



Article

Gold Nanopeanuts as Prospective Support for Cisplatin in Glioblastoma Nano-Chemo-Radiotherapy

Joanna Depciuch ^{1,*}, Justyna Miszczyk ¹, Alexey Maximenko ¹, Piotr M. Zielinski ¹,
Kamila Rawojc ², Agnieszka Panek ¹, Pawel Olko ^{1,†} and Magdalena Parlinska-Wojtan ^{1,†}

¹ Institute of Nuclear Physics Polish Academy of Sciences, 31-342 Krakow, Poland; justyna.miszczyk@ifj.edu.pl (J.M.); alexey.a.maximenko@gmail.com (A.M.); piotr.m.zielinski@ifj.edu.pl (P.M.Z.); agnieszka.panek@ifj.edu.pl (A.P.); pawel.olko@ifj.edu.pl (P.O.); magdalena.parlinska@ifj.edu.pl (M.P.-W.)

² Nuclear Medicine Unit, Department of Endocrinology, The University Hospital, 31-501 Krakow, Poland; k.rawojc@gmail.com

* Correspondence: joanna.depciuch@ifj.edu.pl

† Equal contribution as senior authors.

Received: 30 September 2020; Accepted: 25 November 2020; Published: 29 November 2020



Abstract: Herein, we propose newly designed and synthesized gold nanopeanuts (Au NPs) as supports for cisplatin (cPt) immobilization, dedicated to combined glioblastoma nano-chemo-radiotherapy. Au NPs offer a large active surface, which can be used for drugs immobilization. Transmission electron microscopy (TEM) revealed that the size of the synthesized Au NPs along the longitudinal axis is ~60 nm, while along the transverse axis ~20 nm. Raman, thermogravimetric analysis (TGA) and differential scanning calorimetry (DSC) measurements showed, that the created nanosystem is stable up to a temperature of 110 °C. MTT assay revealed, that the highest cell mortality was observed for cell lines subjected to nano-chemo-radiotherapy (20–55%). Hence, Au NPs with immobilized cPt (cPt@AuNPs) are a promising nanosystem to improve the therapeutic efficiency of combined nano-chemo-radiotherapy.

Keywords: gold nanopeanuts; new shape; support; biomedical application

1. Introduction

Glioblastoma multiforme (GBM) is one of the most common and aggressive malignant brain tumors [1,2]. In GBM treatment, surgery, chemotherapy and radiotherapy are used [1]. Unfortunately, due to the location of tumor cells close to the brain and complex character of the tumor, categorized clinically into four different grades, GBM exhibits a poor prognosis and high rates of recurrence [1,3]. Radiation oncologists put in a lot of efforts to preferentially sensitize tumors to radiation, while minimizing effects in normal tissues and critical organs. One of the possibilities is the introduction of high-atomic number (Z) materials into the tumor cells [4]. One of the candidates can be gold, as it has a high atomic number and a high mass energy coefficient [5]. Moreover, the development of nanotechnology allows synthesizing differently shaped gold nanoparticles having such dimensions, which will allow them to accumulate in cancer tissue, due to the leaky intra-tumoral blood vessels and poorly formed intra-tumoral lymphatics [6–11]. Furthermore, gold nanoparticles are biocompatible, therefore they can be used as drug carriers [12]. Thus, a nanosystem can be created by immobilizing chemotherapeutic drugs molecules on the surface of gold nanoparticles (Au NPs), which can be used in combined nano-chemo-radiotherapy being a promising, revolutionary approach for the treatment of cancer [13,14]. The drugs, which are generally used in cancer treatment are cisplatin

(cPt) or other platinate derivatives. The effects of cPt involve creating crosslinks between adjacent and within the same DNA strands. The formation of these crosslinks prevents DNA replication and cell division [15,16]. Unfortunately, chemotherapeutic drugs cause neurotoxicity, nephrotoxicity and ototoxicity effects in normal cells [17]. Over the years, different methods to reduce diverse side effects have been investigated [18,19]. The nanosystem (Au NPs + cPt) can be very effective, because its size will allow a direct delivery of the drug only to the cancer cells, which have a different morphology of blood vessels compared to healthy cells [20,21].

Currently, the most effective therapy against glioblastoma treatment is radiotherapy. The efficiency of this therapy is recognized as satisfactory, however, side effects are devastating for the organism, resulting in a poor condition of the patients after the treatment [22]. Therefore, scientists are working to continuously improve the success of radiotherapy with a simultaneous reduction of side effects, e.g., by combining it with conventional chemotherapy or, in recent years, with the addition of nanoparticles (NPs) like gold [23,24]. Consequently, herein we propose a combined nano-chemo-radiotherapy treatment for glioblastoma cell lines. For this purpose, we designed a new nanosystem consisting of gold nanopeanuts (Au NPes) with cisplatin immobilized on their surface, which will be added into the glioblastoma cells and subsequently treated by radiotherapy [25]. The peanut-like shape of the Au NPs was designed in a way to obtain a larger active surface but keep the cytotoxicity of the NPs as low as for spherical NPs.

2. Results

2.1. Characterization of NPs

The bright field scanning transmission electron microscopy (BF STEM) image of the Au NPes is shown in Figure 1a. Indeed, the synthesized Au NPes have a peanut-like shape with nicely rounded edges, as expected in the design process. The size of the obtained NPes is ~60 nm along the longitudinal axis, while along the transverse axis ~20 nm. The information about the structure of the synthesized nanoparticles was acquired using X-ray diffraction (Figure 1d). The XRD pattern of the Au NPes was refined with the Rietveld method as shown in Figure 1d. Within the detection limit, all peaks could be attributed to standard Bragg reflections (111), (200), (220), (311) and (222) of Au nanocrystals with a face-centered cubic lattice [26,27], and the calculated cell parameter of the Au nanopeanuts was equal to 4.078 Å with uncertainties of ~0.001 Å. The average crystallite size of the Au NPes, estimated in the framework of micro-structural analysis from Fullprof, was around 18 nm and corresponded nicely to the size of Au NPes along the transverse axis determined by TEM.

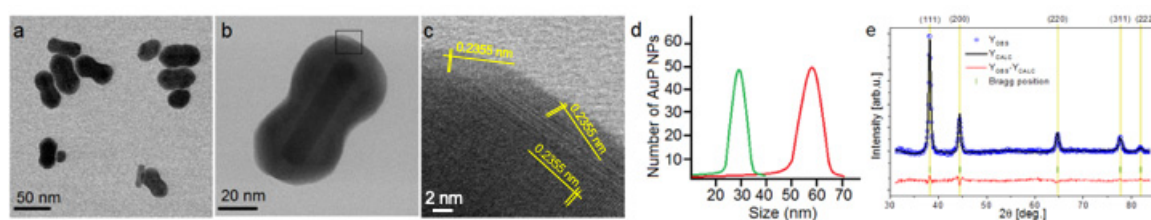


Figure 1. Overview BF STEM (a,b); HRSTEM image with indicated lattice distances of Au corresponding to the {111} planes. (c), size distribution of longitudinal (red curve) and transverse (green curve) axis (d) and XRD (e) taken for Au NPes. Experimental (blue dots) and calculated (solid black line) Rietveld refinement plot of the XRD pattern for the Au NPes. The red line (YOBS—YCALC) represents the difference between the observed and calculated data. Tick marks show allowed Bragg reflections (color online).

2.2. Verification of Success of Functionalization and cPt Immobilization Process

In this study, we show a successful functionalization of Au NPes, which is very important for an effective delivery of the drug to the cancer cells. Raman spectra of the four samples i.e., cisplatin

(Figure 2a, black spectrum), the pure MHDA (Figure 2a, orange spectrum), the Au NPs + MHDA (Figure 2a, blue spectrum), and the cPt@Au NPes (Figure 2a, pink spectrum) were acquired. In the Raman spectrum of the MHDA sample, a peak of the thiol group ($-SH$) at 2900 cm^{-1} is visible [28]. The disappearance of this peak in the functionalized and cPt containing nanoparticle samples confirms a successful attachment of the MHDA to the surface of gold nanoparticles. Moreover, in the Raman spectrum of cPt@Au NPes (Figure 2a, pink spectrum) a peak corresponding to the $C=O$ vibrations (1680 cm^{-1}) is observed [28]. This group is responsible for linking cPt with the functionalizing surfactants on the Au NPs surface [29]. Both observations provide the evidence on the success of Au NPes functionalization and cPt immobilization.

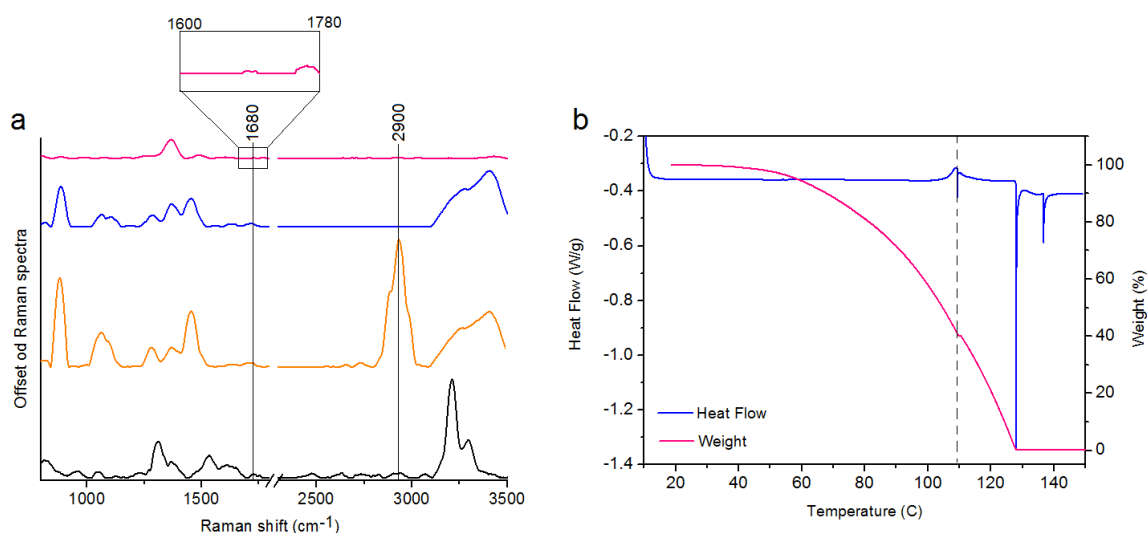


Figure 2. Raman spectra of: cPt (spectrum black), the pure MHDA (spectrum orange), the Au NPs + MHDA (spectrum blue), cPt@Au NPes (spectrum pink) (a); TGA and DSC data of cPt@Au NPes showing the solvent removal and decomposition of the product (b).

The results of TGA and DSC experiments, indicate that the cPt@Au NPes sample remains thermally stable up to $100\text{ }^{\circ}\text{C}$ at a $5\text{ }^{\circ}\text{C min}^{-1}$ heating rate, Figure 2b. The shape of the TGA signal points towards a strong evaporation of the solvent from the liquid sample visible between ca. $68\text{ }^{\circ}\text{C}$ (5% weight loss) and $119\text{ }^{\circ}\text{C}$ (59.7% weight loss), followed by its chemical decomposition from ca. $120\text{ }^{\circ}\text{C}$ to $138\text{ }^{\circ}\text{C}$ (40.03% weight loss). The DSC thermogram shows no signs of any significant thermal anomalies up to $110\text{ }^{\circ}\text{C}$. The anomalies registered above that temperature, as well as the baseline shift are effects of rapid boiling and decomposition of the sample or destabilization of MHDA [30]. However, in this experiment the stability of the nanosystem in the temperature range between $20\text{ }^{\circ}\text{C}$ and $40\text{ }^{\circ}\text{C}$ (room temperature–body temperature) is the most important.

2.3. Impact of Studied Nano-Chemo-Radiotherapy Approach on Cell Viability

Figure 3 shows the viability of the control and the non-irradiated U118 MG (Figure 3a) and U251 MG (Figure 3b) cell lines incubated with cPt, Au NPes or cPt@Au NPes for 3, 6, 24 and 48 h. The MTT assay showed a slight, but continuous decreasing in the viability of the treated cell lines with increasing incubation time for all investigated samples. The differences in viability observed between the two studied cell lines might be explained by the large degree of heterogeneity found in tumors [31]. The addition of cPt resulted in 1–15% mortality, depending on the cell line and incubation time. The most prominent effects in cell killing were observed for Au NPes and cPt@Au NPes. Studies show that nanoparticles can easily cross or interact with the cell membranes inducing antiproliferative activity and consequently cell death [32]. Interestingly, the addition of cPt@Au NPes caused a gradual decrease of cell viability, varying from 72–75% for 3h incubation to 44–53% for cell lines incubated for 48 h. However, significant differences between the addition of Au NPes vs. cPt@Au NPes were observed only for the U 251 MG cell line ($p < 0.05$). Au NPes coupled with cPt better inhibit the

growth of GBM cells compared to free cisplatin and spherical Au NPs with attached cPt [33]. It could be due to the larger active surface of gold nanopeanuts compared to spherical Au NPs, which allow for the attachment of a higher density of cPt. Consequently, the local concentration of the drug in the tumor can be much higher, then when cPt is administered intravenously. As already mentioned, the main advantage of the nanopeanuts is their shape, until now not described in literature. They can be compared to nanorods, which have sharper ends, and are thus more cytotoxic, than spherical Au NPs. In another work [34], the authors show that a concentration of 0.5×10^{-6} mg/mL is sufficient to cause a 20% mortality of cancer cells, while a concentration of 2.93×10^{-6} mg/mL of NPs has to be added to cancer cells to cause the same mortality effect. This is most probably due to the rounded ends of the nanopeanuts, having a similar shape to spherical nanoparticles, known for their lowest cytotoxic properties [35].

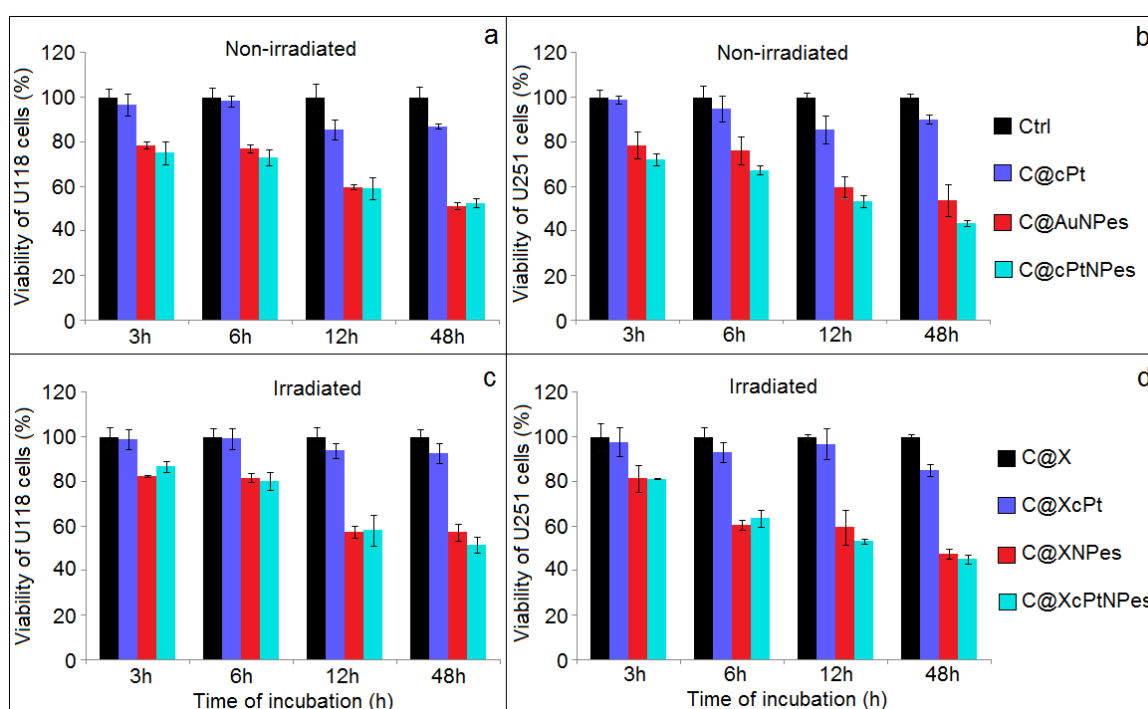


Figure 3. Comparison of the viability of U118 MG and U251 MG cell lines determined via the MTT assays in not-irradiated (a,b) and irradiated (c,d) cells by 2 Gy of X-rays after different time of incubation (3, 6, 24 and 48 h) with cisplatin, Au NPs and cPt@Au NPs and compared with controls.

Irradiating with 2 Gy X-ray dose resulted in a gradual decrease of cell viability for both cell lines cultured with cPt, Au NPs or cPt@Au NPs as a function of incubation time after irradiation (Figure 3c,d). cPt@Au NPs were more efficient in inducing the U118 MG cell killing compared to Au NPs, which is evidenced by a significant decrease in the viability measured 48 h after irradiation ($p < 0.05$). Numerous factors, in addition to the genetic status mentioned above, have shown to influence the response of gliomas after radiotherapy [36]. The observed differences may be caused by inherent cellular radiation sensitivity between studied cell lines, the mechanism of radiation damage repair and the status of proliferation rates [37]. Independently on the culture additive (cPt, Au NPs or cPt@Au NPs), the cell mortality was higher with X-ray irradiation than without. Summarizing, for both cell lines the highest mortality was observed for combined nano-chemo-radiotherapy approach using the cPt immobilized on nanopeanuts nanosystem, rather than radiotherapy or chemotherapy alone. However, these differences are significant when we compare these results with C@XNPes cells.

Moreover, we also studied using FT-Raman and Fourier Transform InfraRed (FTIR) spectroscopy, the chemical changes in cells caused by cPt, Au NPs, cPt@Au NPs in combination with and

without X-ray irradiation. The results of these experiments are presented in supplementary material (Figure S1–S3, Table S1).

3. Materials and Methods

3.1. Materials

Cetrimonium bromide (CTAB), chloroauric acid tetrahydrate (HAuCl_4), silver nitrate (AgNO_3), sodium borohydride (NaBH_4), sodium citrate ($\text{Na}_3\text{C}_6\text{H}_5\text{O}_7$), L-ascorbic acid ($\text{C}_6\text{H}_8\text{O}_6$), 16—mercaptohexadecanoic acid (MHDA), dimethylformamide (DMF), pentafluorophenyl (PFP), *N*, *N*-diisopropylethylamine (DIPEA), *N*-cyclohexyl-*N'*-(2-morpholinoethyl) carbodiimide metho-*p*-toluenesulfonate (CMC) and all other chemicals were purchased from Sigma–Aldrich (Darmstadt, Germany).

3.2. Methods

3.2.1. Au Nanorods Synthesis

Synthesis of Au Nanoseeds

0.364 g of CTAB was dissolved in 5 mL of water. Next, 5 mL of solution formed by dissolving 0.0017 g chloroauric acid tetrahydrate in 10 mL of water, were added. Finally, 0.6 mL of 100×10^{-3} M sodium borohydride was added to this solution. The solution was permanently under vigorous stirring. The reaction was stopped when the solution color changed to red.

Synthesis of Au Nanopeanuts

0.364 g of CTAB was dissolved in 5 mL of water. Next, 0.2 mL of solution formed by dissolving 0.0135 g silver nitrate in 20 mL of water, was added. Subsequently, 0.0017 g chloroauric acid tetrahydrate was dissolved in 5 mL of water and was added to the solution. Finally, 70 μL of Au nanoseed solution formed by dissolving 0.1386 g L-ascorbic acid in 10 mL of water and 30 μL of Au nanoseeds were added to the previous solution.

3.2.2. Functionalization of Au NPes

In order to attach the drugs to the stabilized Au NPes 5 mM 16—mercaptohexadecanoic acid (MHDA) was added into Au NPes solutions and was incubated overnight at 4 °C. After rinsing with dimethylformamide (DMF), the MHDA-covered Au-structures were incubated in DMF solution of 20 mM pentafluorophenyl (PFP) and 20 mM *N*, *N*-diisopropylethylamine (DIPEA) and 20 mM *N*-cyclohexyl-*N'*-(2-morpholinoethyl) carbodiimide metho-*p*-toluenesulfonate (CMC), during 30 min at 25 °C. After repeated rinsing with DMF and centrifugation, the cisplatin solution was added and incubated for 30 min. at 25 °C. Consequently, the final concentration of cPt in the NPes surface was 1.71×10^3 cPt molecules per one nanopeanut. In the immobilization process, an amide group is responsible for the coupling of COOH from MHDA with NH_3 from cisplatin by covalent bond. The scheme of functionalization Au NPes is shown in Figure 4.

3.2.3. TEM Characterization

The synthesized nanoparticles were imaged using transmission electron microscopy (TEM) using the high-angle annular dark field detector (HAADF) in the scanning mode. The observations were executed on an aberration-corrected FEI Titan electron microscope equipped with a FEG cathode working at 300 kV. To evaluate the particle size distribution, the diameter of 100 nanoparticles was measured on HRSTEM images acquired at different areas of TEM grids.

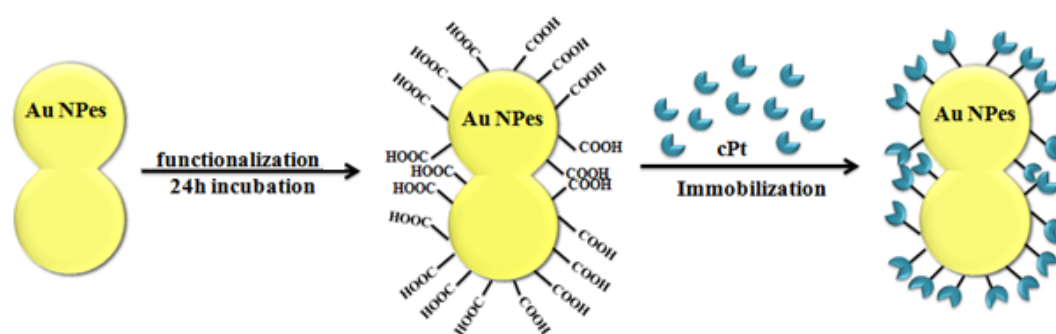


Figure 4. Scheme of the Au NPes functionalization process.

3.2.4. X-ray Diffraction

The crystal microstructure of the Au NPes was assessed using a two-circle laboratory diffractometer Panalytical X'Pert Pro. The measurements were performed in the standard θ - 2θ geometry using a lamp with the Cu anode working at 40 kV and 30 mA. The X-ray beam emitted by the X-ray tube was converted into a parallel beam by a divergence slit with a constant height $1/2^\circ$, a parabolic graded W/Si mirror with an equatorial divergence less than 0.05 and by a mask of constant width of 20 mm, limiting the width of the beam. The diffracted beam optics were composed of the anti-scatter slit with a height of 8.7 mm, 0.04 rad Soller slit collimator, a curved graphite monochromator to remove the contribution of the Cu K β radiation and the semiconductor silicon stripe detector with active length of 2.122° . The nanoparticles dispersion was dried on a zero-background holder and was mount on a sample spinner with rotation time of 16 s. The data were collected in the range between 20 – 80° (2θ) with a step size of 0.08° . The time per step was equal to 7000 sec. Fullprof software was used for diffractogram fitting, lattice constants and the coherent scattering length evaluation [38].

3.2.5. Calorimetric Measurements

Calorimetric measurements were carried out with a TA Instruments' DSC 2500 differential scanning calorimeter equipped with a liquid nitrogen LN2P pump. The samples (ca. 1–3 mg) were placed in aluminum pans and crimped with hermetic lids. The thermal behavior of the samples was studied under dry N5.0 pure nitrogen purge (25 mL min^{-1}) in a temperature range from 10°C to 200°C at 5 and $10^\circ\text{C min}^{-1}$ heating rate and at 5°C min^{-1} cooling rate. The samples were held isothermally at the minimum and maximum temperature for 5 min. Calibrations of temperature and enthalpy were performed using an indium standard. TRIOS software was used to calculate the peak temperatures and the enthalpy values of the registered thermal events. The TGA measurements were performed using a TA Instruments' TGA 5500 thermogravimetric analyzer with high temperature platinum pans. The samples were either directly placed in open $100 \mu\text{L}$ platinum pans or previously enclosed inside hermetic aluminum pans to the limit the evaporation rate. In the case of aluminum pans, a hole of 0.9 mm diameter was punched through the lid of the container right before the start of the measurements. The samples were heated at a rate of 5 or $10^\circ\text{C min}^{-1}$ rate up to 500°C under a flow of N5.0 pure nitrogen (25 mL min^{-1}). The temperature calibration was carried out using nickel and aluminium tandards.

3.2.6. Cell Lines

Two human glioblastoma cell lines (U118 MG, U251 MG) were used as an in vitro model. The U-118 MG was obtained from the ATCC[®] (American Type Culture Collection, Virginia, No. HTB-15[™]) and was continuously cultured in Dulbecco's modified Eagle's medium (DMEM, ATCC[®], No. 30-2002). The U251 MG (No. 09063001) human glioblastoma astrocytoma cell line was purchased from PHE (Public Health England, Salisbury, UK) culture collections and cultured in Dulbecco's modified Eagle's medium (DMEM, high glucose, GlutaMAX[™], Gibco[®], No. 31966021, Thermo Fisher Scientific,

Waltham, MA, USA). The cells were maintained in 25 cm² tissue culture flasks (TPP[®], No. 90026,) and the cultures were supplemented with 10% fetal bovine serum (FBS, Gibco[®], No. 10270106), in a humidified incubator at 37 °C with 5% CO₂. When 70% confluent cell monolayer was reached, the cells were detached with Trypsin/EDTA solution 1× (Sigma-Aldrich. No. T4049, Darmstadt, Germany) until complete cell detachment. The cell suspension with trypsin inactivated by a 5-fold dilution with fresh growth medium was spun down (3 min, 700 rpm) in 15 mL conical tubes, and the cell pellet was then resuspended in a fresh growth medium for cells scoring.

3.2.7. Irradiation and Dosimetry

Single X-ray dose of 2 Gy was given to each dish or microplate (one dose per each plate containing a set of different samples) by a Philips X-ray machine (model MCN 323) at 250 kV, 10 mA, the dose rate of 2 Gy/min operating at the IFJ PAN. Detailed information about setup and dosimetry are provided in our previous studies [39]. Control (non-irradiated) and radiation plates were rinsed in a similar manner and kept out of the incubator (during radiation) for the same amount of time. After irradiation, all plates were immediately placed back to the incubator. Cell survival was assessed with the MTT assay and chemical changes were measured by spectroscopic experiments (see supplementary materials).

3.2.8. Cell Viability Experiments

For MTT experiments, carried out in triplicates for each trial, 200 µL of suspension containing about 2500 cells of the U118 MG and U251 MG cell lines, respectively, were seeded per well in 96-well microplates (TPP[®], No. 92096) and incubated for 72 h. A quarter of these cells was left without any further treatment and used as a control. From the rest of the 72 h incubated cells, the old medium was aspirated and cisplatin (5 µM) or Au NPes (2.93 × 10⁻⁶ mg/mL) or cPt@Au NPes (5 µM) were added to obtain a final volume of 110 µL per well. Similarly, both cell lines after 72 incubation and cells with the addition of cisplatin (5 µM) or Au NPes (2.93 × 10⁻⁶ mg/mL) or cPt@Au NPes (5 µM) were irradiated (see 2.8). The MTT tests were performed on all cells, including the reference cells, before and after irradiation, with and without additions after 3, 6, 24 and 48 h. The description of all cell samples, which were studied in MTT, Raman and FTIR experiments, is presented in Table 1.

Table 1. Description of cells samples.

No.	Sample	Name of Samples in the MTT, Raman and FTIR Results
1	Control samples of cell lines U118 and U251 (cells without addition other substances)	Ctrl
2	Cells cultured with Au NPes	C@Au NPes
3	Cells cultured with 5 µM cisplatin	C@cPt
4	Cells cultured with Au NPes functionalized by cisplatin	C@cPtNPes
5	Control samples X-ray treated	C@X
6	Cells cultured with Au NPes and X-ray treated	C@XNPes
7	Cells cultured with 5µM cisplatin and X-ray treated	C@XcPt
8	Cells cultured with NPs functionalized by cisplatin and X-ray treated	C@XcPtNPes

3.2.9. MTT Assay

The MTT reagent (10 µL, final concentration 0.5 mg/mL, Roche, Mannheim, Germany, No. 11465007001) was added to each well and incubated for the following 4 h at 37 °C. For solubilization of the resultant formazan product, 100 µL of the solubilization solution (10% *v/v* sodium dodecyl sulphate and 0.01 M HCl, Roche, Mannheim, Germany) was added to each well for overnight incubation. The absorbance at 590 nm was measured using a Tecan Spark microplate reader (Tecan Trading AG, Männedorf, Switzerland) [40].

3.2.10. Analysis of Cell Viability Data

In the MTT test, data for each treatment point shows an average from three parallel wells with a standard deviation (\pm S.D.). For each well, five measurements at different positions were performed. To obtain pure cellular absorption, the absorption rate of the wells without cells was subtracted from the absorption of the wells with cells. According to the following equation based on Sadri A. [41] and explained by Zakrzewska K. [2], there is a direct association between the pure absorption and the rate of viable cells:

$$A_s/A_{ref} \cdot 100\% = v_c \quad (1)$$

where A_s is the mean absorption of the measured sample, A_{ref} is the mean absorption of the reference sample and v_c is the percentage of viable cells.

The data were analyzed and presented graphically using Microsoft Office Excel 2013. The quantitative results were finally compared with the T test. P value < 0.05 was considered to be statistically significant.

3.2.11. Sample Preparation for Spectroscopic Experiments

In spectroscopic experiments, the U118 MG and U251 MG cells (125×10^5 cells in a volume of 0.2 mL) were placed in 100 mm dishes (Sarstedt, No. 83.3902, Nümbrecht, Germany) and incubated for 72 h. The samples were prepared in the same way as for the MTT experiments. Then, the cells were detached, collected into 15 mL conical tubes, spun down (3 min, 700 rpm). The cell pellet was resuspended in 4 mL of 0.9% NaCl and once again spun down. The supernatant was carefully removed, and the pellets were measured by FTIR and Raman spectroscopy.

3.2.12. FTIR Spectroscopy

EXCALIBUR FTS-3000 spectrometer working at room temperature was used for all measurements. All spectra were recorded by attenuated total reflection (ATR) with a ZnSn crystal. For that purpose, 0.5 mL of the cell containing solution was deposited on the ATR ZnSn crystal. The spectra were recorded in the range from 4000 to 500 cm^{-1} . Each spectrum was obtained by averaging 64 scans recorded at a resolution of 4 cm^{-1} . OPUS software was used for baseline correction and normalization of the obtained spectra.

3.2.13. FT-Raman Spectroscopy

FT-Raman spectra were acquired with a Nicolet NXR 9650 FT-Raman Spectrometer equipped with an Nd:YAG laser (1064 nm) and a germanium detector. The measurements were performed in the between 150 and 3.700 cm^{-1} using laser power of 1 W. An unfocused laser beam was used with a diameter of approximately 100 μm and a spectral resolution of 8 cm^{-1} . Omnic/Thermo Scientific software was used to process the Raman based on 128 scans.

4. Conclusions

In the present study the efficiency of combined nano-chemo-radiotherapy treatment for glioblastoma cell lines was examined. For this purpose, we designed a new nanosystem consisting of gold nanoparticle (Au NPs) with surface immobilized cisplatin, which was added into the glioblastoma cells, which were subsequently subjected to X-ray radiation. TEM in combination with XRD revealed that the Au NPs are crystalline and their size is around 60 nm along the longitudinal axis, while it is ~20 nm along the transverse axis. The functionalization of the Au NPs as well as the immobilization success and stability of cPt on the Au NPs surface were verified by Raman spectroscopy. The TGA and DSC measurements showed that the created nanosystem is stable in the temperature range between 0 °C to 110 °C. The MTT assay showed that the highest mortality of cells was visible in the cells treated by combined therapy. Furthermore, FTIR and Raman spectra of cancer cells cultured with cisplatin immobilized on Au NPs surface and irradiated by X-rays showed the most

visible chemical changes in the cells, especially in the functional groups building DNA, proteins and lipids compounds. Summarizing, the novel gold nanoparticles are a promising support for delivering cPt into the glioblastoma cells and thus a promising nanosystem to improve the therapeutic efficiency of combined nano-chemo-radiotherapy.

Supplementary Materials: Supplementary materials can be found at <http://www.mdpi.com/1422-0067/21/23/9082/s1>.

Author Contributions: J.D. together with J.M. and K.R. conceived the idea, carried out the experiments and measurements, wrote the manuscript as well as the statistics, tables and figures with support from M.P.-W. M.P.-W. performed the TEM observations and corrected all the manuscript. A.P. verified the applied MTT method, planned and carried out X-ray irradiations. A.M. performed analyzed the XRD measurements, while P.M.Z. acquired and interpreted the DCS and TGA scans. P.O. provided a part of funds, as well as technical expertise in correcting the manuscript. All authors read and approved the final manuscript.

Funding: This study was partially funded by the Horizon 2020 UE project entitled “INfraStructure in Proton International REsearch”, INSPIRE, No. 730983; National Science Centre, Poland Grant No. DEC-2013/09/D/NZ7/00324 (access to laboratory equipment) and MNiSW 7150/E-338/M/2014.

Acknowledgments: The research was partially performed at the Institute of Nuclear Physics Polish Academy of Sciences using the equipment purchased in the frame of the project co-funded by the Malopolska Regional Operational Program Measure 5.1 Krakow Metropolitan Area as an important hub of the European Research Area for 2007–2013, project No. MRPO.05.01.00-12-013/15. The authors gratefully acknowledge the technical staff for help in X-ray irradiation and laboratory procedures and the Institute of Engineering Materials and Biomaterials of the Silesian University of Technology for the use of the Titan FEI TEM instrument. Finally, we would like to express our gratitude to Pik Instruments for the partial sponsoring of this research. Dr Monika Kula is acknowledged for the use of the Raman instrument located at Polish Academy of Sciences, The Franciszek Górski Institute of Plant Physiology.

Conflicts of Interest: The authors declare no conflict of interest.

References

1. Glaser, T.; Han, I.; Wu, L.; Zeng, X. Targeted nanotechnology in glioblastoma multiforme. *Front. Pharmacol.* **2017**, *8*, 166. [[CrossRef](#)]
2. Zakrzewska, K.E.; Samluk, A.; Wierzbicki, M.; Jaworski, S.; Kuwin, M.; Sawosz, E.; Chwalibog, A.; Pijanowska, D.G.; Pluta, K.D. Analysis of the cytotoxicity of carbon-based nanoparticles, diamond and graphite, in human glioblastoma and hepatoma cell lines. *PLoS ONE* **2015**, *10*, e0122579. [[CrossRef](#)]
3. Holland, E.C. Glioblastoma multiforme: The terminator. *Proc. Natl. Acad. Sci. USA* **2000**, *97*, 6242–6244. [[CrossRef](#)]
4. Rosa, S.; Connolly, C.; Schettino, G.; Butterworth, K.T.; Prise, K.M. Biological mechanisms of gold nanoparticles radiosensitization. *Cancer Nanotechnol.* **2017**, *8*, 2. [[CrossRef](#)]
5. Zhao, X.; Pan, J.; Li, W.; Yang, W.; Qin, L.; Pan, Y. Gold nanoparticles enhance cisplatin delivery and potentiate chemotherapy by decompressing colorectal cancer vessels. *Int. J. Nanomed.* **2018**, *13*, 6207–6221. [[CrossRef](#)]
6. Boisselier, E.; Astruc, D. Gold nanoparticles in nanomedicine: Preparations, imaging, diagnostics, therapies and toxicity. *Chem. Soc. Rev.* **2009**, *38*, 1759–1782. [[CrossRef](#)]
7. Dreaden, E.C.; Austin, L.A.; Mackey, M.A.; El-Sayed, M.A. Size matters: Gold nanoparticles in targeted cancer drug delivery. *Ther. Deliv.* **2012**, *3*, 457–478. [[CrossRef](#)]
8. Jain, S.; Hirst, D.G.; O’Sullivan, J.M. Gold nanoparticles as novel agents for cancer therapy. *Br. J. Radiol.* **2012**, *85*, 101–113. [[CrossRef](#)]
9. Hainfeld, J.F.; Dilmanian, F.A.; Slatkin, D.N.; Smilowitz, H.M. Radiotherapy enhancement with gold nanoparticles. *J. Pharm. Pharmacol.* **2007**, *60*, 977–985. [[CrossRef](#)]
10. Molavi, O.; Xiong, X.B.; Douglas, D.; Kneteman, N.; Nagata, S.; Pastan, I.; Chu, Q.; Lavasanifar, A.; Lai, R. Anti-cd30 antibody conjugated liposomal doxorubicin with significantly improved therapeutic efficacy against anaplastic large cell lymphoma. *Biomaterials* **2013**, *34*, 8718–8725. [[CrossRef](#)]
11. Maeda, H.; Matsumura, Y. EPR effect based drug design and clinical outlook for enhanced cancer chemotherapy. *Adv. Drug Deliv. Rev.* **2011**, *63*, 129–130. [[CrossRef](#)]
12. Shahbazi, M.-A.; Shresta, N.; Makila, E.; Araujo, F.; Correia, A.; Ramos, T.; Sarmiento, B.; Salonen, J.; Hirvonen, J.; Santos, S.A. A prospective cancer chemo-immunotherapy approach mediated by synergistic CD326 targeted porous silicon nanovectors. *Nano Res.* **2015**, *8*, 1505–1521. [[CrossRef](#)]

13. Nowak, A.K.; Lake, R.A.; Robinson, B.W. Combined chemoimmunotherapy of solids tumours: Improving vaccines. *Adv. Drug Deliv. Rev.* **2006**, *58*, 975–990. [[CrossRef](#)]
14. Lee, I.H.; An, S.; Yu, M.K.; Kwon, H.K.; Im, S.H.; Jon, S. Targeted chemoimmunotherapy using drug-loaded aptamer-dendrimer bioconjugates. *J. Control. Release* **2011**, *155*, 435–441. [[CrossRef](#)]
15. Takahara, P.M.; Rosenzweig, A.C.; Frederick, C.A.; Lippard, S.J. Crystal structure of double-stranded DNA containing the major adduct of the anticancer drug cisplatin. *Nature* **1995**, *377*, 649–652. [[CrossRef](#)]
16. Lipiec, E.; Ruggeri, F.S.; Benadiba, C.; Borkowska, A.M.; Kobierski, J.D.; Miszczyk, J.; Wood, B.R.; Deacon, G.B.; Kulik, A.; Dietler, G.; et al. Infrared nanospectroscopic mapping of a single metaphase chromosome. *Nucleic Acids Res.* **2019**, *47*, e108. [[CrossRef](#)]
17. Davidi, E.S.; Dreifuss, T.; Motiei, M.; Shai, E.; Bragilovski, D.; Lubimov, L.; Kindler, M.J.J.; Popovtzer, A.; Don, J.; Popovtzer, R. Cisplatin-conjugated gold nanoparticles as a theranostic agent for head and neck cancer. *Head Neck* **2018**, *40*, 70–78. [[CrossRef](#)]
18. Dhar, S.; Gu, F.X.; Langer, R.; Farkhzad, O.C.; Lippard, S.J. Targeted delivery of cisplatin to prostate cancer cells by aptamer functionalized Pt(IV) prodrug-PLGA-PEG nanoparticles. *Proc. Natl. Acad. Sci. USA* **2008**, *105*, 17356–17361. [[CrossRef](#)]
19. Schechter, B.; Arnon, R.; Wilchek, M. Polymers in drug delivery: Immunotargeting of carrier-supported cis-platinum complexes. *React. Polym.* **1995**, *25*, 167–175. [[CrossRef](#)]
20. Wei, L.; Zhao, X.; Du, B.; Li, X.; Liu, S.; Yang, X.-Y.; Ding, H.; Yang, W.; Pan, F.; Wu, X.; et al. Gold nanoparticle-mediated targeted delivery of recombinant human endostatin normalizes tumour vasculature and improves cancer therapy. *Sci. Rep.* **2016**, *6*, 30619.
21. Li, W.; Li, X.; Liu, S.; Yang, W.; Pan, F.; Yang, X.Y.; Du, B.; Qin, L.; Pan, Y. Gold nanoparticles attenuate metastasis by tumor vasculature normalization and epithelial-mesenchymal transition inhibition. *Int. J. Nanomed.* **2017**, *12*, 3509–3520. [[CrossRef](#)]
22. Mann, J.; Ramakrishna, R.; Magge, R.; Wernicke, A.G. Advances in radiotherapy for glioblastoma. *Front. Neurol.* **2017**, *8*, 748. [[CrossRef](#)]
23. Haume, K.; Rosa, S.; Grellet, S.; Smialek, M.A.; Butterworth, K.T.; Solovyov, A.V.; Prise, K.M.; Golding, J.; Mason, N.J. Gold nanoparticles for cancer radiotherapy: A review. *Cancer Nanotechnol.* **2016**, *7*, 8. [[CrossRef](#)]
24. McQuaid, H.N.; Muir, M.F.; Taggart, L.E.; McMahon, S.J.; Coulter, J.A.; Hyland, W.B.; Jain, S.; Butterworth, K.T.; Schettino, G.; Prise, K.M.; et al. Imaging and radiation effects of gold nanoparticles in tumours cells. *Sci. Rep.* **2016**, *6*, 19442. [[CrossRef](#)]
25. Smilowitz, H.M.; Meyers, A.; Rahman, K.; Dymont, N.A.; Sasso, D.; Xue, C.; Oliver, D.L.; Lichtler, A.; Deng, X.; Tarmu, L.J.; et al. Intravenously-injected gold nanoparticles (Au NPs) access intracerebral F98 rat gliomas better than AuNPs infused directly into the tumor site by convection enhanced delivery. *Int. J. Nanomed.* **2018**, *13*, 3937–3948. [[CrossRef](#)]
26. Suk, I.-K.; Ohta, H.; Waseda, Y. High-temperature thermal expansion of six metallic elements measured by dilatation method and X-ray diffraction locality synthetic sample: At T=293 K. *J. Mater. Sci.* **1988**, *23*, 757–760.
27. Sneha, K.; Sathishkumar, M.; Kim, S.; Yun, Y.-S. Counter ions and temperature incorporated tailoring of biogenic gold nanoparticles. *Proc. Biochem.* **2010**, *45*, 1450–1458. [[CrossRef](#)]
28. Bazylewski, P.; Divigalpitiya, R.; Fanchini, G. In situ Raman spectroscopy distinguishes between reversible and irreversible thiol modifications in L-cysteine. *RSC Adv.* **2017**, *5*, 2964–2970. [[CrossRef](#)]
29. Deregowska, A.; Depciuch, J.; Wojnarowska, R.; Polit, J.; Broda, D.; Nechai, H.; Gonchar, M.; Sheregii, E. Study of optical properties of glutathione capped gold nanoparticles using linker (MHDA) by Fourier transform infrared spectroscopy and surface enhanced Raman scattering. *Int. J. Biotechnol. Bioeng.* **2013**, *7*, 80–83.
30. Chandekar, A.; Sengupta, S.K.; Whitten, J.E. Thermal stability of thiol and silane monolayers: A comparative study. *Appl. Surface Sci.* **2010**, *256*, 2742–2749. [[CrossRef](#)]
31. Balca-Silva, J.; Matias, D.; Do Carmo, A.; Dubois, L.G.; Goncalves, A.C.; Girao, H.; Canedo, N.H.S.; Correia, A.H.; De Souza, J.M.; Sarmenzo-Ribeiro, A.B.; et al. Glioblastoma entities express subtle differences in molecular composition and response to treatment. *Oncol. Rep.* **2017**, *38*, 1341–1352. [[CrossRef](#)]
32. Kumar, V.; Sharma, N.; Maitra, S.S. In vitro and in vivo toxicity assessment of nanoparticles. *Int. Nano Lett.* **2017**, *7*, 243–256. [[CrossRef](#)]

33. Coluccia, D.; Figueiredo, C.A.; Wu, M.Y.; Riemenschneider, A.N.; Diaz, R.; Luck, A.; Smith, C.; Das, S.; Ackerley, C.; O'Reilly, M.; et al. Enhancing glioblastoma treatment using cisplatin-gold nanoparticle conjugates and targeted delivery with magnetic resonance-guided focused ultrasound. *Nanomedicine* **2018**, *14*, 1137–1148. [[CrossRef](#)]
34. Gonçalves, D.P.N.; Rodriguez, R.D.; Kurth, T.; Braya, L.J.; Binner, M.; Jungnickela, C.; Gürf, F.N.; Poser, S.W.; Schmidt, T.L.; Zahn, D.R.T.; et al. Enhanced targeting of invasive glioblastoma cells by peptide-functionalized gold nanorods in hydrogel-based 3D cultures. *Acta Biomater.* **2017**, *58*, 12–25. [[CrossRef](#)]
35. Alphandéry, E. Nano-Therapies for Glioblastoma Treatment. *Cancers* **2020**, *12*, 242. [[CrossRef](#)]
36. Han, X.; Xue, X.; Zhou, H.; Zhang, G. A molecular view of the radioresistance of gliomas. *Oncotarget* **2017**, *8*, 100931–100941. [[CrossRef](#)]
37. Taghian, A.; Suit, H.; Pardo, F.; Gioioso, D.; Tomkinson, K.; DuBois, W.; Gerweck, L. In vitro intrinsic radiation sensitivity of glioblastoma multiforme. *Int. J. Radiat. Oncol. Biol. Phys.* **1992**, *23*, 55–62. [[CrossRef](#)]
38. Rodriguez-Carvajal, J. FullProf: A program for Rietveld refinement and pattern matching analysis. *Tech. Rep. CEA-CNRS Saclay Fr.* **1990**, *127*, 12–20.
39. Miszczyk, J.; Rawojć, K.; Panek, A.; Swakoń, J.; Prasanna, P.G.; Rydygier, M. Response of human lymphocytes to proton radiation of 60 MeV compared to 250 kV X-rays by the cytokinesis-block micronucleus assay. *Radiother. Oncol.* **2015**, *115*, 128–134. [[CrossRef](#)]
40. Roman, M.; Wrobel, T.P.; Panek, A.; Efeouglu, E.; Wiltowska-Zuber, J.; Paluszkiwicz, C.; Byrne, H.J.; Kwiatek, W.M. Exploring subcellular responses of prostate cancer cells to X-ray exposure by Raman mapping. *Sci. Rep.* **2019**, *9*, 8715. [[CrossRef](#)]
41. Sadri, A.; Changizi, V.; Eivazadeh, N. Evaluation of glioblastoma (U87) treatment with ZnO nanoparticle and X-ray in spheroid culture model using MTT assay. *Radiat. Phys. Chem.* **2015**, *115*, 17–21. [[CrossRef](#)]

Publisher's Note: MDPI stays neutral with regard to jurisdictional claims in published maps and institutional affiliations.



© 2020 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (<http://creativecommons.org/licenses/by/4.0/>).