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Evolution of brachytherapy for prostate cancer

Nicholas G. Zaorsky1, **Brian J. Davis**2, **Paul L. Nguyen**3, **Timothy N. Showalter**4, **Peter J Hoskin**5, **Yasuo Yoshioka**6, **Gerard C. Morton**7, **Eric M. Horwitz**¹

¹Department of Radiation Oncology, Fox Chase Cancer Center, 333 Cottman Avenue, Philadelphia, PA 19111-2497, USA.

²Department of Radiation Oncology, Mayo Clinic, 200 First St Sw, Charlton Bldg/Desk R - SL Rochester, MN 5590, USA.

³Department of Radiation Oncology, Brigham and Women's Hospital, 75 Francis St BWH. Radiation Oncology, Boston, MA 02115, USA.

⁴Department of Radiation Oncology, University of Virginia, 1240 Lee St, Charlottesville, VA 22908, USA.

⁵Mount Vernon Cancer Centre, Rickmansworth Road, Northwood, Middlesex HA6 2RN, UK.

⁶Department of Radiation Oncology, Cancer Institute Hospital of the Japanese Foundation for Cancer Research, 3-8-31 Ariake, Koto-ku, Tokyo 135-8550, Japan

⁷Department of Radiation Oncology, Odette Cancer Centre, Sunnybrook Health Sciences Centre, 2075 Bayview Ave, Toronto, ON, M4N 3M5, Canada.

Abstract

Brachytherapy BT), using low-dose-rate (LDR) permanent seed implantation or high-dose-rate (HDR) temporary source implantation, is an acceptable treatment option for select patients with prostate cancer of any risk group. The benefits of HDR-BT over LDR-BT include the ability to use the same source for other cancers, lower operator dependence, and — typically — fewer acute irritative symptoms. By contrast, the benefits of LDR-BT include more favourable scheduling logistics, lower initial capital equipment costs, no need for a shielded room, completion in a single implant, and more robust data from clinical trials. Prospective reports comparing HDR-BT and

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Correspondence to: N. G. Z. nicholaszaorsky@gmail.com.

Author contributions

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Competing interests statement

The MEDLINE and PubMed databases were searched, using PICOS/PRISMA methods for original articles and guidelines focusing on prostate cancer brachytherapy published between 1970 and 2016. The search terms used were "prostate cancer" and "brachytherapy" combined with any of: "high dose rate" or "low dose rate." All papers identified were English-language full-text articles. The reference lists of identified articles were searched for further papers. Additionally, the ClinicalTrials.gov database was searched for ongoing clinical trials.

LDR-BT to each other or other treatment options (such as external beam radiotherapy (EBRT) or surgery) suggest similar outcomes (evidence level 1). The 5-year freedom from biochemical failure rates for patients with low-risk, intermediate-risk, and high-risk disease are >85%, 69–97%, and 63–80%, respectively. Brachytherapy with EBRT (versus brachytherapy alone) is an appropriate approach in select patients with intermediate-risk and high-risk disease (evidence level 1). The 10-year rates of overall survival, distant metastasis, and cancer-specific mortality are >85%, <10%, and <5%, respectively. Grade 3–4 toxicities associated with HDR-BT and LDR-BT are rare, at <4% in most series, and quality of life is improved in patients who receive brachytherapy, compared with those who undergo surgery (evidence level 1).

> Prostate cancer is one of the most frequently diagnosed cancers diagnosed in the developed world, with 1.4 million incident cases and $293,000$ deaths in 2013 .¹ Local tumour control is associated with improved outcomes in patients with organ-confined (T1 or T2) prostate cancer, even in the presence of high-risk features, which include PSA >20 ng/ml and Gleason score $8-10$.² Treatment options for nonmetastatic prostate cancer typically include active surveillance (AS), radical prostatectomy and radiotherapy.³ Radiotherapy can be administered in the form of external beam radiotherapy (EBRT) using various fractionation options, and brachytherapy (BT), either high-dose-rate (HDR-BT) or low-dose-rate (LDR-BT), given alone or combined with EBRT.⁴ The Prostate Testing for Cancer and Treatment (ProtecT) trial suggests that radiotherapy offers similar outcomes and improved toxicity and quality of life over surgery.⁵⁻⁷

> Brachytherapy is an excellent treatment option for patients of all disease groups, according to the American Brachytherapy Society (ABS) guidelines,^{8, 9} the Groupe Européen de Curiethérapie / European Society for Radiation Oncology (GEC/ESTRO), and the European Society for Radiation Oncology / European Urologic Association / European Organisation for Research and Treatment of Cancer (ESTRO/EAU/EORTC) guidelines.^{10, 11} Specifically, LDR-BT is defined as 2 Gy/h , and consists of the permanent implantation of sealed sources (seeds) in the prostate. 8 HDR-BT is defined as 12 Gy/h and consists of insertion of a temporary source into a target volume (which contains cancer cells) via a remote afterloader using catheters implanted in the prostate and computer optimization to optimize dose distribution.⁹ The dose fall-off of both LDR- and HDR-BT is rapid, with $< 10\%$ of dose delivered to tissue > 4 cm away from the source (FIG 1A). LDR-BT and HDR-BT can be used as monotherapies for some patients with low-risk disease. Furthermore, EBRT combined with brachytherapy, also known as 'LDR-BT boost' or 'HDR-BT boost,' is hypothesized to further improve local control compared with monotherapy, and to improve outcomes in certain patients with intermediate-risk or high-risk disease (FIG 1B). Various boost schedules are used (FIG 1C): in HDR-BT boost, the implantation can be performed after EBRT, interdigitated with EBRT, or before EBRT; by contrast, in LDR-BT boost, EBRT is usually delivered before the implant is inserted.⁴

This Review considers the evolution of brachytherapy from its inception to contemporary practice, including its historical background and the current indications and contraindications of brachytherapy use compared with EBRT and surgery. The underlying radiophysics and technical aspects, including dosimetric quality constraints, radiobiology,

cost, clinical outcomes and toxicities, and appropriate follow-up monitoring will also be discussed.

Historical background

The history of LDR-BT

Radioactivity was accidentally discovered by Henri Becquerel in 1896.¹² Radium was discovered by Marie and Pierre Curie just 3 years later in 1899, and was used for the treatment of malignant disease in $1901 -$ just 5 years after its discovery.¹³ The use of prostatic brachytherapy was first reported in 1911, when radium was administered temporarily via a urethral catheter.^{14, 15} In 1917, transperineal implantation of radium was performed in New York.16 Several cohorts of patients were treated with radium brachytherapy in the USA during the 1920s; however, this approach was not favoured because prostate cancer was believed to be a relatively radioresistant cancer and it was thought that local control could not be obtained without significant toxicity.¹⁷

At Iowa State University in the 1950s, LDR-BT was performed by injecting 198Au colloid solution intratumorally via open and closed approaches.¹⁸ In this series, the 5-year survival was 48% , which was similar to other reported techniques at the time.^{18, 19} Despite the encouraging results, brachytherapy was still not accepted for several reasons. Firstly, reports of experience with EBRT began to be published in the 1960s, and this technique did not require anaesthesia and also was also associated with promising results and minimal morbidity.²⁰ Furthermore, ¹⁹⁸Au is a relatively high-energy isotope and, therefore, more challenging radiation safety precautions were necessary.

In the 1970s, Dr. Willet F. Whitmore and colleagues at Memorial Sloan–Kettering Cancer Center began to use 125I seeds for prostate cancer implants via an open surgical procedure that included a bilateral pelvic lymphadenectomy.^{21, 22} This 125 I technique was associated with several advantages over existing methods for EBRT and brachytherapy.¹⁴ Firstly, the open procedure permitted direct assessment of both the prostate and the lymph nodes. Secondly, the open approach permitted the precise placement of radioactive material, thus increasing the total tumour dose while minimizing exposure to the rectum and bladder. Thirdly, staging and implantation were performed at the same time. Notably, open procedures and intraprocedure staging are no longer performed in contemporary practice; by contrast, novel anatomical and functional imaging methods (including CT, MRI, and PET) have replaced invasive staging²³ and implantations are now performed via a transperineal approach.

Finally, 125I has several benefits in comparison to 198Au, which had been used in previous decades.14 125I has a lower energy, requiring less challenging radioprotection and providing improved dosimetry. 125 I has a low half-dose volume — that is, the volume of tissue receiving 50% of the minimum tumour dose — compared with 198 Au: 2 cm versus 6 cm. 24 125I also has a relatively long half-life of 60 days, providing extended periods of radiation to the target tissue. This extended duration of radiation was hypothesized to be radiobiologically favourable because of the long doubling time of prostate cancer cells, and

because it would allow for the repair of normal tissues, thereby minimizing acute genitourinary toxicities.²¹

In the 1970s and 1980s, patients who were selected for ¹²⁵I LDR-BT were anaesthetized, placed in a modified lithotomy position, and an infraumbiliical incision was made to perform the implantation.²⁴⁻²⁷ A bilateral pelvic lymph node dissection was performed, and the prostate was exposed. The prostate gland was mobilized by incising the endopelvic fascia bilaterally. Caliper measurements were used to assess the prostate dimensions: a needle was directed through the gland in the anteroposterior direction using a needle, with a finger placed in the rectum to prevent rectal perforation. Next, a nomogram was used to calculate the 3D volume. A computer was used to derive the matched peripheral dose, which was the absorbed dose at the periphery of an ellipsoid with the same dimensions. Doses at the centre of the gland were typically much higher than those at the periphery. Given the morbidity of incision, the limits of assessing prostate dimensions, and poor dose distribution and low total dose of ^{125}I , clinical outcomes were poor in many patients.²⁸

The application of transrectal ultrasonography (TRUS) to guide LDR-BT was successfully introduced in the 1980s.29 TRUS -guided LDR-BT was first developed in Denmark in the late 1970s, but with disappointing early clinical outcomes, likely related to suboptimal seed placement and dosimetry.^{30, 31} The lack of uniform dosimetry and the use of combination EBRT resulted in rectal ulcers.30-32

As techniques improved, ^{125}I and ^{103}Pd became the most commonly used isotopes in nonrandomized trials through the late 1980s.³³ TRUS-guided LDR-BT became a standard technique in the USA and elsewhere by the late 1990s because of improved associated outcomes and use of a less-invasive procedure compared with laparotomy-based suprapubic approaches.34,35 In the USA, LDR-BT was subsequently endorsed for treatment of low-risk prostate cancer by numerous organizations, including the ABS and the American Society for Radiation Oncology (ASTRO).³⁶

Although TRUS-guided LDR-BT is still a standard-of-care treatment option for men with prostate cancer, potential technical limitations of LDR-BT exist. Firstly, loose LDR-BT seeds — particularly those that are not held by a strand (termed 'stranded') — can migrate. ³⁷ Secondly, permanent implantation of radioactive material in the body, as is carried out for LDR-BT means that the implant emits a small but detectable dose of radiation for some months after implantation. Additionally, correct seed placement if highly operatordependent, seed cannot be adjusted once they are deposited. Thus, dosimetry might among implants. Furthermore, the multiple radioactive seeds required — ~100 seeds might need to be custom made for a particular date — is costly. By contrast, HDR-BT procedures use a single, reusable, 192 Ir source that lasts 3 months. However, relative cost is debatable, because in certain environments seeds are cheaper than HDR-BT, particularly if multiple HDR-BT fractions are used. Furthermore, LDR-BT exposures staff to radiation, although this exposure is very minimal.38 Finally, acute irritative urinary symptoms frequently occur as the radioactive sources of LDR-BT decay (FIG 1B). The acute toxicity period is more pronounced but shorter in duration for ^{131}Cs , which has a half-life of 9.7 days; by contrast,

the acute toxicity is less pronounced but longer in duration (by months) for 125 I, which has a half-life of 59 days.

History of HDR-BT

In the late 1980s, analysis of CT-based dosimetry revealed that dose coverage of LDR-BT plans was often lower than in the preplans. Thus, investigators explored the use of HDR-BT with 192 Ir to overcome these limitations³⁹, theorizing that the higher energy 192 Ir HDR-BT isotope would enable dose delivery to the periphery of the prostate in a highly conformal manner, assuring good tumour coverage and minimizing the dose to the adjacent bladder and rectum.39 Furthermore, this approach would enable the dose to differentially delivered within the peripheral zones of the prostate where the bulkier portions of carcinoma typically reside; $40,41$ this dose distribution would also limit dose to the central region that contains the urethra.³⁹

A TRUS-guided remote afterloading system (RALS) was first introduced in 1980 to deliver a high radiation dose to the prostate while limiting exposure of the surrounding tissues (FIG 1A) and to address some limitations of TRUS-guided LDR-BT, including high dependence on the operator for proper seed placement, inability to adjust seeds once they are deposited, and variability of dosimetry among implants.35 HDR-BT began to be used as a boost with EBRT in Sweden, Germany, Japan, the UK, and the USA in the 1980s and 1990s.^{35, 39, 42, 43}

HDR-BT boost was attempted before HDR-BT monotherapy because it was theorized to be an improvement over LDR-BT boost. With HDR-BT boost, staff would be completely protected from radiation exposure, and the procedure could be more widely applied, because abdominal surgery could be avoided.42 Safety and efficacy of HDR-BT boost was subsequently illustrated in Phase I/II and Phase III trials.⁴⁴⁻⁵⁶

By the 1990s, HDR-BT boost had been evaluated in many studies worldwide. In Osaka, Japan, a trial of HDR-BT monotherapy was initiated after a year of using HDR-BT boost, and the reports on HDR-BT monotherapy have been published since the year 2000.⁵⁷⁻⁶⁰ According to the authors, HDR-BT monotherapy was felt to be more advantageous than HDR-BT boost because with monotherapy the high dose per fraction of brachytherapy would not have to be reduced. Furthermore, any extracapsular spread of disease could be covered by dose from the needles. In the USA, a trial of HDR-BT monotherapy was conducted from 1999 to 2000, and the results were published in 2001.⁶¹ Patients with lowintermediate-risk prostate cancer were treated with HDR-BT, 38 Gy in four fractions of 9.5 Gy each, delivered twice a day over 2 days. None of the patients developed severe acute toxic effects.

The use of HDR-BT addresses some of the issues associated with LDR-BT, but it has its own disadvantages. For example, HDR-BT must be performed in a shielded room instead of an operating room, as in the case of LDR-BT; thus, start-up costs are associated with ensuring an appropriate environment. HDR-BT is typically performed in 1–3 implants and the catheters are left inside the patient to deliver 1–6 fractions in total. Typically, fractions must be separated by >6 h in order to capture cancer cells during the radiosensitive G2/M phase and allow DNA repair of normal cells. As an increased number of implants are used,

the risk of procedure-related events, including infection and bleeding, is also increased. 58, 62, 63 Furthermore, as many fractionation options are available for HDR-BT, no single dose for HDR-BT has been standardized, unlike for LDR-BT.

Current trends

The use of brachytherapy to treat patients with localized prostate cancer in the USA and western Europe has been steadily declining since 2003. In the USA, brachytherapy use (either as monotherapy or boost) reached a peak in 2002, with 17% of all prostate cancer patients receiving the therapy; in 2010, the rate decreased to 8% (FIG 2).⁶⁴ For intermediaterisk patients, use of brachytherapy boost decreased from 33% in 2004 to 12% in 2013; and for high-risk patients, use dropped from 27% to 11%.⁶⁵

The declining use of brachytherapy could be due to several reasons. Firstly, according to data from 2015, 30% of US medical school graduates are not aware of brachytherapy as a definitive treatment modality for cancer, and 10% do not believe that radiation therapy alone can be used to cure cancer.^{66, 67} Additionally, the declining rate of brachytherapy use in the USA might be due to the low and declining number of prostate brachytherapy procedures performed by residents.68-70 For example, the number of LDR-BT implantations performed in academic year 2006–2007 was 1,106 total, with a median of 14 per resident, and a range of 0–129. By academic year 2010–2011, the total number increased to 1,990, but the number of residents grew, and the median decreased to just 10 LDR-BT implantations per resident, with a range of $0-122.68-70$

The number of HDR-BT prostate implantations performed by trainees in the USA as a whole has been negligible. In academic year 2006–2007, the total number was 234 (median of 0 per resident; range 0–38); in academic year 2010–2011, the total number of was 336 (median of 0 per resident, range $0-71$).⁷⁰ Graduates are unlikely to develop the necessary skill to do the procedures with such few cases, as the associated learning curve means that $>$ 20 cases are likely necessary to perform the procedure acceptably without supervision.⁷¹⁻⁷³ By contrast, the number of Accreditation Council for Graduate Medical Education (ACGME)-accredited radiation oncology residency programmes has been growing: from 76 in 2011 to 89 in 2014. These data suggest that a growing number of graduating radiation oncology residents have a declining experience in brachytherapy for prostate cancer.

The use of brachytherapy could also be declining owing to developments in EBRT. EBRT developed in parallel with brachytherapy during the 1990s and 2000s, and employed hypofractionated regimens that used doses similar to HDR-BT. In 2001, development of the robotic arm linear accelerator used to deliver stereotactic body radiotherapy (SBRT) in dose fractionation schemes similar to HDR-BT was reported.^{74, 75} SBRT is a type of EBRT delivered as a single fraction lasting up to 45 min per day, for a total of \sim 5 treatments, each about 6–9 Gy, over ~2 weeks. As of 2016, no randomized trials comparing brachytherapy with any form of EBRT, including SBRT, have been performed.⁷⁶ Importantly, the dosimetric distribution of brachytherapy provides superior conformality and dose concentration to EBRT, in part because the X-rays do not pass through the bowel and bladder in order to reach the prostate (FIG 1B).^{4, 74}

Indications and contraindications to brachytherapy for prostate cancer

All patients require a biopsy to determine tumour Gleason score, pretherapy serum PSA measurement ,and clinical tumour classification with digital rectal examination and possible imaging with a CT of the pelvis before initiation of any form of treatment, as these prognostic factors determine risk classification.3, 77 Over 80% of prostate cancer patients do not die of their disease;⁷⁸ thus, maintaining quality of life is key in all patients. All patients should have their urinary and erectile function assessed with validated questionnaires, including the American Urologic Association (AUA), International Index of Erectile Function (IIEF-5), and/or Expanded Prostate Cancer Index Composite (EPIC), before treatment begins.3, 79

Indications

The National Comprehensive Cancer Network (NCCN) risk group classification for low-risk disease includes cancers with Gleason score $\,$ 6, serum PSA \lt 10 ng/ml, and clinical tumour classification T1 or T2a. For intermediate-risk disease, patients have Gleason score 7, or PSA 10 ng/ml 20 ng/ml or clinical tumour classification of T2b or T2c. For high-risk disease, patients have Gleason score 8–10, serum PSA >20 ng/ml, or clinical tumour classification of T3a. Additionally, in more recent versions of the NCCN guidelines³ and in studies of HDR-BT boost, $45, 46, 48, 50, 80-87$ a 'very-high' risk classification is made. In the NCCN guidelines, this includes patients with T3b–T4 disease, primary Gleason score 5, or >4 cores with Gleason score 4–5. In studies of HDR-BT boost, $45, 46, 48, 50, 80-87$ the definition is more heterogeneous and typically includes patients with multiple high-risk features; for example, Gleason 8 and a serum PSA level >20 ng/ml.

The NCCN guidelines state that brachytherapy monotherapy and boost (that is, in combination with EBRT) can be used as first-line therapies in the management of men with prostate cancer of all risk groups (Table 1).³ Monotherapy is an option for those with lowrisk disease and favourable intermediate-risk disease (evidence level 2, compared with EBRT). Brachytherapy boost is an option for patients with high-risk or very-high-risk disease. For high-risk patients, brachytherapy boost is preferred to brachytherapy or EBRT monotherapy because of improved outcomes (evidence level 1), based on retrospective evidence 88 and prospective studies. $54, 89$ For purposes of this Review, we consider high-risk and very-high-risk disease as a single high-risk category because the outcomes and toxicities are typically reported without dichotomization.

Contraindications

The presence of ataxia telangiectasia or pre-existing rectal fistula are absolute contraindications to any type of radiotherapy. Additionally, TRUS-guided brachytherapy has more contraindications than EBRT, including absence of a rectum meaning that TRUS guidance cannot be performed. Other relative contraindications include pubic arch interference, a large prostate or a urethral defect associated with previous transurethral resection of the prostate (TURP), a low peak urinary flow rate of $\langle 10 \text{ cm}^3/\text{s}$, and a postvoid residual volume >100 cm³.^{4, 8, 9} In the past, a gland size of >60 cm³ was generally considered a relative contraindication for LDR-BT, but LDR-BT can now easily be

performed for large prostates using 3D planning with CT or ultrasonography (rather than the caliper measurements performed in the $1950s$).⁹⁰ However, a large prostate can be accompanied by urinary bother symptoms, which would be exacerbated in the postimplant period. Additionally, the patient must be able to tolerate general anaesthesia. Multiple implantation procedures, typically 1–3 (to deliver 1–6 fractions), can be necessary for HDR-BT (FIG 1B). The procedure is typically performed under general anaesthesia; thus, a patient would need to be anaesthetized 1–3 times, and needles might need to be placed through the perineum 1–3 times, although one insertion followed by twice daily treatments

Androgen deprivation therapy (ADT) can be used with either form of brachytherapy in certain patients with intermediate-risk and high-risk disease or as a means of prostate cytoreduction in any patient.⁹¹ With respect to risk group, ADT is almost always recommended for patients with high-risk disease because it has been shown to improve overall survival in prospective trials of EBRT; ADT is typically recommended in patients with 'unfavorable' intermediate-risk prostate cancer — that is, those with primary Gleason pattern 4, $>50\%$ positive biopsy cores, or multiple intermediate-risk factors.⁹² However, the effect of ADT–brachytherapy combination on survival has not been confirmed as it has been with EBRT.^{91, 93-99}

Radiophysics and technical aspects

is common.

Target delineation

The GEC–ESTRO guidelines^{10, 11} provide detailed instructions for brachytherapy target delineation. Several differences exist in target volume expansions of brachytherapy ¹⁰⁰ versus EBRT (FIG 3).^{101, 102} The gross tumour volume (GTV) is the gross demonstrable extent and location of the malignant growth; it consists of the primary tumour — which for prostate cancer has historically been defined as the entire gland as well as any visualized extension into surrounding normal tissues — the regional lymph nodes, or distant metastases based on clinical data (that is, physical examination, anatomical imaging with CT and MRI, and functional and molecular imaging).^{101, 102} For both forms of brachytherapy, GTV is typically not contoured, unless gross disease — either intraprostatic or extraprostatic — is noted on imaging. The clinical target volume (CTV) encompasses the GTV as well as areas at risk for subclinical cancer involvement. The CTV can include a margin around the prostate GTV, and it might include adjacent regions at risk of having subclinical disease. For example, this might include the seminal vesicles and expansion for extraprostatic extension (EPE). For brachytherapy, the CTV is equivalent to the entire prostate gland, including the prostate capsule plus any macroscopic extracapsular disease, and a 3D expansion of 3 mm. The CTV is typically constrained anatomically by the anterior rectal wall and bladder base. 10 , 11 This definition is similar to that used in EBRT planning guidelines.^{101, 102}

The planning target volume (PTV) encompasses the CTV plus an additional margin to account for patient movement, setup error, and organ movement (for example, bladder or rectal distention). For prostate cancer treated with EBRT, the PTV is typically $\text{CTV} + 0.5 -$ 1.0 cm.^{101, 102} For brachytherapy, no further PTV expansion is required.^{10, 11} In the case of LDR-BT, once the needles are deposited, the dose cloud would cover the CTV, even if the

patient were to move or if there were organ movement. In the case of HDR-BT, the needles (typically about 12 in number) anchor the prostate while the 192 Ir source moves to the dwell positions for prespecified dwell times to deliver the prescribed dose. During the dose delivery, there should be no uncertainty regarding the position of the needles.

LDR-BT technical aspects

As of 2017, LDR-BT is typically performed with ^{125}I or ^{103}Pd radioisotopes; few centres use 131Cs, but this isotope is also an option (Table 2). The American Brachytherapy Society (ABS) does not recommend the use of one specific radionuclide.⁸ Both ^{125}I and ^{103}Pd have demonstrated excellent long-term outcomes; 131 Cs was introduced in 2004.^{103 125}I has the longest half-life of these three isotopes (59 days); hence, it tends to have a milder toxicity peak, and longer window of low-grade toxicity over 2–5 months. By contrast, ^{131}Cs has the shortest half-life (10 days) and causes more irritative symptoms in the 2–5 weeks following the implantation.

Before implantation, CT or a TRUS planning study can be performed to permit treatment planning as well as to calculate prostate volume so that radioactive seeds for the implant can be ordered. Alternatively, an intraoperative treatment planning approach can be followed, whereby all radiation treatment planning and delivery occurs in real time in a single procedure.¹⁰⁴ Additionally, real-time planning can be performed to overcome the limitations of preimplantation planning.104-106

With pre-implant planning, TRUS is performed a few weeks prior to the implantation, and the 3D placement of seeds, with resultant dose to cover the CTV, is modelled using a computer. However, preimplant dosimetry has limitations, including quality of the image: Distinguishing the density of the prostate parenchyma from the capsule and some of the pelvic floor musculature can be impossible. Moreover, seeds might not be deposited in the exact locations modelled by the programme. Thus, the intraoperative dose coverage might not be the same as that seen on the preoperative scan. With intraoperative planning using TRUS, the seeds are deposited as they would be with an intraoperative plan; if differences in anatomy or dose coverage are evaluated by TRUS-based computer planning, the deposition of additional seeds can be adjusted.

The standard procedure for implantation of brachytherapy seeds uses a transperineal approach under TRUS guidance with a template in place. Efforts are taken to ensure that patient position and TRUS-probe alignment closely replicates the preimplant planning study, if this has been performed. A high-resolution biplanar ultrasonography system operating at 5–12 MHz with dedicated prostate brachytherapy software is used. Fluoroscopy can be used as a complementary imaging modality to TRUS, and is typically used to check seed deposition. Fluoroscopy can be enhanced by the use of differential concentrations of contrast in the bladder and a Foley balloon partially radio-opaque catheter to identify the urethra, and gold fiducial markers implanted at the prostatic base and apex.107 In some centres, fluoroscopy is used for intraoperative dose calculation using image fusion.¹⁰⁸ However, this approach is not considered mandatory for successful LDR-BT.⁸

The ABS^8 recommends that CT-based postimplant dosimetry be performed within 60 days of implantation, in order to achieve good quality assurance.¹⁰⁹ A planning system generates dose–volume histograms, dose–volume statistics, and 2D and 3D isodose curves superimposed on CT and other images, including ultrasonographic and MRI. Careful postimplant assessment provides objective measures of implant quality. Postimplant dosimetry is typically performed on the day of LDR-BT and/or within 30 days after the implant, once the initial oedema has resolved. If logistically feasible and consistent with LDR-BT clinical trials, dosimetry performed at 3-4 weeks postimplant is preferred.¹⁰⁹

The time required for oedema to resolve and, therefore, the optimal time to perform the postimplant scan, depends on the radionuclide used: 16 ± 4 days for $103Pd$ and 30 ± 7 days for $125I$ and seems likely less for $131Cs$, though evidence for the use of $131Cs$ is limited. $8, 9, 110$ Reproducibility of postimplant dosimetry can be improved by using MR–CT image fusion.111, 112 The principle benefit of fusing MRI to the CT is for improved delineation of soft tissue, including the prostate, seminal vesicles, urethra, rectum, bladder, and penile bulb. 23, 113-116 Additionally, multiparametric MRI can help to delineate the GTV, where a focal boost could be administered.^{117, 118} The principal drawback is that many radiation oncology departments do not own a dedicated MRI unit, imaging is expensive (although the overall cost might be the same (119) , some patients might have contraindications to imaging (such as a pacemaker), and the MRI might not substantially improve tissue delineation at the prostatic apex, which is blurred by trauma after catheter insertion.¹¹⁷⁻¹¹⁹

LDR-BT dosimetric quality constraints—Several dosimetric quality constraints must be achieved (Table 2). The ABS, 8 ESTRO/EAU/EORTC, 10 , 11 and the American Association of Physicists in Medicine (AAPM)^{120, 121} recommend specific postbrachytherapy dosimetric parameters, according to the anatomy. The following terminology is used: the D(percent) is the minimum dose to the hottest percentage of the volume. The V(percent) is the percentage volume receiving a particular percent of the dose. The D(cc) is the dose to a specified cubic centimetres of a volume. The dose for any of these parameters can be described as a percent of the prescribed dose or in the Equivalent Dose in 2 Gy fractions (that is, the EQD2), which is converted using a radiobiological formula to approximate the dose of conventionally fractionated EBRT.

The ABS and AAPM recommend reporting dosimetric values in the prostate, bladder, and rectum. In the prostate D90, the minimum dose to the hottest 90% of the prostate volume in Gy, should be >100%. The prostate V100, the percentage volume receiving 100% of the dose, should be >90–95%. The prostate V150, the volume receiving 150% of the dose, should be $<50-60\%$

According to the ASTRO, ABS, and AAPM guidelines, the urethra $UV150$, 122 , 123 the percentage of the urethra that receives 150% of the prescription dose, should be 0. The UD5, or the average dose to the 5% of the hottest urethra volume, should be <150% of the prescribed dose. The urethra UD30 or the average dose to the 30% of the hottest urethra volume, should be $\langle 125\%$ of the prescribed dose. The GEC–ESTRO guidelines¹⁰ provide similar recommendations with slightly different terminology. In the prostatic urethra, the D10, or the dose to 10% of the urethra volume, should be $\langle 150\%$ of the prescription dose. A

secondary parameter, the D30, or the dose to 30% of the urethra, should be <130% of the prescription dose.

In the rectum, the $RV100$, the volume receiving 100% of the dose, should be <1 cc on day 0 dosimetry and $\langle 1.3 \text{ cc} \rangle$ on day 30 dosimetry. According to GEC–ESTRO guidelines, 10 the D2cc, or the dose to hottest 2 cubic centimetres of the rectum should be less than the prescribed dose; and the D0.1cc, the hotspot in the rectum, should be <200 Gy EQD2.

No agreement has been reached regarding the critical structures and dose constraints for postimplant erectile function, although the internal pudendal artery, penile bulb, and neurovascular bundles have been studied.¹²⁴⁻¹²⁶ Gillan *et al.*¹²⁴ calculated the dose from LDR-BT to the internal pudendal arteries. An increased dose to these arteries would purportedly place patients at higher risk of erectile dysfunction. The authors reported that the internal pudendal arteries can be visualized and receive a low but calculable dose from LDR-BT, but the clinical significance of this dose is unknown.¹²⁴ Conversely, Merrick *et al.* 125 report that radiation doses to the proximal penis are predictive of brachytherapy-induced erectile dysfunction; the authors recommend penile bulb D50 and D20 should be maintained \leq 40% and 60%, respectively, of the minimum peripheral dose. Buyyounouski *et al.*¹²⁶ recommend the use of MRI for better delineation of erectile tissues but do not provide dose constraints.

LDR-BT fractionation and sequencing

According to the ABS and GEC–ESTRO guidelines, $8, 10$ the recommended dose of LDR-BT monotherapy using ¹²⁵I is 145 Gy. For LDR-BT boost, the dose is 108–110 Gy. The recommended dose of LDR-BT monotherapy using $103Pd$ is 125 Gy, and that for $131Cs$ is 120 Gy. For LDR-BT boost, the dose is 90–100 Gy. The EBRT dose is 41.4–50.4 Gy at 1.8– 2 Gy fractions per day. Optimal 125I prostate implants should deliver a D90 of 140–180 Gy, based on postimplant dosimetry. Doses of >140 Gy for ^{125}I and > 125 Gy for ^{103}Pd seem to result in similar outcomes in retrospective studies.^{127, 128} For ¹²⁵I, doses >180 Gy are associated with a slight increase in long-term urinary symptoms.¹²⁹

EBRT is generally performed before LDR-BT, with a 2–8 week interval between the two therapies.⁸ No studies have been published investigating either the sequencing of LDR-BT and EBRT or the time interval between the modalities. The downside of delivering LDR-BT before EBRT is that it exposes tissues to radiation simultaneously from both treatments and can theoretically increase toxic effects on normal tissue. By contrast, performing LDR-BT first enables physician assessment of the dose distribution⁸ and the seeds can be used as fiducial markers for daily image guidance during EBRT (FIG 1c).

Technical aspects of HDR-BT

During the HDR-BT procedure, a RALS automatically deploys and retracts a single small radioactive source of 192 Ir along the implant needle at specific positions delivering 12 Gy/h, compared with 0.4–2.0 Gy/h with LDR-BT. The RALS enables a physician to control the position where the HDR source stops (the dwell position) for a predetermined time period (the dwell time). The ¹⁹²Ir used in HDR-BT is contained within the needles placed in the prostate during this temporary implant; thus, the target does not move during radiation,

and seed migration, is not possible, as it is with LDR-BT.^{130, 131} Moreover, the treating clinicians are not exposed to radiation, and source preparation is not required, unlike the case with LDR-BT.132 Furthermore, ultrasonography-based planning minimizes catheter displacement.55, 56, 63

HDR-BT has a number of benefits compared with EBRT and LDR-BT, some of which are theoretical and not yet validated in the clinic. Firstly, HDR-BT has the potential to increase prostate-cancer-cell death and minimize radiation-related toxicity by widening the therapeutic ratio, depending on the fractionation, α/β ratio, and relative biologically equivalent dose (BED).^{35, 63, 75, 133}

Secondly, dosimetry is improved, as a range of dwell times can be employed at each dwell position, with better dose distribution than EBRT (FIG 1B).^{134, 135} Thirdly, the treatment is completed in a few fractions over 1–4 days, which is more convenient for the patient than a protracted course of conventional EBRT.11, 35, 55, 63, 136-140

Notably, both LDR-BT and HDR-BT have excellent dosimetry. Additionally, both forms of brachytherapy are similarly economically favourable versus EBRT. Costs of LDR-BT and HDR-BT take into account initial investment cost, including shielding necessary for HDR-BT, the cost for each implant, as new sources must be used for LDR-BT, the cost of the number of implants per patient, and the number of patients treated with the device, as well as other potential uses for the modality, such as gynaecological implants to additionally treat these cancers using HDR-BT (Table 3).

HDR-BT dosimetric quality constraints—During an HDR-BT procedure, the physician implants the needles, and a dosimetrist or physicist prepares a plan. Next, the physician reviews the plan, and the dosimetrist or physicist mcan make requested changes to the plan. Once the plan is optimized, the physician approves the plan, and the treatment is delivered. The ABS⁹ and GEC–ESTRO¹¹ guidelines state that the CTV V100 should be >90% . The ABS does not provide normal tissue constraints given the heterogeneity in dose fractionation.⁹ The GEC–ESTRO¹¹ guidelines provide constraints, with conversion into the EQD2 (Table 2).

Comparison of dosimetry among EBRT, LDR-BT, and HDR-BT

Both LDR-BT and HDR-BT have favourable dosimetry compared with EBRT. The majority of prostate cancers develop in the peripheral zone of the gland, and brachytherapy plans can be tailored to deposit the highest dose in this zone $(FIG 4a)$.⁴⁰ Furthermore, several caveats to dose prescriptions differentiate EBRT from brachytherapy.

In the 1990s, EBRT was delivered using 3D conformal radiation therapy (3D-CRT), whereby multiple beams were centred on the prostate $(FIG 4B)^{141}$. With 3D-CRT, the maximal point dose was toward the centre of the prostate, near the urethra; the dose decreased gradually toward the periphery of the prostate. Intensity modulated radiation therapy (IMRT) was introduced in the early 1990s as a further refinement in the delivery of highly-conformal radiation because it increases the dose delivered to the tumour volume and minimizes the dose delivered to surrounding organs.³⁵ IMRT was made possible by use of a

multileaf collimator (MLC), a device made up of individual leaves of a high atomic numbered material that can move independently in and out of the path of a photon beam to contour its shape to a tumour, and advanced treatment planning calculation algorithms, which enable inverse optimization of MLC positioning for complex dose delivery.³⁵

The dose distribution created by IMRT is characterized by a concavity or invagination of the edge of the higher doses away from the rectum, rather than a straight edge through the rectum as seen with 3D-CRT. IMRT ensures coverage of the entire prostate gland with dose and minimizes hotspots within the gland. Nonetheless, with IMRT, the prescription dose must be delivered to the PTV, which expands outside of the prostate (FIG 4b). With SBRT (FIG 4b), radiotherapy is prescribed to an isodose line to cover the PTV. Furthermore, the hotspot is in the centre of the prostate toward the urethra; although a urethra dose constraint is provided by clinical trials and guidelines, $101, 102$ the higher dose toward the centre of the gland with SBRT is sometimes unavoidable.74, 75

With LDR-BT and HDR-BT, the dose can be differentially delivered within the peripheral zones of the prostate, and the dose towards the centre of the gland can be minimized (FIG 4c). Furthermore, as the CTV is equivalent to the PTV for brachytherapy, the dose is not prescribed to a large volume outside of the gland. With HDR-BT, the hotspots, assessed by looking at the V150 (or volume receiving 150% of the prescribed dose), are typically smaller than in LDR-BT (FIG 4c); whether this is an advantage or disadvantage is unclear.

HDR-BT fractionation and sequencing

Monotherapy—For HDR-BT monotherapy, various options are available according to GEC–ESTRO¹¹: 34 Gy in four fractions at 8.5 Gy per fraction, 36–38 Gy in four fractions at about 9.25 Gy per fraction, 31.5 Gy in 3 fractions at 10.5 Gy per fraction, and 26 Gy in two fractions at 13.5 Gy per fraction.

Boost—The standard doses used in HDR-BT boost vary among institutions.⁹ Based on systematic reviews, $55, 56$ EBRT is usually delivered to a total dose of 36–54 Gy in 1.8–2.0 Gy fractions and HDR-BT is typically delivered to a total dose of 12–30 Gy in 1–4 fractions. GEC-ESTRO recommends: 45 Gy in 25 fractions over 5 weeks; 46 Gy in 23 fractions over 4.5 weeks, 35.7 Gy in 13 fractions over 2.5 weeks, or 37.5 Gy in 15 fractions over 3 weeks.

A particular brachytherapy dose fractionation schedule has not been recommended by the ABS^9 and various options are available according to GEC–ESTRO: 15 Gy in three fractions at 5 Gy per fraction, 11–22 Gy in two fractions at 5.5–11 Gy fractions; or 12–15 Gy in a single fraction. 11

Thus, for HDR-BT boost, the dose is typically delivered in 1–2 implants, using 2–6 fractions. Each fraction of radiation is 9–15 Gy: a lower dose-per-fraction is used if more fractions are delivered (for example four fractions of 8.5 Gy), or a higher dose-per-fraction is used if fewer fractions are used (for example a single fraction of 15 Gy).^{60, 142-156} The separate insertion schedule results in a greater workload of resource-intensive procedures and a greater anaesthesia time than the single-insertion procedure, which can require

overnight hospital admission and is associated with risks of interfractional catheter displacement.⁶²

Two HDR-BT boost fractionation schedules have evolved most likely because of preference by the physician, centre, and reimbursement models.55, 56 A separate procedure for catheter insertion for each fraction is typically used in European countries. A single insertion followed by $1-4$ fractions delivered over $1-2$ days is favoured in North American centres.⁵¹ Currently, 15 Gy in one fraction is the dose schedule in use in the Radiation Therapy Oncology Group 0924 Phase III trial of dose-escalated radiation therapy with or without pelvic nodal irradiation in HDR-BT.⁶³

Three temporal approaches for combining EBRT and HDR-BT have been described (FIG 1c).55, 56 If EBRT is delivered first, HDR-BT is typically delivered 1–6 weeks later. One benefit of this method is to dose escalate a particular part of the prostate that contains the GTV, though this approach is still investigational. One disadvantage of this method is the oedema caused by EBRT, which can make the implant technically challenging and worsen the toxicity of HDR-BT. Centres are using this method in the USA,47, 82, 152, 157-159 Australia,^{152, 160-162} Europe,^{50, 54, 163, 164} Japan,¹⁶⁵⁻¹⁶⁷ Canada,¹⁶⁸ and the UK.⁵⁴

Alternatively, HDR-BT can be delivered first, with EBRT delivered 1–3 weeks later. With this method, EBRT can be used to compensate for suboptimal implant dosimetry of HDR-BT; furthermore, preimplant radiation-induced oedema and genitourinary symptoms that typically follow EBRT are minimized.169 A disadvantage of this method is the delayed application of radiotherapy to pelvic lymph nodes (if these are included in the treatment volume). This method is in use in Europe (including the UK), 152, 170-172 the USA, 47, 52, 152, 173-176 Australia, 44, 177, 178 China, ^{179, 180} Brazil, ¹⁸¹ Canada.⁵¹

Finally, EBRT can be interdigitated with HDR-BT. This technique combines some of the advantages and disadvantages of the other temporal approaches. EBRT is delivered on days when HDR-BT is not delivered, thus minimizing treatment time prolongation and possible accelerated repopulation that would be present with a split course of radiotherapy. Centres are using the interdigitated method in Europe, ^{45, 46, 80, 182-185} the USA, ^{45, 53, 183, 186} and Japan.166, 187

Radiobiology

Fractionation — which refers to dividing a radiation dose into smaller doses given at least 6 h apart — has several theoretical radiobiological advantages including repair of normal tissue damage, redistribution of cancer cells into radiosensitive phases of the cycle (G2–M), and reoxygenation of the tumour. Thus, fractionation might increase the efficacy of radiotherapy. As the total fractionated radiation dose delivered increases, the number of surviving cells within the treated volume decreases.¹⁸⁸ However, the benefits of an increased total dose are offset by increased toxicity to the surrounding normal tissue.

The α/β ratio is used to describe the dose response of radiation on different tissues. The α/β ratio is thought to be 10 Gy for early-responding tissues, including skin, mucosa, and most malignant tumours, and 3–5 Gy for late-responding tissues, including connective tissues and

muscles. Clinical radiobiological models suggest that prostate cancer has a low α/β ratio (~1.5), compared with most other malignancies.¹⁸⁹ The α/β ratio is an important component of dose equivalent formulae used to convert different fractionation schedules into a common currency. It includes other assumptions in relation to repair and repopulation. A simplified form of the BED formula is often used to relate different fractionation schedules, where n is the number of radiation fractions and d is dose size per fraction: BED = $(nd[1 + d'(\alpha/\beta))$

If the a/B ratio for the tumour is lower than that of the surrounding tissues, as is hypothesized for prostate cancer, increasing the dose per fraction increases the BED more for the tumour than for the normal tissues; that is, the $BED_{1.5}$ increases more than BED_{10} .³⁵ The diverging BED values result in an increase in the therapeutic ratio.^{190, 191} Radiobiological models approximate cell death due to DNA damage from radiation therapy using conventional fractionation, that is, 1.8–2.0 Gy per fraction. However, the models do not account for cell death due to other mechanisms (as seen with $>$ 5 Gy per fraction), including lipid membrane phosphorylation, necroptosis, or immune-mediated death,¹⁹²⁻¹⁹⁵ but, they do account for vasculogenesis secondary to mesenchymal stem cell infiltration.¹⁹⁶ Thus, the higher BED of hypofractionated approaches suggests a theoretical benefit of HDR-BT versus conventionally fractionated EBRT. Similar estimates for the BED of LDR-BT show that optimal ^{125}I prostate implants should deliver a D90 of 140–180 Gy, based on postimplant dosimetry. Doses of <140 Gy are associated with increased biochemical failure rates and doses >180 Gy with a slight increase in long-term urinary symptoms.^{129, 197}

Cost

Brachytherapy is typically much more efficient, in terms of the resources it consumes,¹⁹⁸ than EBRT.35 For radiotherapy, calculation models show that wage costs outweigh the cost of machines, owing to the labour-intensive nature of radiotherapy planning and delivery. ^{139, 140} For treatment of a patient with prostate cancer using 40 fractions of EBRT, staffing of radiotherapy facilities accounts for an estimated 50% of the cost.199 Additionally, although IMRT treatment planning is complex, the planning is only done at the beginning of therapy, while cost builds with the delivery of each fraction.¹³⁶ Thus, changing to a hypofractionated schedule or brachytherapy could decrease the number of work-hours and overall cost of treating each patient.⁷⁵ By contrast, brachytherapy treatment is substantially more efficient — based on American Medicare reimbursements, per-patient costs of conventionally fractionated EBRT with intensity modulation, LDR-BT, and HDR-BT with four fractions, are estimated at \$29,356, \$9,938, and \$17,514 respectively.137 LDR-BT might have a lower initial capital expense requirement than HDR-BT, in part because the kV energy isotopes used for LDR-BT do not require use of a shielded room and the procedure can be performed in an operating room, unlike that of mV energy 192 Ir used for HDR-BT, which requires a special vault. Nonetheless, both forms of brachytherapy are relatively inexpensive.

Clinical outcomes and toxicities

Level 2 evidence regarding outcomes for HDR-BT and LDR-BT suggests they are similar in patients with low-risk and favourable intermediate-risk disease.⁴ Furthermore, level 1

evidence shows improved quality of life with brachytherapy over prostatectomy, based on the results of the Surgical Prostatectomy Versus Interstitial Radiation Intervention Trial (SPIRIT).200 For both types of brachytherapy, the 5-year freedom from biochemical failure (FFBF) outcomes for patients with low-risk, intermediate-risk, and high-risk disease are $>85\%$, 69–97%, and 63–80%, respectively.^{4, 56}

Brachytherapy plus EBRT (as opposed to brachytherapy alone) is an appropriate approach in select patients with intermediate-risk and high-risk disease (evidence level $1)^4$ using either LDR-BT 89 or HDR-BT, $^{54, 201}$ (Table 1;Box 1). Briefly, patients who benefit from brachytherapy boost are typically those with unfavourable-intermediate risk and high-risk disease. Patients receiving boost should have no absolute contraindications to the treatment, including ataxia telangiectasia, a pre-existing rectal fistula, unacceptable operative risks, distant metastases, absence of a rectum such that TRUS-guidance is precluded, or large TURP defect that would result in unacceptable dosimetry. Other factors, including history of previous pelvic radiotherapy, limited life expectancy, and moderate-to-severe urinary symptoms are relative contraindications.

LDR-BT

LDR-BT monotherapy for low-risk disease—Patients with low-risk features deemed suitable candidates for LDR-BT can be appropriately treated with LDR-BT monotherapy. Published studies demonstrate that excellent long-term outcomes can be expected when optimal dosimetric parameters are achieved.202-204 According to a review published by the Prostate Cancer Results Study Group, the 10-year rates of FFBF for patients with low-risk disease receiving LDR-BT monotherapy have been estimated at $>86\%$.²⁰⁵ Rates of prostate cancer distant metastasis, prostate-cancer-specific mortality (PCSM), and overall survival (OS) in these patients are estimated to be $\langle 10\%, \langle 5\%, \text{ and } \rangle 85\%,$ respectively, at 10 years after treatment.²⁰⁵ and grade 3–4 toxicities occur in $\langle 4\%$ of patients (Table 4).

LDR-BT monotherapy or boost for intermediate-risk disease—For patients with intermediate-risk disease, the appropriateness of LDR-BT monotherapy depends on many factors including the required margin of treatment. In pathological series of whole-mount radical prostatectomy specimens of $\langle pT3 \rangle$ disease defined as being organ-confined, $^{206-209}$ the radial extraprostatic extension (EPE) rarely extends >5 mm; the posterolateral region, which is near the seminal vesicles, is at highest risk of $EPE²¹⁰$ Many intermediate-risk tumours have equivalent or even lower risk of adverse pathological features such as EPE, seminal vesicle invasion, or lymph node involvement. Thus, they can be treated with LDR-BT monotherapy.211 A recommended margin of 3 mm around the prostate is used as the planning target volume in all directions, except posteriorly because this would expose the rectum to high doses of radiation. This expansion usually encompasses all EPE in intermediate-risk disease.⁸

In the RTOG 0232 study, which ran from 2003 to 2012, patients with intermediate-risk prostate cancer were randomized to receive LDR-BT alone (with either ^{103}Pd or ^{125}I) or EBRT (45 Gy, partial pelvis, 1.8 Gy/fraction), followed by LDR-BT. Based on the report released in 2016, the addition of EBRT to LDR-BT did not result in superior FFBF (80% at

5 years for LDR-BT and LDR-BT + EBRT), overall survival, distant metastasis rate, or PCSM²¹². Additionally, participants in the LDR-BT-alone arm experienced fewer late events than the EBRT group: 53% versus 37% for any late Grade 2+ effects and 12% versus 7% for any late Grade 3+ effects.

The 10-year rates of FFBF for patients with intermediate-risk disease receiving LDR-BT monotherapy is estimated to be $>65\%$, with most reports around 90%.²⁰⁵ In a multiinstitutional analysis of about 3,000 patients with prostate cancer, including 960 men with intermediate-risk disease, the 8-year FFBF rate was 70%.204 Notably, the majority of these patients were treated before 1999 and fewer than 25% had formal postimplantation quality assurance.109 A survey of 18 brachytherapy practitioners who treated over 10,000 patients with LDR-BT suggested that practitioners employ monotherapy carefully, on a case-by-case basis. ²¹³

LDR-BT boost for high-risk disease—LDR-BT boost is an accepted treatment modality for patients with high-risk disease.^{8, 9} Outcomes and toxicities of LDR-BT boost have been reported from Radiation Therapy Oncology Group (RTOG) 0019²¹⁴, Cancer, Leukemia Group B (CALGB) 99809,²¹⁵ and the Androgen Suppression Combined with Elective Nodal and Dose Escalated Radiation Therapy (ASCENDE-RT, clinical trial number [NCT00175396\)](https://clinicaltrials.gov/ct2/show/NCT00175396).⁸⁹ In ASCENDE-RT, LDR-BT boost was shown to be superior to EBRT in terms of FFBF, bodily pain, general health, sexual function, and urinary function.⁸⁹ Additionally, in a retrospective cohort of 245 patients receiving LDR-BT (with or without a boost) rates of Grade 2 and 3 rectal toxicities were estimated to be 7% and 3%, respectively.²¹⁶ The risk of Grade $\,$ 2 rectal toxicity was 2.8-fold higher in patients receiving supplemental EBRT compared with LDR-BT alone, and the risk of Grade $\overline{3}$ rectal toxicity was 11.9-fold higher (Table 4).²¹⁶ Toxic effects are likely to be due, in part, to patient comorbidities, including increased BMI and hyperglycaemia or hyperinsulinaemia.217, 218 Incontinence is not a common toxic effect after brachytherapy.

ADT in combination with EBRT (in the neoadjuvant, concurrent, and adjuvant settings) has been shown to improve patient outcomes over the use EBRT alone in multiple clinical trials. 91, 93-99, 219-221 However, the data regarding the addition of ADT to LDR-BT patients is less robust than for results regarding EBRT. Merrick et al.²²² reported that 10-year FFBF was improved with the addition of ADT, but overall survival and PCSM were not. In addition, a multi-institutional series reported by Stone *et al.*²²³ showed that patients with Gleason score 8–10 tumours had improved overall survival and freedom from distant metastasis with higher doses (BED_{10} > 220 Gy) of LDR-BT.

HDR-BT

HDR-BT monotherapy for low-risk and intermediate-risk disease—HDR-BT

monotherapy can be used in select (Table 1; Box 1) patients with low-risk and intermediaterisk disease.4, 63 The ABS and GEC–ESTRO guidelines recommend monotherapy for patients with high-risk disease only in a clinical trial or in case-by-case circumstances.^{9, 11} In a systematic review of HDR-BT monotherapy, FFBF rates for patients with low-risk, intermediate-risk, and high-risk disease are $85%$ at up to 5 years.^{60, 142-156} Overall

survival, prostate cancer specific mortality, local recurrence, and distant metastasis rates are typically > 95%, < 4%, < 4%, and < 4%, respectively.⁶³ The highest rate of distant metastasis was reported by Yoshioka and colleagues^{153, 154} but was secondary to their inclusion of a greater number of patients with high-risk disease than other studies. Based on a systematic review, grade 3–4 gastrointestinal or genitourinary toxicity is seen in <5% of patients.⁶³

In one of the largest series of HDR-BT monotherapy from the University of California, Los Angeles (UCLA), 224 the authors reported encouraging outcomes with 6.5 years of follow-up monitoring, which was some of the longest follow-up available at that time, but likely not long enough to draw long-term outcome conclusions. Similar to LDR-BT, HDR-BT monotherapy is associated with excellent and comparable rates of biochemical control, patient survival, treatment toxicity, and erectile preservation.⁶³

HDR-BT boost for intermediate-risk and high-risk disease—HDR-BT boost beneficial in patients with intermediate-risk and high-risk disease because it combines the benefits of conventionally fractionated EBRT or hypofractionated EBRT monotherapy to cover extraprostatic disease with the high radiation dose delivered to the CTV by HDR-BT. 56, 225 Thus, the BED achieved with HDR-BT boost is typically much higher than can be achieved with EBRT alone; at an α/β ratio of 1.5, the BEDs are 200–300 for HDR-BT boost versus ~187 for EBRT monotherapy of 80 Gy in 2.0 Gy fractions (FIG 5).^{56, 226}

Hoskin *et al.*⁵⁴ published one of the few randomized trials performed, including 220 patients randomized to HDR-BT boost versus EBRT alone. After a median follow-up duration of 85 months, a noticeable improvement in was observed in recurrence-free survival for patients who received HDR-BT boost, with a median time to relapse of 116 months compared with 74 months for EBRT alone. The 5-year, 7-year and 10-year estimates of FFBF were 75%, 66% and 46%, respectively, for HDR-BT boost, compared with 61%, 48% and 39%, respectively, for EBRT alone (log rank $P = 0.04$). T3 disease was present in 27% of their population and Gleason score $\frac{7 \text{ in } 58\%}{2 \text{ The } 5\text{-year}}$ and $\frac{7 \text{ - year}}{2 \text{ - year}}$ incidences for patients with any severe urinary symptom were 26% and 31%, respectively for those treated with HDR-BT boost compared with 26% and 30%, respectively, for those given EBRT alone (log rank P $= 0.5$). The authors concluded that HDR-BT boost could have an important role in the treatment of patients with intermediate-risk and high-risk disease.

A number of other prospective studies have been performed using HDR-BT boost. 44-46, 48, 51, 53, 54, 161, 174, 175, 183 In a systematic review of these studies, ⁵⁶ the reported 5year prostate-cancer-specific mortality, overall survival, local recurrence rates, and distant metastasis rates were 99–100%, 85–100%, 0–8%, and 0–12%, respectively. These outcomes are similar to those of LDR-BT, EBRT, and LDR-BT boost^{55, 56} and better than EBRT alone, as reported in ASCENDE-RT.54 Studies reporting outcomes outside of these ranges typically include patients with high-risk and locally advanced disease or exclude patients who have received ADT.^{45, 48, 49, 53, 183}

Based on systematic reviews, 55, 56 the rates of Grade 3–4 genitourinary and gastrointestinal toxicities are $0-12\%$ and $0-8\%$, respectively, in phase I/II studies with 4-year median

follow-up duration44, 46, 48, 52, 53. Furthermore, among studies that compare HDR-BT boost with EBRT alone, the rate of stricture occurrence is considerably higher in the boost arm. 54, 160, 162 RTOG 032147, the first multi-institutional prospective trial using HDR-BT boost in the USA, provided detailed reports of toxicity and stricture occurrence. With a median follow-up period of 2.5 years, RTOG 0321 reported a rate of 2.6% for Grade 3–4 toxic effects, and a rate of urinary stricture of 0.7% ⁴⁷.

The outcomes of HDR-BT boost are encouraging, particularly for high-risk prostate cancer. One of the most important factors associated with outcome analyses is the role of ADT, which is associated with improved rates of FFBF, distant metastasis-free survival, and prostate-cancer-specific survival.^{91, 227} However, the role of ADT is often overlooked and in the systematic reviews of published studies, no multivariate analysis is performed to evaluate the effect of ADT on outcomes.^{55, 56} In the prospective study by Hoskin and colleagues⁵⁴, treatment arm, risk category, and ADT use were significant covariates for biochemical recurrence.

The toxic effects associated with of HDR-BT boost are similarly encouraging, and in systematic reviews of prospective studies, the late Grade 3–4 toxicity rate is <5% (Table 4). 55, 56, 62 By contrast, Grade 3–4 toxicities, including stricture, occur in <3% of patients receiving EBRT alone.^{4, 56, 228} LDR-BT boost RTOG Grade 3–4 genitourinary toxicities, including stricture, from two phase II studies were observed in $13\%^{214}$ and $3\%^{215}$ of patients, and gastrointestinal toxicities were seen in 3%214 and 0%215 of patients. Besides dosimetric quality constraints, characteristics predicting late toxicity include initial presence of symptoms,¹⁵⁷ ADT use,^{157, 180} older age (> ~65 years),^{157, 181} high-risk status,¹⁸⁰ previous transurethral resection of the prostate,^{152, 171} hypertension,¹⁵² and diabetes.²²⁹ Based on these data, HDT-BT is not an ideal treatment modality for all patients with highrisk prostate cancer, and clinicians might choose to use another modality, for example EBRT alone, in elderly patients with comorbidities.

In summary, HDR-BT boost is now a well-established treatment modality for patients with intermediate-risk and high-risk prostate cancer, particularly those without contraindications (Box 1). Similarly, HDR-BT monotherapy is associated with excellent outcomes and toxicity profiles in men with low-risk and favourable intermediate-risk disease. HDR-BT monotherapy studies tend to have a shorter follow-up time and include fewer patients than studies of LDR-BT and EBRT; thus, studies with >10–15 years of follow-up duration that report efficacy and toxicity will not be published until the 2020s.

Salvage for local recurrence after EBRT

Brachytherapy with either LDR-BT or HDR-BT monotherapy are possible treatments for local recurrence after EBRT or LDR-BT.²³⁰⁻²³⁴ Salvage brachytherapy is a promising option, particularly for patients who are not deemed fit for salvage prostatectomy. The NCCN guidelines include few recommendations regarding the approach; 3 thus, referral to a specialty centre with salvage experience is recommended.

Nguyen *et al.*²³⁵ published a prospective phase II study of MRI-guided salvage brachytherapy for 24 men with a rising serum PSA and biopsy-proven, intraprostatic cancer at least 2 years after initial radiotherapy (EBRT or brachytherapy), who had favourable clinical features: Gleason score <8, serum PSA < 0 ng/ml, and negative pelvic and bone imaging studies. They achieved biochemical control in 70% of patients at 4 years after the salvage procedure. The 4-year estimate of grade 3+ gastrointestinal or genitourinary toxicity was 30% and 13 patients required a colostomy and/or urostomy to repair a fistula.

The ideal salvage brachytherapy patient $(Box 2)^{235-238}$ should have biopsy-proven localonly recurrence, preferably with no evidence of widely metastatic disease, or none that cannot be controlled with focal therapy at other sites (for example, SBRT for oligometastatic recurrence).239, 240 Factors that suggest a local-only recurrence are the presence of a nadir after initial therapy, PSA doubling time >1–2 years, recurrent serum PSA measurements <10 ng/mL, and no Gleason 8–10 disease, which is more likely to disseminate241. For patients with widely metastatic disease, the excessive morbidity of local therapy and likely lack of a survival benefit obviate the need for salvage brachytherapy. Next, the patient should have minimal, and preferably no, morbidity from previous radiotherapy, and that treatment should have been performed >4.5 years before the date of salvage brachytherapy.²³⁵ Patients with ongoing toxic sequlae, such as a nonhealing ulcer, are unlikely to benefit from salvage brachytherapy and are more likely to develop further toxic effects, including infection, bleeding, pain, necrosis, and blood clots. Additionally, the patient should have no contraindications to prevent use of pelvic MRI, which is used to delineate the region of recurrence and for brachytherapy planning.235 Finally, the use of a rectal spacer can be considered to minimize radiation dose to the rectum.²³⁸

Ongoing trials

Several studies are currently in progress to directly compare LDR-BT with HDR-BT (Table 5). Additionally, several studies are evaluating the efficacy of HDR-BT for local recurrence. The use of brachytherapy as a focal boost to treat part of the prostate in the area identified to have the cancer focus, either with biopsy or novel imaging, is also under investigation.

Focal therapy aims to minimize the volume of normal tissue irradiated (rectum, bladder, urethra) and maximize the dose to tumour, which is typically identified using imaging studies. In a systematic review of focal therapy in the management of localized prostate cancer that included 2,350 patients across 30 studies, brachytherapy was used in only two of these studies, and one was in the setting of recurrent disease.235 Thus, the ideal patient and dose for focal therapy are not well established; the meta-analysis states that focal therapy was mainly delivered to men with low-risk and intermediate-risk disease.²⁴²

Follow-up monitoring

After brachytherapy, close follow-up monitoring with serum PSA measurements at regular intervals is recommended, as well as a digital rectal examination (DRE). The optimal surveillance frequency following brachytherapy has not been established. According to the NCCN and ABS guidelines, an interval of every 6–12 months is appropriate for most

patients, but those with high-risk disease should be monitored more frequently.^{3, 8} Quality of life (QOL) measurements can include the Short Form-36 (SF-36), the Client Satisfaction Questionnaire-8 (CSQ-8), the Functional Assessment of Cancer Therapy-General (FACT-G), the European Organization for Research and Treatment of Cancer (EORTC) Quality of Life Questionnaire (QLQ)–C30 (EORTC QLQ–C30), the University of California, Los Angeles Prostate Cancer Index (UCLA-PCI), and the Expanded Prostate Cancer Index Composite $(EPIC).$ ⁷⁹ All of these forms capture the recommended quality-of-life components: urinary incontinence, urinary obstruction and irritation, bowel-related symptoms, sexual dysfunction, and hormonal symptoms.243 Among the various metrics, the EPIC, UCLA-PCI, and EORTC are the most frequently used and are preferred.243-247248, 249

Other QOL metrics available include the AUA International Prostate Symptom Score (I-PSS) and the Sexual Health Inventory for Men (SHIM).²⁵⁰ The IPSS is intended to evaluate men with benign prostatic hypertrophy, whereas the SHIM was designed by industry to evaluate therapies for erectile dysfunction^{251, 252} Although these are sometimes used for QOL comparison, they are not preferred as they do not capture such a wide range of data as is collected in the EPIC, UCLA-PCI, or EORTC QLQ-C30.253 For example, the IPSS score does not collect information about incontinence.

PSA kinetics should be monitored after brachytherapy (FIG 6). Biochemical failure can be defined in a number of ways: the ABS and ASTRO favour the use of the Phoenix definition (PSA nadir $+ 2$ ng/ml) following treatment. After LDR-BT, PSA decreases to < 0.3 ng/ml in most men with localized disease.254 Patients should also be monitored for biochemical failure, keeping in mind that the features of benign PSA bounces and biochemical failure overlap substantially, although benign bounce is uncommon after 36 months.²⁵⁵

PSA bounce can occur after any form of radiotherapy, and the clinician must appreciate that PSA bounces are common, do not automatically represent cancer recurrence, and are associated with various patient, cancer, and dosimetric factors (for example, the urethra D90).²⁵⁶ A routine biopsy is not usually recommended; however, before any treatment is recommended or initiated, cancer recurrence needs to be documented by biopsy or imaging. 23, 241 If a rising PSA is noted and prostate biopsy is performed, the biopsy should be done ≥30 months after completion of LDR-BT, or it might be uninterpretable, and a false positive result can be mistakenly determined when actually a benign PSA bounce is likely.²⁵⁷

PSA bounces >1.0 ng/ml are rare after LDR-BT with or without neoadjuvant ADT, occurring in $<10\%$ of patients.²⁵⁸ However, as PSA bounce amplitude increases, the biochemical failure rate also increases.258 By contrast, patients with Gleason score 6 disease are more likely to experience a PSA bounce and have improved FFBF.259 An increased prostatic urethra D90 seems to correlate with the likelihood of having a PSA bounce, and PSA levels typically take 2–3 years to reach the nadir.²⁵⁶

The PSA nadir is typically a very low after HDR-BT, <0.05ng/ml.²⁶⁰ The rate of PSA bounce seems to be more frequent in patients treated with LDR-BT than those who received HDR-BT or EBRT, at 42%, 23%, and 20%, respectively.261 In a series of 114 men treated with HDR-BT boost with hypofractionated EBRT, PSA bounce occurred in 39% of patients

after a median of 16 months. The median magnitude of bounce was 0.45 ng/ml and biochemical failure occurred in 11% of patients who experienced a bounce.²⁶² In a separate series of 67 patients, 43% experienced a PSA bounce; among all patients treated with HDR-BT monotherapy, 28% of patients have a bounce < 1 ng/mL and 15% have a bounce higher than 1 ng/mL 263 Patients who experienced a PSA bounce typically had a lower Gleason score tumour than those who did not experience a bounce and were aged $<$ 55 years.²⁶³ The authors provided several hypotheses for these findings, including more frequent sexual activity among younger patients.

Conclusions

Brachytherapy and brachytherapy boost are excellent first-line therapies in the management of men with prostate cancer. LDR-BT monotherapy is acknowledged as a standard option in low-risk prostate cancer by health organizations internationally. HDR-BT monotherapy can be used as a first-line treatment option in patients with low-risk and intermediate-risk prostate cancer, whereas HDR-BT boost is a well-established treatment modality for certain intermediate-risk and high-risk prostate cancer. ADT can be used in conjunction with either form of brachytherapy.

The outcomes from either form of brachytherapy are generally excellent and superior to EBRT, and the risk of grade 3–4 toxicities is <5% according to most studies. Patients should be followed up every 6–12 months with serum PSA measurement and DRE. Several QOL questionnaires can be used to gauge urinary incontinence, urinary obstruction and irritation, bowel-related symptoms, sexual dysfunction, and hormonal symptoms.

The ideal brachytherapy patient should have no absolute contraindications to the therapy, including ataxia telangiectasia, pre-existing rectal fistula, comorbidity precluding anaesthesia, distant metastases, absence of a rectum, or large TURP defects. Clinicians considering LDR-BT versus HDR-BT should consider the need for a shielded room, initial capital equipment and recurring costs, and operator dependence.

Salvage brachytherapy can be used to treat local recurrence after prior radiation therapy. The ideal patient for salvage therapy has biopsy-proven local-only recurrence with no morbidity from prior radiotherapy. Salvage brachytherapy is best if performed >4.5 years after prior radiation treatment, with the use of advanced image guidance, and with a rectal spacer. Brachytherapy is an excellent treatment option for definitive and salvage treatment of prostate cancer; its continued evolution provides excellent outcomes, limited toxicity, generally excellent quality of life, and a low cost.

GLOSSARY

^α*/*β **ratio**

The α/β ratio describes the shape of the cell surviva curve and the gradient of the two components of cell kill, α and β . The α/β ratio is used to describe the dose response of radiation on different tissues. Prostate cancer cells have a relatively low α/β ratio of 1.5, implying that those cells are more sensitive to doses delivered in larger fraction size. In the

radiobiological linear quadratic equation, it is the dose at which cell killing due to the linear and quadratic components are equal.

Biologically equivalent dose (BED)

A more conceptually useful measure of biological damage to cells than physical dose. It takes into account the α/β ratio, number of radiation fractions, and fraction size. BED = $(nd[1 + d((a/\beta))$. In this formula, *n* is the number of radiation fractions and *d* is dose size per fraction.

Clinical target volume (CTV)

This volume encompasses the GTV as well as areas at risk for subclinical cancer involvement. The CTV can include a margin around the prostate GTV and adjacent regions at risk of having subclinical disease.

D0.1cc or Dmax

The average dose to the hottest point of a volume. The term "D0.1cc" is sometimes used because this approximates the maximum dose to the smallest volume that can be calculated on a computer.

D2cc

The average dose to 2cc of a volume.

D10

The average dose to 10% of a volume, in Gy. The urethra D10 should be <150% of the prescribed dose. This constraint limits the dose to the urethra.

D30

The average dose to 30% of a volume, in Gy. The urethra D30 should be <130% of the prescribed dose. This constraint limits the dose to the urethra.

D90

In prostate cancer brachytherapy, this is the minimum dose in the hottest 90% of a volume, in Gy. The prostate D90% should be >100%. This constraint ensures the prostate volume receives adequate dose.

Dwell time

The time that the ¹⁹²Ir source spends in a predetermined dwell position during HDR-BT. A longer dwell time in a position translates to a greater dose deposited in the volume around the position.

Dwell position

The position where a ¹⁹²Ir source is located during HDR-BT. A combination of dwell positions in different needles allows the delivery of a predetermined dose to the CTV (FIG 1C, right panel).

Equivalent dose in 2 Gy fractions (EQD2)

The "2 Gy-per-fraction equivalent dose." EQD2 = $n * d * ((d + a/\beta)/(2 + a/\beta))$, where The EQD2 uses a mathematical conversion of fractions and dose per fraction, similar to the BED. In this formula, n is the number of radiation fractions and d is dose size per fraction..

Gross tumour volume (GTV)

This is the demonstrable extent and location of the malignant growth; it consists of the primary tumor, which for prostate cancer has historically been defined as the entire gland as well as any visualized extension into surrounding normal tissues, the regional lymph nodes, or distant metastases based on clinical data.

hot spot

A colloquialism used to describe volume outside the PTV which receives dose larger than 100% of the specified PTV dose.

Hypofractionated radiation therapy

A type of EBRT that is delivered as a single 2.1–3.5 Gy fraction lasting 15 minutes per day, five days per week, for about four weeks

intensity modulated radiation therapy (IMRT)

An advanced form of high-precision radiation that conforms the treatment volume to the shape of the tumor. The dose distribution created by IMRT is characterized by a concavity or invagination of the edge of the higher doses away from the rectum, rather than a straight edge through the rectum as seen with 3D-CRT.

multi-leaf collimator (MLC)

A device made up of individual leaves of a high atomic numbered material that can move independently in and out of the path of an X-ray beam to contour its shape to a tumour.

Phoenix definition

Used for measuring biochemical failure after radiotherapy for prostate cancer, defined as the PSA nadir value plus 2 ng/ml

Planning target volume (PTV)

This volume encompasses the CTV plus an additional margin to account for patient movement, setup error, and organ movement

Remote afterloading system (RALS)

Integral to HDR-BT, a RALS automatically deploys and retracts a single small radioactive source along the implant needle at specific positions delivering $\frac{12 \text{ Gy/hr}}{12 \text{ Gy/hr}}$. The RALS allows a physician to control the position where the HDR source stops for a predetermined time periods (the dwell position and dwell time).

*R***V100**

In prostate cancer brachytherapy, this is the volume of the rectum receiving 100% of the dose, and should be ≤ 1 cc.

Stereotactic body radiation therapy (SBRT)

A type of EBRT delivered as a single 3.5–15.0 Gy fraction lasting up to 45 minutes per day, for a total of about five treatments over about 2 weeks

V100

In prostate cancer brachytherapy, this is the percentage of a structure receiving 100% of the dose. For example, the V100 for the prostate should be $> 90\%$, meaning that 100% of the prostate CTV should receive more than 90% of the prescribed dose.

V150

In prostate cancer brachytherapy, this is the percentage of a structure receiving 150% of the dose. The V150 for the prostate CTV should be <50–60%, meaning that <50–60% of the CTV should receive >150% of the prescribed dose.

*U***V5**

In prostate cancer brachytherapy, this is the average dose to 5% of the urethral volume receiving the highest dose. The UV5 should receive <150% of the dose.

*U***V30**

In prostate cancer brachytherapy, this is the average dose to 30% of the urethral volume receiving the highest dose. The UV30 should be <125% of the dose.

*U***V150**

In prostate cancer brachytherapy, this is the volume of the urethra receiving 150% of the prescribe dose. UV150 of the urethra should be 0%, meaning that 0% of the volume should receive 150% of the prescribed dose.

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Key points

- **•** Brachytherapy and brachytherapy boost with low-dose-rate brachytherapy (LDR-BT) or high-dose-rate (HDR)-BT can be used as first-line therapies in the management of prostate cancer patients of all National Comprehensive Cancer Network (NCCN)-defined risk groups.
- **LDR-BT, consisting of a single implant, typically uses** ^{125}I **or** ^{103}Pd **; by** contrast, HDR-BT consists of 1–3 implants and uses 192Ir.
- **•** Benefits of HDR-BT over LDR-BT include the ability to use the same source for other cancers, lower operator dependence, and fewer acute irritative symptoms.
- **•** Benefits of LDR-BT include more favourable scheduling logistics, lower initial capital equipment costs, non-requirement of a shielded room, completion in a single implant, and more robust data from clinical trials.
- **•** Outcomes of HDR-BT and LDR-BT are similar to those of other treatment options, including external beam radiotherapy (EBRT) and surgery, and brachytherapy can also be used in combination with EBRT in intermediaterisk and high-risk disease.
- **•** Severe toxicities of HDR-BT and LDR-BT are rare, although the rate of urethral stricture is increased when brachytherapy boost is performed; incontinence is not associated with any radiotherapy modality.

Box 1 ∣

The ideal patient for definitive brachytherapy

Patients should have the following characteristics:

- For brachytherapy monotherapy: Low-risk disease (Gleason score 6, and PSA <10 ng/ml, and clinical tumour classification T1, T2a), or favorable intermediate-risk disease (Gleason score 7, or PSA 10 ng/ml 20 ng/ml or clinical tumour classification of T2b, T2c) with primary Gleason score 3+4, <50% percent positive biopsy cores, and only a single intermediate-risk feature.
- **•** For brachytherapy boost: High-risk disease (Gleason score 8–10, or PSA >20 ng/ml, or clinical tumour classification of T3a), or unfavourable intermediaterisk disease (Gleason score 7, or PSA 10 ng/ml 20 ng/ml or clinical tumour classification of T2b, T2c) with primary Gleason score $4+3$, 50% percent positive biopsy cores, and multiple intermediate-risk features.

Patients should have none of the following

- **•** Ataxia telangiectasia
- **•** Pre-existing rectal fistula
- **•** Unacceptable operative risks or medically unsuitable for anaesthesia
- **•** Distant metastases
- **•** Absence of rectum such that TRUS-guidance is precluded
- **•** Large TURP defects that preclude seed placement and acceptable radiation dosimetry

Patients should preferably not have the following

- **•** History of previous pelvic radiotherapy
- **•** Limited life expectancy (<10 years)
- **•** Moderate-to-severe urinary symptoms (for example, high IPSS score, typically defined as >20)
- **•** Inflammatory bowel disease
- **•** Increased risk of bleeding
- **•** Large median lobes
- **•** Pubic arch interference
- Patient peak urinary flow rate <10 cm³/s and postvoid residual volume prior to brachytherapy $>100 \text{ cm}^3$
- Large prostate (>60 cm³)

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FIG 1 ∣**. Comparison of LDR-BT, HDR-BT, and EBRT.**

a∣ The dose distribution in water as a function of distance from a point source of three isotopes commonly used for prostate brachytherapy: LDR-BT with 103Pd (light green), LDR-BT with 125 I (dark green), and HDR-BT with 192 Ir (blue). The dose has been normalized to 100% at a distance of 1.0 cm (note log scale). The high energy 192 Ir departs slightly from the inverse square law $(1/r^2)$, whereas the lower energy isotopes of LDR-BT have more absorption over a lower range. b∣ Comparison of LDR-BT, HDR-BT, and conventional or hypofractionated EBRT. The doses (with respect to the patient) are shown in colour (top panel). The dose fractionation of LDR-BT with decay using $103Pd$ (light green) or 125I (dark green) compared with HDR-BT (shown as blue fractions); and EBRT (red fractions) are shown in the middle panel. Notably, brachytherapy requires only 1–5 insertions compared with up to 40 fractions of EBRT. The isodose distributions (lower panel) of brachytherapy are superior to that of EBRT, as X-rays do not pass through the skin. c∣ Brachytherapy boost is defined as the combination of EBRT with HDR-BT or LDR-BT. If EBRT is delivered first, HDR-BT is typically delivered 1–6 weeks later. A possible benefit of this method is to use the HDR-BT to account for suboptimal dosimetry of EBRT. Alternatively, EBRT can be interdigitated with HDR-BT. Finally, HDR-BT can be delivered first and EBRT delivered 1–3 weeks later.

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FIG 2 ∣**. The evolution of brachytherapy for prostate cancer.**

a∣ The use of prostatic brachytherapy was first reported in 1911, when radium was administered temporarily via a urethral catheter.^{14, 15} In 1917, a transperineal implantation of radium was performed in New York.16 During the 1920s, cohorts of patients were treated with radium brachytherapy in the US.

b∣ In the 1950s, LDR-BT was performed with 198Au,18 but by the 1970s 125I seeds were used for prostate cancer implants.²¹ A remote afterloading system (RALS) was developed in the 1980s and used for HDR-BT. With more advanced forms of external beam radiotherapy (EBRT) (for example, 3D conformal radiotherapy and then image-modulated radiotherapy $(IMRT)$,³⁵ EBRT was combined with both forms of brachytherapy to deliver brachytherapy boost.56 EBRT developed in parallel over the 1990s and 2000s to become increasingly hypofractionated.75 In 2001, the development of the robotic arm linear accelerator, which delivers SBRT, led investigators to tout it as "virtual HDR-BT," and they touted this treatment to be a superior and more advanced form of brachytherapy since it could be performed without anesthesia or needles entering the prostate.⁷⁵ As of 2016, no trials comparing the two technologies have been performed,⁷⁶ and the dosimetric distribution of HDR-BT (FIG 1B) is superior to any form of EBRT because X-rays do not pass through the skin of the patient.⁴

c∣ Trends in the use of brachytherapy compared with other modalities of therapy in the USA, from 1998–2013 show that use has declined over the time period. Brachytherapy use reached a high around 2002, when 18% of patients received the therapy. ⁶⁴

d∣ Trends in the use of brachytherapy across risk groups (adapted form Martin, et al⁶⁴). The percentage of patients treated with brachytherapy alone by year from 2004 to 2009 stratified by National Comprehensive Cancer Network (NCCN) risk grouping (upper panel), and percentage of patients treated with brachytherapy boost by year from 2004 to 2009 stratified by NCCN risk grouping (lower panel).⁶⁴

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FIG 3∣**. Target volume definitions.**

a∣ Anteroposterior image of the prostate and seminal vesicles (left). The principle organs at risk include the urethra, bladder, and rectum. The gross tumour volume (GTV; red) is the gross demonstrable extent and location of the malignant growth. The clinical target volume (CTV; light blue) encompasses the GTV as well as areas at risk for subclinical cancer involvement. The planning target volume (PTV; purple) encompasses the CTV plus an additional margin to account for patient movement, set-up error, and organ movement (right).

b∣ For prostate cancer treated with EBRT, the PTV is typically CTV + $0.5 - 1.0$ cm.^{101, 102} The PTV expansion is necessary because the prostate can move owing to nearby organ changes, such as rectal distention (illustrated on the left), and because the patient might be positioned differently on the treatment table (on the right). Movements can be translational, rotational, and deformational. Note that the CTV (blue volume) stays inside of the PTV (purple volume). EBRT (shown in red) covers the PTV by passing through the soft tissues of the pelvis.

c∣ For brachytherapy, the expansion from a CTV to make a PTV can typically be because the set-up error is almost nonexistent. 10 , 11 In the case of LDR-BT, once the needles are deposited, the dose cloud (green cloud) would cover the CTV, even if the patient were to move or if there were organ movement. In the case of HDR-BT, the needles (typically about 12 in count) anchor the prostate while the 192 Ir source moves to the dwell positions, shown as circles inside of the needles, for prespecified dwell times to deliver the prescribed dose (blue cloud).

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FIG 4∣**. Dosimetric comparison of LDR-BT versus HDR-BT**

a∣ The prostate gland is composed of a peripheral zone, central zone, transitional zone, and an anterior fibromuscular layer. The majority of prostate cancers develop in the peripheral zone. ⁴⁰

b∣ Relative dose versus position in tissue. With 3D-CRT, the maximal point dose is towards the centre of the prostate, near the urethra; the dose decreases gradually toward the periphery of the prostate. IMRT (centre) ensures coverage of the entire prostate gland with dose and minimizes hotspots within the gland. Nonetheless, with IMRT, the prescription dose must be delivered to the PTV, which expands outside of the prostate. With SBRT, radiotherapy is prescribed to an isodose line to cover the PTV. Furthermore, the hotspot is again in the

centre of the prostate toward the urethra; although protocols include a urethra dose constraint,^{101, 102} the higher dose toward the centre of the gland with SBRT is sometimes unavoidable.74, 75

c∣ Both LDR-BT and HDR-BT provide excellent dosimetric coverage of the prostate, particularly because they provide excellent coverage of the peripheral zone with a low dose to the urethra. HDR-BT might, in some instances, be superior to LDR-BT because the hotspots assessed by looking at the V150 (or volume receiving 150% of the prescribed dose), are typically smaller in a HDR-BT plan than in the LDR-BT plan.

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FIG 5 ∣**. Biologically equivalent dose (BED) versus** α**/**β **curves for fractionated radiotherapy for prostate cancer.**

BEDs for several major studies of HDR-BT (blue line) are shown compared with the regimen of dose-escalated conventionally fractionated EBRT monotherapy (dashed red line). The use of higher doses per fraction (for example with HDR-BT versus conventionally fractionated EBRT) results in a higher BED at α/β of 1.5 (for prostate cancer) than at α/β of 3.0 (for late toxicity), thereby increasing the therapeutic ratio.

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FIG 6 ∣**. Characteristic PSA curves after treatment.**

Different radiotherapy modalities are associated with different trends in post-treatment PSA. ⁴ The Phoenix definition (PSA nadir $+ 2$ ng/mL, circled on the right) following treatment (in this case, EBRT) is the preferred protocol to define biochemical failure. EBRT typically induces a gradual and inconsistent decrease in PSA to levels that are still detectable. After LDR-BT, PSA has been noted to decrease to <0.3 ng/ml in most men with localized disease, although a much lower decrease is possible. After HDR-BT, PSA nadir is usually very low ≈ 0.05 ng/ml). All radiotherapy modalities can induce a PSA bounce — a temporary elevation in PSA without disease recurrence, circled on the left, which are common and do not automatically represent cancer recurrence.

Table 1∣

Indications and contraindications of brachytherapy compared with external beam radiotherapy

NA: not applicable; IPSS: International Prostate Symptom Score; TRUS: transrectal ultrasonography; TURP: transurethral resection of prostate.

* Excluded on clinical trial: Radiation Therapy Oncology Group 0938 or 0534.

‡ Placement of fiducials for IGRT might be difficult.

§ Depends on intraprostatic versus extraprostatic disease burden.

Table 2∣

Properties of radionuclides and quality planning constraints

Table 3 ∣

Comparison of physician and patient considerations of LDR-BT and HDR-BT

ADT, androgen deprivation therapy; DM, distant metastases; LDR-BT, low-dose-rate brachytherapy; EBRT, external beam radiation therapy; FFBF, freedom from biochemical failure; HDR-BT, high-dose-rate brachytherapy; OR, operating room; PCSS, prostate-cancer-specific survival; OS, overall survival.

Table 4∣

Percentage of late Grade 3–4 toxicities associated with HDR-BT, LDR-BT, and EBRT

Table 5∣

Ongoing studies evaluating brachytherapy for prostate cancer

Abbreviations: ADT: androgen deprivation therapy; EBRT: external beam radiation therapy; HDR-BT: high dose rate brachytherapy; LDR-BT: low dose rate brachytherapy; MRI: magnetic resonance imaging.