobe, and motor sensory network. First, because functional connectivity networks have been detected in low-frequency ranges [Cordes et al., 2001], a frequency filter was applied to remove any components in which high-frequency signal (>0.1 Hz) constituted 50% or more of the total power in the Fourier spectrum. Next, the remaining low-frequency components were spatially sorted in GIFT using masks derived from the wake forest university pick atlas (<http://www.fmri.wfubmc.edu/download.htm>) to identify the DMN, temporal lobe, basal ganglia, prefrontal lobe, and motor sensory network components. For the DMN mask we used precuneus, posterior cingulate, and Brodmann area (BA) 7, 10, and 39 [Correa et al., 2007], for the temporal lobe network mask we used the bilateral insular cortices, for the basal ganglia network we used bilaterally the pallidum, putamen, substantia nigra, subthalamic nucleus, and thalamus [Robinson et al., 2009], for the prefrontal lobe network mask we used BA 8, 9, 10, 11, 44, 45, 46, and 47 and for the motor sensory network mask we used BA 1,2,3, and 4. A spatial correlation of the masks with each of the components was performed and the component that had the best fit with each of the five masks was automatically selected for further analysis (Supporting Information Fig. 1). For each component, we created a sample-specific component group map of all 23 subjects. These maps were used as a binary mask for statistical analyses within the corresponding component.

Statistical Analysis

Group comparison

The z values of the spatial maps represent the fit of a specific voxel BOLD timecourse to the group averaged component's timecourse. Hence, group analyses test the connectivity strength (i.e., signal synchronization) of each voxel to the whole spatial component. For group analyses, spatial maps of the DMN, temporal lobe, basal ganglia, prefrontal lobe, and motor sensory network were entered into SPM5 since the GIFT toolbox only allows one- or two-

sample t -tests. For each component, a full factorial model (Factors: BMI, gender, and visits) was used to examine group differences. The factor "visit" was included to correct for repeated measurement. The resulting statistical maps were masked with the component-specific group map to explore results within this network only. All group tests were thresholded at $P < 0.05$, family-wise error corrected (FWE).

Correlation of Component Maps with Anthropometric and Metabolic Parameters

For each of the five components, a multiple regression analysis was performed, in SPM5, using fasting insulin levels and insulin sensitivity index as covariates to quantify the association between network related functional connectivity and insulin levels. Non-normally distributed variables were logarithmically transformed. Again the resulting statistical maps were masked with the component-specific group map to explore results within this network only. All group tests were thresholded at $P < 0.05$ (FWE).

Since BMI, fasting insulin and insulin sensitivity index are highly related, further statistical analysis was applied to differentiate between BMI and insulin related effects (i.e., r^2 adjusted for BMI or fasting insulin). For this purpose the following procedure was used. Z values of individual GIFT maps were extracted for each peak voxel that showed significant group differences (Full factorial model, SPM5) or significant correlation with fasting insulin or insulin sensitivity index (Multiple Regression, SPM5). To determine BMI or insulin adjusted r^2 , correlations for the extracted z values were calculated by using least-squares regression analysis in JMP. P value of <0.05 was considered statistical significant (JMP Version 8.0.2, SAS Institute, Cary, NC). For a summary sketch for the functional data analysis, see Figure 1.

Blood Sampling and Analysis

Blood glucose was measured by a HemoCue blood glucose photometer using the glucose dehydrogenase method (HemoCueAB, Aengelholm, Sweden). Plasma insulin levels were determined with commercial chemiluminescence assays for ADVIA Centaur (Siemens Medical Solutions, Fernwald, Germany). In addition, all subjects underwent a standard 75g OGTT with determination of glucose and insulin every 30 min from which insulin sensitivity index was calculated as proposed by Matsuda and DeFronzo [Matsuda and DeFronzo, 1999].

Voxel Based Morphometry

The T1 weighted images were processed and examined using the VBM8 toolbox with default parameters (<http://dbm.neuro.uni-jena.de/vbm.html>) implemented in the SPM8 software (Wellcome Department of Imaging Neuroscience Group, London, UK; <http://www.fil.ion.ucl.ac.uk/spm>). Images were bias corrected, tissue classified

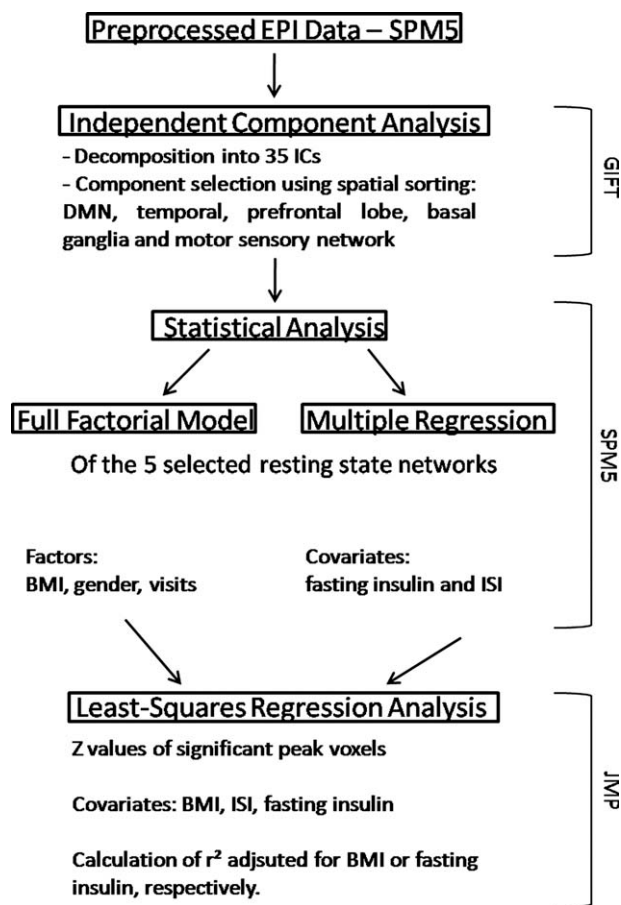


Figure 1.

Data analysis overview. Summary sketch of the data analysis steps. Displayed on the right are the applied software packages. Abbreviations: ICs-Independent Components, BMI-body mass index, ISI-insulin sensitivity index.

and registered using linear and nonlinear transformations, within a unified model [Ashburner and Friston, 2005]. Gray matter (GM) segments were multiplied by the nonlinear components derived from the normalization matrix to preserve actual GM values locally (modulated GM volumes) and not multiplied by the linear components of the registration to account for individual differences in brain orientation, alignment, and size globally. Finally, the modulated volumes were smoothed with a Gaussian kernel of 10 mm full width at half maximum (FWHM).

Voxel-wise GM differences between lean and obese subjects were examined by means of a two-sample *t*-test using age and gender as confounding covariates, which means that the effect of age and gender were removed from the data. To avoid possible edge effects between tissue types, we excluded all voxels with GM values of less than 0.1 (absolute threshold masking). Results were thresholded at $P < 0.05$ (FWE).

RESULTS

Component Identification

By means of Independent Component Analysis (ICA), 35 independent components (ICs) were extracted for the obese as well as for the lean group. Fourteen potentially functional relevant components were extracted for both groups. These components correspond to previously described RSNs, consisting of regions that are involved in working memory, the DMN, motor function, visual and auditory processing, and executive function [Beckmann et al., 2005; Damoiseaux et al., 2006; De Luca et al., 2006]. We additionally found a spatial pattern resembling the basal ganglia network, including the thalamus and supplementary motor areas [Damoiseaux et al., 2008; Di Martino et al., 2008; Robinson et al., 2009]. The 14 functionally relevant components were spatially sorted in GIFT (spatial correlation) using anatomical masks to identify the default mode, temporal lobe, basal ganglia, prefrontal lobe and motor sensory network components ($r = 0.46, 0.34, 0.62, 0.28, \text{ and } 0.30$ respectively) (Supporting Information Fig. 1).

Group Comparison

We analyzed between group differences in corresponding RSNs, using a full factorial model (BMI, gender, visits), of the identified DMN, temporal lobe, basal ganglia, prefrontal lobe and motor sensory network contrasting the individual, back-reconstructed IC patterns. No main effect for gender was observed in the five RSNs. A significant main effect for BMI was observed in the DMN and temporal lobe network ($P < 0.05$, FWE). The precuneus/posterior cingulate cortex (PCC) (BA 7/23) showed increased FC strength bilaterally, whereas the right anterior cingulate cortex (ACC) (BA24) demonstrated reduced FC strength in the DMN in the obese group (Fig. 2 and Supporting Information Table I). The left insular cortex (BA13) revealed reduced FC strength in the temporal lobe network in the obese group (Fig. 3 and Supporting Information Table II). No group differences were observed in the prefrontal lobe, basal ganglia and motor sensory network component.

Correlation of RSN Maps with BMI, Fasting Insulin and Insulin Sensitivity Index

The multiple regression analysis (SPM5) revealed insulin associated functional connectivity in the prefrontal lobe and basal ganglia network ($P < 0.05$, FWE). No relationship was observed between insulin and the DMN, temporal lobe or motor sensory network. As expected, BMI, plasma insulin and insulin sensitivity index were highly correlated within this sample (BMI and insulin: $P = 0.01, r^2 = 0.28$; BMI and insulin sensitivity index: $P = 0.005, r^2 = 0.33$; insulin and Insulin sensitivity index: $P < 0.0001, r^2 = 0.69$).

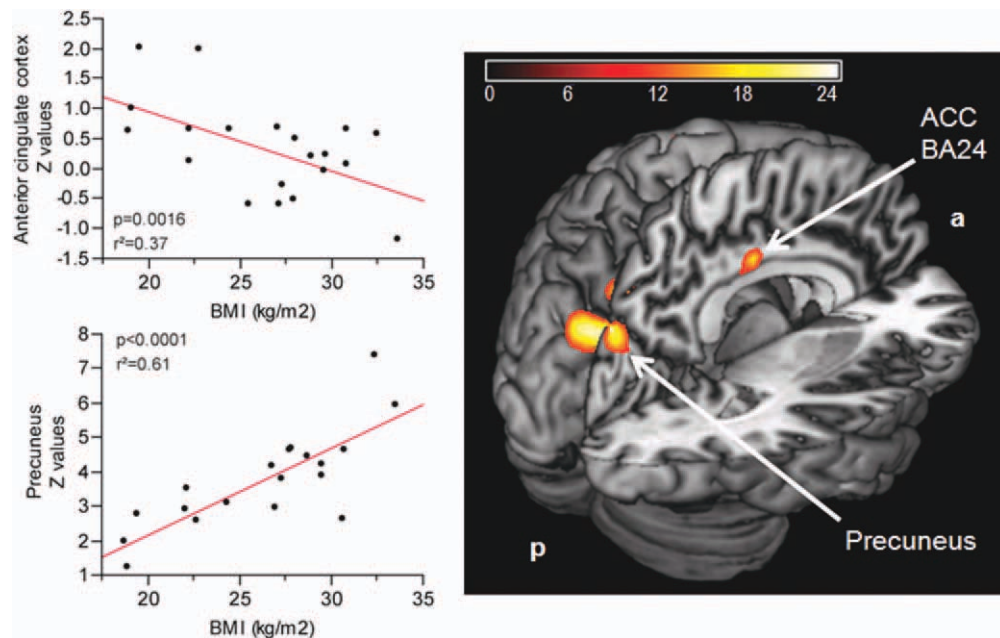


Figure 2.

Contrast of DMN between lean and obese subjects. Color map represents significant ($P < 0.05$, FWE) voxels of altered functional connectivity in obese compared to lean subjects. Color bar represents F-values. The top scatter plot shows significant negative correlation between the right anterior cingu-

late cortex (BA24) ($x = 3, y = -12, z = 36$) and BMI, adjusted for fasting insulin levels. The bottom scatter plot shows significant positive correlation between the left precuneus ($x = -3, y = -78, z = 33$) and BMI, adjusted for fasting insulin levels.

Default mode network. A significant positive correlation was found between the left precuneus ($x = -3/y = -78/z = 33$) FC strength and BMI adjusted for fasting insulin ($P < 0.0001, r^2_{\text{adjusted}} = 0.61$) (see Fig. 2), as well as a negative correlation was found between the right ACC ($x = 3/y = -12/z = 36$) functional connectivity and BMI adjusted for fasting insulin ($P = 0.0016, r^2_{\text{adjusted}} = 0.37$) (see Fig. 2).

insulin sensitivity index adjusted for BMI ($P < 0.0001, r^2_{\text{adjusted}} = 0.65$) (see Fig. 5).

Motor sensory network. No correlations were found with fasting insulin and ISI

Temporal lobe network. A significant negative correlation was found between left insular cortex ($x = -42/y = -6/z = 0$) FC strength and BMI adjusted for fasting insulin ($P = 0.0006, r^2_{\text{adjusted}} = 0.43$) (see Fig. 3).

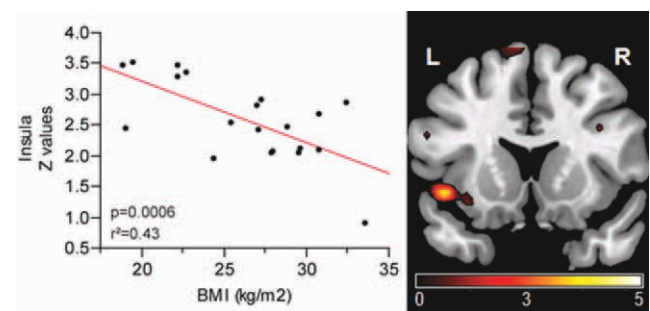


Figure 3.

Contrast of temporal lobe network between lean and obese subjects. Color map represents significant ($P < 0.05$, FWE) voxels of decreased functional connectivity in obese compared to lean subjects. Color bar represents T-values. Scatter plot shows significant negative correlation between the left insular cortex ($x = -42, y = -6, z = 0$) and BMI, adjusted for fasting insulin levels.

Prefrontal lobe network. A significant positive correlation was revealed between left orbitofrontal cortex ($x = -30/y = 45/z = -12$) FC strength and fasting insulin adjusted for BMI ($P = 0.015, r^2_{\text{adjusted}} = 0.22$) (see Fig. 4); a negative correlation was revealed between the left orbitofrontal cortex FC strength and insulin sensitivity index adjusted for BMI ($P = 0.0012, r^2_{\text{adjusted}} = 0.39$) (see Fig. 4).

Basal ganglia network. A significant positive correlation was revealed between right putamen ($x = 33/y = 0/z = -9$) FC strength and fasting insulin adjusted for BMI ($P = 0.009, r^2_{\text{adjusted}} = 0.26$) (see Fig. 5); a negative correlation was revealed between the right putamen FC strength and

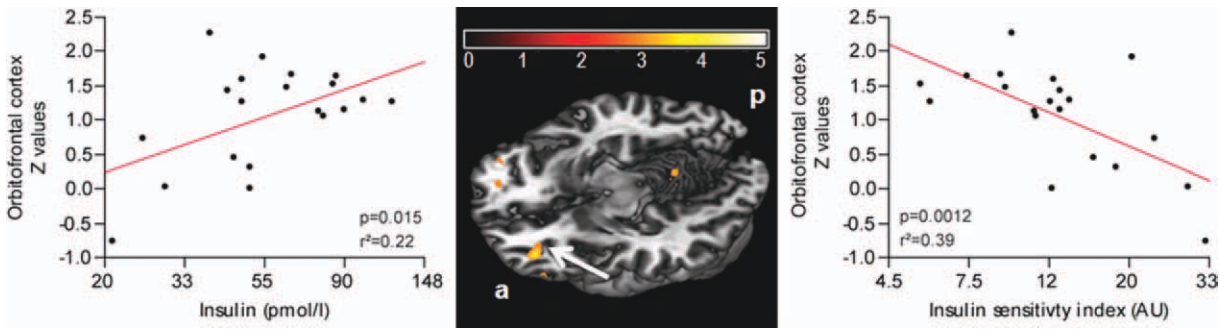


Figure 4.

Relationship between prefrontal lobe network functional connectivity and fasting insulin levels (\log_e -scaled) and insulin sensitivity index (\log_e -scaled) in lean and obese subjects. Color map represents significant ($P < 0.05$, FWE) voxels of insulin associated connectivity. Color bar represents T -values. The left scatter plot

shows a significant positive correlation between the left orbitofrontal cortex ($x = -30, y = 45, z = -12$) and fasting insulin, adjusted for BMI. The right scatter plot shows a significant negative correlation between left orbitofrontal cortex and insulin sensitivity index, adjusted for BMI.

Structural differences between lean and obese subjects

To assess possible causes of altered functional connectivity, we analyzed our data for structural differences between both groups. The voxel-wise analysis revealed no significant GM differences at a threshold of $P < 0.05$ (FWE).

DISCUSSION

The aims of the study were to explore the effects of obesity on the integrity of FC within the DMN, temporal lobe, basal ganglia, prefrontal lobe, and motor sensory network using resting state fMRI and investigate whether a relationship exists between FC strength and BMI, fasting insulin levels and insulin sensitivity of the subjects. We

provide evidence that obese individuals differ substantially during rest in brain networks related to reward and food regulation compared with lean subjects.

Direct group comparison showed altered FC strength in the DMN and temporal lobe network in obese subjects. Regions of the affected RSNs did not differ significantly in volumetric aspects between the two groups, confirming the functional nature of the observed alterations. In the DMN, the PCC/precuneus expressed increased FC strength, whereas the ACC (BA24) expressed decreased FC strength in obese subjects. The PCC, part of the associative cortex, is involved in a wide range of higher order cognitive functions and is highly connected to higher cortical areas, including the prefrontal cortex [Cavanna and Trimble, 2006]. The ACC, on the other hand, is linked

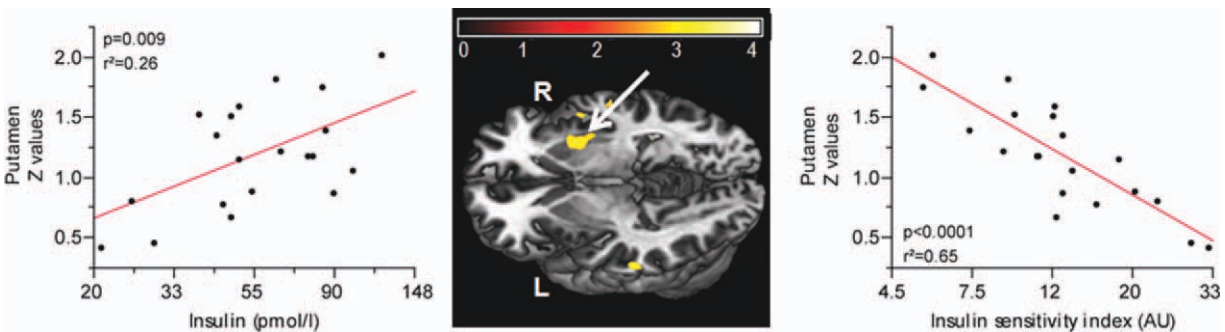


Figure 5.

Relationship between basal ganglia network functional connectivity and fasting Insulin levels (\log_e -scaled) and insulin sensitivity index (\log_e -scaled) in lean and obese subjects. Color map represents significant ($P < 0.05$, FWE) voxels of insulin associated activity. Color bar represents T -values. The left scatter plot

shows a significant positive correlation between the right putamen ($x = 33, y = 0, z = -9$) and fasting insulin, adjusted for BMI. The right scatter plot shows a significant negative correlation between the right putamen and insulin sensitivity index, adjusted for BMI.

primarily to paralimbic and subcortical regions associated with affective and autonomic processes including OFC, nucleus accumbens and hypothalamus [Aharon et al., 2001; Damasio et al., 2000]. Recent evidence suggests that the PCC as well as the ACC activity can be influenced by BMI. PET studies revealed that the precuneus is associated with an enhanced metabolic activity during rest in obese individuals [Wang et al., 2002] and that baseline brain glucose metabolism in prefrontal regions and ACC is negatively correlated with BMI [Volkow et al., 2009]. A functional connectivity study demonstrated that ACC and PCC functional connectivity patterns show common regions implicated in the integration of cognitive and emotional stimuli [Greicius et al., 2003]. Thus, it has been postulated that functional connections between PCC and ACC form a critical link between higher cortical processing and basic processing necessary for calibrating affective and autonomic states [Greicius et al., 2003]. An intriguing speculation, based on our findings and previous results, is that an altered integration between PCC and ACC can contribute to an increased risk to overeat through an imbalance between cognitive and emotional processing. Using ICA, we were able to demonstrate that obese individuals show altered functional connectivity in the PCC and ACC within the DMN. The PCC was positively correlated with BMI, while the ACC (BA24) was negatively correlated with BMI. Nevertheless, additional investigations are needed to exemplify whether these changes are only within the DMN or if there is actually a change in functional connectivity between the PCC and ACC.

In the temporal lobe network, the insular cortex showed decreased FC strength in obese subjects. The insular cortex is considered to be the primary gustatory cortex [Kringelbach et al., 2004], representing an important relay of the neural circuitry connecting the hypothalamus, OFC, and the limbic system [Tataranni et al., 1999]. These areas, including the striatum, comprise the central orexigenic network, which is essential for regulating food intake. Although hunger has been associated with an increase in regional cerebral blood flow (rCBF), satiation has been associated with a decrease in rCBF in the insular cortex, suggesting that the insular cortex is affected by the state of hunger. However, this rCBF decrease was significantly greater in obese individuals [Gautier et al., 2000; Gautier et al., 2001]. Therefore, it has been proposed that obese individuals interpret the state of hunger as more threatening, which is additionally supported by our finding showing that FC strength in the insular cortex after an overnight fast was decreased in proportion to the BMI. Since the insular cortex is part of the central orexigenic network, it is tempting to speculate that overeating may compensate decreased FC strength in the orexigenic network. Interestingly, we did not find altered functional connectivity in the prefrontal lobe, basal ganglia, and motor sensory network in obese compared with lean individuals.

To understand the pathophysiology of excessive food intake in humans, it is crucial to further include hormonal

modulation of eating behavior. Insulin is a prime candidate for feedback mechanisms to downregulate appetite and terminate food intake, as it acutely responds to food intake with a profound and transient increase [Marks et al., 1991; Unger et al., 1991; Zhao and Alkon, 2001]. Additionally, insulin crosses the blood-brain barrier and binds to its widely expressed receptors in the brain [Marks et al., 1991; Unger et al., 1991]. Several studies have illustrated a negative relationship between changes in insulin and rCBF in the OFC and striatum following a meal [Del Parigi et al., 2002; Tataranni et al., 1999]. Moreover, animal studies have shown that insulin decreases the rewarding aspect of food, such as by decreasing dopamine signaling [Figlewicz et al., 1994; Patterson et al., 1998]. The aforementioned findings insinuate that an increase in insulin reduces the rewarding effect of food. Concurrently, our results revealed specific brain areas within the reward system that are sensitive to insulin. The correlation pattern indicates that subjects with higher fasting insulin levels were associated with stronger orbitofrontal and putamen functional connectivity independent of BMI. This implies that higher fasting insulin levels, which are correlated with lower insulin sensitivity indices, are associated with increased FC strength in reward related areas. Assuming that the enhanced FC of the reward system to elevated fasting insulin levels are an "over-activation" of the reward related areas, further increased postprandial insulin levels would not be able to elicit an appropriate reward response to food intake.

Nevertheless, further studies are needed to elucidate the effect of insulin on the reward system

In conclusion, our findings suggest that obesity and insulin levels have substantial influence on brain function during rest in networks supporting reward and food regulation. We report BMI- and insulin-associated FC strength within four RSNs. With an increasing number of individuals becoming obese, a detailed understanding of brain networks supporting food intake is vital. A unique advantage provided by the method we used (resting state fMRI) is that it allows one to examine task-independent network functional connectivity. The absence of a task gets rid of issues as performance differences among groups and practice effects. The enhanced spatial resolution and reliance on endogenous signal rather than radionuclide tracers also make this approach preferable to PET. Increasing evidence suggests that intrinsic brain FC is important for healthy brain function. Changes in intrinsic brain FC have previously been related to several different medical conditions, such as Alzheimer's disease [Greicius et al., 2004], depression [Greicius et al., 2007], schizophrenia [Zhou et al., 2007], and autism [Di Martino et al., 2009]. Our data suggest that the analysis of intrinsic brain FC may enlarge the understanding of obesity and RSN connectivity may be a useful biological marker and treatment target for obesity.

We want to acknowledge some limitations of the this study. First, the number of subjects investigated was rather small; a larger sample size could improve the significance

of the this study. Second, obesity has been associated with reduced cognitive abilities especially in elderly. However, we did not perform any cognitive tests.

ACKNOWLEDGMENTS

The authors thank Maike Borutta and Anna Bury for excellent technical assistant.

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