



Identification of recent exacerbations in COPD patients by electronic nose

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ABSTRACT Molecular profiling of exhaled breath by electronic nose (eNose) might be suitable as a noninvasive tool that can help in monitoring of clinically unstable COPD patients. However, supporting data are still lacking. Therefore, as a first step, this study aimed to determine the accuracy of exhaled breath analysis by eNose to identify COPD patients who recently exacerbated, defined as an exacerbation in the previous 3 months.

Data for this exploratory, cross-sectional study were extracted from the multicentre BreathCloud cohort. Patients with a physician-reported diagnosis of COPD (n=364) on maintenance treatment were included in the analysis. Exacerbations were defined as a worsening of respiratory symptoms requiring treatment with oral corticosteroids, antibiotics or both. Data analysis involved eNose signal processing, ambient air correction and statistics based on principal component (PC) analysis followed by linear discriminant analysis (LDA).

Before analysis, patients were randomly divided into a training (n=254) and validation (n=110) set. In the training set, LDA based on PCs 1-4 discriminated between patients with a recent exacerbation or no exacerbation with high accuracy (receiver operating characteristic (ROC)-area under the curve (AUC)=0.98, 95% CI 0.97-1.00). This high accuracy was confirmed in the validation set (AUC=0.98, 95% CI 0.94-1.00). Smoking, health status score, use of inhaled corticosteroids or vital capacity did not influence these results.

Exhaled breath analysis by eNose can discriminate with high accuracy between COPD patients who experienced an exacerbation within 3 months prior to measurement and those who did not. This suggests that COPD patients who recently exacerbated have their own exhaled molecular fingerprint that could be valuable for monitoring purposes.



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Introduction

Exacerbations have a large impact on the quality of life of COPD patients. These periods of acute worsening that require additional therapy [1] are a prominent cause for the irreversible deterioration of lung function [2, 3] and are responsible for the greatest economic burden of COPD on healthcare expenditure [1]. Several biomarkers that show an association with history and risk of exacerbations have been identified; however, problems with reproducibility ensure that to date none of these have additional value over easily obtained clinical variables [4]. Peripheral blood eosinophil levels seem promising in predicting mortality and exacerbation risk [5], yet ambiguity about cut-off levels and the use of absolute or relative values hamper their use thus far [6].

Other potential biomarkers are volatile organic compounds (VOCs) in exhaled breath. VOCs are produced *via* different metabolic pathways and may reflect local, systemic and exogenous processes in the airways and alveoli [7, 8]. Analysis by gas chromatography combined with mass spectrometry (GC/MS) showed specific metabolic patterns of exacerbations in COPD patients and the ability to predict asthma exacerbations in children [9, 10]. Both GC/MS and pattern analysis of so-called breathprints by an electronic nose (eNose) were able to identify ongoing exacerbations in COPD patients [11, 12]. During follow-up, both methods showed a distinct exhaled breath pattern between exacerbations and stable disease [13]. Furthermore, data from a pilot study suggest that eNose analysis could make a distinction between COPD patients with and without bacterial or viral infections [14], which are important triggers for exacerbations.

Being easy to implement and noninvasive, eNose analysis might also be an appealing monitoring tool that can help to identify patients who exacerbated. However, data to answer this question in COPD are still lacking, and as a first step, there is a need to assess whether it is possible to detect an exacerbation signal in exhaled breath by eNose analysis.

In this proof of principle study, we hypothesised that exacerbations induce changes in exhaled metabolic patterns that can be captured by eNose sensors. If so, eNose technology may be suitable as a user-friendly and noninvasive point-of-care tool to identify patients who recently exacerbated. Therefore, in this study we aimed to determine the accuracy of VOC pattern analysis in exhaled breath by eNose to identify a history of recent exacerbations in COPD patients using maintenance therapy.

Methods

Population

Data for this exploratory, cross-sectional study were extracted from the multicentre BreathCloud cohort [15] that enrolled patients with asthma, COPD and lung cancer in primary, secondary and tertiary care centres in the Netherlands during routine (outpatient) visits. Due to the noninvasive nature of the BreathCloud study, the Amsterdam UMC medical ethical review board provided a waiver for ethical approval (reference: W14_112#14.17.0147, see supplementary material). Informed consent was obtained from each patient before enrolment. Inclusion criteria for the current study were: a physician-reported diagnosis of COPD, reported use of maintenance therapy with long-acting β-agonists and/or use of long-acting muscarinic antagonists, with or without additional therapy with ICS.

Outcome definition

An exacerbation was defined as a worsening of respiratory symptoms requiring the use of treatment with oral corticosteroids (OCS), antibiotics or both [1] during the 3 months prior to the eNose measurement.

Exhaled breath measurement

Exhaled breath analysis was performed by the SpiroNose (Amsterdam UMC, Amsterdam, the Netherlands), an eNose that uses seven cross-reactive metal oxide semiconducting sensors and has been technically validated earlier [16]. During inclusion in the BreathCloud cohort, patients were first required to thoroughly rinse their mouth with water three times. After this, patients were instructed to perform five tidal breaths followed by full inspiration, a 5-s breath-hold and slow maximal expiration towards residual volume. The entire measurement was performed in duplicate, considering an interval of 2 min. Data was captured in real-time and directly sent to the online BreathCloud server, where it was stored. Processing of eNose sensor signals was performed as described previously [15, 16]; more details can be found in the supplementary material.

Statistical analysis

Statistical analysis was performed by R studio version 1.1.463 (Rstudio Inc., Boston, MA, USA) using R version 3.5.1 (The R Foundation for Statistical Computing, Vienna, Austria, with packages: dplyr, caret, pROC and MASS [17–19]). A schematic overview of the statistical analysis is shown in figure 1; more

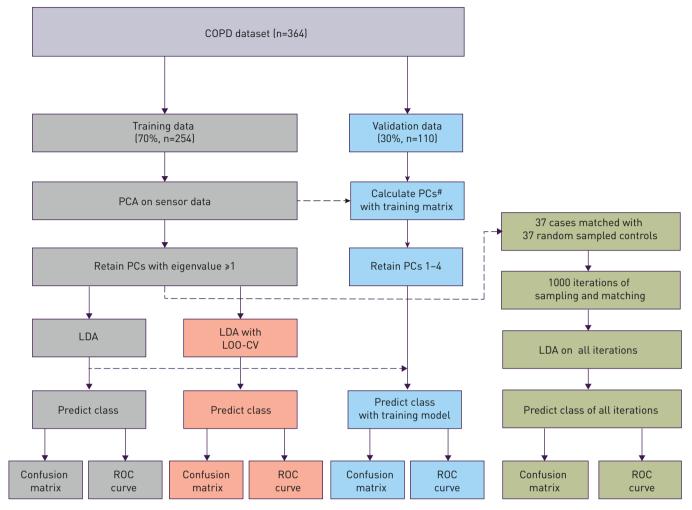


FIGURE 1 Flowchart of statistical analysis. PCA: principal component analysis; PCs: principal components; LDA: linear discriminant analysis; LOO-CV: leave-one-out cross-validation; ROC: receiver operating characteristic. #: Validation data principal components have been calculated by using the same parameters of standardisation and same rotation matrix as those used to calculate the training data principal components.

information on our statistical approach can be found in the supplementary material. Before the analysis, the included patients were randomly divided between a training (±70%) and validation (±30%) set. After this split, a principal component (PC) reduction of the training set eNose signal data was combined with linear discriminant analysis (LDA). Based on the Kaiser criterion [20], the training set PCs with an eigenvalue \geq 1.0 were selected for further analysis. PCs from validation set sensor data were constructed by using the same parameters of standardisation and the same rotation matrix as those used to calculate the training data PCs. Discriminant scores, based on LDA, were used to construct receiver operating characteristic (ROC) curves and calculate the area under the curve (AUC). Internal validation was performed with leave-one-out cross-validation (LOO-CV); for external validation the LDA model that was constructed with the training set was applied to the validation set. Predicted classification based on the LDA was used to construct confusion matrices for the different datasets (training, training with cross-validation and validation). These confusion matrices were subsequently used to calculate overall accuracy, sensitivity, specificity, and positive- and negative predictive values.

Sensitivity analyses

Our dataset was expected to have few cases compared to the number of controls. Therefore, to test the robustness of the model, the cases were matched with an equal amount of random sampled controls [21]. Average accuracy measures and ROC-AUC were calculated for 1000 iterations of this random sampling. The effect of current OCS and/or antibiotics use for exacerbations on the eNose signal was assessed by a secondary analysis excluding current users. Other sensitivity analyses were performed to map the effects on the discriminatory ability of the eNose of ICS use, smoking (both smoking status and pack-years), vital capacity during the measurement and clinical COPD questionnaire (CCQ) scores [22].

Results

In total, 364 patients diagnosed with COPD were enrolled in this study. The patients were randomly divided between a training (n=254) and validation set (n=110). In the training set, 37 patients (14.6%) experienced an exacerbation and in the validation set 13 patients (11.8%). Baseline characteristics of patients in the training set are shown in table 1, and characteristics of patients in the validation set are given in supplementary table S1. Mean age was 66.7 ± 9.3 (training) and 65.9 ± 8.7 (validation) years, percentage of females 47.6% (training) and 43.2% (validation) and median pack-years 36 (training) and 35 (validation). Pre-bronchodilator forced expiratory volume in 1 s (FEV₁) (as % of predicted) was similar in the training and the validation set (61.2% and 57.1%, respectively) as was the FEV₁/forced vital capacity (FVC) ratio (0.49 and 0.45, respectively). In the training set, the only difference between exacerbation/no exacerbation was found in blood eosinophil levels (0.20 cells· μ L⁻¹ versus 0.11 cells· μ L⁻¹) and the number of patients on ICS (78.4% versus 59.0%), both being higher in the exacerbation group. In the validation set, the only difference between exacerbation/no exacerbation was found in age, being higher in the exacerbation group (73.0±7.5 versus 64.9±8.5). No statistically significant differences were found in baseline clinical characteristics between the training and the validation set, although there was a borderline significant difference in pack-years (being higher in the validation set) (supplementary table S2).

Identification of exacerbations

PCs 1–4 were selected to be used in the analysis. In the training set, all these principal components were significantly different between the exacerbation and non-exacerbation groups; in the validation set, this difference was only found for PCs 2–4. The distribution of patients with exacerbations and patients without exacerbations over the different principal components is shown for both sets in figure 2.

LDA was used to create a model and construct ROC curves. The ability to identify patients with a previous exacerbation showed high accuracy in the training set (ROC-AUC=0.98, 95% CI 0.97-1.00), with 95.3% of cross-validated grouped cases correctly classified after LOO-CV (95% CI 91.9-97.5%). This high accuracy was further confirmed in the validation set (AUC=0.98, 95% CI 0.94-1.00) where 95.5% of the grouped cases were correctly classified (figure 3). In comparison with other accuracy measures, sensitivity to

TABLE 1 Patient characteristics	of the training se			
	Total training	Exacerbation	No exacerbation	p-value
Patients n	254	37	217	
Age years	66.7±9.3	64.9±9.5	67.0±9.3	0.21
Female	121 (47.6)	16 (43.2)	105 (48.4)	0.69
Blood eosinophils cells⋅µL ⁻¹	0.12 (0.07-0.23)	0.20 (0.12-0.34)	0.11 (0.06-0.20)	0.02
Blood neutrophils cells.µL ⁻¹	5.83 (4.32-8.26)	6.60 (4.50-9.88)	5.74 (4.30-7.70)	0.27
BMI kg·m ⁻²	26.4 (23.4-30.4)	25.9 (22.7-30.5)	26.5 (23.5-30.1)	0.86
Pre-BD FEV ₁ % pred	61.2±20.9	57.1±21.8	61.9±20.7	0.24
FEV ₁ /FVC ratio	0.49±0.14	0.45±0.14	0.49±0.13	0.15
Patients with exacerbations				
Total		37 (14.6)		
OCS in the past 3 months n		7		
AB in the past 3 months n		9		
AB+0CS in the past 3 months n		12		
Currently using AB n		2		
Currently using OCS n		6		
Currently using AB+OCS n		1		
Patients with ICS	157 (61.8)	29 (78.4)	128 (59.0)	0.04
CCQ score	2.1±1.1	2.3±1.1	2.0±1.0	0.19
CCQ score >3	55 (22.6)	8 (21.6)	47 (21.7)	1.00
Smoking history				0.63
Never	7 (2.8)	1 (2.7)	6 (2.8)	
Ex	168 (66.1)	22 (59.5)	146 (67.3)	
Current	79 (31.1)	14 (37.8)	65 (30.0)	
Pack-years	36 (20–49)	35 (20–42)	36 (20–50)	0.38

Data are presented as mean±sp, n (%) or median (interquartile range), unless otherwise stated. BMI: body mass index; pre-BD: pre-bronchodilator; FEV₁: forced expiratory volume in 1 s; FVC: forced vital capacity; OCS: oral corticosteroids; ICS: inhaled corticosteroids; AB: antibiotics; CCQ: Clinical COPD Questionnaire. p-values correspond to comparisons between exacerbation/no exacerbation.

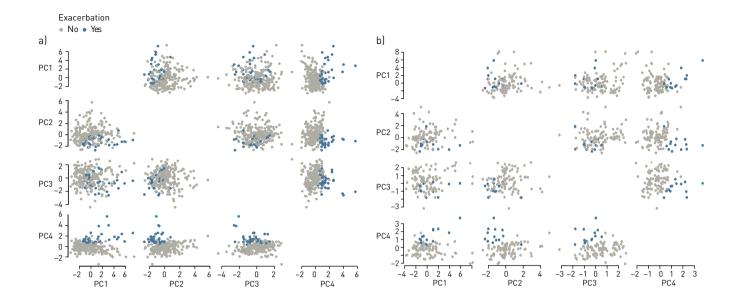


FIGURE 2 Scatter matrices of patients who experienced an exacerbation and those who did not in a) training set (n=254) and b) validation set (n=110). PC: principal component.

identify patients with exacerbations was lower in both the training and validation sets (0.73 and 0.69, respectively). Specificity was 0.99 in both the training and validation sets (table 2).

Robustness of the model

When the 37 cases in the training set were compared with 37 randomly sampled controls, AUC and accuracy value were still high. After 1000 iterations, the average sensitivity increased to 0.88 (95% CI 0.88–0.88) and average specificity somewhat decreased to 0.95 (95% CI 0.95–0.95). Both linear

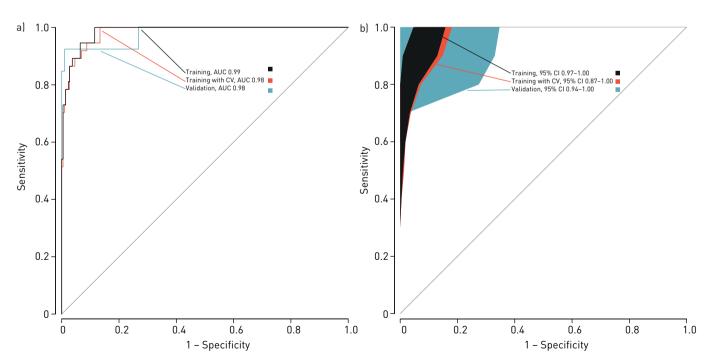


FIGURE 3 Receiver operating characteristic (ROC) analyses showing the accuracy of the linear discriminant model based on principal component reduction in the training set, internally validated training set (through leave-one-out cross-validation) and the independent validation set. a) Curves. b) 95% confidence intervals. CV: cross-validation; AUC: area under the curve; CI: confidence interval.

TABLE 2 Accuracy parameters in the different datasets							
Data	ROC-AUC (95% CI)	Accuracy value (95% CI)	No information rate (NIR)	Sensitivity	Specificity	PPV	NPV
Training set	0.99 (0.97–1.00)	0.95 (0.92-0.98)	0.85***	0.73	0.99	0.93	0.96
Training set LOO-CV	0.98 (0.97-1.00)	0.95 (0.92-0.98)	0.85****	0.73	0.99	0.93	0.96
Validation set	0.98 (0.94-1.00)	0.96 (0.90-0.99)	0.88**	0.69	0.99	0.90	0.96
1:1 case control comparison	0.98	0.91 (0.83-0.97)	0.50****	0.88	0.95	0.95	0.89
(average of 1000 iterations on training set) (95% CI)				(0.88-0.88)	(0.95-0.95)	(0.94-0.95)	(0.89-0.89)

ROC: receiver operating characteristic; AUC: area under the curve; CI: confidence interval; PPV: positive predictive value; NPV: negative predictive value; LOO-CV: leave-one-out cross-validation. **: AUC>NIR: p<0.01; ****: AUC>NIR: p<0.0001.

discriminant models (training/validation set and 1:1 comparison) showed similar loading factors for the principal components that were incorporated as predictors (PCs 1–4, see table 3), thus suggesting a similar contribution of predictors on both models. Omitting the patients that were currently using OCS/antibiotics for respiratory worsening did not impact the discriminatory ability of the eNose (accuracy measures in supplementary table S3). Sensitivity analyses did not show an effect of smoking, health status score, use of ICS or vital capacity on the discriminatory ability of the eNose sensors. The results of these sensitivity analyses can be found in the supplementary material (supplementary table S5 and figures S1–3).

Discussion

This study shows that pattern recognition analysis of exhaled breath by eNose can discriminate with high accuracy between COPD patients on maintenance therapy who experienced an exacerbation within 3 months prior to measurement and those who did not. These results were internally validated and were confirmed in an independent validation set. Furthermore, smoking history, vital capacity during measurement, health status (CCQ score) and the use of ICS did not seem to affect this discriminatory ability. By discriminating between COPD patients who may or may not have experienced a recent exacerbation, point-of-care eNose measurements might be suitable to identify exacerbation-prone COPD patients. The next step is to prospectively collect evidence to confirm this ability.

This is the first study to use exhaled breath analysis by a point-of-care eNose to identify COPD patients who recently exacerbated. These results are in line with studies that showed an ability of eNose and GC-MS to discriminate between periods of stable COPD and acute exacerbations [12, 13]. Furthermore, the current study supports earlier findings showing differences in exhaled metabolic patterns between frequent exacerbators and stable COPD patients [9], infectious/non-infectious COPD exacerbations [11] and data from a pilot study that showed (moderate) ability to discriminate between bacterial/viral infections and stable COPD patients [14]. The ability to detect recent exacerbations shows promise as a means of monitoring COPD patients, as VOCs in exhaled breath have already proved useful in predicting asthma exacerbations in children [10] and predicting response to treatment with OCS in asthma patients [23].

A recent study by Brinkman *et al.* [24] further strengthens this promise, as it showed that in asthma, both GC-MS and eNose are able to correctly classify loss of control in asthma *versus* recovery and *versus* baseline measurements. The eNose used in the current study, the SpiroNose, allows real-time measurements and is easy to use in a clinical setting. In contrast, previous studies often used techniques

Training/validation model		Averaged 1:1 model		
	LD1		LD1 (95% CI)	
PC1	0.23	PC1	0.11 (0.11–0.11)	
PC2	-0.51	PC2	-0.63 (-0.64-(-)0.63	
PC3	-0.29	PC3	-0.12 (-0.13-(-)0.13	
PC4	1.17	PC4	0.84 (0.84-0.84)	

based on GC-MS, and although real-time analysis is possible [9], a major limitation for clinical application is the requirement for highly trained personnel [25].

Strengths of this study are the relatively large sample size, the internal and external validation steps that have been taken to further support the obtained results and the quick and easy-to-use point-of-care device that was employed. The patients who have been enrolled in the BreathCloud cohort were recruited in centres with different levels of care, and there was no need to cease medication use. This resulted in a mixed population that contains patients from primary care to specialised (academic) hospitals, reflecting the general COPD population. The use of physician-reported COPD diagnosis, however, does not rule out the possibility of misdiagnosed patients. Due to the skewed ratio of patients who had experienced a (recent) exacerbation *versus* those who did not, "no exacerbations" was expected to have a disproportionate effect on the outcome. The no information rate indeed showed a high probability to correctly classify the majority class (no exacerbations in our case), and therefore getting similar results with equally sized groups further strengthens our findings.

This was a retrospective study and the current results do not necessarily translate into a prospective scenario. A further limitation of our study is the lack of a new and completely independent validation cohort with similar patients measured with the same type of eNose. Because to our knowledge such a cohort did not exist, we consider the second-best option of dividing our cohort into a training and a validation set justified. Another important limitation of this study is the exacerbation definition. Exacerbations are complex and heterogeneous [26, 27], and thus the use of OCS or antibiotics to treat worsening respiratory complaints may be lacking in sensitivity and/or specificity. It may also be that the detected difference in eNose signals was caused by the administered OCS and antibiotics, as these signals may be influenced by metabolites of the medication. However, we have shown that omitting current OCS/ antibiotic users from the analysis did not change the outcomes. In this study, the timing of the exacerbations was not taken into account, *i.e.* some may have happened 3 months before measurement, some only a week, although the breath signal may be expected to change over time. Furthermore, due to the low number of subjects with >1 recent exacerbation (only 5 out of 36 subjects), we did not investigate the influence of number of exacerbations on exhaled breath profiles.

Earlier research suggested that eNose sensors are able to capture inflammatory profiles in patients [28, 29] and showed signs of a dose–response relationship with blood eosinophil and neutrophil levels [15]. This could suggest that flaring up of inflammation during an exacerbation provides a driving force in the changes in eNose fingerprints. Recently, a large study showed that VOCs identified by GC-MS in exhaled breath are able to discriminate between two important inflammatory phenotypes in asthma: eosinophilic asthma and neutrophilic asthma [30]. This suggests that inflammatory processes might show an effect on exhaled molecular breath patterns (or "breathprints"). Exacerbations have different underlying mechanisms and thus there are differences in metabolic (inflammatory) processes that are altered between different exacerbations [2, 31]. This seems contradictory to the accuracy found in the current study as these results point to a common denominator in all exacerbations. More detailed information on cause and nature of exacerbations could therefore be valuable in future studies.

Although some studies suggested that blood eosinophil levels may be useful to guide corticosteroid treatment in COPD patients and to predict exacerbations [5, 32], the strong signal in our results suggests that eNoses can detect more information on metabolic (inflammatory) processes than blood eosinophils or other biomarkers that are currently used. COPD exacerbations have a distinct signature in peripheral blood that persists for months following the event [33]. This blood signature could be reflected in an exhaled metabolic signature which is in line with our finding that the eNose was able to detect an exacerbation that had occurred up to 3 months prior to measurement. A recent study by VAN VELZEN et al. [13] could further support this, as their results suggested that exhaled breath patterns returned to baseline within 12 weeks after an exacerbation in COPD patients. This could imply that our data represent a signature of a recent previous exacerbation.

The identification of COPD patients who recently experienced an exacerbation by a noninvasive and easy-to-use tool could be of great value in monitoring of COPD patients. Early detection of patients who are unstable on treatment and prediction of risk for exacerbations have been named major clinical dilemmas in chronic diseases of airways [7] and may lead to new interventions that prevent lung deterioration and irreversible damage. A history of exacerbations is currently the best predictor for future exacerbations in COPD [34], and thus the results of the current study are promising. Our results suggest that exhaled breath analysis might be of value in predicting the risk for exacerbations. Future prospective studies should be conducted though to provide insight into the added value of exhaled breath analysis over currently used clinical symptoms. Another implication of our study is that heterogeneity in (exhaled breath composition of) COPD patients is a factor to be reckoned with in future studies. Patient selection

for comparisons with other disease areas should take into account that recent exacerbations in COPD patients could influence breath profiles.

In conclusion, exhaled breath analysis by SpiroNose can accurately identify COPD patients who have experienced an exacerbation during the previous 3 months. The current study suggests that COPD patients who recently exacerbated have their own exhaled molecular breathprint that could be valuable in monitoring of COPD patients. The present data merit an independent validation of our findings by the collection of prospective longitudinal data, which will allow testing as to whether exhaled breath analysis by eNose can predict exacerbations better than we can do at the present time on the basis of clinical symptoms.

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