Association of fast ripples on intracranial EEG and outcomes after epilepsy surgery

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Abstract

Objective

To examine whether fast ripples (FRs) are an accurate marker of the epileptogenic zone, we analyzed overnight stereo-EEG recordings from 43 patients and hypothesized that FR resection ratio, maximal FR rate, and FR distribution predict postsurgical seizure outcome.

Methods

We detected FRs automatically from an overnight recording edited for artifacts and visually from a 5-minute period of slow-wave sleep. We examined primarily the accuracy of removing \geq 50% of total FR events or of channels with FRs to predict postsurgical seizure outcome (Engel class I = good, classes II–IV = poor) according to the whole-night and 5-minute analysis approaches. Secondarily, we examined the association of low overall FR rates or absence or incomplete resection of 1 dominant FR area with poor outcome.

Results

The accuracy of outcome prediction was highest (81%, 95% confidence interval [CI] 67%–92%) with the use of the FR event resection ratio and whole-night recording (vs 72%, 95% CI 56%–85%, for the visual 5-minute approach). Absence of channels with FR rates >6/min (p = 0.001) and absence or incomplete resection of 1 dominant FR area (p < 0.001) were associated with poor outcome.

Conclusions

FRs are accurate in predicting epilepsy surgery outcome at the individual level when overnight recordings are used. Absence of channels with high FR rates or absence of 1 dominant FR area is a poor prognostic factor that may reflect suboptimal spatial sampling of the epileptogenic zone or multifocality, rather than an inherently low sensitivity of FRs.

Classification of evidence

This study provides Class II evidence that FRs are accurate in predicting epilepsy surgery outcome.

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Glossary

CI = confidence interval; DOR = diagnostic odds ratio; EZ = epileptogenic zone; FR = fast ripples; HFO = high-frequency oscillation; NREM = non-REM; SEEG = stereo-EEG; SOZ = seizure onset zone.

High-frequency oscillations (HFOs) >80 Hz, divided into ripples (80–250 Hz) and fast ripples (FRs, >250 Hz), are a promising new biomarker of epilepsy.¹ FRs recorded intracranially with clinical macroelectrodes have proved to be a very specific marker of the seizure onset zone (SOZ)^{2,3} and of postsurgical seizure outcome.^{4–11} However, they are thought to have weak sensitivity^{3,6,8,9,11} because their rate of occurrence is low and they are even absent in some patients in clinical macroelectrode recordings.^{6,9,12}

Because visual HFO identification is highly time-consuming,¹³ most intracranial studies relating interictal HFOs to surgical outcome have used 3- to 20-minute segments of non-REM (NREM) sleep for HFO identification.^{4,5} The rate of HFOs varies across longer time frames according to sleep/ vigilance stage,^{14–17} medication,¹³ and seizure activity.¹⁸ Consequently, a randomly selected short epoch of NREM sleep may not be representative of the whole spectrum of FRs in all patients.¹⁸

Evaluating longer segments is currently feasible with automatic detectors.^{11,17–19} We investigated whether FRs can become a better marker of the epileptogenic zone (EZ) if we use a much longer period of intracranial EEG. We hypothesized that (1) analyzing FRs from a whole-night recording results in higher postsurgical seizure outcome prediction accuracy than analyzing a 5-minute sample of NREM sleep and that (2) absence of channels with a high FR rate or absence of 1 clear FR focus would indicate that the EZ was suboptimally sampled by the implantation scheme or was multifocal and would consequently be associated with a poor outcome.

Methods

Standard protocol approvals, registrations, and patient consents

The Montreal Neurologic Institute and Hospital Review Ethics Board approved the study protocol. Patients signed an ethics board–approved written informed consent before study participation.

Patient sample

Between January 2010 and March 2015, 102 patients underwent stereo-EEG (SEEG) at the Montreal Neurologic Institute and Hospital. The decision to perform the SEEG was exclusively clinical, and electrode locations were decided independently of this study. The inclusion criteria were as follows: (1) resective surgery after the intracranial investigation; (2) \geq 12-month postsurgical follow-up; (3) good-quality preimplantation, peri-implantation, and postsurgical brain

imaging enabling exact localization of individual electrode contacts and resection cavity; (4) \geq 5 implanted electrodes; and (5) at least 1 night (>4 hours of data free of seizures and artifacts) sampled at 2,000 Hz. We chose the 5-electrode minimum to prevent situations in which all available contacts would be included in the resection.²⁰ Forty-three patients fulfilled the inclusion criteria and were included in the analysis.

Intracerebral EEG electrodes were implanted stereotactically with an image-guided system.²¹ During intracranial EEG acquisition, we used a referential montage (an epidural parietal reference electrode contralateral to the suspected EZ), 2,000-Hz sampling frequency, and 0.3-Hz high-pass and 600-Hz low-pass-filters.

FR detection

We marked FRs using a bipolar montage. To mark FRs from the whole-night sample, we used an automatic detector²² that finds increases in the root mean square amplitude of the signal in narrow frequency bands and compares it to the background in a 5-second sliding window. A detection occurs when the root mean square amplitude in any narrow frequency band is at least 3 times larger than the background, during an interval >4 cycles of the central frequency of the band plus the effective duration of the impulse response of the narrowband filter. The detector relies first on a wideband filter (band-pass finite impulse response filters, equiripple, order 200, transition bands of 15-Hz width, pass band from 80 to 500 Hz, weighting factor 10 on the low-frequency stop band) and 5 narrowband filters in the 250- to 500-Hz range (250-285-330-380-435-500 Hz, band-pass finite impulse response filters, equiripple, order 500, transition bands of 5 Hz width, weighting factor 10 on the low-frequency stop band). The Matlab code for the automatic detector is available on request.

The analysis period began when the patient fell asleep and ended when the patient awoke in the morning. We excluded malfunctioning and extracranial channels, channels with recurrent muscle artifacts, and periods with visually detected artifacts (e.g., muscle and movement artifacts during arousals). We also excluded 5 minutes before and after focal electrographic or focal clinical seizures. In case the postictal SEEG attenuation exceeded 5 minutes or the seizures continued in series, we stopped detections 5 minutes preictally and did not resume them postictally. One reader validated visually the first 50 automatically detected FRs for each channel and patient and excluded events produced by artifacts. Hence, we did not exclude events that the validating author would not have

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marked unless they were caused by artifact. Likewise, we did not confirm whether the automatic detector detected all events marked by the human reader. We chose this approach to keep the results of the automatic detector as independent of the human reader as possible. To calculate the validated FR rate, we multiplied the automatic FR rate by the ratio of included events divided by all inspected events.

For comparison with the whole-night recording, 1 reader (blinded to resection area and outcome) marked manually a 5-minute period of NREM sleep independently of the automatic detection following the methodology of previous studies.^{13,23} The display was split vertically with a 0.5-Hz highpass filter (normal SEEG) on the left side and a 250-Hz highpass filter on the right side, with finite impulse response filters used to limit ringing. We regarded an event as an FR if it was visible on the right (250 Hz) and there was no detectable artifact in the normal SEEG. Events had to contain at least 4 consecutive oscillations to be regarded as FRs, and 2 events had to be separated by at least 2 non-HFO oscillations. We then calculated the FR rates per channel on the basis of the whole-night automatic analysis, the 5-minute visual analysis, and automatic analysis of the same 5 minutes as the visual analysis.

Classification of channels

We classified SEEG channels as channels within and outside the operated area by superimposing the electrode contact locations, derived from peri-implantation images, with postsurgical images. We considered bipolar channels removed if at least 1 of the contacts was in the resection cavity or within 5 mm of its borders on the postsurgical MRIs. We chose this 5-mm margin to account for possible sagging, coregistration error, and partial contact resection.²⁴

Surgical outcome

The decision for surgery was based on the intracranial investigation and noninvasive investigations. FR occurrence and rates were not available for the clinicians making the surgical decisions. A board-certified neurologist blinded to the FR results classified the postsurgical seizure outcome as good (Engel class I) or poor (Engel classes II–IV)²⁵ on the basis of documentation of the patients' postsurgical visits.

Statistical analysis

We performed the statistical analyses using IBM SPSS Statistics version 23.0 (IBM Corp, Armonk, NY) and Matlab version R2018b (MathWorks, Natick, MA). On the basis of the reported FR rates in normal brain areas,²⁶ we considered channels with an FR rate <0.2/min normal and discarded them from statistical analyses.

At the group level, we compared the FR resection ratio (number of FR events on removed channels divided by total number of FR events; figure 1), FR channel resection ratio (number of removed channels with FRs divided by total number of channels with FRs), and the maximal FR rate (the rate of the channel with most events) between patients with good and poor outcomes with Mann-Whitney *U* test because these variables were not normally distributed. For effect size, we used Ω , which can take values between -1 and 1 and is centered at zero; values of $|\Omega| = 0.1, 0.3$, and 0.4 are viewed as small, medium, and large effect sizes.²⁷

For our primary study question of determining the accuracy of FRs in epilepsy surgery outcome prediction at a single-patient level, we applied a 0.5 resection ratio threshold as used in previous studies^{20,23} to predict good vs poor outcome. We considered as true positive those patients with poor outcome in whom <50% of FRs or FR channels were resected or in whom no channels showed an FR rate $\geq 0.2/\min$ (and consequently no FRs or FR channels were removed in such cases), as false positive those patients with good outcome in whom <50% of FRs or FR channels were resected or no channels showed an FR rate $\geq 0.2/\min$, as false negative those patients with poor outcome in whom \geq 50% of FRs or FR channels were resected, and as true negative those patients with good outcome in whom \geq 50% of FRs or FR channels were resected. For comparison, we applied a data-driven approach and constructed receiver operating characteristic curves to find the optimal resection ratio threshold that would minimize false predictions in our sample. We calculated the accuracy, sensitivity, specificity, and positive and negative predictive values, as well as diagnostic odds ratios (DORs) including 95% confidence intervals (CIs). The *p* values from the χ^2 test were corrected for multiple comparisons with Bonferroni correction. We considered values of p < 0.05significant.

We also used receiver operating characteristic curves to investigate whether the absence of channels above a certain FR rate threshold was associated with postsurgical seizure

Figure 1 Example of calculation of FR resection ratio and FR channel resection ratio for 1 patient who became seizure-free



Seven channels had \geq 0.2/min fast ripple (FR) rate and were included in the calculations. Bars depict the number of FRs on each of the 7 channels. Dark bars represent resected channels; white bars represent nonresected channels. FR resection ratio clearly exceeds the 0.5 threshold, whereas FR channel resection ratio does not.

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outcome at the individual level (χ^2 test with corresponding DOR and 95% CI) because predefining a threshold was not possible due to lack of prior studies of this issue.

Finally, we investigated whether absence of 1 dominant FR area or its incomplete resection was associated with poor outcome (χ^2 test with corresponding DOR and 95% CI). We considered 1 dominant FR area to exist if the dominant FR channels (defined as the set of highest FR rate channels, in rank order, sufficient to reach ≥ 0.5 PR resection ratio) were confined to a continuous brain area that could be removed in a single resection. This definition included (1) neighboring channels of the same electrode, (2) ipsilateral amygdala and hippocampus, and (3) neighboring neocortical electrodes in the same lobe. On the contrary, we considered several dominant areas to exist in cases when the dominant channels were (1) in different hemispheres, (2) in the same hemisphere but different lobes (unless both were close to the border of the 2 lobes e.g., the parietotemporal area), or (3) in the same lobe but there was a nonactive electrode in between.

Data availability

Raw SEEG files supporting the findings of this study are available (from N. von Ellenrieder) on reasonable request and approval by the ethics boards of the corresponding institutions.

Results

From our initial cohort of 102 patients, 43 (25 women, age 14-55 years) fulfilled the inclusion criteria and qualified for the study (figure 2 and table 1). The postsurgical seizure outcome was good in 15 (35%) patients and poor in 28 (65%). The baseline characteristics (sex, age, age at onset), recording parameters (number of included channels or resected channels, percentage of resected channels, or length of the overnight recording), or pathology did not differ significantly between the patients with good and poor outcomes (table 2). The mean FR rate per channel did not differ significantly between the automatic and visual analysis of the 5-minute segment of NREM sleep (p = 0.069, medians shown in table 2), indicating that the automatic detector and the human reader did not differ in their sensitivity to detect events. The mean length of the analyzed whole-night epoch was 407 (SD 82) minutes per patient. During visual validation, the median of rejected events was 0.2% (interquartile range 1%) per patient. In the whole cohort, only 1 of the original 285 FR channels changed to <0.2/min after visual validation. Visual validation did not significantly affect any of the statistical results presented in the following paragraphs; therefore, we report all results using the automatic wholenight detections without correction based on visual validation.

Resection ratios and outcome

Table 2 shows the medians and interquartile ranges of FR and FR channel resection ratios derived from each analysis

Figure 2 Flowchart of study population



approach. At group level, the resection ratios were significantly higher in patients with good than poor outcome regardless of whether the analysis was based on the whole night or the automatic or visual analysis of 5 minutes of NREM sleep (table 2 provides statistics).

At the individual level, when the predefined 0.5 resection ratio threshold was used, the FR resection ratio calculated from the whole-night recording produced the lowest number of false predictions (8, accuracy 81%, 95% CI 67%–92%, figure 3, A–C). The number of false predictions could be further reduced to 6 by selecting the optimal FR resection ratio threshold of 0.6 (accuracy 86%, 95% CI 72%–95%, figure 3, A and C). Table 3 shows the accuracy, sensitivity, specificity, positive and negative predictive values, and DORs of the FR resection ratios calculated with the different analysis approaches. We excluded the FR channel resection ratio (figure 3B) from the calculations in table 3 because it clearly produced a higher number of false predictions than the FR resection ratio. Figure 3D shows how the predictive accuracy of different FR resection ratios varied between consecutive 5-minute segments. At 2 time points with ≈ 0.6 threshold, the accuracy (88%) exceeds that of the whole-night analysis but mostly remains inferior to it.

Association of FR rate and spatial extent with outcome

The whole-night maximal FR rate was associated with outcome at individual level, so that if no channel showed an FR rate >6/min, the outcome was likely to be poor (21 of 24 patients, DOR 12, 95% CI 3–55, p = 0.001, figure 4). Pathology did not explain the low FR rates because the patients with no channels showing FR rate >6/min fell into various pathology categories, including both mesial temporal and neocortical structures (table 1).

Table 1 Individual patient characteristics and results

Patient	Age/age at onset, y	Resection hemisphere/ area	Pathology	FRs removed vis/ auto 5 min/auto WN, %	Maximal FR rate in WN analysis	No. of dominant FR areas	Resection of dominant FR channels	Engel class
1	26/14	R/F	FCD (nonspecified)	100/100/100	79.2	1	All	IA
2	39/17	R/F	FCD 2B	100/98/100	7.1	1	All	IA
3	29/8	L/F	FCD 2B	13/11/65	6.6	1	All	IA
4	36/16	R/F	FCD 2A	100/87/100	25.6	1	All	IA
5	37/5	L/F	FCD 2B	4/7/17	9.1	1	None	IA
6	55/5	R/A + HC	HS	93/88/92	27.3	1	All	IA
7	43/28	L/T + A + HC	FCD 2A	54/65/68	6.5	1	Partly	IA
8	21/12	R/P	FCD 2B	100/99/99	128.6	1	All	IA
9	28/25	R/T + A	FCD 2A	71/67/—	0.1	_	_	IA
10	37/20	L/T + A + HC	NH	82/70/74	14.3	1	All	IA
11	21/5	R/T + A + HC	Gliosis	100/98/96	33.9	1	All	IA
12	27/17	L/T + A + HC	FCD 3D	100/84/84	0.9	1	All	IB
13	14/3	R/F	FCD 2B	100/81/100	1.4	1	All	IB
14	35/10	R/A + HC	FCD 2A	62/54/63	11.2	1	All	IB
15	41/26	R/A + HC	HS	19/20/17	7.0	1	None	ID
16	32/21	R/TO	FCD 2A	26/15/0	0.6	1	None	IIA
17	38/8	L/O	FCD 1B	0/1/0	18.3	1	None	IIA
18	39/8	L/T	FCD 2A	46/49/42	4.9	1	Partly	IIB
19	36/19	R/F	FCD 2A	0/45/36	0.8	2	Partly	IIB
20	26/12	L/TO	FCD (nonspecified)	71/71/34	2.0	1	None	IIB
21	26/1	L/T + A + HC	HS	0/0/0	1.6	1	None	IIB
22	29/15	L/T (prev A + HC)	FCD 2A, HS	0/0/37	0.5	1	None	IIB
23	36/27	L/T + A + HC	FCD (nonspecified), HS, gliosis	3/5/6	77.3	1	None	IIIA
24	22/17	R/F	FCD 2A	—/38/—	0.2	_	_	IIIA
25	35/30	L/T + A + HC	FCD 2A	3/3/0	7.0	1	None	IIIA
26	30/14	L/T + A + HC	HS	21/32/25	6.6	1	None	IIIA
27	33/18	L/TO	Gliosis	0/1/0	2.3	1	None	IIIA
28	26/7	L/A + HC	Gliosis	67/60/59	32.7	2	Partly	IIIB
29	31/9	L/P + I	Gliosis	100/80/100	4.5	1	All	IIIB
30	42/6	R/F	FCD 2B	0/1/3	4.2	1	None	IVA
31	43/30	L/T + A + HC	Gliosis	30/29/27	2.7	1	None	IVA
32	53/14	L/T + I	Ganglioma	0/5/0	1.4	1	None	IVA
33	36/7	L/F	FCD 2A	1/3/0	3.4	2	None	IVA
34	38/30	L/T + A + HC	Gliosis	100/57/—	0.1	_	_	IVA
35	30/21	R/F	FCD 2A	0/3/0	5.1	1	None	IVA

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Table 1 Individual patient characteristics and results (continued)

Patient	Age/age at onset, y	Resection hemisphere/ area	Pathology	FRs removed vis/ auto 5 min/auto WN, %	Maximal FR rate in WN analysis	No. of dominant FR areas	Resection of dominant FR channels	Engel class
36	22/12	R/TO	NH, FCD 2A, gliosis	66/65/45	4.3	3	Partly	IVA
37	33/10	R/F + T + A + HC	FCD 2B	94/93/95	36.9	1	All	IVB
38	25/10	R/A + HC	Gliosis	76/84/85	11.2	1	All	IVB
39	37/4	L/F	FCD 2A	100/0/—	0.1	_	_	IVB
40	23/18	L/T	FCD 2B	74/79/51	5.2	2	Partly	IVB
41	23/8	L/HC (prev T + A)	Gliosis	0/0/0	5.99	2	None	IVB
42	37/18	R/F + P	Gliosis	0/0/0	3.0	1	None	IVB
43	32/9	L/T + I	Gliosis	0/0/0	0.7	2	None	IVB

Abbreviations: A = amygdala; auto = automatic analysis; F = frontal; FCD = focal cortical dysplasia; FR = fast ripple; HC = hippocampus; HS = hippocampal sclerosis; I = insular; NH = nodular heterotopia; O = occipital; P = parietal; prev = previous surgery; T = temporal neocortical; TO = temporo-occipital; vis = visual analysis; WN = whole night; — = no channels with FR rate \geq 0.2/min.

If the FRs were confined to 1 dominant area and it was completely resected, the outcome was likely to be good (11 of 14 patients, figure 4). On the contrary, 10 of the 11 patients with >1 dominant FR area and 15 of 18 patients in whom the 1 dominant area was not completely resected had poor outcome (DOR 23, 95% CI 4–120, p < 0.001, figure 4).

Discussion

Our data from a large, single-center patient sample show that the FR resection ratio accurately predicts epilepsy surgery outcome at the individual level when whole-night recordings are used. This result agrees with a recent study demonstrating that in some patients HFOs analyzed from a short segment of NREM sleep are not representative of the whole spectrum of HFOs over longer time periods,¹⁸ unlike previously suggested.^{15,28} In addition, in the present study, the absence of channels with a high FR rate or absence of 1 dominant FR area was associated with poor outcome and likely reflects insufficient spatial sampling of the EZ. Previous studies have not addressed the issue of whether the EZ was sufficiently sampled, even though it is a key issue in intracranial EEG investigations.

HFO rates vary overnight, with highest rates in NREM sleep^{14–17,29} and highest pathologic-to-physiologic ratio during the first sleep cycle.²⁹ Although HFO studies have generally concentrated on NREM sleep due to higher number of events, events in REM sleep may be more specific to the EZ.¹⁶ In patients with multifocal seizure onset areas, independent HFO-generating areas can be active at different times, probably reflecting the changing overall epileptic activity of each area.¹⁸

In our study, the length of the analysis period affected the outcome prediction at individual level so that the wholenight approach resulted in higher accuracy than the S-minute approach. Although it would be interesting to evaluate the sleep stages separately in long recordings, we chose to concentrate on the current whole-night approach because it is easily adaptable for clinical use due to its simplicity. The automatic analysis of the artifact-edited whole-night data yielding results similar to those of the visually validated approach further increases the clinical appeal of the whole-night approach.

FRs have proven to be fairly specific to epileptogenic cortex, and FR rates in nonepileptogenic cortex are very low.²⁶ Animal studies show that, whereas ripples can represent physiologic events in mesial temporal structures closely linked to memory consolidation³⁰ and pathologic events in epilepsy models,³¹ FRs are almost exclusively pathologic and closely linked to epileptogenesis.^{32–34} In patients, the specificity of FRs to identify the SOZ^{2,3} and to predict outcome after epilepsy surgery has consistently been higher than that of ripples.^{4,5,8–11,19,35,36} In particular, if high-FR-rate channels remain untouched, the patient is unlikely to become seizure-free.^{6–8,10,11,19,36}

In our study, FRs identified the EZ also with high sensitivity. The EZ is the area of cortex that needs to be removed for seizure freedom³⁷ and is thus conceptually different from the SOZ, the area showing the first ictal changes. Many previous studies reporting low sensitivity examined channel, not patient-level, sensitivity, comparing the FR channels to the resected channels in patients with good outcome,¹¹ to the SOZ channels,² or to the epileptogenicity index zone channels.³ All of these definitions may overestimate or misestimate

Table 2 Baseline characteristics, recording parameters, pathology, FR rates, and FR channels and their resection ratios in patients with good and poor outcomes

	All (n = 43)	Engel class I (n = 15)	Engel classes II–IV (n = 28)	Engel class I vs II–IV, estimate of effect size ^a (95% CI), <i>p</i> Value
Female, n (%)	25 (58)	7 (47)	18 (64)	OR 0.5 (0.1 to 1.7), <i>p</i> = 0.27
Age, mean (SD), y	33 (8)	33 (10)	33 (7)	DM 0 (–5 to 5), <i>p</i> = 0.98
Age at onset, mean (SD), y	14 (8)	14 (8)	14 (8)	DM 0 (–5 to 5), <i>p</i> = 0.90
No. of included channels, mean (SD)	63 (20)	66 (19)	62 (21)	DM 4 (–9 to 17), <i>p</i> = 0.57
No. of resected channels, mean (SD)	12 (8)	12 (7)	12 (8)	DM 1 (–4 to 5), <i>p</i> = 0.83
Percentage of resected channels, mean (SD)	19 (10)	20 (11)	19 (10)	DM 1 (-6 to 8), <i>p</i> = 0.72
Length of the whole-night epoch, mean (SD), minutes	407 (82)	393 (74)	415 (87)	DM -22 (-76 to 31), <i>p</i> = 0.40
Pathology, n (%)				
Hippocampal sclerosis or focal cortical dysplasia type 2	29 (67)	12 (80)	17 (61)	OR 3.6 (0.6 to 11.3), <i>p</i> = 0.21
Mean FR rate per channel, median (IQR), events/min				
Visual 5 min	0.23 (0.52)	0.36 (0.51)	0.22 (0.52)	Ω 0.14 (–0.16 to 0.58), <i>p</i> = 0.25
Automatic 5 min	0.28 (0.48)	0.41 (0.67)	0.19 (0.49)	Ω 0.16 (-0.12 to 0.53), <i>p</i> = 0.26
Automatic whole night	0.20 (0.41)	0.28 (0.64)	0.16 (0.26)	Ω 0.25 (–0.10 to 0.57), <i>p</i> = 0.13
Channels with FR rate ≥0.2/min, median (IQR), n				
Visual 5 min	6 (5)	5 (2)	6.5 (8)	Ω 0.08 (-0.51 to 0.68), <i>p</i> = 0.92
Automatic 5 min	10 (5)	9 (5)	10 (7)	Ω –0.10 (–0.50 to 0.32), <i>p</i> = 0.65
Automatic whole night	6 (5)	6 (3)	5 (7)	Ω 0.24 (–0.19 to 0.67), <i>p</i> = 0.44
FR resection ratio, median (IQR)				
Visual 5 min	0.50 (0.96)	0.93 (0.46)	0.03 (0.71)	Ω 1.00 (0.08 to 1.00), <i>p</i> = 0.001
Automatic 5 min	0.45 (0.77)	0.81 (0.44)	0.10 (0.59)	Ω 0.73 (0.13 to 1.00), <i>p</i> < 0.001
Automatic whole night	0.37 (0.85)	0.88 (0.35)	0.06 (0.44)	Ω 1.00 (0.31 to 1.00), <i>p</i> < 0.001
FR channel resection ratio, median (IQR)				
Visual 5 min	0.48 (0.90)	0.60 (0.54)	0.30 (0.60)	Ω 0.59 (0.20 to 1.00), <i>p</i> = 0.003
Automatic 5 min	0.33 (0.39)	0.44 (0.17)	0.24 (0.45)	Ω 0.48 (0.13 to 0.92), <i>p</i> = 0.01
Automatic whole night	0.39 (0.63)	0.56 (0.43)	0.25 (0.52)	Ω 0.79 (0.31 to 1.00), <i>p</i> = 0.002
Maximal FR rate in the whole-night recording, median (IQR)	5.1 (9.7)	9.1 (20.8)	3.8 (5.5)	Ω 0.34 (0.06 to 0.60), <i>p</i> = 0.02

Abbreviations: CI = confidence interval; DM = difference of the means; FR = fast ripple; IQR = interquartile range; OR = odds ratio.

We used χ^2 test to compare categorical variables and Student independent-sample *t* test or Mann-Whitney *U* test, depending on normality of the data, to compare continuous variables (*p* values uncorrected). ^a As measures of effect size, we used OR for categorical variables, DM for variables following normal distribution, and Ω^{27} for variables not following normal

distribution, with 95% Cls in parentheses. The FR resection ratio and FR channel resection ratio were significantly higher in patients with good vs poor outcome, whereas there were no differences in the other listed parameters.

the EZ, consequently lowering sensitivity because many channels defined this way show no FRs.

The other few studies examining, like our study, the sensitivity of FRs at the patient level showed a large variability between them $(29\%^{19}-90\%^{20})$. This is likely due to different definitions of true and false positives and negatives, which depend on the definition of FR channels and the FR or FR channel resection ratio threshold. We calculated the predictive values

almost identically to a recent study with a comparable sample size,²⁰ yet our prediction accuracy was clearly higher (81% vs 69%). This may be explained by our longer analysis period, but in addition, our study population (age >14 years), methods of intracranial EEG registration (SEEG exclusively), and surgical procedures (sublobar resections exclusively) were more homogeneous than those of the previous study (all ages, SEEG or electrocorticography, any resection type). Our data-driven analysis showed that the optimal FR resection





(A and B) Receiver operating characteristic curves of different (A) fast ripple (FR) and (B) FR channel resection ratios in relation to outcome. Black dots correspond to the predefined 0.5 resection ratio threshold; white circle shows the point of best prediction accuracy of whole-night data, which corresponds to a 0.6 FR resection ratio threshold. (C) FR resection ratios calculated from the whole-night analysis in each patient with good vs poor outcome. Horizontal lines show the predefined 0.5 (solid line) and the optimal 0.6 (dashed line) resection ratio thresholds. Patients with no channels showing an FR rate \geq 0.2/min are displayed according to their outcome on the line marked not available (Na). (D) Outcome prediction accuracy by automatic analysis at consecutive 5-minute segments. The x-axis shows the time from sleep start; the y-axis depicts the FR resection ratio threshold; and colors show the number of incorrect predictions of 43 patients at each time point and resection ratio. Overall, outcome prediction depends on the selection of the 5-minute episode during the overnight recording. Number of incorrect predictions at an \approx 0.6 FR resection ratio. Lowest number of incorrect predictions at any single 5-minute segment is 5 (accuracy 88%). However, number of incorrect predictions of most segments remains above that of the optimal whole-night analysis (i.e., >6 incorrect predictions). Patients who had no channels with an FR rate \geq 0.2/min are included in all figures as true positive (TP; if the outcome was poor) or false positive (FP; if the outcome was good). FN = false negative; TN = true negative.

ratio threshold might be higher than the previously used 0.5. Confirming this observation remains a prospect for future studies.

Despite the good predictive accuracy of the FR resection ratio, this retrospective measure does not provide sufficient information for prospective surgical planning for 2 reasons: it does not tell whether the EZ was sampled or whether the detected FRs originate in areas outside the EZ, and it does not indicate unambiguously which channels to remove because several channel combinations can add up to \geq 50% of total FRs. Previous studies suggested that an ictal increase in HFOs³⁸ and a specific combination of changes in fast and slow activity at ictal onset, an ictal fingerprint,³⁹ would differentiate between the actual onset and propagation areas.

In accordance with our hypothesis, the absence of high FR rate channels and absence of 1 dominant FR area were

associated with a poor outcome, which we interpret as indicating in such cases that the EZ was either suboptimally sampled or was widespread. These 2 measures can be determined prospectively and hence could be used to guide surgical decisions. One might question whether the low FR rates were due to the low sensitivity of the automatic detector because we did not evaluate whether all visually marked events were detected by the detector. Conceptually, this is, however, not relevant because we defined FRs as those detected by the detector (independently of the human reader), and with such a definition, most patients with low FR rates had poor outcome. Second, even in practice, the mean FR rate per channel did not differ significantly between the automatic and visual analysis approaches, indicating that the automatic detector and the human reader did not differ in their sensitivity to detect events. The low FR rates also could not be explained by pathology because the patients with no channels showing FR rate >6/min had various

Table 3 Prediction of surgery outcome by FR resection ratio

	Visual 5 minutes, 0.5 resection ratio	Automatic 5 minutes, 0.5 resection ratio	Automatic whole night, 0.5 resection ratio	Automatic whole night, 0.6 resection ratio
TP, n	19	20	23	25
FP, n	3	3	3	3
TN, n	12	12	12	12
FN, n	9	8	5	3
Accuracy (95% Cl), %	72 (56–85)	74 (59–86)	81 (67–92)	86 (72–95)
Sensitivity (95% Cl), %	68 (48-84)	71 (51–87)	82 (63–94)	89 (72-98)
Specificity (95% Cl), %	80 (52–96)	80 (52–96)	80 (52–96)	80 (52-96)
PPV (95% CI), %	86 (69–95)	87 (70–95)	88 (73–96)	89 (75–96)
NPV (95% CI), %	57 (42–71)	60 (44–74)	71 (51–85)	80 (57–92)
DOR (95% CI)	8.4 (1.9–37.6), <i>p</i> = 0.02	10 (2.2–45.2), <i>p</i> = 0.01	18.4 (3.7–90.5), <i>p</i> = 0.001	33.3 (5.8–190.3), <i>p</i> < 0.001

Abbreviations: CI = confidence interval; DOR = diagnostic OR; FN = false negative (more than the FR ratio resected, Engel classes I–IV); FP = false positive (less than the FR ratio resected, Engel class I); NPV = negative predictive value; PPV = positive predictive value; TN = true negative (more than the FR ratio resected, Engel class I); NPV = negative predictive value; PPV = positive predictive value; TN = true negative (more than the FR ratio resected, Engel class I); TP = true positive (less than the FR ratio resected, Engel classes II–IV). When the predefined 0.5 FR resection ratio threshold (middle 3 columns) is used, the automatic whole-night analysis provides the highest accuracy.

When the predefined 0.5 FR resection ratio threshold (middle 3 columns) is used, the automatic whole-night analysis provides the highest accuracy. Increasing the resection ratio threshold to 0.6 (fourth column) further improved the accuracy of the whole-night approach. The *p* values are corrected for multiple comparisons with Bonferroni correction.

underlying pathologies involving both the mesial temporal and neocortical structures.

Contradicting our hypothesis, 3 patients had good outcome despite low FR rates. One had an ischemic lesion and a focal cortical dysplasia type 3D, and according to the SEEG report, the EZ was thought to have been slightly missed by the electrodes. The other 2 patients had a focal cortical dysplasia type 2, but neither showed the typical interictal SEEG pattern. Because FR generators are very focal,^{40,41} the low FR rate may also here reflect a suboptimal spatial sampling of the EZ, even if it was subsequently included in the resection. This hypothesis could be further supported in the future by examining FRs in patients who underwent implantation of additional electrodes in the course of the SEEG recording. Implanting additional electrodes during SEEG is, however, a rare procedure, and our cohort did not include such patients, so this issue remains a topic for future studies.

If the dominant FR channels were confined to 1 area and removed completely, the outcome was usually good, whereas if they remained untouched, the outcome was usually poor. For prospective surgical planning, this means that if the majority of FRs originate from 1 continuous area, one should consider including this area in the resection. However, this measure is not perfect; 2 patients achieved good outcome even though the dominant FR channels, located in the mesial temporal structures in both cases, remained untouched. A previous study also found interictal FRs bitemporally in patients with temporal lobe epilepsy with unilateral seizure generator and seizure-free outcome after surgery.⁴² The explanation may be a postsurgical decrease of the unresected mesial temporal FRs because in intraoperative electrocorticography the FRs remaining in the postresection recording^{6,7} provide the best prediction of seizure recurrence, not the percentage of removed preresection FRs.⁷

Because we counted each FR on each channel as a separate event, both the FR resection ratio and the definition of dominant FR area depended on the number of contacts sampling each area producing FRs. Hence, these measures can give only an approximation of the FR area and extension of its resection. However, such simple measures are practical, and recent data showing that removing the high-rate channels is as good for outcome prediction as removing the first source channels of HFO networks⁴³ also support their use.

Figure	4	Association	of	the	maximal	FR	rate	and	spatial
		extent of FR	s v	vith	outcome				

Number of dominant FR areas	1	≥2	0 (no channels ≥0.2)
Good	00		-
Poor	0000□□□□□□□□□=●●■		

Each shape corresponds to 1 patient. Circles indicate patients with at least 1 channel with fast ripple (FR) rates >6/min; squares indicate patients without channels showing FR rates >6/min. The fill of the shape shows the completeness of dominant FR channel resection: black = complete, gray = partial (or no channels with FR rate $\geq 0.2/min$), white = none resected.

We excluded data 5 minutes preictally and postictally of short focal seizures, whereas most studies selected epochs at least 2 hours from any seizure. However, HFO rates increase only within seconds,^{44,45} not minutes, preceding seizure onset.^{44,46} To the best of our knowledge, no study has systematically examined the rate of HFOs immediately or shortly postictally. Although this could be seen as a limitation of our study, at the same time, it demonstrates the robustness of the whole-night approach and expands its use to patients with multiple nocturnal seizures.

Our results show that at the individual level the sensitivity of FRs may not be as poor as previously suggested because the absence of high-FR-rate channels was associated with a poor surgical outcome, probably indicating a suboptimal spatial sampling of the EZ rather than inherently low sensitivity of FRs. Our results do not contradict previous claims that FRs cannot define the entire EZ.³ They suggest that FRs mark the core of the EZ and, consequently, that the absence of high-FR-rate channels or 1 dominant FR area presents a red flag that the EZ is suboptimally sampled or may be multifocal. We also show that using a long analysis duration tends to result in more accurate outcome prediction.

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Disclosure

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Appendix Authors

Name	Location	Contribution
Päivi Nevalainen, MD, PhD	Montreal Neurologic Institute and Hospital, McGill University, Quebec, Canada	Design and conceptualization of the study; analysis and interpretation of the data; statistical analysis; drafting the manuscript for intellectual content

Appendix (continued)					
Name	Location	Contribution			
Nicolás von Ellenrieder, PhD	Montreal Neurologic Institute and Hospital, McGill University, Quebec, Canada	Design and conceptualization of the study; analysis and interpretation of the data; statistical analysis; revising the manuscript for intellectual content			
Petr Klimeš, PhD	Montreal Neurologic Institute and Hospital, McGill University, Quebec, Canada	Acquisition and analysis the data; revising the manuscript for intellectual content			
François Dubeau, MD	Montreal Neurologic Institute and Hospital, McGill University, Quebec, Canada	Interpretation of the data; revising the manuscript for intellectual content			
Birgit Frauscher, MD	Montreal Neurologic Institute and Hospital, McGill University, Quebec, Canada	Analysis and interpretation of the data; revising the manuscript for intellectual content			
Jean Gotman, PhD	Montreal Neurologic Institute and Hospital, McGill University, Quebec, Canada	Design and conceptualization of the study; interpretation of the data; revising the manuscript for intellectual content			

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