



Why are we still debating criteria for carotid artery stenosis?

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Abstract: The risk of new or recurrent stroke is high among patients with extracranial carotid artery stenosis and the benefit of carotid revascularization is associated to the degree of luminal stenosis. Catheter-based digital subtraction angiography (DSA) as the diagnostic gold-standard for carotid stenosis (CS) has been replaced by non-invasive techniques including duplex ultrasound, computed-tomography angiography, and magnetic resonance angiography (MRA). Duplex ultrasound is the primary noninvasive diagnostic tool for detecting, grading and monitoring of carotid artery stenosis due to its low cost, high resolution, and widespread availability. However, as discussed in this review, there is a wide range of practice patterns in use of ultrasound diagnostic criteria for carotid artery stenosis. To date, there is no internationally accepted standard for the gradation of CS. Discrepancies in ultrasound criteria may result in clinically relevant misclassification of disease severity leading to inappropriate referral, or lack of it, to revascularization procedures, and potential for consequential adverse outcome. The Society of Radiologists in Ultrasound (SRU), either as originally outlined or in a modified form, are the most common criteria applied. However, such criteria have received criticism for relying primarily on peak systolic velocities, a parameter that when used in isolation could be misleading. Recent proposals rely on a multiparametric approach in which the hemodynamic consequences of carotid narrowing beyond velocity augmentation are considered for an accurate stenosis classification. Consensus criteria would provide standardized parameters for the diagnosis of CS and considerably improve quality of care. Accrediting bodies around the world have called for consensus on unified criteria for diagnosis of CS. A healthy debate between professionals caring for patients with CS regarding optimal CS criteria still continues.

Keywords: Carotid artery stenosis; diagnostic criteria; ultrasound

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Introduction

Atherosclerosis affecting the cervical internal carotid artery (ICA) is an important cause of cerebral infarction, being responsible for 10% to 20% of cases of ischemic stroke (1,2). A primary physical or metabolic injury to the endothelium may trigger an inflammatory response resulting in cellular proliferation and lipid deposition leading to the formation of atherosclerotic plaque (3). The bifurcation of the

common carotid artery (CCA) is particularly prone to plaque formation due to the alterations of wall shear stress caused by the division of blood flow velocities (4). Carotid plaque may progress and protrude into the vessel lumen causing significant arterial narrowing and disruption of laminar flow (3). Finally, progressive arterial narrowing may lead to severe carotid stenosis (CS) or plaque rupture followed by thrombosis and embolism that may compromise cerebral circulation and result in stroke.

The prevalence of asymptomatic extracranial CS in the general population is 4% to 8%, increases with age and is more common in men than in women (5,6). The main factor affecting the risk of stroke among patients with CS is the degree of luminal stenosis (7-9). The annual risk of stroke among patients with asymptomatic carotid disease with less than 60% stenosis is close to 1%, but this risk increases to 3% to 4% for those with stenosis greater than 60% (9). The risk of stroke among patients who have had a previous episode of hemispheric transient ischemic attack, retinal ischemia, or ischemic stroke in the carotid artery territory (symptomatic CS) is much higher, up to 16% in the first year after an index event among medically treated patients (10), and similar to asymptomatic patients, it is closely related to the degree of stenosis (9,11). Moreover, the value of carotid revascularization in patients with asymptomatic and symptomatic CS is predominantly dependent on the severity of stenosis (12-14). Two randomized trials showed a small but significant benefit of carotid endarterectomy (CEA) in patients with asymptomatic CS of >60% (12,13). Likewise, pooled data from large randomized trials in symptomatic CS showed substantial benefit of CEA in patients with stenosis of 70% to 99%, a modest benefit for those with 50% to 69% stenosis, and no benefit or harm for those with <50% stenosis (14). It is therefore critically important to use accurate imaging techniques and diagnostic criteria for the detection and grading of severity of stenosis for the appropriate prognosis and therapeutic considerations in patients with CS. This review addresses the criteria for the diagnosis of CS with special emphasis in the advantages and challenges of carotid duplex ultrasound (CDUS) as a preferred screening and diagnostic tool for CS in clinical practice. After more than sixty years of the use of CDUS in clinical practice, setting the debate on appropriate diagnostic criteria for CS is still needed for the benefit of our patients, their caregivers, and society at large.

Diagnosis of extracranial carotid artery stenosis

The indications to refer symptomatic patients for the evaluation of CS include a transient ischemic attack, amaurosis fugax, or ischemic stroke (15). CS assessment is also commonly included as part of the diagnostic evaluation of non-specific non-hemispheric symptoms such as syncope, although it has been recognized as a low-yield practice (16,17). Screening for CS in the general population, even among those with evidence of atherosclerosis in other

vascular beds (i.e., coronary or peripheral artery disease), is neither indicated nor considered cost-effective (18-20). The rationale against widespread CS screening is based on the high-rate of false negative/positive results among the general population and the potential harm of unnecessary invasive procedures (18). Although more research is required in the field, some authors suggest that screening for CS among high-risk individuals would enable timely implementation of medical therapy to prevent stroke and cardiovascular events (21). Clinically, CS is usually suspected based on the presence of a carotid bruit on physical examination or Hollenhorst plaques on fundoscopy (22). The existence of a carotid bruit correlates poorly with the presence and degree of ICA stenosis (23,24). Nevertheless, the presence of a carotid bruit continues to be a useful clinical sign to identify patients at high risk of cardiovascular events who would benefit from aggressive modification of vascular risks factors (24,25).

Non-invasive tests utilized for the diagnosis of CS include high-resolution duplex ultrasound, time-of-flight and contrast-enhanced magnetic resonance angiography (MRA), and computed tomography angiography (CTA). All of them have demonstrated reasonable sensitivity and specificity when compared to the gold-standard of catheter-based digital subtraction angiography (DSA) (26) (*Table 1*). A meta-analysis of 41 studies including 2,541 patients (4,876 arteries), determined that contrast-enhanced MRA was more accurate than other non-invasive techniques to categorize 70–99% stenosis, yet data for 50–69% stenosis were less reliable (26). The incorporation of a contrast enhanced agent such as gadolinium to conventional MRA enables great distinction between the vessel and surrounding tissue leading to delineation of the vascular lumen independent of flow dynamics (27). In real-world practice, CDUS is often favored as a screening technique for being inexpensive, reliable, and readily available (28). It has been estimated that as many as 80% of patients in the U.S. undergo carotid revascularization after CDUS as the only preoperative diagnostic modality (29). While DSA remains the gold standard for assessing the severity of CS, it is usually reserved for selected situations or when an intervention, generally carotid artery stenting, is planned due to the risks related to the invasiveness of the procedure (30).

In CDUS, the degree of stenosis is graded by assessing the blood flow waveform at the site of greatest arterial narrowing. The procedure is inexpensive, has basically no risks, and represents minimal discomfort to the patient. The

Table 1 Characteristics of different imaging modalities to diagnose extracranial carotid artery stenosis

Diagnostic modality	Sensitivity [†]	Specificity [†]	Cost	Invasiveness	Radiation exposure	Contrast material	Intracranial vasculature	Disadvantages
Carotid duplex ultrasound	85–92%	77–89%	–	Non-invasive	No	No	No	Operator variability Poor differentiation of subtotal from total occlusion Overestimation of stenosis in the presence of contralateral occlusion Variability of diagnostic criteria
CT-angiography	68–84%	91–97%	+	Non-invasive	Yes	Yes	Yes	Susceptible to artifacts caused by calcified plaques Use of IV contrast Underestimation of stenosis
Time-of-flight MR-angiography	82–92%	76–97%	++	Non-invasive	No	No	Yes	Long acquisition time Susceptible to motion artifacts Overestimation of stenosis
Contrast enhanced MR-angiography	88–97%	89–96%	++	Non-invasive	No	Yes (gadolinium)	Yes	Contraindications for undergoing magnetic resonance Long acquisition time Low spatial resolution
Digital subtraction angiography	GS	GS	+++	Invasive	Yes	Yes	Yes	Risk for systemic fibrosis in patients with renal impairment Contraindications for undergoing magnetic resonance Risks associated to invasiveness of the procedure Use of IV contrast Risk of permanent neurological complications (~1%) Requires skilled operators and is done at specialized neurovascular centers

[†], sensitivity and specificity to detect 70–99% carotid stenosis (22). CT, computed tomography; GS, gold standard; MR, magnetic resonance.

standard CDUS examination includes grayscale B-mode imaging, color Doppler imaging, and spectral Doppler velocity evaluation (15,31,32) (*Table 2*). The recommended measurements on spectral Doppler evaluation include the peak-systolic velocity (PSV) and end-diastolic velocity (EDV), both at the distal CCA and ICA (15,31). The highest ICA PSV in the site of stenosis together with plaque and lumen visualization on grayscale and Doppler images are the most practical parameters used to diagnose and grade CS (29,33). Additional parameters include the ICA EDV, the ratio between the ICA PSV and distal CCA PSV (PSVs ratio), and the ratio between the ICA PSV and the CCA EDV, known as the St. Mary ratio (34,35). These parameters are particularly useful when ICA PSV is not representative of the extent of stenosis, such as in the presence of tandem lesions, contralateral high-grade stenosis, elevated CCA velocities, hyperdynamic cardiac state, and low cardiac output (29,36). In addition to velocity parameters, the presence of post-stenotic turbulence on color and spectral Doppler, as well as the morphology of the waveform distal to the area of most severe stenosis, can be useful for identification of high-risk carotid lesions. In cases of carotid near occlusion, velocity parameters may be increased or decreased, thus are not applicable or useful for diagnosis (29). Near occlusion diagnosis is made by demonstration of marked lumen narrowing on B-mode and color Doppler imaging as well as abnormal morphology of the spectral Doppler waveforms (37). Similarly, diagnosis of total carotid occlusion is suspected when there is extensive plaque visualized without detectable lumen on B-mode imaging and no flow on Doppler imaging (37). Diagnostic confirmation with either CTA, MRA or DSA are recommended in the latter two scenarios (29).

Diagnostic criteria for extracranial carotid artery stenosis

Seminal trials that demonstrated the benefit of CEA in patients with symptomatic CS utilized criteria based on DSA imaging to estimate the degree of ICA stenosis (10,38,39). In the North American Symptomatic Carotid Endarterectomy Trial (NASCET) and the Veterans Affairs Cooperative Studies Program (10,39), the degree of luminal stenosis was calculated based on the ratio between the diameter at the point of greatest stenosis and the diameter of the artery at a normal distal segment. In the European Carotid Surgery Trial (ECST), the denominator utilized was an estimate of the original width of the artery at the site

of maximal stenosis (38). Despite major discrepancies in the degree of stenosis between studies, subsequent comparison of the two methods showed that the relation between them was approximately linear and a simple equation is able to convert measurements from one method to the other ($\text{ECST\% stenosis} = 0.6 \times \text{NASCET\% stenosis} + 40\%$) (40,41) (*Figure 1*). For example, a CS of 70% estimated by the NASCET criteria is equivalent to 82% stenosis by the ECST method [$0.6 \times 70 + 40 = 82$]. Both in CTA and MRA, post-processing techniques applying three-dimensional volume-rendering algorithms can produce angiographic images similar to those on DSA and enable stenosis measurements in accordance to NASCET or ECST criteria (42). However, the source of some of inconsistencies on CDUS diagnostic criteria mentioned below originate from applying different DSA protocols (NASCET *vs.* ECST) as the standard reference (43). Most organizations now recommend using the NASCET method when DSA is used to correlate CDUS findings (29,36,43). Although, it is worth mentioning that the NASCET criteria may underestimate the degree of stenosis when there is decreased flow into the post-stenotic ICA due to collateral circulations or tandem lesions, thus resulting in an abnormally decreased diameter of the distal “normal” carotid artery segment.

Since the initial parameters known as the “Strandness Criteria” were published in 1987 (44), many different CDUS approaches to classify the severity of stenosis have been proposed (29,36,43,45-51) (*Table 3*). The Society of Radiologists in Ultrasound (SRU) consensus criteria are widely used and recommend PSV cutoff values of >125 cm/s and >230 cm/s to define stenosis $\geq 50\%$ and $\geq 70\%$, respectively (29). Additional criteria include PSVs ratio >2.0 and EDV >40 for $\geq 50\%$ stenosis, and PSVs ratio >4.0 and EDV >100 cm/s for $\geq 70\%$ stenosis (29). Two successive validation studies reported that PSV >230 cm/s had a sensitivity of 0.95 and 0.99, and specificity of 0.84 and 0.86 for detecting $\geq 70\%$ stenosis (52,53). One of those studies, which used CTA as the reference standard, also evaluated the accuracy of PSV 125–230 cm/s for detecting 50–69% stenosis and reported a sensitivity of 0.93 and specificity of 0.68, which could be significantly improved by using a PSV of 140–230 cm/s resulting in a sensitivity of 0.94 and specificity of 0.92 (52). The Vascular Society of Great Britain and Ireland adopted the PSV cutoff values proposed by the SRU, with an additional cutoff of >400 cm/s to define $\geq 90\%$ stenosis but less than near occlusion (43). The British consensus also encouraged the use of the St. Mary

Table 2 Summary of the Society for Vascular Ultrasound exam protocol performance guidelines for extracranial cerebrovascular duplex ultrasound (32)

	Technique	Comments
Patient positioning	Patient in supine position Head slightly rotated towards the contralateral side	
Instrumentation	Linear transducer 5–7 MHz	Superficial structures may require a higher frequency transducer
	Real-time display of 2D structures	Deeper structures or edematous tissue may require a lower frequency transducer
	<ul style="list-style-type: none"> • Doppler ultrasonic signal documentation • Spectral analysis with color and/or power Doppler imaging 	
	Digital storage capabilities of ultrasound images	
Exam protocol		
B-mode images	Longitudinal image of CCA	Characteristics of plaque should be documented in transverse and longitudinal planes
	Transverse image of the carotid artery bifurcation	Presence of carotid artery stent
	Longitudinal image of the ICA	Any other abnormalities should be documented
	Longitudinal image of the ECA	
Color Doppler images	Longitudinal image of the CCA	Velocity measurements should be obtained from a longitudinal plane at an angle of 60° parallel to the direction of the blood flow/vessel walls
	Transverse image of the carotid artery bifurcation	Maintain a Doppler angle between 45° and 60° whenever possible. Angles greater than 60° must be avoided
	Longitudinal image of the ICA	To obtain peak velocity, utilize color Doppler to note areas of concern and “walk” the spectral Doppler cursor throughout these areas
	Longitudinal image of the ECA	Post stenotic turbulence should be documented when present
Spectral Doppler images	Longitudinal image of the vertebral artery	
	Proximal CCA	In the presence of pathology, spectral waveforms should be recorded proximal to, within, and distal to the lesion
	Mid to distal CCA	Documentation of sites of vascular intervention (i.e., endarterectomy) should include representative waveforms and velocity measurements proximal to the intervention site, within the intervention site, and distal to the intervention site
	Proximal ICA	In the presence of stents, documentation should include: Native artery at the proximal end of the stent; Proximal, mid and distal stent; Native artery at the distal end of the stent
	Distal ICA	Any other abnormalities should be documented
	Proximal ECA	
	Vertebral artery	
Subclavian artery (when appropriate)		

CCA, common carotid artery; ECA, external carotid artery; ICA, internal carotid artery.

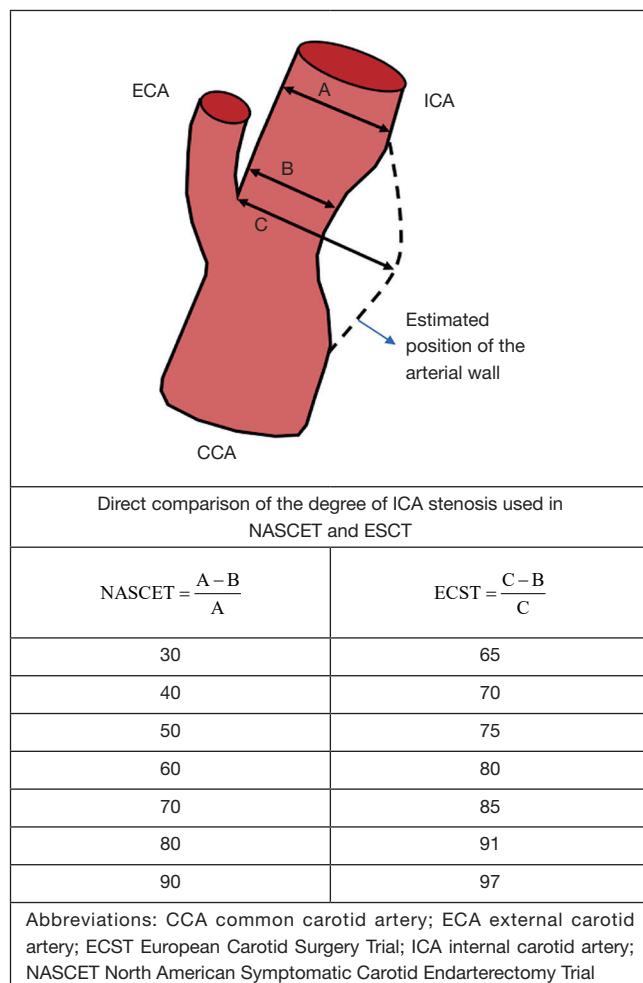


Figure 1 Diagram of the NASCET and ECST methodology for internal carotid artery stenosis measurement (41).

ratio as a robust index able to grade the degree of stenosis in deciles (43,54). For example, a St Mary ratio of 11 indicates 60% stenosis with a sensitivity of 0.91 and specificity 0.94, and a ratio of 14 indicates 70% stenosis with a sensitivity of 0.93 and specificity of 0.93 (54). Caution should be taken when using the St. Mary ratio in situations in which the CCA EDV is bilaterally decreased, such as in retrograde flow due to aortic insufficiency (55) or reduced vessel wall compliance (43).

Other CDUS criteria differ significantly from the Anglo-American recommendations. Recommendations from the German DEGUM (Deutsche Gesellschaft für Ultraschall in der Medizin) include PSV cutoffs values of >200 cm/s

and >300 cm/s (44), while the Swedish EQUALIS (External Quality Assurance in Laboratory Medicine in Sweden) recommend PSV cutoff values of >230 cm/s and >320 cm/s for stenosis of $\geq 50\%$ and $\geq 70\%$, respectively (46). More recently, the Neurosonology Research Group of the World Federation of Neurology recommended a multiparametric approach using both morphological and hemodynamic parameters to define primary and additional criteria in order to overcome common diagnostic errors met when PSV are used in isolation (36). The relative value of such parameters depends on the severity of stenosis. For low-degree stenosis (0–50%), morphological characteristics on B-mode imaging including the thickness and length the plaque, as well as the reduction of diameter in percent, are more meaningful than velocity measurements (36). In moderate stenosis (i.e., 50–59%, 60–69%), morphological criteria are combined with increase in PSV (usually 125–230 cm/s) and no collateral flow present. For hemodynamically severe stenosis ($\geq 70\%$), increase in velocity (>230 cm/s) is accompanied of signs of collateral flow by transcranial Doppler demonstrated by retrograde flow on the ophthalmic artery, cross flow on the anterior cerebral artery, or P1 collateral flow through the posterior communicating artery (36). In the latter, reduced velocity in the post-stenotic segments (i.e., <30 cm/s PSV) and dampened and delayed Doppler waveform morphology, indicates very severe stenosis (>90%) (36).

There is substantial variability from laboratory to laboratory in the CDUS thresholds and derived indices applied to diagnose and grade CS (56–60). Even among accredited vascular testing centers, the diagnostic thresholds for CS severity vary considerably (60). Among 338 accredited centers in the U.S., the PSV threshold for moderate stenosis (50% to 69%) ranged from 110 to 245 cm/s, and the threshold for severe stenosis (>70%) ranged from 175 to 340 cm/s. When applied this wide range of thresholds for moderate stenosis in a population-based sample of individuals aged >65 years, twice as many cases would be assigned the diagnosis of moderate stenosis when the 5th percentile threshold was compared to the 95th percentile. Similarly, in a large cohort of asymptomatic patients who underwent carotid revascularization, one in ten cases would warrant the diagnosis of severe stenosis, thus considered for surgery, in the 5th percentile threshold, but not in the 95th percentile threshold (60). These estimations expose the high clinical impact CDUS diagnostic criteria variations across testing centers may have.

Table 3 Consensus criteria on carotid ultrasound diagnostic criteria for >50% and >70% carotid stenosis

Publication	Grayscale imaging [†]	PSV (cm/s)	EDV (cm/s)	ICA-to-CCA PSV ratio	St Mary ratio [§]	Prestenotic flow (CCA EDV)	Poststenotic flow disturbances	Collateral flow
>50% stenosis								
Grant <i>et al.</i> 2003 (29)	+	>125	>40	>2.0	-	-	-	-
Oates <i>et al.</i> 2009 (43)	-	>125	-	>2.0	>8.0	-	-	-
Arning <i>et al.</i> 2010 (45)	-	>200	-	>2.0	-	-	Moderate	Not present
von Reutern <i>et al.</i> 2012 (36)	+	>125	-	>2.0	-	-	Moderate	Not present
Jogenstrand <i>et al.</i> 2012 (46)	-	> 230	-	-	-	-	-	-
Mozzini 2016 <i>et al.</i> (47)	-	>200	-	>2.0	-	-	-	-
>70% stenosis								
Grant <i>et al.</i> 2003 (29)	+	>230	>100	>4.0	-	-	-	-
Oates <i>et al.</i> 2009 (43)	-	>230	-	>4.0	>14.0	-	-	-
Arning <i>et al.</i> 2010 (45)	-	>300	>100	>4.0	-	-	Present	Present
von Reutern <i>et al.</i> 2012 (36)	-	>230	>100	>4.0	-	Reduced	Present	Present
Jogenstrand <i>et al.</i> 2012 (46)	-	>320	-	-	-	-	-	-
Mozzini 2016 <i>et al.</i> (47)	-	>300	>100	>4.0	-	Reduced	-	-

[†], criteria mention features on grayscale B-mode imaging; [§], St Mary ratio = ICA PSV/CCA EDV. CCA, common carotid artery; EDV, end diastolic velocity; ICA, internal carotid artery; PSV, peak systolic velocity.

Pitfalls and challenges in the use of carotid ultrasound for the diagnosis of extracranial carotid artery stenosis

The main source of variation in CDUS criteria arises from the exponential relation between the angiographic degree of stenosis (considered the gold standard) and the PSV on spectral Doppler originally described by Spencer and Reid (61,62). The steep graph leads to a significant change in velocity despite minimal changes in the angiographic degree of stenosis, particularly in the range of highest clinical relevance (60% to 90%). In addition, the “Spencer Reid curve” may result in reduced velocities in situations of near occlusion which may be misclassified as lower degrees of stenosis (62). A systematic review of 22 data sets found a wide variability between CDUS velocities and percent of stenosis on angiography among published data, which in turn have resulted in the inconsistencies of the different diagnostic thresholds proposed in the literature (59). Moreover, both modalities are not expected to entirely correlate as angiography measures the reduction in the vessel diameter, while PSV as measured by Doppler ultrasound is altered by the reduction in the lumen area,

which is mainly determined by the morphology of the plaque (63). It is therefore that PSV alone is considered insufficient for accurate estimation of the degree of CS (36). Factors relevant to angiographic measurements that may contribute to inconsistencies between CDUS and angiographic degree of stenosis include the presence of noncircular stenoses as well as the pulsatile changes in the lumen diameter that occur between systole and diastole (59). Indeed, as stated in the title of a summary analysis of previously published angiographic and Doppler ultrasound comparative studies, “correlation is futile” (59).

Conditions inherent to the patient may also influence CDUS examinations. Certain variability within patients can be attributed to factors affecting brain physiology such as carbon dioxide exposure, caffeine, lactate, nicotine, and degree of regional brain activation (64-67). Some vessel characteristics such as extensive plaque calcification, increased tortuosity, and tandem lesions, may result in difficult interpretation of CDUS results (29). Overestimation or underestimation of the degree of stenosis may occur when flow velocities are affected by hemodynamic factors such as low cardiac output, irregular heart rhythm, and hyperdynamic cardiac state (43). The

presence of collateral flow, either through the Circle of Willis or the ophthalmic artery, may decrease the post-stenotic pressure and, consequently, the intra-stenotic velocity (68,69). Conversely, the presence of contralateral severe CS or occlusion may falsely elevate CDUS velocities (70,71). Ultimately, the presence of a carotid stent results in higher PSVs and lower EDV and PSV ratio, and therefore it is recommended to be considered for the interpretation of CDUS (60).

Technical considerations that may affect the accuracy of measurements, hence the reliability of CDUS investigations, include completeness of the examination protocol, the angle of insonation, equipment variability, and methods of reporting, which vary significantly from laboratory to laboratory (72,73). The angle of insonation is required to convert the Doppler frequencies into velocities, thus is a critical determinant of the Doppler velocity measurement. It has been estimated that small shifts in angle of insonation result in major discrepancies between studies (74,75). It is important to highlight that an appropriate angle estimation is particularly challenging in situations of turbulent flow or tortuous vessels. Most organizations emphasize that measurements should be done at a fixed angle and recommend an angle of 60 degrees or lower (15,29,31,43), nonetheless, the optimal angle of insonation continues to be a matter of debate (47).

Several professional societies and accrediting bodies including the Intersocietal Accreditation Commission (IAC), the American Institute of Ultrasound in Medicine (AIUM), Society for Vascular Ultrasound (SVU), and the American College of Radiology (ACR) have been tasked to standardize the examination protocols and methods for reporting for CS (Table 2) (15,31,32). These organizations suggest that stenoses above 50% should be graded within a range (i.e., 50–69% or 70% to near occlusion) to provide adequate information for clinical decision making. They also emphasize that each laboratory must apply uniform diagnostic criteria either derived from the literature or from internal validation based on correlation with other imaging modalities or pathological samples (15,31). Accreditation status of a vascular laboratory is an important feature associated with enhanced diagnostic accuracy and reliability (76). However, a recent study reported that only 22% of outpatient cerebrovascular testing facilities in the U.S. which performed testing for Medicare patients were IAC-accredited, and accreditation status varied widely by geographical region (77). Among IAC-accredited testing facilities, there is wide variability of carotid diagnostic

criteria employed by individual laboratories, as well as support for efforts to standardize diagnostic criteria across the board (78). In response to these data, IAC has undertaken an initiative to standardize diagnostic criteria across its accredited laboratories, the first phase of which, a research study to validate the SRU Consensus criteria, compared to DSA, and to propose modification of SRU Consensus parameters for optimized accuracy is due to be released in 2020.

Conclusions

For many reasons, CDUS remains the primary modality for initial diagnosis and monitoring of CS, and plays a central role in the management of patient care and clinical decision making. Although debate continues regarding the optimal diagnostic criteria for diagnosis of carotid artery stenosis, we are closer to accomplishing our goal of standardization of CS criteria worldwide and improving quality of care for these patients.

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