



# The Oral Administration of Lidocaine HCl Biodegradable Microspheres: Formulation and Optimization

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Bushra T ALQuadeib   
Eram KD Eltahir   
Modhi F Alagili

Department of Pharmaceutics, College of  
Pharmacy, King Saud University, Riyadh  
11671, Saudi Arabia

**Purpose:** Lidocaine (LID) is a local anesthetic that is administered either by injection and/or a topical/transdermal route. However, there is a current need to develop efficacious methods for the oral delivery of LID with optimized bioavailability.

**Methods:** We developed oral LID biodegradable microspheres that were loaded with alginate-chitosan with different mass ratios, and characterized these microspheres in vitro. We also developed, and utilized, a simple and sensitive HPLC-tandem mass spectrometry (LC-MS-MS) method for assaying LID microspheres.

**Results:** The mean particle size (MPS) of the LID microspheres ranged from 340.7 to 528.3 nm. As the concentration of alginate was reduced, there was a significant reduction in MPS. However, there was no significant change in drug entrapment efficiency (DEE), or drug yield, when the alginate concentration was either increased or decreased. DSC measurements demonstrated the successful loading of LID to the new formulations. After a slow initial release, less than 10% of the LID was released in vitro within 4 h at pH 1.2. In order to evaluate nephrotoxicity, we carried out MTT assays of LID in two types of cell line (LLC-PK1 and MDCK). LID significantly suppressed the cell toxicity of both cell lines at the concentrations tested (100, 200, and 400ng/μL).

**Conclusion:** Experiments involving the oral delivery of LID formulations showed a significant reduction in particle size and an improvement in dissolution rate. The formulations of LID developed exhibit significantly less toxicity than LID alone.

**Keywords:** lidocaine, oral delivery, alginate-chitosan microspheres, in vitro characterization, dissolution rate, MTT assay

## Introduction

The management perioperative/postoperative pain after any form of surgical treatment requires the administration of a local anesthetic (LA), such as lidocaine, chlorpropocaine, mepivacaine, bupivacaine, or ropivacaine. Under these circumstances, the administration of LA minimizes morbidity after surgery. However, the use of LA in such circumstances is limited due to the relatively short duration of action. Lidocaine, for example, only acts for 1–2 hrs.<sup>1</sup> LAs can be administered either by multiple injections, continuous infusion, or via a topical/transdermal (TT) route. However, these routes of administration are also associated with limitations, such as the need for an infusion device, the need for hospitalization, and the risk of infection.<sup>2,3</sup> In addition, topical anesthetics are limited by poor permeability and slow penetration. Therefore, there is an urgent need to develop a method to deliver LAs orally in a manner that provides the best efficacy.

Correspondence: Bushra T ALQuadeib  
Department of Pharmaceutics, College of  
Pharmacy, King Saud University, P.O. Box  
84428, Riyadh 11671, Saudi Arabia  
Tel +966 505653169  
Fax +966 118052932  
Email bquadeib@ksu.edu.sa

LID is one of the most effective and reliable hydrophilic Las, and is commonly used because of its rapid onset, intermediate action, and low systemic toxicity.<sup>4</sup> Furthermore, LID is commonly administered intravenously, although the intravenous infusion of LID may cause a range of adverse side effects, including seizures, dizziness, nausea, vomiting, and a metallic taste. LID is rarely applied percutaneously due to poor penetration through intact skin.<sup>5</sup>

LID is commonly used as local topical anesthetic, and is widely used for dental surgery due to its rapid onset of action (between 20 s to 1 min), and intermediate duration of efficacy (5–30 min), and is often used to relieve the pain associated with mouth ulcers. LID is available as a viscous gel, or ointment; these formulations are often used to relieve pain and discomfort from a sore throat/mouth. Research shows that LID is efficiently metabolized and only trace amounts are excreted in the urine.<sup>6</sup> Following oral ingestion, LID undergoes extensive initial metabolism, resulting in a bioavailability of approximately 30%.<sup>6</sup>

In an effort to improve and prolong the action of LA, a recent research study described the use of adjuvants for LA, including epinephrine and dexamethasone.<sup>7</sup> Other research studies have considered the use of delivery matrices, such as liposomes, microemulsions, microspheres, microcrystals,<sup>8</sup> cross-linked hydrogels, thermosensitive hydrogels, thermosensitive nanogels,<sup>9</sup> nanoparticles,<sup>10</sup> an aqueous polymer solution, a liquid polymeric matrix, a solid polymeric matrix,<sup>11</sup> a bio-adhesive film,<sup>12</sup> an interpenetrating polymer network (IPN) matrix,<sup>13</sup> lipid-protein-sugar particles and fatty-acid dimer-based polymer,<sup>14</sup> and ceramic-based granules.<sup>15</sup> Moreover, several published articles have considered the use of oral fast disintegrating films<sup>16</sup> and liposomal LID gels<sup>17</sup> with regards to both topical and systemic effects. One recent study reported the oral administration of LID HCL prior to anesthesia for laparoscopy.<sup>18</sup> Other research studies have described the oral delivery of microspheres, consisting of Alginate (ALG) and Chitosan (CS) as mucoadhesive polymers. These microspheres were successfully combined with various drugs, such as glipizide,<sup>19</sup> insulin,<sup>20</sup> ranitidine,<sup>21</sup> metformin,<sup>22</sup> diclofenac,<sup>23</sup> and various other drugs,<sup>24</sup> and showed improved solubility and bioavailability.

The aim of this study was to develop microspheres for the oral delivery of LID consisting of ALG and CS. We then optimized a series of new in vitro, characterized particle sizes, and used transmission electron microscopy (TEM) to determine the surface morphology of the

microspheres. Finally, we investigated drug yield, drug loading, and the LID release rate in vitro.

## Materials and Methods

### Materials

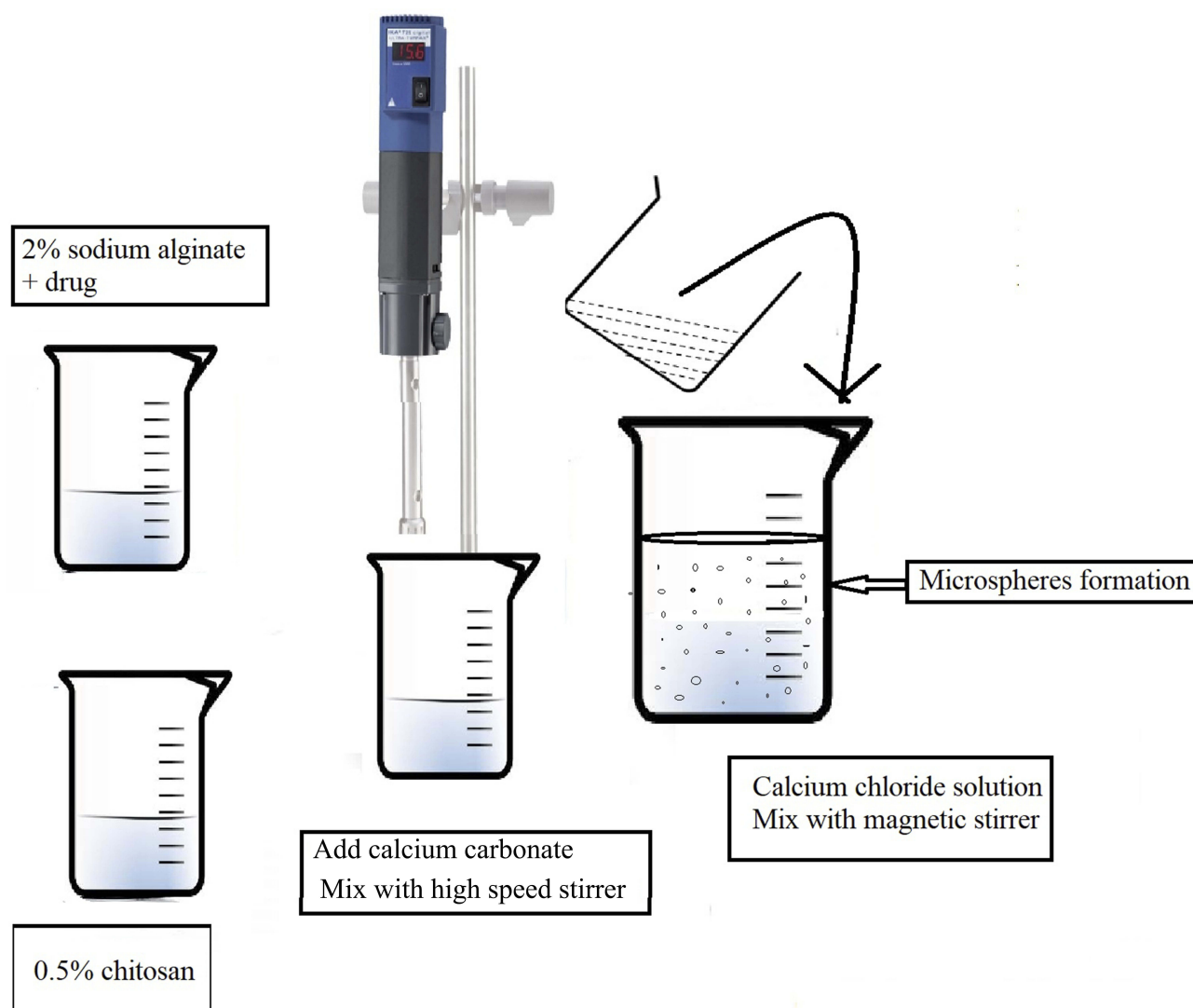
Lidocaine HCL was provided as a gift from Aljazeera Pharmaceutical Industry (Riyadh, Saudi Arabia). Diclofenac sodium (DS) was supplied by Spimaco (Al-Qassim, Saudi Arabia) while sodium alginate (MW about 115,000), was supplied by Fluka Chemie (Buchs, Switzerland). Chitosan (poly(D-glycosamine), deacetylated chitin, high molecular weight) was supplied by Aldrich, Darmstadt, Germany. Rat embryonic cardiomyocytes (H9c2 (2–1) cells) were purchased from the American Type Culture Collection (ATCC) (Manassas, Virginia, USA, ATCC® CRL-1446™), while the LLC-PK1 cell line was purchased from Sigma Aldrich (Taufkirchen, Germany). For the assessment of in vitro nephrotoxicity, we utilized the LLC-PK1 cell line from Sigma Aldrich (Taufkirchen, Germany).

All other reagents and chemicals were of high-performance liquid chromatography (HPLC) analytical grade, and were used as received. Water was deionized and purified with a Milli-Q Reagent Grade water system (Millipore Corporation, Bedford, MX, USA).

### Preparation of Lidocaine HCl Microspheres

LID microspheres were prepared using an extrusion congealing technique, described previously by Tahtat.<sup>25</sup> In brief, solution (1) was created by mixing 2% (w/v) sodium alginate with 25 mg of lidocaine in 40 mL of distilled water at room temperature under mechanical stirring. Solution (2) was then created by dissolving 0.5% chitosan solution in 1% v/v acetic acid (10 mL); the pH was then adjusted to pH 5 using 1 M NaOH. The two solutions were then mixed until homogeneous using a high-speed stirrer (9500 rpm), and an Ultra-Turrax (Ika, Artisan, Illinois, USA), at room temperature for 60 min. Then, calcium carbonate was added to blend the solutions at a ratio of 1:1 to alginate sodium. Next, the mixture was dropped, using a 24 G syringe needle, into 100 mL of calcium chloride solution (1% w/v) containing glacial acetic acid (10% v/v) (Figure 1).

In order to evaluate different mass proportions, four formulations were tested named N1, N2, N3, and N4 which contained alginate to chitosan at a weight/weight ratio of 1.0:0, 0.8:0.2, 0.7:0.3 and 0.6:0.4, respectively.



**Figure 1** Schematic method for preparation of microspheres by extrusion congealing technique.

Smooth and spherical microspheres beads were formed by mechanical stirring for 4 h. The microspheres were then washed with distilled water to remove any remaining calcium chloride. The wet microspheres obtained were then suspended in glutaraldehyde solution (2%) for 48 h at room temperature. Then, the microspheres were washed with hot-distilled water, air-dried, and stored at 4°C. All formulations were prepared in triplicate as a minimum.

## Characterization of the Formulated Lidocaine Microspheres

### Particle Size Analysis

The mean of particle size (MPS) was determined using a Zetasizer NanoZS, Malvern (Almelo, Netherland). Typically, 5 mg of the formulation samples (N1, N2, N3, and N4) were

dissolved in phosphate buffer pH 7.4 (15 mL each), and sonicated prior to measurement. Measurements were taken in triplicate and the mean  $\pm$  standard deviation was calculated.

### Determination of Drug Entrapment Efficiency and Microsphere Yield

Yield is determined using equation (1).

$$\text{yield percentage} = 100 * (\text{weight of the microspheres} / \text{weight of the drug} + \text{excipient}) \quad (1)$$

For drug entrapment efficacy (DEE), we took 5 mg of LID from each microsphere formulation, and dissolved this in 15 mL of phosphate buffer (pH 7.4) overnight. The next day, the solution was sonicated for 15 min and then

analyzed using a mass tandem –liquid chromatography. All experiments were performed in triplicate. The concentration of LID was calculated using the following equation (2).

$$\text{DEE (\%w/w)} = 100 * (\text{Mass of recovered DS} / \text{Initial mass of drug used in formulation}) \quad (2)$$

### Differential Scanning Calorimetry (DSC)

Pure components, as well as drug-loaded microspheres, were measured thermally using a Perkin Elmer DSC-4000, Buckinghamshire, UK. Approximately 2 mg of each sample was weighed and placed into standard aluminum pans, which were then hermetically sealed. An empty pan was used as a reference. The heating rate was 5°C/min, with a temperature range of 30°C to 180°C, and was carried out in a closed-pan system under a stream of nitrogen gas. The apparatus was calibrated with 99.99% indium.

### Transmission Electron Microscopy (TEM)

Next, we investigated the morphology of the formulated LID loaded microspheres by TEM (Jel-1010 Electron microscope, Jeol, Japan). The particulate carriers were negatively stained using uranyl acetate. The stained grid was then air dried and examined immediately under TEM.

## Drug Release from Lidocaine-Loaded Biodegradable Microspheres

In vitro release tests (dissolution) were performed as reported previously,<sup>16</sup> using US Pharmacopeia XXXII dissolution apparatus 2 (paddle), along with 900 mL medium; experiments were carried out with stirring at 75 rpm and the temperature was maintained at 37 ± 0.5°C. Dissolution media were evaluated in three different pH media (a 0.1 N hydrochloric acid solution (pH 1.2), and two citrate-phosphate buffers (pH 4.5, and 7.4)). A LID sample, equivalent to 25 mg of lidocaine, was placed on the surface of the dissolution medium. At appropriate time intervals (0, 0.5, 1, 2, 3, 4, 5, 6, 8 and 24 h), 2.0 mL samples were withdrawn from each vessel, and mixed with 1.0 mL of internal standard (IS) (10 µg/mL) and 5.0 mL of methanol: water (75:25). The solution was then filtered through a 0.22 µm Millipore membrane filter and analyzed using a validated UPLC assay, as described below. The volume was replaced each time with 2 mL of fresh medium, which

was maintained at a temperature of 37 ± 0.5°C to maintain a sink condition. All samples were tested in triplicate.

## Analyzing the Kinetics of Drug Release

To evaluate the drug release kinetics for LID formulations, we used several different dissolution models, including zero, first, Higuchi and Korsmeyer–Peppas order. The slope of each model represented the release rate. The most appropriate model was selected by determining the best fitting (R<sup>2</sup>) values.

## Chromatographic Conditions

Drug analysis was carried out with a Waters Acquity UPLC™ system fitted with an autosampler. An Acquity UPLC™ BEH Shield RP18 (1.7 µm column, 2.1 × 50 mm, Waters Corp, Milford, MA, USA) was used for separation, and the column temperature was maintained at 25°C. The gradient elution for UPLC analysis consisted of two solvent compositions: solvent (A) (10 mM ammonium formate (pH 3 ± 0.2), containing 0.2% formic acid and 1% acetonitrile), and solvent (B) (acetonitrile containing 0.2% formic acid). The gradient elution of solvent A:B was increased from 30% to 85% of solvent A within 3.3 min, then reduced back to 30% of solvent A, with a flow rate of 0.25 mL/min. The total run time was 4.0 min. Data were collected in multi-channel analysis mode and processed using MassLynx™ V 4.1 software the TargetLynx™ V 4.1 program (Waters Corp., Milford, MA, USA) was used to analyze the data. The UPLC was connected to a triple quadrupole tandem-mass detector (Water, Corp), with a positive ion mode electrometry ionization (ESI) source for mass spectroscopy detection. The optimal mass spectroscopy parameters were as follows: cone voltage = 27V; desolvation temperature = 400°C, and collision energy of 20 eV. Argon was used as the collision gas at a pressure of approximately 0.25 Pa. The optimized collision energy for lidocaine was 22 eV.

The precision and accuracy of the developed LC-MS/MS method were measured for the concentration range of 0.5–20 ng/mL; there were no significant differences between the inter- and-intra-day analysis (p>0.05) of quality control samples. A linear relationship was observed over the investigated concentration range, with a correlation coefficient of r>0.994 (n=6/day). The assay was able to detect LID concentrations without any form of modification.



## In vitro Cell Viability and Cytotoxicity Assays

In order to evaluate in vitro cardiotoxicity, we used rat embryonic cardiomyocytes (H9c2 (2–1) cells). These cells were cultured in Dulbecco's Modified Eagle Medium (DMEM) supplemented with 10% fetal bovine serum, containing 4 mmol of glutamine and penicillin-streptomycin (100 U/mL) in 75 cm<sup>2</sup> tissue culture flasks. Cells were maintained in a humidified incubator in an environment of 95% air/5% CO<sub>2</sub>, and a temperature of 37°C. For cytotoxicity and ultrastructural studies, cells were seeded in 96-well microliter plates, and 12-well plates, respectively.

In order to investigate in vitro nephrotoxicity, we used the LLC-PK1 cell line. This cell line was grown in an RPMI-1640 culture medium (Sigma St. Louis, MO) and supplemented with 10% (v/v) bovine fetal serum (Invitrogen Co Ltd, Carlsbad, CA), 100 IU of penicillin/mL, and 100 mg/mL of streptomycin (Sigma, St. Louis, MO). Cells were subsequently grown in 75 cm<sup>2</sup> flasks (TPP, Sigma Aldrich, St. Louis, MO), and kept at 37°C in an environment containing 5% CO<sub>2</sub>.

Cells (H9c2 and LLC-PK1) were seeded into 12 well plates and suspended in 1.0 mL of medium. After incubation for 1 day, cell cultures were treated with 100, 200, and 400 ng/μL of culture medium alone (control), or with standard LID and LID formulations (N1, N2, N3, and N4), and incubated for another 2 and 24 hrs. The cells were then pelleted by centrifugation at 1000 rpm for 3 min and then supernatant discarded prior to re-suspension in 0.5 mL of fresh medium without FBS. Cells were then incubated with 500 μg/mL of MTT for a further 2 hrs at 37°C in an environment containing 5% CO<sub>2</sub>. Next, we added 800 μL of isopropanol to each well, and after 10 min, determined the absorbance at 570 nm. The number of viable cells in the treated wells was then compared to the number of viable cells in the untreated wells in order for us to determine the overall cell viability (%). Tests were performed in triplicate from three independent experiments. No ethics approval was required from the Institutional Review Board, the experiment only featured commercial cell lines.

### Stability Studies

The freeze-thaw stability of the plasma samples was evaluated by exposing quality control samples to three freeze (–20°C) and thaw (room temperature) cycles for different time intervals including the 0, 1, 2, and 4 days, as well as one and 3 weeks, then additionally tested after 1 and 3

months of preparation and storage at –20°C. The samples were analyzed by a UPLC system, as described previously.

## Results and Discussion

### Formulation Development and Optimization

The major factor underlying the successful encapsulation and release of drugs from microspheres is the production method. In addition, a range of other factors can also have a strong impact on drug delivery rates, including the type of polymer, the molecular weight of the polymer, the nature of any excipients added to the microsphere formulation, and the size of the microspheres.

Microspheres consisting of ALG-CS polymers are formulated by three common techniques: spray-drying, extrusion, and emulsification/gelation. The extrusion and emulsification/gelation technique has already been applied to encapsulate various types of drugs in the pharmaceutical and biotechnology industry.<sup>24</sup> More recently, alginate–chitosan loaded drugs have been developed to improve the bioavailability of a large number of drugs.<sup>19–24,26,27</sup>

### Mean Particle Size, Poly Disparity Index, and Zeta Potential

The particle size (MPS) measurements for all of the developed formulations were in the nano-range (340.6 ± 21.5 to 528.3 ± 14.7 nm; Table-1). A significant reduction in MPS was observed when we reduced the amount of sodium alginate. These findings are consistent with previous literature relating to vancomycin-encapsulated chitosan–alginate microparticles.<sup>28</sup> The size of the microspheres was not correlated with zeta potential (ZP) values, drug loading, and/or drug yield. A negative surface charge was observed for all of the measured nano-microspheres (> –29; Table 1). This finding was in agreement with previous studies using sodium alginate diclofenac microspheres, which also showed negative ZP measurements (–35 mV).<sup>23</sup>

### Determination of Drug Entrapment Efficiency and Microsphere Yield

Table 1 shows the percentage yield, and drug encapsulation efficiency (DEE), of the developed formulations. There was no correlation between the concentrations of alginate, or the size of microspheres (MPS), with either the DEE or drug yield. These results are consistent with results from several previous studies.<sup>29–31</sup>

**Table 1** Mean Particle Size, Drug Encapsulation, and Drug Yield of Developed Formulations. Each Value Is the Mean  $\pm$  Standard Deviation of at Least Three Experimental Determinations

	Sodium Alginate: Chitosan Ratio	Mean Particle Size (nm) (n=3, $\pm$ SD)	Zeta Potential (n=3, $\pm$ SD)	Drug Encapsulation Efficiency (n=3, $\pm$ SD)	Drug Yield (n=3, $\pm$ SD)
N1	1.0: 0	528.3 $\pm$ 14.7	-26.4 $\pm$ 1.7	29.2 $\pm$ 4.6	41.3 $\pm$ 2.5
N2	0.8: 0.2	507.3 $\pm$ 17.4	-27.3 $\pm$ 2.1	30.7 $\pm$ 4.1	41.1 $\pm$ 4.0
N3	0.7: 0.3	487.3 $\pm$ 22.5	-25.2 $\pm$ 2.6	29.4 $\pm$ 3.5	42.3 $\pm$ 3.5
N4	0.6: 0.4	340.7 $\pm$ 21.5	-29.7 $\pm$ 1.1	28.7 $\pm$ 2.6	42.6 $\pm$ 2.8

## Thermal Analysis

Differential scanning calorimetry (DSC) studies of the pure LID produced an endotherm sharp peak corresponding to a melting point of 81°C, indicating that LID HCl is crystalline (Figure 2). A similar endothermic peak was reported in previous studies.<sup>32–34</sup> Both sodium alginate and chitosan are crystalline and semi-crystalline polymers; this is because of their linear and regular structures. These compounds melt at temperatures ranging from 60°C to 100°C, due to the loss of water.<sup>32,35</sup> The sharp drug peak was not evident in the LID formulations (N1, N2, N3, and N4); this was due to the LID being solubilized in a melted mass during the heating cycle of the DSC studies, or because the drug may have been present in its amorphous state in the polymer matrix. A similar phenomenon has been observed for tetracaine in water.<sup>36</sup>

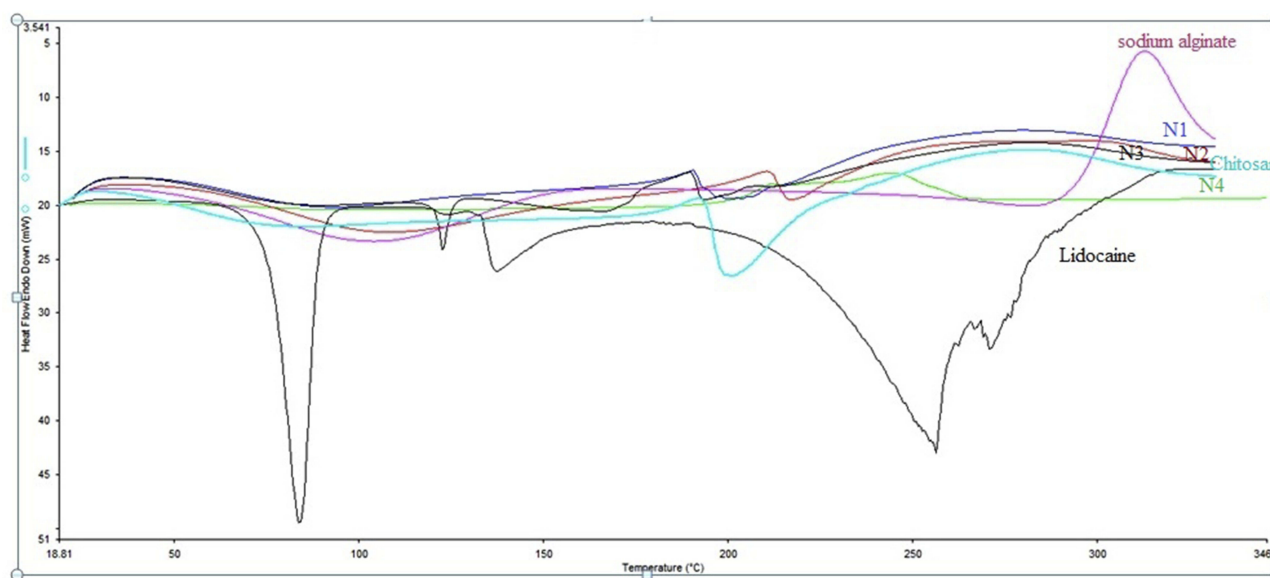
## Transmission Electron Microscopy of LID

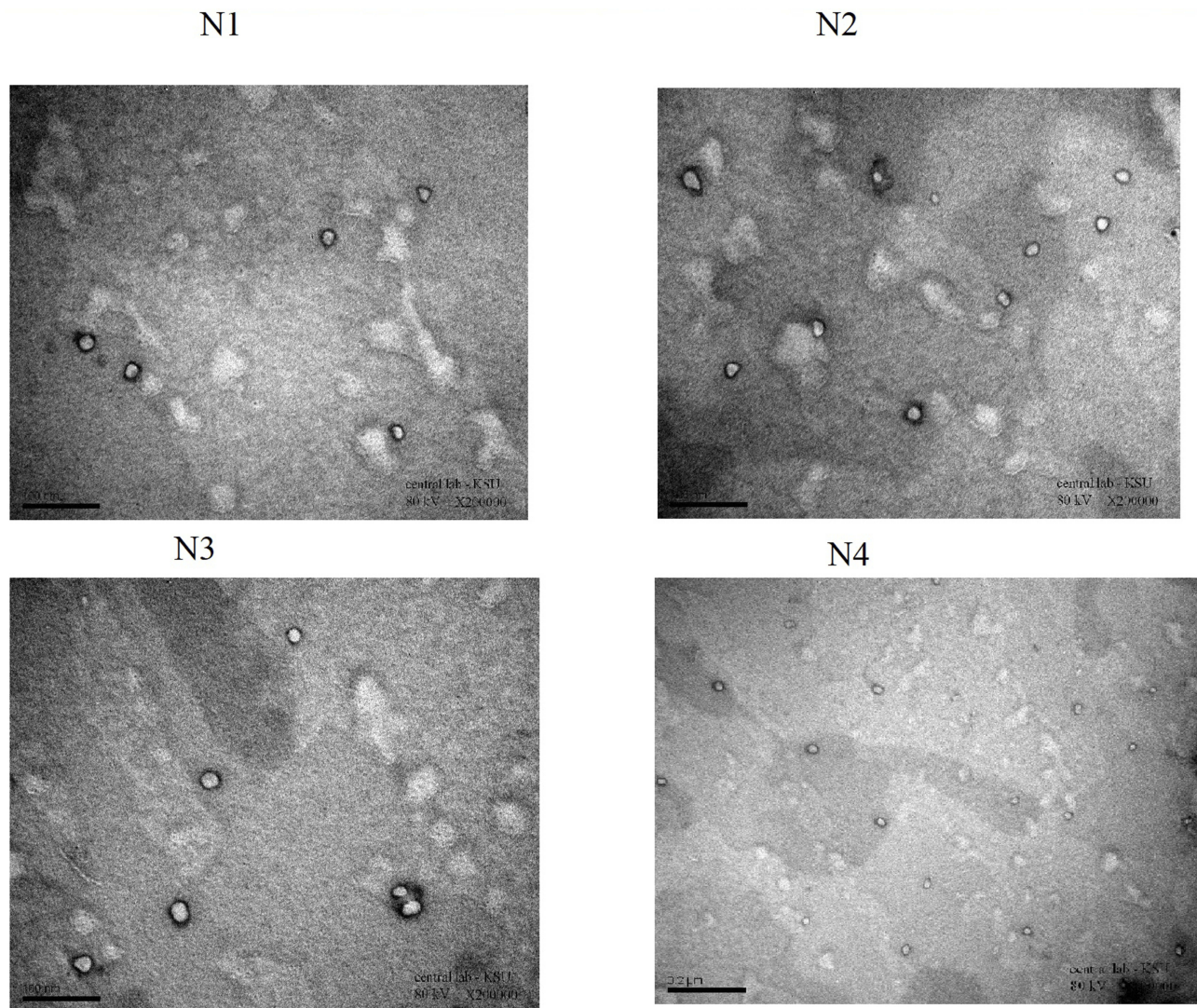
Next, we examined the morphology of the microspheres using TEM (Figure 3). TEM images showed that the microspheres

in our formulations were almost spherical, with some irregularities at the periphery of the particles. The particle size of the formulations developed, as determined by TEM, was in agreement with MPS data.

## In vitro Release Studies

Since LID and chitosan exhibit pH-dependent solubility,<sup>37–40</sup> the pH of the dissolution medium will affect the dissolution of the drug from the microspheres, as shown in Figure 4a, b and c, at pH 1.2 (stomach), pH 4.5 (lysosomes), and pH 7.4 (equivalent to blood pH), respectively. At all pH values, the rate of LID release from the microspheres occurred in a biphasic process. The burst effect occurred slowly (<10%) within the first 60 min; this was followed by a slower release step. The initial burst release of LID from the microspheres may be attributed to the drug being adsorbed on to the surface; the drug can then readily diffuse into the media, thus creating the observed burst release. After 60 min, we observed a sustained form of drug release, indicating that the LID had been successfully incorporated into the microspheres. Compared to low pH

**Figure 2** DSC Thermogram of pure Lidocaine, pure sodium alginate, pure chitosan, and the developed microspheres formulations (N1, N2, N3, and N4).



**Figure 3** TEM images for Lidocaine microspheres formulations (N1, N2, N3, and N4).

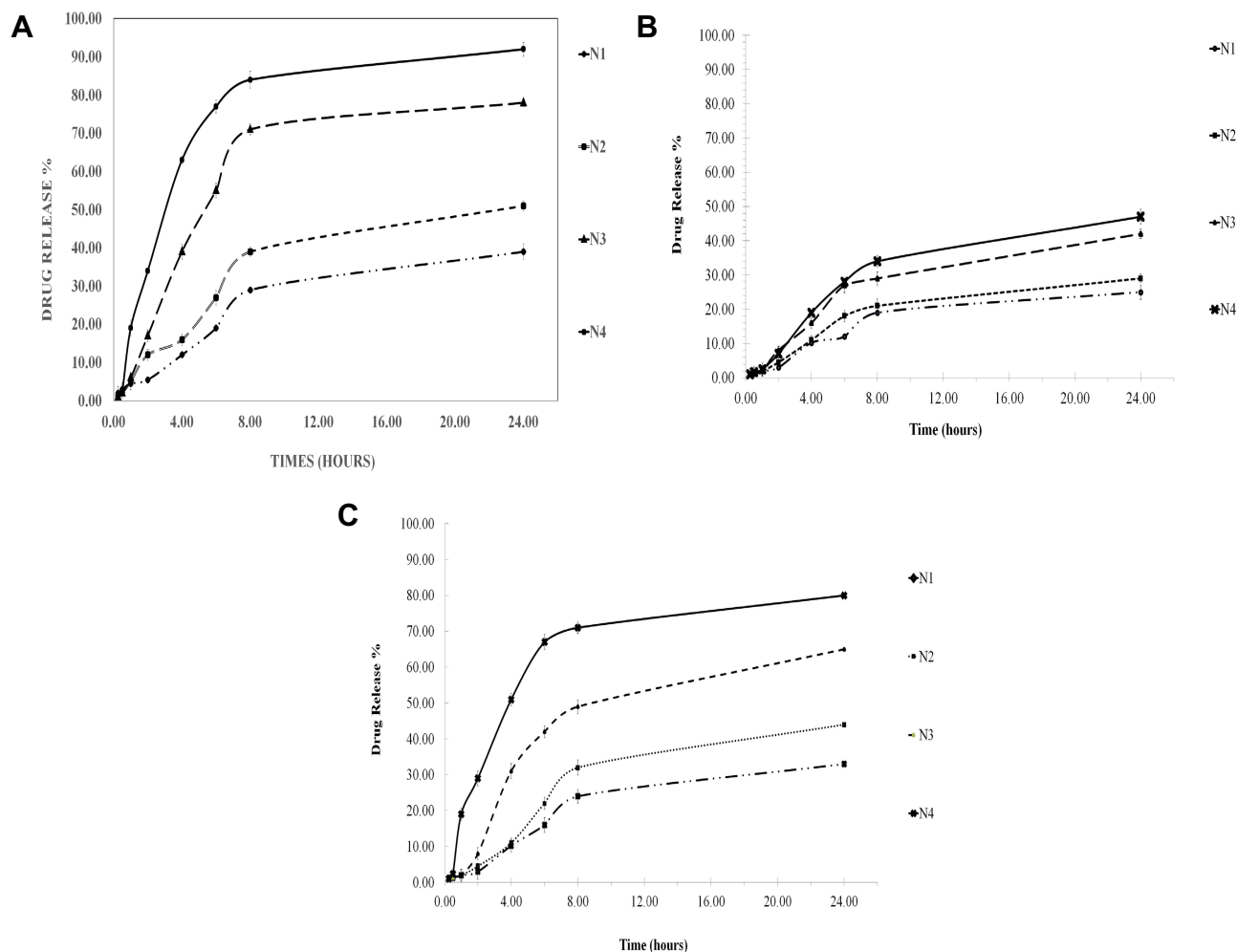
(pH 1.2), there was a significant enhancement in drug release between pH 4.5 and 7.4. Thus, an acidic medium appeared to yield optimal results. This is in agreement with previous literature<sup>2</sup>. The resulting alginate–chitosan microspheres exhibited a release behavior that was dependent on pH.<sup>29</sup>

Less than 10% of the burst release of the drug was leached from the microspheres; this was consistent across all pH values tested. Approximately 25–94% of the LID was released after 24 h, depending upon the pH conditions. The highest release rate was observed at pH 1.2, followed by pH 4.5 and pH 7.4 (Figure 3); these findings are related to the pKa values of LID. As pH increases, the ionized lidocaine diffused out of the polymeric matrix more easily (Figure 3). Similar phenomena were observed for LID chitosan, and hyaluronic acid bioadhesive transdermal,<sup>44</sup> and for the release of sunitinib, an anticancer agent, from magnetic chitosan nanoparticles.<sup>41</sup>

In addition, the observed pH-dependent pattern was consistent with the previously described drug release behavior of indomethacin-crosslinked chitosan–Malginate microspheres, in which a higher pH caused lower rates of indomethacin release due to greater crosslinking in the microspheres.<sup>27</sup> Protonation of the amine groups of the drug is known to improve solubility in an acidic medium. At low pH, alginate and chitosan are known to exist in a gel form, while at neutral pH, the viscous complex will swell and the gel will slowly disintegrate, thus causing the drug to be released.<sup>29</sup>

Moreover, the rate of drug release correlated with the mean particle size, and was fastest for small particles and slowest for large particles; this was the case for all pH conditions tested. The release rate of LID from microspheres was higher in the N4 treatment, followed by the N3, N2, and N1 treatments. For example, after 4 hrs at pH





**Figure 4** (A) Mean percent release profile LID-microspheres ( $\pm$  SD, N=3) in PBS (pH 1.2, 37°C) as dissolution medium from different microspheres for 24 hrs. (B) Mean percent release profile LID-microspheres ( $\pm$  SD, N=3) in PBS (pH 4.5, 37°C) as dissolution medium from different microspheres for 24 hrs. (C) Mean percent release profile LID-microspheres ( $\pm$  SD, N=3) in PBS (pH 7.4, 37°C) as dissolution medium from different microspheres for 24 hrs.

1.2, 12%, 16%, 39%, and 63% of drug release was observed for the N1, N2, N3, and N4 formulations. The higher release rates correlated with lower MPS values. The same correlation was observed at both pH 4.5 and pH 7.4 (Figure 4a, b and c). The same relationship between drug loading and the rate of release was observed in a previous study.<sup>27,44</sup>

## Drug Release Kinetics

The application of different mathematical models for the in vitro release of LID biodegradable beads was interpreted and evaluated by correlation coefficient ( $R^2$ ) analysis (Table 2). Identification of the highest correlation coefficient was used to determine the most suitable mathematical model for drug release kinetics. The Higuchi model showed a higher correlation coefficient ( $R^2$ , Table 2) than the other models. Hence, the drug release

profile for LID relies upon a diffusion mechanism. Hydrophilic nasal gel of LID<sup>42</sup> showed similar results (Higuchi order).

## Chromatography and Selectivity Method Development

We developed a simple and fast UPLC assay for the preparation of LID. We found that the robustness and reproducibility of the assay improved when carried out at pH of 3 as well as the most prominent and stable fragments for LID.

Figure 5 shows MS and MS/MS traces of LID obtained from a blank, and a spiked standard solution of 10 $\mu$ g/mL, in the positive ion mode. All LC-MS/MS data utilized Electrospray ionization (ESI) in positive mode; in negative mode, no signal was acquired. This data was in agreement with a number of previous studies.<sup>43–48</sup> In the MS mode,

**Table 2** Modeling of Lidocaine Release from Different Formulations

Formulation Code	Zero-Order ( $Q_t=Q_0 -kt$ )		First-Order ( $\ln Q_t = \ln Q_0 -kt$ )		Higuchi-Order ( $Q_t = k \sqrt{t}$ )		Korsmeyer–Peppas $Q_t/Q_1 = Kt^n$ ( $n=0.5, 0.75, 1.25$ )	
	R2	K	R2	K	R2	K	R2	K
N1	0.7500	1.932	0.8520	0.026	0.9329	7.848	0.9134	6.174
N2	0.7136	2.570	0.8716	0.041	0.9280	10.539	0.9154	8.756
N3	0.5149	4.255	0.8377	0.122	0.9822	18.090	0.8520	17.726
N4	0.2198	5.281	0.9720	0.227	0.9839	23.436	0.8111	28.179

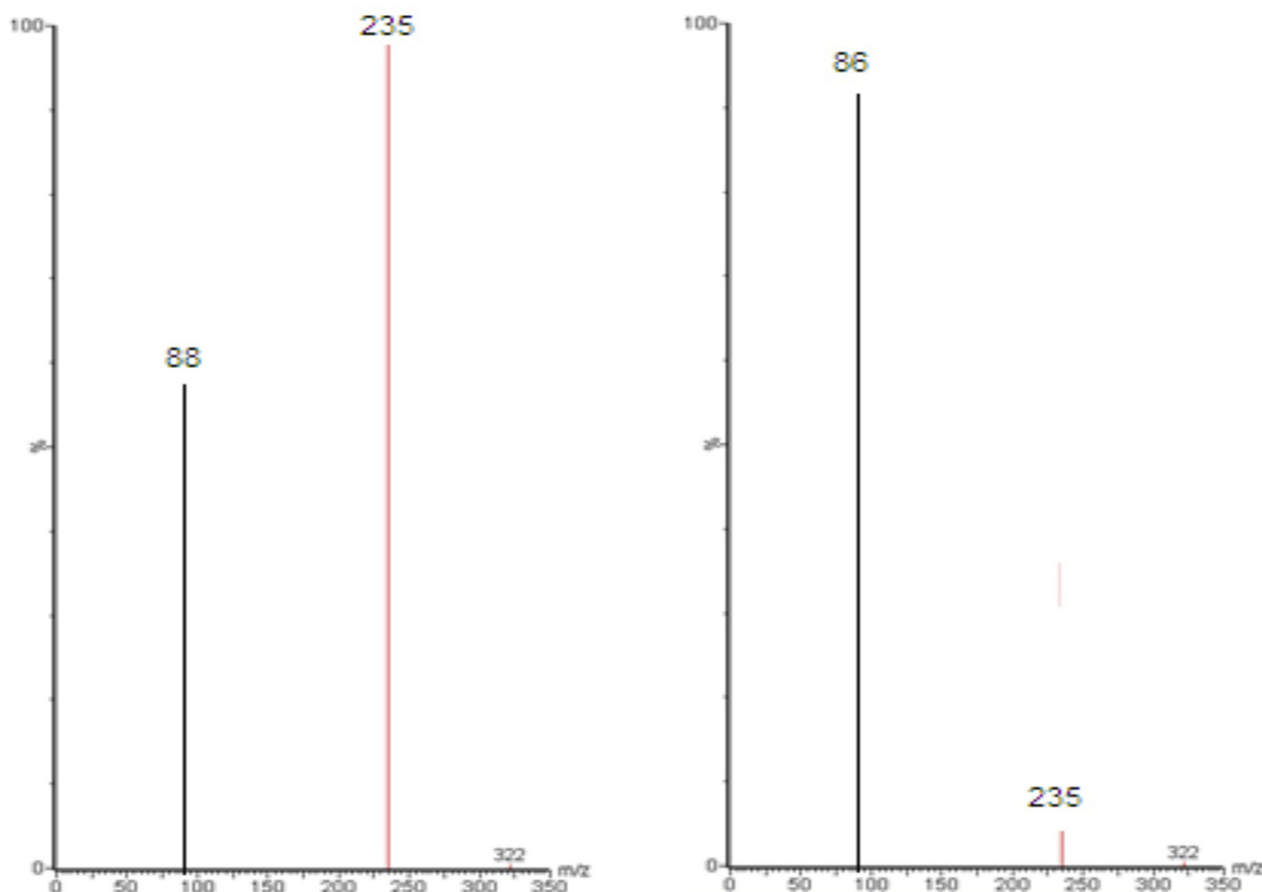
**Notes:** R2 is the correlation coefficient; K is the release rate constant for respective models. Where  $Q_t$  is the amount of drug released at time t,  $Q_1$  is the initial amount of drug k is release rate constants of respective equation.

the precursor ion for LID is the protonated molecular ion  $[M + H]^+$  at  $m/z$  235, while the daughter product ion is at  $m/z$  86 for lidocaine (Figure 5). No interfering peak was detected at retention times that corresponded to LID. Furthermore, no interfering signals were detected from the spiked sample when drugs were frequently co-administered at the relevant drug retention times (Figure 6). This method was validated over a linear range of 10–120

$\mu\text{g/mL}$  ( $Y = 0.0075 X + 0.205$ , in which Y represents the area under the peak (AUP)).

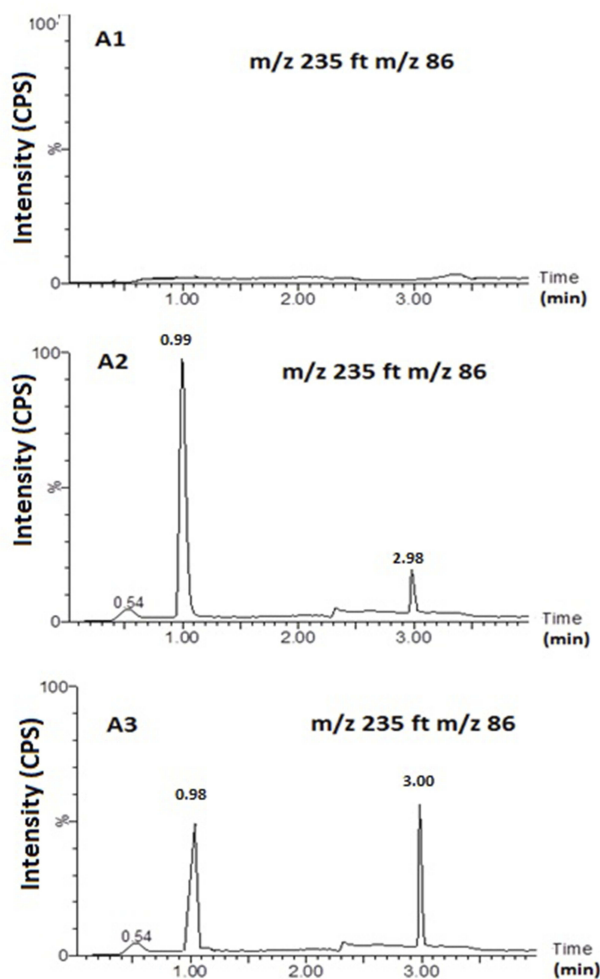
### Carry-Over

Carry-over was determined by analyzing two processed control samples after a ULOQ sample over three separate runs. We did not observe eluting peaks with areas >20% of the LLOQ when the quality control samples were directly



**Figure 5** Full-scan product ion spectra of  $[M + H]^+$  of Lidocaine parent (A) drug and daughter (B).





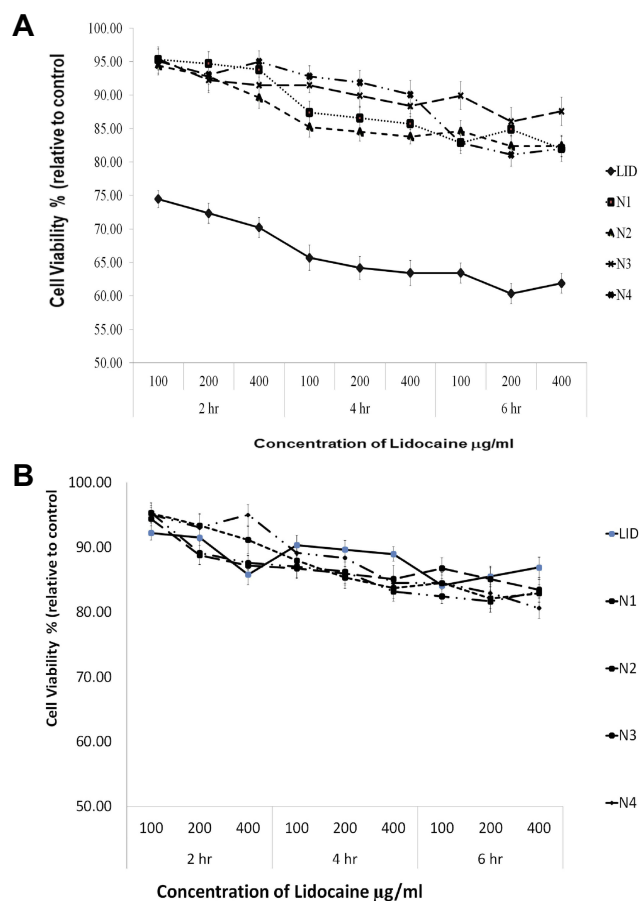
**Figure 6** Representative MRM Chromatograms. Blank sample (A1); Spiked sample (A2; Lidocaine (10 ng/mL) and Clopedogril (10 ng/mL)); sample form N3 formulation (A3). Column: An acquity UPLCTM BEH Shield RP18 (1.7  $\mu$ m column, 2.1  $\times$  50 mm, Waters Corp, Milford, MA, USA).

injected after ULOQ samples. Therefore, the data met the criteria for carry-over.

## In vitro Cell Viability and Cytotoxicity Assays

Both the cardio toxicity and nephrotoxicity of both LID and LID formulations (N1, N2, N3, and N4) were tested in two cell lines (H9c2 (2–1) and LLC-PK1 cells, respectively), at different concentrations (100, 200, and 400 ng/mL), for a duration of 2, 4, 6 and 24 hrs.

Previous research has shown that LID exerts cardio-toxic effects<sup>48</sup>. Figure 7a shows that pure LID is cardio-toxic, while the new LID microspheres formulations were safe. The LID microspheres formulations remained viable over different concentrations, even at 400 ng/mL (at which more than 80% of cells were viable). In addition, a dose-



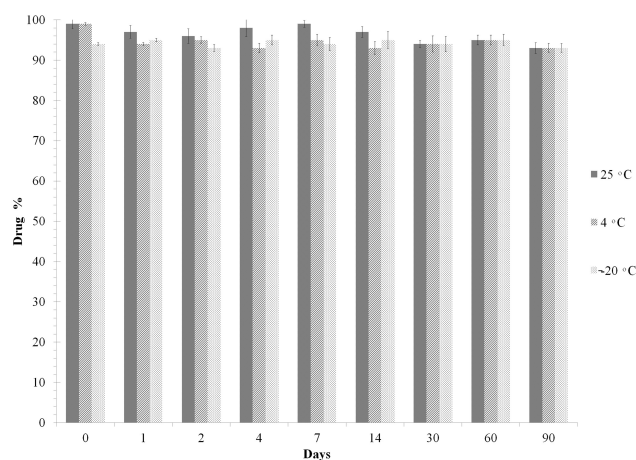
**Figure 7 (A)** The viability of H9c2 (2–1) cells after exposed to tested LID-alginate-chitosan microspheres formulations (100, 200, 400 ng/ $\mu$ L and control) after 2,4 and 6 hrs determined by MTT assay. Data represent mean  $\pm$  SD (n=3). **(B)** The viability of LLC-PK1 cells after exposed to tested LID-alginate-chitosan microspheres formulations (100, 200, 400 ng/ $\mu$ L and control) after 2.4 and 6 hrs determined by MTT assay. Data represent mean  $\pm$  SD (n=3).

dependent reduction in viability was observed within the 2 hrs test. Data show that LID microsphere formulations were less toxic than the LID itself. The same observations were obtained at 4 and 6 hrs.

LID is known to be safe for the kidney. Figure 7b shows that the pure drug, as well as the LID microsphere formulations, were safe as cell viability exceeded 80%. Furthermore, the LID microsphere formulations were safe over a different concentration range, as cells remained viable, even at concentrations as high as 400 ng/mL.

## Stability

In order to determine the best storage temperature for the microspheres, we conducted a stability study. LID and IS remained stable for up to 90 days at room temperature (samples were processed in autosampler vials at 25°C). Furthermore, these drugs remained stable for up to 3 months



**Figure 8** Freeze-thaw stability of LID at different temperatures. Data represent mean  $\pm$  SD (n=3).

when stored at 4°C and -20°C. Therefore, all samples were stored at 4°C for same-day analysis by LC/MS/MS. Chromatographic analysis showed that there was no significant freeze/thaw degradation after three repetitive cycles (<10% degradation) for either LID or IS (Figure 8).

This study has limitations that should be considered testing different concentrations of both polymers (alginate, chitosan) as well as addition of different stabilizers. Further studies are now needed to investigate the pharmacokinetic and pharmacodynamics of the formulated biodegradable LID microspheres to elucidate the specific patterns of in vivo release, and to develop the potential of the microspheres as an oral delivery system.

## Conclusions

We developed a novel LID oral formulation that improves the solubility of LID and enhances the release of LID in vitro. These innovative LID microsphere formulations had a mean particle size that was in the nano range. Different ratios of alginate and chitosan were used to create different types of microsphere. We observed that MPS reduced as the concentration of alginate was reduced; there was no correlation with either drug loading or drug yield. Our data suggest that the formulations developed are viable and effective, and can be used as a novel oral delivery system for LID. Moreover, these new LID microspheres exhibited significantly less cardiac toxicity than LID alone.

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## Disclosure

The authors report no conflicts of interest in this work.

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