Europe PMC Funders Group Author Manuscript Dent Mater. Author manuscript; available in PMC 2024 November 01.

Published in final edited form as: Dent Mater. 2024 March 03; 40(5): e1–e13. doi:10.1016/j.dental.2024.02.016.

Methodological approaches in graded dental ceramics

Sivaranjani Galia,* , **Suhasini Gururaja**b, **Zulekha Patel**^c

aDept. of Prosthodontics, Faculty of Dental Sciences, M.S.Ramaiah University of Applied Sciences, Bangalore 560054, India

^bDept. of Aerospace Engineering, Auburn University, AL 36849, USA

^cDept. of Prosthodontics, Faculty of Dental Sciences, M.S.Ramaiah University of Applied Sciences, Bangalore 560054, India

Abstract

Background—Functionally graded materials (FGM) with indistinct boundaries potentially eliminate the damaging stresses occurring at the interfaces. FGM applications in dental ceramics have enhanced their fatigue resistance and interfacial toughness.

Objectives—This scoping review aims to map graded designs in dental ceramics, distinguish their methodological approaches with their material characteristics and properties, and understand the factors affecting the outcomes of each of the graded approaches.

Methods—A systematic electronic search was performed with the databases MEDLINE (PubMed), Scopus, Cochrane Library, EBSCO, and Google Scholar along with a manual search.

Results—About 2675 articles were initially found from all the searches with no date restriction till July 2023. After rejecting duplicates and based on exclusion criteria, about 52 articles were included.

Significance—Methodological approaches in grading such as glass-infiltration and silicainfiltration have been investigated on pre-sintered zirconia. The type of infiltration and the method of infiltrate application significantly influenced the phase transformation of zirconia, its microstructure, surface hardness, fracture toughness, flexural strength, wear, and fatigue strength of graded dental zirconia. Interlayers were accommodated between metal-ceramic and veneer-core all-ceramic layers. Fractions of zirconia-porcelain and alumina-porcelain showed high bending strength and better stress distribution. The results of finite element analysis studies predicted that using 10-layered graded layers reduced the stresses at the crown-cement-dentin interface.

Keywords

Dental ceramics; Graded dental ceramics; Functionally graded materials; Glass infiltration and Silica infiltration

^{*}Corresponding author. sivaranjanigali.pr.ds@msruas.ac.in, nature79gali@gmail.com (S. Gali).

1 Introduction

Functionally graded materials are well-established in nature, and are evident in various biological structures like plants, animals, human teeth, bones, and bio-tissues. In the case of natural teeth, which can be considered a biological composite, they possess a combination of a fragile outer enamel and a resilient inner dentin with a vital pulp, resulting in an unique hierarchical structure that blends toughness, hardness, and resilience [1–4]. In the realm of engineering applications, the concept of functionally graded materials has been explored. This approach facilitates the creation of a seamless gradient across material interfaces to meet specific property requirements [5–8]. Functionally graded materials (FGM) are categorized based on material types and designs and are produced through processes involving gradation and consolidation [5]. Methods for achieving gradation typically involve powder metallurgy, hot pressing, cold pressing, sintering, infiltration, centrifugal casting, slip casting, and thermal spraying. One notable advantage of functionally graded materials (FGM) is the absence of distinct boundaries, which eliminates weak links and results in superior mechanical properties [9–11].

The concept of functionally graded materials (FGM) has also found applications in dental prosthetic systems, particularly in the enhancement of fatigue resistance and strength for dental ceramics. Functionally graded designs were employed to mitigate stress concentrations that typically arise at the interfaces in two-layered dental ceramic systems. This was achieved by reducing the differences in elastic moduli, which alleviates stresses from ceramic-ceramic interfaces (i.e. porcelain veneered zirconia [12,13]. These graded designs, when incorporated into all-ceramic systems, have demonstrated positive outcomes, including improved resistance to damage. Graded layers tend to reduce flexure and contact-induced tensile stresses in the graded zone, thereby, offering more favorable stress distribution. They also exhibit improved mechanical and cementation properties such as resistance to chipping, sliding contact damage, and flexure-induced cementation radial fractures [14–17].

After conducting an initial search on Scopus, Google Scholar, and Cochrane databases (from 2003 to April 5th, 2023), it was found that there were no recent scoping reviews available on graded dental ceramic systems. The objectives of the review are to map graded designs in dental ceramics, distinguish their methodological approaches, and understand the factors affecting the outcomes of each of these graded approaches. This scoping review can serve as a valuable resource to identify the gaps in the development and application of grading in dental ceramic systems and provide guidance for future research endeavors in the field of graded dental ceramics.

2 Methods

The study's protocol followed the framework proposed by Peters et al. according to the Joana Briggs Institute [18]. The protocol can be accessed at this link: 10.11124/JBIES-23– 00143. Additionally, the reporting of this scoping review adhered to the PRISMA Extension for Scoping Reviews [19]. The scoping review questions were "What are the methodological approaches that have been investigated for graded dental ceramics" "What are the material

characteristics, and properties of graded dental ceramics" and "What are the factors influencing the outcomes of each of the graded approaches?

2.1 Inclusion and exclusion criteria

In vitro and experimental studies consisting of functionally graded designs, such as infiltration, compositional gradient, and bio-inspired or biomimetic approaches in dental ceramics were included. Studies investigating the performance of graded dental ceramics regardless of the ceramic material, design, and properties ranging from mechanical, biological, and optical, to other clinically relevant characteristics were considered. Studies that utilized finite element analysis to evaluate stress distributions in functionally graded design structures were incorporated. Studies on functionally graded designs unrelated to dentistry were not considered. Studies on functionally graded designs in dentistry, but not related to dental ceramics were not included. The search was limited to articles written in English due to resource constraints and difficulty in accessing specialized databases and translation services.

2.2 Search strategy

A systematic electronic search was conducted in four databases (PubMed, Scopus, Cochrane, and EBSCO) without any date restrictions (last executed on July 30th, 2023) and was limited to articles written in the English language. The search strategy was based on MeSH terms and specific free-text terms from PubMed, which were adapted for the Scopus and Web of Science databases. All titles and abstracts were subject to the inclusion criteria of observational, interventional studies, studies published in English, and peer-reviewed indexed journals. Narrative reviews, systematic reviews, case reports, case series, letters to the editor, commentaries, studies that were not graded, studies that were not related to dentistry, and studies that were related to other disciplines in dentistry, other than dental ceramics were excluded.

2.3 Study selection

Two researchers, SG and ZP, conducted a joint effort in article identification by individually assessing titles and abstracts, considering predefined eligibility criteria and relevance. The records retrieved were then categorized into three groups: "include," "exclude," or "uncertain." For those falling into the "include" and "uncertain" categories, full-text articles were chosen for a more in-depth evaluation, with SG and ZP conducting this phase independently. Any discrepancies that arose during the screening process were addressed through discussion and consensus, with a third reviewer, SGU, providing additional input as needed.

2.4 Data extraction

Data extraction was performed and presented using tables and illustrations. It focused on describing author information, country, publication year and journal based on the criteria of peer-reviewed with high impact factor. Additionally, detailed information about the methodological approaches of the functionally graded concept, properties and testing methodologies used to evaluate and study conclusions were included.

3 Results

3.1 Search and selection of studies

A search approach combining controlled MeSH terms and text words is presented in Table 1. The PRISMA flow diagram of the study selection process is shown in Fig. 1. About 2675 articles were initially found from all the searches combined from articles published with no date restriction till July 30th, 2023. After removing the duplicates ($n = 1676$), 999 articles remained for screening. After reviewing the titles and abstracts, 930 articles were excluded as they failed to meet the inclusion criteria. The full text of the remaining articles $(n = 73)$ was further examined and reviewed. A summary of the excluded articles along with reasons for exclusion is explained in the PRISMA flowchart. About 52 articles met the inclusion criteria and were included in the systematic review. There was a significant agreement between the 2 reviewers (SG and ZP) for the articles that were screened through titles and abstracts and for articles selected through the full text (Kappa=1, $P < .001$).

3.2 Analysis of selected studies

Fig. 2 presents the frequency distribution of countries pursuing research in graded dental ceramics. Most of the studies were from the USA and Brazil. The methodological approaches to grading dental ceramics can be classified as infiltration through glass or silica sol, interlayers, and compositional gradients. Schematic illustrations of each of the methodological approaches of graded dental ceramics are presented in Fig. 3. Data extraction for each methodological approach is presented in Table 2, Table 3, and Table 4, respectively. While thirty-four studies investigated the graded infiltration method on presintered zirconia, only fourteen studies evaluated interlayers, and four studies investigated compositional gradients.

4 Discussion

Factors affecting the outcomes of each of the methodological approaches of infiltration, compositional gradients, and interlayers in grading dental ceramics are discussed in the following paragraphs.

4.1 Grading through infiltration

Thirty-four studies investigated the graded infiltration method on pre-sintered zirconia of which, twenty-five studies were on glass infiltration $[14–16]$ $[20–41]$. Six studies investigated silica infiltration by sol-gel method [42–47]. Three studies investigated both techniques of silica infiltration and glass infiltration [48–50]. Most studies investigated pre-sintered zirconia, with infiltration either using glass or silica to develop damageresistant dental ceramic systems. In other studies, motivations differed such as four studies investigated the bond strength of zirconia to resin cement, and three studies studied the bond strength between porcelain and zirconia. Research has extensively examined the effects of both glass and silica infiltrations on pre-sintered zirconia, assessing aspects such as fatigue, bond strength, wear, and long-term performance, including color and translucency properties.

Infiltration involves adding glass or silica to porous ceramic materials like pre-sintered zirconia. Graded glass infiltrations have benefits such as easy application addressing issues like glaze detachment and improving resistance to chipping [14–16] [20–41]. Silica infiltration enhances adhesion to resin cement with zirconia [42–47].

4.1.1 Characteristics of glass, and silica sol—Various types of glasses were employed for infiltration, as shown in Table 2. Zhang's research team utilized a lanthanumbased glass with specific attributes, including a similar coefficient of thermal expansion $(10^5$ X 10^{-6} /C) within the range of 25 to 450 °C, translucency, a high melting point, and resistance to crystallization. The infiltrating glass must possess a similar coefficient of thermal expansion to zirconia ceramic, a low elastic modulus, and Poisson's ratio comparable to the ceramic substrate. A gradual increase in elastic modulus from the glass surface to the underlying ceramic helps reduce residual stresses and the risk of flexural damage at the margins and connector regions of dental prostheses. The graded design structure also enhances resistance to sliding contact and facilitates both esthetics and adhesive bonding on the occlusal and intaglio surfaces of zirconia ceramics [14–16] [20–25]. Sawada's research group employed a slurry conditioner composed of a blend of silicate ceramic and quartz [26,27,31]. Campos's research group, used silica sol for silica infiltration, obtained through an aqueous sodium metasilicate solution via ion exchange resin [42,43,46].

4.1.2 Method of application of glass slurry and silica sol—Infiltration techniques for glass, involved the use of the slurry approach, applying glass slurry with a brush onto the pre-sintered zirconia surfaces. This involved mixing glass powder with distilled water. Thick, medium, and small artisan brushes with either single or two coatings were used. A concentration of 500 μg/ml was used to produce the fluorapatite glass-ceramic slurry [41]. Two studies used spin coating method [28,30].

Silica, however, was applied differently, using the immersion method, with varying soaking and drying times across studies. Soaking durations ranged from 60 s to 5 days, dried at temperatures of 60 °C to 100 °C for periods spanning 20 min to 2 days. Some studies utilized catalysts like ammonium carbonate to adjust pH, typically between 2 and 7, employing two immersion cycles [42–47,50]. These catalysts significantly reduced infiltration time and, with more frequent immersion, improved flexural strength and surface consistency.

4.1.3 Thickness of glass and graded or infiltrated layers—In the following discussions, it is important to distinguish between the thickness of the superficial glass layer and the graded or infiltrated layer. The infiltrated layer is the thickness of the perpetration of glass through the porous pre-sintered zirconia driven through capillary action, compared to the surface glass layer.

In studies based on Zhang's glass infiltration method, the infiltrated layers contained approximately 45% glass near the interfaces of the residual glass layer. The thickness of the residual glass layer was reported to be within the range of 15–40 μm, while the thickness of the infiltration was 120 ± 10 µm [20,21]. In another study, the surface residual glass

had a thickness of 300 μm, and the infiltrated glass-zirconia layer measured 2000 μm [25]. For yet another study, the external glass layer was 20 μm thick, and the infiltrated layer was 60 μm thick [14]. The thickness of the infiltrated layer was approximately 900–1000 μm in controlled conditions [29]. For glass-infiltration in 3Y and 5Y zirconia, the thickness of glass layer was reported as 28 μm, with the glazed layer measuring 22 μm [50]. In the context of graded dental implants, the thickness of the infiltrated glass layer ranged from 100 μm to 150 μm [37].

In silica infiltration, the thickness of the silica film was measured at 10 μm [46]. Some other studies observed a thickness of 5 μm for the conditioner and 6 μm for silica [43,44]. It's worth noting the varying thickness of the glass and infiltrated layers. The thickness of the infiltrated layer was greater than that of the external glass layer, perhaps due to the capillary forces driving the glass to perpetrate through the porous pre-sintered zirconia. The difference between low thickness of silica compared with the glass layer could be investigated in future research studies. The use of a slurry brush application for glass infiltration and its viscosity could have resulted in thicker layers compared to silica infiltration using immersion. Irrespective of the thickness of the glass or silica layers, the gradual change in modulus from top to bottom is known to enhance contact damage resistance in graded structures [14].

4.1.4 Characteristics of pre-sintered zirconia—Pre-sintered zirconia was available either as prefabricated blanks or powder compacts of 5.18 mol% zirconia isostatically cold pressed at 200 MPa, and pre-sintered in air from 1100 $^{\circ}$ C to 1400 $^{\circ}$ C for 1 h [14–16,20–25]. Only five studies performed experiments using full-contour crowns and bridges [16,36,48– 50]. Ultra translucent 5Y zirconia with feldspathic glass was used [33].

4.1.5 Effect of infiltration on zirconia—The effect of infiltration on phase assemblage, microstructure, surface hardness, fracture toughness, surface roughness, contact angle, flexural strength, chipping resistance, wear, shear bond strength, and survival rates of zirconia will be discussed in the following sections.

4.1.5.1 Phase assemblage and microstructure: The phase composition of dental zirconia subjected to glass infiltration displayed the presence of a glassy layer where lanthanumbased glass was used for infiltration [15, 20,24]. Following glass infiltration, characteristic tetragonal peaks of zirconia remained unchanged and were apparent. However, an increased presence of the monoclinic phase was observed with a minor t-m transformation [25,27,42]. The glass content was virtually eliminated close to the graded interface [14–16,20–24]. This results in the formation of a three-dimensional network structure consisting of residual glass traces, glass-coated zirconia grains, and intergranular voids. This structure enhances the bond strength of infiltrated zirconia to adhesive resin cement by providing an ideal surface morphology for silanization. SEM images revealed the presence of porosities in Bioglassinfiltrated zirconia [31,38]. In sol-gel-based glaze application, there was a formation of monoclinic zirconia accompanied by the development of large grains near the graded glass interface. This microstructure resembled zirconia's response to low-temperature degradation, which leads to the formation of the monoclinic phase with an increase in grain size. Monoclinic zirconia grains exhibit lower density and are larger than tetragonal grains.

This incongruity contributes to compressive stresses around cracks, thereby enhancing the material's strength [42].

In silica sol infiltration, microstructure revealed diffusion of silica and a reaction with zirconia, leading to the formation of an intermediate crystalline phase that is highly resistant to corrosion. The phase assemblage of silica-infiltrated zirconia revealed the presence of a zirconia silicate phase, along with the tetragonal and cubic phases of zirconia. The silicainfiltrated zirconia contained 24% of $ZrSiO₄$ and 48% tetragonal zirconia [42–47].

4.1.5.2 Surface hardness: In the studies, Vickers microhardness was employed with varying loads, including 200 g and 20 N. Bioglass-infiltrated zirconia exhibited relatively low hardness (9.51 GPa) when compared to the control group of sintered zirconia (14 GPa) and sand-blasted zirconia. This lower hardness can be attributed to the surface microstructure and nature of the glass. However, this reduced hardness may offer potential benefits in terms of minimizing antagonist wear and improving adhesion to resin cement, particularly on the intaglio surface of zirconia crowns [38].

Similarly, sol-gel-based glaze-infiltrated zirconia displayed lower hardness (6.97 GPa) in contrast to the control group, which had a hardness of 13.7 GPa [46]. On the other hand, silica infiltration resulted in improved structural homogeneity and hardness for the infiltrated monolithic zirconia, with a hardness of 14.79 GPa, which was higher than that of the control zirconia. This improvement in hardness can be attributed to the filling of surface irregularities with silica and the reaction of silica gel with polycrystalline zirconia, forming a harder material, zirconium silicate [43,44].

4.1.5.3 Fracture toughness: Vickers indentation hardness was employed under a 50 N load to assess fracture toughness using the indentation method. The fracture toughness of glass-infiltrated zirconia was found to be approximately 3.76 MPa \cdot m^{\wedge 0.5}, which was similar to the fracture toughness of the zirconia control group, measuring at 3.53 MPa·m^{\wedge 0.5 [20]. In} silica-infiltrated zirconia, there was a reduction in fracture toughness, which was measured at 4.72 MPa \cdot m^{\wedge 0.5}, as compared to the control zirconia with a fracture toughness of 5.84 MPa \cdot m^{\wedge 0.5}. The measurement in this case was conducted using the micro-indentation technique [51]. However, the method of measuring indentation fracture toughness is variable as it tends to overstate the material's resistance to crack growth.

For sol-gel-infiltrated zirconia, the fracture toughness was determined to be 3.82 MPa·m^{\wedge 0.5}, while untreated zirconia had a fracture toughness of 5 MPa·m $\frac{1}{6}$ [46]. This reduction in the fracture toughness of the infiltrated specimens was attributed to the presence of glass among the grains, which decreased bonding at their boundaries, along with an increase in the yttria content due to the formation of zirconium silicate (ZrSiO4). The application method appeared to have influenced the uniformity of the silica coating, impacting interfacial fracture toughness [46].

4.1.5.4 Surface roughness and contact angle: Glass-infiltrated zirconia exhibited a relatively high surface roughness of approximately 3.21 μm, which was significantly higher than that of sintered zirconia with a surface roughness of 0.45 μm [38]. This difference in

surface roughness may be attributed to the melting and diffusion of glass particles during the sintering process of pre-sintered zirconia coated with Bioglass, resulting in surface irregularities.

In contrast, zirconia infiltrated with a sol-gel glaze demonstrated low surface roughness, measuring at 0.08 μm, which was notably lower than both commercial glaze and sintered zirconia with surface roughness values of 0.66 μm [46]. This reduction in surface roughness was attributed to the thermal compatibility of the glass and zirconia, as well as the favorable surface interaction that resulted in good wettability of glass and zirconia, allowing for a uniform glass coating with low surface roughness.

The contact angle between the zirconia substrate and the infiltrated glass was measured in two studies using the sessile drop technique, with one study utilizing drop shape analysis [27]. It was observed that the contact angle decreased with an increase in temperature, measuring at 43.2° at 1200 °C [25]. Infiltrated zirconia exhibited a low contact angle, indicating good wettability with resin cement [42]. Moreover, the contact angle of the conditioner-coated surface was favorable, measuring 36.2°, and it was further improved with etching (39.8°) and sandblasting (36°) [27].

4.1.5.5 Flexural strength: In studies involving glass and silica infiltration, biaxial flexural strength tests were conducted, with a focus on evaluating the Weibull modulus and characteristic strength. In all these studies, the strength values of infiltrated zirconia were consistently higher than those of un-infiltrated zirconia [14,28,31,33,41–46]. Silicainfiltrated zirconia exhibited high Weibull modulus values (m=15) and a characteristic strength of 768 MPa, which was notably higher than that of un-infiltrated zirconia. This increase in strength was attributed to several factors, including improved surface homogeneity and the filling of surface flaws with silica. Additionally, the gradation of elastic moduli through infiltration contributed to enhanced load-bearing capacity due to the formation of $ZrSiO₄$ on the surface [42]. In bio-inspired designs, where silica-infiltrated zirconia was tested on the tensile side, it showed even better Weibull modulus (m=9.59) and a characteristic strength of 834 MPa, making it the most reliable group according to Weibull analysis of biaxial flexural strength [44]. In another study, the Weibull modulus and strength of sol-gel glaze-infiltrated zirconia were higher (m=8.51, characteristic strength=946 MPa) than those of control zirconia (m=7.09, characteristic strength=775 MPa) [46].

Graded ceramics that incorporated low modulus glass demonstrated high critical loads to flexural fracture. This outcome was attributed to the infiltration of glass into the flaws or defects of zirconia, resulting in a reduction in tensile and flexural stress at the interface [15,20]. Bioglass-coated zirconia showed flexural strength values comparable to untreated zirconia, with values of 618 MPa and 718 MPa, respectively [45]. Conditioner-coated zirconia exhibited high flexural strength values, regardless of whether sandblasting was applied, with a Weibull modulus (m) of 9.65 and a characteristic strength of 920 MPa. The conditioner's role was to form a composite with the underlying zirconia, thereby preventing the reverse transformation of zirconia. Weibull modulus values appeared to be more dependent on surface homogeneity and the presence of defects [31].

4.1.5.6 Shear bond strength and chipping resistance: Shear bond strength tests were conducted in four separate studies, with one of them employing a micro-shear bond strength test. Additionally, two studies utilized interfacial fracture energy tests to assess bonding quality. Three of these studies focused on the bond strength between porcelain and zirconia infiltrated with glass. One of these studies identified a significantly higher bond strength when using graded glass zirconia cores with veneering porcelain compared to traditional bilayered systems, registering at 24.3 MPa, whereas the control group yielded a bond strength of 9.2 MPa. In another study, no significant difference was observed in bond strength between porcelain and conditioned zirconia, with values falling within the range of 21–24 MPa [25,26]. The interfacial fracture was also investigated in graded glass-infiltrated zirconia, revealing no apparent delamination between the graded glass layer and zirconia [23]. This strong bond effectively improved chipping resistance by preventing median cracks from developing under contact forces [23,32]. It's noteworthy that unstable channel cracks at the porcelain-zirconia interface were replaced by a single channel crack located at the interface of the graded glass layer and zirconia [32]. Furthermore, veneered conventional zirconia displayed superior resistance to scratching and debonding compared to other materials [47].

In comparison to silica infiltration, glass infiltration demonstrated better interfacial toughness, largely due to the irregularities in silica infiltration during immersion. Additionally, three studies explored the bond strength of glass-infiltrated zirconia to resin cement. In zirconia coated with conditioner, the adhesion between resin cement and zirconia decreased after infiltration, registering at 6.5 MPa. However, sandblasting conditioner-coated zirconia significantly enhanced the bond strength to 14.3 MPa, emphasizing the importance of mechanical retention to improve resin cement adhesion to zirconia [31]. Further-more, Bioglass-infiltrated zirconia exhibited a shear bond strength of 3.73 MPa after undergoing thermocycling, thanks to the silicate-rich and etchable rough surface created by the Bioglass infiltrate [38].

4.1.5.7 Fatigue: Two studies evaluated the fatigue of glass-infiltrated zirconia crowns. The fatigue limits of the full-contour 3-unit fixed dental prosthesis of glass-infiltrated zirconia showed higher fatigue limits of staircase tests than silica-infiltrated and sintered zirconia [48]. The initial load to fracture and step-size were higher in glass-infiltrated (2264 N; 113) than in silica-infiltrated (1833 N; 91) than in untreated zirconia (1335 N; 66). The high fatigue limits are due to the filling of granular spaces by infiltrated glass, with lower elastic modulus, wherein it can resist fracture to a better distribution of stresses. However, there was a high variation of fatigue values which could be due to different thicknesses of the residual glass layer. Silica-infiltrated zirconia showed low variation in fatigue due to surface homogeneity [48]. Sliding contact fatigue of glass-infiltrated zirconia and monolithic demonstrating lifetimes were 10^6 to 10^7 orders of magnitude longer than that of porcelainveneered zirconia of $62,000 + 28,500$ cycles [23].

Sliding fatigue tests revealed high fatigue values for graded bio-inspired with porcelain infrastructure with silica-infiltrated zirconia than conventional design and graded designs of silica-infiltrated zirconia infrastructure and porcelain veneer. The Weibull parameters beta and eta were, respectively: Traditional 1.30 and 2.3×10^6 cycles, and graded was 1.95 and

 2.3×10^6 cycles. Thus, the Traditional and Graded crowns presented greater susceptibility to failure due to fatigue, while the Bioinspired and Graded Bioinspired crowns showed no fatigue effect using 100 N load, showing beta and eta of values of 17×10^6 cycles. [49]. Silica-infiltrated showed less sliding fatigue wear, with the lowest volume loss and silica clusters formation on the zirconia surface results in an elastic gradient and reducing stress concentrations.

4.1.5.8 Wear: Three separate studies examined the sliding wear of infiltrated zirconia, employing different wear apparatus, loads, frequencies, and cycles. The studies utilized three distinct wear testing machines: the Oregon Health Science University (OHSU) oral wear simulator, which applied a 50 N load at a frequency of 1 Hz for 450,000 cycles; a contact-sliding-lift-off mouth-motion cyclic loading machine, which subjected the material to an electrodynamic fatigue testing machine with a 200-N load for 1.25 million cycles at a loading rate of 1000 N/s (approximately 2 Hz); and a mechanical machine that operated under a 200 N load at a frequency of 4 Hz for 1.25 million cycles [35,36,50].

The findings showed that silica-infiltrated and polished-glazed zirconia caused less wear to the opposing dental structures. Interestingly, the specific type of zirconia used (3Y or 5Y) did not have a significant impact on the amount of wear experienced by the antagonist. Notably, polished glass-infiltrated zirconia demonstrated the most favorable wear performance, exhibiting minimal surface damage and reduced abrasiveness on the opposing dental structures. Additionally, combining the techniques of polishing and glass infiltration on the occlusal surface of monolithic zirconia crowns led to decreased wear on both the ceramic crown itself and the opposing dental structures [35,36].

4.1.5.9 Survival probability: Glass-infiltrated, silica-infiltrated, polished, and glazed table-top zirconia restorations underwent sliding wear tests, and the number of cycles until failure was recorded. Silica infiltration led to a decrease in the survival probabilities of zirconia restorations, falling below 85%. This reduction in survival probabilities was attributed to the incomplete immersion method used for the crowns, which affected the depth of infiltration. Interestingly, the type of zirconia, whether it was 3 mol% or 5 mol% yttriastabilized, did not have a significant impact on the volume loss experienced by the opposing dental structures. However, 3 mol% yttria-stabilized zirconia exhibited higher survival probabilities when compared to 5 mol% yttria-stabilized zirconia and lithium disilicate. It's worth noting that lithium disilicate table-tops also showed survival probabilities lower than 85% [50].

4.1.5.10 Fractography: Typically, ceramics showcase distinct fractographic attributes, due to their brittle nature and unique fracture behavior. These features include a polished surface, often seen during rapid fractures, radial patterns stemming from the point of impact, cleavage planes indicating preferred crack paths, and a lack of significant deformation before sudden failure. Microscopic details like hackle and chevron marks near cracks, secondary fracture features, and the influence of grain boundaries further characterize ceramic fractures. About twenty-four studies reported fractographic features of glass and silica-infiltrated zirconia. The fractographic features of infiltrated zirconia varied depending on the loading conditions [52].

Under sliding contact fatigue, glass-infiltrated samples displayed lateral chipping and cracks in the glass layer. Crushed glass around the rim of the crater with fine fractures emanating from flaws at the leading edge of the crater were observed [23]. Cracking was the primary flaw in graded crowns compared to delamination in porcelain-veneered zirconia [49]. The glass-infiltrated zirconia bridges under staircase fatigue predominantly experienced failures originating from the pontic's occlusal surface [48]. In silica-infiltrated zirconia under sliding contact fatigue, edge chipping fracture was observed in silica-infiltrated 3 mol% yttria-stabilized zirconia. Partial cone cracks with quasi-plastic deformation on the contact area, and edge chipping resulting from cone cracks were observed [50].

The failure modes after the flexural strength test showed the following observations. Glass-infiltrated zirconia failed from defects on the sub-surface than on the surface in glazed zirconia [46]. Glass-infiltrated zirconia emerged stronger with the presence of cracks compared to catastrophic fractures of the bio-inspired design of zirconia. Strong bonding between the glass infiltrated and the underlying zirconia substrate, was attributed to the intersection of cracks at the interface and penetration to the zirconia sublayer without causing delamination. This results in significantly enhanced resistance to chipping in glass-infiltrated zirconia [15,20]. The failure modes after shear bond strength showed glass-infiltrated zirconia with a rough surface indicating high fracture energy compared to branching of cracks in porcelain-veneered zirconia [32]. Bioglass-infiltrated zirconia had high bond strength with the absence of cracks and fractures [38].

Scratch testing of silica-infiltrated zirconia revealed susceptibility to damage, displaying spalling and cracks under minimal loads, compared to conventional zirconia [44]. In silicainfiltrated zirconia, fracture starting points appeared as semi-elliptical flaws, contrasting with the patterns observed in conventional zirconia as mist hackles and compression curls [42]. Silica-infiltrated zirconia with veneering porcelain resulted in various damages like cracks, buckling, and wedging spallations, causing delamination at comparatively lower loads compared to conventional veneered zirconia. The observed cracks extended to the zirconia-porcelain interface, suggesting a weaker interaction likely due to porcelain pores, with the fracture's origin on the zirconia [43].

The prerequisites for glass-infiltration of zirconia encompass the following criteria. Ensuring that the glass frit has a strong affinity for zirconia, promoting interlayer diffusion, and thereby creating a robust bond. Selecting a glass with an average coefficient of thermal expansion (CTE) equal to that of zirconia, which serves to minimize any residual stress. Opting for a glass material with low viscosity, making it amenable to infiltration at the specific experimental temperature. Choosing a glass that is chemically compatible with zirconia to prevent any adverse chemical degradation when exposed to a reactive environment.

4.2 Interlayers

Fourteen studies investigated on interlayers for functionally graded dental restorations. Differences in the properties of metal-ceramics in a bilayered dental restorations lead to thermal and mechanical stresses at their interface, often causing bond failures. The incorporation of a smooth transitional interlayer has been observed to enhance the bond

strength between metal or veneer and ceramic core. Graded bioinspired design showed favourable stress distribution as zirconia on the surface absorbs the higher stresses and protects the weak porcelain from potentially destructive tensile stresses [58]. FGM layer between zirconia and dentin substrate withstand high critical loads of 2640 N under 1000 N/s loading rates compared to control groups of 2099 N [56]. Under pop-in Hertzian loads, zirconia ceramics with underlying FGM layers showed radial cracks beneath zirconia with partial cracking at the interface of zirconia-FGM [56,58].

Around seven studies employed FEA for analyzing stress under loading conditions in functionally graded dental ceramics. One study applied phase stress analysis, and five studies investigated thermal residual stresses. Only two studies were experimental. Most studies were on metal-ceramics, two studies were on zirconia-porcelain, and one each as on feldspathic porcelain-garnet and monolithic ceramic crown. Finite element studies differed in the models, software used, element size, structure, and loading conditions (Table 3). Analytical models such as laminate theory and Hsueh's model were utilized for the prediction of stresses in graded zirconia systems [63]. Factors affecting interlayers were the thickness of the layer, its location, and the type of prosthesis. The design of the layers differed either as an interlayer between metal-ceramic or as a 10-layered functionally graded ranging from 100–1000 μm at interfaces of all-ceramic core-veneer, ceramic core-cement, or dentin. The results indicated a reduction in maximum principal stress and thermal residual stress in all-ceramic and metal-ceramic restorative designs [53–66].

4.3 Compositional gradients

Functionally Graded Materials (FGM) are composite materials with a diverse composition, creating a gradient in properties from one side to the other. These property gradients enhance the material's mechanical performance and its ability to withstand thermal and mechanical stresses [10,67–70]. Varying volume fractions of zirconia and porcelain across the graded structures were processed using powder stacking. Further, conventional and spark plasma sintering methods were employed [67–69]. Factors such as the number of layers with volume fractions, the thickness of each layer, the particle size of each constituent, and the type of sintering influenced their properties, as shown in Table 4.

4.4 Research gaps & future recommendations

Having good wettability with zirconia stands out as the most significant factor in the infiltration process. In silica-infiltrated zirconia, a critical step involves immersing presintered zirconia in silica sol to create a uniform coating, which plays a pivotal role in enhancing the material's properties. Additionally, the process of silica infiltration necessitates the use of a catalyst to expedite the infiltration and increase the frequency of immersion. The outlined future research areas for infiltrated zirconia requires investigations of pH cycling and temperature effects on material performance, introducing fluorescent agents to enhance optical properties, and its response to cyclic loading and resistance to failures from occlusal contact. Additionally, understanding toughening transformation mechanisms of infiltrated zirconia and its resilience against chemical degradation is also necessary. Translating the findings from finite element analysis studies that involve the use

of ten-layered graded layers between cement and crown to reduce interfacial stresses into experimental studies to validate their practical application needs to be explored.

5 Conclusions

Methodological approaches in grading have been majorly investigated in dental pre-sintered zirconia. The type of infiltration and the method of infiltrate application have a significant influence on the phase transformation of zirconia, its microstructure, surface hardness, fracture toughness, and fatigue strength of graded dental zirconia.

- **•** Glass infiltration with slurry brush yielded thicker graded layers compared to silica infiltration with immersion.
- **•** Silica-infiltration forms zirconium silicate at the superficial graded layer unlike non-reactive glass-infiltration
- **•** Enhanced hardness and lowered fracture toughness were observed in silica infiltration than in glass-infiltration.
- **•** Surface roughness depends on the contact angle of the infiltrated glass or silica irrespective of the infiltration method.
- **•** The infiltration method did not affect the strength of zirconia in glass-infiltration, however in silica-infiltrations, the reliability and strength improved.
- **•** Both glass and silica-infiltration enhanced bonding with resin cement and porcelain veneers
- **•** Glass-infiltrated zirconia is more fatigue-resistant and has a higher survival probability than silica-infiltrated zirconia
- **•** Silica-infiltrated zirconia is more wear-resistant than glass-infiltrated zirconia
- **•** Interlayers accommodated between metal-ceramic and veneer-core ceramic layers enhanced their bond strength
- **•** Fractions of zirconia-porcelain and alumina-porcelain showed high bending strength and dynamic modulus.
- **•** 10 layered graded layers between cement and crown was predicted to reduce interfacial stresses in finite element analysis studies, its feasibility needs to be explored.

Acknowledgements

This research was funded by DBT/Wellcome Trust India Alliance Early Career Fellowships for Clinicians and Public Health Research with the grant number IA/CPHE/18/1/503943.

References

[1]. Rasmussen ST, Patchin RE. Fracture properties of human enamel and dentin in an aqueous environment. J Dent Res. 1984; 63 (12) 1362–8. [PubMed: 6595288]

- [2]. Meredith N, Sherriff M, Setchell DJ, Swanson SAV. Measurement of the microhardness and young's modulus of human enamel and dentine using an indentation technique. Arch Oral Biol. 1996; 41 (6) 539–45. [PubMed: 8937644]
- [3]. Habelitz S, Marshall SJ, Marshall GW Jr, Balooch M. Mechanical properties of human dental enamel on the nanometre scale. Arch Oral Biol. 2001; 46 (2) 173–83. [PubMed: 11163325]
- [4]. Cuy JL, Mann AB, Livi KJ, Teaford MF, Weihs TP. Nanoindentation mapping of the mechanical properties of human molar tooth enamel. Arch Oral Biol. 2002; 47 (4) 281–91. [PubMed: 11922871]
- [5]. Niino M, Hirai T, Watanabe R. The functionally gradient materials. J Jap Soc Compos Mat. 13: 257–264.
- [6]. Report on Fundamental study on relaxation of thermal stress for high temperature material by tailoring the graded structure. Department of Science and Technology Agency; 1992.
- [7]. Shanmugavel P, Bhaskar GB, Chandrasekaran M, Mani PS, Srinivasan SP. An overview of fracture analysis in functionally graded materials. Eur J Sci Res. 2012; 68 (3) 412–39.
- [8]. Mahamood, Rasheedat M; Akinlabi, Esther T; IAENG. Shukla, Mukul; Pityana, Sisa. Functionally Graded Material: An Overview; Proceedings of the World Congress on Engineering 2012 Vol III WCE 2012, July 4 - 6, 2012, London, UK;
- [9]. Besisa DH, Ewais E. Chapter 1 Advances in Functionally Graded Ceramics Processing, Sintering Properties and Applications. 2018.
- [10]. Suresh R. Graded materials for resistance to contact deformation and damage. Science. 2001; 292 2447 [PubMed: 11431558]
- [11]. Kieback B, Neubrand A, Riedel H. Processing techniques for functionally graded materials. Mater Sci Eng: A. 2003; 362: 81–106.
- [12]. Petit C, Palmero P. Functionally graded ceramics for biomedical applications: concept; manufacturing, properties. Int J Appl Ceram Tech. 2018; 15 (4) 820–40.
- [13]. Rahbar N, Soboyejo WO. Design of functionally graded dental multilayers. Fatigue Fract Eng Mater Struct. 2011; 34: 887–97.
- [14]. Zhang Y, Sun MG, Zhang D. Designing functionally graded materials with superior load-bearing properties. Acta Biomater. 2012; 8: 1101–8. [PubMed: 22178651]
- [15]. Zhang Y, Kim JW. Graded structures for damage resistant and aesthetic all-ceramic restorations. Dent Mater. 2009; 25 (6) 781–90. [PubMed: 19187955]
- [16]. Zhang Y, Chai H, Lee JJW, Lawn BR. Chipping resistance of graded zirconia ceramics for dental restorations. J Dent Res. 2012; 91 (3) 311–5. [PubMed: 22232142]
- [17]. Zhang Y. Overview: Damage resistance of graded ceramic restorative materials. J Eur Ceram Soc. 2012; 32: 2623–32. [PubMed: 22778494]
- [18]. Peters MD, Marnie C, Tricco AC, Pollock D, Munn Z, Alexander L, et al. Updated methodological guidance for the conduct of scoping reviews. JBI Evid Synth. 2020; 18 (10) 2119–26. [PubMed: 33038124]
- [19]. Tricco AC, Lillie E, Zarin W, O'Brien KK, Colquhoun H, Levac D, et al. PRISMA extension for scoping reviews (PRISMA-ScR): checklist and explanation. Ann Intern Med. 2018; 169 (7) 467–73. [PubMed: 30178033]
- [20]. Zhang Y, Chai H, Lawn BR. Graded structures for all-ceramic restorations. J Dent Res. 2010; 89 (4) 417–21. [PubMed: 20200413]
- [21]. Kim JW, Liu L, Zhang Y. Improving the resistance to sliding contact damage of zirconia using elastic gradients. J Biomed Mater Res Part B: Appl Biomater. 2010; 94 (2) 347–52.
- [22]. Zhang Y, Kim J-W. Graded zirconia glass for resistance to veneer fracture. J Dent Res. 2010; 89 (10) 1057–62. DOI: 10.1177/0022034510375289 [PubMed: 20651092]
- [23]. Ren L, Janal MN, Zhang Y. Sliding contact fatigue of graded zirconia with external esthetic glass. J Dent Res. 2011; 90 (9) 1116–21. [PubMed: 21666105]
- [24]. Chai H, Lee JJ, Mieleszko AJ, Chu SJ, Zhang Y. On the interfacial fracture of porcelain/ zirconia and graded zirconia dental structures. Acta Biomater. 2014; 10 (8) 3756–61. [PubMed: 24769152]

- [25]. Liu R, Sun T, Zhang Y, Zhang Y, Jiang D, Shao L. The effect of graded glass–zirconia structure on the bond between core and veneer in layered zirconia restorations. J Mech Behav Biomed Mater. 2015; 46: 197–204. [PubMed: 25814206]
- [26]. Spintzyk S, Yamaguchi K, Sawada T, Schille C, Schweizer E, Ozeki M, et al. Influence of the conditioning method for pre-sintered zirconia on the shear bond strength of bilayered porcelain/ zirconia. Materials. 2016; 9 (9) 765. [PubMed: 28773885]
- [27]. Sawada T, Spintzyk S, Schille C, Zöldföldi J, Paterakis A, Schweizer E, et al. Influence of pre-sintered zirconia surface conditioning on shear bond strength to resin cement. Materials. 2016; 9 (7) 518. [PubMed: 28773641]
- [28]. Park S, Oh Gyejeong, Jang Kyung-Jun, Ji Min-Kyung, Kim Ji Hyun, Kim Jin Won, et al. Effect of infiltration with ferric oxide containing glass on the color and mechanical properties of zirconia. Key Eng Mater. 2016; 696: 113–7.
- [29]. Sun T, Guo M, Cheng Y, Ou L, He P, Liu X, et al. Graded nano glass-zirconia material for dental applications-part II biocompatibility evaluation. J Biomed Nanotechnol. 2017; 13 (12) 1682–93. DOI: 10.1166/jbn.2017.2379 [PubMed: 29490756]
- [30]. Oh GJ, Yoon JH, Vu VT, Ji MK, Kim JH, Kim JW, et al. Surface characteristics of bioactive glass-infiltrated zirconia with different hydrofluoric acid etching conditions. J Nanosci Nanotechnol. 2017; 17 (4) 2645–8.
- [31]. Sawada T, Schille C, Zöldföldi J, Schweizer E, Geis-Gerstorfer J, Spintzyk S. Influence of a surface conditioner to pre-sintered zirconia on the biaxial flexural strength and phase transformation. Dent Mater. 2018; 34 (3) 486–93. [PubMed: 29301652]
- [32]. Chai H, Mieleszko AJ, Chu SJ, Zhang Y. Using glass-graded zirconia to increase delamination growth resistance in porcelain/zirconia dental structures. Dent Mater. 2018; 34 (1) e8–14. DOI: 10.1016/j.dental.2017.11.004 [PubMed: 29183670]
- [33]. Mao L, Kaizer MR, Zhao M, Guo B, Song YF, Zhang Y. Graded ultra-translucent zirconia (5Y-PSZ) for strength and functionalities. J Dent Res. 2018; 97 (11) 1222–8. [PubMed: 29694258]
- [34]. Volpato CA, Carvalho ÓS, Pereira da Cunha MR, da Silva FS. Evaluation of the color and translucency of glass-infiltrated zirconia based on the concept of functionally graded materials. J Prosthet Dent. 2019; 121 (3) 547–e1.
- [35]. Kaizer MR, Moraes RR, Cava SS, Zhang Y. The progressive wear and abrasiveness of novel graded glass/zirconia materials relative to their dental ceramic counterparts. Dent Mater. 2019; 35 (5) 763–71. [PubMed: 30827797]
- [36]. Kaizer MR, Bano S, Borba M, Garg V, Dos Santos MB, Zhang Y. Wear behavior of graded glass/ zirconia crowns and their antagonists. J Dent Res. 2019; 98 (4) 437–42. [PubMed: 30744472]
- [37]. Fabris D, Fredel MC, Souza JC, Silva FS, Henriques B. Biomechanical behavior of functionally graded S53P4 Bioglass-zirconia dental implants: experimental and finite element analyses. J Mech Behav Biomed Mater. 2021; 120 104565 [PubMed: 34087536]
- [38]. El-Wassefy NA, Özcan M, Abo El-Farag SA. Effect of simultaneous sintering of Bioglass to a zirconia core on properties and bond strength. Materials. 2021; 14 (23) 7107 [PubMed: 34885262]
- [39]. Kumar NK, Nair A, Thomas PM, Hariprasad L, Brigit B, Merwade S, et al. Zirconia surface infiltration with low-fusing glass: a surface treatment modality to enhance the bond strength between zirconia and veneering ceramic. J Conserv Dent: JCD. 2022; 25 (5) 492. [PubMed: 36506626]
- [40]. Zhou M, Zhang X, Zhang Y, Li D, Zhao Z, Wang Q, et al. Construction of nanostructured glass-zirconia to improve the interface stability of dental bilayer zirconia. Nanomaterials. 2023; 13 (4) 678. [PubMed: 36839046]
- [41]. Zhang Y, Gaoqi Wang, Tingting Kong, Shuo Yao, Junling Wu. Infiltrating fluorapatite glassceramics on the surface of dental 3% yttria-stabilized zirconia to enhance bond strength. Surf Coat Technol. 2023; 461 129436
- [42]. Campos TM, Ramos NC, Machado JP, Bottino MA, Souza RO, Melo RM. A new silicainfiltrated Y-TZP obtained by the sol-gel method. J Dent. 2016; 48: 55–61. [PubMed: 27012859]

- [43]. Reis AF, Ramos GF, Campos TM, Prado PH, Vasconcelos G, Borges AL, et al. The performance of sol-gel silica coated Y-TZP for veneered and monolithic dental restorations. J Mech Behav Biomed Mater. 2019; 90: 515–22. [PubMed: 30453115]
- [44]. Toyama DY, Alves LM, Ramos GF, Campos TM, de Vasconcelos G, Borges AL, et al. Bioinspired silica-infiltrated zirconia bilayers: Strength and interfacial bonding. J Mech Behav Biomed Mater. 2019; 89: 143–9. [PubMed: 30273833]
- [45]. Yamada M, Valanezhad A, Egoshi T, Tashima Y, Watanabe I, Murata H. Bioactive glass coating on zirconia by vacuum sol-dipping method. Dent Mater J. 2019; 38 (4) 663–70. DOI: 10.4012/ dmj.2018-222 [PubMed: 31189794]
- [46]. Campos TM, de Melo Marinho RM, Ribeiro AD, do Amaral Montanheiro TL, da Silva AC, Thim GP. Microstructure and mechanical properties of fully sintered zirconia glazed with an experimental glass. J Mech Behav Biomed Mater. 2021; 113 104093 [PubMed: 33022517]
- [47]. Ramos NC, Kaizer MR, Campos TM, Kim J, Zhang Y, Melo RM. Silica-based infiltrations for enhanced zirconia-resin interface toughness. J Dent Res. 2019; 98 (4) 423–9. [PubMed: 30763138]
- [48]. Villefort RF, Amaral M, Pereira GK, Campos TM, Zhang Y, Bottino MA, et al. Effects of two grading techniques of zirconia material on the fatigue limit of full-contour 3-unit fixed dental prostheses. Dent Mater. 2017; 33 (4) e155–64. [PubMed: 28118929]
- [49]. Ramos GF, Ramos NC, Alves LM, Kaizer MR, Borges AL, Campos TM, et al. Failure probability and stress distribution of milled porcelain-zirconia crowns with bioinspired/traditional design and graded interface. J Mech Behav Biomed Mater. 2021; 119 104438 [PubMed: 33798936]
- [50]. Alves LM, da Silva Rodrigues C, de Carvalho Ramos N, Buizastrow J, Campos TM, Bottino MA, et al. Silica infiltration on translucent zirconia restorations: effects on the antagonist wear and survivability. Dent Mater. 2022; 38 (12) 2084–95. [PubMed: 36446649]
- [51]. Anstis G, Chantikul P, Lawn B, Marshall D. A critical evaluation of indentation techniques for measuring fracturetoughness: I, direct crack measurements. J Am Ceram Soc. 1981; 46: 533–8. DOI: 10.1111/j.1151-2916.1981.tb10320.x
- [52]. Scherrer SS, Lohbauer U, Della Bona A, Vichi A, Tholey MJ, Kelly JR, et al. ADM guidanceceramics: guidance to the use of fractography in failure analysis of brittle materials. Dent Mater. 2017; 33: 599–620. [PubMed: 28400062]
- [53]. Okazaki M, Wang X, Toguchi Ms, Taira M, Takahashi J, Matsuo C, et al. Improvement of bond strength in metal-ceramic systems using a gold intermediate layer. Dent Mater J. 1998; 17 (3) 163–73. [PubMed: 9893497]
- [54]. Henriques B, Gonçalves S, Soares D, Silva FS. Shear bond strength comparison between conventional porcelain fused to metal and new functionally graded dental restorations after thermal-mechanical cycling. J Mech Behav Biomed Mater. 2012; 13: 194–205. DOI: 10.1016/ j.jmbbm.2012.06.002 [PubMed: 22922336]
- [55]. Huang M, Wang R, Thompson V, Rekow D, Soboyejo WO. Bioinspired design of dental multilayers. J Mater Sci: Mater Med. 2007; 18: 57–64. [PubMed: 17200814]
- [56]. Niu X, Rahbar N, Farias S, Soboyejo W. Bio-inspired design of dental multilayers: experiments and model. J Mech Behav Biomed Mater. 2009; 2 (6) 596–602. [PubMed: 19716103]
- [57]. Rahbar N, Soboyejo WO. Design of functionally graded dental multilayers. Fatigue Fract Eng Mater Struct. 2011; 34 (11) 887–97.
- [58]. Du J, Niu X, Rahbar N, Soboyejo W. Bio-inspired dental multilayers: effects of layer architecture on contact-induced deformation. Acta Biomater. 2013; 9 (2) 5273–9. [PubMed: 22940125]
- [59]. Cui C, Sun J. Optimizing the design of bio-inspired functionally graded material (FGM) layer in all-ceramic dental restorations. Dent Mater J. 2014; 33 (2) 173–8. [PubMed: 24583648]
- [60]. Henriques B, Gonçalves S, Soares D, Silva FS. Shear bond strength comparison between conventional porcelain fused to metal and new functionally graded dental restorations after thermal–mechanical cycling. J Mech Behav Biomed Mater. 2012; 13: 194–205. [PubMed: 22922336]

- [61]. Henriques B, Miranda G, Gasik M, Souza JC, Nascimento RM, Silva FS. Finite element analysis of the residual thermal stresses on functionally gradated dental restorations. J Mech Behav Biomed Mater. 2015; 50: 123–30. [PubMed: 26122789]
- [62]. Henriques B, Fabris D, Souza JC, Silva FS, Mesquita-Guimarães J, Zhang Y, et al. Influence of interlayer design on residual thermal stresses in trilayered and graded all-ceramic restorations. Mater Sci Eng: C. 2017; 71: 1037–45.
- [63]. Askari E, Flores P, Silva F. A particle swarm-based algorithm for optimization of multi-layered and graded dental ceramics. J Mech Behav Biomed Mater. 2018; 77: 461–9. [PubMed: 29028598]
- [64]. Fabris D, Souza JC, Silva FS, Fredel M, Mesquita-Guimarães J, Zhang Y, et al. Thermal residual stresses in bilayered, trilayered and graded dental ceramics. Ceram Int. 2017; 43 (4) 3670–8. [PubMed: 28163345]
- [65]. Penteado MM, Tribst JPM, Dal Piva AM, Ausiello P, Zarone F, Garcia-Godoy F, et al. Mechanical behavior of conceptual posterior dental crowns with functional elasticity gradient. Am J Dent. 2019; 32 (4) 165–8. [PubMed: 31436935]
- [66]. Sait F, Saeidi N, Korkmaz T. Finite element analysis of FGM dental crowns using phase-field approach. J Mech Behav Biomed Mater. 2023; 138 105629 doi: 10.1016/j.jmbbm.2022 [PubMed: 36535094]
- [67]. Tsukada G, Sueyoshi H, Kamibayashi H, Tokuda M, Torii M. Bending strength of zirconia/ porcelain functionally graded materials prepared using spark plasma sintering. J Dent. 2014; 42 (12) 1569–76. [PubMed: 25280989]
- [68]. Al-Maqtari AA, Razak AA, Hamdi M. 3D Finite element analysis of functionally graded multilayered dental ceramic cores. Dent Mater J. 2014; 33 (4) 458–65. [PubMed: 25087658]
- [69]. Madeira S, Mesquita-Guimarães J, Ribeiro P, Fredel M, Souza JC, Soares D, et al. Y-TZP/ porcelain graded dental restorations design for improved damping behavior–a study on damping capacity and dynamic Young's modulus. J Mech Behav Biomed Mater. 2019; 96: 219–26. [PubMed: 31055212]
- [70]. Suteja IA, Kim J, Zhang S, Gal CW, Choi YJ, Park H, et al. Fabrication of color-graded feldspathic dental prosthetics for aesthetic and restorative dentistry. Dent Mater. 2023; 39 (6) 568–76. DOI: 10.1016/j.dental.2023.03.021 [PubMed: 37088587]

Fig. 1. PRISMA 2020 flow diagram of the search.

Fig. 2. Frequency distribution of countries researching graded dental ceramics.

Graded Designs in Dental Ceramics

Fig. 3. Schematic illustration of functionally graded designs in dental ceramic systems.

Table 1

Search strategy of each database.

GZG structure demonstrated

 \overline{a}

L,

Table 3 Data extraction of studies using interlayers.

Table 4 Data extraction of studies using compositional gradients.

S. No.	Author and year	Journal	Country	Material Characteristics	Properties evaluated	Results
1.	Tsukada 201467	Journal of Dentistry	Japan	Zirconia-Porcelain Yttria-stabilized tetragonal zirconia (Y-TZ) powder- High Fusing Porcelain Y-TZP/ porcelain volume fractions were as follows: $100/0$ 90/10 80/20 70/30 0/100	Three-point bending test, density, thermal stress estimation, Weibull analysis, Young's modulus, coefficient of thermal expansion.	Graded structure effectively increased the bending strength of Y-TZP/porcelain-composite materials.
2.	Maqtari 201468	Dental Materials Journal	Malaysia	Varied compositions were estimated by applying the "rule of mixture" (ROM) for the following: Zirconia (100%) without Alumina, Zirconia $(80\%) +$ Alumina (20%) Zirconia (60%) + Alumina (40%), Zirconia $(50\%) +$ Alumina (50%) First layer consisting of Zirconia (100%) (without Alumina) with Second Layer of Zirconia (80%) + Alumina (20%) First layer consisting of Zirconia (100%) (without Alumina) with a Second Layer of Zirconia (60%) + Alumina (40%) First layer of Zirconia (100%) (without Alumina) with Second Layer of Zirconia (50%)+Alumina (50%)	Stress distribution using Finite element analysis	von Mises stress, tensile stress, and compressive stress in functionally graded structures were reduced.Reduced shear stress were observed in functionally graded veneer-core-cement-dentin interfaces.
3.	Madeira 201969	Journal of the Mechanical Behaviour of Biomedical Materials	Portugal Brazil	Zirconia-porcelain Yttria-stabilized tetragonal zirconia (Y-TZ) powder-Dental Porcelain Y-TZP/porcelain volume (%) fractions were of $0/100$, $20/80$, $40/60$, 60/40, 80/20 and 100/0.	Damping capacity, dynamic Young's modulus, microhardness, dynamic mechanical analysis	Increased damping capacity was exhibited by porcelain matrix composites, whereas a higher dynamic modulus was exhibited by zirconia- rich composites.
4.	Suteja 202370	Dental Materials	Korea	Cerium-Porcelain and Yttrium aluminum garnet cerium (YAG-Ce)- Feldspathic Porcelain (FP). Y-FP layers (volume %) with shade from bottom to top of 180 layers $(0/100)$, Yellow 140 layers (25/75), decreasing yellow 100 layers $(50/50)$, decreasing yellow 90 layers (75/25), slightly whiter 70 layers and $(100/0)$ slightly whiter.	Slurry viscosity, flowability, UV sensitivity, curing penetration, density, shrinkage; CIE lab color difference and flexural strength	Functionally graded additive manufacturing (FGAM) technique successfully reproduced color gradation by manipulating the composition shift of FP and YAG:Ce. This result underscores the potential of FGAM as a promising alternative for producing dental prosthetics with improved esthetic appeal.