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### EXPLORING IN VIVO PLACENTAL MICROSTRUCTURE IN HEALTHY AND GROWTH-RESTRICTED PREGNANCIES THROUGH DIFFUSION-WEIGHTED MAGNETIC RESONANCE IMAGING

Nickie ANDESCAVAGE, MD<sup>1,4</sup>, Wonsang YOU, PhD<sup>2</sup>, Marni JACOBS, PhD<sup>3,4</sup>, Kushal KAPSE, MS<sup>2</sup>, Jessica QUISTORFF, MPH<sup>2</sup>, Dorothy BULAS, MD<sup>2,5</sup>, Homa AHMADZIA, MD<sup>6</sup>, Alexis GIMOVSKY, MD<sup>6</sup>, Ahmet BASCHAT, MD<sup>7</sup>, Catherine LIMPEROPOULOS, PhD<sup>2,4,5</sup>

<sup>1</sup>Division of Neonatology, Children's National Health System, 111 Michigan Ave. NW, Washington, DC 20010

<sup>2</sup>Division of Diagnostic Imaging & Radiology, Children's National Health System, 111 Michigan Ave. NW, Washington, DC 20010

<sup>3</sup>Division of Biostatistics & Study Methodology, Children's National Health System, 111 Michigan Ave. NW, Washington, DC 20010

<sup>4</sup>Department of Pediatrics, George Washington University School of Medicine, 2300 Eye St. NW, Washington, DC 20052

<sup>5</sup>Department of Radiology, George Washington University School of Medicine, 2300 Eye St. NW, Washington, DC 20052

<sup>6</sup>Division of Maternal Fetal Medicine, Department of Obstetrics and Gynecology, George Washington University School of Medicine, 2300 Eye St. NW, Washington, DC 20052

<sup>7</sup>Department of Gynecology and Obstetrics, Johns Hopkins Center for Fetal Therapy, 600 North Wolfe Street, Nelson 228, Baltimore, MD 21287

#### Abstract

**Introduction**—Gross and microstructural changes in placental development can influence placental function and adversely impact fetal growth and well-being; however, there is a paucity of in-vivo tools available to reliably interrogate in vivo placental microstructural development. The objective of this study is to characterize in-vivo placental microstructural diffusion and perfusion in healthy and growth-restricted pregnancies (FGR) using non-invasive diffusion-weighted imaging (DWI).

Corresponding Author: Catherine Limperopoulos, Ph.D., Children's National Health System, 111 Michigan Ave. NW, Washington, D.C. 20008, climpero@childrensnational.org, Tel: 202-47605293.

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**Methods**—We prospectively enrolled healthy pregnant women and women whose pregnancies were complicated by FGR. Each woman underwent DWI-MRI between 18 and 40 weeks

gestation. Placental measures of small (D) and large (D\*) scale diffusion and perfusion (f) were estimated using the intra-voxel incoherent motion (IVIM) model.

**Results**—We studied 137 pregnant women (101 healthy; 36 FGR). D and D\* are increased in late-onset FGR, and the placental perfusion fraction, *f*, is decreased (p<0.05 for all).

**Discussion**—Placental DWI revealed microstructural alterations of the in-vivo placenta in FGR, particularly in late-onset FGR. Early and reliable identification of placental pathology *in vivo* may better guide future interventions.

#### Keywords

Placenta; fetal growth restriction (FGR); magnetic resonance imaging (MRI); diffusion weighted imaging (DWI); intra-voxel incoherent motion analysis (IVIM)

#### Introduction

Placental insufficiency deprives the developing fetus of essential metabolites necessary for normal growth and brain development, resulting in fetal growth restriction (FGR). FGR remains a leading cause of stillbirth and a major risk factor for premature birth, cerebral palsy and lifelong morbidity (1–3). Despite advances in fetal diagnostic techniques, there are few current clinical tools that directly and noninvasively assess placental function in utero, often presenting late in placental dysfunction (4, 5). Similarly, despite histopathology descriptions of altered placenta development in FGR, there are no current clinical tools to assess in vivo microstructural development of the placenta (6, 7).

Diffusion-weighted magnetic resonance imaging (DW-MRI, or DWI) measures the movement of water molecules in a given space. In the human body, the molecular diffusion of water is impacted by cell membranes, tissue cellularity and the extracellular space, resulting in decreased diffusion across areas of increased tissue cellularity (8). These principles have been used in biomedical imaging to provide clinical insight into local microstructural integrity, without the need for invasive measures or exogenous contrast (8). The intravoxel incoherent motion (IVIM) analysis approach of DWI capitalizes on differences in tissue organization and the vascular system to inform microstructural development, namely tissue cellularity and microcirculation of a given region (9). The primary metrics of IVIM include (a) the diffusion coefficient, D, an estimate of small-scale diffusion, reflective of tissue cellularity, (b) the pseudo-diffusion coefficient, D\*, an estimate of large scale diffusion and microcirculation of regional capillary networks and (c) the perfusion fraction, f, the percent of moving blood volume in a given region.

DWI and IVIM analyses have also been applied to the study of the human placenta, and revealed regional abnormalities in the perfusion fraction in high-risk pregnancies (10–12). However much less is known about changes in placental water diffusion through-out pregnancy, either in healthy or pathologic states. The objective of this study was to delineate the in vivo diffusion properties of the human placenta in pregnancies with established fetal growth restriction (FGR) as well as healthy, uncomplicated pregnancies to explore in vivo

placental microstructure. We hypothesized that placental perfusion fraction and diffusion coefficients would be reduced in FGR compared to healthy controls due to microstructural alterations in the growth-restricted placenta, evidenced by postnatal histopathology that show inflammatory changes in villous development, as well as vascular changes including thrombosis and infarction in early- and late-onset FGR (7, 13). Furthermore, we hypothesized that diffusion properties would differ in distinct sub-groups of FGR, reflecting the pathologic differences in functional and microstructural placental development across high-risk populations (14).

#### Methods

#### Subjects

We recruited pregnant women with singleton pregnancies after 18 weeks gestation as part of a longitudinal prospective observational study at Children's National Health Systems (CNHS) which includes up to two detailed fetal-placental evaluations through advanced MRI, neonatal evaluations and long-term follow-up of this cohort through early childhood. This study is designed as a cross-sectional analysis of placental development from the first fetal-placental evaluation using IVIM. A pregnancy was considered complicated by FGR if the estimated fetal weight was < 10th centile from standard sonographic measures (15) and there was no evidence of congenital anomalies or infections; FGR cases were excluded if there was evidence of congenital infections or dysmorphic features. Healthy controls had no significant past medical history, without chronic or pregnancy induced illnesses, including normal screening studies at the time of enrollment. Exclusion criteria for either group included any maternal contraindications to MRI for either group. The study was approved by the hospital's Institutional Review Board and written informed consent was obtained from all participants.

#### Imaging: MRI acquisition

All women underwent the same MRI imaging protocol on a 1.5T Discovery MR450 scanner (GE Healthcare, Milwaukee, Wisconsin) using an 8-channel cardiac array (receive only) coil (USAI, Aurora, OH). Pregnant women were positioned in the left lateral or supine position, based on maternal preference for their comfort. The coil array was positioned covering the entire abdomen and pelvis to improve spatial resolution.

Dedicated anatomic single shot fast spin echo (SSFSE) fat suppressed T2-weighted images were acquired in the maternal axial or coronal plane for full placental coverage (TE=160ms, TR=1100ms, 4mm slice thickness). Pulsed gradient spin echo (PGSE) sequences were acquired (TE =53.8 ms, TR=8000 ms, data matrix size 96×96, filed of view (FOV)  $420\times420$ mm<sup>2</sup>, 4mm slice thickness) with the following b-values: 0, 25, 50, 114, 243, 500, 543, 800, 900 sec/mm<sup>2</sup>, diffusion time=25ms. Each MRI was reviewed by a pediatric radiologist to evaluate for placental malformations.

#### Imaging: Post-processing

Manual delineation of the region of interest (ROI) for the entire placenta was created on the b value of 25sec/mm<sup>2</sup> of the PGSE sequence, using ITK-SNAP. The corresponding T2

weighted image was used as anatomical reference (Figure 1) using the amniotic space as the fetal boundary and the internal uterine wall as the maternal boundary. The diffusion weighted signals were averaged over the entire ROI and IVIM parameters were calculated from the averaged signals.

Motion correction between volumes was performed using the image registration toolkit (IRTK) (26). We then performed an intravoxel-incoherent motion (IVIM) analysis to measure the diffusion coefficient (D, estimate of small scale diffusion), pseudo-diffusion coefficient (D\*, estimate of large scale diffusion) and the perfusion fraction (*f*, percent of moving blood volume).

#### Sonography

All pregnancies complicated by FGR underwent complete fetal sonographic assessment of both anatomy and Doppler evaluation as part of the study protocol on the same day as the MRI study using a LOGIQ E9 ultrasound scanner (GE Healthcare, WI). Abdominal circumference, head circumference, femur length and estimated fetal weight were measured and plotted according to gestational age GA (15). Fetal middle cerebral (MCA) and umbilical arterial (UA) flow velocities were measured using a pulse-wave Doppler, and pulsatility indices (PI) were calculated. The cerebroplacental ratio (CPR) was calculated by dividing the middle cerebral artery pulsatility index by the umbilical artery pulsatility index (27). Subjects were classified into the sub-group of abnormal Doppler studies if the CPR was less than 1 (28). All sonographic studies were reviewed by a single attending radiologist as per institutional protocol.

Healthy control pregnancies underwent complete fetal echocardiographic assessment using a Vivid 7 ultrasound scanner (GE Healthcare, Waukesha, WI) as part of an adjunct prospective study. Fetal middle cerebral and umbilical arterial flow velocities were measured using a pulse-wave Doppler; pulsatility indices, CPR and z-scores (derived from normal references) were calculated (28).

#### **Clinical data**

Clinical and demographic data were extracted from the maternal and neonatal charts, including race, ethnicity, maternal co-morbidities, fetal sex, and gestational age at study. Neonatal outcomes included gestational age and birthweight at delivery. Available placental pathology reports were also extracted from the medical record, and scored as normal or abnormal, based on pathology report.

#### **Biostatistics**

Group comparisons between FGR and controls were evaluated by independent samples t-test or independent chi-square as appropriate. Linear and non-linear associations between IVIM measures and GA at study, maternal age, birth weight and GA at birth, alone and by fetal sex, were evaluated using generalized linear regression; quadratic terms were included in models to evaluate non-linear associations. Additional adjustments for potential comorbidities were evaluated and subsequently accounted for in diffusion and perfusion fraction analyses, including maternal age, fetal gender and GA at MRI, using ANCOVA.

Least squares means estimates were used for pairwise comparisons. Categorical outcomes for normal-abnormal placental pathology reports within FGR cases were analyzed via independent samples t-test. Associations with neonatal outcomes were also investigated. SAS 9.4 software was used for all analyses (29); a two-tailed p-value of 0.05 was considered significant.

#### Results

#### Subjects

We studied 137 pregnant women, 101 recruited as normal controls and 36 with FGR. In the control group, 94 women delivered term, appropriate for gestational age (AGA) infants, 3 (2.97%) delivered preterm, and 4(3.96%) delivered small for gestational age (SGA) infants, with birth weights  $< 10^{\text{th}}$  centile. Only the 94 healthy women with term, AGA infants were included for the group analyses between controls and FGR cases in order to compare FGR to true healthy controls, while the full cohort of 101 healthy recruits were included in the neonatal outcomes analysis to fully evaluate associations with placental diffusion. Women diagnosed with FGR were further categorized into (1) early onset and late onset (diagnosed in second vs. third trimester), (2) those with or without abnormal Doppler studies of the fetal circulation (namely, CPR < or > 1), and (3) significant maternal comorbidities. Five FGR cases (14%) were noted to have maternal hypertensive disorders (chronic hypertension, gestational hypertension and preeclampsia) and there were no cases of FGR with maternal diabetes mellitus or autoimmune disorders. Of the five FGR cases with maternal hypertensive disorders, 3 also had a CPR <1.0 at the time of evaluation. Approximately onethird (31%) of pregnancies were diagnosed early (in the second trimester) while the remainder were diagnosed in the third trimester and 41.6% of FGR cases overall had abnormal Doppler studies. Additional clinical characteristics are noted in Table 1.

#### Small-scale water diffusion (D) comparisons in healthy versus FGR pregnancies

Average small-scale water diffusion among healthy controls with normal birth outcomes was  $1.76 \times 10^{-3} \text{ mm}^2/\text{s}$ , with a negative association between D and advancing gestational age ( $\beta$ = -0.01, p=0.06) (Supplementary Figure 1). While there was no significant difference in D between controls and FGR cases overall, there was a significant *increase* in D in late-onset FGR compared to controls and to early-onset FGR (Table 2). D was associated with pregnancy outcome diffusion was associated with gestational age at birth (non-linear association, p=0.05 Figure 2)..

#### Large-scale water pseudo-diffusion (D\*) comparisons in healthy versus FGR pregnancies

Average D\* among healthy controls with normal birth outcomes was  $36.80 \times 10^{-3} \text{ mm}^2/\text{s}$ , with no significant association between D\* and advancing gestational age). There was no significant difference in D\* between controls and FGR cases overall,, however D\* was greater in late-onset FGR compared to controls (Table 2).

 $D^*$  was associated with pregnancy outcome with a similar non-linear association with gestation age at birth (p=0.05 Figure 3) as well as birth weight (p=0.15).

#### Perfusion Fraction, f

The average perfusion fraction among healthy controls with normal birth outcomes was 40.65%,. Overall, pregnancies complicated by FGR had lower perfusion fraction compared to controls, even when accounting for GA at the time of evaluation (p=0.19) (Table 2). Interestingly, late-onset FGR had the lowest perfusion fraction when compared to controls or early-onset FGR (Table 2). We did not detect any association with placental perfusion fraction and pregnancy outcomes, namely gestational age at birth weight, or birth weight.

#### IVIM measures and placental pathology in FGR pregnancies

Placental pathology reports were available in the medical records for 22 subjects with FGR (61%). Eighty-two percent of the placentas were noted to weigh less than the  $3^{rd}$  centile for gestational age (30) and 68% had noted abnormalities in thrombi, fibrin deposition, inflammatory changes and accelerated villous maturation. However, there were no significant associations between IVIM measures of D, D\* and f and pathology findings (p = 0.59–0.80).

#### Discussion

#### **Principal Findings**

Despite several formative studies describing placental perfusion in the human pregnancy through DWI, the microstructural properties of the *in vivo* placenta remain poorly understood (10, 11, 31–35). In this work, we use DWI to report on microstructural development of the in vivo human placenta in a large cohort of healthy women with normal pregnancy outcomes, as well as pregnancies complicated by FGR. We show placental diffusion, pseudodiffusion and perfusion fraction are significantly different in late-onset FGR, which has not been previously reported. There were no significant differences in placental microstructure for pregnancies complicated by FGR with a CPR <1, though D, D\* and f trended lower in this group. Similarly, pregnancies complicated by FGR with maternal hypertensive disorders trended lower in D and D\*, with similar f, although again, these did not achieve statistical significance.

#### Principles of Diffusion Weighted Imaging and Placental Interpretations

Diffusion of water molecules in biologic tissues is primarily constrained by cell membranes and macromolecules (8). In biomedical imaging, decreased small-scale diffusion is largely interpreted to indicate increased cellular density or regional fibrosis (36), while large-scale pseudo-diffusion represents the diffusion of water molecules in blood, or the microcirculation (36). It is important to note that the application and interpretation of IVIM in the placenta has not been fully delineated or validated with ex vivo pathology. However, extending these basic principles of DWI and IVIM suggests that in the placenta, water movement would be most constrained within the highly cellular villi, and least constrained within the open intervillous space. Similarly, it is also worthwhile to note that there is likely significant correlation between pseudo-diffusion (D\*) and the moving blood fraction (f) given the relatively open areas of the intervillous space. However, despite these limitations, the in vivo findings of this study coupled with known pathological changes in placental insufficiency are in line with these interpretations.

#### Lessons from Placental Histopathology & Clinical Outcomes

Characterizing placental pathology has been challenging due to both variability in clinical and histopathologic definitions, as well as the wide variety of lesions described within a single clinical entity (37, 38). The pathology of late-onset FGR is not as well understood as other forms of FGR. Histologically, placental changes are much more variable and often time, unremarkable in late-onset FGR (39). If placental changes are noted, there is an increased incidence of vascular lesions, including infarction. In this study, late-onset FGR was significantly associated with increased small-scale and large-scale water diffusion of the placenta. In addition, late-onset FGR had the most significant reduction in *f*, or the percent of moving blood, which may result from such vascular lesions. However, further studies are needed to better understand the pathologic changes in the placenta of late-onset FGR and the relationship with these in vivo DWI findings.

Conversely, maternal vascular underperfusion, common in preeclampsia-eclampsia and FGR, is characterized by placental hypoplasia grossly, and by villous hypoplasia and accelerated villous maturation histologically (40–42). Conversely, there are reports of *increased* placental weight associated with decreased distal villous hypoplasia in preeclampsia (43). Likewise, villous hypoplasia has been described in both early-onset FGR and pregnancies with abnormalities of umbilical artery resistance, as seen with reduced CPR (39, 44). Interestingly, there is one report of 5 cases of maternal vascular underperfusion and retrospective analysis of placental DWI that revealed reduced diffusion compared to placental diffusion in normal pregnancies (45). Similarly, our data suggests reduced small-scale diffusion through IVIM analysis in our cohort of FGR cases with maternal hypertensive disorders, including preeclampsia. There is a similar suggestion of decreased small-scale diffusion in early-onset FGR and FGR cases with decreased CPR.

While the cellular mechanisms that may explain these findings are unclear, our data suggests that IVIM may provide insight into *in vivo* microstructural and microvascular development. Furthermore, there appears to be an optimal range of diffusion and pseudo-diffusion parameters, as measure by IVIM analyses, associated with birth outcomes, including term birth with normal birth weights.

#### **Strengths and Limitations**

In this work, we show that DWI can detect important differences in the placenta of growthrestricted pregnancies when compared to healthy controls, particularly in late-onset FGR, with notable trends in FGR with decreased CPR or FGR with MHD. Despite the many strengths of this work, there are important limitations that deserve mention. First, while IVIM analysis can distinguish differential diffusion properties across tissue classes, it is highly dependent on the number and range of b values acquired (9). While our MRI acquisition protocol was sensitive enough to detect important differences in healthy and high-risk pregnancies, the optimal sequences, correction methods and analysis models for placental diffusion remain to be determined (46). Secondly, the objective of this study was to

characterize placental diffusion and perfusion in high-risk pregnancies with established FGR.

However, as discussed throughout the manuscript, there are multiple pathologic pathways that can converge to result in fetal growth anomalies. While our data suggests that IVIM may be able to distinguish between early- and late-onset FGR, some of the sub-group analyses were limited by the smaller sample sizes – particularly pregnancies complicated by FGR with MHD. Nonetheless, these data present intriguing trends that should be further studied in larger cohorts of individual high-risk conditions. Similarly, we were unable to identify any significant relationships between in vivo placental development and ex vivo histopathology. The temporal evolution of placental development and disease from the point of imaging to the point of delivery and pathology evaluation may have confounded our findings. However, these analyses were further limited by the retrospective data collection of the pathology reports. Nonetheless, relating these findings prospectively with planned placental pathology evaluations is needed to validate these findings, as well as the proposed interpretations. Lastly, while we were able to identify important relationships between in vivo placental water diffusion and birth outcomes, the predictive validity and clinical relevance of these findings require confirmation in larger cohorts and with long-term neurodevelopmental outcome. These studies are currently underway.

#### Conclusions

While advances in prenatal care have improved pregnancy outcomes and fetal mortality, there remain significant limitations in identifying early and sensitive biomarkers of placental health (47–49). In this work, we proposed that in vivo placental microstructure can be assessed with diffusion weighted imaging, and identify potential markers of aberrant placental development in high-risk pregnancies. Once mechanisms of placental growth and function become better established, future screening, surveillance and treatment can be tailored to individual maternal-fetal dyads and improve short- and long-term pregnancy outcomes.

#### Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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#### Abbreviations

FGR	fetal growth restriction
MRI	magnetic resonance imaging
DWI	diffusion weighted imaging

IVIM	intra-voxel incoherent motion anlaysis
D	diffusion coefficient
D*	pseudo-diffusion coefficient
f	perfusion fraction

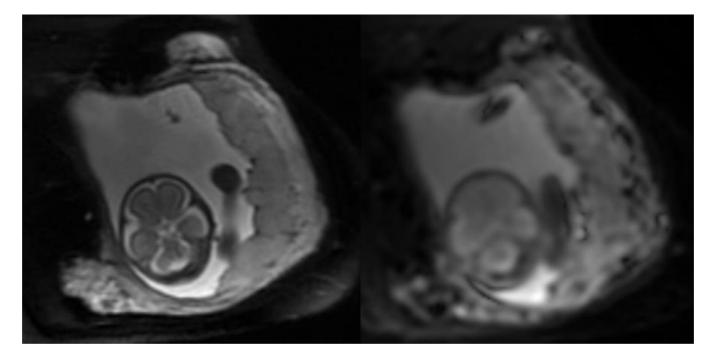
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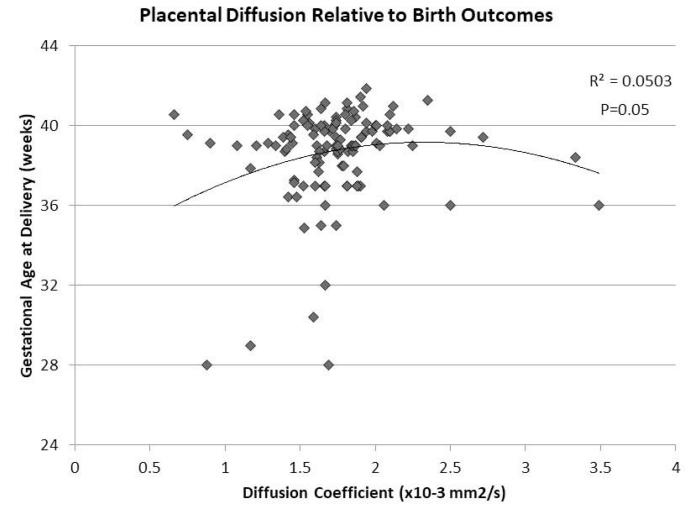
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- Placental dysfunction can impact both maternal and fetal well-being
- Histologic changes in placental development have been described in fetal growth restriction
- Microstructural changes of the placenta remain difficult to identify *in vivo*
- Diffusion weighted magnetic resonance imaging is used to described *in vivo* microstructure
- Small scale diffusion and the perfusion fraction of the *in vivo* placenta is reduced in fetal growth restriction



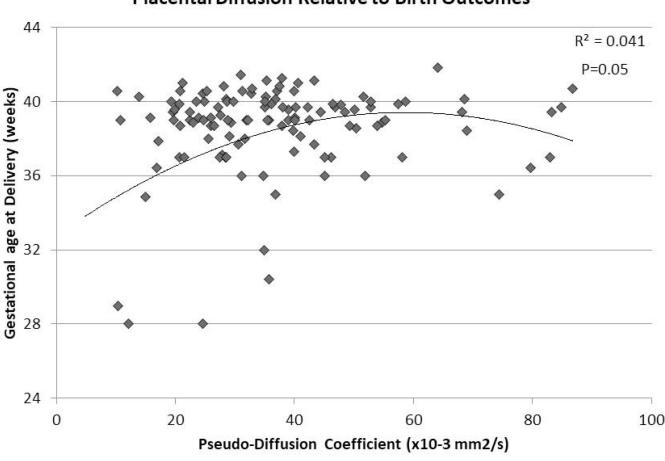
#### Figure 1:

Example of magnetic resonance images (MRI), including the T2Weighted anatomic image of the placenta (A), and the corresponding Diffusion weighted image (DWI) (b0 acquisition) (B) at 25 weeks gestation.



#### Figure 2:

The diffusion coefficient (D) of the *in vivo* placenta through IVIM analyses of DWI and pregnancy outcomes; namely gestational age at birth.



#### **Placental Diffusion Relative to Birth Outcomes**

#### Figure 3:

The pseudo-diffusion coefficient (D\*) of the *in vivo* placenta through IVIM analyses of DWI and pregnancy outcome; namely gestational age at.

# Table 1:

Clinical Characteristics

Maternal Age (years) $29.9 \pm 6.9$ Gestational Age at MRI (weeks) $29.1 \pm 5.8$ Fetal Gender, Male (n, %) $52 (51.5\%)$	6.9 5.8	cy + LVc	
Age at MRI (weeks) r, Male (n, %)	5.8	7.0 - 7.17	0.10
r, Male (n, %)		$31.0 \pm 3.8$	0.07
	5%)	13 (36.1%)	0.17
Neonatal Data			
Gestational Age at birth (weeks) $39.35 \pm 1.55$	1.55	$36.91 \pm 3.19$	0.0001
Birth weight (grams) $3288 \pm 438$	438	$2312 \pm 663$	0.0001
Birth weight (z-score) $-0.18 \pm 0.77$	0.77	$-1.52\pm0.73$	0.0001

# Table 2.

Placental diffusion metrics across healthy and high-risk pregnancies

Small Scale Diffusion (D*) $1.76$ $1.74$ $1.74$ $1.74$ Large Scale Pseudo-Diffusion (D*) $36.80$ $36.80$ $34.14$ $34.14$ $36.80$ $34.14$ $36.80$ $34.14$ $36.80$ $36.80$ $36.80$ $36.80$ $36.16$ $37.68$ $37.68$ $37.68$ $37.68$ $37.68$ $37.68$ $37.68$ $37.68$ $37.68$ $37.68$ $37.64$ $39.42^{d}$ $39.413^{d}$ $39.413^{d}$		Control (n=97)	FGR (n=36)	1=36)	p-value <sup>a</sup>
$36.80$ $34.14$ $40.65$ $37.68$ $40.65$ $37.68$ $7.05$ $37.68$ $1.76$ $1.50$ $1.76$ $1.50$ $1.76$ $1.50$ $1.76$ $1.50$ $36.80$ $23.56$ $36.80$ $23.56$ $36.80$ $23.56$ $40.65$ $45.94$ $40.65$ $45.94$ $7.76$ $34.13^c.d$ $7.76$ $34.16^c.d$ $7.76$ $38.51$ <tr< td=""><td>Small Scale Diffusion (D)</td><td>1.76</td><td>1.7</td><td>4</td><td>0.76</td></tr<>	Small Scale Diffusion (D)	1.76	1.7	4	0.76
$40.65$ $37.68$ Control (n=97)         Early-Onset FGR (n=11)         Late-Onset FGR (n=25) $1.76$ $1.50$ $1.87^{c.} d$ $36.80$ $23.56$ $39.42^{d}$ $36.80$ $23.56$ $39.42^{d}$ $36.80$ $23.56$ $39.42^{d}$ $40.65$ $45.94$ $34.13^{c.} d$ $1.76$ $1.82$ $1.66$ $1.76$ $1.82$ $1.66$ $1.76$ $1.82$ $1.66$ $1.76$ $1.82$ $1.66$ $36.80$ $37.51$ $29.23$ $36.80$ $37.51$ $29.23$ $40.65$ $37.60$ $38.51$ $20.0000$ $1.70$ $1.66$ $1.76$ $1.79$ $29.23$ $1.76$ $38.51$ $29.23$ $36.80$ $37.50$ $38.51$ $1.76$ $1.79$ $1.66$ $1.76$ $1.79$ $1.50$ $1.76$ $23.07$ $23.07$	Large Scale Pseudo-Diffusion (D*)	36.80	34.	[4	0.42
Control (n=97)         Early-Onset FGR (n=11)         Late-Onset FGR (n=25) $1.76$ $1.50$ $1.87^{c.} d$ $36.80$ $23.56$ $39.42^{d}$ $36.80$ $23.56$ $39.42^{d}$ $40.65$ $45.94$ $34.13^{c.} d$ $40.65$ $56.80$ $39.42^{d}$ $1.76$ $75.94$ $34.13^{c.} d$ $1.76$ $1.87$ $56.76^{c.}$ $1.76$ $1.82$ $1.66^{c.}$ $1.76$ $1.82$ $1.66^{c.}$ $36.80$ $37.51$ $29.23^{c.} d$ $40.65$ $37.50$ $38.51$ $20.00000$ $37.50$ $38.51$ $0.00000$ $37.50$ $38.51$ $0.00000$ $1.79$ $1.50^{c.}$ $0.176$ $0.53.07$ $36.80$ $0.65$ $35.60$ $23.07$	Perfusion Fraction $(f, \%)$	40.65	37.	58	0.19
$1.76$ $1.50$ $1.87^{c.}d$ $36.80$ $23.56$ $39.42^{d}$ $36.80$ $23.56$ $39.42^{d}$ $40.65$ $45.94$ $34.13^{c.}d$ $40.65$ $5GR, CPR > 1 (n=21)$ $FGR, CPR < 1 (n=15)$ $Control (n=97)$ $FGR, CPR > 1 (n=21)$ $FGR, CPR < 1 (n=15)$ $1.76$ $1.82$ $1.66$ $34.13^{c.}d$ $1.76$ $1.82$ $1.66$ $34.13^{c.}d$ $1.76$ $1.82$ $1.66$ $34.13^{c.}d$ $10.65$ $37.51$ $29.23$ $36.80$ $10.65$ $37.50$ $38.51$ $29.23$ $10.66$ $37.60$ $38.51$ $29.23$ $10.65$ $56.0$ $38.51$ $7.3$ $10.76$ $1.79$ $1.50$ $1.50$ $10.65$ $35.60$ $23.07$ $23.07$		Control (n=97)	Early-Onset FGR (n=11)	Late-Onset FGR (n=25)	p-value <sup>b</sup>
$36.80$ $23.56$ $39.42^d$ $30.42^d$ $40.65$ $45.94$ $39.42^d$ $40.65$ $45.94$ $54.13^c$ . $d$ Control (n=97)FGR, CPR >1 (n=21)FGR, CPR <1 (n=15)	Small Scale Diffusion (D)	1.76	1.50	$1.87^{c, d}$	<0.05 <sup>c,d</sup>
$40.65$ $45.94$ $34.13^{C.}d$ $40.65$ $FGR, CPR > 1 (n=21)$ $FGR, CPR < 1 (n=15)$ $1.76$ $1.82$ $1.66$ $1.76$ $1.82$ $1.66$ $36.80$ $37.51$ $29.23$ $36.80$ $37.51$ $29.23$ $40.65$ $37.60$ $38.51$ $200trol (n=97)$ $FGR, No MHD (n=31)$ $FGR, + MHD (n=05)$ $1.76$ $1.79$ $1.50$ $1.76$ $1.79$ $1.50$ $36.80$ $35.60$ $23.07$ $40.65$ $37.33$ $41.90$	Large Scale Pseudo-Diffusion (D*)	36.80	23.56	$39.42^{d}$	<0.05 <sup>d</sup>
Control (n=97)         FGR, CPR >1 (n=21)         FGR, CPR <1 (n=15)           1.76         1.82         1.66           36.80         37.51         29.23           40.65         37.60         38.51           Control (n=97)         FGR, No MHD (n=31)         FGR, + MHD (n=05)           1.76         1.79         1.50           1.76         35.60         33.51           36.80         35.60         33.51           1.76         1.79         1.50           1.76         1.79         1.50           36.80         35.60         23.07           40.65         37.33         41.90	Perfusion Fraction (f, %)	40.65	45.94	$34.13^{c, d}$	<0.05 <sup>c,d</sup>
1.76         1.82         1.66           36.80         37.51         29.23           36.80         37.50         38.51           40.65         37.60         38.51           Control (n=97)         FGR, No MHD (n=31)         FGR, + MHD (n=05)           1.76         1.79         1.50           1.76         35.60         1.50           36.80         35.60         23.07           40.65         37.33         41.90		Control (n=97)	FGR, CPR >1 (n=21)	FGR, CPR <1 (n=15)	p-value $b$
36.80         37.51         29.23           40.65         37.60         38.51           Control (n=97)         FGR, No MHD (n=31)         FGR, + MHD (n=05)           1.76         1.79         1.50           36.80         35.60         23.07           40.65         37.33         41.90	Small Scale Diffusion (D)	1.76	1.82	1.66	NS
40.65         37.60         38.51           Control (n=97)         FGR, No MHD (n=31)         FGR, + MHD (n=05)           T         1.76         1.79         T.50           36.80         35.60         23.07         40.65         37.33         41.90	Large Scale Pseudo-Diffusion (D*)	36.80	37.51	29.23	NS
Control (n=97)         FGR, No MHD (n=31)         FGR, + MHD (n=05)           1.76         1.79         1.50           36.80         35.60         23.07           40.65         37.33         41.90	Perfusion Fraction $(f, \%)$	40.65	37.60	38.51	NS
1.76         1.79         1.50           36.80         35.60         23.07           40.65         37.33         41.90		Control (n=97)	FGR, No MHD (n=31)	FGR, + MHD $(n=05)$	p-value $b$
36.80         35.60           40.65         37.33	Small Scale Diffusion (D)	1.76	1.79	1.50	NS
40.65 37.33	Large Scale Pseudo-Diffusion (D*)	36.80	35.60	23.07	NS
	Perfusion Fraction $(f, \%)$	40.65	37.33	41.90	NS

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<sup>a</sup>Based on independent samples t-test

 $\boldsymbol{b}_{\rm Tairwise}$  comparisons based on least squares means estimates from ANOVA

 $c_{\rm significantly}$  different from control at p<0.05

 $d \over significantly different from early-onset FGR at <math display="inline">p < 0.05$ 

Abbreviations: FGR=fetal growth restriction, CPR=cerebroplacental ratio, MHD=maternal hypertensive disorders (namely, gestational hypertension, chronic hypertension and preeclampsia)