



OPEN

Force–velocity profile during vertical jump cannot be assessed using only bodyweight jump and isometric maximal voluntary contraction tasks

Nejc Šarabon^{1,2}✉, Žiga Kozinc^{1,3} & Goran Marković^{4,5}

Recently, the two-point method of force–velocity (F–V) profiling of multi-joint human movements has been introduced and validated. In this study, we investigated the validity of estimating the jumping F–V profile using only bodyweight jump and isometric maximal voluntary contraction (MVC) task. Participants ($n = 30$) performed 3 repetitions of squat (SJ) and counter-movement jumps (CMJ), each at loads that were progressively increased by 10 kg increments, with the number of loads depending on the individual's ability. Then, 3 isometric MVC trials were performed in 3 knee angles (30°, 60° and 90°). F–V profiling of SJ and CMJ were performed using the multiple-point method, the two-point method, and the novel Jump-MVC method. The results showed poor to fair validity of the novel Jump-MVC method for assessing jumping F–V profile (most ICC < 0.5, most CV > 10%, significant systematic bias present, and the presence of proportional bias). The exception was the estimation of theoretical maximal power, which was highly valid for both SJ and CMJ (ICC = 0.91–0.95; CV = 5.0–6.3%). In contrast, validity of the two-point method was excellent (all ICC > 0.90; CV = 2–6%). Although additional studies are needed, present results suggest that the F–V profiling of vertical jumps should be performed using the two-point method with distal loads.

It is well documented that vertical jumping performance in athletes is associated with athletic performance^{1–5}, notably sprinting^{1–3} and change-of-direction ability^{4,5}. Parameters associated with vertical jump performance have been shown to be highly reliable^{6–10}. While force plates are considered a gold standard for vertical jump testing, lower-cost alternatives, such as certain jumping (i.e. contact) mats^{11–13} also provide trustworthy estimation of jump height. Although jump height, along with force- and power-related parameters assessed during vertical jumps are associated with athletic performance, these variables represent only a limited aspect of jumping ability and cannot distinguish between force-, velocity- and power producing capacity^{14,15}. For this reason, there has recently been an increased interest in exploring the individual's force–velocity (F–V) profile^{16–21}.

Inverse linear relationship between force/torque and linear/angular velocity has been documented for several multi-joint movements²². It has been shown that performing resistance exercise can alter the F–V profile^{19,23} and that these changes in F–V profile depend on the type of resistance exercise¹⁹. It was also shown that athletes of different sports are characterized by substantially different F–V profiles²⁴. Furthermore, theoretical simulations have shown that an optimal F–V profile (i.e. the slope of the inverse linear F–V relationship) that maximizes jump height exist for a given individual's power capabilities, push-off distance and the angle of push-off²⁵. Further research has demonstrated that using the postulated optimal F–V relationship as a guide for prescription of individualized training improves vertical jumping performance¹⁹. Although improving maximal theoretical power (P_{max}) is the most straightforward way to improve vertical jump performance, the results of the aforementioned study showed that individualized training, based on the F–V profile may also contribute to these improvements,

¹Faculty of Health Sciences, University of Primorska, Polje 42, 6310 Izola, Slovenia. ²Laboratory for Motor Control and Motor Behavior, S2P, Science To Practice, Ltd, Tehnološki Park 19, 1000 Ljubljana, Slovenia. ³Andrej Marušič Institute, University of Primorska, Muzejski trg 2, 6000 Koper, Slovenia. ⁴Faculty of Kinesiology, University of Zagreb, Horvaćanski zavoj 15, 10110 Zagreb, Croatia. ⁵Motus Melior Ltd, Hektorovičeva ul. 2, 10000 Zagreb, Croatia. ✉email: nejc.sarabon@fvz.upr.si

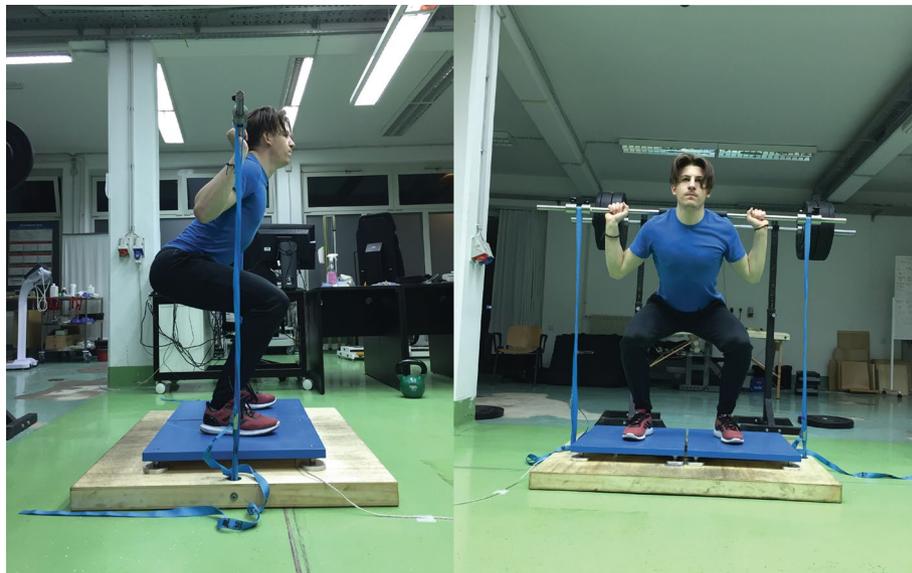


Figure 1. The set-up and positioning during isometric MVC tasks. The length of the bands was adjusted to ensure 30°, 60° and 90° knee angles.

without even increasing P_{\max} . Therefore, assessment of individual's F–V profile can provide valuable information that can help optimize the strength and conditioning programs.

The traditional multiple-point protocol was shown to be potentially fatiguing²⁶, time-consuming and, from the authors practical experience, also potentially dangerous. Building on the fact that F–V relationship is approximately linear and usually very strong²², Jaric¹⁵ and Garcia-Ramos & Jaric¹⁴ proposed that multiple loads could be replaced with only two loads, without producing significant testing errors (i.e. the two-point method). This was confirmed for several movement tasks, including vertical jumps, cycling, bench press throws, and bench pull²⁷. Recently, Garcia-Ramos and colleagues²⁶ tested the two-point method, which involved performing the jump only with zero additional load and with a high load (75 kg). They reported that this protocol is less fatiguing, reliable and valid (compared to the common multiple-point method) for determining F–V profiles for both squat jump (SJ) and counter-movement jump (CMJ). Thus, this approach represents an important optimization of the protocol for F–V profile assessment. While the previous studies have mostly used fixed loads (such as 75 kg in the study by Garcia-Ramos et al.²⁶), the validity of the two-point methods that use the high load relative to the individual's strength ability remains unknown. Although no direct evidence is available on the injury risk of weighted jumping with high loads, very high compressive forces on the lumbar spine (6–10 times body weight) have been reported during half-squats with the loads in the range 0.8 to 1.6 times body weight²⁸. Due to ballistic nature of vertical jumps, these compressive loads on the lumbar spine are likely even higher during weighted jumps. In addition, heavy-load resistance exercise has been associated with injury risk²⁹, and jumps are known to induce considerable forces on the lower limbs³⁰.

The primary aim of this study was to investigate whether the high load within the two-point approach could be replaced with a maximal isometric voluntary contraction (MVC) task, performed in body configuration similar to the one during the push-off phase of jumping. Specifically, we compared the F–V profiles and associated force, velocity and power parameters, obtained by (1) the multiple-point method, (2) the two-point method using bodyweight jumps and high load jumps and (3) a novel Jump-MVC method, using bodyweight jump data and force obtained during an MVC task, performed in a position that resembles the push-off phase. We hypothesized that both the novel Jump-MVC two-point method and the original two-point method^{14,15} are valid approaches for assessing individual's F–V profile and associated parameters during vertical jumping.

Methods

Participants. The study population was comprised of 30 young athletes and recreationally active individuals with ≥ 3 years of experience with resistance exercise (21 men; age: 24.2 ± 3.8 years; body height: 180.1 ± 5.9 cm; body mass: 78.8 ± 8.6 kg, 9 women; age: 26.1 ± 2.8 years; body height: 169.6 ± 7.5 cm; body mass: 67.1 ± 10.4 kg). Exclusion criteria were any musculoskeletal injuries and pain syndromes within the previous 12 months and any other health problems that could interfere with the procedure or cause damage to the participants. Participants were thoroughly informed about the protocol in advance and were assured that they may withdraw from the experiment at any point. Informed consent was signed prior to the beginning of the experiment. The protocol was conducted in accordance with the Helsinki declaration and Oviedo convention and was approved by the Republic of Slovenia's National Medical Ethic Committee (Approval number: 0120–690/2017/8). The participant displayed on Fig. 1 has provided written informed to publish his image alongside the manuscript.

Study design and procedure. The experiment was conducted in a single session, lasting approximately 90 min. First, the participants performed a warm-up, consisting of 6 min of light aerobic exercise, 13 dynamic stretching exercises (1 set of 6 repetitions each) and 5 bodyweight resistance exercises (1 set of 10 repetitions each). Because not all participants were familiar with the vertical jumping technique, they performed 8 repetitions of SJs and CMJs, with the purpose to familiarize with the task. Technique, but not maximal effort, was emphasized during these introductory jumps.

The main protocol involved performing SJ and CMJ tasks with different loads on a bilateral force plate (Kistler KiJump, Type 9229A, Kistler Instruments, Winterthur, Switzerland). The load was provided with 20-kg Olympic barbell and free weights. Participants always started with zero additional load. In this condition, a lightweight (<0.5 kg) plastic bar was used instead of the barbell to ensure comparable position to loaded conditions. The next load was set at 20 kg (using only the barbell), and then, the load was gradually increased by adding 10 kg until when and any difficulties in maintaining balance before, during or after the jumps were visually observed by the examiners or if the participants expressed any concerns of continuing, for which they were asked after each load. The protocol was also terminated in case of jump height below 7.5 cm. Three repetitions of SJ and CMJ were performed at each load, and the jump with the maximal achieved height was taken for further analyses. The order of the jump types (SJ and CMJ) were randomized between participant and was kept the same for each participant as the loads increased. The break between repetitions was set at ~60 s, and the break between different loads was set at ~3 min. Longer breaks were provided at higher loads when participants reported fatigue. The starting position of the SJ^{31,32} and the depth of the countermovement of the CMJ³³ can heavily influence vertical jump parameters. Therefore, the starting height for SJ and the CMJ depth were recorded and kept constant throughout the trials (the knee angle at 90°). For SJ, an elastic band was positioned for each individual on the appropriate height to be in contact with participants' buttocks when the desired angle was reached^{31,32}. For the CMJ, the elastic band was moved slightly posteriorly relative to the participants to avoid interference and one examiner stood nearby the participant with a straightedge to visually control the countermovement depth.

The session concluded with performing isometric MVC in three positions that closely resembled phases of the push off action, with ground reaction forces being recorded. The positions were determined by the knee angles of 30°, 60° and 90°. The order of positions was randomized between participants. Participants were required to exert maximal force against a bar, tightly strapped to the floor in a way that allowed it to be lifted only to a height corresponding to the respective knee angle value (Fig. 1). Three repetitions, with a 3-s period of maximal exertion, were performed at each knee angle, with 1-min brakes provided between repetitions and between conditions. All participants successfully completed the protocol without any complaints.

Data processing and outcome measures. Ground reaction force signals were sampled at 1000 Hz and smoothed using a flow arithmetic mean filter (5 ms) as default pre-set by the manufacturer. The trials were captured with the MARS Software (Kistler, Winterthur, Switzerland), which enables immediate and reliable³⁴ calculation of the mechanical jump variables. For the purposes of this study, the average force (F_A), average velocity (V_A) and average power (P_A) during the push off phase of the best jump (largest jump height) trial within each condition was used. Based on the F_A and V_A data across loading condition, the F–V relationship was determined using least squares linear regressions. The intercepts with force axis and velocity axis were calculated to determine the predicted force in isometric conditions (F_0) and maximal theoretical velocity (V_0), respectively. The F–v profile was calculated as the slope of the F–v linear relationship, using the following equation^{25,26,35}:

$$F\text{-}V\text{ Slope} = -\frac{F_0}{V_0}$$

Finally, the theoretical maximal power (P_{\max}) was calculated as in the previous F–V studies^{23,26,35,36}, pertaining to jumping performance:

$$P_{\max} = \frac{F_0 V_0}{4}$$

For the Jump-MVC method, the same approach was then used to calculate F–V Slope, F_0 , V_0 and P_{\max} , by using only the data from jumps with no additional load and isometric MVC in the linear regression. For the MVC task, only force was recorded, and V_A was assumed to be zero. These computations were performed using either force data from the best trial for one of the conditions (one knee angle) or the average force of the three MVCs at all three angles. Finally, we calculated the same parameters based only on the bodyweight jump and the highest load for each individual, in order to compare our Jump-MVC method to the original two-point method, as assessed previously by Garcia-Ramos and colleagues²⁶, but with high load dictated by individual's capabilities.

Statistical analysis. All statistical analyses were performed using SPSS Statistics (Version 20.0, Armonk, NY: IBM Corp.). Descriptive statistics was calculated and reported as mean ± standard deviation. The normality of the data distribution was checked with Shapiro–Wilk test. The differences between the mean values for isometric force among different knee angle conditions was tested with repeated measures analysis of variance and Bonferonni-corrected post-hoc t-tests. The validity of the Jump-MVC and original two-point methods in comparison to the gold standard multiple-point method was tested in several ways. First, we calculated two-way mixed single ($ICC_{3,1}$) and average ($ICC_{3,k}$) intra-class correlation coefficients with respective 95% confidence intervals. The agreement was interpreted as: fair (ICC 0.40–0.59); moderate (ICC 0.60–0.74), and good to excellent (ICC 0.75–1.00)³⁷. Second, Bland–Altman plots were also used to further elucidate the agreement between different methods. Third, we used paired-sample t-tests for assessing systematic bias between the meth-

ods, and we calculated the standard error of measurement (SEM) and coefficients of variation (CV (%) = SEM/mean × 100) to explore within-individual variation. Finally, ordinary least products (OLP) regression was used to assess bias between the multiple-point and the Jump-MVC method. OLP provides estimates for the intercept and slope of a regression line that accounts for variability in both the x and y axis data. Fixed and proportional bias can be inferred from these estimates using their confidence intervals³⁸. Fixed bias is present if the confidence interval of the intercept estimate does not include 0. Proportional bias is present if the confidence interval of the slope estimate does not include 1³⁸. In this study, the reported confidence intervals are bias-corrected accelerated confidence intervals derived from bootstrapping the estimates with 10,000 repetitions. The reliability (i.e. the inter-repetition consistency) of MVC trials and single-jump parameters was assessed by ICC, using the same cut-off values as above, and the CV. For all analyses, the outcomes were considered as statistically significant at $p < 0.05$.

Results

The variables related to the F–V relationship (F_0 , V_0 , P_{\max} and F–V slope) were normally distributed for multi-point method ($p = 0.076$ – 0.770), two-point method ($p = 0.066$ – 0.601) and for the Jump-MVC method, regardless of the knee angle condition from which the data was used for F–V relationship calculation ($p = 0.089$ – 0.892).

Reliability. The reliability (i.e., the inter-repetition consistency) of force measurements during MVC trials was excellent according to the ICC for the knee angles of 30° (ICC = 0.92; 95%CI: 0.80–0.96), 60° (ICC = 0.91; 95%CI: 0.78–0.96) and 90° (ICC = 0.95; 95%CI: 0.92–0.99). Moreover, CV values were acceptable for 30°, 60° and 90° angle (CV = 6.7, 8.3 and 1.6%, respectively).

Similarly, the reliability of jump height was excellent in bodyweight (ICC = 0.97; 95%CI: 0.92–0.99) and loaded conditions (ICC = 0.87–0.96; 95% CI: 0.69–0.99). P_A was also analyzed and were also shown as highly reliable for bodyweight jumps (ICC = 0.96; 95% CI: 0.90–0.99) and loaded jumps (ICC = 0.84–0.97; 95% CI: 0.67–0.99). Note that reliability analysis was not done for the 100 kg load, as only 2 participants completed this task (see below for details).

Jumping ability and strength. There was a substantial between-participant variability of the highest load that the jumps could be performed with (range: 30–100 kg). All participants completed the jumps with at least additional 30 kg. The rest of the loads were achieved by different number of participants as follows: 29 participants up to 40 kg, 25 up to 50 kg, 21 up to 60 kg, 19 up to 70 kg, 10 up to 80 kg, 6 up to 90 kg and 2 up to 100 kg). The average SJ height achieved with the highest load was 10.1 ± 0.3 cm (range = 6.3–15.4 cm). The average CMJ height achieved with the highest load was 11.5 ± 0.4 cm (range = 6.7–17.6 cm).

There was also a high variability between participants in bodyweight jumping performance, with SJ heights in no load condition ranging from 22.5 cm to 42.7 cm (mean value: 31.8 ± 0.07 cm), and CMJ heights in no load condition ranging from 22.1 cm to 47.9 cm (mean value: 34.2 ± 0.07 cm). The force exerted during MVC differed between the three knee angle conditions. The highest mean maximal force was observed at the 30° knee angle (3072.9 ± 631.6 N; range: 1646.6–4204.1 N), followed by the 60° knee angle (2796.9 ± 638.8 N; range: 1593.8–4223.0 N) and the 90° knee angle (1691.3 ± 266.7 N; range: 1178.0–2349.1 N). This difference was statistically significant ($F = 185.4$; $p < 0.001$), with pairwise t-tests showing statistically significant differences between all pairs (all $p < 0.001$).

For the SJ, the F_A recorded during the jump with the highest load achieved was $54.8 \pm 8.1\%$ of the force during MVC task with 30° knee angle, $60.8 \pm 11.2\%$ of the force during MVC with 60° knee angle and $98.2 \pm 12.3\%$ of the force during MVC with 90° knee angle. For the CMJ, the F_A recorded during the jump with the highest load achieved was $59.2 \pm 9.3\%$ of the force during MVC task with 30° knee angle, $65.6 \pm 12.7\%$ of the force during MVC with 60° knee angle and $106.2 \pm 14.1\%$ of the force during MVC with 90° knee angle.

Linear force–velocity relationships. For both vertical jumps, the relationship between F_A and V_A across multiple loads, as assessed by Pearson's correlation coefficient, was very strong and consistent across participants (SJ: $r = -0.95 \pm 0.03$, range: 0.84–0.99; CMJ: $r = -0.95 \pm 0.04$, range: 0.83–0.99).

Validity of the two-point method. A comparison of F–V profiles, calculated with the original two-point and with Jump-MVC method for one participant, is shown on Fig. 2. For both SJ and CMJ, the validity of the two-point method was excellent for the slope of the F–V relationship (ICCs = 0.96 and 0.95), and all associated parameters (ICC for $F_0 = 0.97$ and 0.98; for $V_0 = 0.98$ and 0.91; for $P_{\max} = 0.99$ and 0.97). Detailed results are presented in Table 1.

Validity of the Jump-MVC method. For most parameters associated with F–V profiling, the Jump-MVC method was not in agreement with the multiple-point method when using isometric data from measurements at a single knee angle condition. Using the averaged data across the three angles somewhat improved the agreement, although the validity, particularly the estimations of V_0 and F–V slope remained poor (Tables 2 and 3). Figure 3 displays Bland–Altman plots for the comparison of multiple-point and Jump-MVC method, using average knee angle data. These results were shown for display as the most reliable (in comparison with single-angle conditions).

Specifically, for the SJ, F–V slope estimation was at best fair (ICCs = 0.570) when the mean of the MVC data from all the three knee angle conditions was used. Even using this approach, there was a statistically significant overestimation of the F–V slope ($p = 0.001$). When single knee angle approaches were used, the agreement was

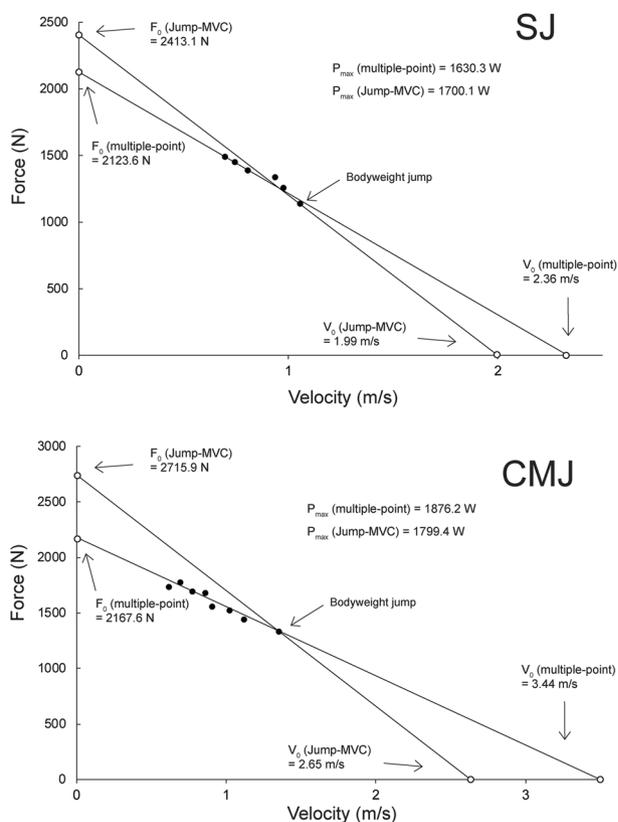


Figure 2. Graphical representation of F–V profiling for a sample subject using multiple-point method and Jump-MVC method, using mean force data from the 30, 60 and 90° angles. SJ—Squat jump, CMJ—countermovement jump, F_0 —maximal force, V_0 —theoretical maximal velocity, P_{max} —maximal power.

	Mean scores		Intra-class correlation		Within-individual error		Systematic error		
	Multiple-point method	Two-point method	ICCs	ICCa	SEM	CV%	t	Sig	ES
Squat jump									
F_0 (N)	2244.2 ± 418.8	2252.7 ± 419.2	0.984 (0.964–0.993)	0.990 (0.982–0.996)	53.6	2.38 (1.86–3.32)	–0.56	0.582	0.01
V_0 (m/s)	2.40 ± 0.51	2.37 ± 0.50	0.975 (0.944–0.989)	0.980 (0.971–0.994)	0.1	3.35 (2.62–4.67)	1.03	0.314	0.04
P_{max} (W)	1330.3 ± 304.5	1322.7 ± 307.1	0.991 (0.979–0.996)	0.990 (0.990–0.998)	29.6	2.23 (1.74–3.10)	0.91	0.372	0.03
F–V slope	–984.0 ± 297.3	–1001.7 ± 324.6	0.962 (0.917–0.983)	0.980 (0.957–0.991)	60.5	–6.09 (–4.76 to –8.48)	1.03	0.312	0.04
Counter movement jump									
F_0 (N)	2193.5 ± 379.4	2206.4 ± 360.4	0.986 (0.968–0.994)	0.990 (0.984–0.997)	44.5	2.02 (1.58–2.81)	–1.02	0.316	0.04
V_0 (m/s)	4.50 ± 0.83	4.50 ± 0.83	0.907 (0.800–0.958)	0.950 (0.889–0.979)	0.3	5.73 (4.47–7.97)	–0.04	0.969	0.00
P_{max} (W)	2450.6 ± 554.3	2484.8 ± 633.4	0.967 (0.927–0.985)	0.980 (0.962–0.993)	107.8	4.37 (3.41–6.077)	–1.12	0.273	0.05
F–V slope	–506.1 ± 137.3	–506.0 ± 128.3	0.949 (0.887–0.977)	0.970 (0.940–0.988)	30.7	–6.05 (–4.73 to –8.43)	–0.02	0.986	0.00

Table 1. Validity of the two-point method for assessment of the force–velocity profile during vertical jumping. F_0 —maximal isometric force; V_0 —maximal theoretical velocity; P_{max} —maximal power; ICCs—single measures intra-class correlation coefficient; ICCa—average measures intra-class correlation coefficient; SEM—standard error of measurement; CV%—coefficient of variation; ES—Effect size (Cohen’s d).

	Mean scores		Intra-class correlation		Within-individual error		Systematic error		
	Multiple-point method	Jump-MVC	ICCs	ICCa	SEM	CV%	t	Sig	ES
MVC Angle 30°									
F ₀ (N)	2244.2 ± 418.8	2962.4 ± 639.3	0.402 (-0.093–0.760)	0.570 (-0.206–0.864)	269.1	10.34 (8.07–14.38)	-9.44	0.000	0.79
V ₀ (m/s)	2.40 ± 0.51	1.84 ± 0.34	0.365 (-0.106–0.719)	0.530 (-0.237–0.837)	0.25	11.75 (9.18–16.35)	7.95	0.000	0.72
P _{max} (W)	1330.3 ± 304.5	1346.6 ± 310.9	0.949 (0.888–0.977)	0.970 (0.941–0.988)	70.2	5.24 (4.095–7.30)	-0.82	0.418	0.03
F–V slope	-984.0 ± 297.3	-1674.6 ± 498.2	0.261 (-0.089–0.628)	0.410 (-0.194–0.772)	250.7	-18.8 (-14.7 to -26.2)	9.74	0.000	0.80
MVC Angle 60°									
F ₀ (N)	2244.2 ± 418.8	2691.8 ± 627.0	0.481 (-0.035–0.769)	0.640 (-0.073–0.869)	318.3	12.92 (10.07–17.93)	-4.97	0.000	0.51
V ₀ (m/s)	2.40 ± 0.51	2.02 ± 0.49	0.440 (0.006–0.723)	0.610 (0.011–0.839)	0.33	15.01 (11.72–20.82)	4.02	0.000	0.40
P _{max} (W)	1330.3 ± 304.5	1329.5 ± 313.1	0.950 (0.890–0.978)	0.970 (0.942–0.989)	70.5	5.3 (4.14–7.38)	0.04	0.970	0.00
F–V slope	-984.0 ± 297.3	-1422.8 ± 508.1	0.330 (-0.087–0.653)	0.490 (-0.190–0.790)	292.4	-24.30 (-18.97 to -33.81)	5.30	0.000	0.54
MVC Angle 90°									
F ₀ (N)	2244.2 ± 418.8	1673.3 ± 278.6	0.305 (-0.085–0.681)	0.460 (-0.185–0.810)	196.4	10.028 (7.83–13.95)	10.28	0.000	0.81
V ₀ (m/s)	2.40 ± 0.51	4.48 ± 2.51	0.089 (-0.140–0.374)	0.160 (-0.326–0.544)	1.68	48.75 (38.062–67.81)	-4.4	0.000	0.45
P _{max} (W)	1330.3 ± 304.5	1830.2 ± 873.2	0.322 (-0.040–0.622)	0.480 (-0.084–0.767)	502.9	31.83 (24.85–44.28)	-3.51	0.002	0.34
F–V slope	-984.0 ± 297.3	-450.3 ± 182.8	0.131 (-0.074–0.428)	0.230 (-0.161–0.599)	185.3	-25.85 (-20.18 to -35.96)	-10.2	0.000	0.81
MVC Angle: Mean of 30°, 60° and 90° angles									
F ₀ (N)	2244.2 ± 418.8	2442.5 ± 489.8	0.725 (0.349–0.883)	0.840 (0.517–0.938)	210.0	8.96 (7.00–12.47)	-3.34	0.003	0.32
V ₀ (m/s)	2.40 ± 0.51	2.18 ± 0.50	0.565 (0.218–0.783)	0.720 (0.358–0.878)	0.31	13.76 (10.74–19.14)	2.48	0.021	0.20
P _{max} (W)	1330.3 ± 304.5	1311.7 ± 309.5	0.955 (0.902–0.980)	0.970 (0.949–0.990)	64.9	4.92 (3.84–6.84)	1.01	0.324	0.04
F–V slope	-984.0 ± 297.3	-1182.6 ± 363.4	0.570 (0.131–0.803)	0.720 (0.232–0.891)	192.3	-17.76 (-13.86 to -24.70)	3.65	0.001	0.36

Table 2. Validity of the Jump-MVC method for assessment of the force–velocity profile in squat jump. F₀—maximal isometric force; V₀—maximal theoretical velocity; P_{max}—maximal power; MVC—maximal voluntary contraction; ICCs—single measures intra-class correlation coefficient; ICCa—average measures intra-class correlation coefficient; SEM—standard error of measurement; CV%—coefficient of variation; ES—Effect size (Cohen's d); Note that for the two-point methods, the F₀ is the actual maximal isometric force (i.e. recorded during maximal voluntary contraction).

poor (ICCs = 0.131–0.330), with larger differences between the mean values. The accuracy of the F₀ estimation was poor for all of the single knee angle conditions (ICCs = 0.305–0.481) and moderate when data from all angles were combined (ICCs = 0.725). The F₀ was significantly overestimated for 30° and 60° knee angle conditions, but underestimated for 90° angle (all $p < 0.001$). Similar as for the F₀, the V₀ estimation was poor for all the single knee angle conditions (ICCs = 0.089–0.440), and fair when the combination of angles was used (ICCs = 0.565). In contrast to the F₀, the V₀ was significantly underestimated for the 30° and the 60° knee angle conditions, but overestimated for the 90° angle (all $p < 0.001$). Estimation of the P_{max} was excellent for all approaches (ICCs = 0.949–0.955), except when 90° knee angle was used (ICCs = 0.322). Detailed results for the SJ trials are presented in Table 2.

Similarly, for the CMJ, F–V slope estimation, using either individual angles or the combination of angles, was poor (ICCs = 0.133–0.481). F₀ was statistically significantly (all $p < 0.001$) overestimated when data from the 30° knee angle, the 60° knee angle or mean of the three angles was used to compute the F–V relationship, and the estimation was poor to fair (ICCs = 0.293–0.590). If only the data from the 90° knee angle condition was used, there was no statistically significant systematic effect ($p = 0.220$), and the agreement was moderate (ICCs = 0.721). Estimation of V₀ had poor agreement, regardless of the approach (ICCs = 0.177–0.449), with statistically significant underestimation for all conditions (all $p < 0.001$), except when 90° knee angle data was used ($p = 0.519$). P_{max} estimation had high to excellent agreement for all approaches (ICCs = 0.762–0.918), but there were statistically significant effects for all knee angle conditions ($p = 0.001–0.021$), except for the 90° knee angle ($p = 0.180$). Detailed results for the CMJ trials are presented in Table 3.

	Mean scores		Intra-class correlation		Within-individual error		Systematic error		
	Multiple-point method	Jump-MVC method	ICCs	ICCa	SEM	CV%	t	Sig	ES
MVC Angle 30°									
F ₀ (N)	2193.5 ± 379.4	3123.3 ± 670.9	0.293 (-0.075–0.673)	0.450 (-0.162–0.804)	290.85	10.94 (8.54–15.22)	-11.30	0.000	0.84
V ₀ (m/s)	4.50 ± 0.83	2.98 ± 0.55	0.177 (-0.067–0.520)	0.300 (-0.144–0.684)	0.45	12.16 (9.50–16.92)	11.78	0.000	0.85
P _{max} (W)	2450.6 ± 554.3	2296.1 ± 499.1	0.894 (0.599–0.962)	0.940 (0.749–0.981)	139.27	5.87 (4.58–8.16)	3.93	0.001	0.39
F–V slope	-506.1 ± 137.3	-1090.8 ± 336.9	0.133 (-0.069–0.435)	0.230 (-0.148–0.606)	186.58	-23.37 (-18.25 to -32.51)	11.08	0.000	0.84
MVC Angle 60°									
F ₀ (N)	2193.5 ± 379.4	2831.9 ± 680.8	0.361 (-0.104–0.698)	0.530 (-0.232–0.822)	349.9	13.93 (10.87–19.38)	-6.44	0.000	0.63
V ₀ (m/s)	4.50 ± 0.83	3.40 ± 0.97	0.319 (-0.105–0.659)	0.480 (-0.234–0.794)	0.61	15.40 (12.024–21.42)	6.38	0.000	0.63
P _{max} (W)	2450.6 ± 554.3	2329.9 ± 565.9	0.911 (0.757–0.964)	0.950 (0.862–0.982)	148.3	6.20 (4.84–8.63)	2.88	0.008	0.26
F–V slope	-506.1 ± 137.3	-913.1 ± 372.2	0.180 (-0.101–0.492)	0.300 (-0.226–0.660)	223.5	-31.49 (-24.59 to -43.81)	6.44	0.000	0.63
MVC Angle 90°									
F ₀ (N)	2193.5 ± 379.4	2273.04 ± 468.5	0.721 (0.468–0.866)	0.830 (0.638–0.928)	223.39	10.0 (7.81–13.92)	-1.26	0.220	0.06
V ₀ (m/s)	4.50 ± 0.83	4.71 ± 1.92	0.426 (0.043–0.700)	0.590 (0.082–0.823)	1.13	24.48 (19.12–34.06)	-0.65	0.519	0.02
P _{max} (W)	2450.6 ± 554.3	2591.6 ± 906.1	0.762 (0.536–0.887)	0.860 (0.698–0.940)	361.25	14.33 (11.19–19.93)	-1.38	0.180	0.07
F–V slope	-506.1 ± 137.3	-555.9 ± 235.2	0.481 (0.125–0.730)	0.640 (0.222–0.844)	137.99	-25.98 (-20.29 to -36.15)	1.27	0.214	0.06
MVC Angle: Mean of 30°, 60° and 90° angles									
F ₀ (N)	2193.5 ± 379.4	2556.4 ± 515.4	0.590 (-0.053–0.848)	0.740 (-0.111–0.918)	214.67	9.03 (7.05–12.57)	-5.97	0.000	0.60
V ₀ (m/s)	4.50 ± 0.83	3.74 ± 1.01	0.449 (-0.021–0.739)	0.620 (-0.044–0.850)	0.59	14.36 (11.21–19.97)	4.53	0.000	0.46
P _{max} (W)	2450.7 ± 554.3	2345.0 ± 594.3	0.918 (0.797–0.965)	0.950 (0.887–0.982)	150.97	6.30 (4.92–8.76)	2.47	0.021	0.20
F–V slope	-506.1 ± 137.3	-734.2 ± 251.8	0.339 (-0.098–0.671)	0.500 (-0.217–0.803)	136.51	-22.01 (-17.19 to -30.62)	5.91	0.000	0.59

Table 3. Validity of the Jump-MVC method for assessment of the force–velocity profile in countermovement jump. F₀—maximal isometric force; V₀—maximal theoretical velocity; P_{max}—maximal power; MVC—maximal voluntary contraction; ICCs—single measures intra-class correlation coefficient; ICCa—average measures intra-class correlation coefficient; SEM—standard error of measurement; CV%—coefficient of variation; ES—Effect size (Cohen's d); Note that for the two-point methods, the F₀ is the actual maximal isometric force (i.e. recorded during maximal voluntary contraction).

According to the OLP regression analysis, proportional bias was present for F–V slope (regardless of the knee angle data for Jump-MVC method) for both jumps (Fig. 4). Moreover, V₀ was most consistently found to exhibit proportional bias (Fig. 4). For both SJ and CMJ, fixed bias was found only of F–V slopes (Fig. 4).

Discussion

The purpose of this study was to explore the validity of the novel Jump-MVC method for assessment of jumping F–V profile and associated parameters. In contrast to previous two-point methods, which are based on distal loads, we used a combination of bodyweight jumps and isometric MVC tasks to compute F–V profiles. This novel approach, which used bodyweight jump and isometric MVC, did not prove as a valid method for F–V profiling for jumping tasks, except for the estimation of P_{max}. Specifically, most jumping F–V profile parameters, derived using the Jump-MVC method, had poor to fair agreement with the multiple-point method, while also presenting significant systematic and proportional bias. In contrast, excellent validity of slightly modified version of the two-point method that was assessed by Garcia-Ramos and colleagues²⁷ was confirmed by our results.

In principle, the linearity of the F–V curve should span from isometric contractions (during which F₀ is generated) to high velocity movements, such as bodyweight jumping, and likely beyond¹⁶. The linear F–V relationships for both jumps in our study were strong ($r = -0.95$). Some authors have suggested that F–V relationship during single-joint isokinetic tasks might be slightly curvilinear³⁹. If this is also the case with multi-joint movements, the overestimation of the maximal isometric force in our study could be partially attributed to non-linearity of the F–V relationship near the zero velocity. However, this is obscured by substantially different force values recorded at different knee angle conditions. Unfortunately, previous studies have rarely used isometric contractions for F–V

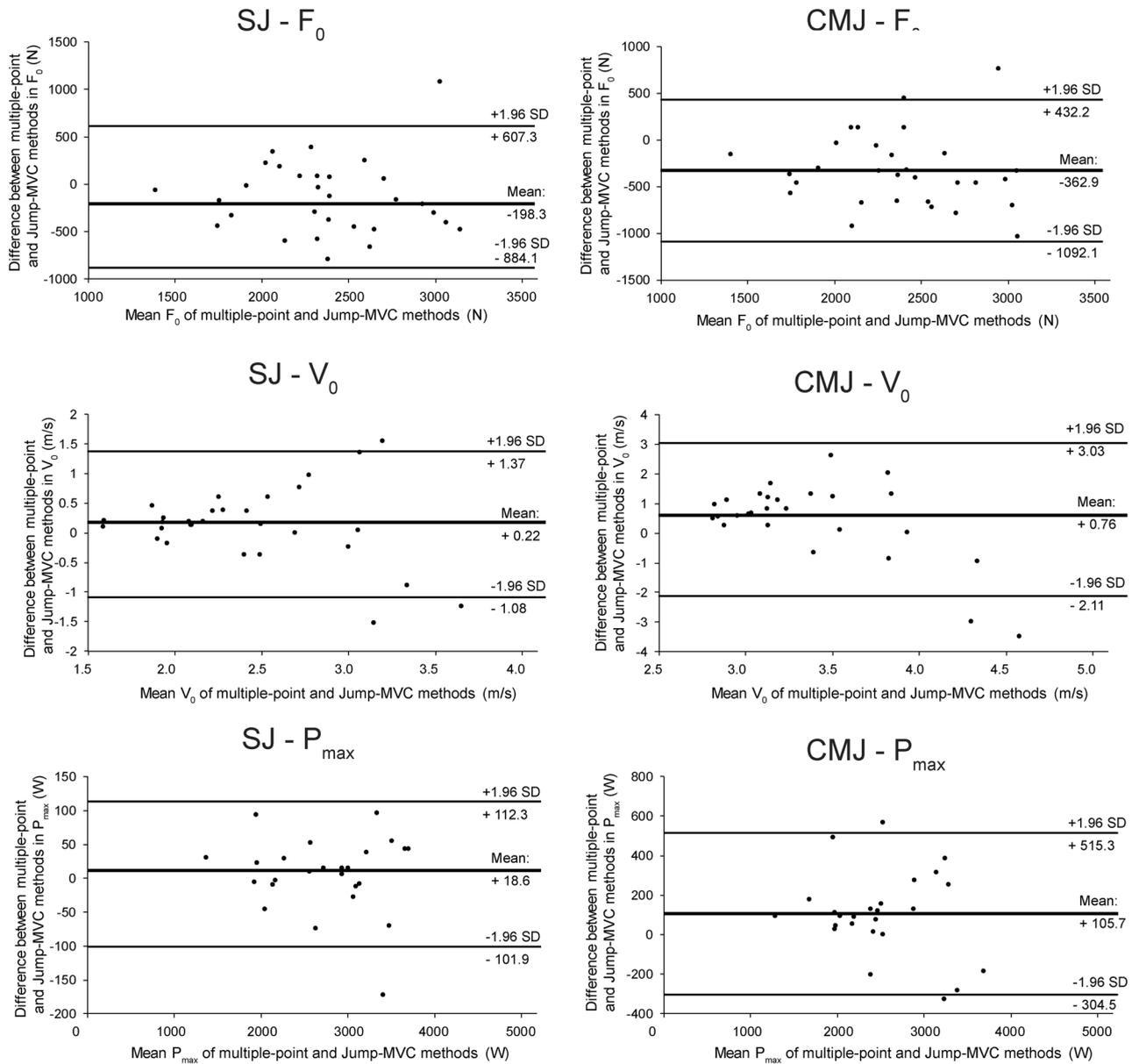


Figure 3. Bland–Altman plots of agreement between multiple-point method and Jump-MVC method, using mean force data from the 30, 60 and 90° angles. SJ—Squat jump, CMJ—countermovement jump, F_0 —maximal force, V_0 —theoretical maximal velocity, P_{max} —maximal power, SD—standard deviation.

profiling or comparison of predicted and measured F_0 . There is some evidence that a force plateau is observed when approaching zero velocity in single-joint isokinetic movement⁴⁰, however, this is in contrast with our results and does not explain the inaccuracies of the method we used for F - V profiling. A recent study demonstrated good fit of 1RM (repetition maximum) force during half-squat task to squat jump F - V profile⁴¹. The 1RM force was lower (~5%) than predicted from F - V relationship, but this discrepancy was much smaller than what we observed in our study. However, the 1RM task in the former study did not involve purely isometric conditions (mean vertical velocity: 0.22 m/s). Using 1RM task instead of a jump with high load might therefore be possible instead of using purely isometric MVC. Meanwhile, the reason behind poor agreement between predicted F_0 and isometric MVC force remains unknown. Possibly, reduced demands for maintaining stability allowed the participants to exert larger forces than they would do in unstable conditions, such as jumping with high loads. It remains unknown whether different methods for isometric MVC measurement would yield different results, for instance, using climbing harness secured to the floor by straps.

It seems that isolating the MVC force recordings to one angle or combination of angles does not provide a reliable estimation of the force capacity through the entire push-off phase, although the validity of the F_0 estimation was good for SJ if the mean force data from all three angles was used. Perhaps, including more angles and selecting among those would improve the outcomes. Given that F_0 during SJ was overestimated when MVC was performed with 30° or 60° knee angle, but underestimated when 90° knee angle was used, there is a possibility

plots indicate that the largest disagreements between multiple-point and Jump-MVC methods are present for participants with highest F_0 and V_0 values.

In addition to improving two-point method with isometric tasks, future research should consider exploring whether the two-point methods could be reliably performed outside laboratory settings (i.e. using jumping mats or smartphone applications that enable calculation of jump height from flight time). It has been confirmed that an alternative multiple-point method (commonly referred to as Samozino's method), which involves computing the F–V profile using jump heights calculated from flight times, is valid and reliable³⁶. Recently, good reliability and validity was also confirmed for the two-point method using this approach³¹. This method currently appears as the best alternative to the standard force plate measurements in terms of time efficiency, fatigue avoidance and safety. The interest of various two-point methods for F–V profiling is rapidly increasing for other movements as well, with important methodological advances recently being made for cycling³⁵ and bench press exercise⁴⁵.

Several limitations of the present study should be acknowledged. The sample of participants were comprised of athletes and active individuals. It is possible that the reliability of the two-point methods is population specific. Moreover, while sufficient rest was provided between jumping tasks, it cannot be excluded that fatigue has compromised the performance when the loads were highest (the load was gradually increased in our study). It should be also noted that we did not randomize the order of loads, and we cannot exclude the possibility that this could affect the results of our study. Furthermore, while knee angle was strictly standardized, trunk and ankle position were not. Possibly, more rigorous standardization of the task could affect the outcome of the study. Although the straps were very strongly fixated and never yielded during the experiments, it could have been that the participants were uncomfortable with the MVC task and did not produce their maximal effort. Finally, there was a high between-participant variation in jumping ability, mirrored in bodyweight jump height, as well as the highest load that they performed the jumps with. This could have had an important effect on the outcomes of statistical analyses, as some of the used measures, notably the ICC⁴⁶, are sensitive to the sample heterogeneity. Moreover, many participants were not familiar with vertical jumping testing. Although familiarization trials were provided for both jump types, we cannot exclude the possibility that a certain degree of errors in our study occurred as a consequence non-familiarity with the tasks.

Conclusion

This study explored the validity of the original and the novel Jump-MVC two-point methods for assessment of F–V profile during jumping. While the excellent validity of a two-point method was confirmed, the novel approach, using bodyweight jump and isometric task proved to have poor to fair validity. Therefore, the two-point method using distal loads is currently the best option for F–V profiling of vertical jumps. Further research should explore different simplifications of the F–V profiling protocols and the feasibility of on-field testing alternatives.

Consent for publication

The participant displayed on Fig. 1 has provided written informed to publish his image alongside the manuscript.

Received: 16 January 2020; Accepted: 5 October 2020

Published online: 05 November 2020

References

- Meylan, C. *et al.* Single-leg lateral, horizontal, and vertical jump assessment: reliability, interrelationships, and ability to predict sprint and change-of-direction performance. *J. Strength Cond. Res.* **23**, 1140–1147 (2009).
- Rodríguez-Rosell, D., Mora-Custodio, R., Franco-Márquez, E., Yáñez-García, J. M. & González-Badillo, J. J. Traditional vs. sport-specific vertical jump tests. *J. Strength Cond. Res.* **31**, 196–206 (2017).
- Loturco, I. *et al.* Performance changes and relationship between vertical jump measures and actual sprint performance in elite sprinters with visual impairment throughout a Parapan American games training season. *Front. Physiol.* **6**, 323 (2015).
- Henry, G. J., Dawson, B., Lay, B. S. & Young, W. B. Relationships between reactive agility movement time and unilateral vertical, horizontal, and lateral jumps. *J. strength Cond. Res.* **30**, 2514–2521 (2016).
- Barnes, J. L. *et al.* Relationship of jumping and agility performance in female volleyball athletes. *J. Strength Cond. Res.* **21**, 1192 (2007).
- Cordova, M. L. & Armstrong, C. W. Reliability of ground reaction forces during a vertical jump: implications for functional strength assessment. *J. Athl. Train.* **31**, 342–345 (1996).
- Cormack, S. J., Newton, R. U., McGuigan, M. R. & Doyle, T. L. A. Reliability of measures obtained during single and repeated countermovement jumps. *Int. J. Sports Physiol. Perform.* **3**, 131–144 (2008).
- Moir, G. L., Garcia, A. & Dwyer, G. B. Intersession reliability of kinematic and kinetic variables during vertical jumps in men and women. *Int. J. Sports Physiol. Perform.* **4**, 317–330 (2009).
- Moir, G., Shastri, P. & Connaboy, C. Intersession reliability of vertical jump height in women and men. *J. Strength Cond. Res.* **22**, 1779–1784 (2008).
- Thomas, C., DosSantos, T., Comfort, P. & Jones, P. Between-session reliability of common strength- and power-related measures in adolescent athletes. *Sports* **5**, 15 (2017).
- Pueo, B., Lipinska, P., Jiménez-Olmedo, J. M., Zmijewski, P. & Hopkins, W. G. Accuracy of jump-mat systems for measuring jump height. *Int. J. Sports Physiol. Perform.* **12**, 959–963 (2017).
- Buckthorpe, M., Morris, J. & Folland, J. P. Validity of vertical jump measurement devices. *J. Sports Sci.* **30**, 63–69 (2012).
- Pueo, B., Jimenez-Olmedo, J. M., Lipinska, P., Buško, K. & Penichet-Tomas, A. Concurrent validity and reliability of proprietary and open-source jump mat systems for the assessment of vertical jumps in sport sciences. *Acta Bioeng. Biomech.* **20**, 51–57 (2018).
- García-Ramos, A. & Jaric, S. Two-point method: A quick and fatigue-free procedure for assessment of muscle mechanical capacities and the 1 repetition maximum. *Strength Cond. J.* **40**, 54–66 (2018).
- Jaric, S. Two-load method for distinguishing between muscle force, velocity, and power-producing capacities. *Sport. Med.* **46**, 1585–1589 (2016).
- Cuk, I. *et al.* Force–velocity relationship of leg extensors obtained from loaded and unloaded vertical jumps. *Eur. J. Appl. Physiol.* **114**, 1703–1714 (2014).

17. Cuk, I. *et al.* Force–velocity property of leg muscles in individuals of different level of physical fitness. *Sport. Biomech.* **15**, 207–219 (2016).
18. Morin, J.-B. & Samozino, P. Interpreting power–force–velocity profiles for individualized and specific training. *Int. J. Sports Physiol. Perform.* **11**, 267–272 (2016).
19. Jiménez-Reyes, P., Samozino, P., Brughelli, M. & Morin, J.-B. Effectiveness of an individualized training based on force–velocity profiling during jumping. *Front. Physiol.* **7**, 677 (2017).
20. Nikolaidis, P. T., Rosemann, T. & Knechtle, B. Force–velocity characteristics, muscle strength, and flexibility in female recreational marathon runners. *Front. Physiol.* **9**, 1563 (2018).
21. Feeney, D., Stanhope, S. J., Kaminski, T. W., Machi, A. & Jaric, S. Loaded vertical jumping: Force-velocity relationship, work, and power. *J. Appl. Biomech.* **32**, 120–127 (2016).
22. Jaric, S. Force-velocity relationship of muscles performing multi-joint maximum performance tasks. *Int. J. Sports Med.* **36**, 699–704 (2015).
23. Iglesias-Soler, E. *et al.* Changes in the force-velocity mechanical profile after short resistance training programs differing in set configurations. *J. Appl. Biomech.* **33**, 144–152 (2017).
24. Giroux, C., Rabita, G., Chollet, D. & Guilhem, G. Optimal balance between force and velocity differs among world-class athletes. *J. Appl. Biomech.* **32**, 59–68 (2016).
25. Samozino, P., Rejc, E., di Prampero, P. E., Belli, A. & Morin, J.-B. Optimal force–velocity profile in ballistic movements—altius. *Med. Sci. Sport. Exerc.* **44**, 313–322 (2012).
26. García-Ramos, A., Pérez-Castilla, A. & Jaric, S. Optimisation of applied loads when using the two-point method for assessing the force-velocity relationship during vertical jumps. *Sport. Biomech.* <https://doi.org/10.1080/14763141.2018.1545044> (2018).
27. Zivkovic, M. Z., Djuric, S., Cuk, I., Suzovic, D. & Jaric, S. A simple method for assessment of muscle force, velocity, and power producing capacities from functional movement tasks. *J. Sports Sci.* **35**, 1287–1293 (2017).
28. Cappelz, A. Compressive loads in the lumbar vertebral column during normal level walking. *J. Orthop. Res.* **1**, 292–301 (1984).
29. Keogh, J., Hume, P. A. & Pearson, S. Retrospective injury epidemiology of one hundred one competitive oceaania power lifters: The effects of age, body mass, competitive standard, and gender. *J. Strength Cond. Res.* **20**, 672–681 (2006).
30. Faigenbaum, A. D., Myer, G. D., Naclerio, F. & Casas, A. A. Injury trends and prevention in youth resistance training. *Strength Cond. J.* **33**, 36–41 (2011).
31. Janicijevic, D. *et al.* Assessment of the force-velocity relationship during vertical jumps: influence of the starting position, analysis procedures and number of loads. *Eur. J. Sport Sci.* <https://doi.org/10.1080/17461391.2019.1645886> (2019).
32. Janicijevic, D. *et al.* The force–velocity relationship obtained during the squat jump exercise is meaningfully influenced by the initial knee angle. *Sport. Biomech.* <https://doi.org/10.1080/14763141.2020.1727559> (2020).
33. Pérez-Castilla, A., Rojas, F. J., Gómez-Martínez, F. & García-Ramos, A. Vertical jump performance is affected by the velocity and depth of the countermovement. *Sport. Biomech.* <https://doi.org/10.1080/14763141.2019.1641545> (2019).
34. Hébert-Losier, K. & Beaven, C. M. The mars for squat, countermovement, and standing long jump performance analyses: Are measures reproducible?. *J. Strength Cond. Res.* **28**, 1849–1857 (2014).
35. García-Ramos, A. *et al.* Assessment of the two-point method applied in field conditions for routine testing of muscle mechanical capacities in a leg cycle ergometer. *Eur. J. Appl. Physiol.* **118**, 1877–1884 (2018).
36. Jiménez-Reyes, P. *et al.* Validity of a simple method for measuring force-velocity-power profile in countermovement jump. *Int. J. Sports Physiol. Perform.* **12**, 36–43 (2017).
37. Fleiss, J. L. *The Design and Analysis of Clinical Experiments* (Wiley, New York, 1999).
38. Ludbrook, J. Linear regression analysis for comparing two measurers or methods of measurement: But which regression?. *Clin. Exp. Pharmacol. Physiol.* **37**, 692–699 (2010).
39. Grbic, V. *et al.* A Novel two-velocity method for elaborate isokinetic testing of knee extensors. *Int. J. Sports Med.* **38**, 741–746 (2017).
40. Prietto, C. A. & Caiozzo, V. J. The in vivo force-velocity relationship of the knee flexors and extensors. *Am. J. Sports Med.* **17**, 607–611 (1989).
41. Rivière, J. R., Rossi, J., Jimenez-Reyes, P., Morin, J. B. & Samozino, P. Where does the one-repetition maximum exist on the force-velocity relationship in squat?. *Int. J. Sports Med.* **38**, 1035–1043 (2017).
42. Perez-Castilla, A. & García-Ramos, A. Evaluation of the most reliable procedure of determining jump height during the loaded countermovement jump exercise: Take-off velocity vs. flight time. *J. Strength Cond. Res.* **32**, 2025–2030 (2018).
43. Pérez-Castilla, A., McMahon, J. J., Comfort, P. & García-Ramos, A. Assessment of loaded squat jump height with a free-weight barbell and smith machine: comparison of the takeoff velocity and flight time procedures. *J. Strength Cond. Res.* **34**, 671–677 (2020).
44. Cuevas-Aburto, J., Ulloa-Díaz, D., Barboza-González, P., Chiroso-Ríos, L. J. & García-Ramos, A. The addition of very light loads into the routine testing of the bench press increases the reliability of the force-velocity relationship. *PeerJ* **6**, e5835 (2018).
45. Pérez-Castilla, A., Jaric, S., Feriche, B., Padial, P. & García-Ramos, A. Evaluation of muscle mechanical capacities through the two-load method: optimization of the load selection. *J. Strength Cond. Res.* **32**, 1245–1253 (2018).
46. Hopkins, W. G. Measures of reliability in sports medicine and science. *Sports Med.* **30**, 1–15 (2000).

Acknowledgements

The study was supported by the Slovenian Research Agency through the programme ‘Kinesiology of mono-structural, polystructural and conventional sports’ [P5-0147 (B)] and the project TELASI-PREVENT [L5-1845] (Body asymmetries as a risk factor in musculoskeletal injury development: studying aetiological mechanisms and designing corrective interventions for primary and tertiary preventive care).

Author contributions

N.S. and G.M. conceptualized the study. N.S. and Z.K. carried out the measurements. N.S., Z.K., and G.M. analyzed the data. Z.K. wrote the first manuscript draft. N.S., G.M. and Z.K. finalized the paper.

Competing interests

The authors declare no competing interests.

Additional information

Correspondence and requests for materials should be addressed to N.Š.

Reprints and permissions information is available at www.nature.com/reprints.

Publisher’s note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.



Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit <http://creativecommons.org/licenses/by/4.0/>.

© The Author(s) 2020