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Harnessing cyanine photooxidation: from slowing photobleaching to near-IR uncaging

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Abstract

Light provides a uniquely powerful stimulus to help visualize and/or perturb biological systems. The use of tissue penetrant near-IR wavelengths enables *in vivo* applications, however the design of molecules that function in this range remains a substantial challenge. Heptamethine cyanine fluorophores are already important tools for near-IR optical imaging. These molecules are susceptible to photobleaching through a photooxidative cleavage reaction. This review details efforts to define the mechanism of this reaction and two emerging fields closely tied to this process. In the first, efforts that slow photooxidation enable the creation of photobleaching resistant fluorophores. In the second, cyanine photooxidation has recently been employed as the cornerstone of a near-IR uncaging strategy. This review seeks to highlight the utility of mechanistic organic chemistry insights to help tailor cyanine scaffolds for new, and previously intractable, biological applications.

Introduction

Optical methods that probe and/or alter biological processes are central to biomedicine. Near-IR light (~650–900 nm) is dramatically more tissue penetrant than visible light, facilitating *in vivo* applications [1]. Nevertheless, improved chemical tools are required to fully realize the benefits of these wavelengths. In the context of imaging, there is a significant need for long wavelength fluorophores with enhanced chemical/photochemical stability and improved optical properties [2,3]. With regard to altering biology and treating disease, existing near-IR methods typically rely on the local generation of toxic levels of reactive oxygen species (ROS) through 'photodynamic' approaches [4]. By analogy to the significant utility of existing photocaging approaches for cell-based studies, many *in vivo* biomedical applications would be possible if diverse chemotypes could be site-specifically released with near-IR light [5[•],6].

Indocyanine fluorophores, often referred to as 'Cy' dyes, are used for a variety of fluorescence-based applications. Heptamethine variants form the basis of many, if not most, clinical near-IR imaging efforts, as well as many preclinical studies. One example, indocyanine green (ICG, 1, Figure 1a), is an FDA-approved diagnostic agent used in a variety of clinical contexts [7,8]. Another example, the bioconjugatable IRDye-800CW (2),

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is in clinical trials as an optical beacon to guide the surgical resection of squamous cell carcinoma [9]. As with many fluorophores, cyanines are prone to light-dependent decomposition, or photobleaching. Somewhat unusually, cyanine photobleaching derives from a well-defined photooxidative cleavage reaction, which is exemplified by the conversion of ICG to carbonyls **3** to **6** in Figure 1b [10]. This review describes efforts to define the mechanism of this photooxidative reaction and two fields where this process plays a central role (Figure 1c). In the first, chemists seek to develop molecules with improved photooxidative reactions have been used to create near-IR photocaging strategies. In both cases, organic chemistry provides critical insights, and the molecular entities, to enable biological advances

Cyanine photooxidation: mechanistic studies

Building on seminal studies from the Kodak laboratories, various reports have described the oxidative cleavage products that derive from cyanine photolysis [11,12,13[•]]. Although the products are well defined, key mechanistic details have been described disparately. For example, the relevant ROS have been variably assigned as singlet oxygen ($^{1}O_{2}$), hydrogen peroxide (H₂O₂), or hydroxy radical ([•]OH) [13[•]]. In general, we have been guided by the notion — first suggested in the Kodak study and invoked elsewhere — that the formation of carbonyl products is best understood through the $^{1}O_{2}$ -mediated dioxetane formation/ cycloreversion mechanism shown in Figure 2a.

Seeking further insights for the complex and relatively minimally studied case of heptamethine cyanines, we recently carried out a set of mechanistic studies using compound 7 [14[•]]. The major reaction pathway was analyzed following either photolysis or exposure to candidate ROS. These studies revealed that only ${}^{1}O_{2}$ (generated either chemically or through independent photosensitization), and not other candidate ROS, is capable of inducing C-C cleavage at 2 of the 4 feasible reaction sites along the cyanine polyene. These results nearly match those obtained by direct photolysis (Figure 2b,c). Moreover, MS/MS fragmentation of a near-IR light-dependent $[7 + O_2]^+$ adduct — the putative dioxetane intermediate provides ions corresponding to carbonyls 8-11. Finally, a quantum mechanical analysis of the photooxidative pathway indicated that the relative ground state energy of the intermediate dioxetanes correlates closely with the observed product distribution (Figure 2d). Together, these studies provide strong evidence that the major photooxidation pathway of heptamethine cyanines entails ¹O₂-mediated cleavage of the polyene via dioxetane intermediates. Despite these insights, a number of questions remain. In particular, an understanding of the dramatic differences in photo-chemical stability between cyanines would be quite useful. For example, trimethine and pentamethine cyanines are substantially less susceptible to photodegradation than the heptamethine variants described above [15,16].

Slowing photooxidation to create stable fluorophores

The creation of photobleaching resistant fluorophores will broaden the time interval over which phenomena of interest can be observed [17,18]. For example, signal stability is crucial for single molecule microscopy [19^{••}]. This is also true for fluorescence-guided surgical

interventions, where significant light exposure over long timeframes is inescapable [20,21]. Three different strategies have been pursued with cyanine derivatives: (1) altering electron density, (2) encapsulation, and (3) the use of triplet-state quenchers (TSQs).

As ${}^{1}O_{2}$ is a highly electrophilic species, a reasonable strategy to reduce photooxidation involves removing electron density from the cyanine polyene. Two different strategies have been explored. In the first, a cyano functional group was attached directly to the polyene of a merocyanine derivative [22]. In the second, the aromatic rings of a bisbenzothiazole pentamethine cyanine were perfluorinated [23]. In both cases, the resulting fluorophores were significantly more photostable than the corresponding compounds lacking these modifications. Further efforts with this particularly direct approach are likely to be productive.

The concept of chromophore encapsulation garners inspiration from Green Fluorescent Protein (GFP), where the positioning of the chromophoric element inside a β -barrel motif provides needed rigidity and improved stability. Cyanine encapsulation was first explored by Anderson and coworkers using irreversibly rotaxane encapsulated hepta- and pentamethine cyanines [24,25,26]. Elegant work by Smith and coworkers has also explored this concept with squarine-based dyes [27,28]. In both instances, the encapsulated dyes are more resistant to photochemical and chemical degradation than the free molecules, and, in the case of the latter, the complexes have been applied in a variety of imaging contexts. An alternative approach to encapsulate chromophoric elements entails the combination of exogenously provided small molecules and genetically encoded protein hosts. Armitage and coworkers have realized this concept using single-chain variable fragment (scFv) antibodies that were evolved to bind a family of cyanines [29,30]. These molecules are nearly non-fluorescent initially, but, upon binding to the expressed protein host, become dramatically more fluorescent with significant improvements in photo-stability.

Another approach to slow photobleaching is to reduce the generation of ${}^{1}O_{2}$ and other ROS. In principle, lowering the quantum yield of intersystem crossing (Φ_{ISC}) and/or shortening the triplet state lifetime (τ_{T1}) should achieve this goal. Efforts in this area draw from the development of antifade buffers for microscopy. These buffers often contain redox active small molecules, for example quinones, thiols, nitroaryls, or, most recently, Ni(0) salts, and are frequently used in combination with enzymatic oxygen exclusion [31,32,33,34[•]]. The requirement of high concentrations (mM) of the redox active molecule(s) imposes certain limitations, including rendering this approach incompatible with many live-cell and tissue imaging applications. Thus, intramolecular tethering is a reasonable tactic to increase the effective concentration of the redox partner. Recently, Blanchard and coworkers dramatically illustrated this concept through generation of Cy3, Cy5, and Cy7 modified with the putative TSQs nitrobenzene, trolox, and 1,3,5,7-cyclooctatetraene (COT) [35,36]. These conjugates exhibit improvements in stability as measured in bulk solution and at the single molecule level. Recent mechanistic studies have shown that the impact on τ_{T1} varies and is highly dependent on the identity of the TSQ and even the linker, although some of these issues may be solvent dependent $[37^{\circ}, 38]$. This concept has also been explored through recent studies by Cordes and coworkers using both DNA tethering strategies and direct covalent attachment [39,40,41]. In total, these studies reveal that various features of cyanine photooxidation,

including kinetic parameters, are subject to modification. Future efforts based on mechanistic insights may provide molecules functionally nearly immune to photobleaching.

Cyanine photooxidation for photocaging

Uncaging reactions that use near-IR light will enable the site-specific delivery of bioactive compounds in complex physiological settings. This is a challenging chemical problem because the modest photonic energy of these wavelengths is not easily translated into bond cleavage [42•]. While two-photon methods are useful, the scope of possible applications is somewhat limited because uncaging only occurs in the small focal volumes excited by pulsed laser sources (nanoliters to picoliters) [43,44]. The first single-photon uncaging methods used metallic nanoparticles through uncaging mechanisms that rely on localized heating or upconversion [45,46]. Recently, strategies that release payloads from custom-built liposomal formulations have also emerged [47^{••},48,49]. Also desirable are small molecule approaches, which, along with their bioconjugates, still comprise the vast majority of clinical modalities. Only recently have such methods started to appear. Exciting0 progress has been achieved with the use of ${}^{1}O_{2}$ -cleavable olefinic linkers in combination with porphyrin and phthalocyanine-based photo-sensitizers and with contact quenching-induced scission of Co-C bonds [50[•],51,52,53,54,55[•]]. Long wavelength uncaging cleavage strategies using the BOPIDY scaffold have also recently appeared [56[•],57,58,59].

Inspired by the well-defined photooxidation chemistry described above, we set out to employ the heptamethine cyanine scaffold as the chemical backbone of a near-IR uncaging strategy. We reasoned that this ubiquitous, albeit typically deleterious, photobleaching reaction could be adapted for this new use. Also motivating this effort was the long-standing observation that cyanines are quite non-toxic, even after protracted irradiation. The chemical design of our first cyanine photooxidation-dependent uncaging strategy is shown in Figure 3a [60[•]]. The uncaging reaction sequence entails photooxidative cleavage of **12** at the C2/C1' and C2'/C3' bonds to afford **13** and **14**, which then spontaneously hydrolyze to release **15**. These steps liberate a secondary amine, which cyclizes onto a pendant carbamate to release phenol-containing payloads (**16**). The mechanistic premise of this strategy is that photooxidation products **13** and **14** are much more susceptible to hydrolysis under physiological conditions than starting **12** (perhaps due to increased iminium character in the key C4'-*N* bond).

Compound **17** (Figure 3b), which releases the absorbance reporter 4-nitrophenolate, was used to spectroscopically characterize the uncaging reaction. Irradiation with modest flux of 690 nm light (1 mW/cm² from an LED source) decreases the cyanine absorption ($t_{1/2} = 8.5$ min) with concommitant appearance of the 4-nitrophenolate signal ($t_{1/2} = 40$ min) (Figure 3c, left). The effect of intermittent irradiation was also examined. The profile of cyanine absorption decrease correlates directly with irradiation, while the nitrophenolate signal increases in interim periods (Figure 3c, right). Time course studies using mass spectrometry showed that intermediates corresponding to **13** and **14** accumulate upon irradiation and then decrease in a light-independent manner. In total, these results are consistent with the proposed mechanism; photooxidation of the cyanine initiates the process and subsequent light-independent steps, hydrolysis and cyclization, are needed prior to phenol uncaging.

Irradiation of compound **18** provides a useful yield of the estrogen receptor antagonist 4hydroxycyclofen (59%), while displaying excellent stability in the dark. Caged **18** was used to control gene expression in combination with a Cre-ER^T transgenic cell line. In line with prior observations, we demonstrated that cyanines that release only non-toxic payloads have little effect on mammalian cell viability upon irradiation. This absence of significant phototoxicity may initially seem surprising, given that the photooxidative reaction described above involves ¹O₂. However, the modest toxicity is consistent with the observation that heptamethine cyanines are weak ¹O₂ generators ($\Phi \approx 0.01-0.001$) [61,62]. Moreover, generated ¹O₂ rapidly destroys the chromophoric element through the photooxidation reaction, limiting the potential to accumulate toxic ROS levels.

Applications in drug delivery

Near-IR drug delivery strategies could complement, or improve upon, existing light-based therapeutic methods that rely on photosensitizer-dependent mechanisms. In particular, the ability to target highly potent molecules specifically to disease sites could enable novel therapeutic strategies. Our efforts to date have focused on antibodydrug conjugates (ADCs). ADCs provide numerous benefits, including excellent pharmacological properties Using cyanine photooxidation for near-IR uncaging. (a) General reaction sequence for uncaging of phenol-containing payloads from 12 using 690 nm light. Compound 12 is converted to hydrolytically labile 13 and 14 via ¹O₂-mediated photooxidation of the polyene. Subsequent hydrolysis at the C4' position provides amine 15, which spontaneously cyclizes to uncage phenol 16. (b) Representative phenols successfully uncaged using the strategy shown in (a). (c) Spectroscopic characterization of uncaging using 17. Absorbance traces at 400 nm (blue) and 680 nm (red) with (solid line) or without (dashed line) 1 mW/cm² 690 nm irradiation of a 50 µM solution of 7 (HEPES buffer). Irradiation with 690 nm light leads to cyanine photooxidation (indicated by a decrease in cyanine absorption at (even with quite complex payloads) and antigen targeting. While the recent clinical progress of ADC strategies is remarkable, cleavage approaches using endogenous cellular processes, e.g. disulfide or peptidic linkers, have little inherent tumor selectivity [63,64]. As a consequence, undesirable release, either in circulation or in benign tissue, is often a significant issue [65,66,67].

Cyanine-based ADC linkers could enable small molecule delivery with high precision through the combination of antibody targeting and near-IR light mediated release. Light provides an external stimulus to precisely time and target the critical small molecule release event, in principle ameliorating dose-limiting toxicities arising from 'off-target' cleavage. We have prepared and characterized first generation cyanine photocaged conjugates of combretastatin A4 (CA4), a potent tubulin polymerization inhibitor, and panitumumab (Pan), a clinically used anti-EGFR antibody (Figure 4) [68*]. This approach appends a bioconjugatable linker to the carbamate functional group (Figure 4a). The key NHS ester was prepared through a 7-step sequence and conjugated to Pan through lysine labeling. Pan was chosen because several near-IR light-accessible tumor types, including head and neck, ovarian, and bladder, are often EGFR+. We validated that these conjugates efficiently release CA4 upon irradiation, display high dark stability, and maintain EGFR binding.

This construct enabled *in vitro* and *in vivo* characterization, which was carried out partly through a collaboration with our colleague at the National Cancer Institute, Dr. Kobayashi. The growth inhibitory activity of the conjugate was highly light dependent (irradiated $IC_{50} = 16$ nM *vs.* unirradiated $IC_{50} = 1.1 \mu$ M, a ~70-fold window, Figure 4b). Furthermore, no inhibitory effects were observed using a version of the antibody conjugate that releases only biologically inactive phenol, indicating that the observed cytotoxicity is solely a consequence of drug release. We also evaluated the internalized and cell surface bound antibody fraction. A significant reduction in cell viability was observed only upon

irradiation in the EGFR+ cell line, with little effect in either the EGFR– cell line or in the absence of irradiation (Figure 4c). Mouse imaging studies using the near-IR fluorescence of the cyanine conjugate were also carried out. Selective tumor accumulation was observed, with high tumor-to-background ratios obtained at 1 day post-injection. Moreover, significant signal is still observed 7 days post-injection, suggesting high stability of the cyanine component.

As a prelude to *in vivo* drug delivery studies, we assessed if tumor irradiation could be used to deplete the fluorescence signal. Encouragingly, the cyanine fluorescence signal, which was stable under typical imaging conditions, can be depleted using external irradiation from a 690 nm PDT laser (Figure 4d). Future efforts that investigate more potent payloads are likely needed to overcome the modest cell-surface concentrations of relevant tumor-associated antigens, such as EGFR [69].

Conclusions

Indocyanines are already essential tools for a variety of fluorescence-based applications. Controlling the photo-chemical oxidative cleavage process of this privileged scaffold will enable currently intractable applications in imaging and drug delivery. Given the centrality of fluorescence imaging to biomedical research, the generation of photobleaching-resistant fluorophores will have a significant impact in many fields. In the context of drug delivery, cyanine-based approaches will allow bioactive molecules to be delivered to sites of interest in complex physiological settings. In this latter area, the development of novel, biologically useful bond cleavage strategies complements complements the significant progress in bioorthogonal bond *forming* reactions [70,71•]. Chemists' capacity to create and then deploy precisely controlled molecular entities for imaging and drug delivery presents a variety of opportunities. The integration of mechanistic organic chemistry insights, complex molecule synthesis, and advanced imaging and biomedical techniques will be needed.

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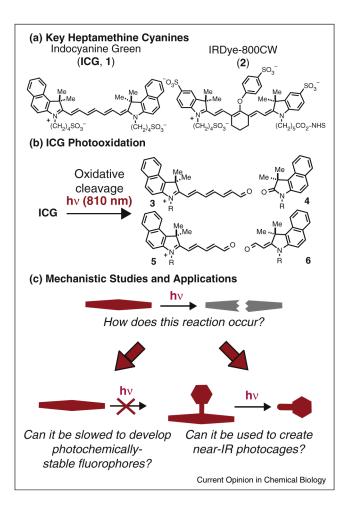


Figure 1.

Overview. (a) Heptamethine cyanines that have been used extensively for *in vivo* fluorescence imaging. (b) Photooxidation of ICG to carbonyl products **3-6**. (c) Understanding the mechanism of cyanine photobleaching enables efforts to generate photochemically stable near-IR fluorophores and near-IR uncaging strategies.

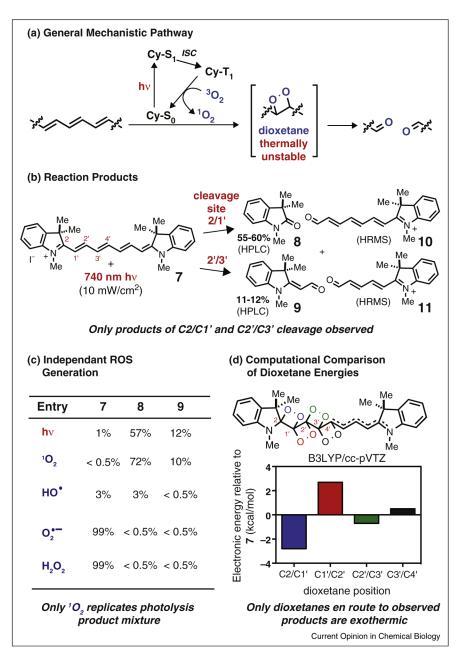


Figure 2.

Probing the mechanism of cyanine photooxidation. (a) General reaction pathway. (b) Carbonyl products 8-11 resulting from regioselective formation and then cleavage of dioxetanes at the C2/C1' and C2'/C3' positions on the polyene. (c) Relative product mixture resulting from exposure of 7 to either 740 nm light or candidate ROS. Only ${}^{1}O_{2}$ produces product ratios similar to those obtained with direct photolysis. (d) Energies of possible dioxetane intermediates en route to carbonyl products.

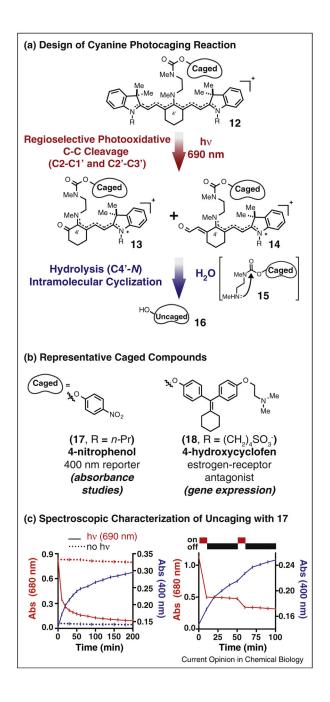


Figure 3.

Using cyanine photooxidation for near-IR uncaging. (a) General reaction sequence for uncaging of phenol-containing payloads from 12 using 690 nm light. Compound 12 is converted to hydrolytically labile 13 and 14 *via* $^{1}O_{2}$ -mediated photooxidation of the polyene. Subsequent hydrolysis at the C4' position provides amine 15, which spontaneously cyclizes to uncage phenol 16. (b) Representative phenols successfully uncaged using the strategy shown in (a). (c) Spectroscopic characterization of uncaging using 17. Absorbance traces at 400 nm (blue) and 680 nm (red) with (solid line) or without (dashed line) 1 mW/cm² 690 nm irradiation of a 50 μ M solution of 7 (HEPES buffer). Irradiation with 690 nm light leads to cyanine photooxidation (indicated by a decrease in cyanine absorption at

680 nm, left) and uncaging of 4-nitrophenolate (indicated by an increase in its absorption at 400 nm). No such effects are observed in the absence of irradiation. In intermittent irradiation experiments (right), cyanine absorption decreases only upon exposure to 690 nm light, while 4-nitrophenolate absorption increases in interim dark periods due to accumulation and then release from intermediates **13** and **14**.



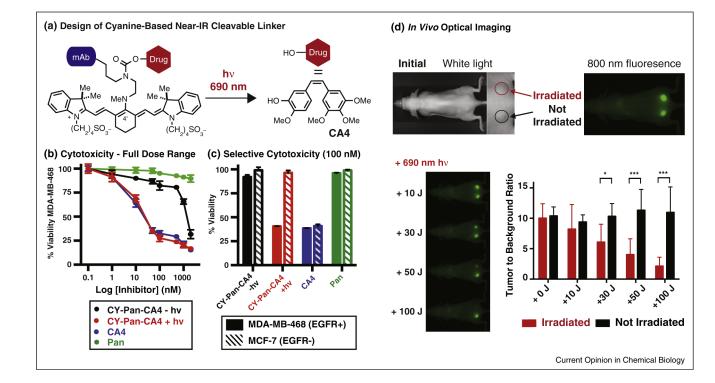


Figure 4.

Cyanine uncaging applied to drug delivery. (a) Design of a near-IR light-cleavable ADC *via* conjugation of a cyanine-caged drug to a monoclonal antibody (CY-Pan-CA4). (b) Light-dependent growth inhibition of EGFR+ cells is observed upon exposure to ADC and 690 nm irradiation. Significantly diminished (~70-fold) CA4 effects are observed in the absence of irradiation, indicating high dark stability. (c) Incubation of EGFR+ and EGFR- cells with conjugate followed by a media exchange prior to photolysis leads to CA4 effects only in the receptor-positive and irradiated cell line. (d) Selective tumor localization is obtained in an EGFR+ double xenograft model. Irradiation of one tumor with a 690 nm laser ablates the cyanine fluorescence signal after 100 J (~3 min), with no effect on the signal of the unirradiated tumor.