RESEARCH ARTICLE



Microwave assisted synthesis of polyacrylamide grafted polymeric blend of fenugreek seed mucilage-Polyvinyl alcohol (FSM-PVA-g-PAM) and its characterizations as tissue engineered scaffold and as a drug delivery device

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Received: 7 September 2018 / Accepted: 2 January 2019 / Published online: 2 February 2019 © Springer Nature Switzerland AG 2019

Abstract

Microwave assisted synthesis of graft copolymer of polymeric blend of Fenugreek seed mucilage (FSM)-Polyvinyl alcohol (PVA) with acrylamide (AM) was done by free radical polymerization using ammonium per sulfate (APS) as initiator. Varying amount of AM and APS was used to optimize the best grade based on highest percentage grafting efficiency and investigated with intrinsic viscosity measurement, Fourier Transformation infrared spectroscopy (FTIR),¹³C NMR spectra, X-ray diffraction, elemental analysis, Thermogravimetric analysis, Scanning electron microscopy. The results of intrinsic viscosity indicate that the optimized sample GF4 has longer chain length than in comparison to the native mucilage and thus exhibits more swelling tendencies and thus can be used as very good controlled release matrix system. The thermal analysis and X-ray indicates that GF4 is more stable and possess more amorphous properties than the native FSM. The NMR and FT-IR studies reveal that in GF4 there is prominent presence of amide and the hydroxyl groups indicating that grafting mechanism has efficiently taken place. Histological studies & SEM image for optimized grade implanted on animals revealed sufficient tissue growth and exhibited biodegradability proving the material to be biocompatible and suitable to be used as tissue engineered scaffolds. The controlled release behavior of the optimized polymeric system GF4 was evidenced by 95% release of loaded drug Enalapril maleate for 16 h.

Keywords Graft copolymer · Metronidazole · Histopathology · Scaffold · Fenugreek seed mucilage

Introduction

The use of green chemistry design for polymer synthesis has eliminated the use of most toxic chemicals creating an environment free from chemical pollution [1]. Thus, chemical free radiation induced free radical initiated synthesis of various types of polymers like graft copolymer has brought a breakthrough in the field of modified polymers to be used in drug

Electronic supplementary material The online version of this article (https://doi.org/10.1007/s40199-019-00237-8) contains supplementary material, which is available to authorized users.

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delivery and other biomedical applications [2]. The modification of a natural polysaccharide with another synthetic substance thereby retaining the chemical and physical properties of natural and synthetic polymers is mainly done by the process of graft polymerization [3, 4]. Also the modification of natural polymers by synthetic polymers improves their shelf life and stability, preventing from instant biodegradation and can be used in controlled release of potent drugs [5, 6]. In case of drug delivery, efficient controlled and extended release is mostly expected from any good formulations. The use of graft copolymers can serve the purpose of retarding the drug release by forming an efficient drug matrix which will slowly swell and erode to release the drugs in a controlled fashion preventing the peak and valley release pattern as expected in conventional delivery [7]. Besides the use of these modified polymers in drug delivery, other significant applications in tissue engineering are of importance. The biomedical nature of such modified polymers mainly depends on their abilities to

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interact with the living cells, cyto-compatibility and their macromolecular structure to form the three-dimensional (3D) structure to mimic the cells [8]. The use of natural polysaccharides is advantageous as they are nontoxic and biodegradable in nature [7]. Several polysaccharides are utilized for preparation of graft copolymer with vinyl or acryl monomers [4]. The acrylamide monomers have varied applications in the field of drug delivery, flocculation, stabilizing agents etc. [9]. Various plant sources like seeds, leaves, bark have plenty mucilage content as rich source of polysaccharides. Fenugreek seeds are one such source sufficient amount of mucilage and can be used for preparation of modified polymers [10]. Previously, there are several evidences of research on fenugreek seed mucilage grafted copolymers with acrylamide [10], but till date no where there are any evidences for the polymeric blend of fenugreek seed mucilage with Polyvinyl alcohol (PVA) grafted with acrylamide (AM) used as tissue scaffold. The current research is based on preparation of grafted polymeric blend of Fenugreek seed mucilage-Polyvinyl alcohol (FSM-PVA-g-PAM) with polyacrylamide for its use as polymeric tissue scaffold and its drug release properties.

Experimental

Fenugreek seed (*Trigonella foenum-graecum***) mucilage (FSM)** was extracted by milling the soaked seeds in hot water to yield a thick mucilaginous solution which was filtered four times through very fine muslin cloth. For deproteinization, the mucilage solution was treated with solution of 0.3 N Ba(OH)₂– 5% aqueous ZnSO4.7H2O [10]. Acrylamide (AM), Ammonium Per sulfate (APS)(SD, Fine-Chem Ltd., India), Poly(vinyl alcohol)(CDH, New Delhi) were used as received.

Synthesis of FSM-PVA-g-PAM graft copolymer and its purification

The graft copolymer was prepared by using microwave assisted process by varying different concentration of **APS** and **AM** using **APS** as the redox initiator [11] as shown in composition

Table 1. The time for the reaction was kept constant. Initially the required quantity of polymers (FSM with PVA) along with calculated amount of monomer AM were taken in a glass beaker and dissolved in milipore water (100 ml) stirred on a magnetic stirrer maintained at temperature 50 °C till all the polymers dissolve and then later APS is added and stirred for another 15 min. The mixture in the glass beaker was microwaved keeping the time constant at 40s till the polymer mixture thickens to gel consistency. The reaction vessel was immediately taken out and placed aside in ice bath for cooling. The unreacted PVA, monomer, APS and any other byproducts if formed are removed by using acetone as a solvent to obtain the purified graft copolymer [12, 13]. Reaction detail is outlined in Scheme 1. The optimization of the best grade of FSM-PVA-g-PAM is done using % Grafting Efficiency as shown in Eq. 1 [14-16]. The synthesized graft copolymer was dried in a hot air oven and ground to fine powder.

$$\% Grafting \ Efficiency = \frac{Weight \ of \ Graft \ copolymer-Weight \ of \ Polymer}{Weight \ of \ monomer} \times 100$$

(1)

Characterization and analysis

The intrinsic viscosity measurement of all the prepared grades of graft copolymer were done using Ubbelodhe viscometer (capillary pore size 0.36 mm, measuring viscosity range from 0.3-1 mm²/s) at 25 °C. Other characterizations of graft copolymer along with the pure polymers and monomer was done by using Fourier Transformation Infrared Spectroscopy (FTIR) (Shimadzu, FTIR-8400S) using KBr pellets from 4000 to 400 cm⁻¹ [16]. Thermo-gravimetric analysis (TGA) (Model: DTG-60; Shimadzu, Japan) was performed in an inert atmosphere (nitrogen) from 30 °C to 400 °C at the heating rate of 10 °C/min [17] .X-ray diffraction (XRD) was done with PW 1840 diffractometer and PW 1729 X-ray generator, which were used for the study to produce Cu-Ka radiation with the scattering angle (2) varied from 10 to 800 [16]. 13C Nuclear

Sl.No.	Grade Code	Weight in gm					%	Microwave	% GE
		Pure FSM	PVA	AM	APS	Yield	Yield	time (Sec)	
1	GF1	0.5	0.5	10	0.2	8.752	78.142	30Sec	77.52
2	GF2	0.5	0.5	10	0.25	8.342	74.151	30Sec	73.42
3	GF3	0.5	0.5	10	0.15	7.166	64.269	30Sec	61.66
4	GF4	0.5	0.5	15	0.2	15.572	96.123	30Sec	97.146
5	GF5	0.5	0.5	20	0.2	18.934	89.311	30Sec	89.67
6	GF6	0.5	0.5	25	0.2	21.382	81.611	30Sec	81.528

Table 1Composition of graftcopolymer of FSM-PVA-g-AM

Scheme 1 Reaction Mechanism of formation of graft-copolymer of Fenugreek seed mucilage (FSM)-Polyvinyl alcohol (PV-OH) with Acrylamide. Ammonium

persulphate(NH₄)₂S₂O₈) is used as initiator in the initiation step leading to the formation of free radical on the Polymer blend of FSM with PV-OH and the monomer Acrylamide attaches to the free radical sites on to the Fenugreek seed mucilage-PVA and further propagates to form Polyacrylamide grafted copolymer in the Propagation step and later terminated by addition of acetone in the termination step



magnetic resonance (NMR) was also done for the confirmation of grafting reaction in optimized graft copolymer which was compared with that pure FSM.

Intrinsic viscosity measurement

Intrinsic viscosity measurements of the aqueous solution of graft copolymer of different concentration (0.1, 0.05, 0.025 & 0.0125% *w*/*v*) were carried out with the help of Ubbelohde viscometer with a capillary diameter of 0.36 mm (constant 0.001) at 25 ± 0.1 °C in triplicate. The flow time was measured for polymeric solution. The intrinsic viscosity was calculated by plotting specific viscosity/concentration(η_{sp}/C) versus concentration (*C*) and then taking the intercept at *C* = 0 of the fitted straight line [6, 18].

FTIR spectroscopy

FTIR of optimized grade GF4 is done for the confirmation of structure. Sample was taken in 1:100 ratio by KBr and mix evenly in porcelain dish. About 10 mg of mixed sample was moved in sample holder and pressed evenly to make flat surface. The transmittance recorded between 4000 and 500 cm-1 on FTIR spectroscopy (Shimadzu, FTIR-8400S) [19].

Thermal analysis

The thermal stability of vacuum-dried samples of pure FSM, GF4, PVA and acrylamide were examined using thermal gravimetric analyzer (Shimadzu, Japan, DTG-60) and heated from room temperature to 700 °C in a nitrogen atmosphere at a heating rate of 10 °C/min [10].

XRD

The sample mainly pure FSM, PVA and GF4 were diffracted for 2θ value ranging from 20 to 80° at 2° /minute and chart speed of $2^{\circ}/2$ cm/ 2θ (Bruker AXC D8 Advance, Germany) [10].

13C NMR studies

Solid state ¹³C NMR spectroscopy was performed for native gum and GF-4. The analysis was performed by inserting about 300 mg of sample respectively in ceramic rotor on a JEOL ECX 400 (Peabody, MA, USA) spectrometer functioned at 75 MHz [20].

Surface morphology

The scanning electron microscopy of the GF4 was done in powdered form using SEM, Model Jeol JSM –6390 LV. The SEM photographs are used for characterizations of the surface morphology of the grafted polymer [9, 10].

Elemental analysis

The elemental analysis of FSM and GF4 was undertaken with an Elemental Analyzer (SEM, Jeol JSM -6390 LV). The estimation of three elements, i.e. carbon, nitrogen, oxygen was undertaken [21].

Invitro drug release studies

Preparation of tablets

The tablets of Enalapril Maleate using the optimized GF4 graft copolymer was prepared by hand powdering the graft polymer [22] and then weighing out a 225 mg of polymer along with 25 mg of drug which is 10% of total weight of the polymer and passing the mixture through a 20mesh sieve and to this mixture around 0.01 mL of water was added just to moisten the mixture and triturated. The dough was then hand molded to form a pellet like structure as shown in.

In-vitro release study

The in-vitro dissolution study of Enalapril Maleate from graft copolymer in the form of tablets as shown in Fig. 1, was carried out in a basket type 8-station dissolution test apparatus Dissolution apparatus(TDT -08 1), Electrolabs,



Fig. 1 FTIR Spectra of FSM (Fenugreek seed mucilage); PVA (Polyvinyl alcohol); Acrylamide (AM); Graft copolymer (GF4)

TDT-08 L, Mumbai, India, with stirring speed of 50 rpm using phosphate buffer of pH 6.8 as dissolution medium under sink conditions at 37 °C \pm 0.5 °C.Periodically, 10 ml of the solution was withdrawn from the dissolution medium and was filtered with a 0.45 µm (µ) membrane filter disc and analyzed by Double beam spectrophotometer (UV-1800), Shimadzu Corporation, Japan, at 205 nm for the drug [23]. Same volume of dissolution medium was replaced back after each sampling to maintain sink condition. The kinetic data obtained from the release profiles were also evaluated by fitting into different kinetic models.

Assessment of mice subcutaneous tissue response graft copolymer as tissue engineered scaffold

The experiment was conducted following the institutional animal use and care regulations of Birla Institute of Technology, Mesra, Ranchi (Institutional Animal ethical Committee of Birla Institute of Technology, Mesra, Ranchi, Approval number 1972/PH/BIT/25/17/IAEC). Male mice were housed under standard conditions with a controlled temperature of 25 °C and a light/dark cycle of 12/12 h. The animals were divided in two groups i.e. control & test each consisting of 6 animals [24]. Hairs on the skin were completely removed using hair removal cream. Then, the exposed skin of the animals was sterilized using povidone iodine. An incision was done and pure cotton ball as the control and cotton ball coated with solution of graft copolymer as the test material were placed in the skin pockets and stitched. After 15 days, each group was euthanized, and the test and control materials were taken out and freeze dried [25] and observed under SEM for the evidence of any cell growth on the scaffolds. Isolated liver, kidney & scaffold applied local tissue were preserved in formalin for histological procedures for determination of any toxicity. After collection, the carcasses were disposed by burial [24].

Histological procedure

Excised tissues from local site and liver were fixed in 10% formalin solution for 5 days. All tissues were processed by embedding in paraffin wax and then sectioned at 3 μ m thicknesses, mounted on glass slides, deparaffinized and stained with Haematoxylin–Eosin (HE). Images were taken with an optical microscope (Leica, DME) [24].

Results and discussion

Synthesis of FSM-PVA-g-PAM

FSM-PVA-g-PAM has been synthesized using microwave irradiation. Initially for all grades of graft copolymer

preparation, the quantity of polymers FSM, PVA and AM were kept constant. Only the ratio of APS was varied in the grades, to check at which concentration of APS, maximum % GE was achieved. At this stage, grade GF1 was having the highest %GE. Later, optimization of the monomer AM was quantified by keeping all the other contents constant and finally grade GF4 was selected as the optimum grade with maximum %GE and was further evaluated. The optimized graft copolymer was based on the % grafting efficiency. Generally, % grafting is used as the parameter for optimization of the best grade, but in the present process, the % grafting parameter did not provide expected results as there was continuous increase in grafting with the increase in monomer concentration. Thus, to get appropriate results, % grafting was utilized as the optimization parameter.

Characterizations

Intrinsic viscosity

The present optimized grade GF4 has higher intrinsic viscosity value when compared to other grades. The values of intrinsic viscosity of all the different grades of graft copolymer sample are given in Table 2. The graphs of intrinsic viscosities of all the grades are shown in Fig. S1. The intrinsic viscosity of a polymeric solution is a measure of the hydrodynamic volume of the polymer in solution which in turn depends on the polymer molecular weight, its structure, nature of the solvent and temperature of the medium. For the polymers which have a low intrinsic viscosity indicates that the hydrodynamic volume is less as it may be due to the smaller branched chains and for the polymers having large intrinsic viscosity, their hydrodynamic volume is also higher as this may be due to the reason for the long linear grafted chains on to the polymer backbone [19]. This may be an advantageous factor as more the hydrodynamic value, there may be more swelling and thus this can be an essential factor in controlling the release rate of drug from the polymeric matrix.

FTIR spectroscopy

The FTIR spectra of FSM shows characteristic peaks at 3598 cm^{-1} which corresponds to -OH [26] -CO stretching at 1017.72 [10, 11],-CH₃ stretching at 2919.77 cm⁻¹ as shown in Fig. 1 and Table S2. It is observed that the FTIR spectrum of GF4 is different from the FSM by the introduction of a small peak of secondary amide RCONHR at 1643 cm⁻¹, broad and medium –NH stretching at 2997 and 3352 cm⁻¹ [26]. The broadening in the spectra in GF4 after 3000 cm⁻¹ may be due to the overlapping of – NH(amide) and –OH groups of mucilage.

Thermal analysis

The TGA thermograms of FSM and FSM-PVA-g-PAM copolymer GF4, are shown in Fig. 2. In case of pure fenugreek seed mucilage FSM, there is only single stage degradation, where as in case of grafted copolymer GF4, there are multiple stages of degradation with very less amount of weight loss which is very high in case of pure mucilage. The percent weight loss in case of pure FSM and that of GF4 till 275 °C, was almost equal to about 18-20%, but after 275 °C, in case of FSM, there is a drastic weight loss whereas in case of GF4, there was very less amount of weight loss, which itself indicates that graft copolymer GF4, is more stable than that of pure polymer. Moreover, as in case of PVA, the percent weight loss after 275 °C is 137.55%, whereas in case of AM, the percent weight loss after 250 °C is only 13%. The percentage weight loss with an increase in temperature in both the cases is summarized in Table S3. The results showing less amount of % weight loss in case of GF4, when compared to pure FSM, PVA and AM, gives a clear indication that the polyacrylamide chains grafted with the polymer blend of pure FSM along with PVA contributed more stability towards temperature and thermal decomposition behavior [10].

X-ray diffraction

The XRD diffractograms of the pure native FSM shows broadened sharp peaks whereas in case of PVA and AM

Table 2A comparative tabledepicting formula, intrinsicviscosities & % graftingefficiency of the graft copolymergrades

Polymer grade	Amount of Fenugreek seed mucilage(gm)	Amount of PVA (gm)	Amount of Acrylamide(gm)	Time of irradiation (Sec)	Intrinsic viscosity (dl/g)	% GE
GF1	0.5	0.5	10	40s	10.849	77.52
GF2	0.5	0.5	10	40s	3.9431	73.42
GF3	0.5	0.5	10	40s	7.619	61.66
GF4	0.5	0.5	15	40s	10.881	92.0
GF5	0.5	0.5	20	40s	5.6557	89.67



Fig. 2 Thermograms of FSM (Fenugreek seed mucilage); PVA (Polyvinyl alcohol); Acrylamide (AM); Graft copolymer (GF4)

sharp peaks are evident in Fig. 3. But in case of GF4, the diffractogram does not have any sharp peaks and is almost bluntly broadened, which is different from the pure FSM, which indicates that GF4 will be easily soluble in aqueous phase [27]. The XRD diffractograms of the pure native FSM showing not so prominent sharp peaks indicates its partial crystalline nature [10], whereas in case of PVA and AM sharp peaks indicate their pure crystalline nature. In case of GF4, the presence of broad blunt diffractogram indicates the amorphous characteristics of the sample which will be easily soluble in aqueous phase. Also, this change in GF4 indicates that a solid phase was formed after grafting process and this led to the destruction of the crys-

talline nature of the polymer blend of mucilage and Polyvinyl alcohol [10].

NMR spectra

The 13C-NMR resonances of mucilage revealed the peaks as shown in Table 3. The NMR spectra of Pure Fenugreek seed mucilage (FSM) and that of GF4 are shown in Fig. 4a and b A small downfield shift of all the backbone carbons of the polysaccharide in the copolymer in comparison to those of the parent was observed, except for C-1 carbon showing upfield shift of 1.71 ppm in the copolymer as shown in Table 3. This may have



S. No.	Polysacchari	de (mucilage)	After Grafting with		
1.	172.89 —	-> Carboxylic acid	180.84 → Amide		
2			106.23		
	104.18 —	→ Anomeric carbon	104.52		
3	101.45				
4	96.24	Secondary alcohols			
5	83.25		81.79		
6	71.80		71.8820		
7	63.51		42.91		
	レノ		26.93		

Table 3 NMR peaks along with their interpretations

been due to the introduction of the acrylamide moiety onto the polysaccharide, which is expected. The PVA also contributes to the upfield shift due to presence of secondary alcohol groups.

Surface morphology

The scanning electron microscopic photographs of both the native FSM and that of GF4 are shown in Fig. 5a. The rough uneven surface of GF4 confirms the modification in the native fenugreek seed mucilage polymer by another polymer, thereby indicating the grafting of acrylamide (AM) over polymeric blend of FSM with PVA as shown in Fig. 8 [28].

Elemental analysis

The results of presence of different elements like oxygen, nitrogen, hydrogen and carbon are shown in Fig. 5b. This is also observed in practice from the elemental analysis result as summarized in Table S 4. The results as observed from Fig. 5b, confirms the presence of a considerable percent of nitrogen in GF4 compared to the pure FSM which also confirms that AM whose basic elemental content is nitrogen in the form of $-CONH_2$, chains have been grafted on the backbone of polymeric blend of FSM and PVA [21].

In-vitro drug release studies

The drug release from graft copolymer grades GF1, GF2, GF3, GF4 and GF5 were done in presence of phosphate buffer of pH 6.8 and a comparative release profile was

plotted for % Drug release versus time & drug release kinetics was calculated as depicted in Fig. 6, GF4 gives a prolonged release in a controlled fashion than in comparison to other grades. As soon as the graft copolymer tablet interacts with aqueous media, water diffuses into the tablet thereby causing the swelling of the matrix and this swelling continues and a monotonically hydrostatic pressure is developed within the tablets [29]. With the increase in swelling and decreased solubility of the grafted polymeric matrix, the polymeric matrix gets depleted slowly with slow diffusion of the drug from the matrix. The decreased solubility of the grafted copolymer GF4 shows decreased solubility due to increased grafting efficiency [30] and thus the grade GF4 shows controlled release properties by prolonging the release for more than 16 h uniformly as shown in Fig. S 5. The release kinetics of the optimized grade GF4 follows Higuchi model with R^2 value almost nearing to 1 when compared to other drug release kinetic models as shown in Fig. 3, thereby showing that the polymeric matrix forms a permeable matrix [31] with diffusion type of release since value of n =0.309 [32], as shown in Fig. S 5.

Assessment of response of graft copolymer scaffold towards mice tissue

All wounds experienced gradual healing without infection, after completion of 15 days, both the standard and test groups showed a complete loss of keratin layer and the epidermis was devoid of prickle cells. Efficient healing was confirmed by the existence of hair follicles and mature fibrous tissue. This was a clear indication towards the facility of moist environment at the site of



Fig. 4 a spectra for Pure Fenugreek seed mucilage (FSM) b NMR spectra for optimized Graft copolymer GF4



Fig. 5 a: Surface morphology Graft copolymer GF4 and Pure FSM b Elemental spectra of Pure FSM and GF4

the wound, which enabled the rapid epithelialization [33]. The scanning electron microscopy of the control cotton ball and the test cotton ball are shown in Fig. 7 to detect the growth of cells on to the polymer which can be used as tissue scaffold. The figure indicate that the cells have proliferated and differentiated onto the cotton ball as well as onto the cotton ball coated with GF4, [33] which also suggested that the inserted material are highly biodegradable in nature as shown in Fig. 7a and b.



Fig. 6 Comparative drug release profile

Histological investigations

The histology slide of the local tissue, liver and kidney was investigated for both the control and test animals for detection of any obvious toxicity as shown in Fig. 8a-d. From the local tissue slides as shown in Fig. 8a and b, it is quite evident that there was denser growth of spindle shaped fibroblasts [34], collagen and granular cells as compared to that of control tissue [33]. The increased quantity of these cells in the local test tissue indicates that wound healing is rapid. Since collagen enhances the growth of extracellular matrix and thus its increase indicates rapid wound healing in the local test tissue. Foreign body giant cells observed in minor quantity in case of test shown in Fig. 8a and b, an inflammatory response are most common at the interface of both tissue and scaffold which is previously reported in several literature [35, 36]. These results ensure the nontoxic nature of the graft copolymer GF4 as well as its efficiency to be utilized as a template material for tissue growth. Also, the histological evaluation of the test liver and kidney when compared with control tissues as shown in Fig. 8c and d respectively suggests that the test material do not pose any toxicity in liver and kidney.

However, in this article, it can be visualized that our FSM-PVA-g-PAM is a versatile material having broader application. This novel material has potential to be applied in both tissue scaffold & drug delivery devices. The applicability of this material needs to be explored widely. In-depth toxicity study & applicability in some higher animal models like **Fig. 7 a** and **b** representing SEM images of the tissue growth on the control and Graft Copolymer GF4



dog, monkey and human need to be explored. Full phase clinical trial need be observed to check the effect of material in the long run.

Conclusion

The graft copolymer of FSM-PVA-g-PAM was successfully prepared by microwave irradiation process using ammonium per sulfate as the redox initiator. The percentage grafting

Fig. 8 a Photomicrographs of histology of Control local tissue area stained with hematoxylin and eosin on day 15 after surgery captured by Leica Microscope at 40X respectively and f,c and I, represent spindle shaped fibroblast, collagen and Foreign body giant cells respectively b Photomicrographs of histology of Test local tissue area stained with hematoxylin and eosin on day 15 after surgery captured by Leica Microscope at 40X respectively and f,c and I, represent spindle shaped fibroblast, collagen and Foreign body giant cells respectively. c Photomicrographs of histology of liver of Test and control mice stained with hematoxylin and eosin on day 15 after surgery captured by Leica Microscope at 40X d: Photomicrographs of histology of kidney of control and test mice stained with hematoxylin and eosin on day 15 after surgery captured by Leica Microscope at 40X

efficiency increased with increasing quantity of redox initiator but up to a certain limit and then again decreased, and whereas in presence of monomer the grafting efficiency continuously increased and thus the highest grafting efficiency value was taken as the best grade. The intrinsic viscosity of the optimized grade GF4 showed that the sample has longer polymeric chains leading to more swelling and delayed drug release. Moreover, the characterization of GF4 was done with FTIR, XRD, NMR, and TGA. The elemental analysis confirmed the presence of nitrogen along with carbon and oxygen in the sample GF4.



The in-vitro tissue growth on the graft copolymer sample was successful and histopathological studies of the local tissues along with the liver and kidney showed that the sample is non-toxic. The in-vitro drug release from the optimized grade took place for more than 16 h and the release kinetics to followed Higuchi model with diffusion type of release from the matrix. This versatility makes the material suitable for tissue engineering scaffold & drug delivery device.

Acknowledgments The authors acknowledge the instrumental support of Central Instrumentation Facility, Birla Institute of Technology, Mesra, for sophisticated instrument to carry out this experiment.

Author's contributions The experimental study was done by Corresponding author Trishna Bal (TB) as a part of her reserach work who did all the practical experiments and drafted the article. The other coauthor, Sabyasachi Swain (SS) did the insertion of the polymeric scaffolds in animals. All authors read and approved the final copy of the text.

Compliance with ethical standards

Conflict of interest The authors declare that there is no conflict of interest.

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