REVIEW PAPER



# Cellulose-based virus-retentive filters: a review

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Abstract Viral filtration is a critical step in the purification of biologics and in the monitoring of microbiological water quality. Viral filters are also essential protection elements against airborne viral particles. The present review first focuses on cellulosebased filter media currently used for size-exclusion and/or adsorptive filtration of viruses from biopharmaceutical and environmental water samples. Data from spiking studies quantifying the viral filtration performance of cellulosic filters are detailed, i.e., first, the virus reduction capacity of regenerated cellulose hollow fiber filters in the manufacturing process of blood products and, second, the efficiency of virus recovery/concentration from water samples by the viradel (virus adsorption–elution) method using charge modified, electropositive cellulosic filters or conventional electronegative cellulose ester microfilters. Viral analysis of field water samples by the viradel technique is also surveyed. This review then describes cellulose-based filter media used in individual protection equipment against airborne viral pathogens, presenting innovative filtration media with virucidal properties. Some pros and cons of cellulosic viral filters and perspectives for cellulose-based materials in viral filtration are underlined in the review.

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**Keywords** Cellulose filter media  $\cdot$  Virus filtration  $\cdot$ Viral clearance - Adsorption–elution method - Filtering facepieces

### Abbreviations





# Other abbreviations





# 1 Introduction

Virus capture/purification/concentration is critical in a number of biopharmaceutical and clinical applications. Validation of virus clearance is essential in the manufacture of therapeutic proteins, in particular blood products (Bryant and Klein [2007](#page-28-0); Klamroth et al. [2014](#page-31-0); de Mendoza et al. [2012](#page-29-0); Radosevich and Burnouf [2010;](#page-32-0) Shukla et al. [2007\)](#page-33-0). On the other hand, large-scale, efficient purification schemes of viruses/ virus-like particles are required for the production of prophylactic vaccines and gene therapy vectors (Rodrigues et al. [2007;](#page-32-0) Segura et al. [2006](#page-33-0), [2011;](#page-33-0) Vicente et al. [2011a](#page-33-0), [b\)](#page-33-0). Virus inactivation technologies are commonly used to fulfil viral safety. They include physical (e.g., heat application, ultraviolet- and gamma irradiation) and chemical methods (e.g., solvent/detergent treatments) or their combination (e.g., exposure to photosensitizer plus UV light) (Bryant and Klein [2007](#page-28-0); Klamroth et al. [2014](#page-31-0); Klein and Bryant [2009;](#page-31-0) Pelletier et al. [2006](#page-32-0); Prowse [2013](#page-32-0); Radosevich and Burnouf [2010](#page-32-0); Solheim [2008](#page-33-0)). Common methods for virus capture include filtration

(Charcosset [2006](#page-28-0); Grein et al. [2013;](#page-30-0) Liu et al. [2010](#page-31-0); van Reis and Zydney [2007](#page-33-0)) and chromatography in column or membrane configurations (Charcosset [2006;](#page-28-0) Gottschalk [2008](#page-29-0); Liu et al. [2010;](#page-31-0) Orr et al. [2013;](#page-32-0) van Reis and Zydney [2007;](#page-33-0) Segura et al. [2011](#page-33-0)). Viral filtration is usually the final purification step in the downstream processing of biopharmaceutical products, e.g., monoclonal antibodies (Fig. 1), following one or more chromatography ''polishing'' steps that contribute to the overall virus removal efficiency of the process before concentration of the purified product. Filtration technologies are also extensively used for the capture and concentration of waterborne viral pathogens (Gibson [2014](#page-29-0)) from drinking, environmental, recreational or waste water

samples (Cashdollar and Wymer [2013](#page-28-0); Ikner et al. [2012\)](#page-30-0). In addition, particulate air filters are used in personal respiratory protective equipment (i.e., face masks and respirators) (Bunyan et al. [2013](#page-28-0); Cohen and Birkner [2012;](#page-28-0) Rengasamy et al. [2004](#page-32-0)) to ensure shortrange protection of wearers against airborne pathogens–which include a number of viruses (Tang et al. [2006\)](#page-33-0)—and in air purifiers/cleaners to limit longrange aerosol transmission of infection in healthcare settings (Hyttinen et al. [2011](#page-30-0); Tang et al. [2006\)](#page-33-0).

Cellulosic membrane microfilters have been used routinely for ages in laboratories to perform the socalled ''sterile filtration'' (cold sterilization), i.e., the absolute removal of bacteria, yeasts and molds but not viruses (Walsh and Denyer [2012\)](#page-33-0) from heat-sensitive



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liquid media. However, many virus filtration devices currently implemented are made from cellulose and its derivatives. Some eighty years ago, Gradocol, graded collodion (cellulose nitrate) membrane filters (Elford [1931;](#page-29-0) Bauer and Hughes [1934](#page-28-0)) have been extensively used in ultrafiltration to estimate the size of several medically important viruses such as foot-and-mouth disease (Galloway and Elford [1931\)](#page-29-0), vaccinia (Elford and Andrewes [1932](#page-29-0)), herpes (Elford et al. [1933](#page-29-0)), poliomyelitis (Elford et al. [1935](#page-29-0)) and influenza (Elford et al. [1936\)](#page-29-0) (see also Ferry ([1936\)](#page-29-0) for an exhaustive review). Later on, commercial mixed cellulose ester filters with very low pore size, namely VF (virus fine), VM (virus medium) and VC (virus coarse) grade filters produced by Millipore (Billerica, MA, USA—a subsidiary of Merck KGaA, Darmstadt, Germany), have also been applied to virus ultrafiltration for grouping by size assessment (Hsiung [1965](#page-30-0)).

As part of a series of papers surveying the antiviral applications of polysaccharide-based materials, the present review focuses on viral filtration using cellulosic filter media—most of which are commercially available products that have been extensively tested over the past twenty years for the removal/concentration/purification of viral particles from liquid samples, i.e., biopharmaceutical (namely blood products) and environmental (raw or treated) water samples. The application of cellulose-based filters in individual respiratory protective devices protecting the wearer against airborne viral pathogens is also detailed. Polysaccharide-based chromatographic adsorbents for viral clearance or recovery/purification of viruses or virus-like particles will be presented elsewhere.

### 2 Viral filtration in the downstream purification processes of biopharmaceuticals

In the processing of biological products, virus removal from the product stream while providing maximum product recovery is a critical task. It is more particularly difficult to eliminate small viral particles such as parvoviruses, which may contaminate blood products and mammalian cell cultures used in the production of recombinant proteins (Charcosset [2006](#page-28-0)). Viral filters developed to answer this challenge are typically membrane (screen) filters ensuring a size-based rejection of viral particles via a sieving mechanism. Given the size of viruses, ranging roughly from 20 (Parvoviridae) to 400 nm (Poxviridae) (Segura et al. [2011\)](#page-33-0), viral filtration stands between microfiltration and ultrafiltration among pressure-driven filtration processes (Fig. [2](#page-4-0)), though it is frequently but incorrectly (van Reis and Zydney [2007](#page-33-0)) classified as nanofiltration (Burnouf et al. [2005\)](#page-28-0).

# 2.1 Regenerated cellulose hollow fiber (HF) membrane filters

Common virus filtration membranes are made from poly(ethersulfone) (PES), poly(vinylidene fluoride) (PVDF), and regenerated cellulose (Burnouf and Radosevich [2003;](#page-28-0) Carter and Lutz [2002;](#page-28-0) Liu et al. [2010;](#page-31-0) van Reis and Zydney [2007\)](#page-33-0). Among the latter, the commercial PlanovaTM filters (Asahi Kasei Medical, Tokyo, Japan) have been widely used to clear viruses from biologically produced pharmaceuticals, in particular blood products. Planova filters are composed of cuprammonium regenerated cellulose HF (Bemberg<sup>TM</sup> cupro fibers), prepared from cellulose cuprammonium spinning solution via microphase separation under precise spinning conditions (Tsurumi et al. [1990b](#page-33-0), [c\)](#page-33-0). The wall of each HF has a threedimensional web structure of pores consisting of large, bulky void pores interconnected by fine capillaries (Tsurumi et al. [1990a](#page-33-0), [b](#page-33-0), [c\)](#page-33-0) (Fig. [3](#page-4-0)). During filtration, as the feed solution containing the product of interest is circulated through the HF bore, viruses accumulate in the large, bulky void pores of the fiber network while the product solution passes through the capillary pores. Since the HF wall is several tens of micrometers thick (Fig. [4](#page-5-0)), viruses are captured gradually inside the porous structure that can be considered multi-layered (100–200 layers) (Hongo-Hirasaki et al. [2006\)](#page-30-0). Hence, Planova filters behave like ''membrane depth filters'' (Walsh and Denyer [2012](#page-33-0)) operating on the basis of size exclusion. They offer a choice of 4 nominal mean pore sizes, namely 15 nm (15N), 19 nm (20N), 35 nm (35N) and 72 nm (75N)—the large pore 75N model being essentially used as a prefilter to remove impurities or aggregates prior to final virus filtration—and can be operated in normal (dead-end/flow through) or tangential flow (cross flow) filtration mode (Phillips et al. [2007](#page-32-0)).

Planova filters have emerged to answer a publichealth problem of worldwide magnitude, i.e., blood contamination by HIV (Hamamoto et al. [1989](#page-30-0); Manabe et al. [1989](#page-31-0)) and hepatitis viruses (Yuasa

<span id="page-4-0"></span>

Fig. 2 The separation spectrum for filtration membranes. Adapted from Fröhlich et al.  $(2012)$  $(2012)$ 



Fig. 3 Schematic representation of the void pore structure of regenerated cellulose hollow fibers used in Planova filters. Adapted from Makino et al. ([1994\)](#page-31-0)

et al. [1991;](#page-34-0) Sekiguchi et al. [1989,](#page-33-0) [1990](#page-33-0)). Table [1](#page-5-0) gives examples of viral clearance studies assessing the capacity of Planova filters to remove viruses from blood products. In these viral clearance assays,

product streams resulting from successive, scaleddown purification steps representative of the manufacturing process of the product (Kundu and Reindel [2007\)](#page-31-0), were artificially contaminated (''spiked'') with model viruses of different sizes (Table [2\)](#page-6-0) (at much higher concentrations than what might be commonly found in the product intermediate) before being submitted to filtration. The virus removal efficiency of the filtration step was expressed as LRV (log reduction value, i.e., log ratio of the viral load in the spiked product feed stream to that recovered in the product filtrate), which implies that residual virus infectivity can never be reduced to zero but may be greatly reduced mathematically (ICH [1999\)](#page-30-0). Minimum LRV values were most frequently given. They were estimated when no viruses could be detected in filtered samples taking into account the detection limit of the assay (viral titer estimated as 1 infectious unit per sample volume). From the measured LRVs, the filtration operation is usually classified as effective  $(LRV > 4)$ , moderately effective  $(1 < LRV < 4)$  or

<span id="page-5-0"></span>

Table 1 Virus reduction factors (LRVs) achieved by filtration with Planova filters in the manufacturing process of different blood products (confidence intervals not shown)



 $a$  DE dead-end (normal) mode, T tangential mode. Filters were associated in series in DE and in parallel in T

<sup>b</sup> See Table [2](#page-6-0)

<sup>c</sup> Filtration step combined with pepsin treatment at pH 4.4

<sup>d</sup> Experiments were performed in duplicate; the lowest LRV is given. The filtration step was combined with low pH (4.4) inactivation for enveloped viruses (BVDV, HIV, PRV)

<sup>e</sup> Seven plasma proteins (and 2 types of Planova filters) were involved (mean LRV values are given)

([2006\)](#page-30-0)

Family <sup>a</sup>	Acronym Name		Relevant <sup>b</sup> /model for <sup>c</sup>	References	
Parvoviridae (ssDNA, NE)	<b>B19 V</b>	Human parvovirus <b>B19</b>	Relevant	Furuya et al. $(2006)$ and Terpstra et al. $(2006)$	
$18 - 26$ nm	<b>CPV</b>	Canine parvovirus	<b>B19 V</b>	Gröner (2014), Gröner et al. (2012), Koenderman et al. $(2012)$ and Terpstra et al. $(2006, 2007)$	
	<b>PPV</b>	Porcine parvovirus	<b>B19 V</b>	Caballero et al. $(2014)$ , Chtourou et al. $(2007)$ , Dichtelmüller et al. (2012), Furuya et al. (2006) and Gröner et al. (2012)	
Picornaviridae (ssRNA, NE) $22 - 30$ nm	<b>HAV</b>	Hepatitis A virus	Relevant	Chtourou et al. (2007), Furuya et al. (2006), Gröner $(2014)$ , Roberts et al. $(2010)$ and Terpstra et al. $(2007)$	
	<b>EMCV</b>	Encephalomyocarditis virus	<b>HAV</b>	Furuya et al. (2006, Roberts et al. (2010), Terpstra et al. (2006), Koenderman et al. (2012), Caballero et al. (2014)	
Flaviviridae	<b>WNV</b>	West Nile virus	Relevant/HCV	Caballero et al. $(2014)$ and Gröner et al. $(2012)$	
(ssRNA, E) $40 - 60$ nm	<b>BVDV</b>	Bovine viral diarrhea virus	<b>HCV</b>	Caballero et al. $(2014)$ ; Chtourou et al. $(2007)$ , Dichtelmüller et al. (2012), Furuya et al. (2006), Gröner $(2014)$ , Gröner et al. $(2012)$ , Koenderman et al. $(2012)$ and Terpstra et al. $(2006, 2007)$	
Retroviridae (ssRNA, E) $80 - 120$ nm	$HIV-1$	Human immunodeficiency virus 1	Relevant	Caballero et al. $(2014, Chtourou et al. (2007),$ Dichtelmüller et al. (2012), Gröner 2014 (2012), Koenderman et al. (2012), Roberts et al. (2010) and Terpstra et al. (2006, 2007)	
Herpesviridae (dsDNA, E) 180-250 nm	$SuHV-1$ (PRV)	Suid herpes virus 1 (pseudorabies virus)	HSV, CMV	Caballero et al. (2014), Chtourou et al. (2007), Dichtelmüller et al. (2012), Furuya et al. (2006), Gröner (2014), Gröner et al. (2012), Koenderman et al. (2012) and Terpstra et al. $(2006, 2007)$	

<span id="page-6-0"></span>Table 2 Main characteristics of viruses used to evaluate the viral clearance efficiency of Planova filters

 $ss$  single stranded,  $ds$  double stranded,  $E$  enveloped,  $NE$  nonenveloped

<sup>b</sup> Known to be a frequent contaminant of blood products

 $C$  HCV Hepatitis C virus, HSV herpes simplex virus, CMV cytomegalovirus

ineffective  $(LRV < 1)$  (Phillips et al. [2007](#page-32-0)). Since filtration complements other viral clearance methods in the downstream processing of biotherapeutics (Brorson [2007](#page-28-0); Klamroth et al. [2014;](#page-31-0) Shukla et al. [2007\)](#page-33-0), several studies quoted in Table [1](#page-5-0) also report LRVs for common virus reduction steps such as inactivation by pasteurization (Gröner [2014](#page-30-0); Gröner et al. [2012;](#page-30-0) Terpstra et al. [2007](#page-33-0)) or solvent/detergent treatment (Dichtelmüller et al. [2012;](#page-29-0) Terpstra et al.  $2006$ ), and chromatographic capture (Gröner  $2014$ ; Gröner et al. [2012\)](#page-30-0). Virus removal during the plasma fractionation process (Bryant and Klein [2007\)](#page-28-0) leading from the crude plasma pool to the product (immunoglobulin here) stream has also been quantified (Dichtelmüller et al. [2012;](#page-29-0) Koenderman et al. [2012](#page-31-0); Terpstra et al. [2006\)](#page-33-0). Overall virus reduction factors obtained by addition of successive LRVs are given in these works, as illustrated by Table [3.](#page-7-0)

In the virus spiking studies quoted in Table [1](#page-5-0), the actual viral filtration step was preceded by prefiltration to eliminate viral and/or protein aggregates that might be present in the spiked product solution. The presence of aggregated viruses may lead to overestimation of size exclusion effectiveness while contributing with protein aggregates to the fouling of viral filters, which reduces the membrane hydraulic permeability and may affect virus retention (Phillips et al. [2007](#page-32-0)). Pre-filtration was performed on the spike-virus stock suspension (Caballero et al. [2014](#page-28-0); Gröner et al. [2012](#page-30-0); Roberts et al. [2010](#page-32-0)) on the product intermediate before virus inoculation (Gröner et al. [2012;](#page-30-0) Koenderman et al. [2012\)](#page-31-0), and/or on the virus

Manufacturing process	Virus reduction factors $(log_{10})$					
	<b>HIV</b>	<b>BVDV</b>	<b>PRV</b>	<b>HAV</b>	Parvovirus <sup>a</sup>	
Pasteurization	>6.8	>9.3	4.7	3.9	$\geq 3.8^{\rm b}$	
Ion exchange chromatography	3.3	3.0	2.1	1.3	$3.4^\circ$	
20 N virus filtration	>6.0	> 5.8	>7.2	> 5.5	$3.4^\circ$	
Overall virus reduction factor	>16.1	>18.1	>14.0	>10.7	>10.6	

<span id="page-7-0"></span>**Table 3** Virus reduction capacity of the manufacturing process of Beriate<sup>®</sup>. Adapted from Gröner ([2014\)](#page-30-0)

<sup>a</sup> Virus reduction factor demonstrated for

<sup>b</sup> B19 V (relevant human parvovirus)

<sup>c</sup> CPV (model virus for B19V)

spiked material (Chtourou et al. [2007](#page-28-0); Dichtelmüller et al. [2012](#page-29-0); Koenderman et al. [2012;](#page-31-0) Terpstra et al. [2006,](#page-33-0) [2007](#page-33-0)). For pre-filtration of the virus preparation, micro filters with a pore size adapted to the spike virus size, i.e., slightly lower than the virus size, were used to remove cell aggregates but not single viral particles—usual pore sizes ranging between 0.1 and 0.45  $\mu$ m. Micro filters with 0.1–0.2  $\mu$ m pore size (Koenderman et al. [2012;](#page-31-0) Terpstra et al. [2007;](#page-33-0) 2006), but also 75N (Dichtelmüller et al. [2012\)](#page-29-0) and 35N (Chtourou et al. [2007](#page-28-0)). Planova viral filters were used to pre-filtrate the spiked product solution. In the latter work, the association in series of 35N and 15N filters led to efficient removal of small viruses such as PPV (Chtourou et al. [2007](#page-28-0)). This was not the case when 35N was used as the main viral filter after pre-filtration with  $75N$  (Dichtelmüller et al.  $2012$ ), which confirms previous date showing that the 35 nm pore size was too large to retain the smallest viral particles (Furuya et al. [2006](#page-29-0); Hongo-Hirasaki et al. [2006\)](#page-30-0).

Both 20N (Caballero et al. [2014;](#page-28-0) Furuya et al. [2006](#page-29-0); Gröner [2014](#page-30-0)) and 15N (Caballero et al. [2014;](#page-28-0) Roberts et al. [2010](#page-32-0); Terpstra et al. [2007](#page-33-0); 2006) Planova filters and their combination (Gröner et al. [2012](#page-30-0); Koenderman et al. [2012\)](#page-31-0) showed effective virus removal over a wide range of viral particle sizes (Table [1](#page-5-0)). As a general rule, the removal efficiency of the filters increased with the ratio of pore size to virus size, as illustrated by Gröner  $(2014)$  $(2014)$  and Terpstra et al.  $(2007)$  $(2007)$ . This was also demonstrated by Roberts et al. ([2010\)](#page-32-0) by filtrating poliovirus type 1 (a picorvanirus) through Planova filters manufactured with different pore sizes, ranging between 15  $(LRV = 6.9)$  and 35 nm  $(LRV = 0.2)$ . The two-filter combinations were globally more efficient than single filters at removing small viruses from spiked protein intermediates, though two 15N filters connected in parallel for tangential filtration (Koenderman et al. [2012](#page-31-0)) yielded LRVs quite similar to those obtained using 15N alone (Terpstra et al. [2006\)](#page-33-0). Care should be taken when comparing vertically the data collected in Table [1](#page-5-0), however. In addition to the sizes of viral particles and filter pores, the results of such virus-spiking studies are dependent on a number of process parameters such as the filtration operating conditions (filtration mode, transmembrane pressure, volume per filter area, temperature…), the characteristics of the product feed stream (pH, conductivity, nature and concentration of the product…), or else the purity level and concentration of the virus spike. Moreover, several studies include pre-filtration (Dichtelmüller et al. [2012](#page-29-0)) or viral inactivation (Koenderman et al. [2012](#page-31-0); Terpstra et al. [2006\)](#page-33-0) in the calculation of LRVs. This variability in test conditions for filtration-based virus removal makes difficult any comparison between LRVs collected from multiple sources as in Table [1](#page-5-0), even though some results (Caballero et al. [2014](#page-28-0); Hongo-Hirasaki et al. [2006;](#page-30-0) Roberts et al. [2010\)](#page-32-0) contradict its influence on filtration performance, underlining the robustness of the filtration process. Also, some variations in virus removal capacity may occur between commercial filter modules owing to their manufacture from different batches of HF, as illustrated by Roberts et al. [\(2010](#page-32-0)) for 15N filters.

## 2.2 Cellulose-fiber depth filters with inorganic filter aid

Like membrane microfiltration, depth filtration is widely used as a clarification step in biopharmaceutical purification to ensure removal of cell debris, large aggregates and contaminants from the product stream prior to purification processes such as column/membrane chromatography and viral filtration/inactivation steps (Liu et al. [2010;](#page-31-0) van Reis and Zydney [2007](#page-33-0); Vicente et al. Vicente et al. [2011a,](#page-33-0) [b](#page-33-0)). Commercially available depth filters currently employed in bioprocessing are composed of cellulose fibers with a porous inorganic filter aid and a resin binder, generally cationic. For instance, the Zeta Plus<sup>TM</sup> filter media (3 M Purification Inc.– formerly Cuno, Meriden, CT, USA) is composed of a cellulose fiber depth matrix containing silica-based filter-aid material and positively charged by chemical bounding of a cationic charge modifier (Ostreicher [1991](#page-32-0)). Varying retention ratings are available  $(0.1-1.0 \mu m)$ . The triple layered A1HC filter media from EMD Millipore include two depth filtration layers (cellu- $\log +$  diatomaceous earth) of different grades and a 0.1 lm-pore-size microporous membrane pre-filter made of mixed cellulose esters (van Reis and Zydney [2007\)](#page-33-0). Hence, these cellulosic depth filters rely on both size exclusion and electrostatic adsorptive binding to effect separation (Liu et al. [2010\)](#page-31-0). In viral spiking studies (Barnette et al. [2012](#page-27-0); Dichtelmüller et al. [2012;](#page-29-0) Zhou et al. [2008](#page-34-0)), they were found to retain viral particles whose surface is negatively charged over a wide range of pH as their isoelectric points (pI) range most frequently between 3.5 and 7.0, with a mean value of  $5.0 \pm 1.3$  (Michen and Graule [2010\)](#page-32-0).

#### 3 Viral monitoring of environmental waters

Viruses are recognized as a major cause of waterrelated disease (Bosch et al. [2008;](#page-28-0) Fong and Lipp [2005;](#page-29-0) Gibson [2014;](#page-29-0) Hamza et al. [2011\)](#page-30-0). Enteric viruses, more particularly, which are associated primarily with gastrointestinal illness (Bosch et al. [2008;](#page-28-0) Fong and Lipp [2005;](#page-29-0) Gibson [2014;](#page-29-0) Hamza et al. [2011\)](#page-30-0), are implied in most waterborne viral outbreaks (Gibson [2014](#page-29-0); Hamza et al. [2011](#page-30-0)). All types of water, including waters used for drinking (surface or ground supplies), recreational waters (fresh, marine, and swimming pool), agricultural waters for irrigation (rivers and groundwater) and waste waters (sewage or industrial effluents), have been shown to be potential vehicles for virus transmission (Bosch et al. [2008](#page-28-0)). Contamination is most frequently of fecal origin (Bosch et al. [2008](#page-28-0); Wong et al. [2012](#page-34-0)). Although viral levels may be high at the contamination source, e.g., concentrations ranging between  $10^5$  and  $10^{11}$  virus particles per gram of feces are referred to in the literature (Michen and Graule [2010](#page-32-0)), viral concentrations as low as 1–10 viral particles per liter may be found in environmental water (Julian and Schwab [2012\)](#page-31-0). Since enteric viruses display high infectivity (Fong and Lipp [2005](#page-29-0); Julian and Schwab [2012](#page-31-0)), such titers may constitute a health risk and should be detected for reliable surveillance of viral pathogens in water. As a consequence, efficient concentration methods are needed to capture viruses in large-volume water samples and release the retained viral material in concentrated form. Most common methods are based on filtration processes (Cashdollar and Wymer [2013](#page-28-0); Ikner et al. [2012](#page-30-0)). In particular, virus adsorption– elution (viradel) filter methods have been widely implemented since the 1970s (Cashdollar and Wymer [2013\)](#page-28-0). Briefly, in a viradel method, viruses from aqueous samples are reversibly adsorbed to microporous filters and then eluted from the filters in a small liquid volume (APHA, AWWA and WEF [1998](#page-27-0)). Adsorbent filters carry electrical charges and virus retention occurs via electrostatic interaction rather than by size exclusion. In other words, viradel filters act as depth filters rather than sieves. Contrary to viral filters that retain viruses by a sieving mechanism to achieve complete viral clearance, their pore size lies in the microporous range, which allows the high flow filtration necessary for virus capture in large water samples. Positively or negatively charged filters can be used in a viradel procedure, among which those made of cellulosic materials have been dominant over the last few decades.

#### 3.1 Electropositive filters

Since their pI is below the pH of natural water (i.e., around neutrality) (Michen and Graule [2010\)](#page-32-0), the surface charge of most waterborne viruses is usually negative under normal environmental conditions. Hence, electropositive filters have been logically developed to concentrate viruses in water through electrostatic adsorption. Recently used as virus-retentive prefilters in IgG manufacturing processes (Bar-nette et al. [2012;](#page-27-0) Dichtelmüller et al. [2012](#page-29-0)) (see above), the Zeta Plus<sup>TM</sup> S Series depth filter disks commercialized by 3 M Purification had also been

<span id="page-9-0"></span>



<span id="page-11-0"></span>



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II; genotype 4; Pan-1, primate calicivirus; PV-1, poliovirus type 1; MS-2, F-RNA coliphage; ØX174, somatic coliphage

 $j^k$ . See notes to Table [4](#page-9-0)

<span id="page-13-0"></span>

j J  $\overline{\phantom{a}}$ J, j  $\overline{a}$ 

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 $^{\circ}$  EV, human enterovirus; HAdV, human adenovirus; HAdV-A/-C/-F, human adenovirus species A/C/F; HAdV-40/-41, human adenovirus species F, type 40/41; HAstV, human astrovirus; HAV, hepatitis A virus; NLV GII, Norwalk-li EV, human enterovirus; HAdV, human adenovirus; HAdV-A/-C/-F, human adenovirus species A/C/F; HAdV-40/-41, human adenovirus species F, type 40/41; HAstV, human astrovirus; HAV, hepatitis A virus; NLV GII, Norwalk-like virus (norovirus) genogroup II; NoV, norovirus; NoV GI/GII, norovirus genogroup I/II; PV-3, human poliovirus type

3; ReoV, reovirus (respiratory enteric orphan virus); RV, rotavirus; RV-A, rotavirus A

<sup>f</sup> Human coxsackieviruses, echoviruses (enteric cytopathogenic human orphan viruses) and polioviruses Human coxsackieviruses, echoviruses (enteric cytopathogenic human orphan viruses) and polioviruses

<span id="page-14-0"></span>



<sup>h</sup> Water samples were spiked with a mixture of 3 viruses that were eluted together Water samples were spiked with a mixture of 3 viruses that were eluted together

i Water samples were spiked with a mixture of 5 viruses that were eluted together. Median recovery values are given Water samples were spiked with a mixture of 5 viruses that were eluted together. Median recovery values are given

<sup>1</sup> Obtained by multiplying the recovery yields of the two concentration steps evaluated separately j Obtained by multiplying the recovery yields of the two concentration steps evaluated separately

 $^k$  Calculated as (recovery yield)  $\times$  (volume reduction factor)  $\kappa$  Calculated as (recovery yield)  $\times$  (volume reduction factor)

<sup>2</sup> Springer

<span id="page-16-0"></span>



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Table 8 continued



Rigotto et al. (2010) ( $\emptyset = 142$  mm), and Haramoto et al. (2004) ( $\emptyset = 293$  mm +  $\emptyset = 47$  mm). In both methods, filters were rinsed with 0.5 mM H<sub>2</sub>SO<sub>4</sub>, pH 3.0 before virus Rigotto et al. ([2010](#page-32-0)) ( $\emptyset = 142$  mm), and Haramoto et al. ([2004](#page-30-0)) ( $\emptyset = 293$  mm +  $\emptyset = 47$  mm). In both methods, filters were rinsed with 0.5 mM H<sub>2</sub>SO<sub>4</sub>, pH 3.0 before virus elution using 1 mM NaOH (pH 10.8). In parentheses, secondary concentration step applied: CU, centrifugal ultrafiltration; PEGP, polyethylene glycol precipitation elution using 1 mM NaOH (pH 10.8). In parentheses, secondary concentration step applied: CU, centrifugal ultrafiltration; PEGP, polyethylene glycol precipitation <sup>b</sup> No MgCl<sub>2</sub> added  $^{\circ}$  No MgCl<sub>2</sub> added

° Combination of storm water and untreated sewage Combination of storm water and untreated sewage

<sup>d</sup> The average volume, total number and number of virus-positive (for at least one virus type in a mixture of viruses or for a given virus type) samples are given The average volume, total number and number of virus-positive (for at least one virus type in a mixture of viruses or for a given virus type) samples are given

<sup>e</sup> BAdV, bovine adenovirus; EV (human enterovirus); HAdV, human adenovirus; HPyV, human polyomavirus; HAstV, human astrovirus; HAV, hepatitis A virus; NoV, norovirus; NoV GI/GII/GIV, norovirus genogroup I/II/IV; NV GI/GII, Norwalk virus (norovirus) genogroup I/II; PMMoV, pepper mild mottle virus; RV, rotavirus; RV-A, BAdV, bovine adenovirus; EV (human enterovirus); HAdV, human adenovirus; HPyV, human polyomavirus; HAstV, human astrovirus; HAV, hepatitis A virus; NoV, norovirus; NoV GI/GII/GIV, norovirus genogroup I/II/IV; NV GI/GII, Norwalk virus (norovirus) genogroup I/II; PMMoV, pepper mild mottle virus; RV, rotavirus; RV-A, rotavirus A; SaV, sapovirus (Sapporo-like virus); TTV, torque teno virus rotavirus A; SaV, sapovirus (Sapporo-like virus); TTV, torque teno virus

f AiV, (Aichi virus), BKPyV (BK polyomavirus), EVs, HAdVs, JCPyV (JC polyomavirus), NoV GI/GII/GIV, RV-A, SaVs AiV, (Aichi virus), BKPyV (BK polyomavirus), EVs, HAdVs, JCPyV (JC polyomavirus), NoV GI/GII/GIV, RV-A, SaVs

<span id="page-19-0"></span>tested earlier for concentration of viruses in water samples of different origins (Table [4](#page-9-0)). More recent studies made use of Zeta Plus<sup>TM</sup> 1 MDS microfilters, however (Table [5](#page-11-0)). In these works, pure (e.g., distilled), tap, environmental or sewage water samples were seeded with varying enteric viruses that are common waterborne pathogens, i.e., members of the families Picornaviridae (polioviruses, coxsakieviruses, teschoviruses), Adenoviridae (adenoviruses), Caliciviridae (noroviruses, caliciviruses) and Reoviri-dae (rotaviruses) (Fong and Lipp [2005\)](#page-29-0), or bacteriophages (enterobacteria phages) that are considered as alternative indicators of fecal contamination and as index organisms for the presence of enteric viruses in waters (Goodridge and Steiner [2012](#page-29-0)). Naturally contaminated waters containing sufficient levels of indigenous viruses, more particularly bacteriophages, were also used in addition to spiking studies sensu stricto (Table [4](#page-9-0)). Following sample filtration, viral particles adsorbed to the filter were eluted in concentrated form using a variety of eluting solutions, the most common eluent consisting of a slightly alkaline (pH 9.0–9.5) protein solution (i.e., beef extract), frequently buffered with glycine–NaOH or another amino acid solution (sometimes supplemented with salt to aid disruption of electrostatic interactions between viruses and filters (Shields and Farrah [1983\)](#page-33-0), a chaotropic agent (e.g., urea) or a surfactant (e.g., Tween 80) to affect virus-filter hydrophobic interactions (Farrah et al. [1981\)](#page-29-0). Eluted viruses were quantified—using plaque titer assays, 50% tissue culture infectious dose  $(TCID<sub>50</sub>)$ , quantitative realtime PCR (qPCR) and reverse-transcription PCR (RTqPCR) (Hamza et al. [2011\)](#page-30-0)—to assess the recovery efficiency of the filtration step by comparing to input titers. This efficiency depends on a number of process parameters including the filter type and filtration conditions (e.g., filtration rate and pressure), the elution buffer composition and eluting conditions, the nature, input titer and titration method of the tested virus—in addition to the water matrix characteristics that may affect virus quantification and filter performance (Borchardt et al. [2013\)](#page-28-0). Hence, Tables [4](#page-9-0) and [5](#page-11-0) display a wide range of recovery yields.

In practical tests aimed at the detection of naturallyoccurring viruses in field, large-volume water samples, the filtration (adsorption–elution) step is usually a primary concentration step which is followed by a secondary one to reach the virus detection threshold,

e.g., organic flocculation (Katzenelson et al. [1976\)](#page-31-0) or PEG precipitation (Lewis and Metcalf [1988\)](#page-31-0). The recovery yield of such two-step concentration processes was evaluated in several studies using seeded or naturally contaminated water samples (Tables [4](#page-9-0), [5](#page-11-0)). As a general rule, the viral loss due to secondary concentration was balanced by a huge increase in concentration factor allowing virus detection in water concentrates from large-volume samples, as reported by Chang et al. ([1981\)](#page-28-0) and Raphael et al. [\(1985](#page-32-0)) for indigenous enteroviruses in wastewater and rotaviruses in sewage-polluted surface water, respectively. After determining the optimal elution conditions for 1 MDS disk-adsorbed noroviruses following filtration of spiked distilled water samples, Lee et al. ([2011\)](#page-31-0) (Table [5](#page-11-0)) applied the optimized procedure to the detection of noroviruses in environmental water. They combined adsorptive filtration using 1 MDS cartridge with organic flocculation to enrich viruses from largevolume surface (200 l) and ground (500 l) water samples. This integrated two-step process led to high volume reduction factors, i.e., 10,000 and 25,000 for surface and ground water samples, respectively  $(200-500\times$  for filtration,  $50\times$  for organic flocculation), but its recovery efficiency was not evaluated by spiking studies. In the same way, beside spiking



Fig. 5 Relative survivability<sup>a</sup> (RS) of MS2 viruses on filters<sup>b</sup> treated with different concentrations of DAS suspension. Error bars ( $n = 3$ ) are shown. Taken from Woo et al. ([2012\)](#page-34-0). <sup>a</sup>Ratio of the virus survival factor in the treated filter to that in the untreated filter, where the virus survival factor in a filter is the number of viruses recovered by elution from the filter divided by the number of viruses removed by the filtration process. <sup>b</sup>PF PP filter from commercial surgical mask ( $Du$ Pont<sup>TM</sup> 01361N).  $CCF$  coarse pore cellulose filter paper (Whatman<sup>TM</sup> Grade 54,  $22 \mu m$  pore size),  $FCF$  fine pore cellulose filter paper (Whatman<sup>TM</sup> Grade 50, 2.7 µm pore size)

studies like those detailed in Table [5,](#page-11-0) 1 MDS filter cartridges have been widely applied to concentrate enteric viruses in water samples of different origins (Table [6](#page-13-0)), ranging from large-volume samples of weakly contaminated water intended for drinking or drinking water production (Borchardt et al. [2003,](#page-28-0) [2004;](#page-28-0) Lee et al. [2014](#page-31-0); Sedmak et al. [2005](#page-32-0); Verheyen et al. [2009\)](#page-33-0) to wastewater samples with high viral content—to assess the virus removal efficiency of wastewater treatment plants (Kuo et al. [2010](#page-31-0); Simmons et al. [2011\)](#page-33-0). In these tests of field water samples for enteric viruses, 1 MDS filtration was mainly combined with second-stage concentration by organic flocculation as detailed by Fout et al. [\(2001](#page-29-0)) in the USEPA (United States Environmental Protection Agency) manual of methods for virology. The elution of filter-adsorbed viral particles was mostly performed with an alkaline beef extract solution supplemented or not with glycine (buffers EB3 and EB1 in Table [5](#page-11-0)). The work by Verheyen et al. [\(2009](#page-33-0)) is an exception to these common procedures. To concentrate viruses in small-volume samples from drinking water sources, these authors used two filter cartridges in series with no additional concentration step and an alkaline powdered milk solution as elution buffer. They found that 20% (3/15) and 13% (32/247) of surface and ground (well) water sources, respectively, were contaminated with adenoviruses, with very few samples positive to rotavirus (0/15 surface water samples, 6/247 well water sources). Despite the differences in virus concentration methods, these results compare with those obtained by Xagoraraki et al. ([2007\)](#page-34-0) and Cheong et al. ([2009\)](#page-28-0) for adenovirus detection in surface (14/58 samples, 24%) and ground water (4/29 samples, 14%), respectively. They also agree with data reported by Borchardt et al. ([2003\)](#page-28-0) and Cheong et al. [\(2009](#page-28-0)) showing the low contamination level of ground water by rotavirus. It is worth noting here, however, that the number of positive samples reported in these viral analyses of water (and the others quoted in Table [6\)](#page-13-0) is dependent on the sensitivity of the detection techniques used to assess the presence of viruses, i.e., nucleic acid-based amplification methods such as conventional PCR, reverse-transcription PCR (RT-PCR), nested PCR, real-time PCR/RT-PCR or integrated cell culture PCR (ICC/PCR) to determine virus infectivity (Fong and Lipp [2005](#page-29-0); Hamza et al. [2011,](#page-30-0) Mattison and Bidawid [2009;](#page-31-0) Watzinger et al. [2006\)](#page-34-0) with different detection thresholds.

It emerges from this glance at literature that cellulose-based electropositive filters are still commonly used for viral monitoring of water. These filters are expensive, however, and face competition with cheaper products, in particular nanoalumina fiber filters and glass wool filters (Cashdollar and Wymer [2013;](#page-28-0) Wong et al. [2012\)](#page-34-0). The former, NanoCeram<sup>TM</sup> filters manufactured by Argonide Corporation (Sanford, Fla., USA), are composed of nanosized (2 nm diameter), alumina-based {mainly boehmite,  $\gamma$ -AlO(OH)} fibrilles dispersed in a microglass fiber matrix, resulting in an electropositive filter media with 2–3 lm average pore size (Tepper and Kaledin [2005,](#page-33-0) [2006](#page-33-0)). The latter consist of commercial sodocalcic glass wool coated with mineral oil (type Bourre 725 QN/TECH Loose Wool, Isover Saint-Gobain, Courbevois, France), hand packed into columns or filter holders in the laboratory (Vilagines et al. [1993\)](#page-33-0). These glass wool filters harbor electropositive sites while presenting hydrophobic surface characteristics. Efficient enrichment of (seeded or/ and) indigenous viruses from various water samples using NanoCeram (Gibbons et al. [2010;](#page-29-0) Ikner et al. [2011;](#page-30-0) Pang et al. [2012](#page-32-0)), and glass wool (Deboosere et al. [2011](#page-29-0); Lambertini et al. [2008;](#page-31-0) Wyn-Jones et al. [2011\)](#page-34-0) filters has been reported in recent years (see also Cashdollar and Wymer [2013;](#page-28-0) Wong et al. [2012](#page-34-0)). Compared with 1 MDS filters (Table [5](#page-11-0)), NanoCeram filters showed similar (Lee et al. [2011\)](#page-31-0), slightly lower (McMinn [2013\)](#page-31-0) or higher (Karim et al. [2009](#page-31-0)) virus concentration efficiency.

#### 3.2 Electronegative filters

Commercially available under different pore sizes  $(0.025-8.0 \mu m)$ , mixed cellulose ester membrane filters are negatively charged over a wide range of pH values, their overall negative charge increasing with pH (Kessick and Wagner [1978](#page-31-0)). Microporous filters in the  $0.1-0.45$  µm pore size range have been used for ages in laboratory and industry for size-based filtration of bacterial particles and cell debris (surface filters). These and larger pore size filters have been shown to retain enteroviruses, however, despite the much smaller size of viral particles compared to the nominal mean diameter of filter pores (Cliver [1968](#page-28-0)). The presence of salts enhanced virus adsorption to cellulose ester membranes, this effect increasing with the cation valence (i.e.,  $Al^{3+} > Mg^{2+} > Na^{+}$ ) (Wallis et al. [1972](#page-33-0)). Acidification of the viral suspension also improved virus adsorption efficiency, even in the absence of exogenously added salts (Sobsey et al. [1973\)](#page-33-0). These early results were later confirmed by Lukasik et al. ([2000\)](#page-31-0), who investigated the influence of mono-, di-, and trivalent salts (NaCl,  $MgCl<sub>2</sub>$ , and  $AICl<sub>3</sub>$ ) on the adsorption of poliovirus and enterobacteria phages to the MF-MilliporeTM membrane filter type HA  $(0.45 \mu m)$  pore size) and the electropositive  $3M^{TM}$  Zeta Plus<sup>TM</sup> 1 MDS microfilter at neutral or acidic pH. At pH 7, salts promoted virus adsorption to HA filter while affecting adsorption to 1 MDS filter. At pH 3.5, more than 95% of the viruses tested adsorbed to HA filter with or without salt added to the viral suspension—the salts interfering again with viral adsorption to 1MDS filter. Furthermore, the addition of urea or Tween 80 to the salt solution affected virus adsorption to both filters at pH 3.5 and HA filter at pH 7. In agreement with previous studies by the same group (Haramoto et al. [2004](#page-30-0), [2005](#page-30-0); Lukasik et al. [\(2000](#page-31-0)) explained these results by the antichaotropic effect of salts that increased hydrophobic interactions between filters and viruses and was impaired by the chaotropic agent or the detergent. At neutral pH, charge screeening by salt addition reduced electrostatic attractive and repulsive forces between viruses and 1 MDS or HA filter, respectively. Cation-mediated cross-complexation between negative groups on virus and filter surfaces (Kessick and Wagner [1978\)](#page-31-0) and, more particularly, strengthened hydrophobic virusfilter interactions contributed to improving the adsorption efficiency of HA filter. At acidic pH, viruses displayed a positive surface charge and their electrostatic interactions with HA filter switched from repulsive to attractive—and inversely for electropositive 1 MDS filter. The presence of salt probably affected these interactions but was balanced by the promoting effect of salt on hydrophobic interactions.

Hence, most tests reported so far for virus concentration from water samples using cellulose ester filters (essentially HA filters) have been performed after addition of multivalent cations (mainly  $Mg^{2+}$ ) to the water samples with or without pH adjustment to an acidic level. According to Katayama et al. ([2002\)](#page-31-0), the virus-loaded filters were rinsed with an acidic solution to eliminate remaining cations before elution with NaOH or other alkaline buffers. Haramoto et al. [\(2004](#page-30-0), [2005,](#page-30-0) [2007a\)](#page-30-0) proposed a variation in the method that consisted in pre-conditioning the filter with  $Al^{3+}$  ions. Aluminum chloride was passed through the filter, making an electropositive ion coating, which avoided cation addition to the water sample. The recovery efficiency of both protocols has been evaluated by seeding water samples with enteric viruses and bacteriophages and quantifying eluted viruses (Table [7\)](#page-14-0). Similarly to spiking studies (Tables [4](#page-9-0), [5](#page-11-0)) and viral analyses of field water samples (Table [6](#page-13-0)) with electropositive filters, the HA-based filtration/elution process was frequently associated with a secondary concentration step to increase virus concentration factors. Here, centrifugal ultrafiltration  $(CU)$  using commercial Millipore (Centriprep®, Centricon<sup>®</sup> or Amicon<sup>®</sup>) concentrators was the elective concentration method. These CU units contain a low adsorptive regenerated cellulose membrane (Ultracel®) whose nominal molecular-weight cutoff ranges between 3 and 100 kDa—a MWCO value of 50 kDa being most frequently selected for secondary concentration of eluted viruses. They are routinely used in laboratories to purify and concentrate biomacromolecules such as peptides, proteins, and nucleic acids from small-volume biological samples (e.g., 2–15 ml for the Centriprep filter unit). Tested or not for virus recovery by spiking experiments, the combined concentration procedures have been extended to the detection of enteric viruses in field water samples including tap (Haramoto et al. [2004](#page-30-0)), sea (Katayama et al. [2002\)](#page-31-0), river (surface) (Fong et al. [2010;](#page-29-0) Hamza et al. [2009](#page-30-0); Haramoto et al. [2005](#page-30-0)) and waste (Fong et al. [2010;](#page-29-0) Katayama et al. [2008\)](#page-31-0) water (Table [8](#page-16-0)). Samples with different volumes were collected according to the water source, i.e., sample volumes increased as the expected contamination level decreased. For instance, Katayama et al. ([2002\)](#page-31-0) applied HA filtration, followed by acid rinse of the filter, viral elution with NaOH and secondary concentration of the eluate by CU, to concentrate naturally occurring viruses (noroviruses, enteroviruses and HAV—hepatitis A virus) in seawater samples. Based on the volume reduction factor (2-l sample/2 ml final concentrate, i.e., 1000) and the recovery yield of the two-step process (Table [7](#page-14-0)), a virus concentration factor of 670 was reached. Only HAV virus was not detected in any sample tested. Later on, Katayama et al. [\(2008](#page-31-0)) followed the same protocol to concentrate enteric viruses in the raw influent of a wastewater treatment plant. Samples of 100-ml volume were collected and submitted to the two-step concentration

process, yielding a volume reduction factor of c. 140. The four tested kinds of enteric viruses were detected in all 72 wastewater samples but one lacking norovirus GI (NoV GI). Using PEG precipitation as the secondary concentration step, Hamza et al. ([2009\)](#page-30-0) tested river water samples for contamination by enteric viruses and bacteriophages. A volume reduction factor of 5000 (10-l sample/2 ml final concentrate) and virus concentration factors ranging between 1000 (norovirus) and 5000 (adenovirus) (see Table [7](#page-14-0) for recovery yields) were obtained. All 41 analyzed samples were found positive for enteric viruses. Human adenovirus and norovirus were detected in 97.5 and 32% of the samples, respectively. Haramoto et al.  $(2004)$  $(2004)$  illustrated the ability of  $Al^{3+}$ -coated filters to concentrate viruses from large-volume freshwater samples without salt addition by detecting noroviruses in tap water from Tokyo University. Tap water samples (303-l average volume) underwent two successive filtration/elution steps using 293-mm and 47-mm diameter HA filters prior to concentration by CU (final volume: 0.9 ml), which ensured a volume reduction factor higher than 300,000. However, the virus recovery efficiency of the 3-step concentration process was not evaluated. Ten of the 98 tested samples were found positive for noroviruses. These results compare to those reported by Lee et al. ([2011\)](#page-31-0) (Table [5](#page-11-0)) using 1 MDS cartridge with organic flocculation to enrich noroviruses from large surface and ground water samples.

Despite these promising data, the two viradel methods based on electronegative filters (i.e., addition of MgCl<sub>2</sub> to water samples or filter coating with  $Al<sup>3+</sup>$ ions before filtration) have been essentially implemented for viral analysis of waters containing high amounts of indigenous viruses, requiring limited sample volumes (Table [8](#page-16-0))—electropositive filter cartridges being more adapted to virus concentration from large volumes of weakly contaminated water (Table [6](#page-13-0)). Beside the above-mentioned work by Haramoto et al. ([2004\)](#page-30-0), only two studies among those detailed in Table [8](#page-16-0) describe virus detection in environmental water samples with low viral content, namely drinking water sources after chlorination or without treatment (Rigotto et al. [2010](#page-32-0)) and groundwater from artesian wells (Chironna et al. [2012\)](#page-28-0). Both studies used small-volume samples and CU as secondary concentration step, yielding a modest volume reduction factor of 1000. Very few from 202 artesian well water samples were found positive to the tested enteric viruses: none for HAV and enterovirus, 1 for rotavirus and 4 for norovirus (Chironna et al. [2012](#page-28-0)). A large proportion (50%) of samples from drinkingwater supplies was positive to adenovirus, however (Rigotto et al. [2010](#page-32-0)). These data are compatible with viral analyses of groundwater and water intended for drinking performed using 1 MDS filtration as the first virus concentration step (Table [6\)](#page-13-0). It should be noted, however, that the same remark applies to data collected in Table [8](#page-16-0) as to those in Table [6](#page-13-0) concerning the numbers of virus-positive samples, i.e., their dependence on the virus detection method. This can be illustrated by the two following examples. Using ICC-PCR (measuring infectious viruses), Katayama et al. ([2002\)](#page-31-0) detected enteroviruses in 4 of 6 seawater samples from bathing beach, but no sample was found positive by direct RT-PCR. De Paula et al. ([2007\)](#page-29-0) found 48/52 river water samples positive for HAV by quantitative real-time RT-PCR, but only 12/52 by nested RT-PCR.

### 3.3 HF ultrafiltration

As attested by the large body of literature data quoted above, virus adsorption–elution methods using electropositive or electronegative filters are routinely applied to the primary concentration of waterborne viruses, each type of filter possessing its own advantages and drawbacks. Ultrafiltration is considered another filtration-based option to concentrate viruses from water samples (Cashdollar and Wymer [2013](#page-28-0); Ikner et al. [2012\)](#page-30-0). It has been indicated earlier that CU with microconcentrators based on cellulose ultrafiltration discs is commonly used as a secondary concentration step following the viradel process. Hollow fiber ultrafiltration (HFUF), however, is considered a potential technique for primary concentration of viruses from large-volume water samples, yielding better virus recoveries than the viradel method performed with either electropositive or electronegative filters (Cashdollar and Wymer [2013](#page-28-0)). Commercial HFUF devices operated in cross-flow mode have been applied to the simultaneous concentration of biological particles, including viruses, spiked in tap (Polaczyk et al. [2008\)](#page-32-0) or reclaimed (Liu et al. [2012](#page-31-0)) water samples, to virus recovery from seeded tap (Rhodes et al. [2011](#page-32-0)) and estuarine (Hernandez-Morga et al. [2009\)](#page-30-0) water samples, and also, more rarely, to virus recovery from field water samples (Grassi et al. [2010;](#page-30-0) Hernandez-Morga et al. [2009](#page-30-0)). Most of these devices are dialyzers that contain synthetic HF made from polysulfone. Following the early work by Belfort et al. [\(1976\)](#page-28-0) showing that polysulfone HF membranes were superior to cellulose acetate ones for virus concentration, virus concentration experiments using HFUF dialyzers equipped with HF manufactured from cellulose are scarce. An example is given by Liu et al. [\(2012](#page-31-0)). They showed that the Exeltra Plus 210 cellulose triacetate HF dialyzer (Baxter Healthcare Corp., Deerfield, IL, USA) and the Optiflux<sup>®</sup> F200NR polysulfone dialyzer (Fresenius Medical Care, Walthamm, MA, USA) provided similar recovery efficiencies for MS2 and UX174 bacteriophages, Escherichia coli, Clostridium perfringens spores, and Cryptosporidium parvum oocysts from spiked 10-l and 100-l samples of reclaimed water.

#### 4 Protection against airborne viruses

An array of viral infections can be transmitted by the airborne route, in particular via aerosols (droplet nuclei) (Coia et al. [2013;](#page-28-0) Tang et al. [2006](#page-33-0); Tellier [2006;](#page-33-0) Verreault et al. [2008](#page-33-0)). Even though virus inactivation rates in the atmosphere are generally higher than those of bacterial and fungal contaminants, virus-containing aerosols can spread worldwide (Després et al.  $2012$ ). The threat of viral outbreaks and pandemics such as those caused by SARS coronavirus (Yu et al. [2004\)](#page-34-0) and highly pathogenic strains of influenza A virus (Tellier [2006](#page-33-0)), allied with the fear of bioterrorism using viruses (e.g., smallpox and hemorrhagic fever viruses) (Barras and Greub [2014](#page-28-0)) as biological weapons, has encouraged the search for efficient protection equipment against aerosolized virus-containing particles.

Individual respiratory protective devices consist in respirators, i.e., air-filtering face masks designed to protect the wearer against inhalation of a hazardous atmosphere (here airborne infectious aerosols)—opposing to surgical masks designed to protect the environment from contaminants generated by the wearer's exhaled breath (i.e., prevention of surgical infections) (Bunyan et al. [2013](#page-28-0)). Currently, most "filtering facepiece" (FFP) respirators have a multilayer composite structure with a central filtering layer

displaying electret properties (Gralton and McLaws [2010\)](#page-29-0). These electret filters (Thakur et al. [2013](#page-33-0)) are produced by imparting an electrostatic charge to a nonwoven fibrous mat composed of synthetic polymer fibers such as poly(propylene) (PP) (mainly), poly( butylene terephthalate), poly(tetrafluoroethylene) and poly(carbonate) fibers. Electrostatic charging of the filter media is commonly obtained by corona discharge, triboelectrification and electrostatic spinning (Tsai et al. [2002](#page-33-0)). Electret filters collect particles through the combined action of mechanical and electrostatic forces (Podgórski [2010](#page-32-0); Wang [2001](#page-34-0)). Various FFP respirators are available on the market, classified according to their protection efficiency against particulate aerosols. For instance, a N95 respirator certified under NIOSH 42 CFR 84 US regulations (NIOSH [1995](#page-32-0)) and the equivalent FFP2 mask meeting the EN 143:2000 European standard (CEN [2000\)](#page-29-0) should retain respectively at least 95 and 94% of influent particles (NaCl particles are used as nonbiological surrogate particles) (Rengasamy et al. [2009\)](#page-32-0). First worn by surgical teams a hundred years ago to prevent bacterial contamination of patient's open wounds, early surgical masks were constructed from layers of cellulose materials, more particularly cotton cellulose (gauze) (Haller and Colwell [1918\)](#page-30-0) and derivatives (Arnold [1938](#page-27-0)) (see also Belkin [1997](#page-28-0)). Much more recently, face masks made from cotton fabrics have been tested as alternative respiratory protective equipment against pandemic outbreaks such as influenza (Dato et al. [2006;](#page-28-0) Davies et al. [2013;](#page-29-0) Rengasamy et al. [2010](#page-32-0)). Like respirators, current commercially available surgical face masks include several layers of non-woven fabrics with, frequently, a cellulose inner layer in contact with the wearer's face to improve wearer's comfort. However, the filtering layer, usually made of meltblown fibers (Ghosh [2014\)](#page-29-0), is devoid of electret properties. Since particulate filtration is only mechanical, i.e., less efficient than that of respirators, most surgical masks are not certified for use as respiratory protective devices, standard tests to evaluate their filtration efficacy being less stringent (Oberg and Brosseau [2008\)](#page-32-0).

While a number of studies have confirmed that surgical masks logically offer lower protection than respirators against aerosol particles, the effectiveness of both types of face masks at preventing viral respiratory infection, in particular influenza, is still a matter of controversy (Bin-Reza et al. [2012](#page-28-0); Cowling et al. [2010](#page-28-0); Gralton and McLaws [2010\)](#page-29-0). The improper facial fit of respirators (Bunyan et al. [2013](#page-28-0); Coia et al. [2013;](#page-28-0) Weiss et al. [2007](#page-34-0)) may affect their protection efficiency against infectious aerosols. It allows particulate flows outside the filtration area of the mask, resulting in face-seal leaks, i.e., the leakage of infectious particles around the edges of the mask (Grinshpun et al. [2009](#page-30-0); Lei et al. [2013\)](#page-31-0). Mask seal leakage can be minimized by applying existing guidelines for correct donning and fit checking of respirators (Coia et al. [2013\)](#page-28-0). Moreover, human face and head form models have been proposed as a tool for designing respirators with improved protection efficiency, simulating interactions between faces and facemasks and describing their fit (Golshahi et al. [2013;](#page-29-0) Lei et al. [2012\)](#page-31-0). The accumulation of viral particles at the surface and within the filtration media of respirators, where they can remain viable and infectious for extended periods of time (Coulliette et al. [2013](#page-28-0); Sakaguchi et al. [2010](#page-32-0)), is another significant problem with which respirator wearers are confronted in the prevention of viral transmission and spread. Incorrect mask handling by the wearer may lead to accidental self-inoculation, cross-contaminations affecting both other healthcare workers and patients, and contamination of fomites (Casanova et al. [2008](#page-28-0)). Furthermore, the risk of virus reaerosolization from respirators during extended use, if limited, cannot be ruled out (Fisher et al. [2012\)](#page-29-0). Recommendations for respirator doffing do exist but have proven insufficient to prevent virus transfer from respirator to healthcare employees' hands and clothing (Casanova et al. [2008](#page-28-0)). Adding antiviral properties to the filtration process may contribute to limit the risk of viral transmission by improper handling of used respirators. A number of virucidal facemasks have been developed and patented over the past 15 years (Tiliket et al. [2011](#page-33-0)), some of which are commercially available. In the SpectraShield<sup>TM</sup> Plus respirator masks designed by Nexera Medical Inc. (Fort Lauderdale, Fla.) (Haas [2008\)](#page-30-0), for instance, two layers of filter media are sandwiched between (inner and outer) antimicrobial layers where a silver–copper zeolite (carrier) antimicrobial agent (Agion<sup>®</sup> antimicrobial, Sciessent LLC, Wakefield, Mass.) is embedded around the core of synthetic fibers (Fosshield®, Foss Manufacturing, Hampton, NH). The Biofriend<sup>TM</sup> Biomask<sup>TM</sup> FFP

respirator, manufactured by Filligent Ltd. (Hong Kong) and distributed by Medline Industries, Inc. (Mundelein, Ill.), is another four-layered device in which the melt-blown PP filtration layer is inserted between an inner layer of spunbond PP and two antiviral layers, namely a cellulose/polyester layer containing copper and zinc ions and an outer layer of spunbond PP treated with a low pH (citric acidacidified) hydrophilic plastic coating (Davison [2012](#page-29-0); Stewart et al. [2014](#page-33-0)). The outer layer absorbs infectious aerosol droplets and viruses are denaturated by exposure to citric acid. In the second layer, inactivation of viruses with damaged structures is completed by the virucidal effect of divalent metal cations. Contributing to the overall antiviral efficiency of the structure, the cellulosic component of this layer is a sulphated or sulfonated rayon fabric (Stewart et al. [2012,](#page-33-0) [2014\)](#page-33-0) to which a variety of viral human pathogens bind via the cationic sites of viral envelopes/capsids.

Beside the commercial Biomask<sup>TM</sup> respirator, various composite structures designed for filtration– inactivation of airborne microbial contaminants, where cellulosic materials play an active antimicrobial role, have been patented in recent years (Baney et al. [2012;](#page-27-0) Bernard [2006;](#page-28-0) Nakamura and Nakamura [2011](#page-32-0); Tsutsumi [2009;](#page-33-0) Zhang et al. [2012;](#page-34-0) Zhong [2011](#page-34-0)). Several of them are based on bacterial cellulose layers/coatings provided with an antimicrobial component, i.e., silver (Zhong [2011](#page-34-0)) or zeolite-supported silver (Nakamura and Nakamura [2011\)](#page-32-0) nanoparticles, and chitosan (Zhang et al. [2012\)](#page-34-0). The respiratory protective mask described by Zhong [\(2011](#page-34-0)) comprises a three-layer bacterial cellulose membrane whose middle layer contains silver nanoparticles. The antimicrobial facemask invented by Nakamura and Nakamura [\(2011](#page-32-0)) includes two base cloth elements both of which are made of a woven textile (gauze), a nonwoven cellulose fabric (e.g., rayon), or a porous sheet (e.g., a 0.3–0.5 mm sliced sheet of urethane sponge). The first base cloth is filled with bacterial cellulose nanofibers that retain silver zeolite and a humectant (e.g., trehalose or 1,3-butylene glycol) in their network structure. Additional antimicrobial properties are provided to the mask by impregnating the second base cloth with a carboxylic acid (e.g., citric acid). Zhang et al. ([2012\)](#page-34-0) also used bacterial cellulose in a composite antimicrobial material suitable for respiratory protective masks. A nonwoven polymer fabric

was coated with a film of bacterial cellulose mixed with poly(vinyl alcohol)—to improve the film-forming properties, mechanical strength and air permeability of the coating—and chitosan, a non-sulfated polysaccharide produced commercially by deacetylation of chitin that displays strong antibacterial potency (Kong et al. [2010](#page-31-0); Rabea et al. [2003\)](#page-32-0) and, to a lesser extent, antiviral activity (Rabea et al. [2003;](#page-32-0) Wang et al. [2012](#page-34-0)).

In the antimicrobial air filtration device proposed by Bernard [\(2006](#page-28-0)), cellulose derivatives—more particularly, cellulose acetate phthalate (CAP), a common pharmaceutical excipient for enteric coating of tablets and capsules with antiviral activity (Pirrone et al. [2011\)](#page-32-0)—were used as ''biocidal prophylactic compounds'' to provide the classical filter media (e.g., a nonwoven PP web, electrostatically charged or not) with antimicrobial properties. Cellulose derivatives could be incorporated as fibers or particles (micronized fibers) into the air filtration device either in a separate layer positioned before or after the filter media, or deposited onto the outer surface of the filter media relative to the air flow direction. To illustrate this invention, handsheets prepared from CAP fibers intermixed or not with CAP particles were successfully tested for virucidal efficacy by exposure to an aerosol challenge of enterobacteria phage ØX174.

By exploiting the antimicrobial properties of dialdehyde polysaccharides such as starch and cellulose dialdehydes, Baney et al. ([2012\)](#page-27-0) proposed a new method for producing low-cost virucidal filters suitable for respiratory protective masks. The treatment of a standard cellulose filter paper (Whatman<sup>TM</sup> Grade 50 filter paper) with sodium periodate improved its antiviral potency due to oxidation of some cellulose to dialdehyde cellulose inside the filter. Challenged with aerosols of MS2 enterobacteria phage at high relative humidity (90% at 23  $^{\circ}$ C), the treated filter showed higher filtration efficiency than a control, untreated one, i.e., better removal of viable viral particles (Plaque Forming Units) joined to a lower resistance to air flow (pressure drop)—due to increased pore size distribution (Woo et al. [2011](#page-34-0)). Higher inactivation of MS2 virus by the treated filter was also highlighted, confirming an improvement of its disinfection capa-bility (Woo et al. [2011\)](#page-34-0). However, the filtration and inactivation of airborne viruses were less effective at lower moisture content of the filter, i.e., at air humidity levels commonly encountered in hospital settings, in

particular operating rooms (Balaras et al. [2007](#page-27-0)). Furthermore, the inhalation resistance of the treated filter remained too high for application to respiratory protective masks. The same pros and cons apply to cellulose paper filters treated by immersion into aqueous suspensions of dialdehyde starch (DAS) (Woo et al. [2012\)](#page-34-0). While this treatment did not affect the removal efficiency of viable MS2 viruses from aerosols at high relative humidity, virus survival on the treated filters was reduced (Fig. [5](#page-19-0)) and the pressure drop decreased as DAS concentration increased. The drop in air flow resistance remained insufficient for practical application to respirators. DAS treatment of a PP filter from a commercial FFP mask did not modify the filtration parameters (virus removal efficiency and pressure drop) of the filter but significantly improved its biocidal efficacy (Fig. [5](#page-19-0))—an opening of this treatment towards the development of virucidal facemasks. Another example of cellulose filter material treated with cellulose derivatives to yield antiviral properties is given by Tsurumi (Tsutsumi [2009](#page-33-0)). This inventor devised a low-cost virucidal mask filter made of a standard cellulose nonwoven fabric impregnated with water extracts of sulfonated or aminated styrenegraft cellulose. To reinforce the water retention properties of the filter media, a superabsorbent resin such as poly(acrylic acid) was added to the graft cellulose extract before impregnation of the fabric or incorporated into a separate layer covering the impregnated fabric. Low (hydrogen ions from sulfonic acid groups) or high (hydroxyl ions generated by aminated groups) pH conditions inside the hydrated material were claimed to make it virucidal against influenza A virus and caliciviruses. The patent gives no illustration of such antiviral properties, however.

Studies published by Tiliket et al. ([2011\)](#page-33-0) and Catel-Ferreira et al. [\(2015](#page-28-0)) present another type of cellulosebased material for airborne virus filtration in which a low-cost nonwoven cellulose material, i.e., commercial Kimwipes (KW) wipes (Kimberly-Clark Worldwide, Inc., Dallas, Tex.), was chemically modified by coating with a synthetic polymer, i.e., poly(ethylen-imine) (PEI) (Tiliket et al. [2011\)](#page-33-0) or grafting of an antiviral agent, i.e., catechin (Catel-Ferreira et al. [2015\)](#page-28-0). The filtration efficiency of the modified filter media was first tested on aerosolized T4D viruses (Enterobacteria phage T4, Doermann's strain T4D). Then the treated filter was inserted inside a commercial medical mask in place of its cellulosic layer (Kolmi M24001 mask, Kolmi-Hopen, Saint-Barthe´le´my-d'Anjou, France), and the reconstructed mask was challenged with TD4 aerosols to evaluate its virus removal efficiency. Both treatments significantly improved the virus capture factor (ratio of upstream to downstream PFU contents) of KW cellulose wipes and of reconstructed commercial masks compared to original masks and to masks reconstructed with untreated wipes. In these studies, the breathability of reconstructed masks was not quantified, nor was the virus survivability on the modified filter media. However, additional filtration experiments using aerosols of influenza A virus (low pathogenic H5N2 strain) showed that challenged viral particles accumulated in PEI functionalized KW layers with no loss in number and infectivity (Tiliket et al. [2011\)](#page-33-0). Thus these modified masks showed no virucidal effect, the PEImodified layers behaving like an electret media owing to the polycationic character of PEI. On the other hand, since catechin and catechin-grafted wipes showed antiviral activity against T4D viruses in liquid media (Catel-Ferreira et al. [2015](#page-28-0)), it may be assumed that part of viruses accumulated in excess in the treated wipes were inactivated by the polyphenol agent, i.e., the reconstructed masks were actually virucidal.

Despite these few examples, the use of cellulosic media in filtration devices aimed at the capture of airborne viral particles remains now very limited compared to filtration of virus-contaminated liquid samples. While patented, several cellulose-based, virucidal filter media designed for insertion in air filtering face masks have not been commercially developed yet.

Besides the wearing of personal respiratory protective equipment, another aspect of the fight against airborne infections lies in the decontamination of indoor air in healthcare facilities, and, more generally, of air processed through heating, ventilating and air conditioning (HVAC) systems in the built environment. High Efficiency Particulate Air (HEPA) filters are the primary technology used for particulate removal in these collective protection devices—allied with UV irradiation, ozonation or air ionization to yield indoor air decontamination (Bolashikov and Melikov [2009;](#page-28-0) Jacob et al. [2013](#page-30-0))—and may be complemented with a photytocatalyst such as  $TiO<sub>2</sub>$ to improve the inactivation of accumulated microorganisms (Chen et al. [2010](#page-28-0); Pigeot-Remy et al. [2014](#page-32-0)). Since HEPA filters are essentially made of glass fibers, they are beyond the scope of this review and their virus-retentive properties will not be detailed further.

### 5 Conclusion

Most frequently associated with other virus reduction (virus clearance of biopharmaceuticals) or concentration (viral analysis of water) steps, size-exclusion and/ or adsorptive (charge mediated) filtration is an essential tool to fight against viral contaminants in aqueous media. Owing to inherent properties of cellulose, including mechanical strength and hydrophilicity (that opposes protein adsorption and biofouling), allied with widespread availability and biocompatibility, cellulose-based materials are still widely present in viral filters. Developed commercially over the past thirty years, several cellulosic filter media have been and continue to be used for both routine analyses in laboratories and academic research studies aimed at improving the filtration performance, generating a wealth of data quantifying the efficiency of virus removal or recovery/concentration from biologic or water samples, respectively.

As concerns biopharmaceutical compounds, these data arise from validation studies of the filtration step performed by spiking intermediate biologic solutions (mostly blood proteins) from multistage purification processes with known titers of viral particles. Regenerated cellulose HF Planova filters N15–N35, operated in the dead-end mode as a single filter or two units in series, were shown to provide LRV values ranging between 4 and 7, on the average. Increasingly tested since their launching in 1989, these cellulosic filters compete with filter media made of synthetic polymers such as PVDF (e.g., Viresolve<sup>®</sup> NFP—Normal Flow Parvovirus—from EMD Millipore; Ultipor<sup>®</sup> VF Grade DV20/DV50 from Pall Corporation, Port Washington, NY) or PES (e.g., Millipore Viresolve<sup>®</sup> Pro; Virosart<sup>®</sup> HS/HC/CPV from Sartorius Stedim Biotech, Aubagne, France). The hydrophilic nature of cellulose fibers is a definite advantage of Planova filters over others for virus removal from protein solutions, minimizing flux decline due to proteindominated filter plugging (cake formation) at constant pressure (normal-flow) filtration (Rathore et al. [2014](#page-32-0)). However, they are usually operated at lower flow rate than filters made of synthetic polymers whose operating pressure is higher. Hydrophilic modified PVDF <span id="page-27-0"></span>membrane filters designed for virus removal from high-concentration protein solutions at high flow rate are being developed by several manufacturers, including Asahi-Kasei (i.e., Planova<sup>TM</sup> BioEX filters, launched in 2009).

Many studies have also been reported to assess the virus concentration efficiency of the viradel method using spiked water samples, prior to the detection of waterborne viral contaminants in field water samples. In this method, cellulosic filters, whether positively or negatively charged, are used for adsorptive capture of viruses before virus recovery by elution with a lowvolume eluent. Electropositive filters are more particularly suitable for virus capture in low-contaminated, high-volume water samples, e.g., samples of groundwater or source water for drinking water production (Table [6](#page-13-0)). Though routinely used, these filters are expensive and face competition with nanoalumina fiber filters (e.g., the patented Ahlstrom Disruptor electroadsorptive filter) (Levi [2011](#page-31-0)) and glass wool filters, which are cheaper. On the other hand, efficient virus adsorption by electronegative filters—the standard, cost-effective mixed cellulose ester membrane microfilters—requires impractical sample pre-treatment: their use is limited to viral analysis of highlycontaminated waters, for which small-volume samples are sufficient (Table [8](#page-16-0)).

Cellulose nanomaterials may represent a promising perspective for cellulosic materials in their application to viral filtration of liquid samples, yielding filtration membranes with higher mechanical strength, water permeability, surface hydrophilicicy and resistance to biofouling (Carpenter et al. [2015\)](#page-28-0). Ma et al. ([2011\)](#page-31-0) have presented a composite membrane consisting of an electrospun poly(acrylonitrile) nanofibrous scaffold deposited on a non-woven poly(ethylene terephthalate) support. This two-layered membrane was coated by a layer of cellulose nanofibers and tested for retention of MS-2 phages. At acidic pH, phage particles were adsorbed by the negatively charged cellulose nanofiber coating, yielding a LRV value  $>3.7$ . Later on, the same nanofibrous composite membrane was doped with cellulose nanofibers functionalized by grafting with poly(vinylamine) (Wang et al. [2013](#page-34-0)). MS-2 phages were adsorbed at neutral pH onto positively charged amino-modified nanofibers, with a LRV value of 4. Metreveli et al. ([2014\)](#page-31-0) and Asper et al. (2015) have presented a size-exclusionbased filter paper made of pure cellulose nanofibers for

removal of swine influenza A and murine leukemia viruses, respectively. These non-woven materials could be tailored to ensure efficient virus retention (Gustafsson and Mihranyan [2016a](#page-30-0)). Self assembled into nanosheets to yield ''mille feuille'' structures, they showed efficient removal of parvoviruses (Gustafsson et al. [2016b](#page-30-0)): maybe a new filtration media for viral clearance?

A number of air filtration devices designed for individual protection against airborne viruses also include cellulosic materials. While published data on the filtration performance of cellulosic media for removal of viruses from air are scarce, industrial research is more apparent, in particular in Asian countries (China, Japan) where airborne pollution is a matter of great concern—the main objective being to add virucidal properties to the filtration media so as to inactivate accumulated viral particles. Therefore, some innovative media have been patented over the past few years with, however, no commercial development to date.

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